
Welcome to
Advanced Skills
for
Modern Radiation Therapy
- RTT only -

Prague 2017

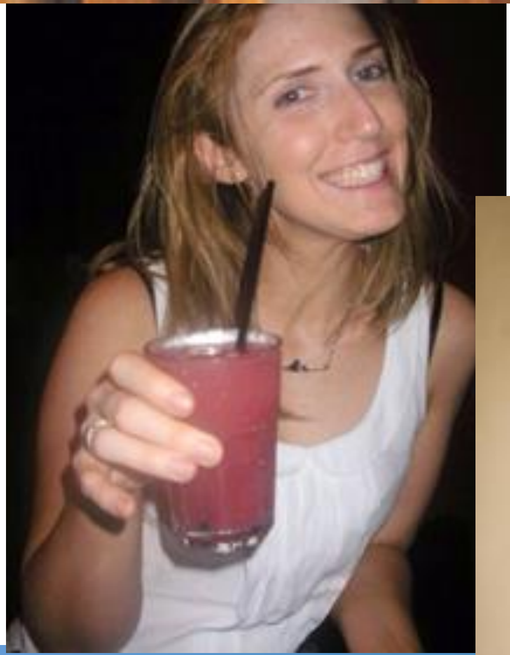
Fourth run!

- Amsterdag
- Copenhagen
- Dublin

Faculty of Nuclear Sciences and Physical Engineering

Local organizer:
Hana Stankusova, radiation oncologist
University Hospital Motol, Prague

Faculty



Elizabeth ‘Liz’ Forde - RTT -

Faculty

Mirjana
Josipovic
- Physicist -

REGION H

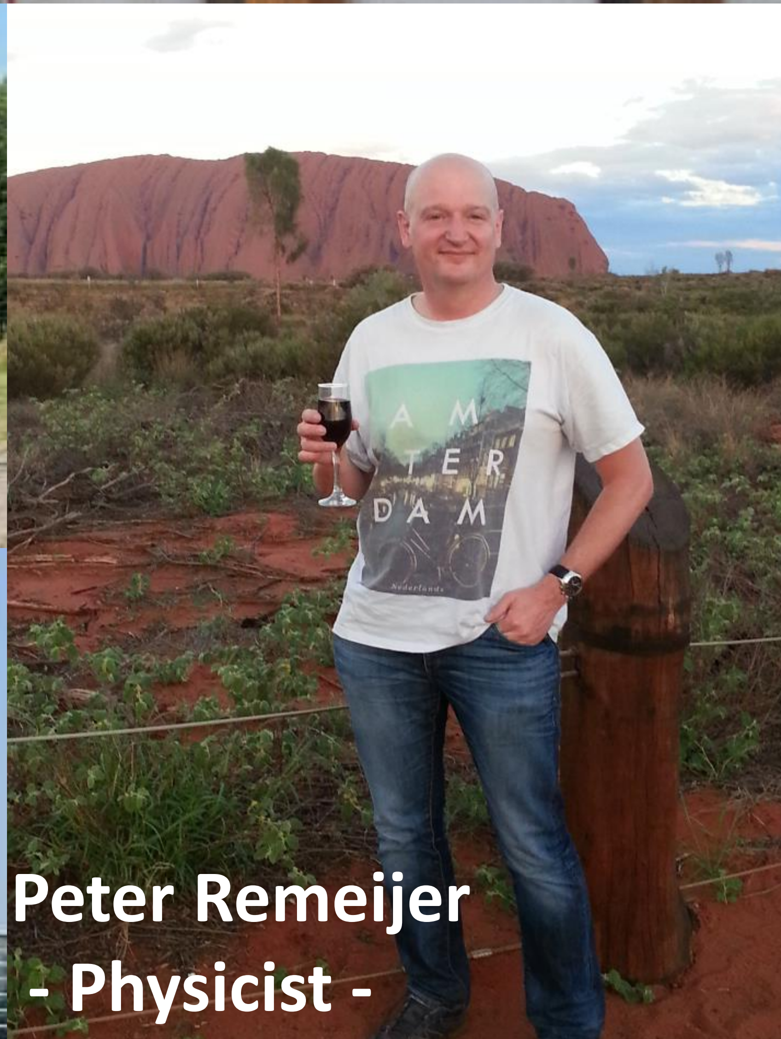
Rigshospitalet

Faculty

Faculty

Sophia Rivera
- Physician -

Faculty



Peter Remeijer
- Physicist -

Faculty

Jose Luis Lopez

- Physician -

Melissa Vanderijst

ESTRO – project manager

ESTRO
European Society for
RADIOTHERAPY
& ONCOLOGY

Rianne de Jong

Course Director - RTT

1 Australia
1 Austria
1 Bosnia Herzegovina
6 Czech Republik
5 Denmark
2 Malta
3 Poland
2 Portugal
2 Slovenia
1 Spain
2 Switzerland
5 Netherlands
3 Turkey
1 United Kingdom

34 Participants
+
7 Faculty
+
4 Company delegates
+
1 ESTRO

VARIAN medical systems

Elekta

ESTRO School

Program

4.5 days

24 lectures ~30 minutes

5 workshops

1 site visit

1 social event

ESTRO School

Social Event

Tuesday June 13

18.30 @Main Square Jan Hus Monument

Followed by Dinner

ESTRO School

Program

 - *All* steps of modern Radiation Therapy -

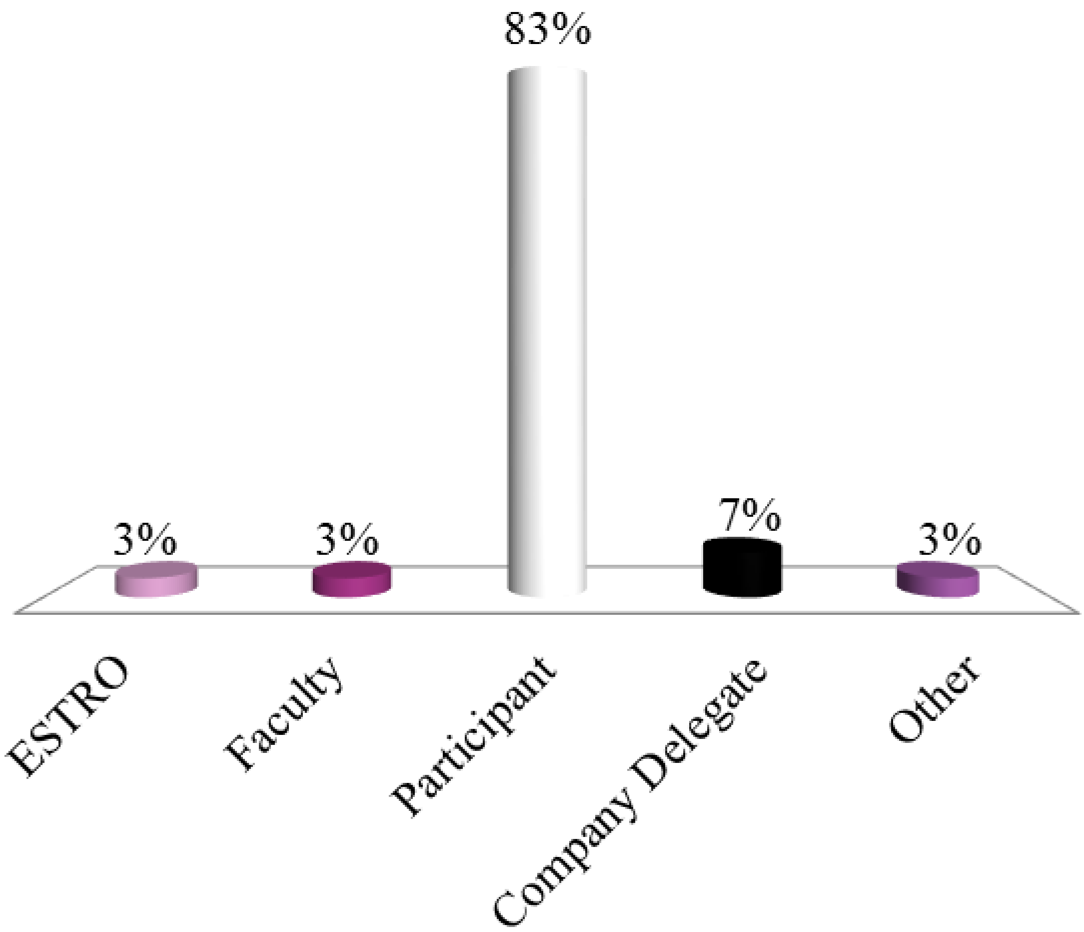
Turning Point

Turning Point

A little test!

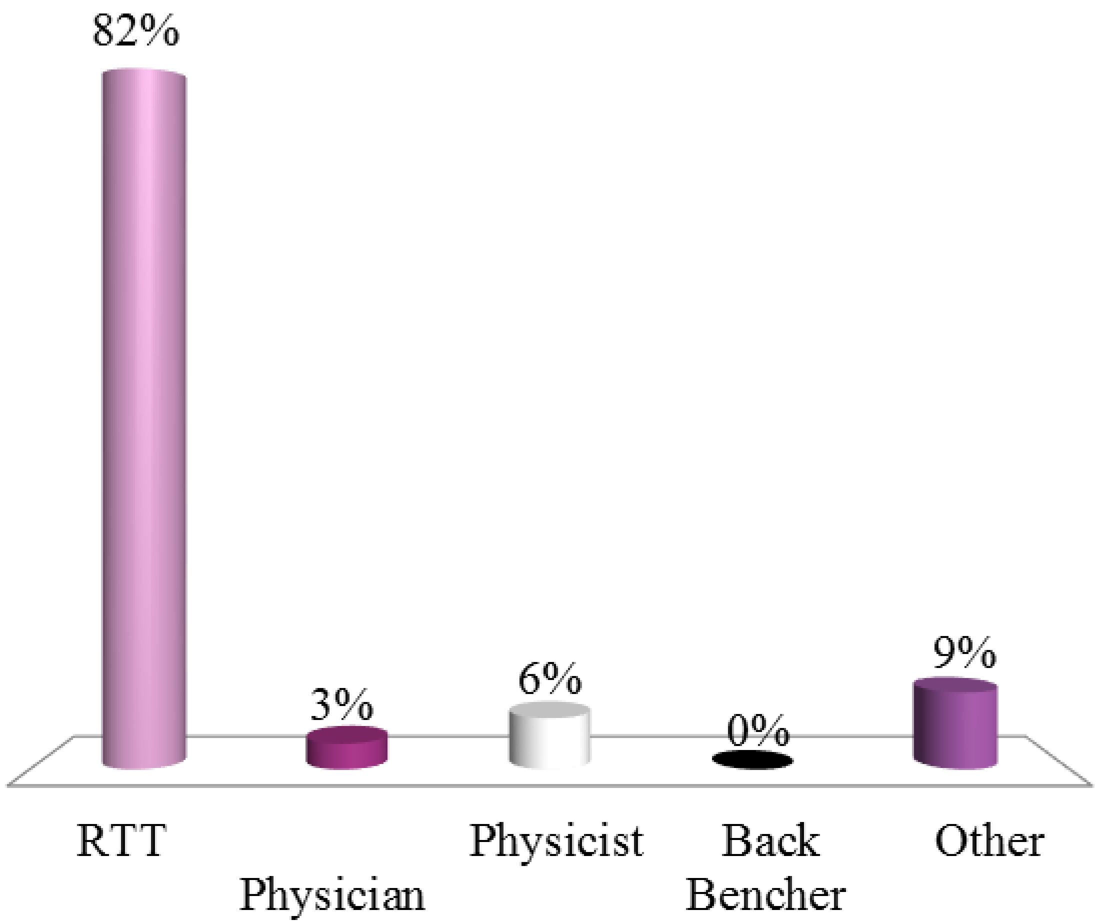
Who is in the room?

A. ESTRO
B. Faculty
C. Participant
D. Company Delegate
E. Other



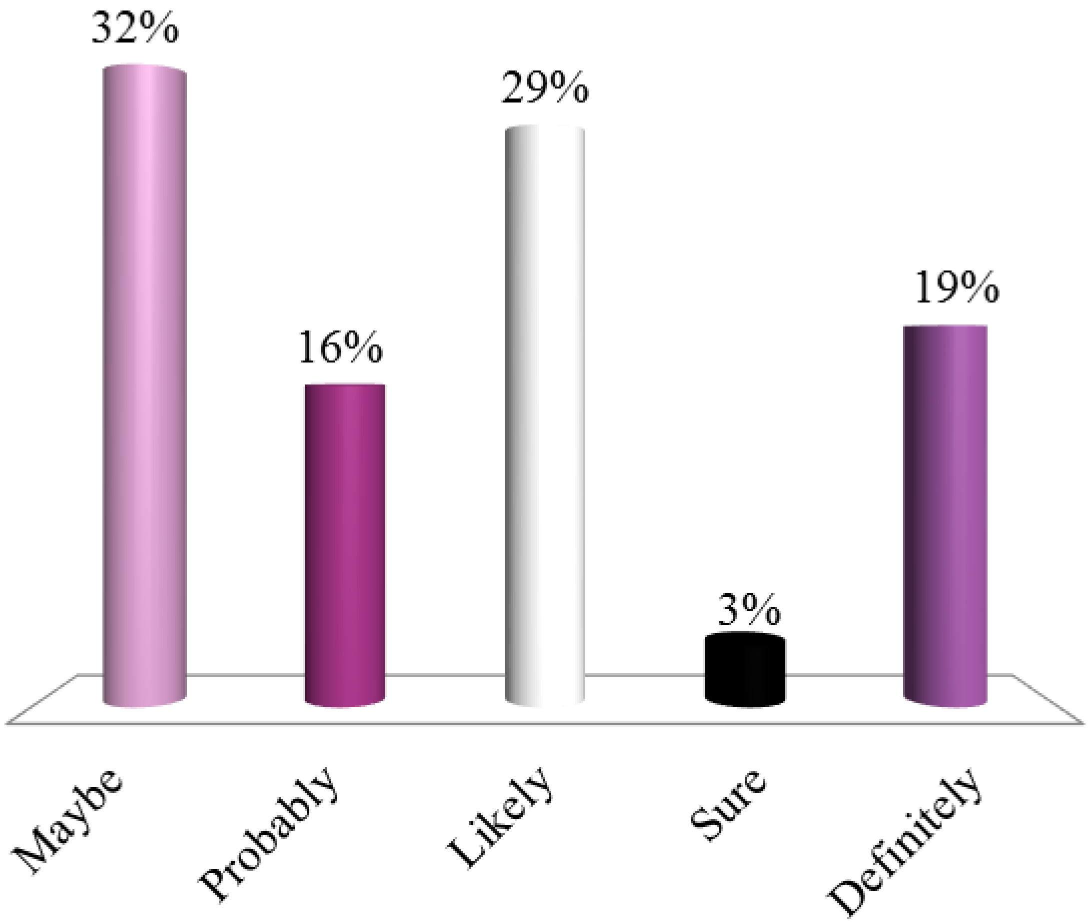
Who is in the room?

A. RTT
B. Physician
C. Physicist
D. Back Bencher
E. Other



Who is joining for beers @end of day?

A. Maybe
B. Probably
C. Likely
D. Sure
E. Definitely



Laptops – workshops

- Delineation
- Margin calculation
- Safety issues & prospective risk analysis

Questions?

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School

WWW.ESTRO.ORG/SCHOOL

RTT's Perspective on modern Radiation Therapy

Rianne de Jong *RTT,*
Academic Medical Centre
Amsterdam

NKI-AVL
Het Nederlands Kanker Instituut
Antoni van Leeuwenhoek Ziekenhuis

Prague 2017

m.a.j.dejong@amc.uva.nl

ESTRO School

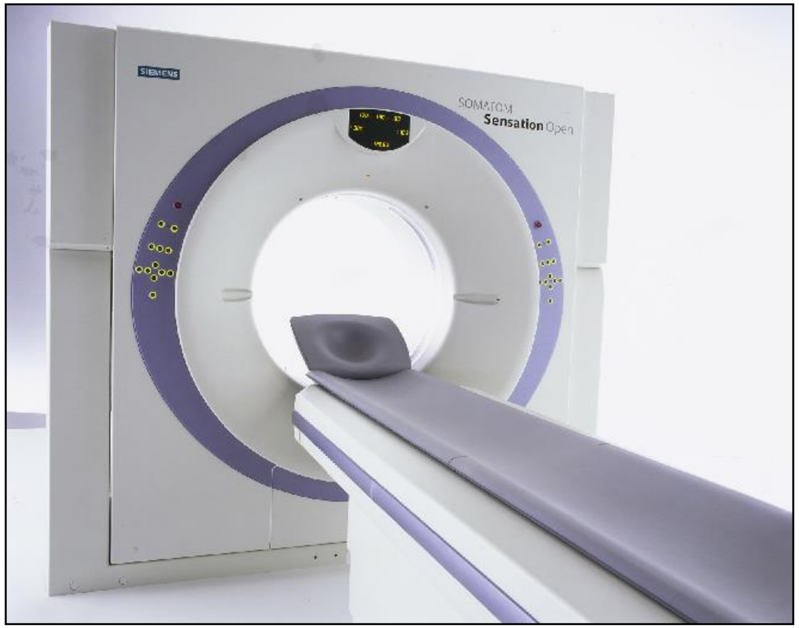
Introduction

Changes over the last years

Simulation:

from fluoroscopy to CT

2 D

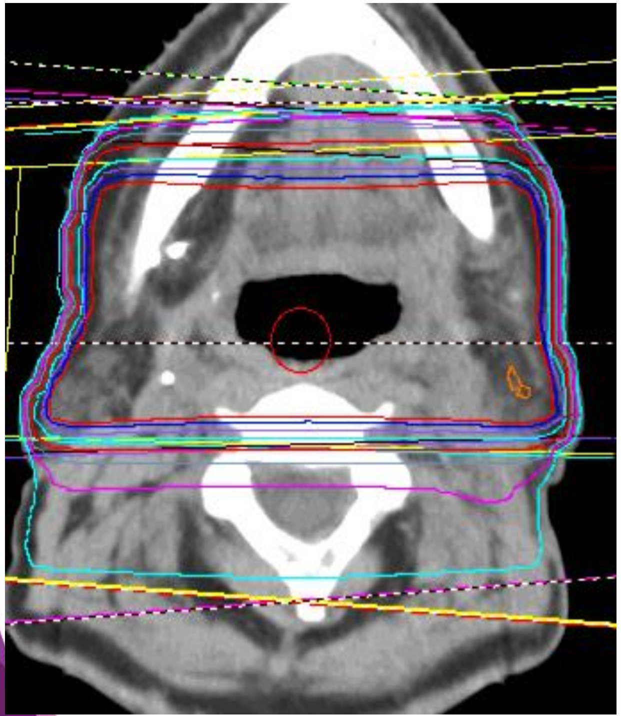


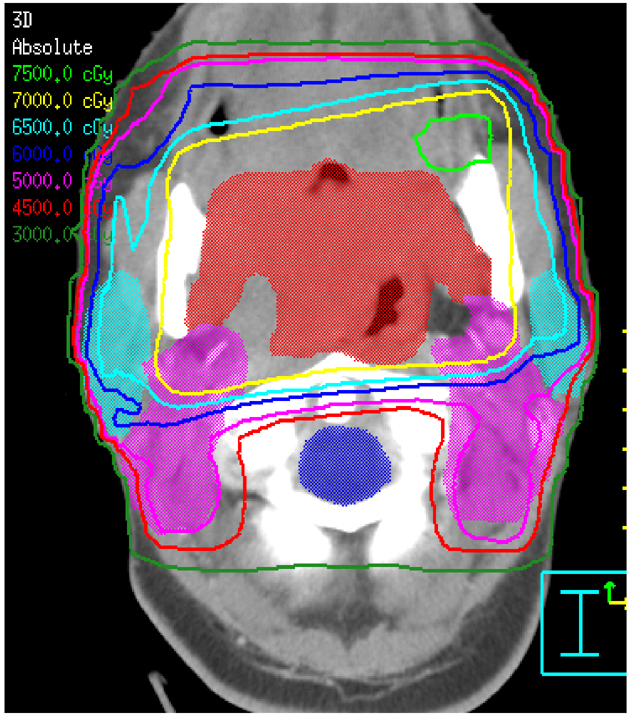
3 D

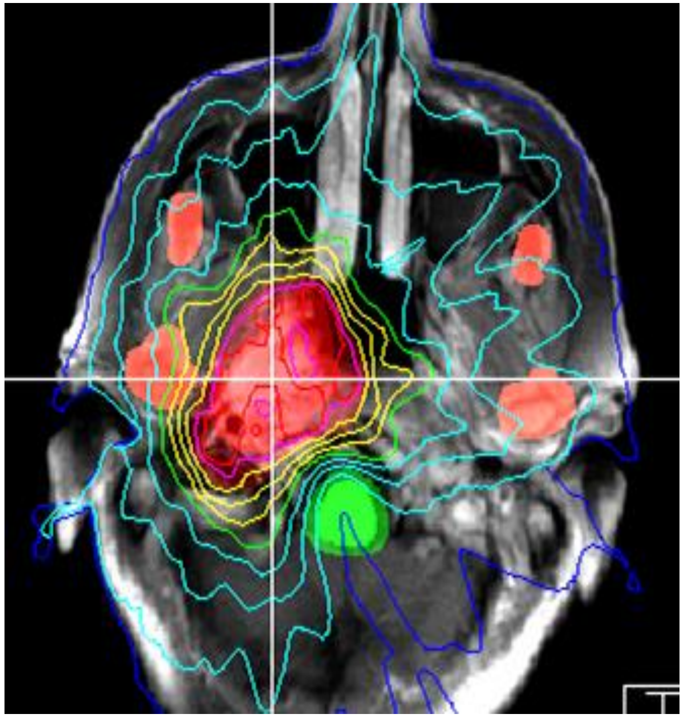
Introduction

Treatment planning:

from conventional to conformal to IMRT & arc therapy







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Introduction

Treatment machine:

From patient set-up with skin marks to additional patient set-up verification

- Portal imaging (2D MV)
- Kilo voltage imaging (3D kV)



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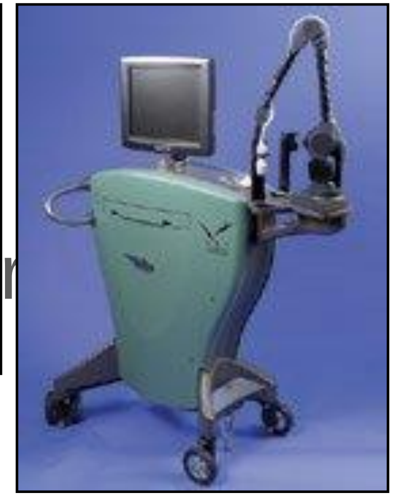

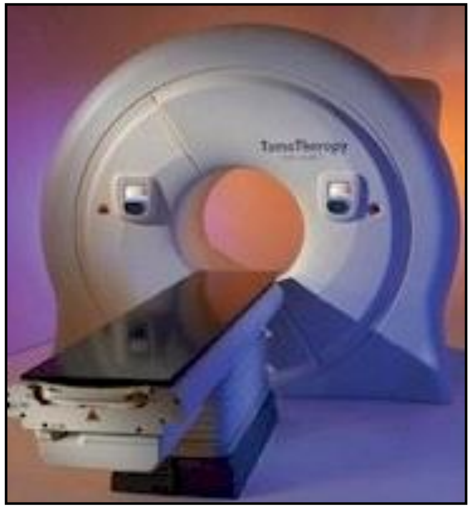

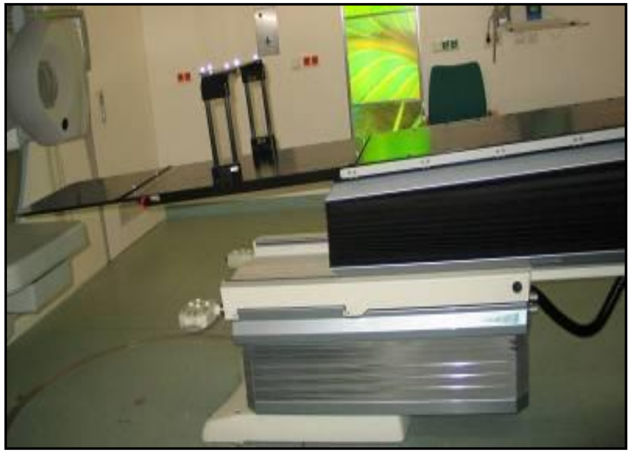

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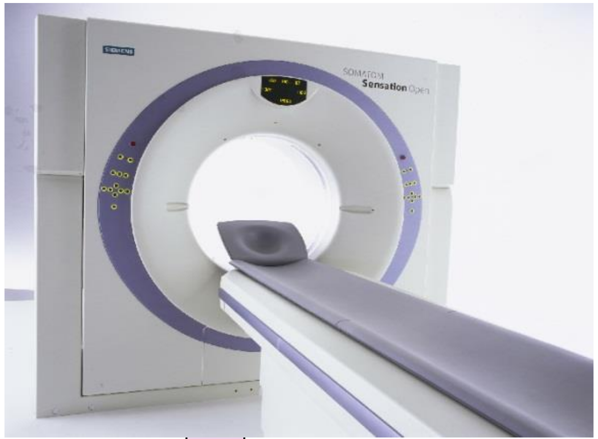
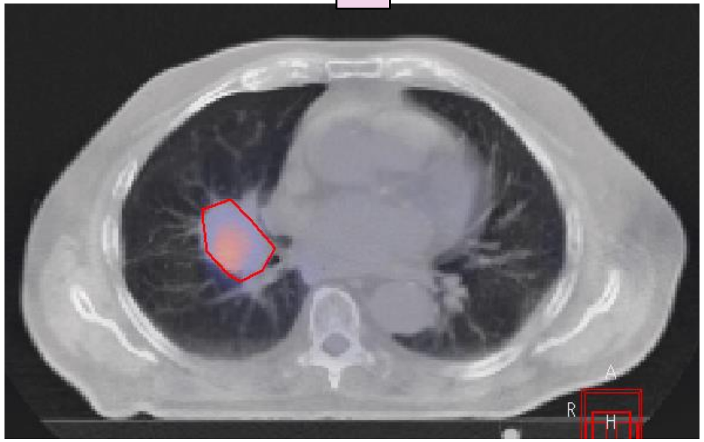
Introduction

Tattoo, align and scan patient





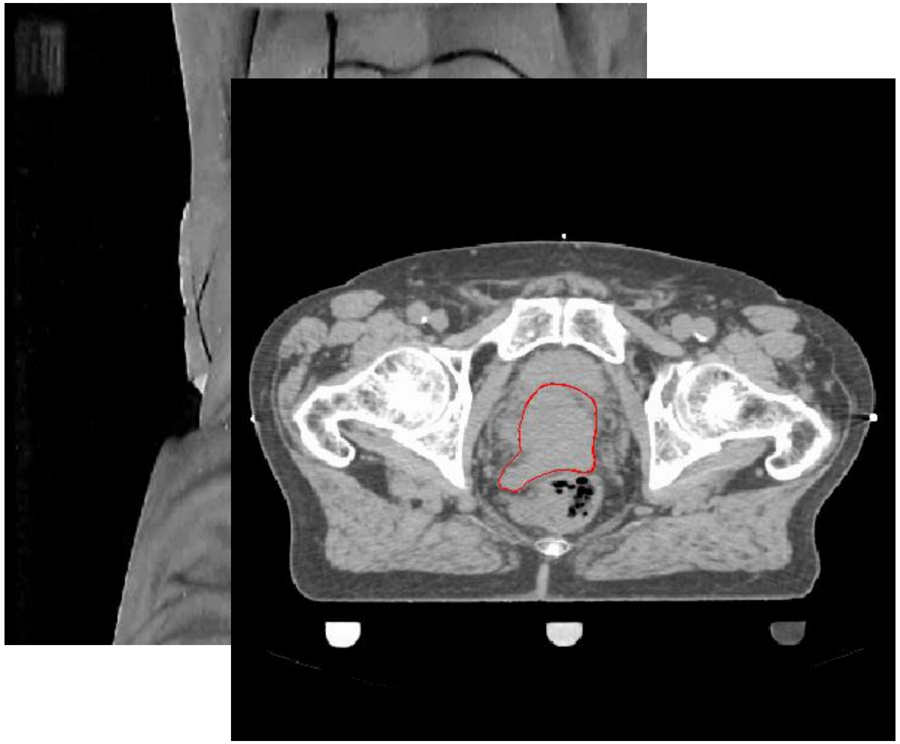
Draw target and plan treatment on RTP

Align patient on machine on tattoos and treat (many days)

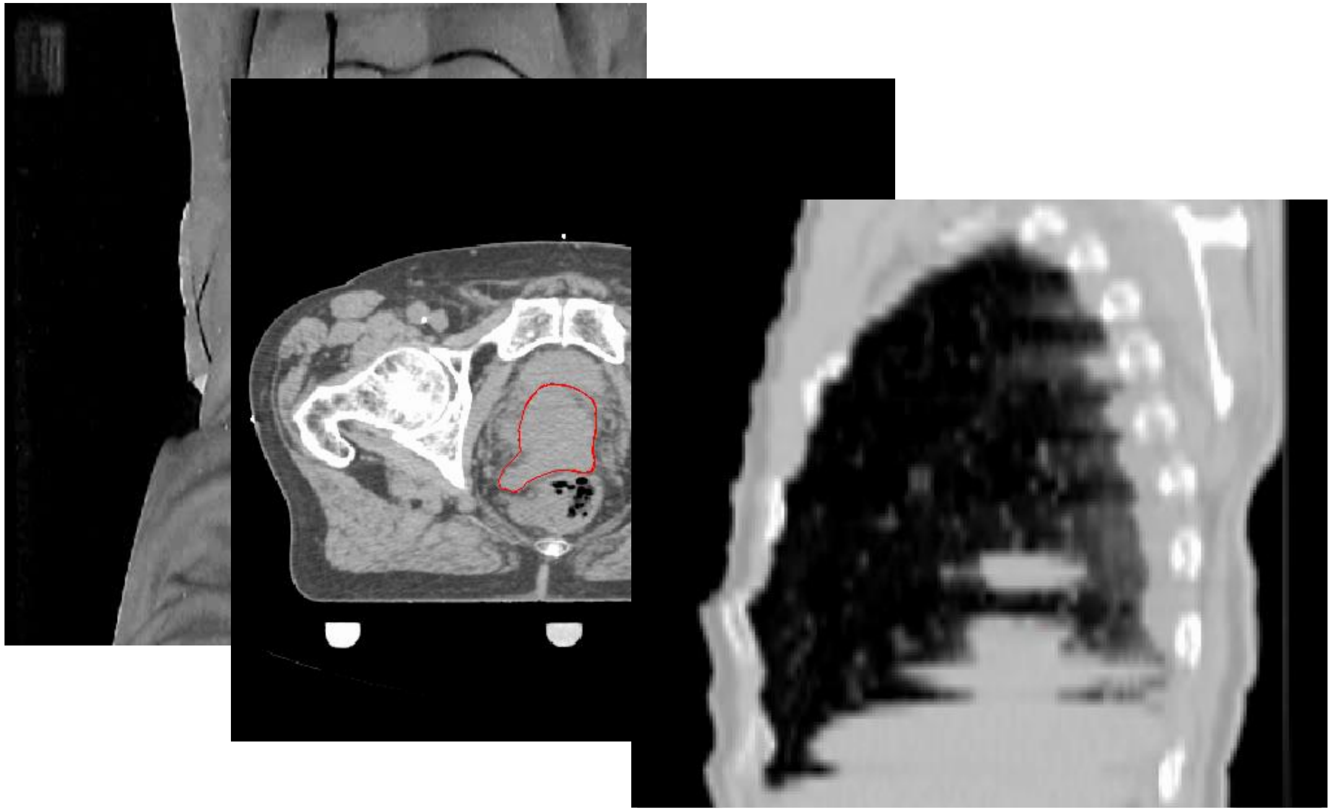
In principle this procedure should be accurate…

Introduction

Introduction

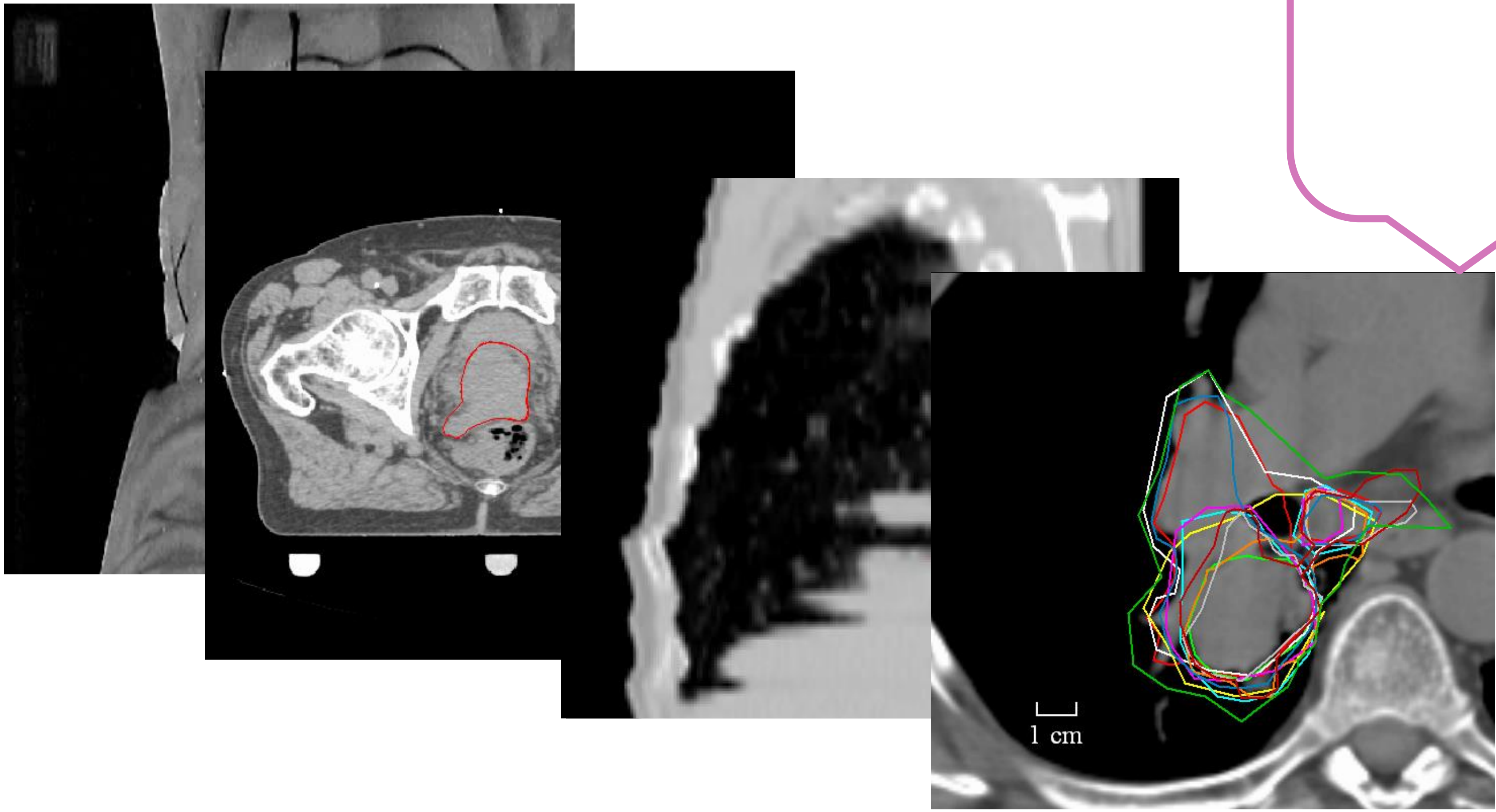


Introduction

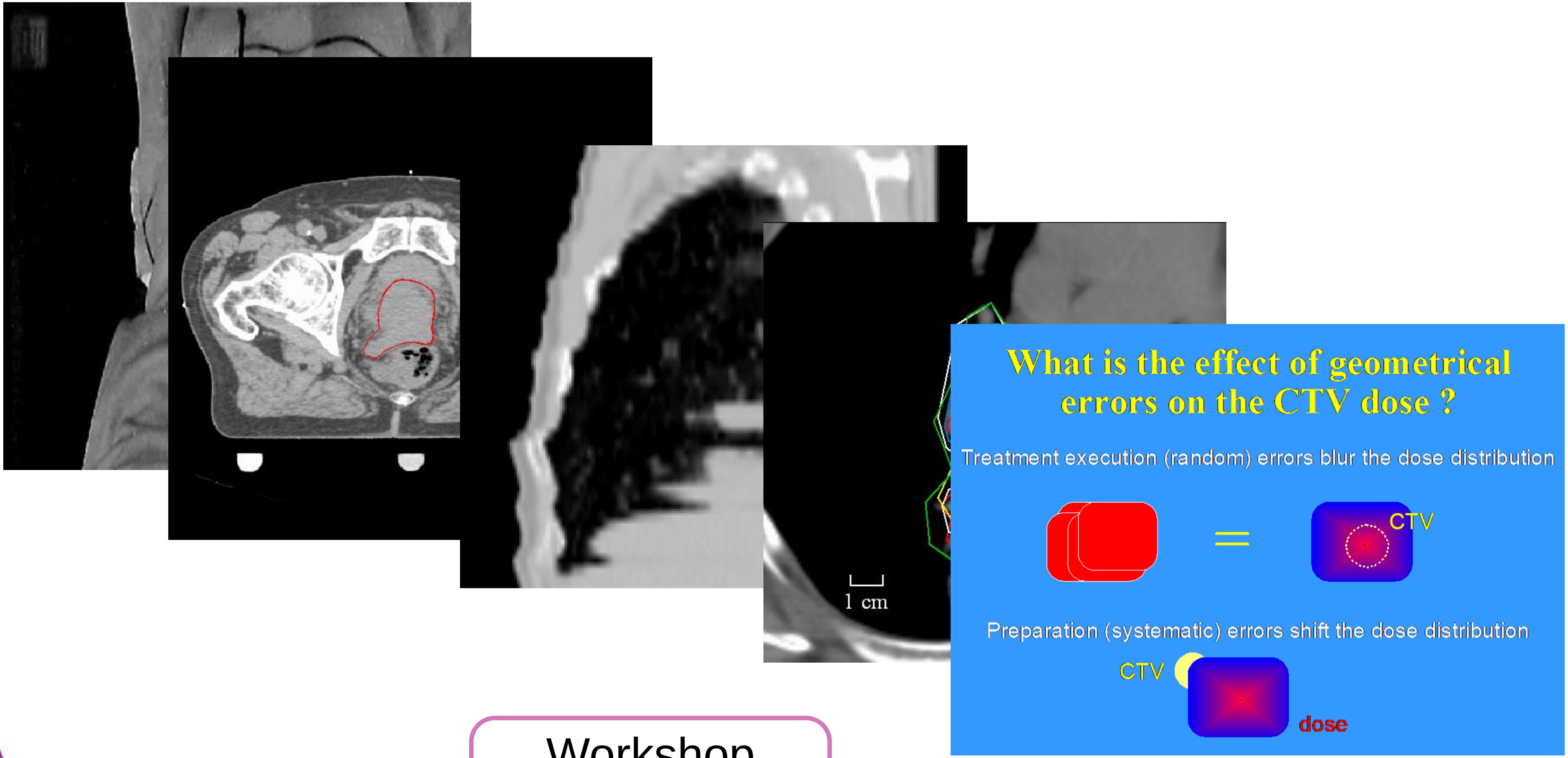


Introduction

Workshop
Sofia
Elizabeth
Jose
Peter



Introduction



Workshop
Peter

RTT's Job

The RTTs job

- Patients education
  - Pre-treatment imaging
- Simulation
- Treatment Planning
- Treatment
  - *Image guidance*
  - *Research & Development*

→ Some sort of specialization in one step of the treatment chain:

Sometimes controversial: all-round RTT is considered optimal job description.

Patient education

2 departments, 2 solutions:

AMC	AvL
• 4 RTTs	3 RTT's assistent
• 20%	80% time spent
• 30%	100% patient coverage
• Combined	not combined with working on treatment machines

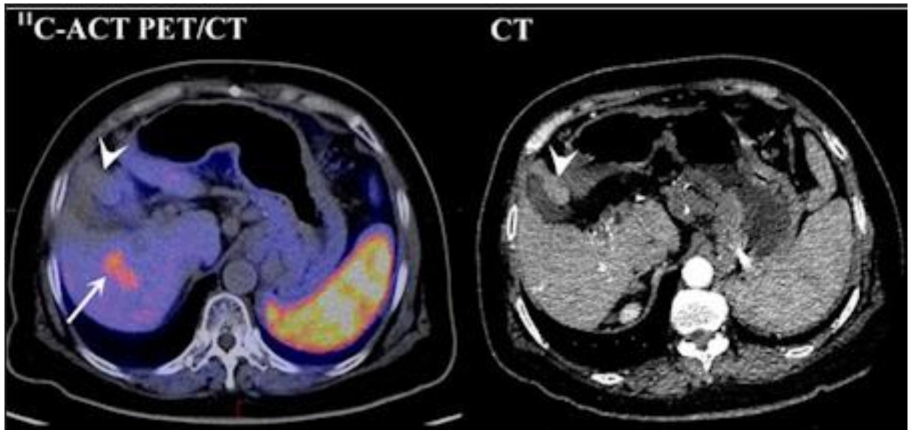
Only 1 slide…? *Very important to the patient!*

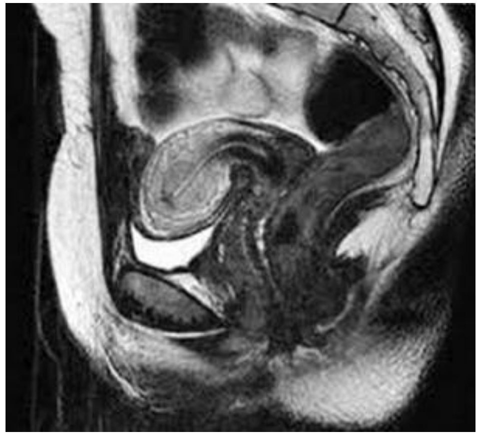
Pre-treatment Imaging: PET/MRI/CT

Often combined use with radiology department:

Always one RTT from radiation therapy

- Trained in delivering contrast agents
- Focused on patient positioning: registration images for delineation





Simulation CT

RTTs working on CT combined with working on the treatment machines

Sub group only working on CT

- Contrast agents
- 4D CT
- Breath hold CT

Treatment Planning

RTTs working on Treatment Planning combined with working on the treatment machines.

Sub group working treatment planning only – research and development.

Physicist only in the loop when outside of tolerance Physician have to sign off on the plans

- Multi modality registrations
- Delineation of Organs at Risk
- IMRT → VMAT (all curative intent treatments)

Treatment

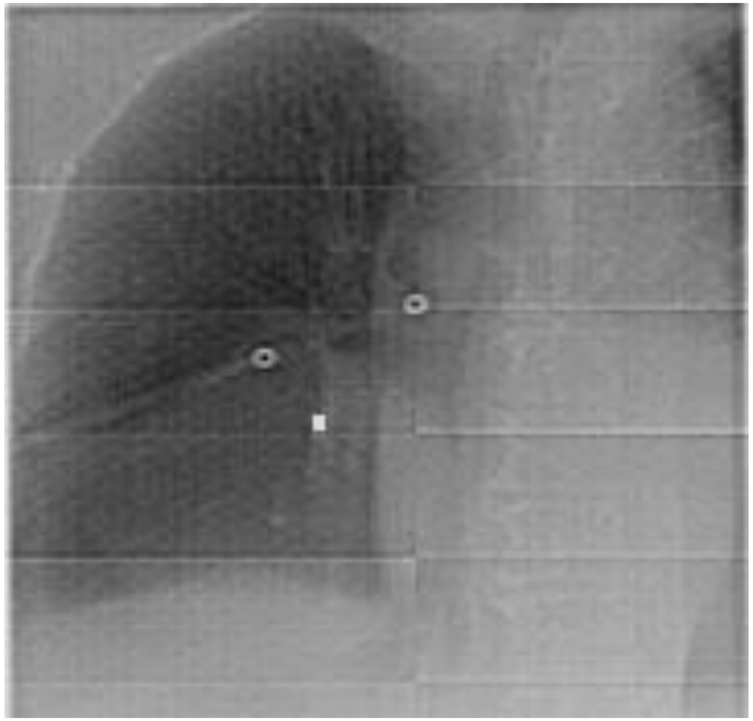
3 RTTs per machine when breaks are scheduled

4 RTTs per machine for full program

Patient Support

Support patients and their relatives and friends:

During RT in RTT's working area for support and transparency

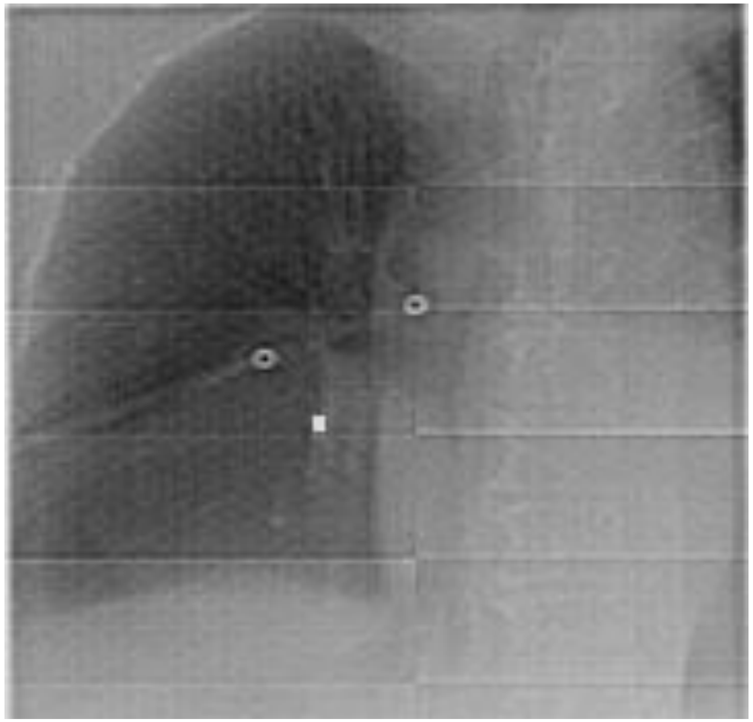


Portal image

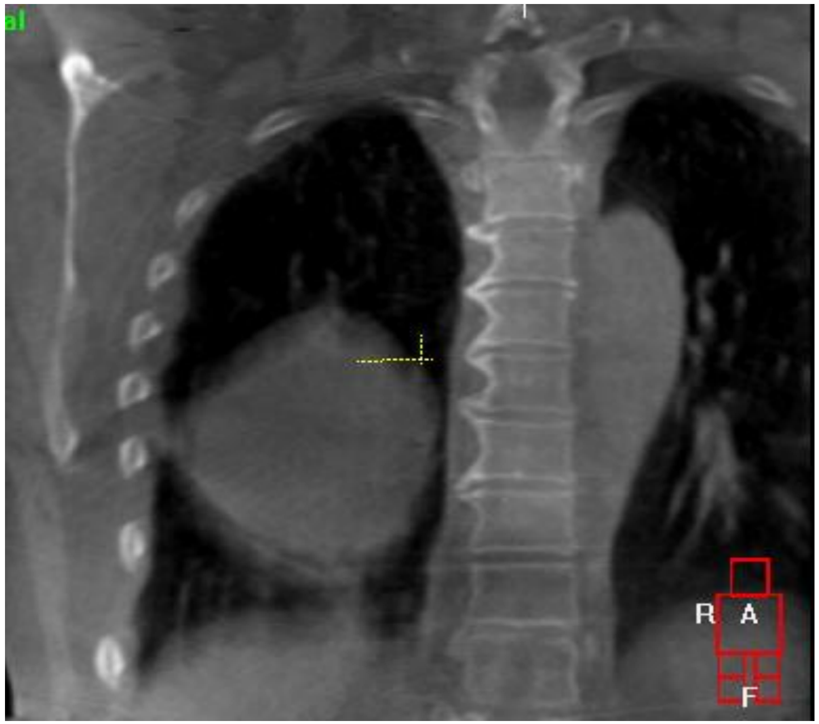
Patient Support

Support patients and their relatives and friends:

During RT in RTT's working area for support and transparency



Portal image



CBCT image

Starting IGRT (3d)

IGRT

- It is at the end of the treatment chain
- It involves all RTTs! Not only working on the treatment machine
- It requires understanding of all steps in radiation therapy
- It is still evolving: MRI-linac!

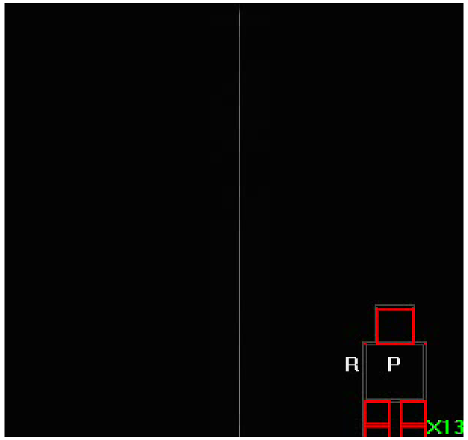
Implementing CBCT

June 2003:

- 4 RTT's
- 2 Physicists
- Patient program in the morning
- CBCT in the afternoon
- 8 months of validation

Implementing CBCT: validation of the system

3D match



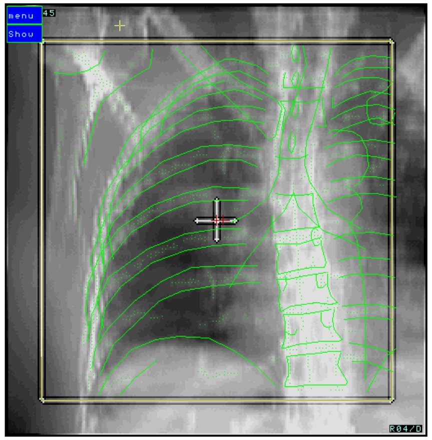
Cross validation

Planning CT

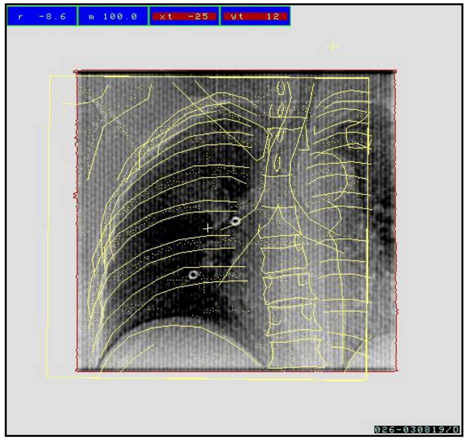
same ?

Cone beam CT

DRR +Template



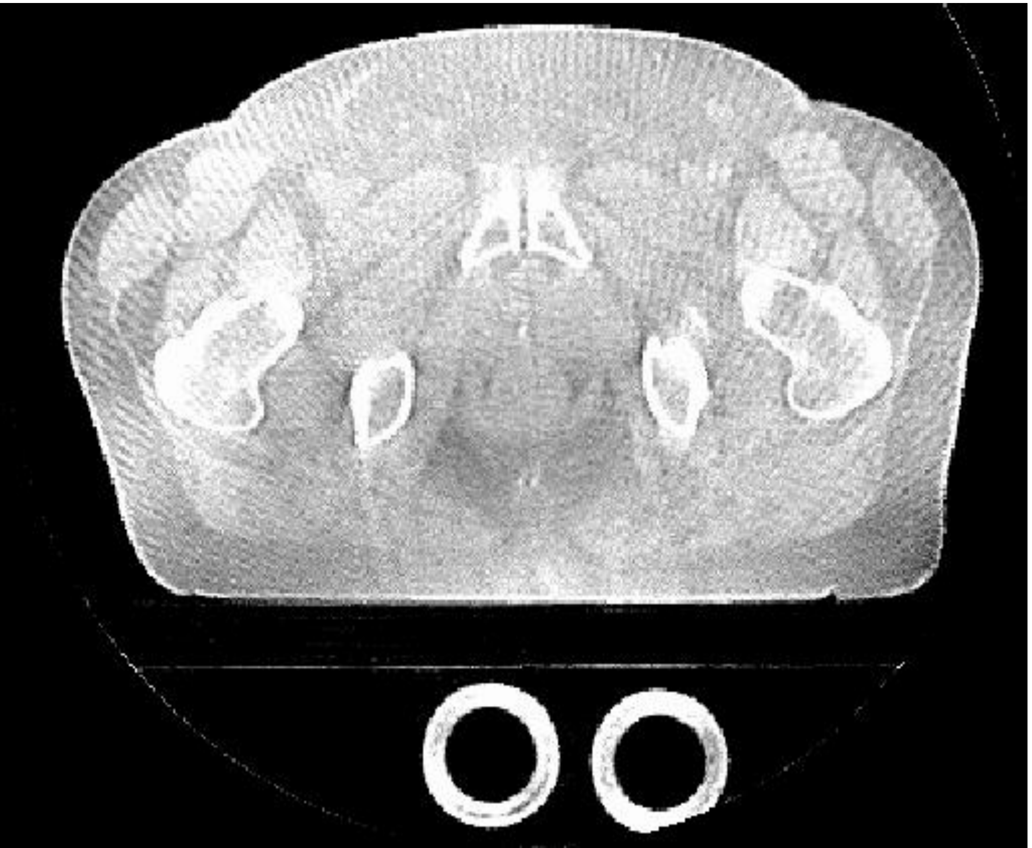
MV image

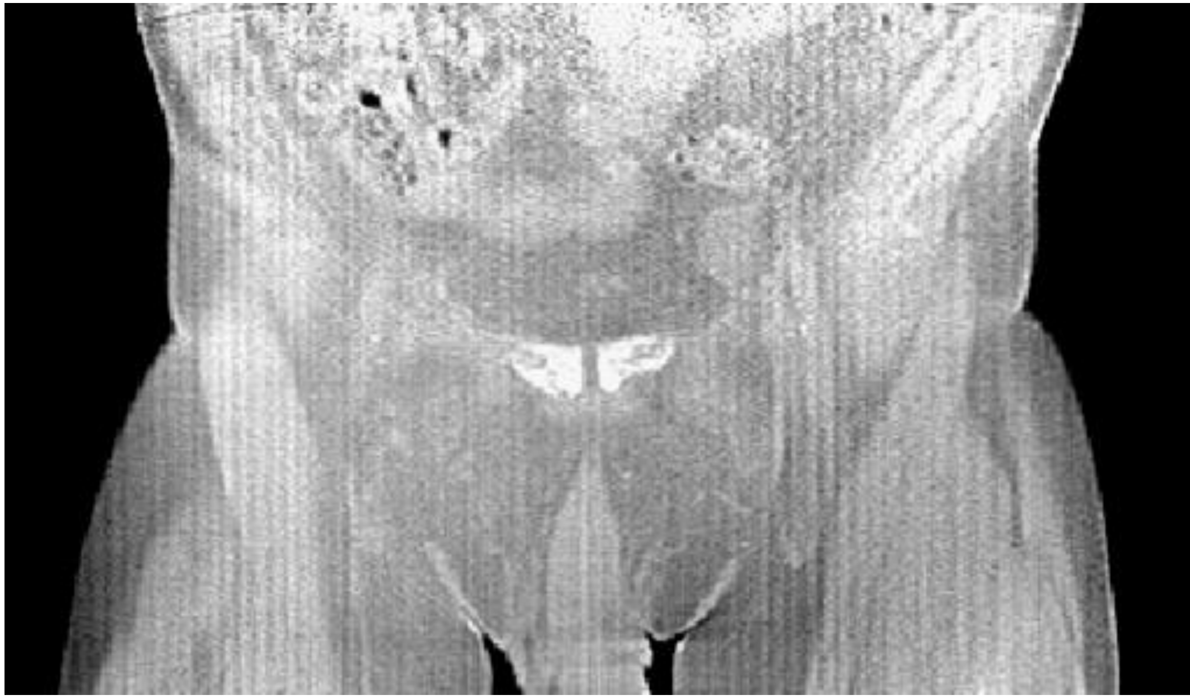


2 x 2D match AP/LAT

Implementing CBCT: designing imaging presets

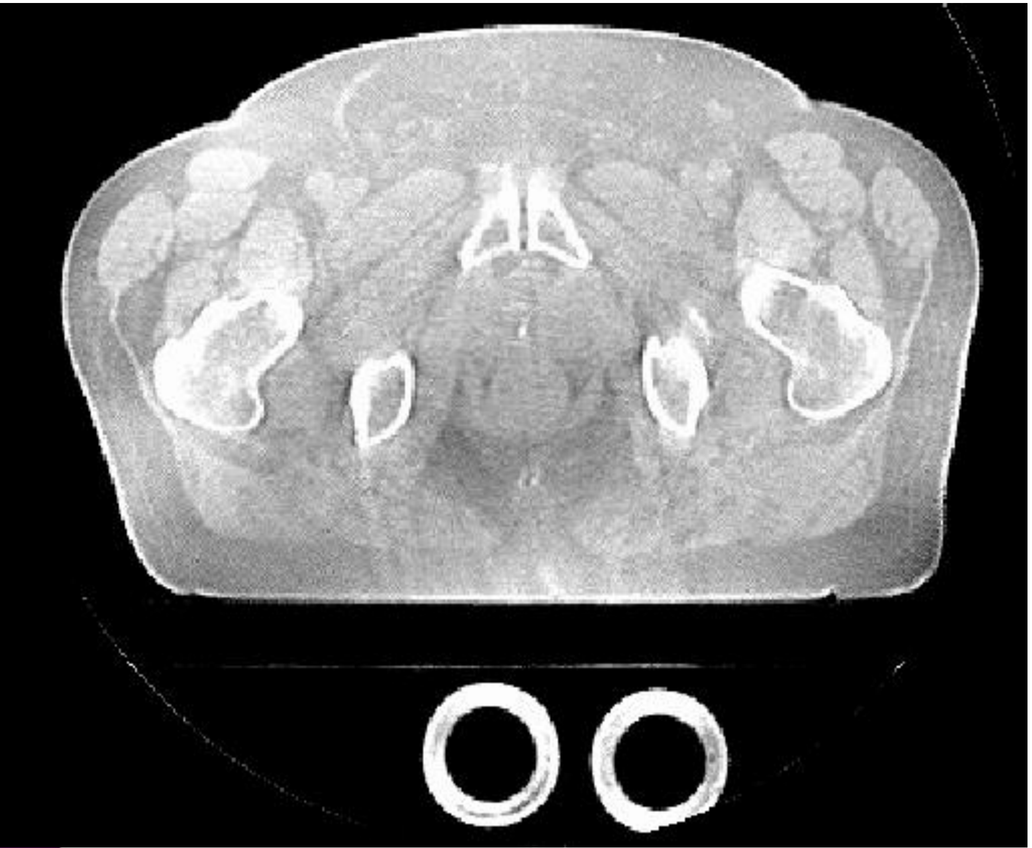
320 Projections 1.5 – 3 cGy





Implementing CBCT: validation of the system

640 Projections 1.5 – 3 cGy



Implementing CBCT:
role of RTT

- Understanding basic physics and technical aspects of new imaging modality
  - IQ: artefacts
- Implementing in daily workflow
  - Protocols, manuals and working instructions
- Setting up training program for RTT's

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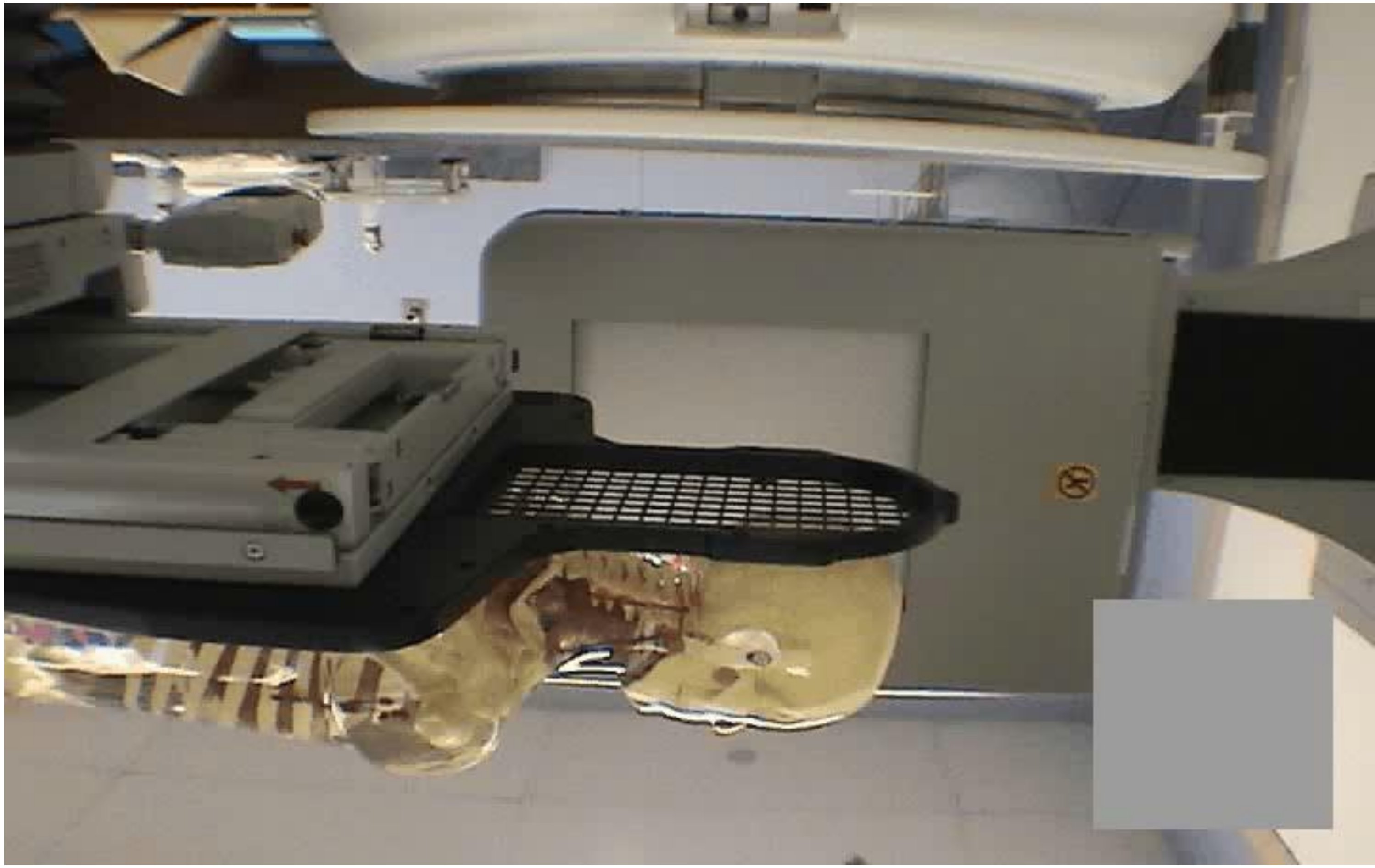
Starting clinical use of CBCT

RTT's responsibilities:

- Acquisition of CBCT
- Registration bony anatomy (CBCT)
- Evaluation registration (CBCT)
- Evaluation of treatment !
- Execute decision rules off-line and on-line protocols

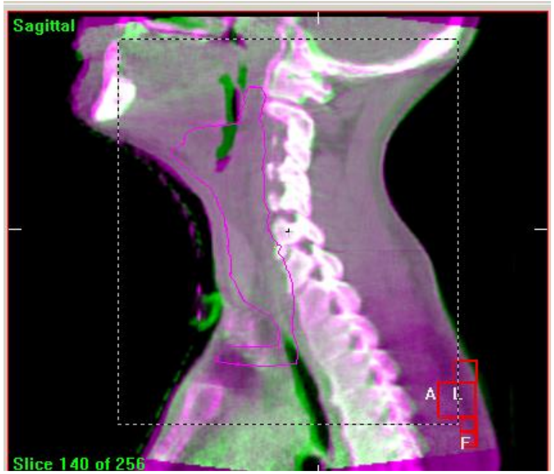
→ Same as portal imaging and a bit extra

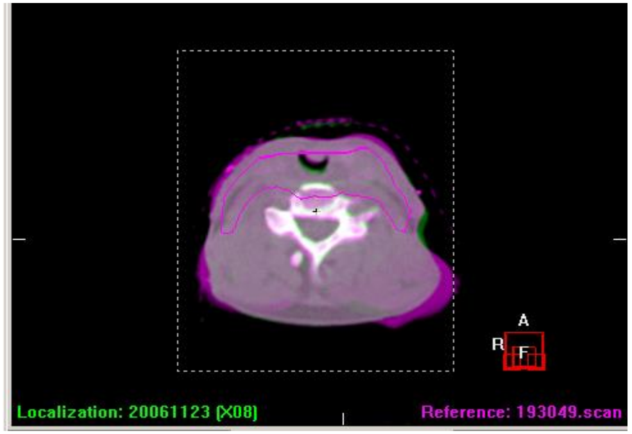
Clinical daily routine



Courtesy to Doug Moseley (PMH) Jan-Jakob Sonke (AvL)

Clinical daily routine - registration

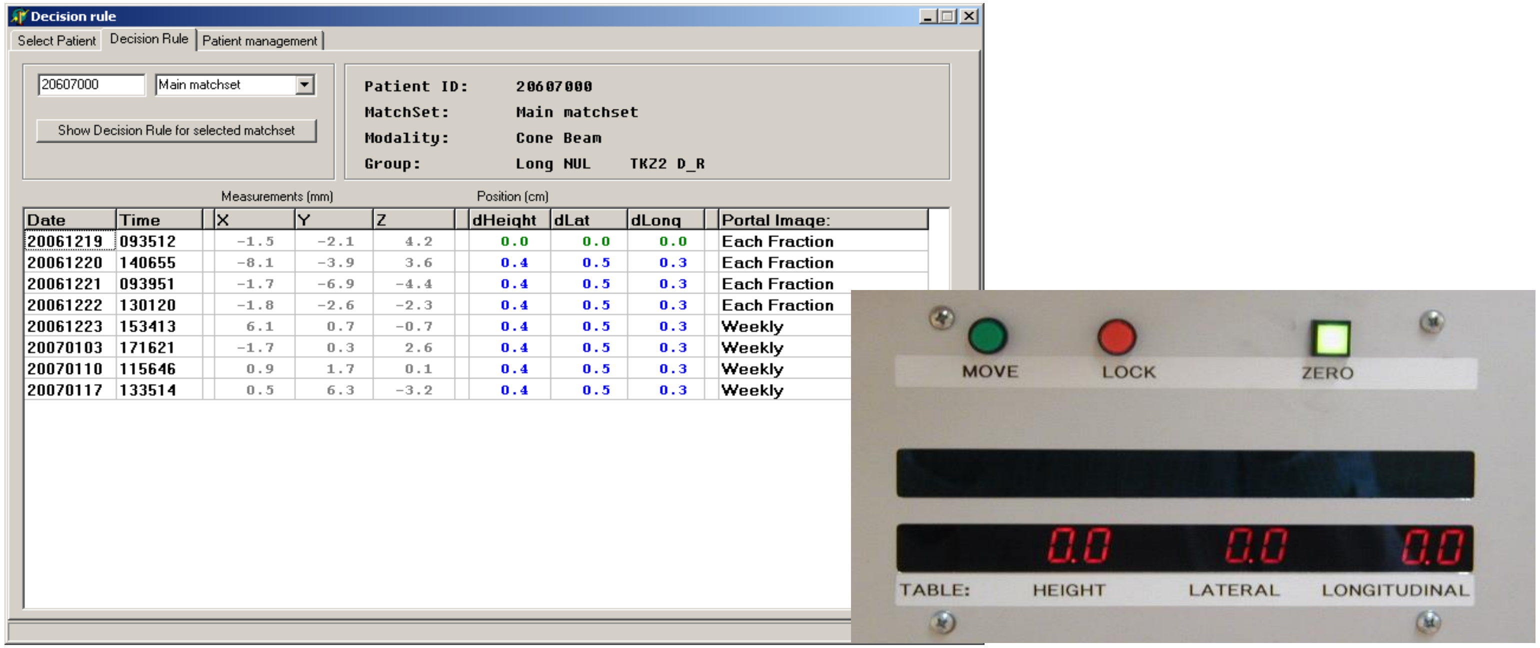




Automatic registration

CBCT scan

KV imaging – off/online correction



Decision rule

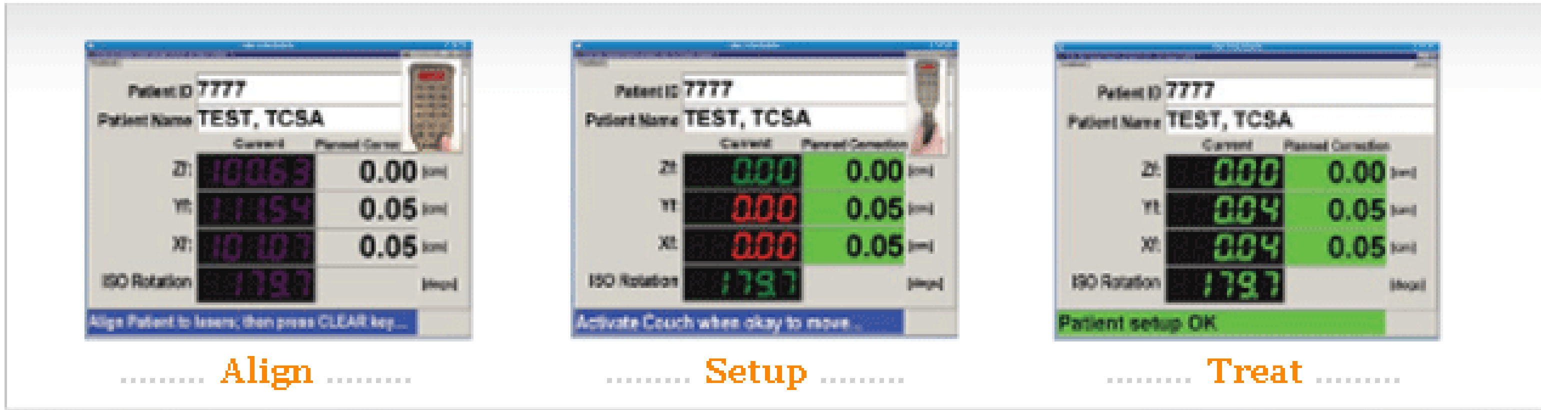
Select Patient | Decision Rule | Patient management

20607000 | Main matchset

Show Decision Rule for selected matchset

Patient ID: 20607000
MatchSet: Main matchset
Modality: Cone Beam
Group: Long NUL TKZ2 D_R

Date	Time	X	Y	Z	dHeight	dLat	dLong	Portal Image:
		Measurements (mm)			Position (cm)			
20061219	093512	-1.5	-2.1	4.2	0.0	0.0	0.0	Each Fraction
20061220	140655	-8.1	-3.9	3.6	0.4	0.5	0.3	Each Fraction
20061221	093951	-1.7	-6.9	-4.4	0.4	0.5	0.3	Each Fraction
20061222	130120	-1.8	-2.6	-2.3	0.4	0.5	0.3	Each Fraction
20061223	153413	6.1	0.7	-0.7	0.4	0.5	0.3	Weekly
20070103	171621	-1.7	0.3	2.6	0.4	0.5	0.3	Weekly
20070110	115646	0.9	1.7	0.1	0.4	0.5	0.3	Weekly
20070117	133514	0.5	6.3	-3.2	0.4	0.5	0.3	Weekly



Managing IGRT
(3d)

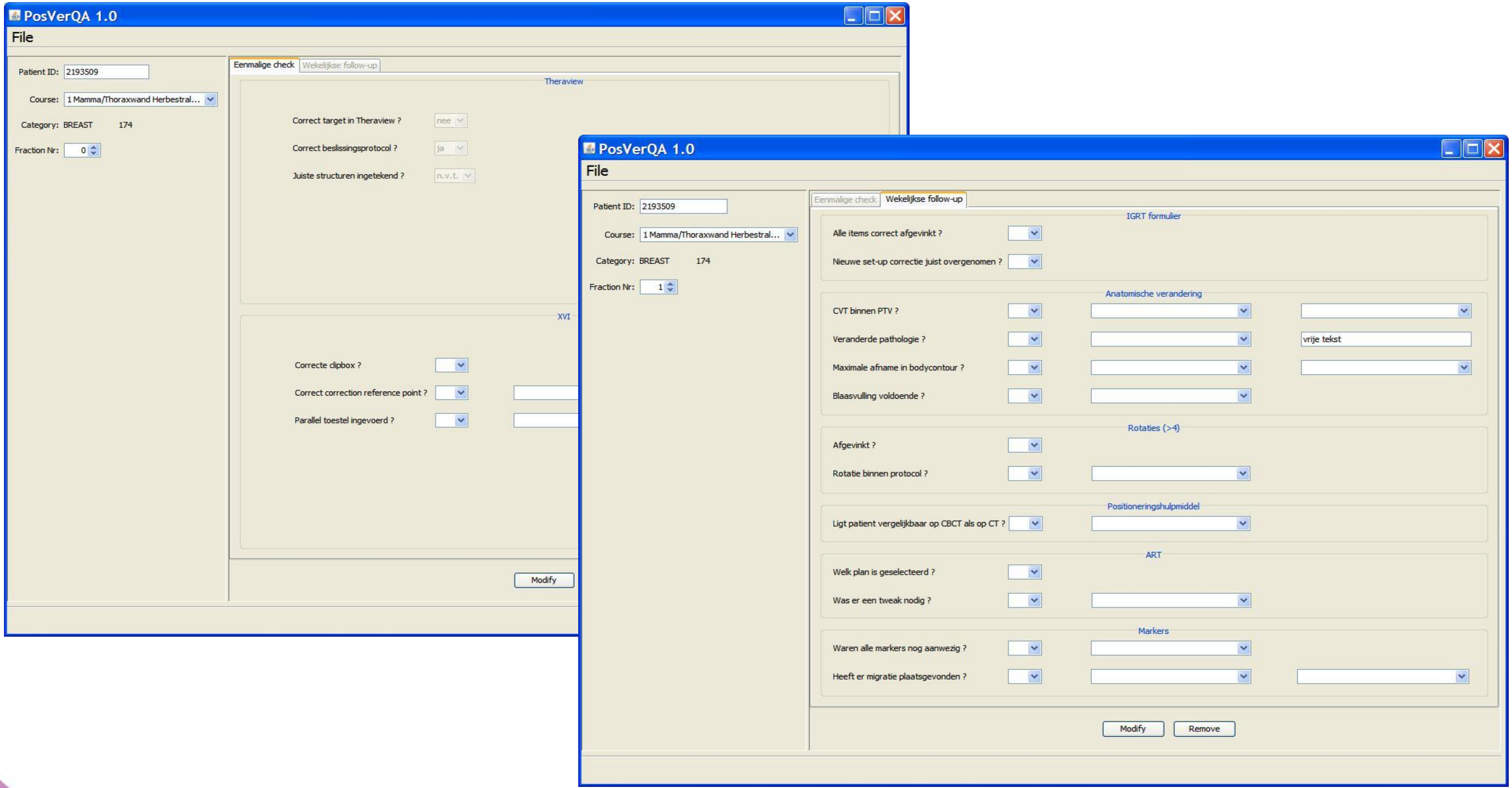
Managing CBCT

@AMC

5 RTT's with a focus on IGRT:

- **Track, check patients**
- First contact of changes occur
- Training and education
- Manuals and protocols
- Data collection & handling

Track & check patients



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Managing CBCT

@AMC

5 RTT’s with a focus on IGRT:

- Track, check patients
- **First contact of changes occur**
- Training and education
- Manuals and protocols
- Data collection

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Anatomical Changes

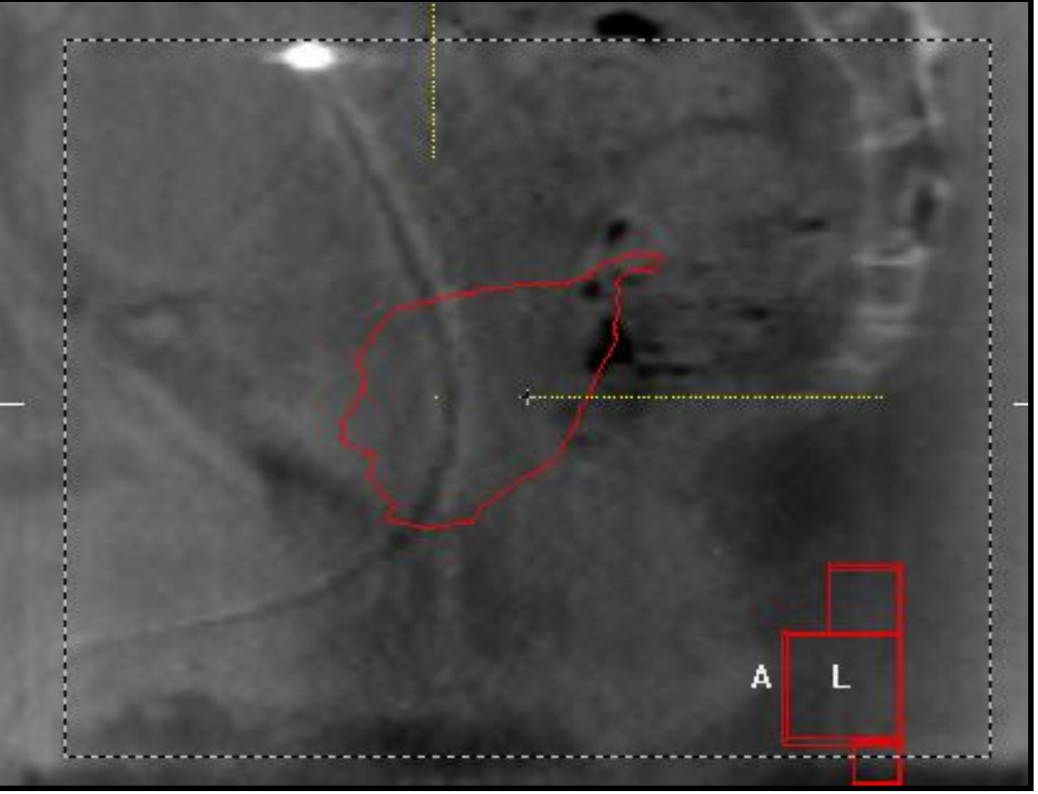
RTT should be trained in:

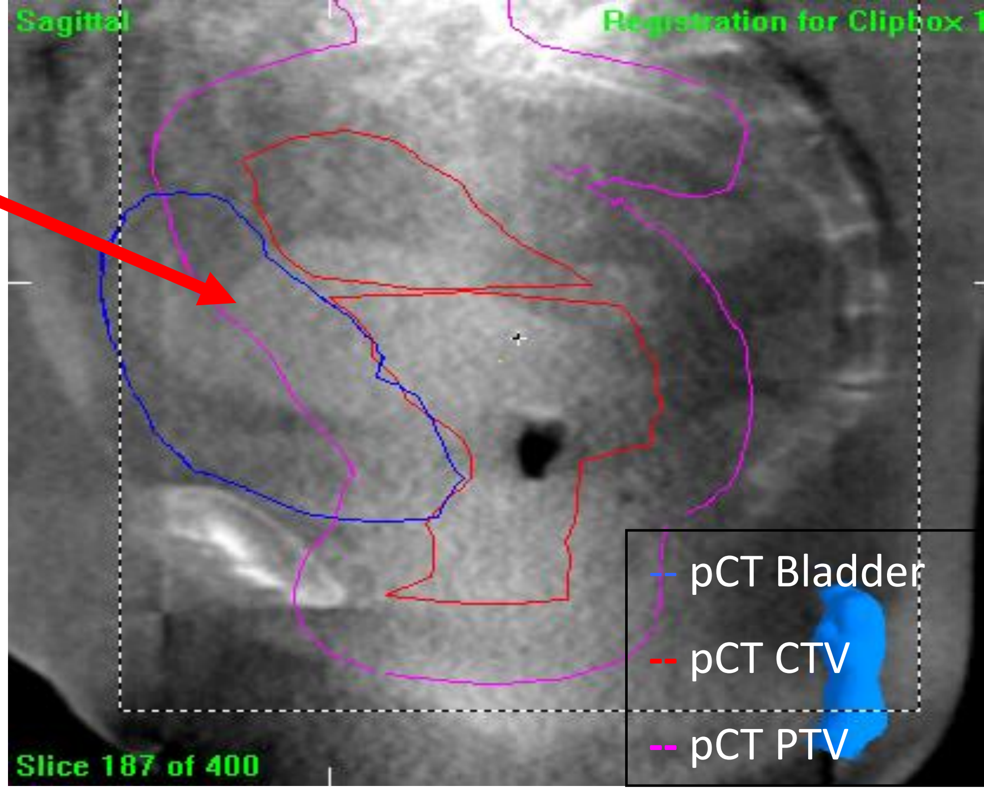
Recognizing patient changes/anatomical changes that have an influence on radiation treatment: Target coverage and/or dose distribution

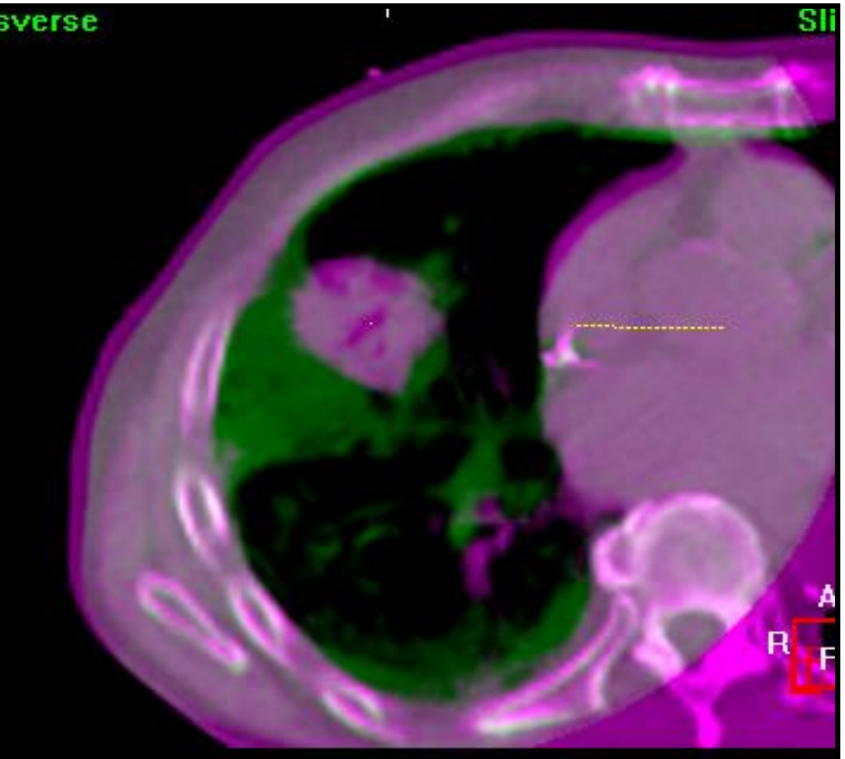
&

RTT should have:

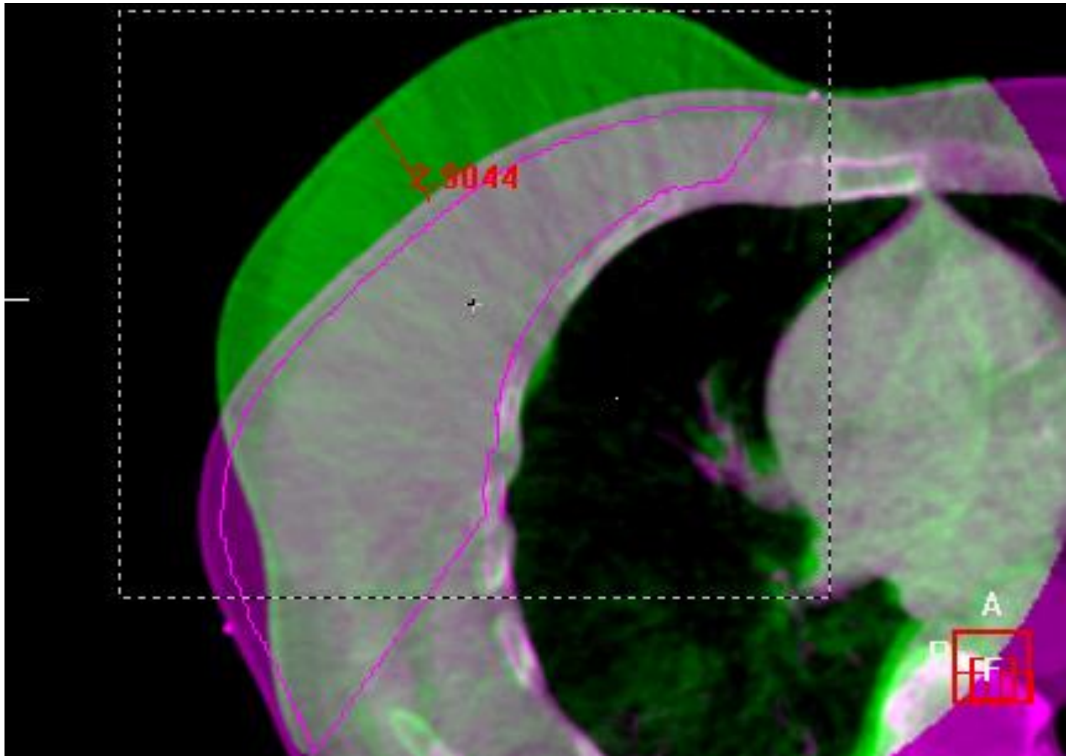
a management system for anatomical changes that flag the changes that may need intervention of some sort.







Ref CT
CBCT



Anatomical Changes

The important questions:

1: Is the target volume (CTV or GTV) within PTV?

2: Is the dose distribution compromised?

Green	Level green, no action needed.
Yellow	Level yellow, the radiation oncologist is notified by email, but no response is required to continue treatment.
Orange	Level orange, the treating radiation oncologist (or back-up colleague) is informed by email and a response is required before the next fraction.
Red	Level red changes, the radiation oncologist must be consulted immediately before the treatment fraction is allowed to be delivered.

ANTONI VAN LEEUWENHOEK
NEDERLANDS KANKER INSTITUUT

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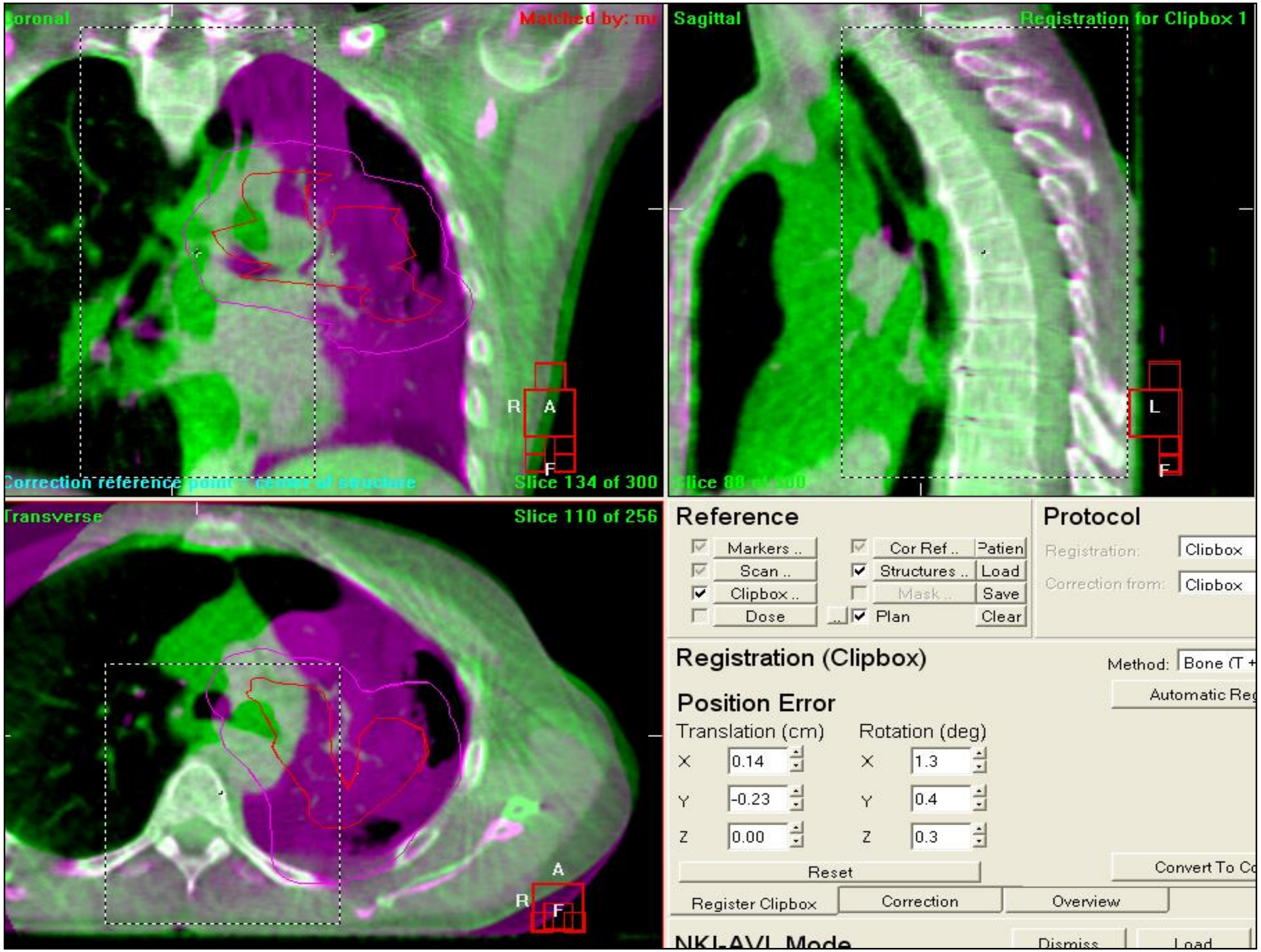
http://www.avl.nl/media/291805/xvi_engelse_protocols_16_7_2014

Level 1 Atelectasis resolved



GTV is not within PTV

Dose distribution is compromised

Anatomical Changes

Or keep it very simple:

Contact the IGRT-group when

- GTV is outside of PTV
- Anatomical changes > 1 cm

Managing CBCT

@AMC

5 RTT's with a focus on IGRT:

- Track, check patients
- First contact of changes occur
- **Training and education**
- Manuals and protocols
- Data collection

Managing CBCT

3 lectures (1h)

- Theraview: Portal imaging system and decision rule management system
- geometrical errors & correction strategies
- CBCT incl artefacts, image quality

2 Workshop (2x1.5h) in registration and image evaluation

Challenge: it affects all RTT's, so large group needs to be trained and kept up to date!

Managing CBCT

@AMC

5 RTT's with a focus on IGRT:

- Track, check patients
- First contact of changes occur
- Training and education
- **Manuals and protocols**
- **Data collection**

Managing CBCT

5 RTT’s:

- Track, check patients
- First contact of changes occur
- Training and education
- **Manuals and protocols**
- **Data collection**

→ These RTT’s also work in the clinic

Implementing IG&ART

Research department → Clinic

Multi disciplinary group to implement, research and evaluate IGRT protocols:

- Physicists
- Physicians
- RTT's
- Software developers
- Post-docs/PhD students

Introducing IGRT

Also applicable for development and implementation in other steps of the radiation therapy chain!

RTT **:**

Evaluation of bulk of data: for example

- Inter fraction set up variability
- Intra fraction stability
- Organ motion or deformation
- Testing new (software) tools

Design & implementation new protocols

Training and education in house

Protocols and manuals

Clinic!

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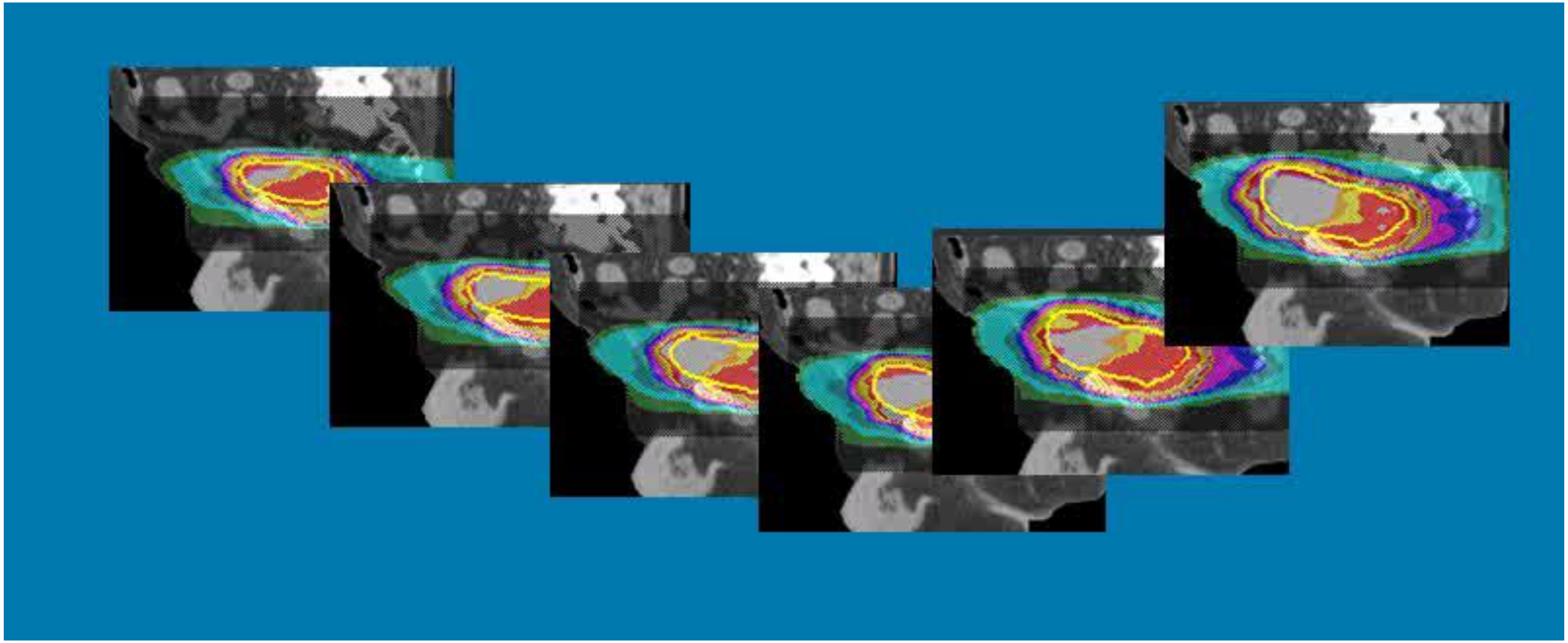
Shifting responsibilities @ treatment machine

ART: Library of Plan

Dealing with daily volume changes



Courtesy Danny Schuring,
Catharina Ziekenhuis, Einhoven

Treatment Procedure

- Lipiodol demarcation of tumor by urologist
- Full & empty bladder CT scan
- Instructions to ensure full bladder
  - – Good hydration prior to treatment
  - – Empty bladder 1 hr before treatment
  - – Drink 2 – 3 glasses
  - – Continuous steering during treatment

- Cone-beam CT at start of treatment
- Selection of “plan of the day” based on bladder filling

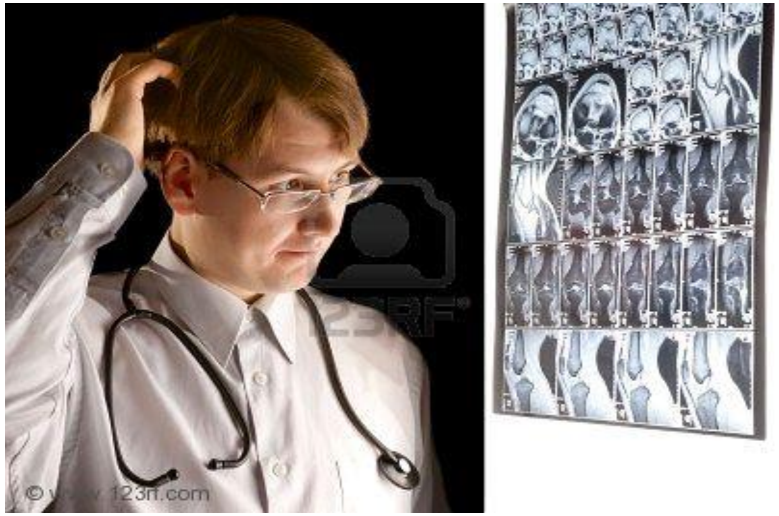
Courtesy Danny Schuring,
Catharina Ziekenhuis, Einhoven

Daily plan selection

- Daily plan selection at linac

  ⇓

  Shift in responsibilities!



- Current practice: selection by physicist or specialized technologist

Courtesy Danny Schuring,
Catharina Ziekenhuis, Einhoven

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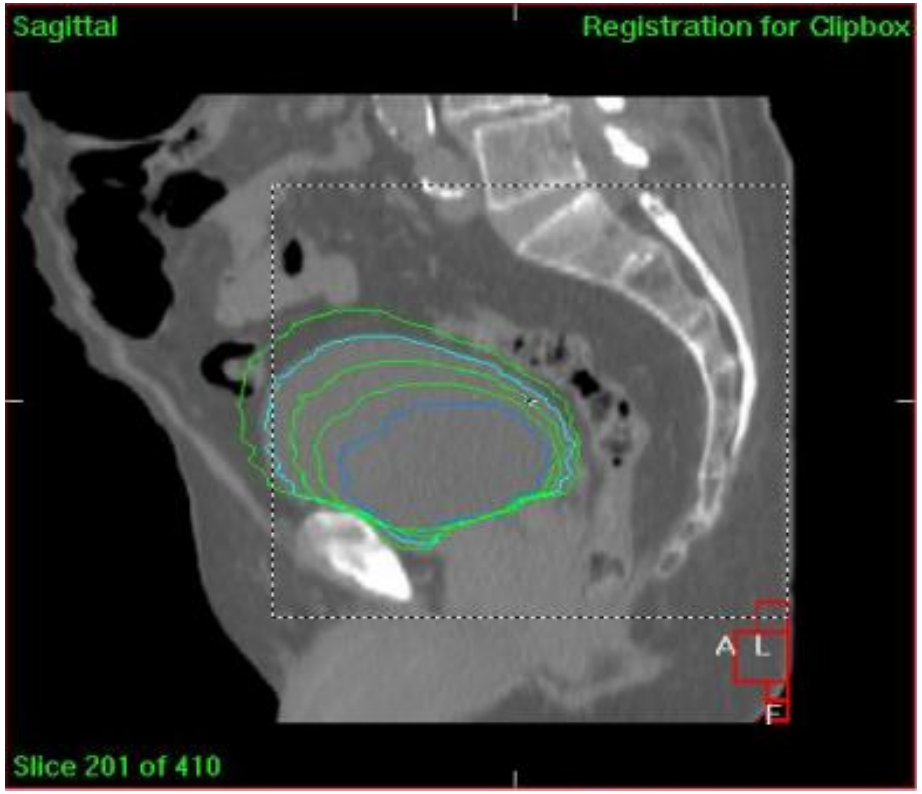
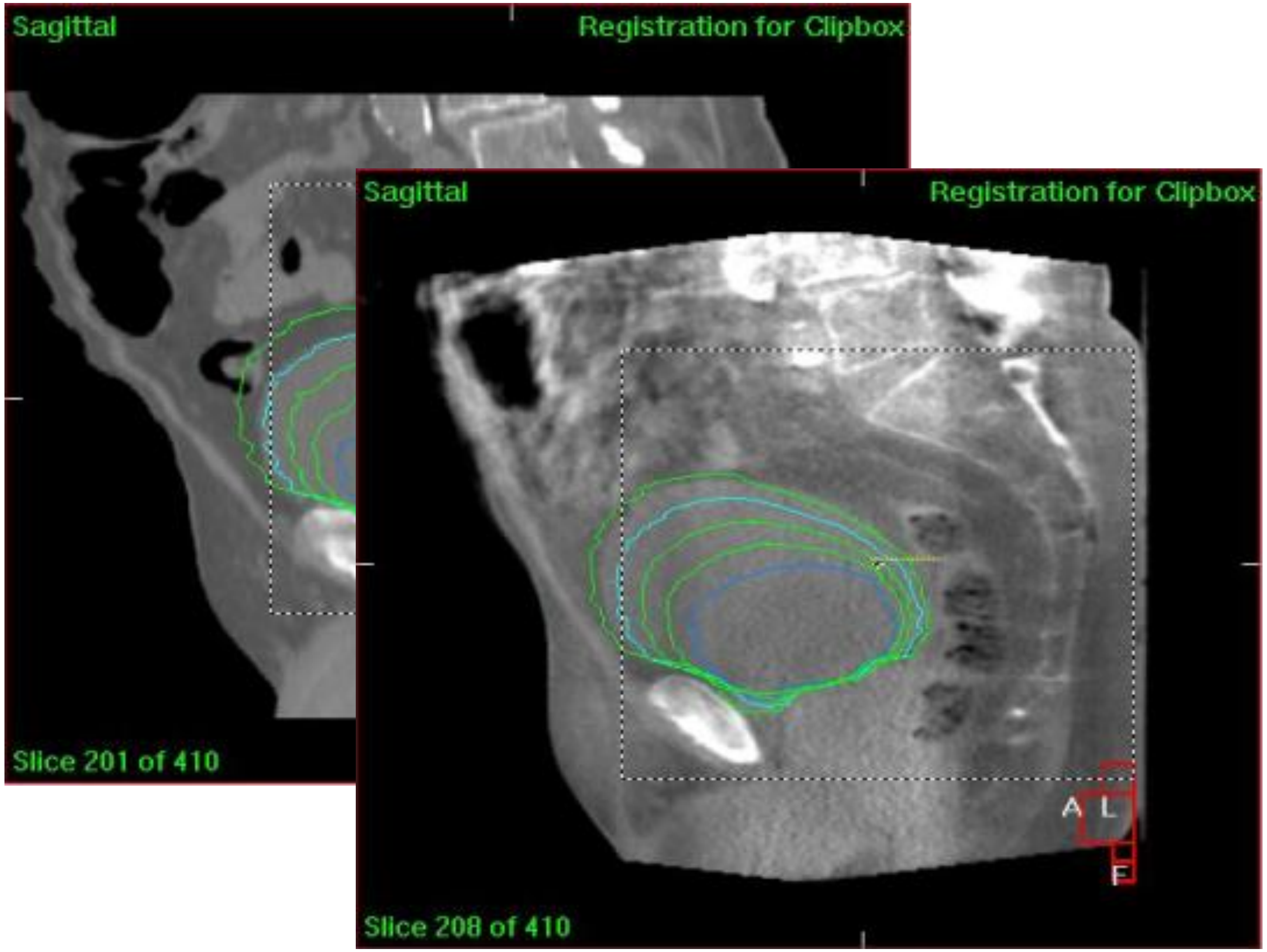
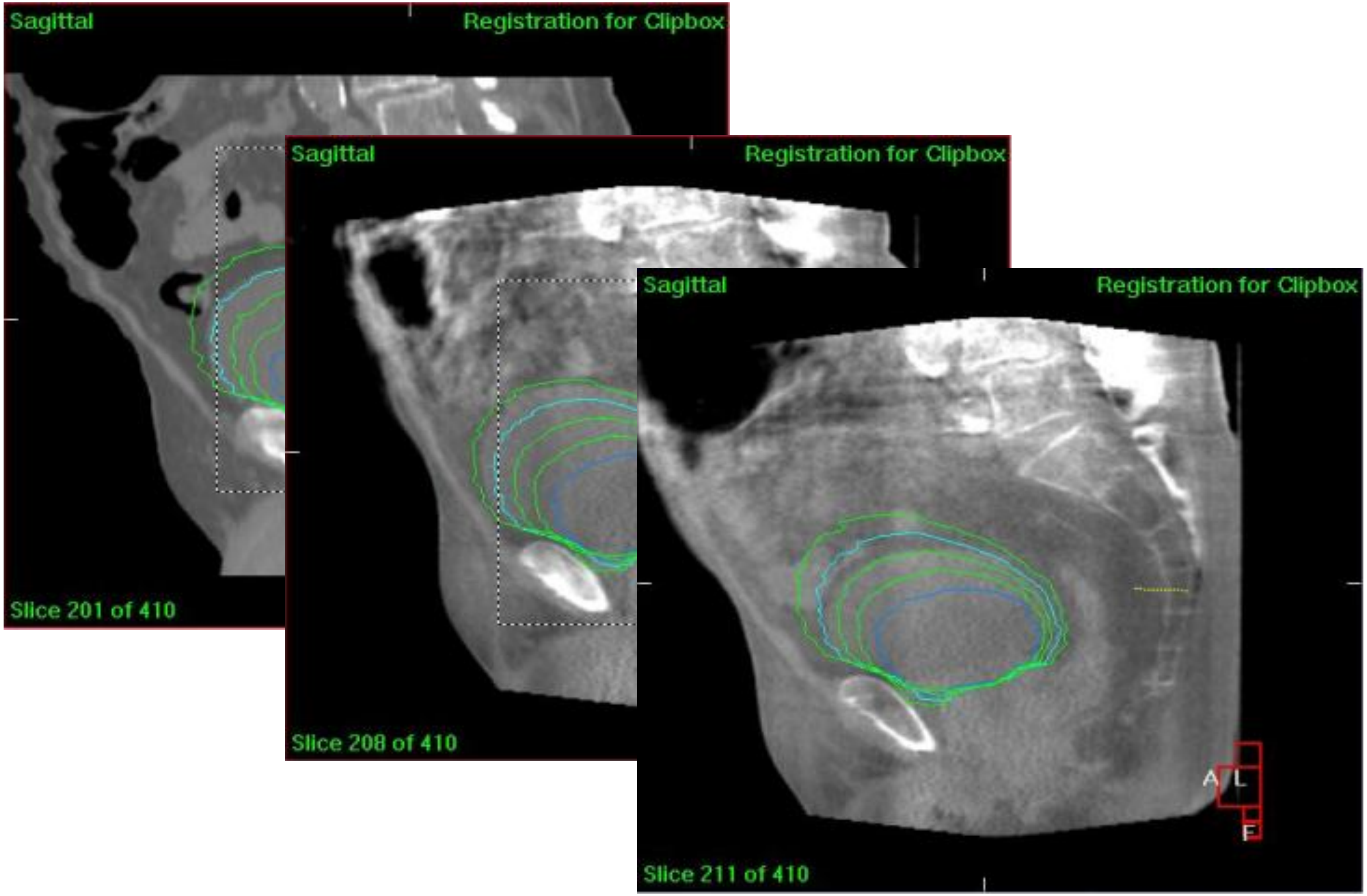
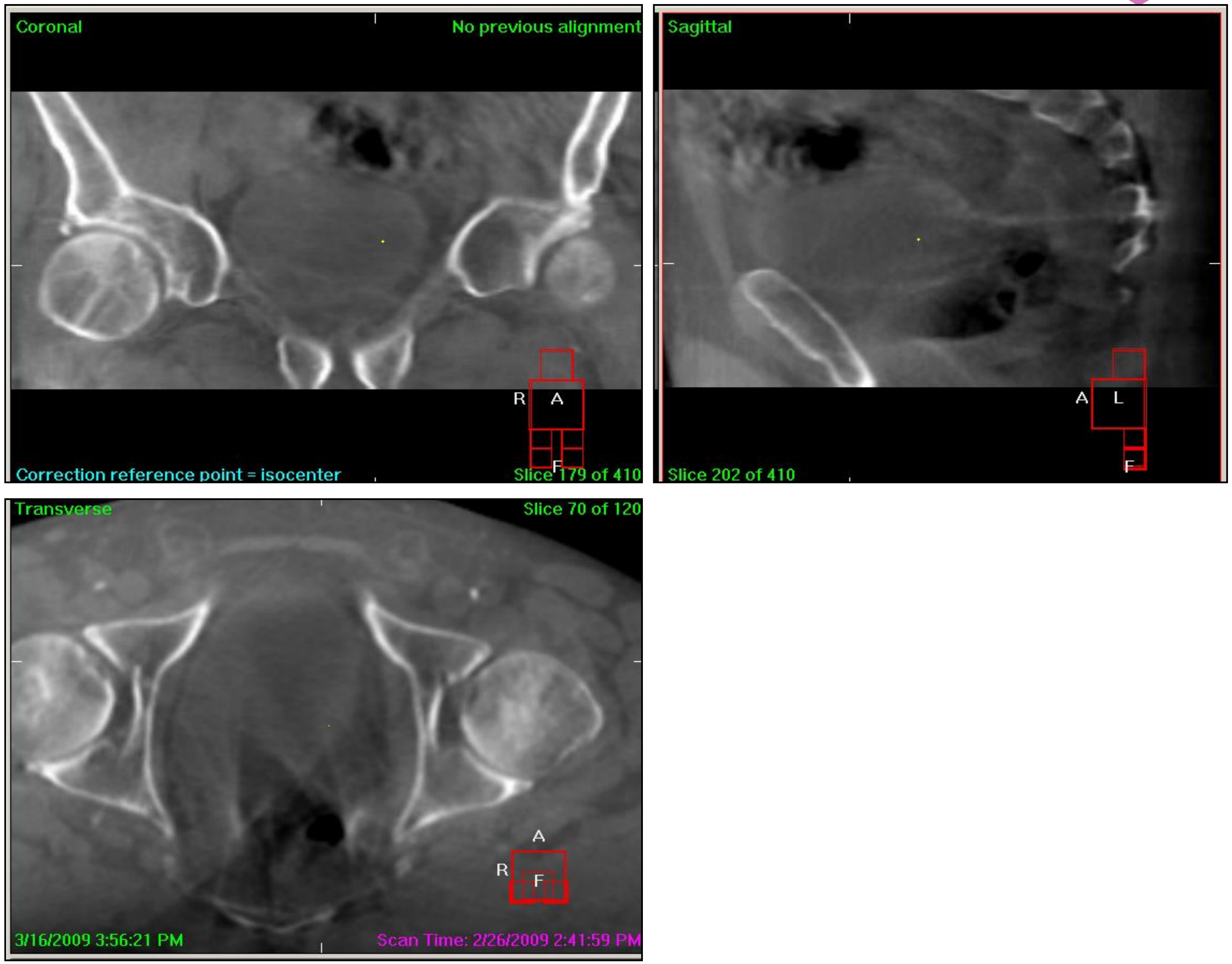

Sagittal
Registration for Clipbox
A
L
F
Slice 201 of 410


Sagittal
Registration for Clipbox
Slice 201 of 410
Sagittal
Registration for Clipbox
A
L
F
Slice 208 of 410

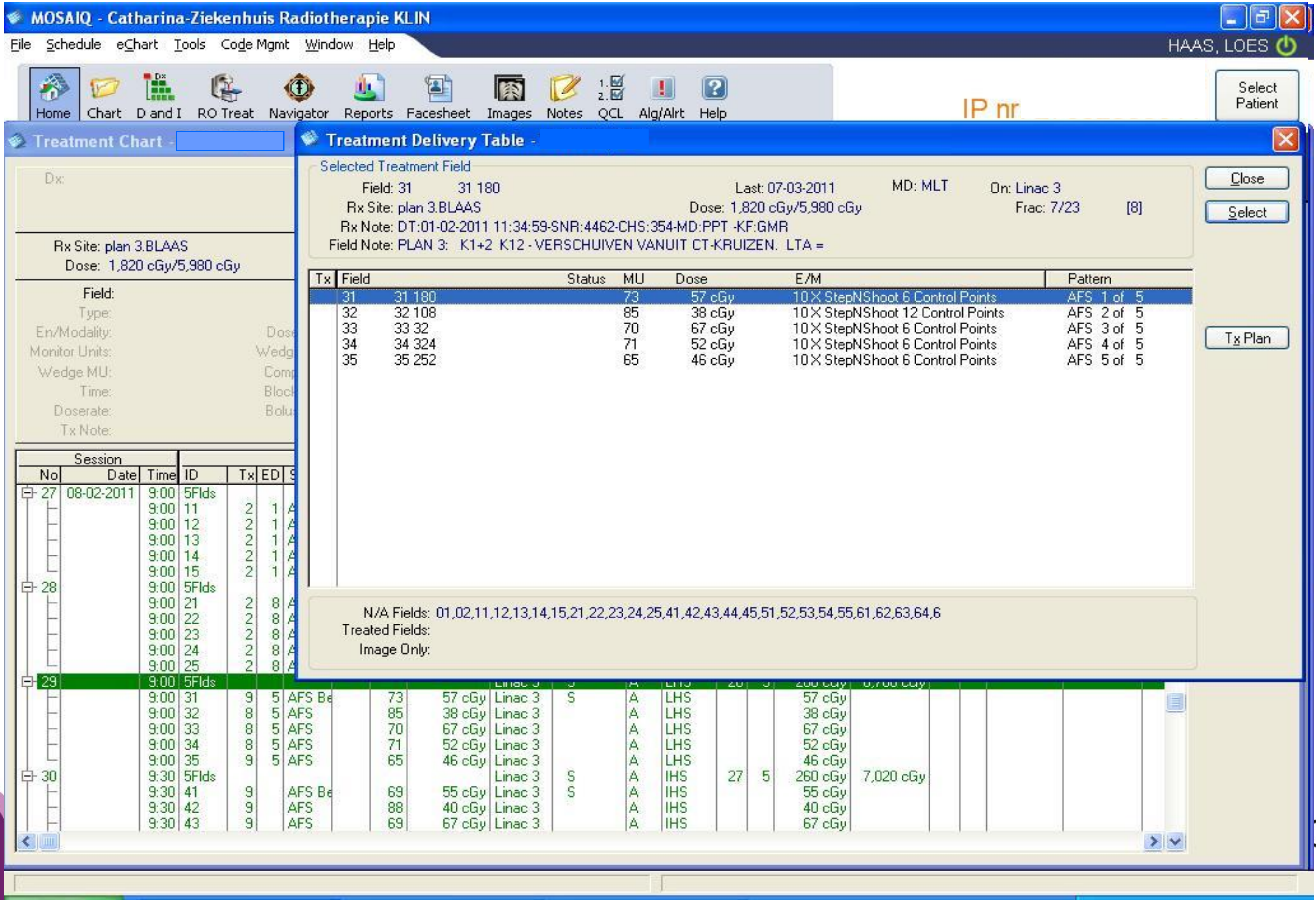

Sagittal
Registration for Clipbox
Slice 201 of 410
Sagittal
Registration for Clipbox
Slice 208 of 410
Sagittal
Registration for Clipbox
Slice 211 of 410
A
L
F

XVI quality

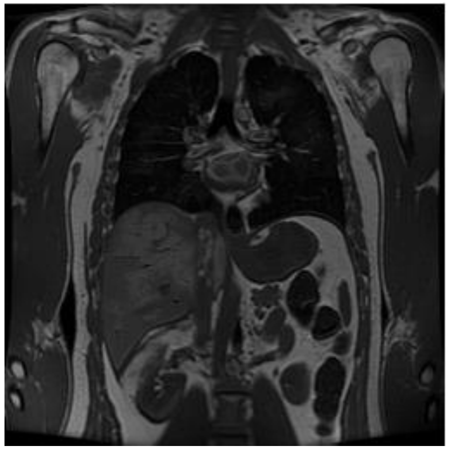
Workshop
Rianne



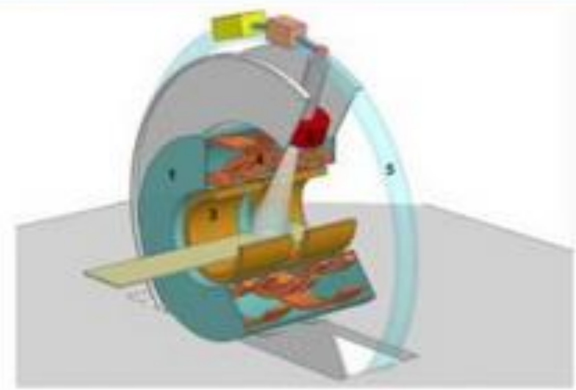
Plan selection in Mosaiq



1 step further; MR inside the treatment room



U Utrecht-Philips Elekta



Viewray-MRIdian MRI-Cobalt

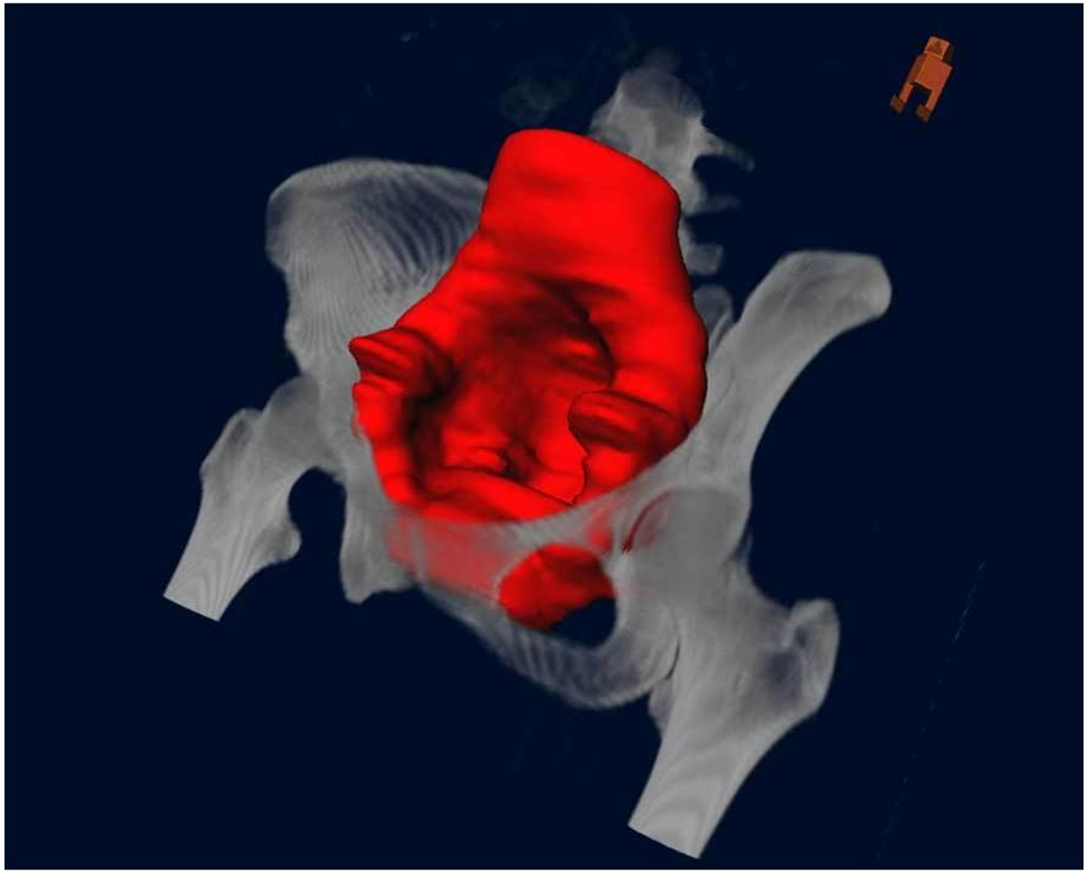
http://www.viewray.com

Diagnostic quality scan at treatment

Allows for:

- online re-planning
- online correction intra-fraction motion
- ART: accumulate doses for adaptation
- Treatment response assessment for adaptation

MR for online replanning – needs contouring

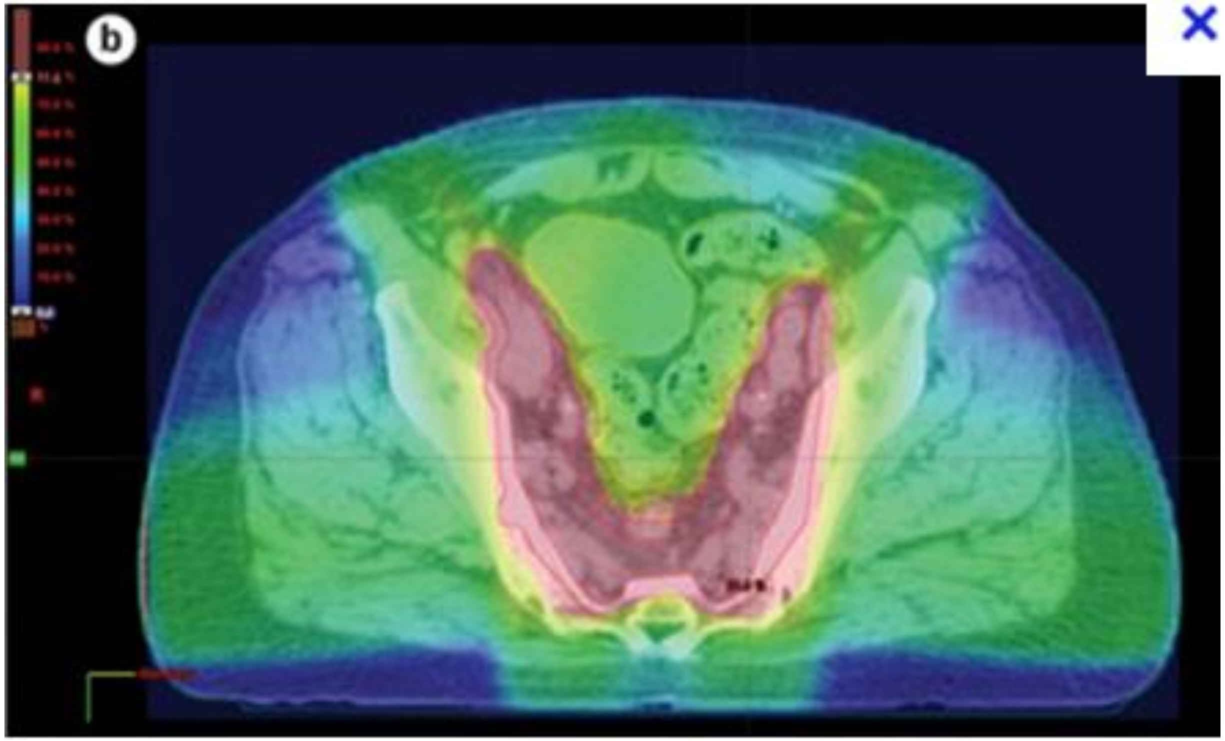


Approval of segmentation?

- OAR's
- Target volume

Peter

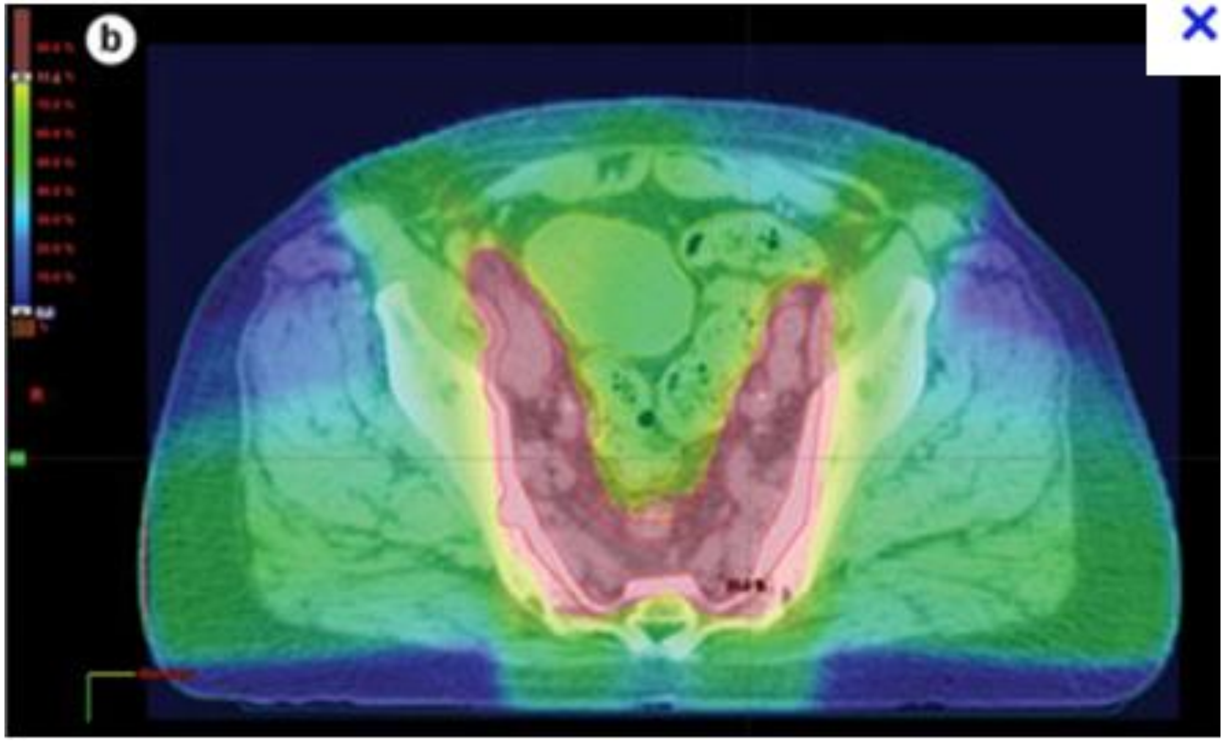
MR for online replanning – needs replanning



Approval of new plan?

- OAR's
- Target volume

MR for online replanning – needs replanning



Approval of new plan?

- OAR's
- Target volume

Treatment planning & IGRT become best friends!

Summary

Modern Radiation Therapy is a multi disciplinary effort

Modern Radiation Therapy has openened up the field for RTTs:

- Patients education
    - Pre-treatment imaging PET/MRI/CT
- CT simulation
- Treatment Planning
    - Research and Development
- Treatment
    - *Image guidance*
- Research & Development

Still evolving!

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Acknowledgments

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Anja Betgen

Suzanne van Beek

Catharina Ziekenhuis

Danny Schuring

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Questions & Discussion

m.a.j.dejong@amc.uva.nl

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Patient Preparation and Positioning

Martijn Kamphuis MSc MBA

(Slides: Rianne de Jong)
Academic Medical Center, Amsterdam

Prague 2017

m.kamphuis@amc.nl

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Aim of Patient preparation and positioning

→ Minimize the difference in patient position

1. between simulation and treatment sessions
2. during the treatment session

→ Maximize the distance between target volume and organs at risk

Tools:

- Immobilization and fixation
- Patient compliance

Tools of Patient preparation and positioning

→ Immobilization

Daily set-up **reproducibility** and **stability** through the use of fixation or aiding devices

Expectation management

- This aim of this talk is not to show the best devices

- Understanding the rationale behind it

- Choice for device will be based on:
  - ➢ Economics
  - ➢ Local availability
  - ➢ Literature
  - ➢ Experience

- Link to important review at the end of the .ppt

Tools of Patient preparation and positioning

"My diabetic research shows that test subjects are 98% more likely to take their diabetic pills if the pills are covered in chocolate."

Minimize the difference in patient position

→ **Minimize the difference in patient position**

1. **between simulation and treatment sessions**
2. during the treatment session

→ Maximize the distance between target volume and organs at risk

Tools:

- Patient compliance
- Immobilization and fixation

Aim of Patient preparation and positioning

→ **<u>Minimize</u> the difference in patient position between simulation and treatment sessions: *inter*-fraction motion**

Tools:

Patient compliance:

- Pelvic patients using diet / drinking protocol

Immobilization and fixation:

- Head&Neck using head support
- Lung using 4D CBCT.

Prostate patients

Reconstructed

CBCT

Prostate patients

To improve image quality:

Dietician

- Mild regimen of laxatives
- Diet

Fixed treatment times

Prostate patients

	gas	faeces	moving gas
no diet	68%	61%	45%
with diet	42%	23%	22%

- reduced percentage of faeces and gas
- reduced percentage of moving gas, hence improved image quality

Prostate patients

Lips et al. Ijrobp 2011

- 739 patients without diet, 205 patients with diet
- Diet instructions on leaflet
- No reduction of **intrafraction** movement

McNair et al. 2011

- 22 patients using questionaires
- Rectal filling consistency not improved
- Diet + fixed treatment times, **no laxatives**

Conclusion:

- Drinking and dietery protocol are needed for clear patient communication **BUT**
- **Won't solve the whole problem of intra/interfraction motion (additional tools are needed)**

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Aim of Patient preparation and positioning

→ **Minimize the difference in patient position between simulation and treatment sessions: *inter*-fraction motion**

Tools:

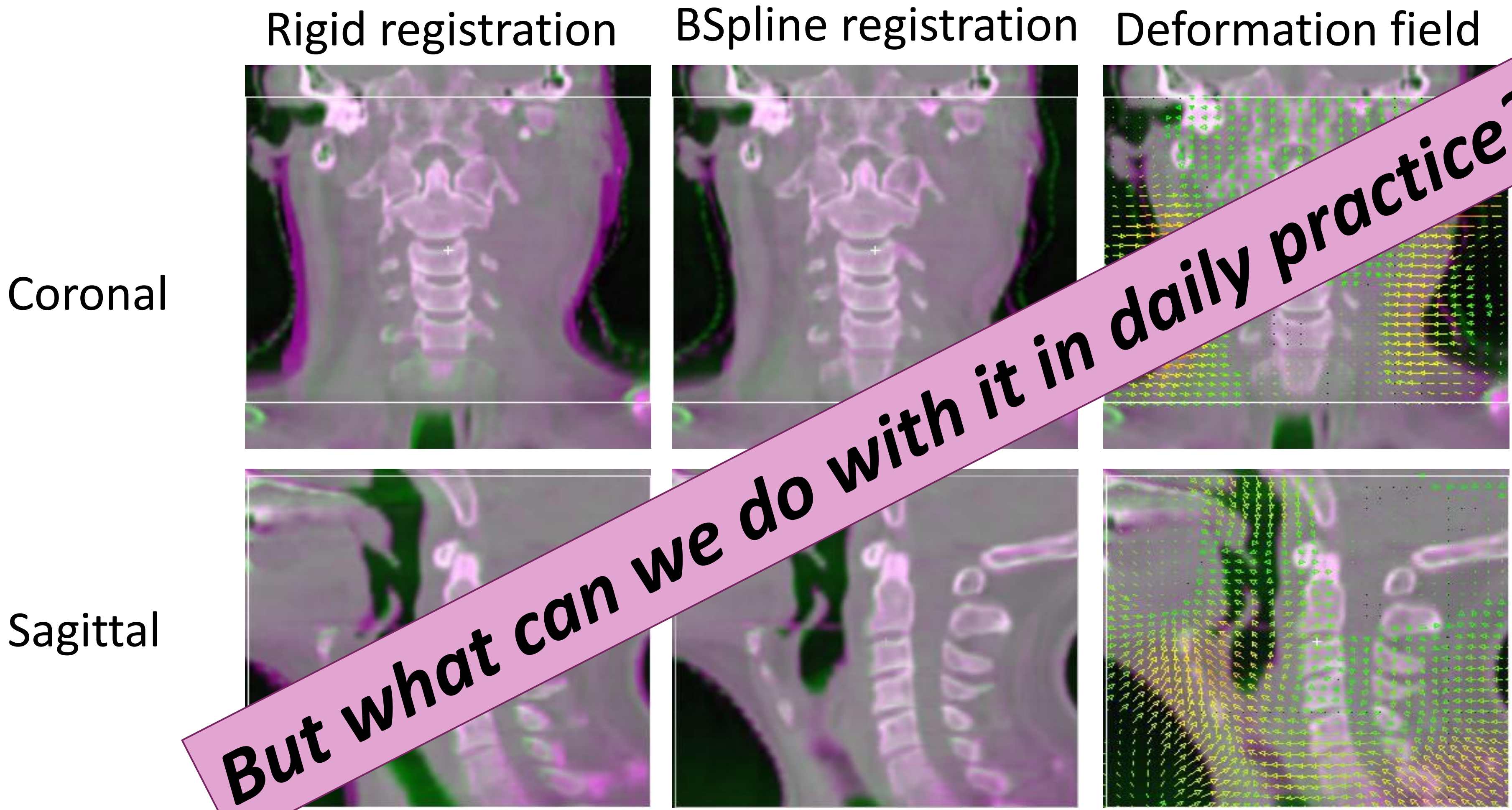
Patient compliance:

- Pelvic patients using diet / drinking protocol

Immobilization and fixation:

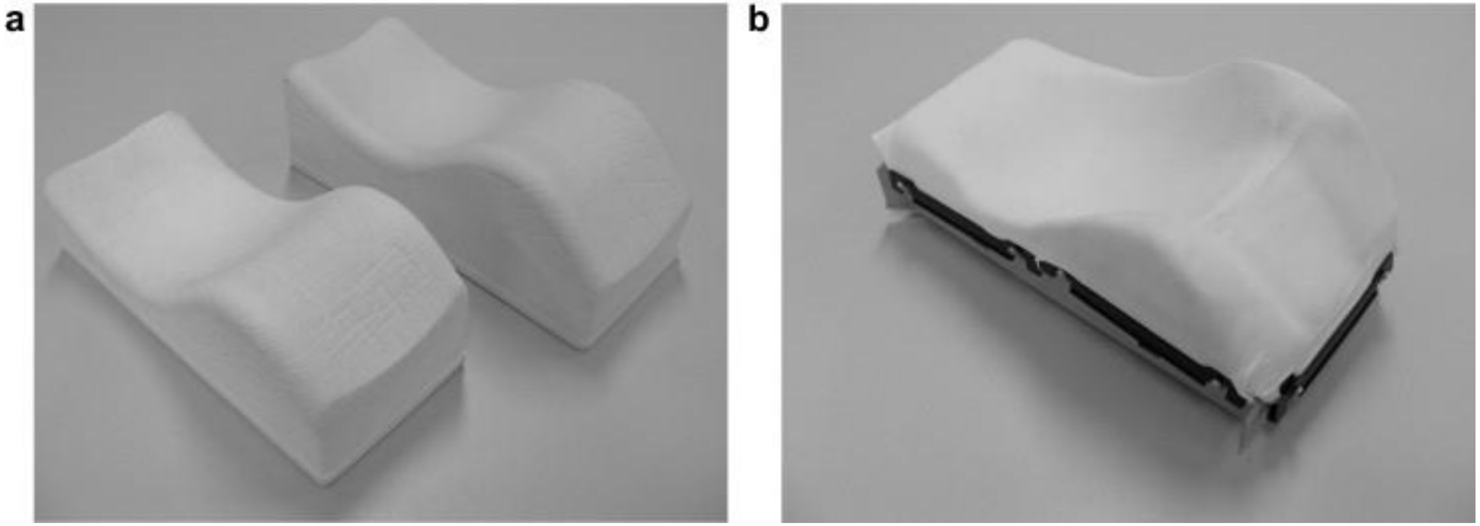
- **Head&Neck using head support**
- **Unfortunate differences**

Head&Neck patients: head support



But what can we do with it in daily practice?

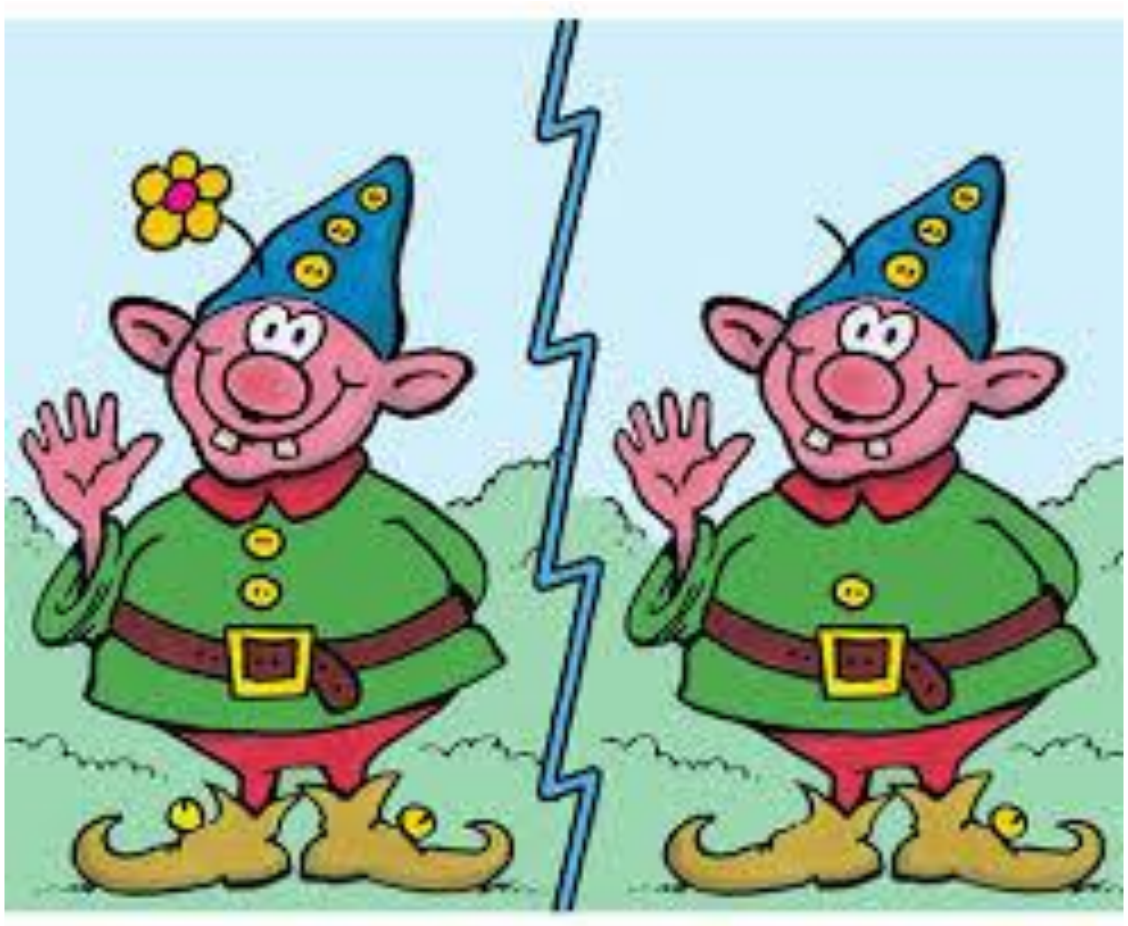
Head&Neck patients: head support



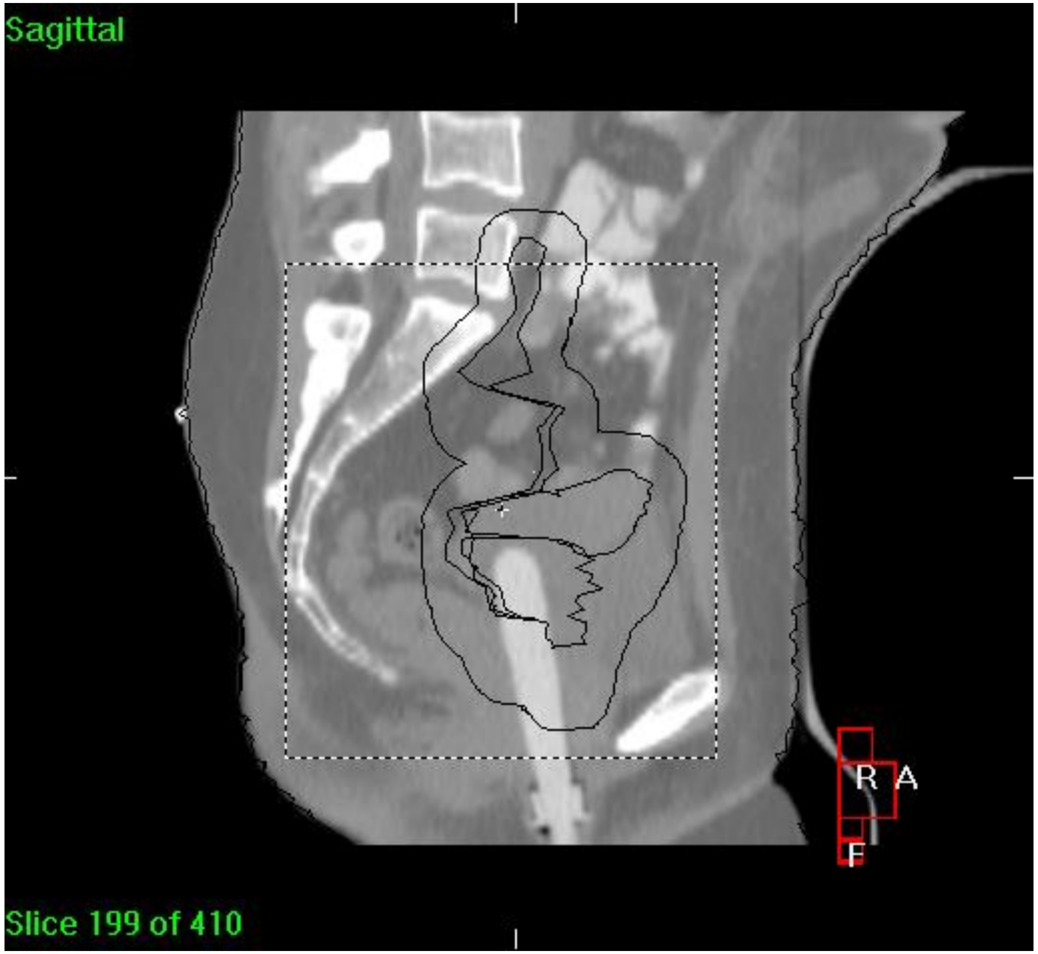
- Reduction of the average difference between fractions in set up of the bony anatomy.
- Reduction in the difference of the shape of the bony anatomy between fraction.

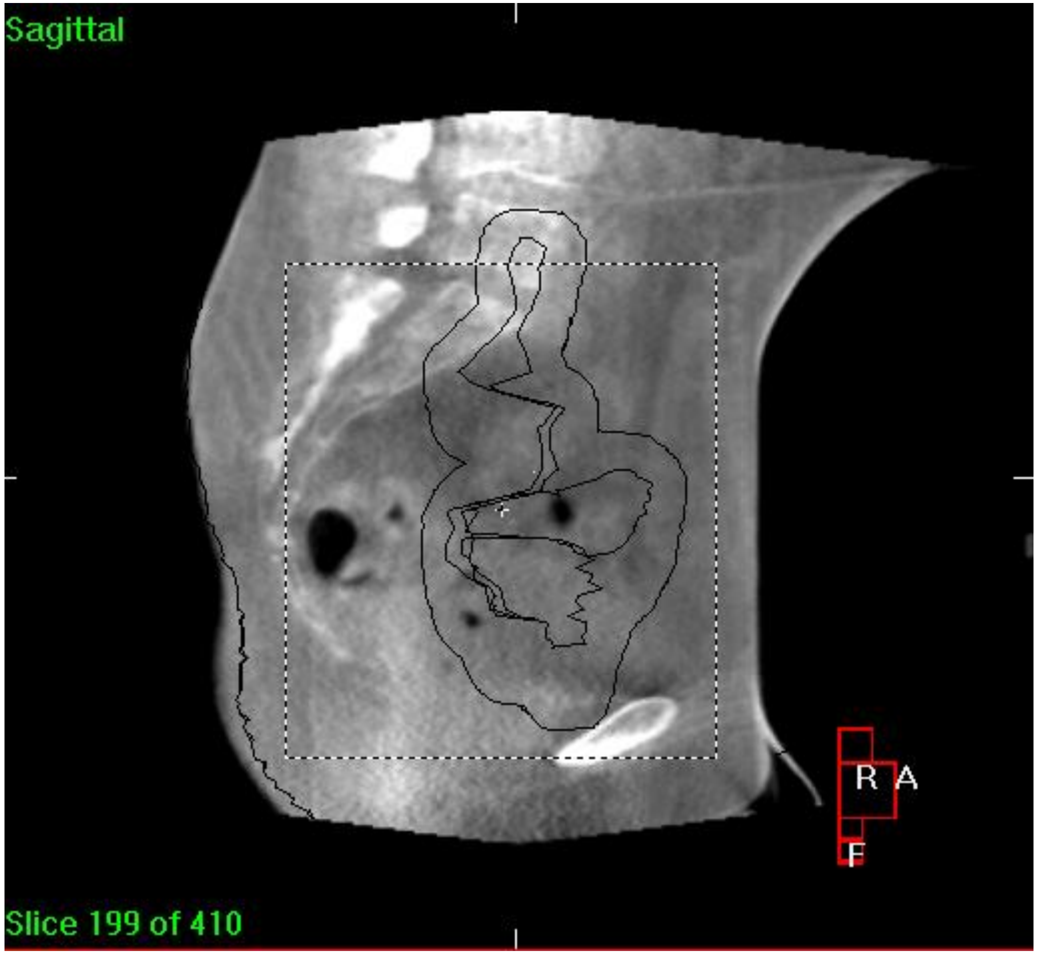
Creating unfortunate differences

- Between CT and treatment

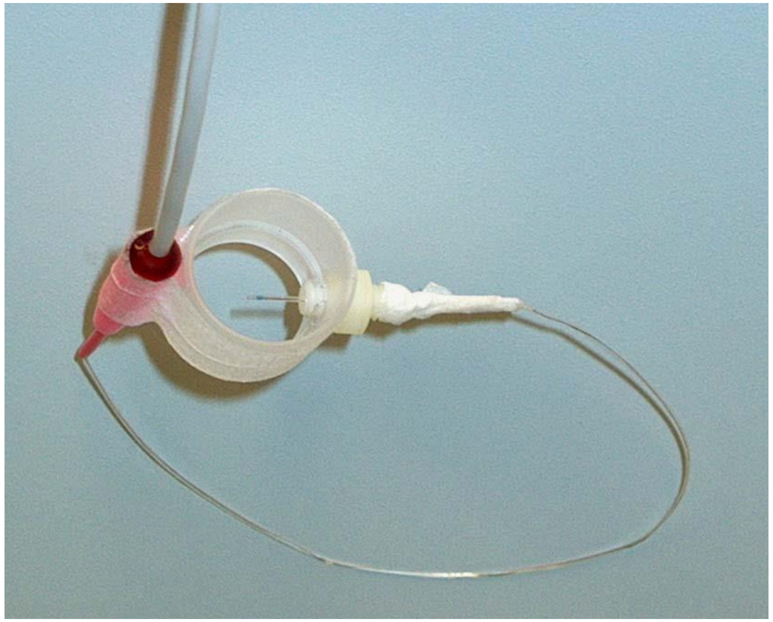


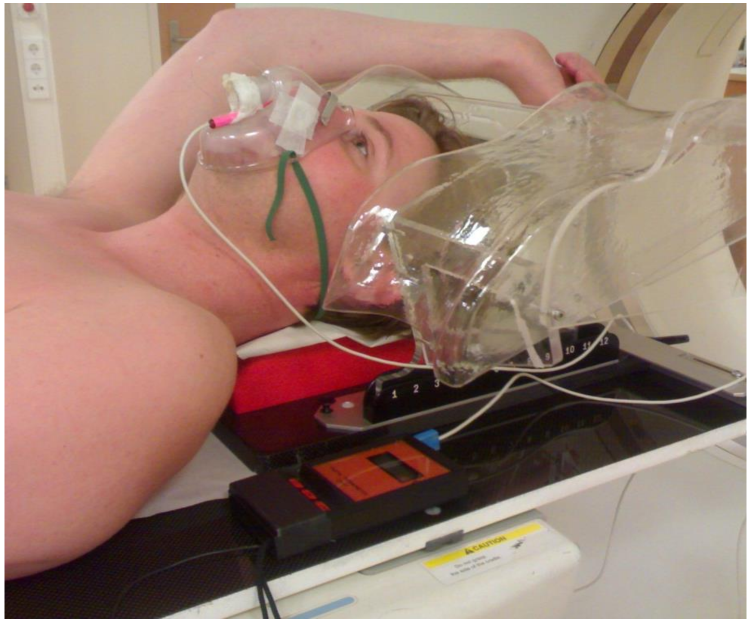
Example 1: Look for differences..





Example 2: Respiratory monitoring system





- 4D CBCT scans with and without oxygen mask
- 3D tumor motion was assessed for tumor mean position and amplitude

Respiratory monitoring system

With oxygen mask

	LR (cm)	CC (cm)	AP (cm)
Σ	0.18	0.23	0.23
σ	0.16	0.19	0.19
Mean	0.06	0.03	0.00

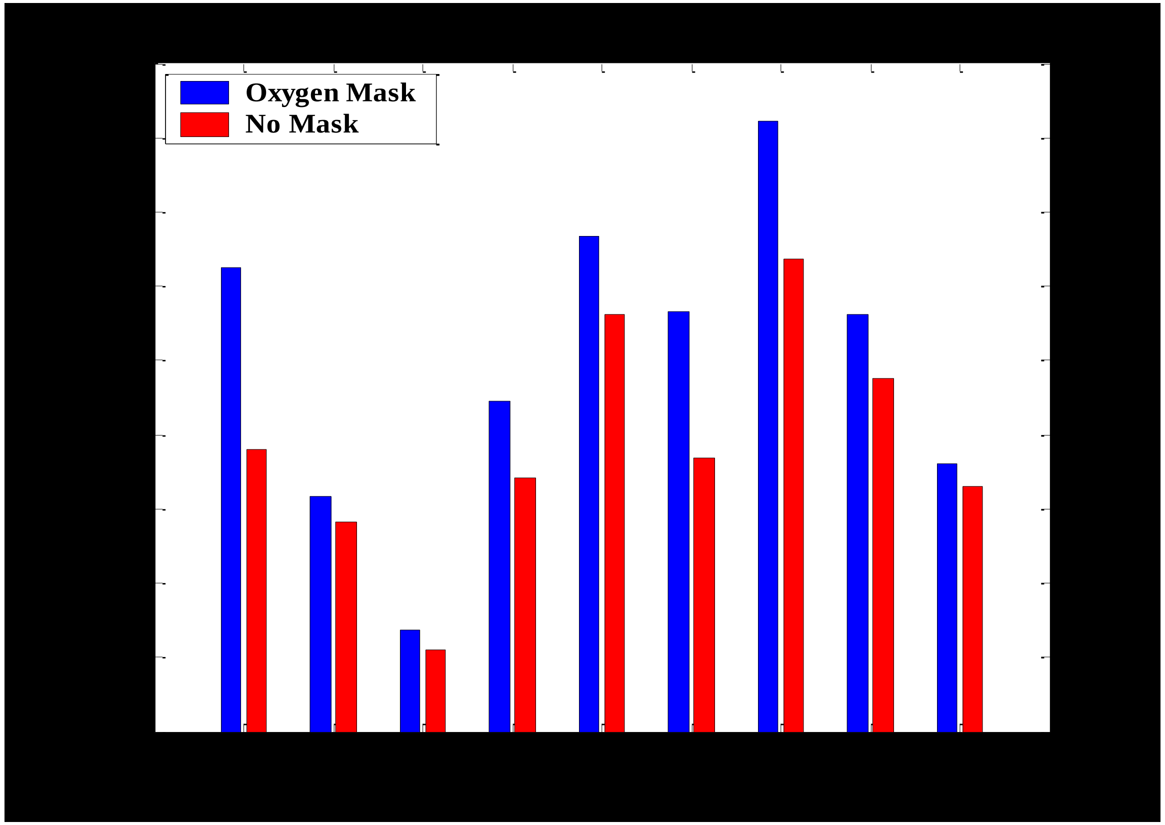
Without oxygen mask

	LR (cm)	CC (cm)	AP (cm)
Σ	0.15	0.21	0.22
σ	0.18	0.17	0.20
Mean	0.04	0.08	-0.09

No significant difference in tumour mean position

J. Wolthaus, M. Rossi

Respiratory monitoring system



M = 29%, SD = 19%, p = 0.0017

Difference in breathing amplitude!

J. Wolthaus, M. Rossi

Deformable registration decreases the need for good immobilization

A. True
B. False

Aim of Patient preparation and positioning

→ **<u>Minimize</u> the difference in patient positioning during the treatment session: *intra*-fraction motion**

Tools:

Increasing patient compliance:

- Practical session SBRT

Immobilization and fixation:

- Lung using 4D CBCT.

Practical session

In case of hypofractioned RT:

- Patient visit the linac
- Session is completely performed but no Gray's are given

Advantages:

- Patient gets acquinted with workflow
- Set-up accuracy can be assesed:
  - ➢ is the intra# motion acceptable?
- Is it do able for the patient?
- Is the image quality sufficient?
- Precautions can be made:
  - ➢ Pain/stress relief
  - ➢ Additional margins/replanning

Stability with prolonged treatment time

Hypo fractionated lung

On-line lung tumor match with CBCT: 3 x 18 Gy
(first protocol design without arc therapy and inline scanning)

Aligning the patient:	5 min
First CBCT scan:	4 min
Registration:	5 min
Manual table shift:	3 min
Second CBCT scan:	4 min
Evaluation CBCT scan:	1 min
Beam delivery:	25 min
Post treatment CBCT scan:	4 min

Stability with prolonged treatment time

Antoni van Leeuwenhoek Hospital

100x real speed

Stability with prolonged treatment time

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Stability with prolonged treatment time

59 Patients, 3 fractions per patient

		LR (mm)	CC (mm)	AP (mm)
Residual Inter-fraction	GM	0.2	0.6	-0.6
	Σ	0.8	0.8	1.0
	σ	1.1	1.1	1.4
Intra-fraction	**GM**	**0.0**	**1.0**	**-0.9**
	Σ	**1.2**	**1.3**	**1.9**
	σ	**1.2**	**1.4**	**1.7**

Antoni van Leeuwenhoek Hospital

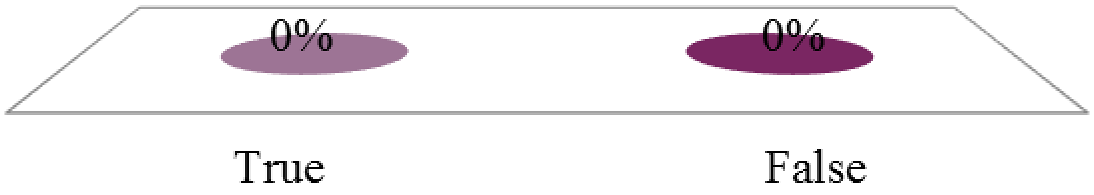
Intrafraction motion is the motion of a patient within a session

A. True
B. False

Patient compliance won't impact intrafraction motion

A. True

B. False



Minimize the difference in patient position

→ Minimize the difference in patient position

1. between simulation and treatment sessions
2. during the treatment session

→ **Maximize the distance between target volume and organs at risk**

Tools:

- **Immobilization and fixation**
- **Patient compliance**

Minimize the difference in patient position

→ **<u>Maximize</u> the distance between target volume and organs at risk**

Tools:

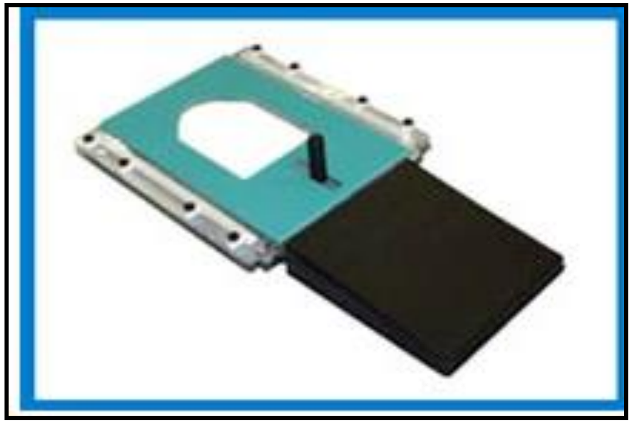
Immobilization and fixation:

- Bellyboard for pelvic patients

Patient compliance:

- Breath hold for breast patients

Belly board pelvic patients



Belly board

Belly board pelvic patients

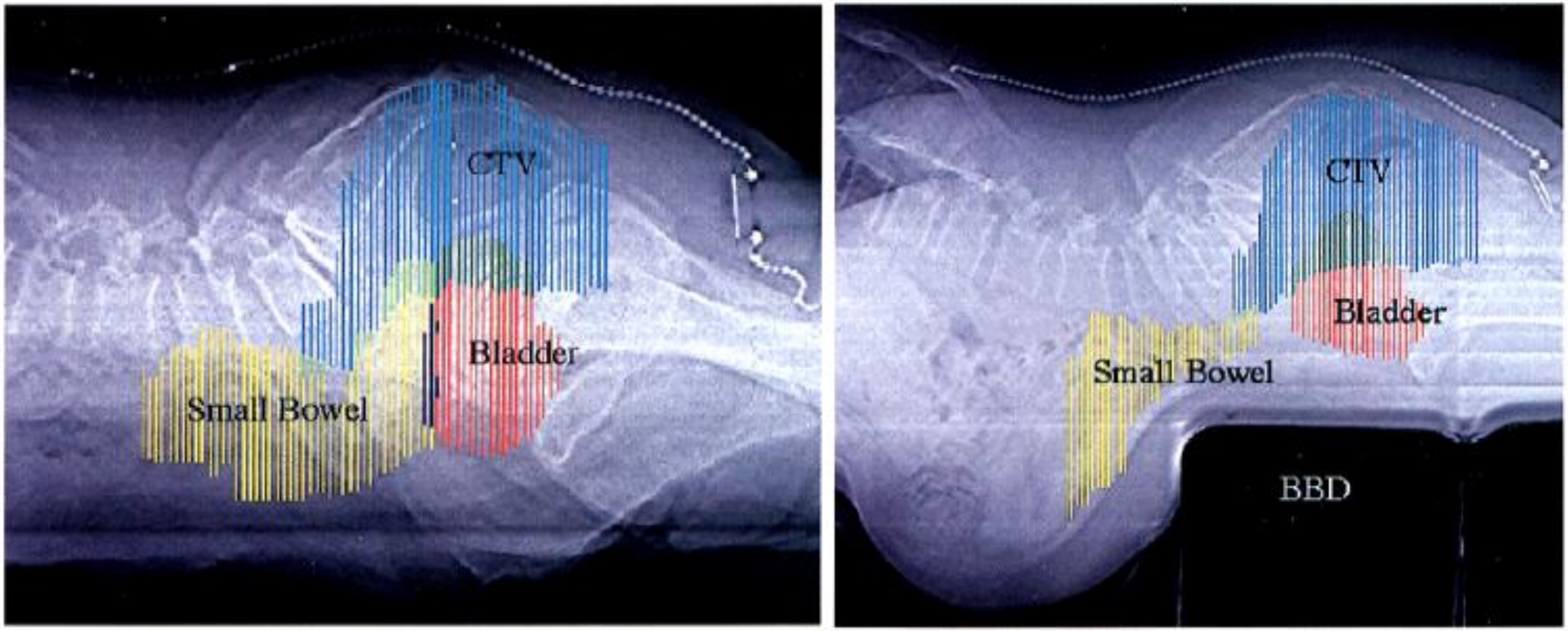
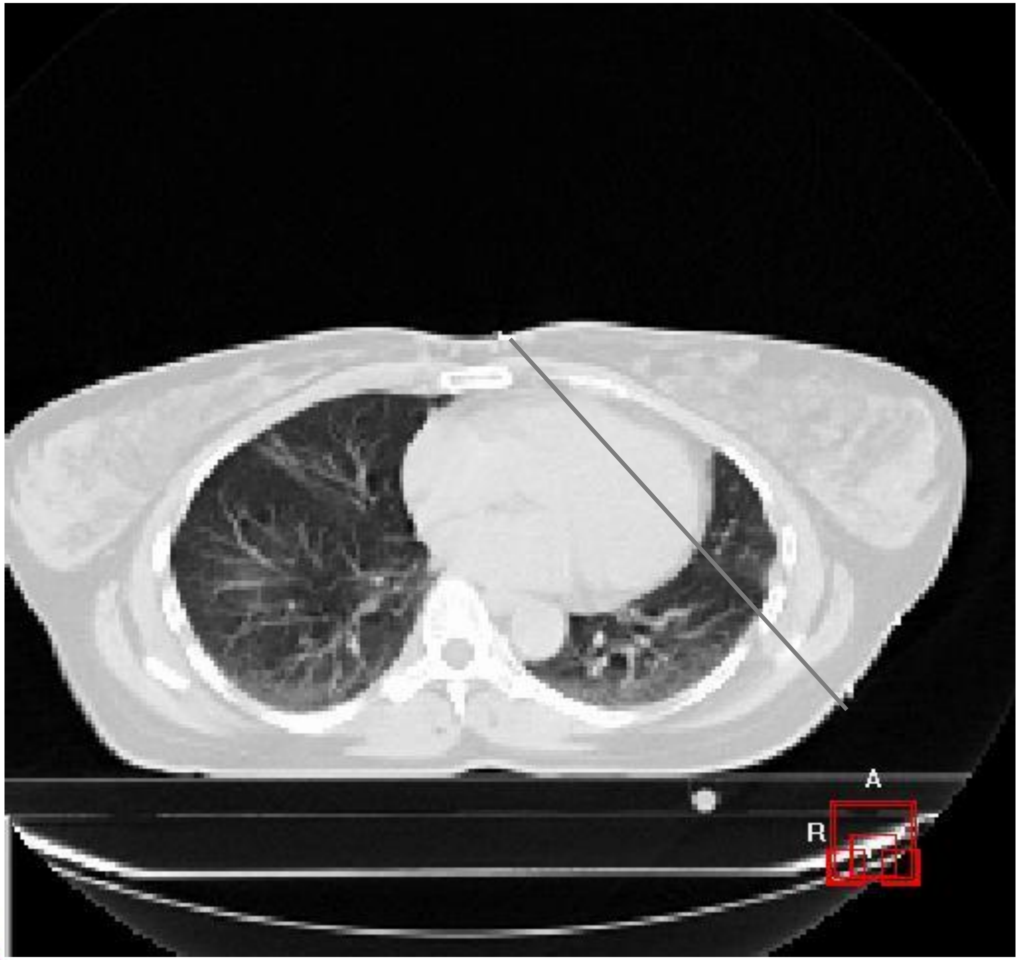


Fig. 2. Pilot localization, lateral view is shown (a) for simulation without BBD and (b) with BBD. The clinical target volume (CTV), small bowel, and bladder are shown. Note a dramatic shift in small bowel in the cephalic direction with the BBD.

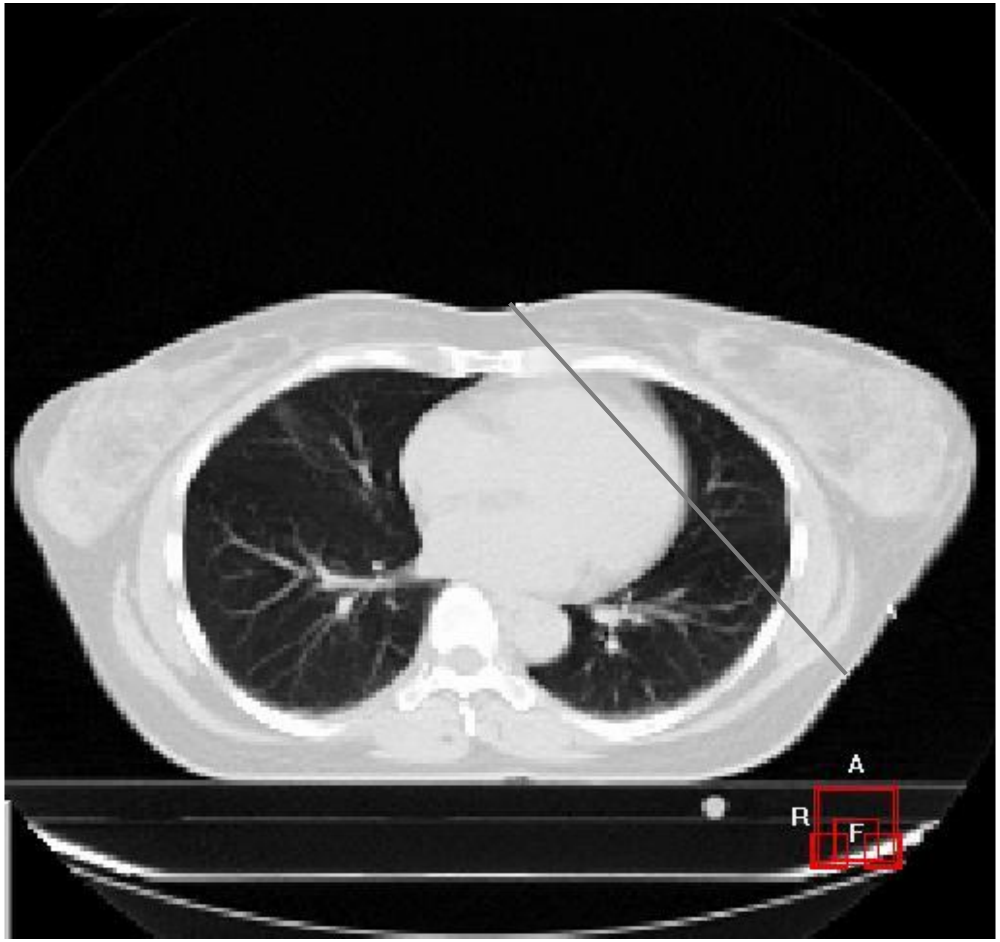
Das *et al*, 1997

Breath hold for breast patients

Normal inspiration

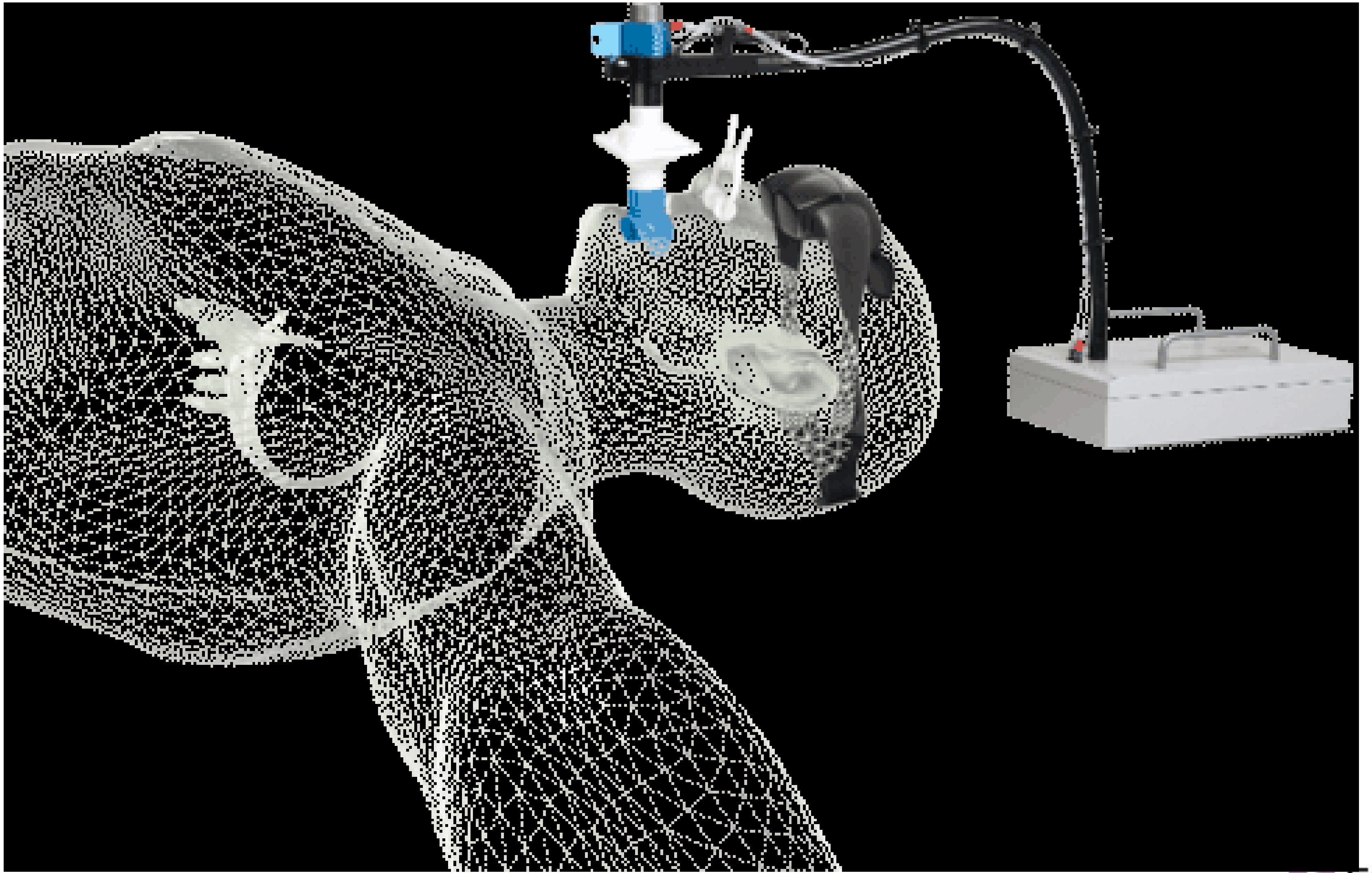


Deep inspiration



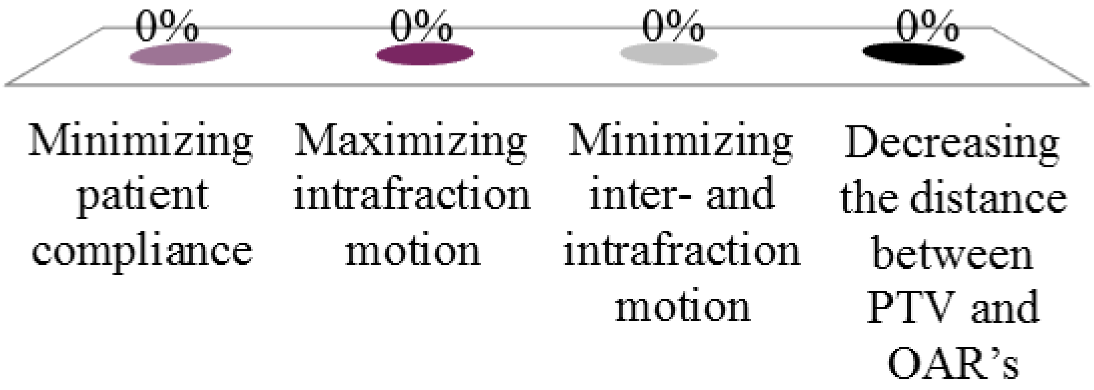
J. Sonke

Essential: education & compliance



Patient preparation and immobilization aims at:

A. Minimizing patient compliance
B. Maximizing intrafraction motion
C. Minimizing inter- and intrafraction motion
D. Decreasing the distance between PTV and OAR's



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Conclusion

The first step in radiation therapy is to minimize

- the difference in patients anatomy and set-up between CT en treatment
- the difference in patients anatomy and set-up between treatment days

and to maximize

- patient stability
- the distance between target volume and organs at risk

Conclusion

The first step in radiation therapy is to minimize

- the difference in patients anatomy and set-up between CT en treatment
- the difference in patients anatomy and set-up between treatment days

and to maximize

- patient stability
- the distance between target volume and organs at risk

IGRT & ART?

Rotations

Deformations

Offline protocol

OAR

Conclusion

https://espace.cern.ch/ULICE-results/Shared%20Documents/D.JRA_5.1_public.pdf

‘Recommendations for organ depending optimized fixation systems’

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Pre-treatment imaging

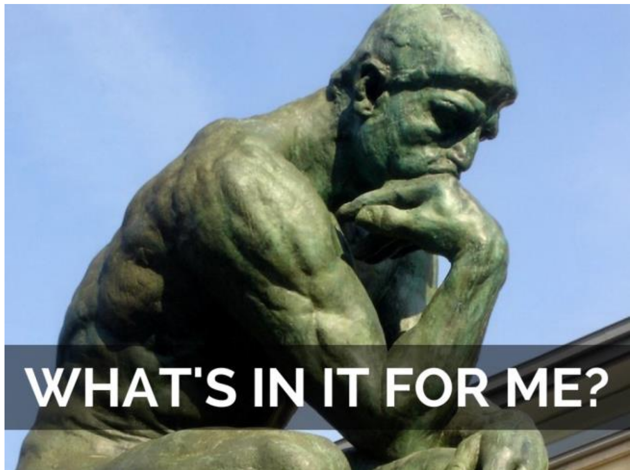
Mirjana Josipovic

Dept. of Oncology, Rigshospitalet
& Niels Bohr Institute, University of Copenhagen
Denmark

Advanced skills in modern radiotherapy
June 2017

Intended learning outcomes

- Illustrate the importance of a particular pre-treatment imaging modality for radiotherapy
- Comprehend the additional value of applying combined information from several imaging modalities for radiotherapy planning
- Identify uncertainties of pre-treatment imaging modalities

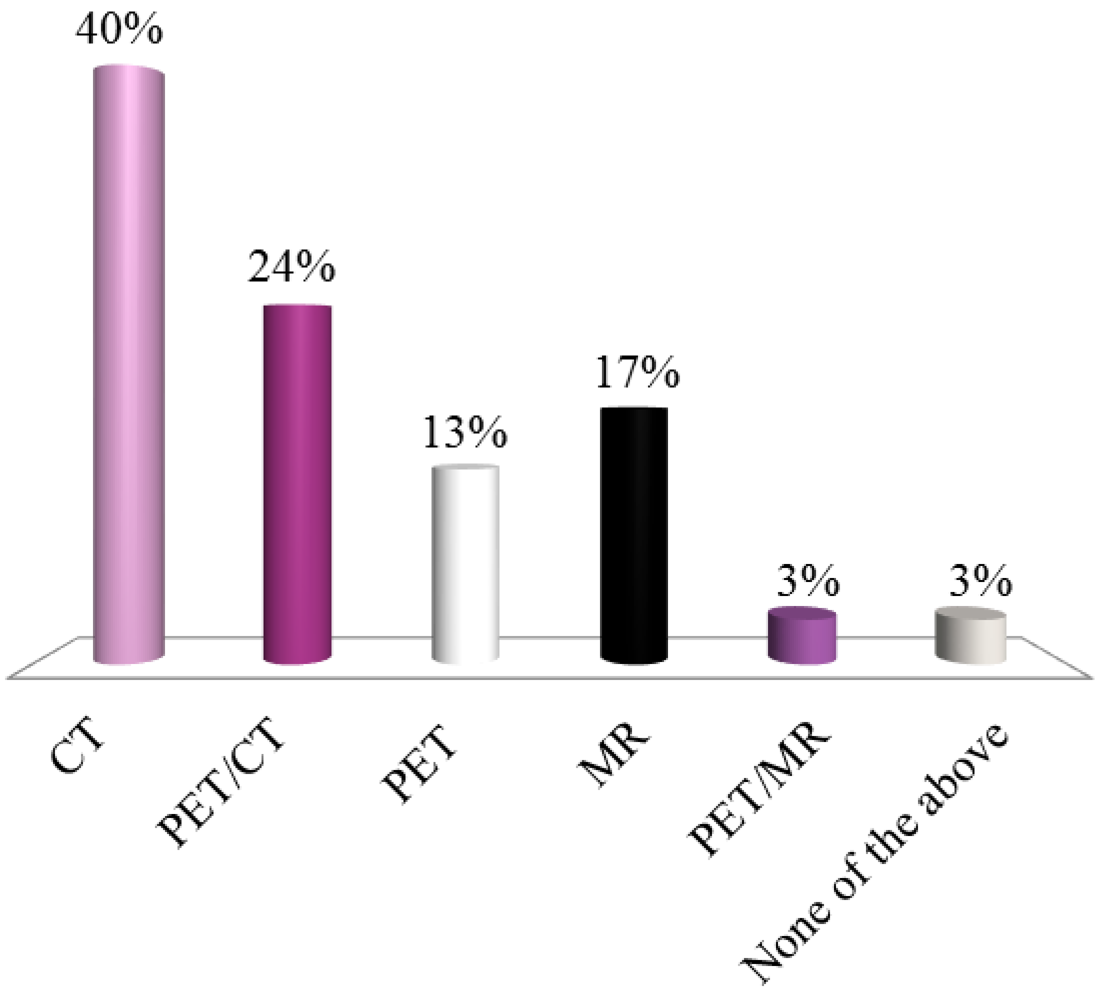


Pre-treatment imaging for radiotherapy

- CT: computed tomography
- PET: positron emission tomography
- MR: magnetic resonance

Do you have experience with…?

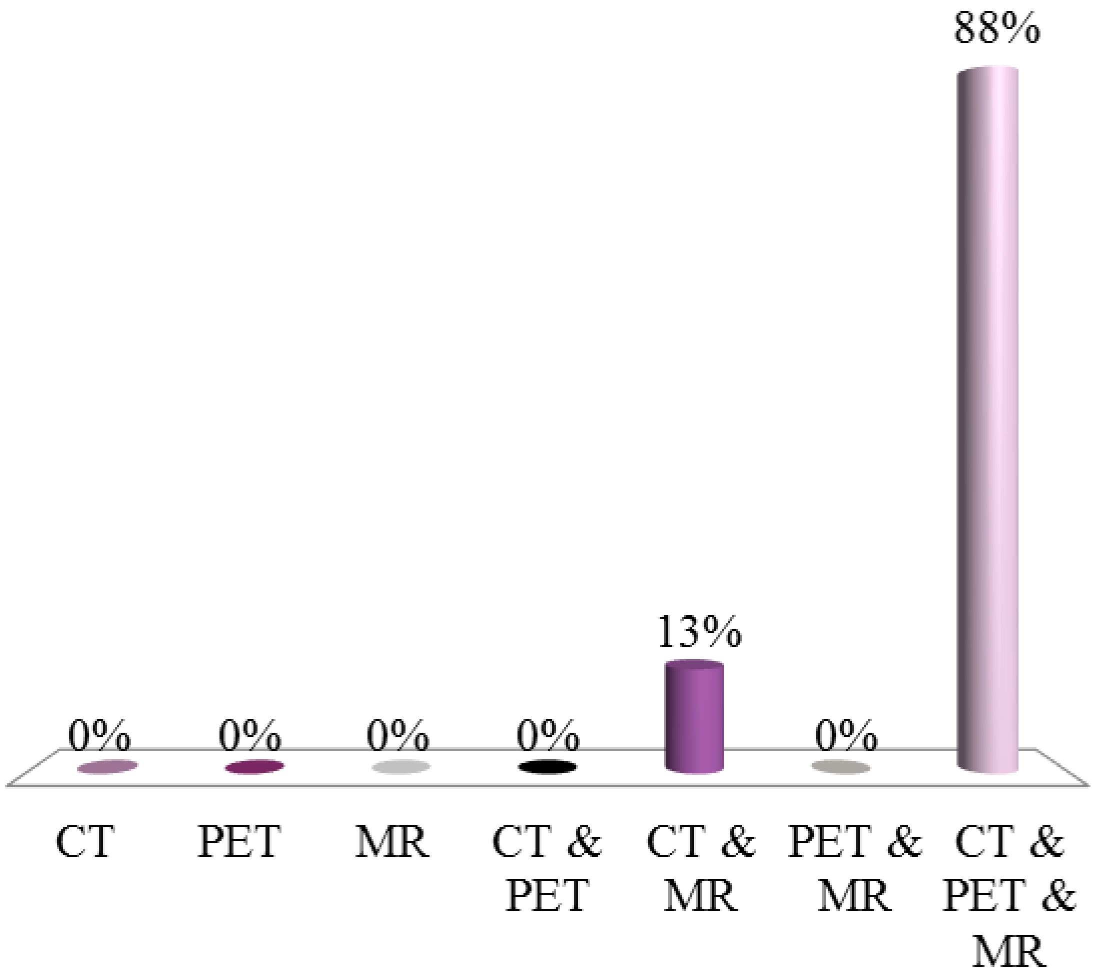
A. CT
B. PET/CT
C. PET
D. MR
E. PET/MR
F. None of the above



Multiple answers possible!

Which imaging modalities do we need for modern state of the art radiotherapy?

A. CT
B. PET
C. MR
D. CT & PET
E. CT & MR
F. PET & MR
G. CT & PET & MR



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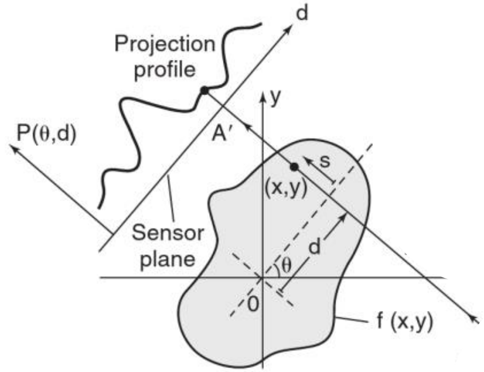
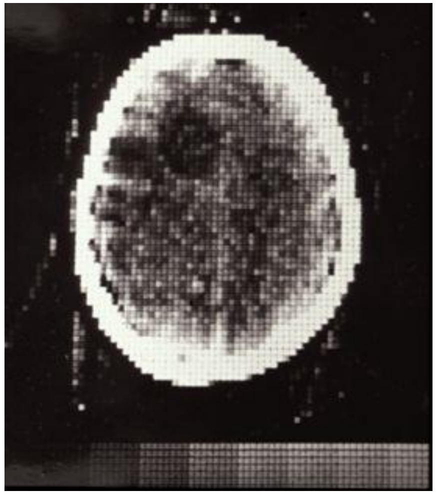
CT chronology



- 1917 mathematical grounds for CT reconstruction
- 1971 first clinical CT
- 1990 spiral CT
- 1993 dual slice
- 2003 32-slice
- Today : ultrafast volume-scanning
  dual source, dual energy



80x80 matrix
5 min rotation time

1024x1024 matrix
< 0.3 s rotation time

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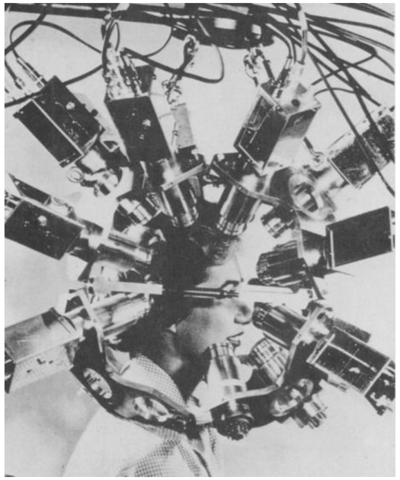
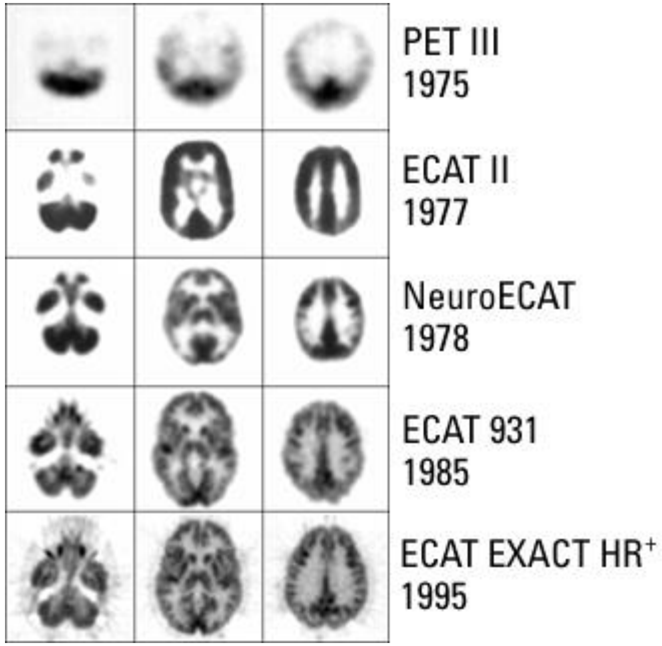
PET chronology

- 1930's radioactive tracers
- 1953/66 multidetector device
- 1975 back projection method for PET
- 1979 fluorine 18 deoxy glucose (FDG)
- 2000 PET/CT "medical invention of the year"

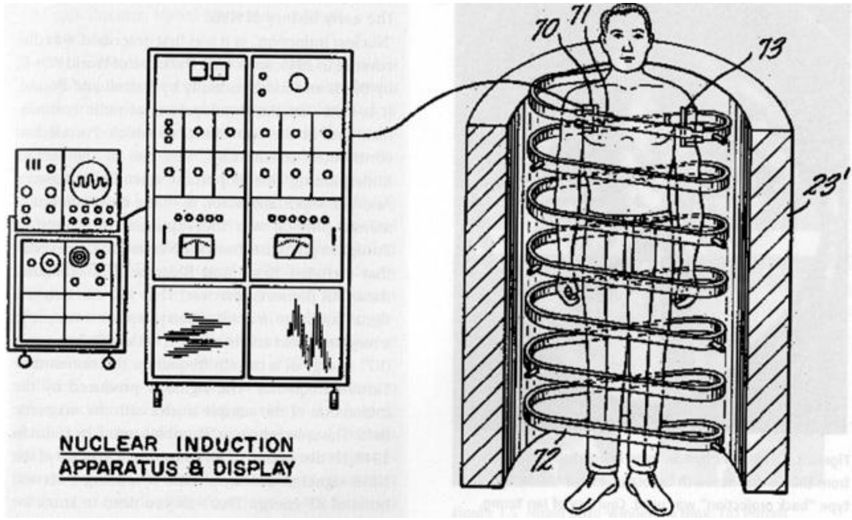


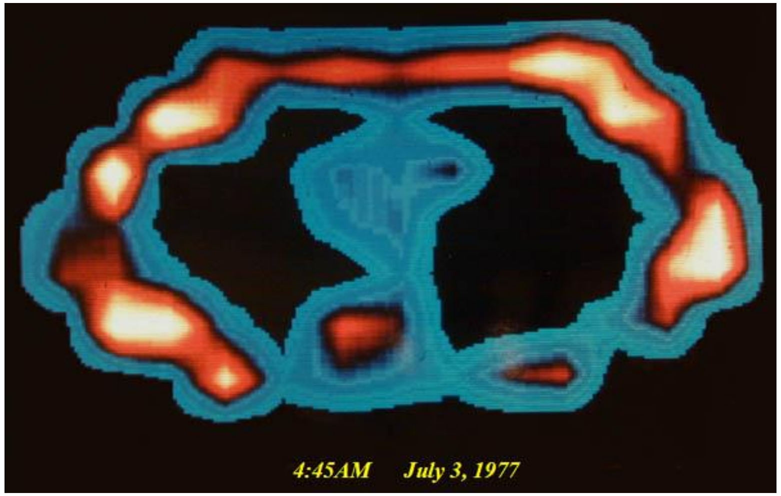
Wagner et al. 1998



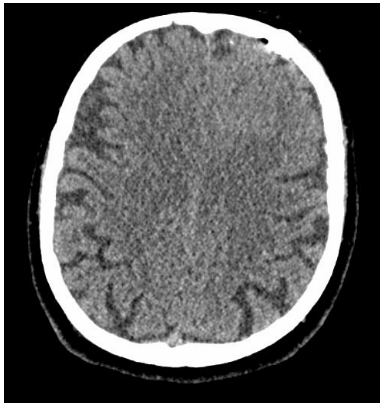
MR chronology

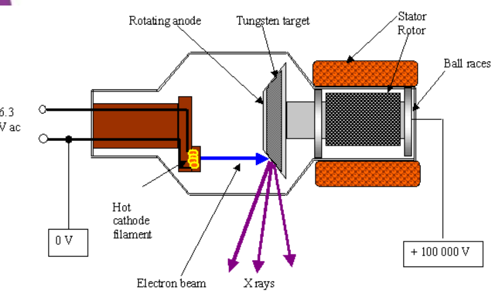
- 1937 nuclear magnetic resonance
- 1956 Tesla unit
- 1972 Damadian invention
- 1977 first MR scan
- 1993 functional MR



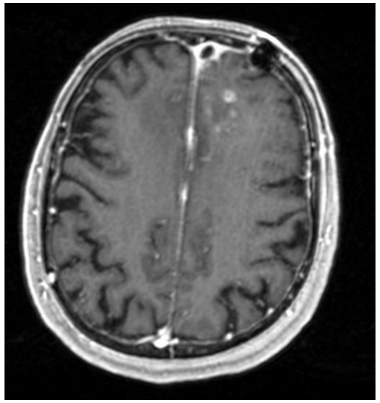


CT

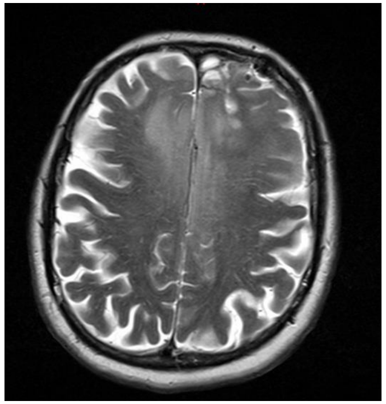




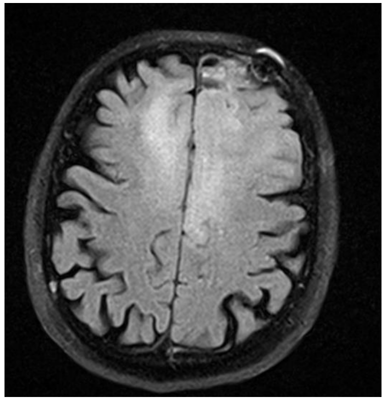
MR



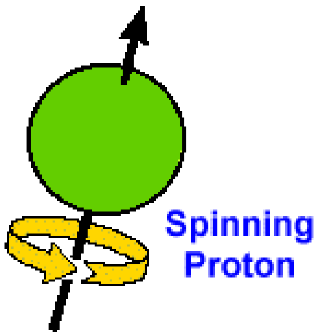
T1



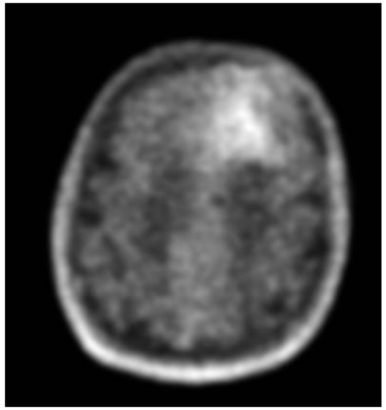
T2

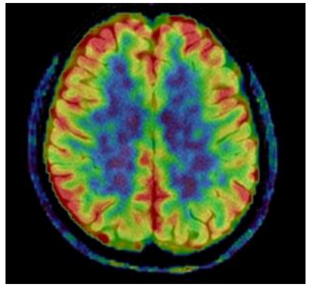


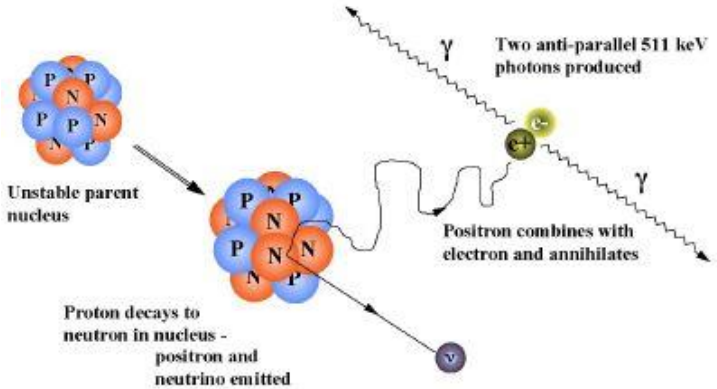
flair



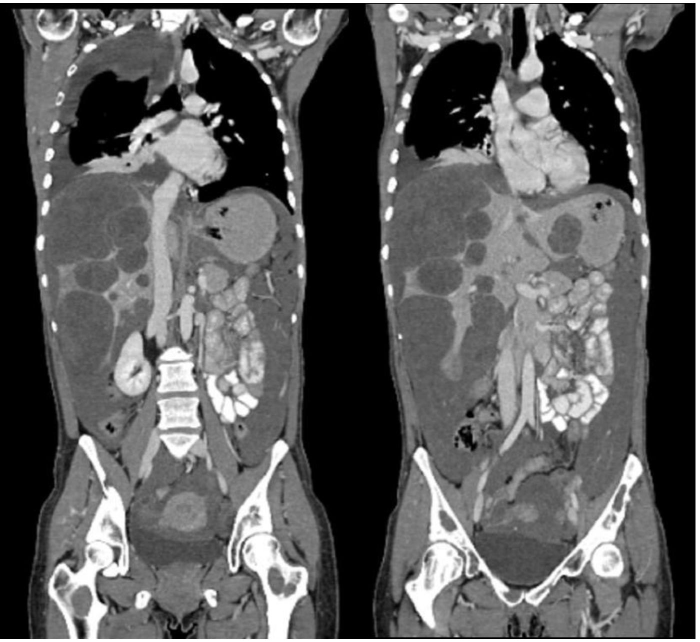
PET



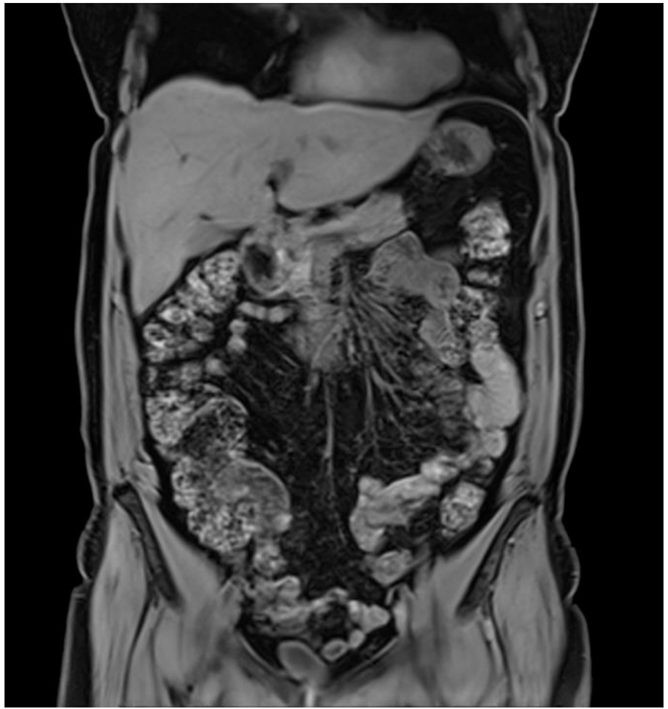




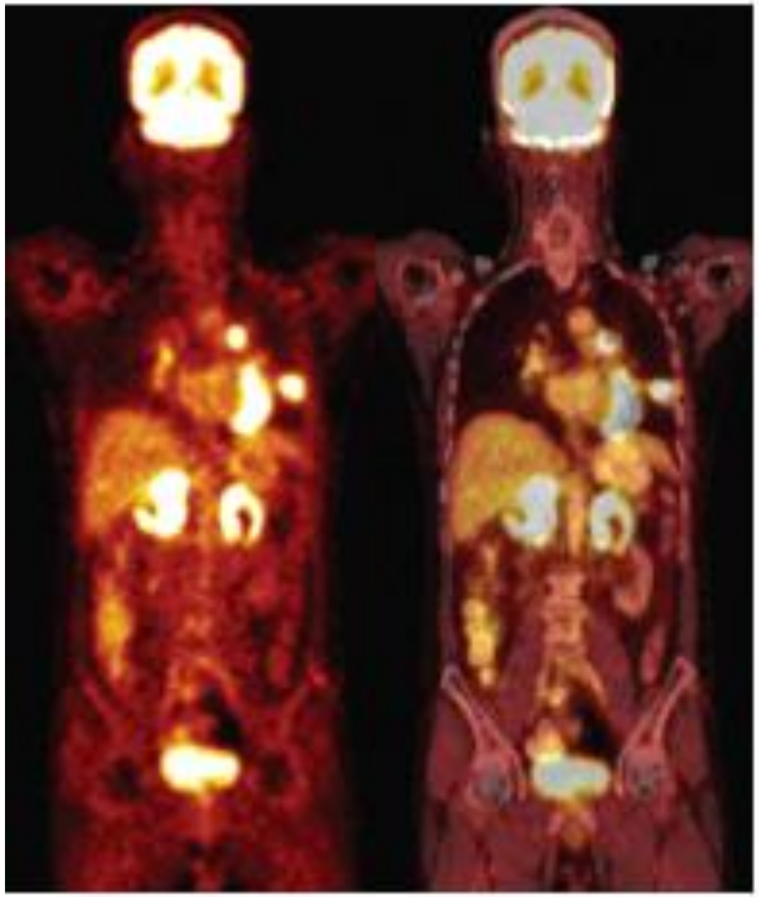
CT



MR



PET



What do we see?

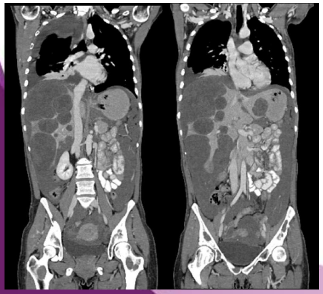
- Morphology
  - ➢ CT, MR

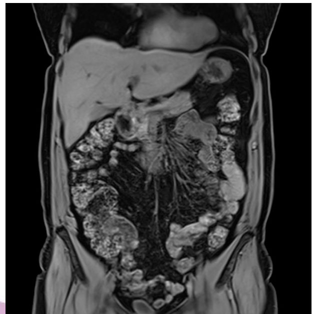
(patologic) anatomy

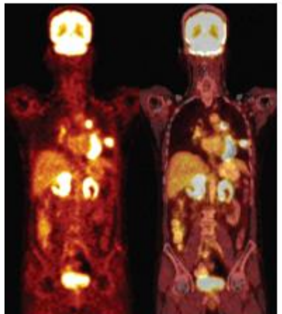
- Biological processes
  - ➢ PET, MR

Tumour metabolism

Perfusion
Organ function







Diagnostic imaging vs RT imaging

- Diagnostic
  - ➢ What is this?

- RT planning
  - ➢ Where is this?

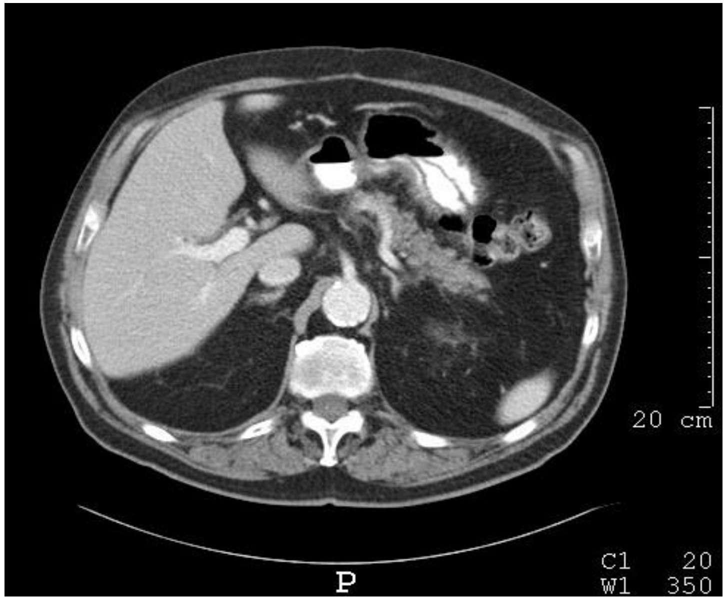
Why we need CT

CT numbers = Hounsfield units

The grey tones on the CT image represent the attenuation in every pixel/voxel

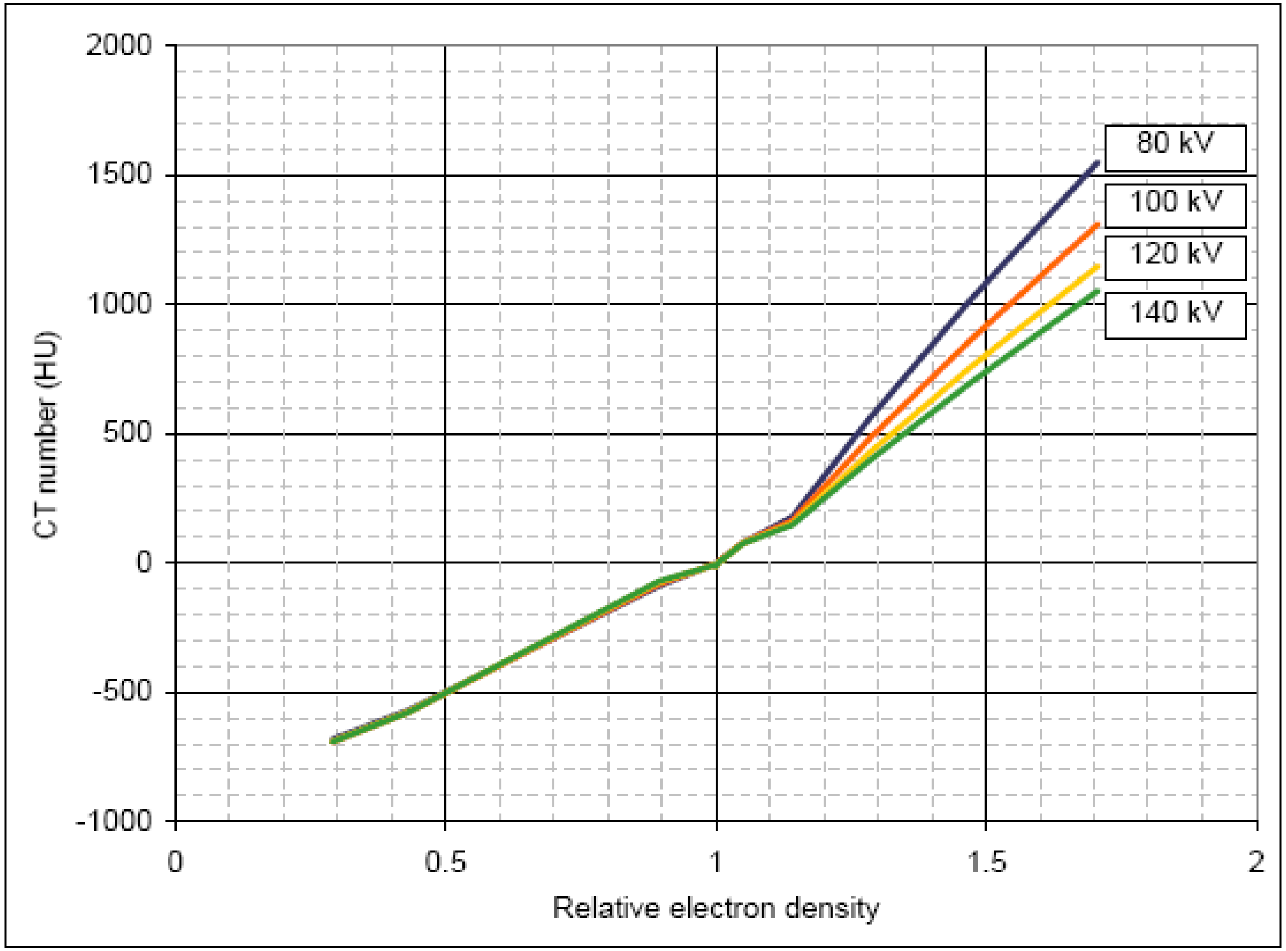
The grey tones are expressed in Hounsfield units (HU)
– CT numbers:

$$HU = \frac{\mu_{obj} - \mu_{water}}{\mu_{water}} \times 1000$$



Hounsfield units → electron density

Figure 4. CT number against electron density at a range of kVs



Necessary for dose calculation

Calibration curve needed for each applied kV

How well can we trust the imaging information?

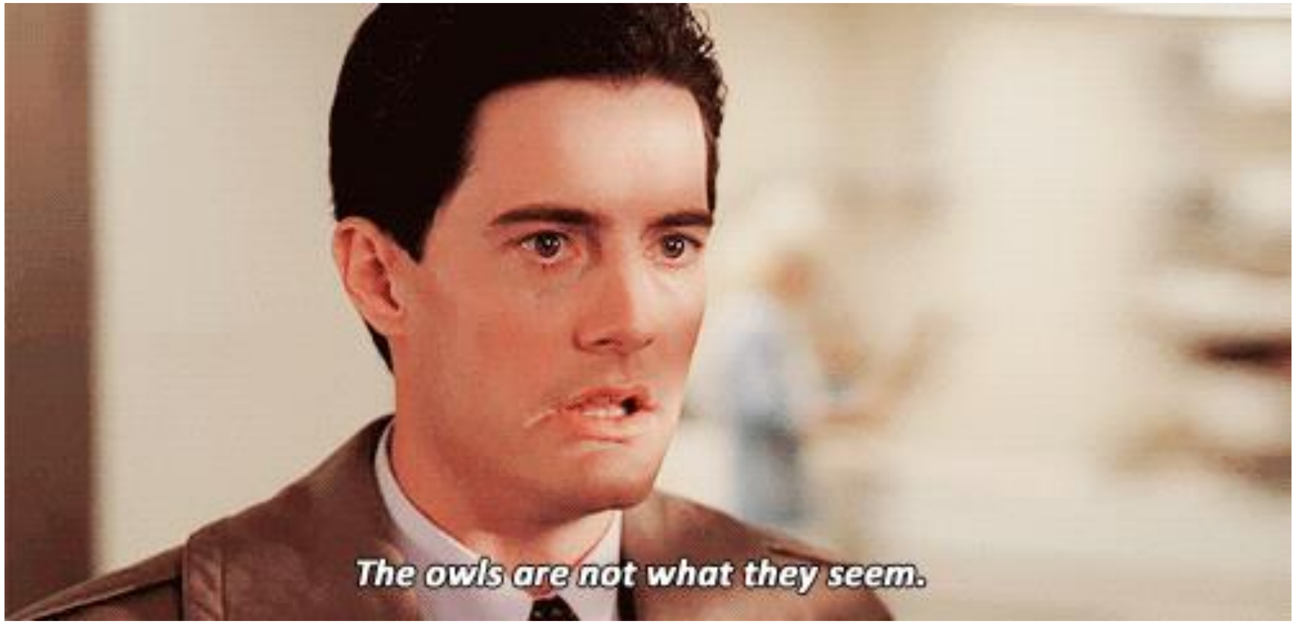


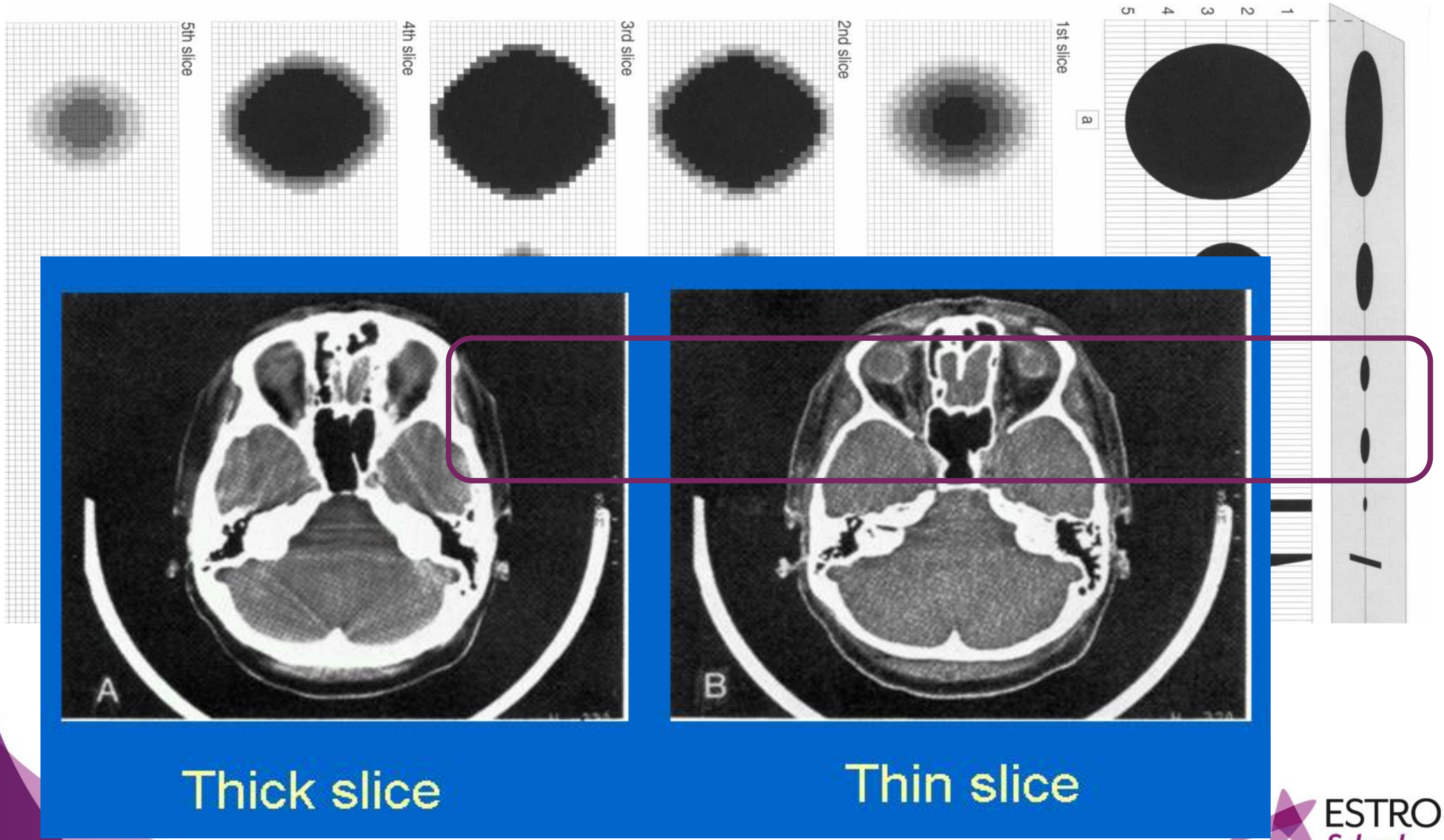
Image artifacts

Definition :

Systematic deviation between the HU in the reconstructed image and the objects correct attenuation's coefficient

- **Partial volume artefacts**
- **Streak artefacts**
- Ring artefacts
- Motion artefacts
- Noise

Partial Volume artefacts

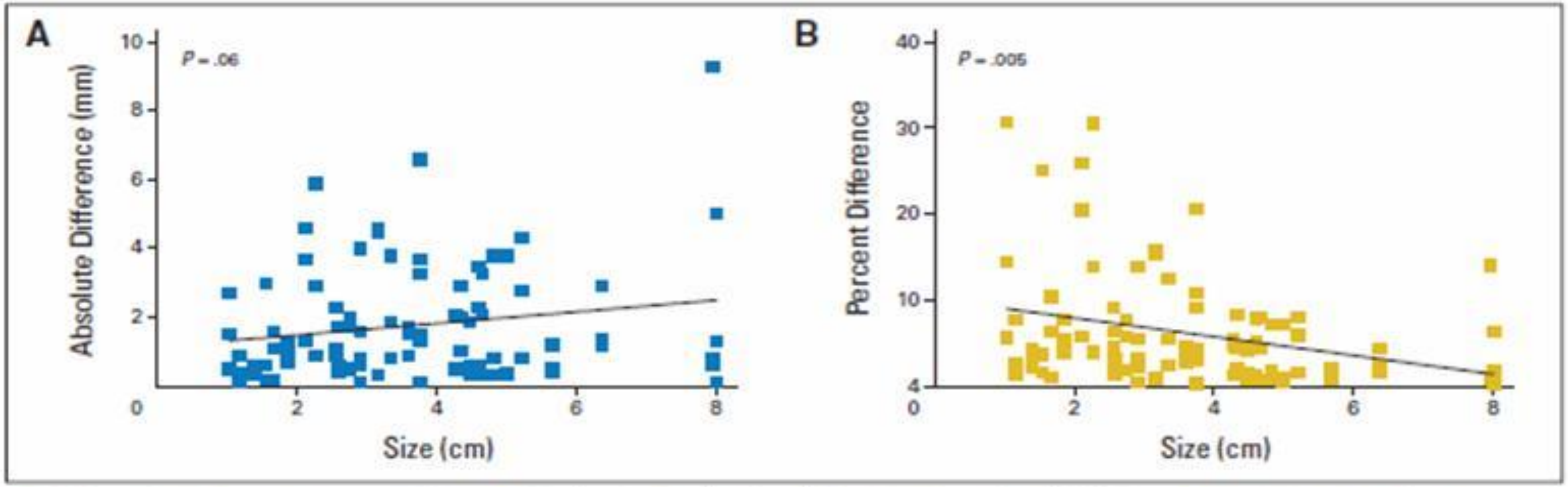


Variability of Lung Tumor Measurements on Repeat Computed Tomography Scans Taken Within 15 Minutes

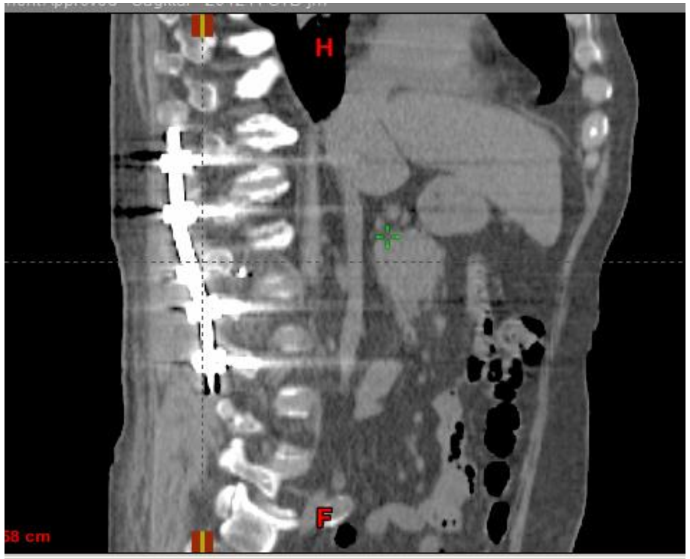
Table 3. Differences in Measurement Variability Depending on Lesion Size, As Calculated From Repeat CT Scans Performed Within 15 Minutes of Each Other

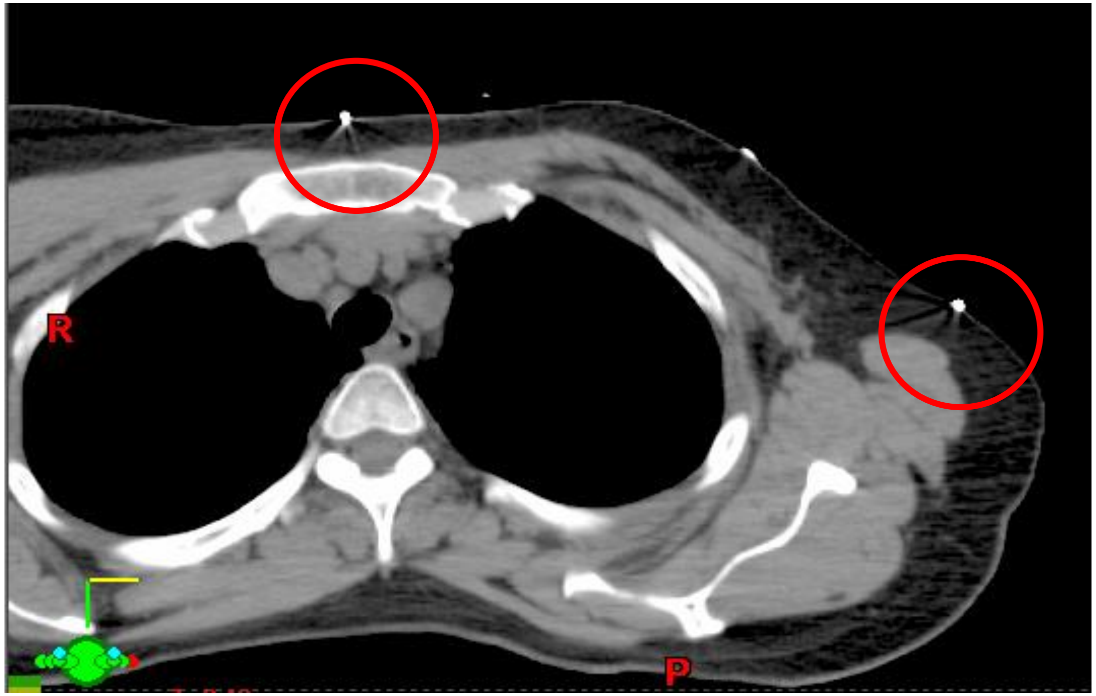
		Example Tumor		
Size of Tumor (cm)	Standard Deviation (mm)	Size (cm)	Range As a Result of Variability (cm)*	% Change As a Result of Variability
1-3	2.0	2	1.6-2.4	± 20
3-5	2.3	4	3.5-4.5	± 12
5-8	3.3	7	6.3-7.7	± 9

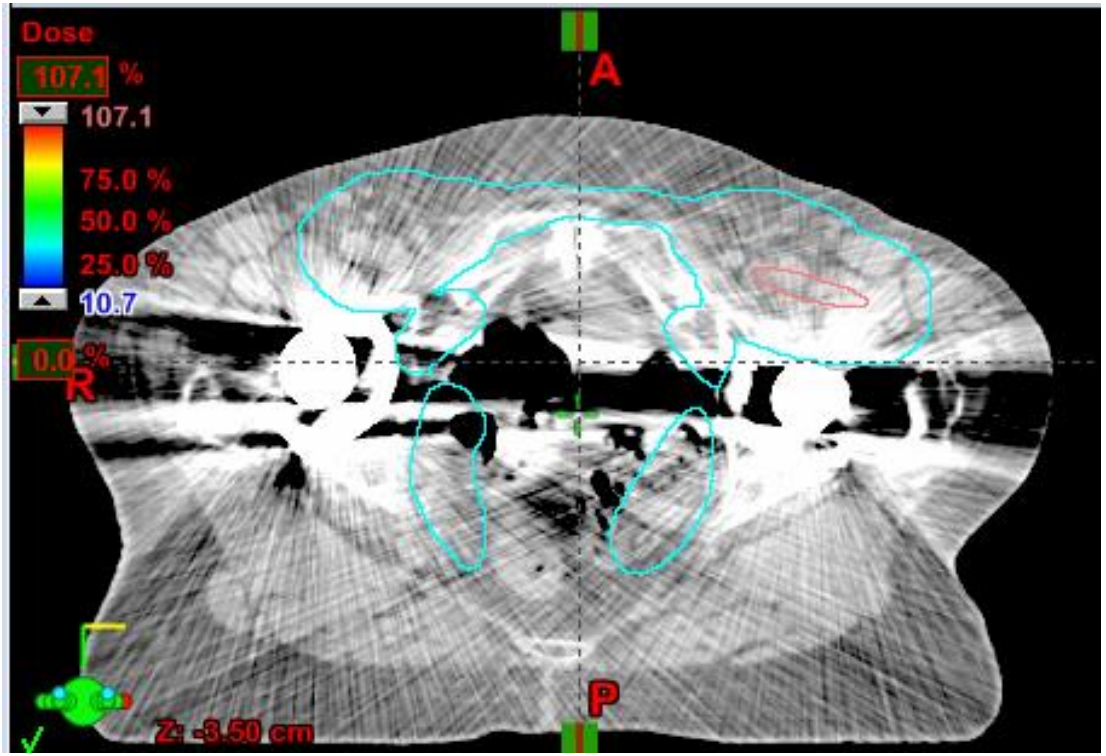
For a lesion measuring 4 cm,
CT variability can lead to measurements from 3.5 to 4.5 cm



Streak artefacts







Metal artifact reducton sw

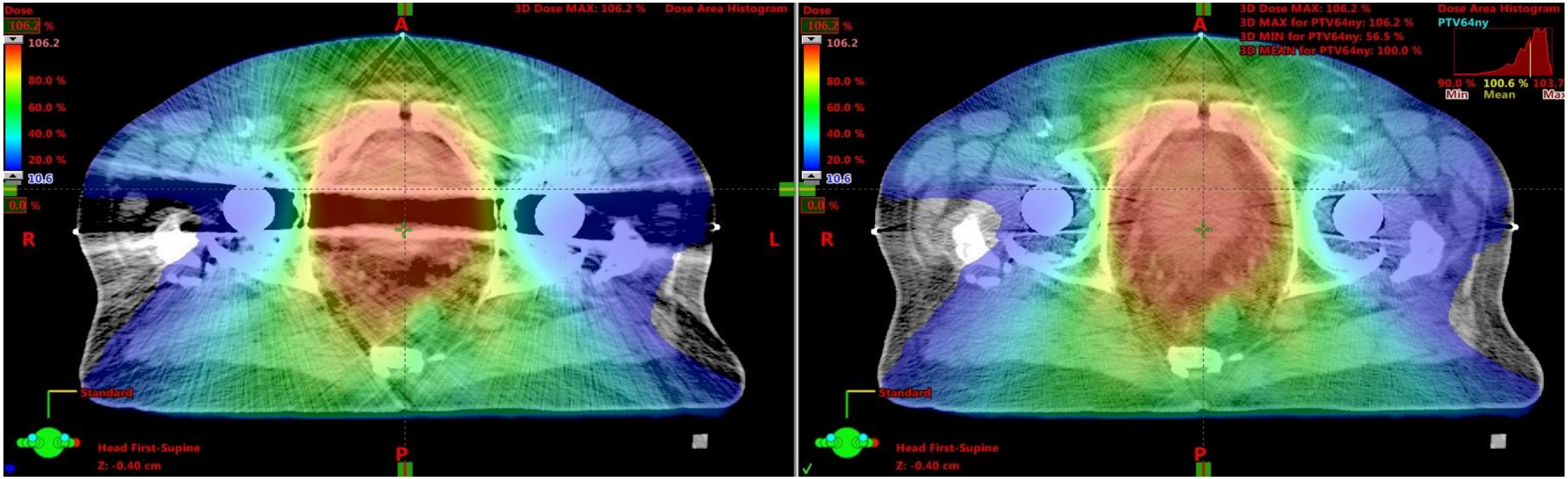
- Dual Energy CT (DECT)
  - Used two different X-ray energies
  - “Virtual monochromatic” scans

- Iterative metal artifact reduction software
  - MAR, iMAR, O-MAR…

MAR - impact on dose planning

Dose calculation for 10 patients with iMAR

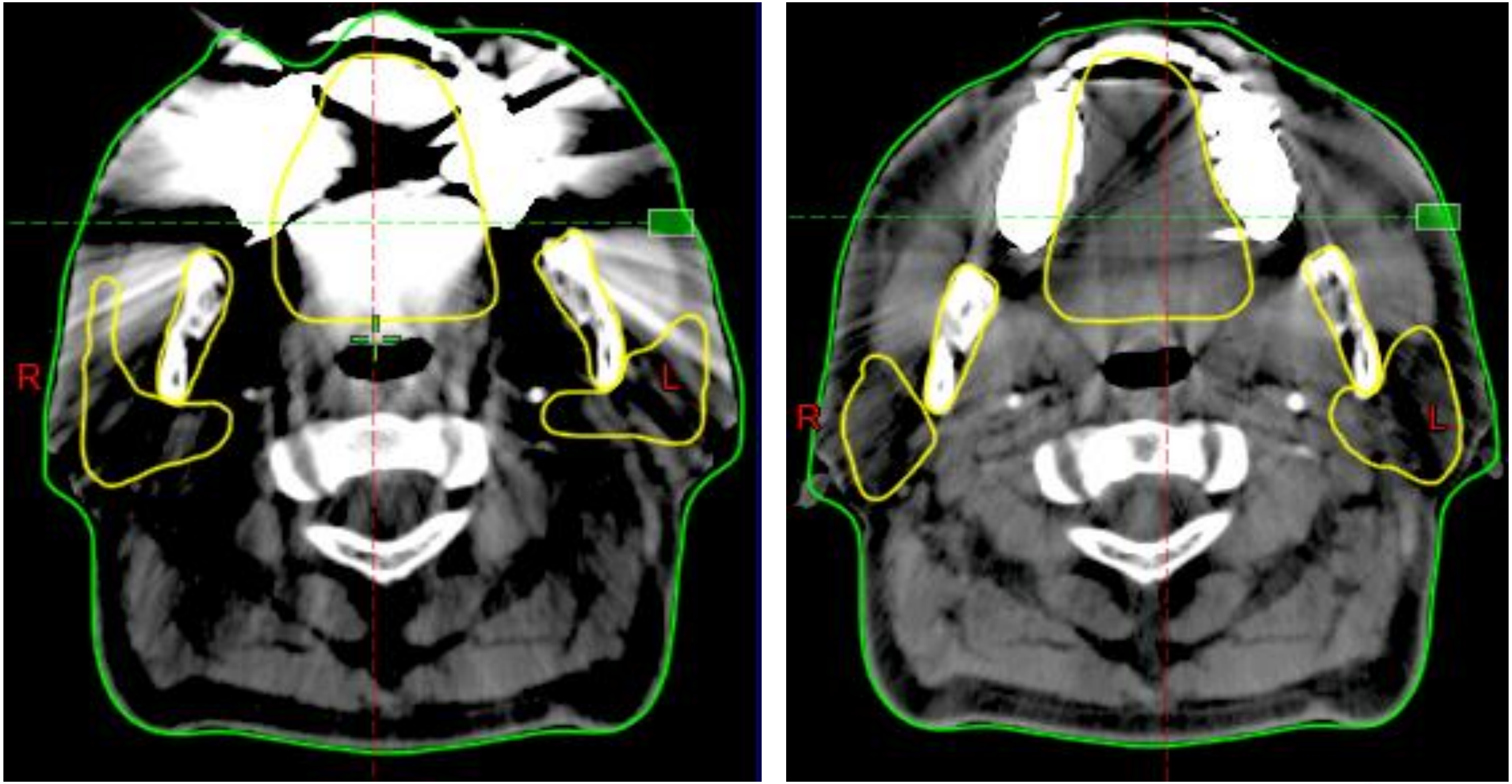
- No difference in dose compared to manual override



Images courtesy of Laura Rechner, Rigshospitalet

MAR- impact on contouring

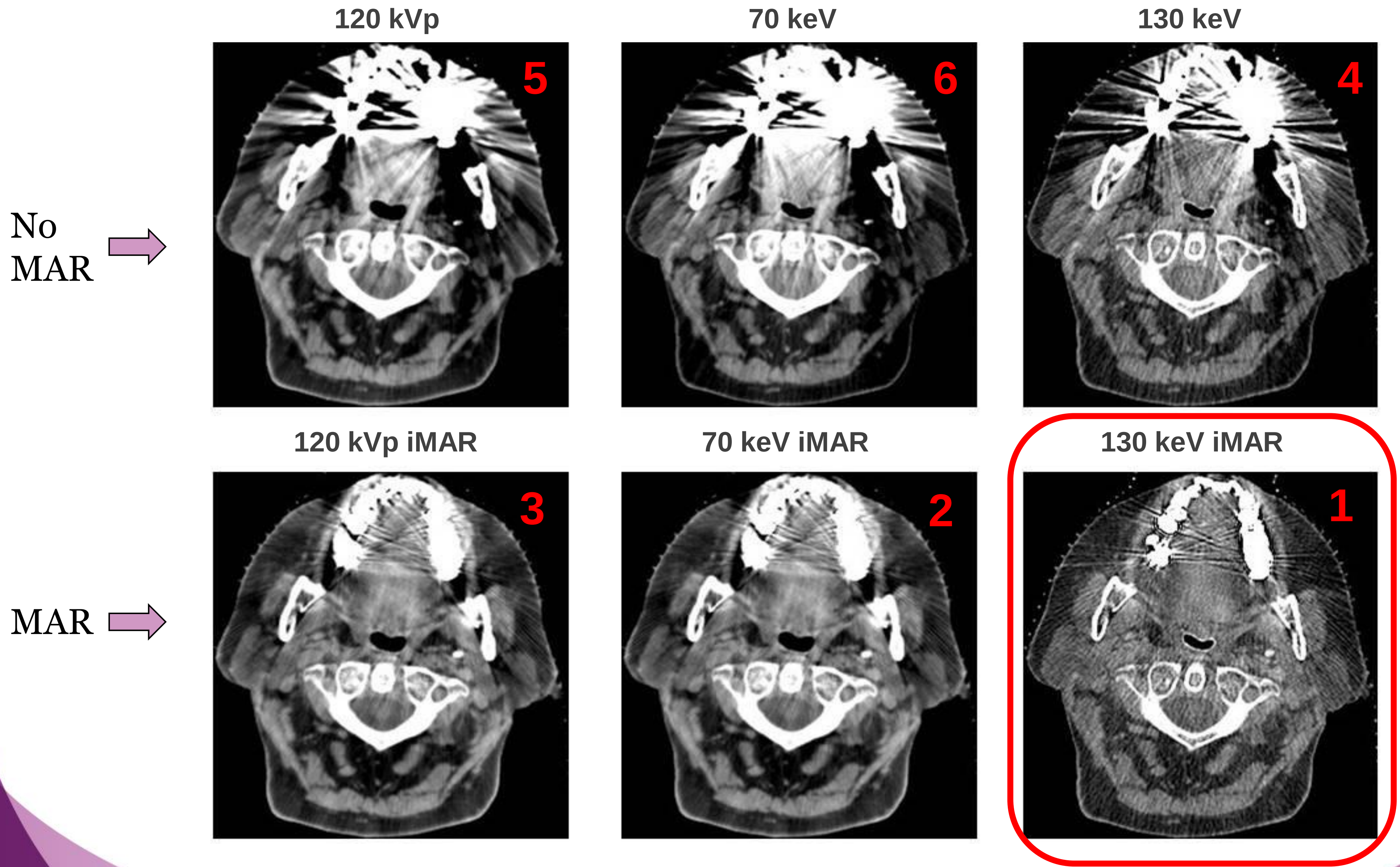
- Head and neck contouring by a radiation oncologist



Images courtesy of Jeppe Friborg, Rigshospitalet

MAR combined with dual energy scan

- **Which images do radiologists & oncologists prefer?**



Manuscript in preparation Kovacs, Rechner *et al*

MAR combined with dual energy scan

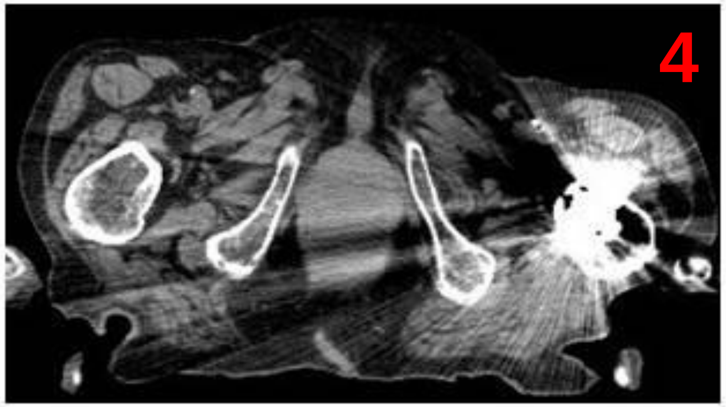
- **Which images do radiologists & oncologists prefer?**

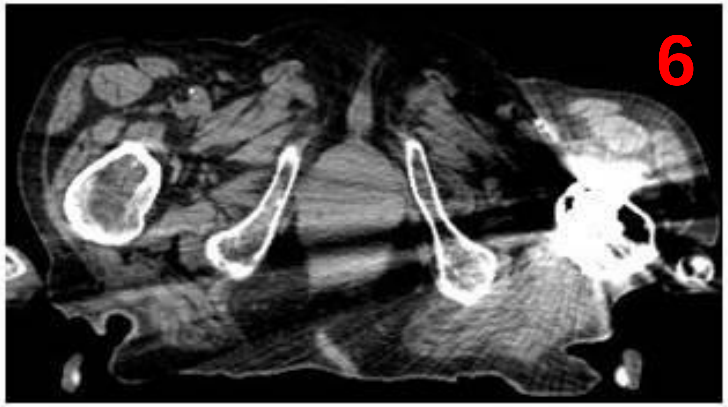
No MAR

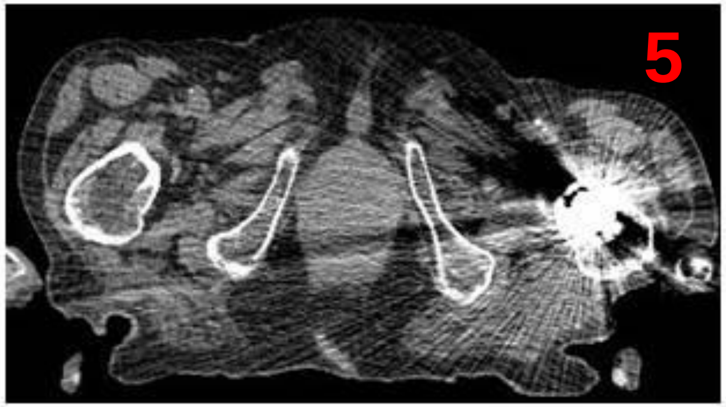
120 kVp

70 keV

130 keV



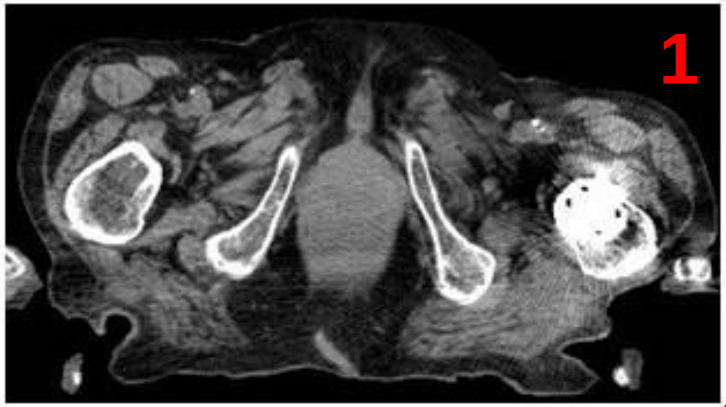


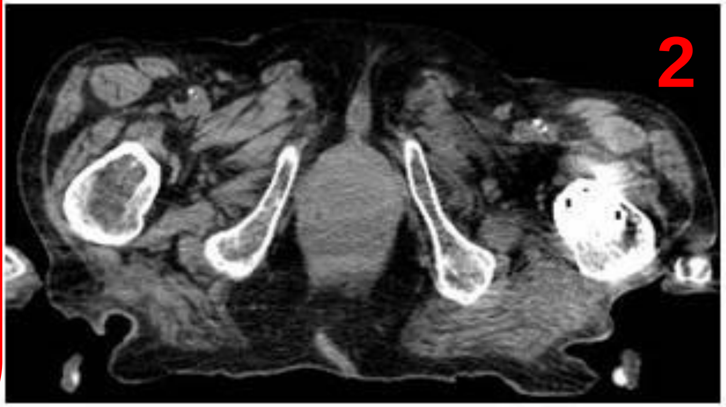


120 kVp iMAR

70 keV iMAR

130 keV iMAR





MAR

Manuscript in preparation Kovacs, Rechner *et al*

Imaging for RT planning

- Has to be precise
- Has to provide safe judgment of the extent of the disease

- CT images are base for treatment planning

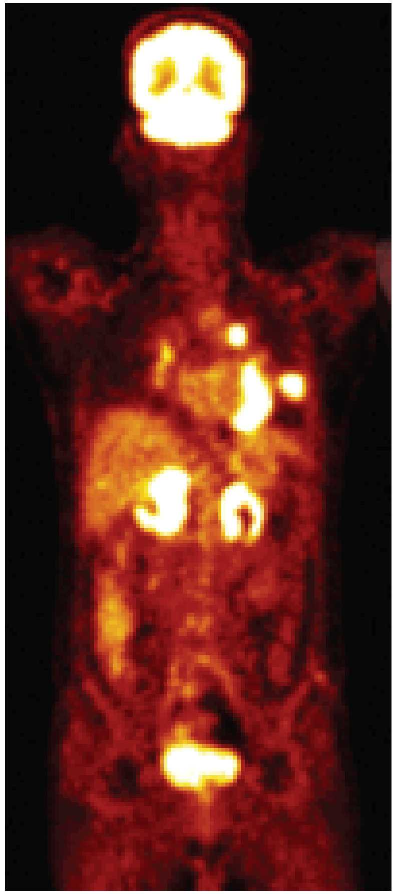
BUT

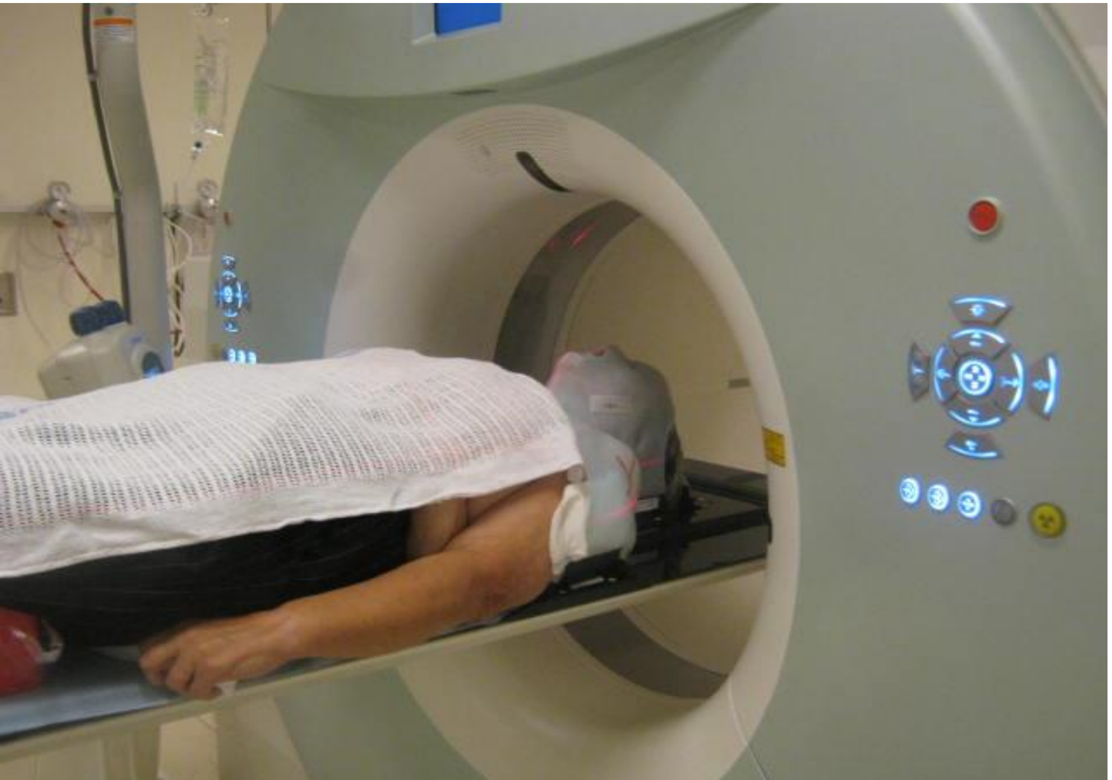
- On CT, it can be difficult to discriminate vital tumour tissue from scar tissue, oedema, atelectasis, surrounding soft tissu…

- CT can not stage correctly
  - ➢ detect small metastases
  - ➢ detect distant metastases

Added value of PET CT for radiotherapy

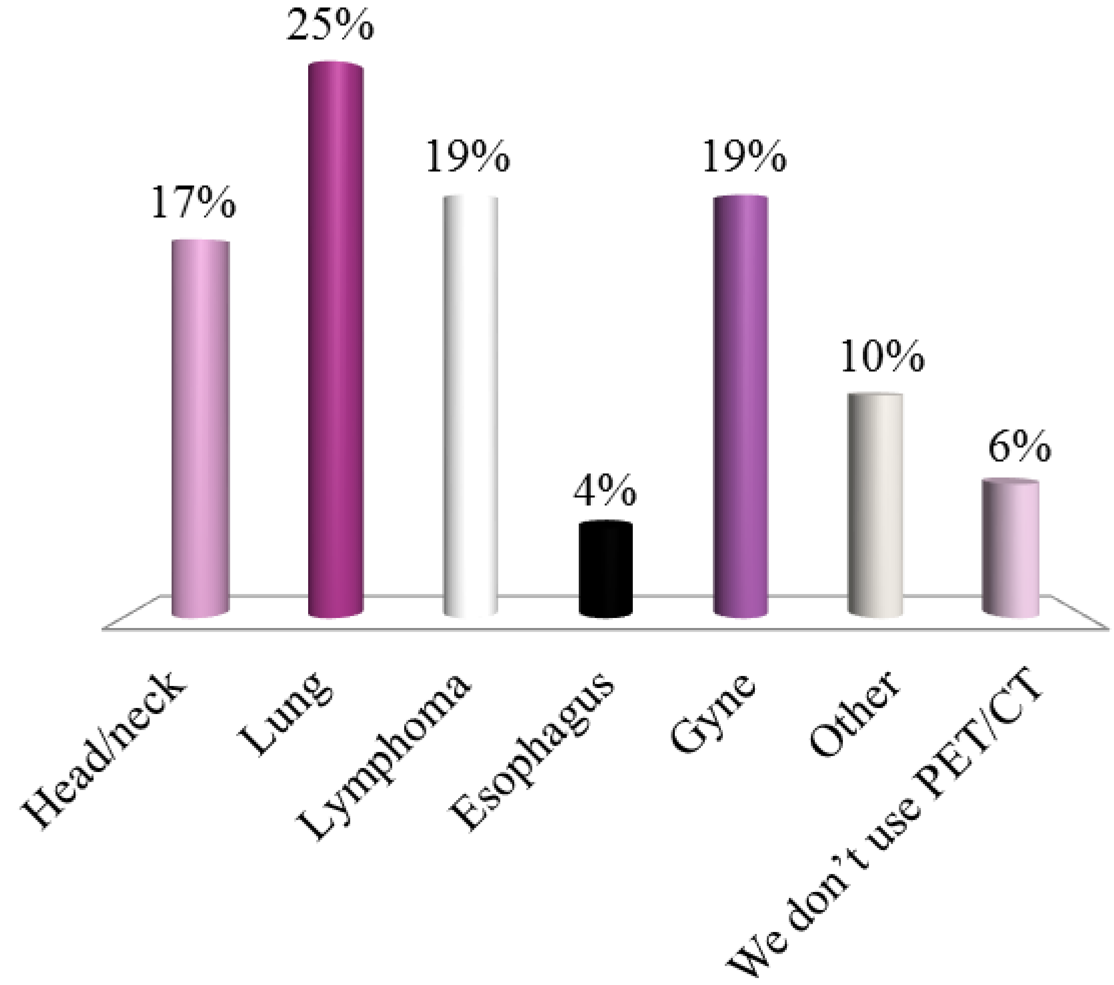
- Improved delineation consistency
- Improved staging





Which sites do you plan with PET/CT?

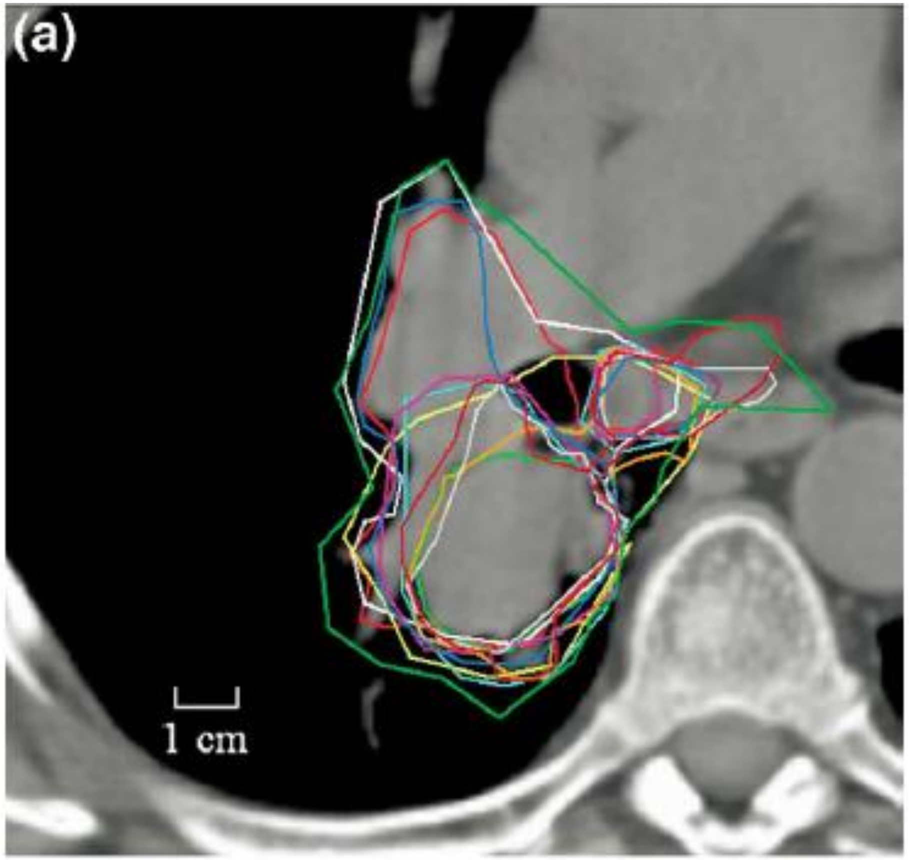
A. Head/neck
B. Lung
C. Lymphoma
D. Esophagus
E. Gyne
F. Other
G. We don’t use PET/CT



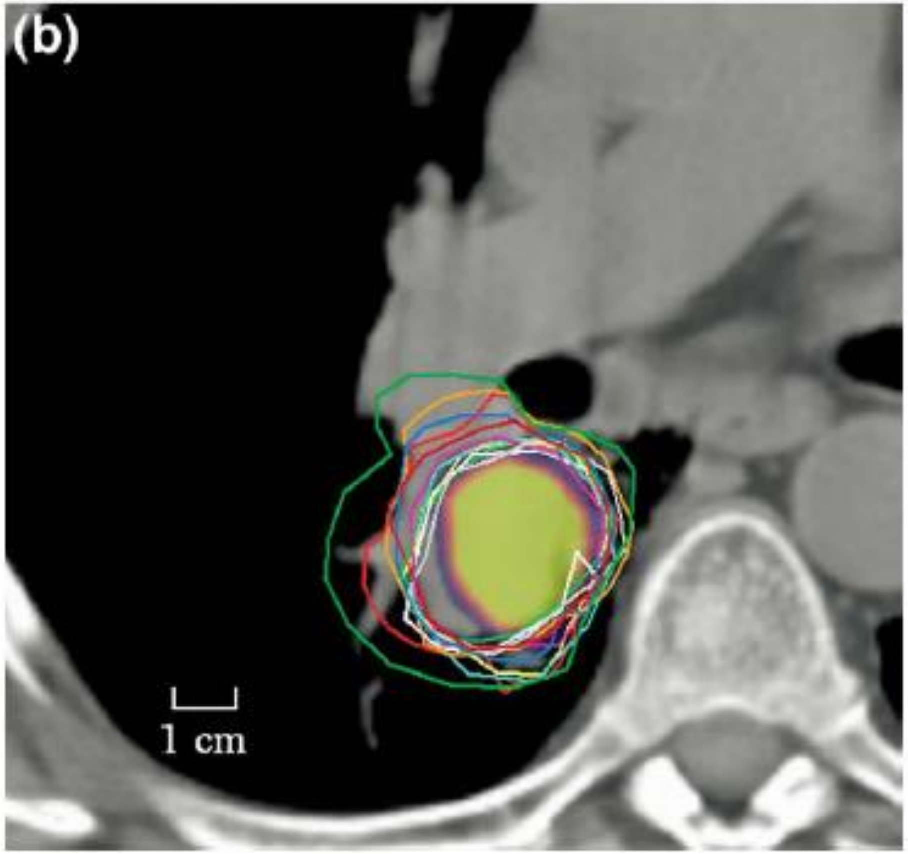
Multiple answers possible!

Improved delineation consistency

CT based



PET/ CT based

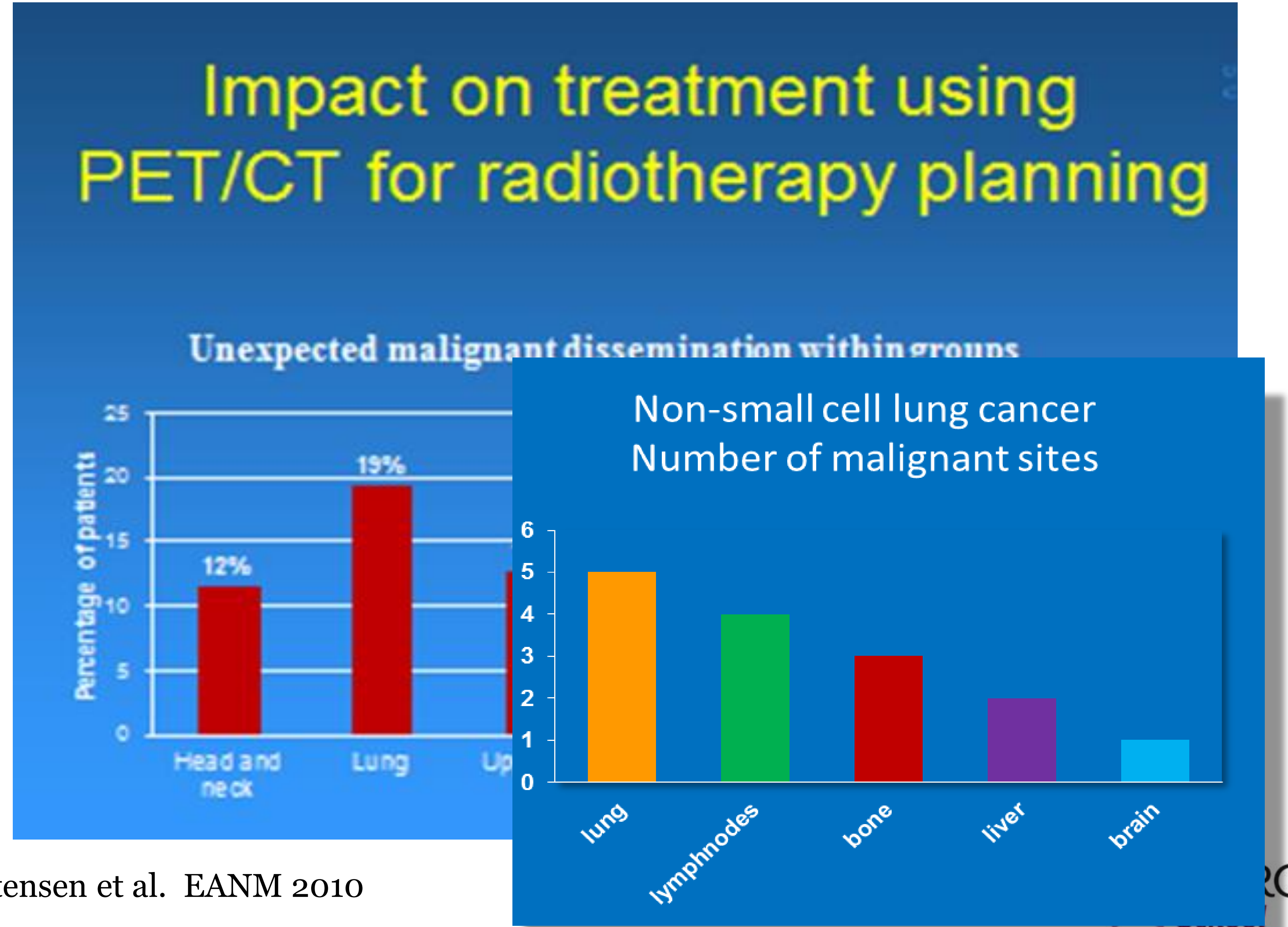


Steenbakkers IJROBP 2006

Improved staging

Always WB PET/CT at therapy scan.

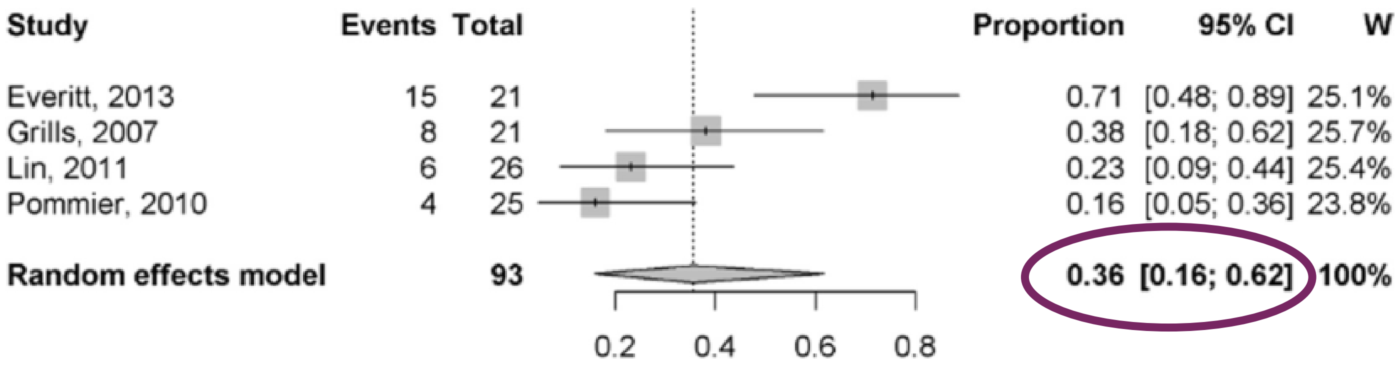
Changing treatment strategy!



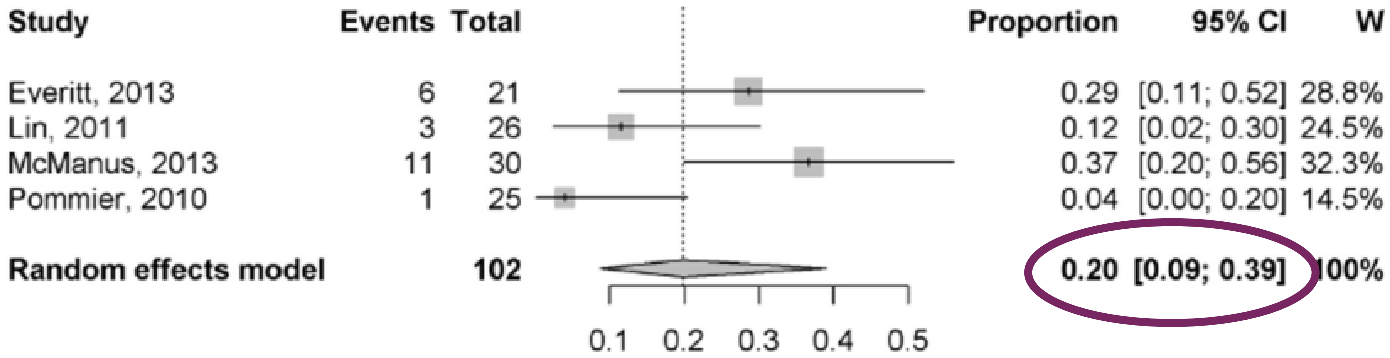
Christensen et al. EANM 2010

Impact of PET in lung cancer RT

Staging PET not available



Change in target definition



Change in treatment intent

Hallquist et al. RO 2017

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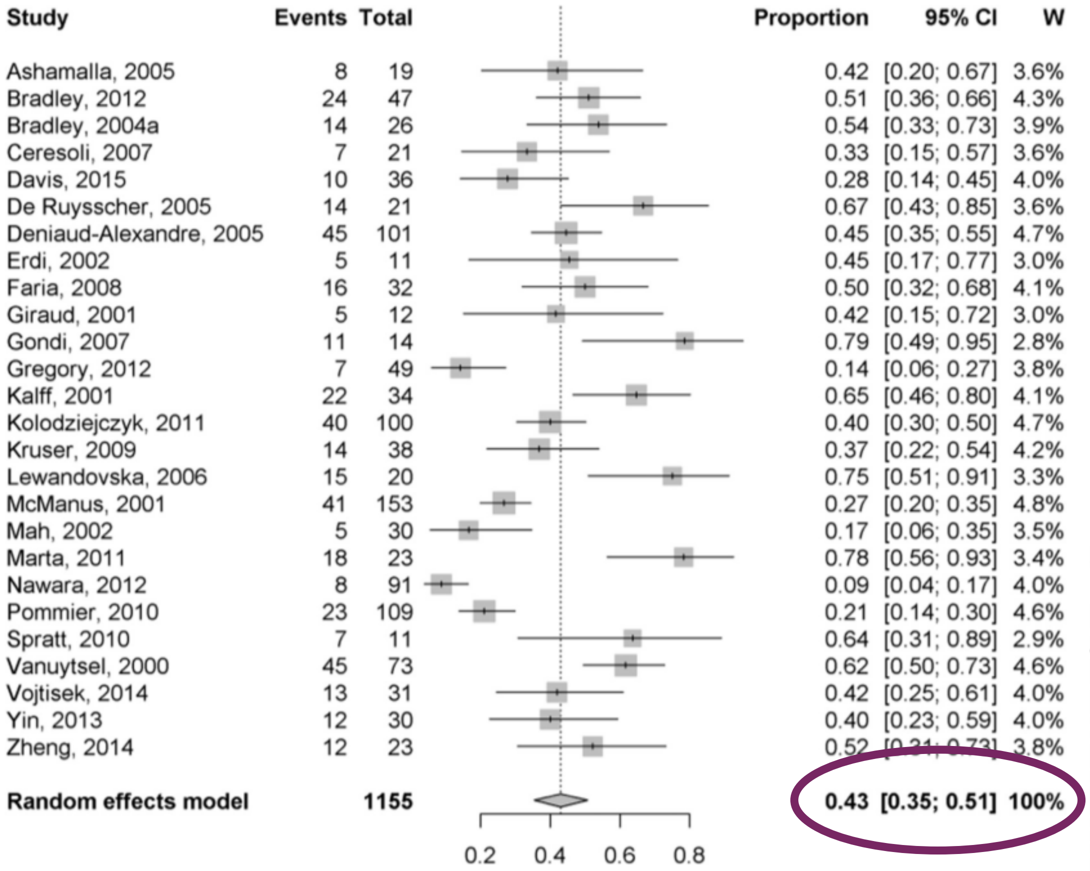
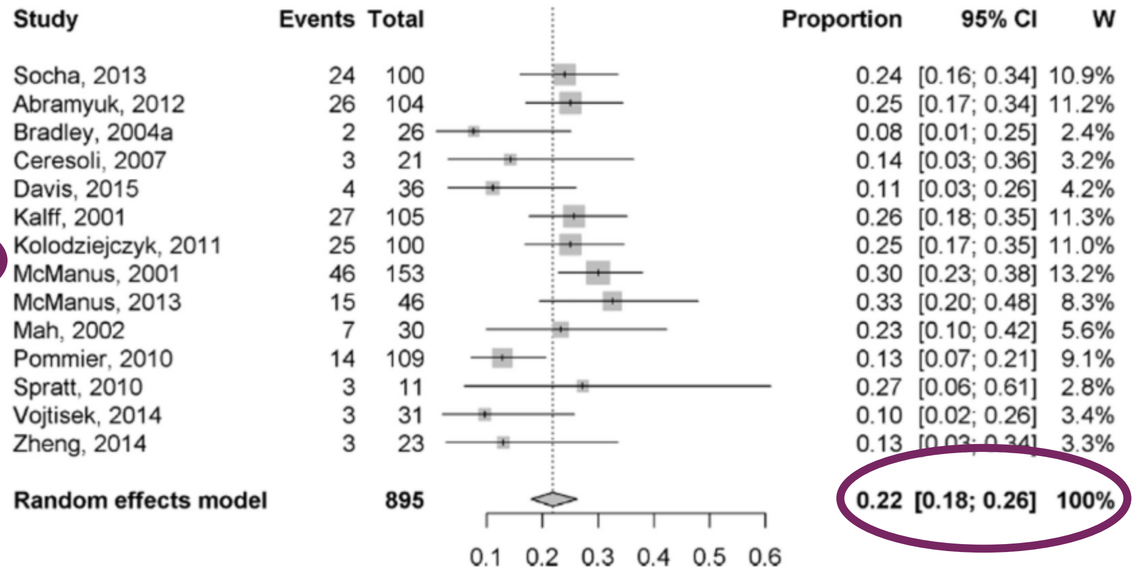
Impact of PET in lung cancer RT

Staging PET available



Change in target definition

Change in treatment intent



Hallquist et al. RO 2017

Impact of PET in lung cancer RT

- Change in target definition: in 2 out of 5 patients
- Change in treatment intent: in 1 out of 5 patients

Radiotherapy and Oncology 123 (2017) 71–77

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Radiotherapy and Oncology

journal homepage: www.thegreenjournal.com

Systematic review

Positron emission tomography and computed tomographic imaging (PET/CT) for dose planning purposes of thoracic radiation with curative intent in lung cancer patients: A systematic review and meta-analysis

CrossMark

Andreas Hallqvist [a,*], Charlotte Alverbratt [a], Annika Strandell [b], Ola Samuelsson [b], Emil Björkander [c], Ann Liljegren [c], Per Albertsson [a]

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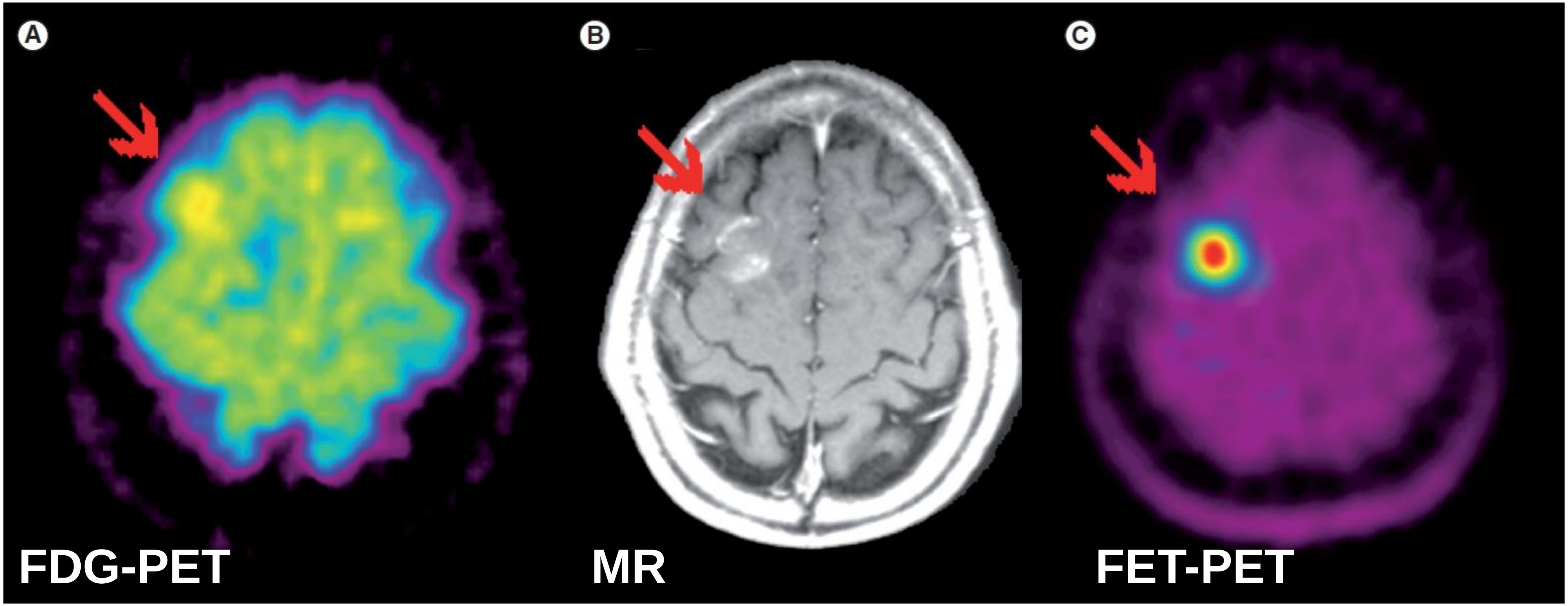
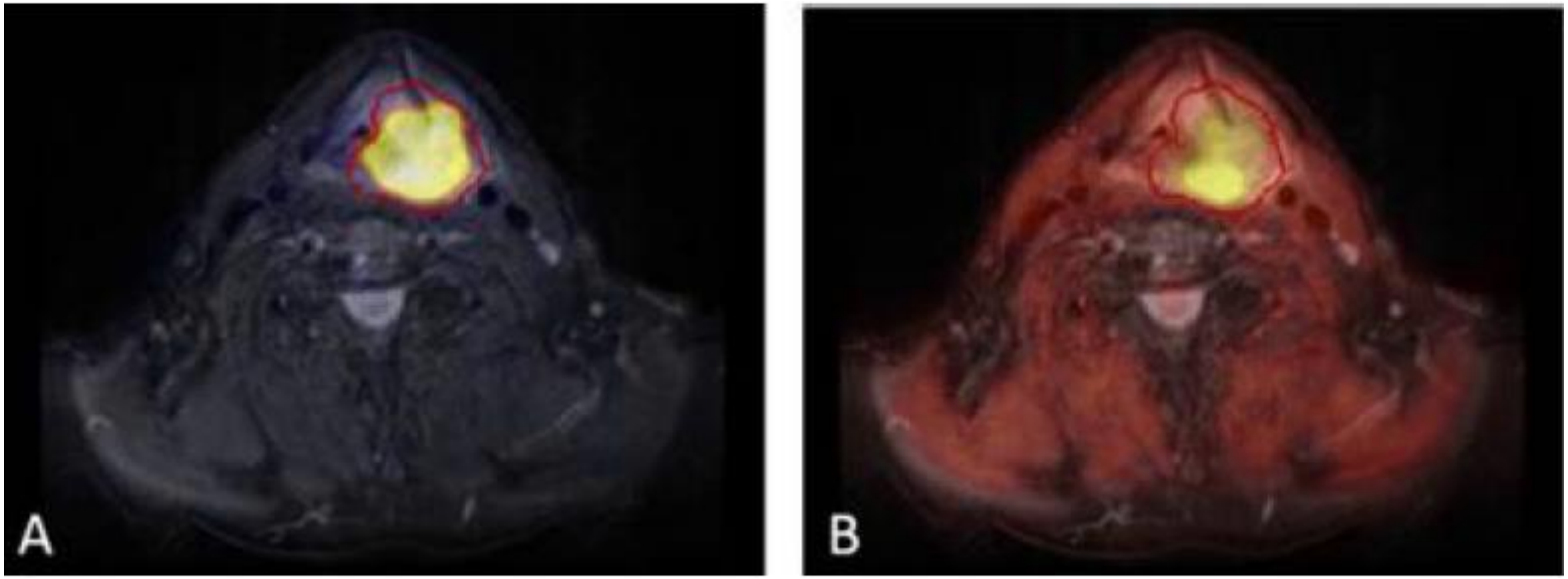
PET imaging of brain tumours



- 18F-Fluoro-Ethyl-Tyrosin (FET), aminoacid uptake

BD Kläsner et al. *Expert Rev. Anticancer Ther 2010*

PET imaging of hypoxia with FMISO

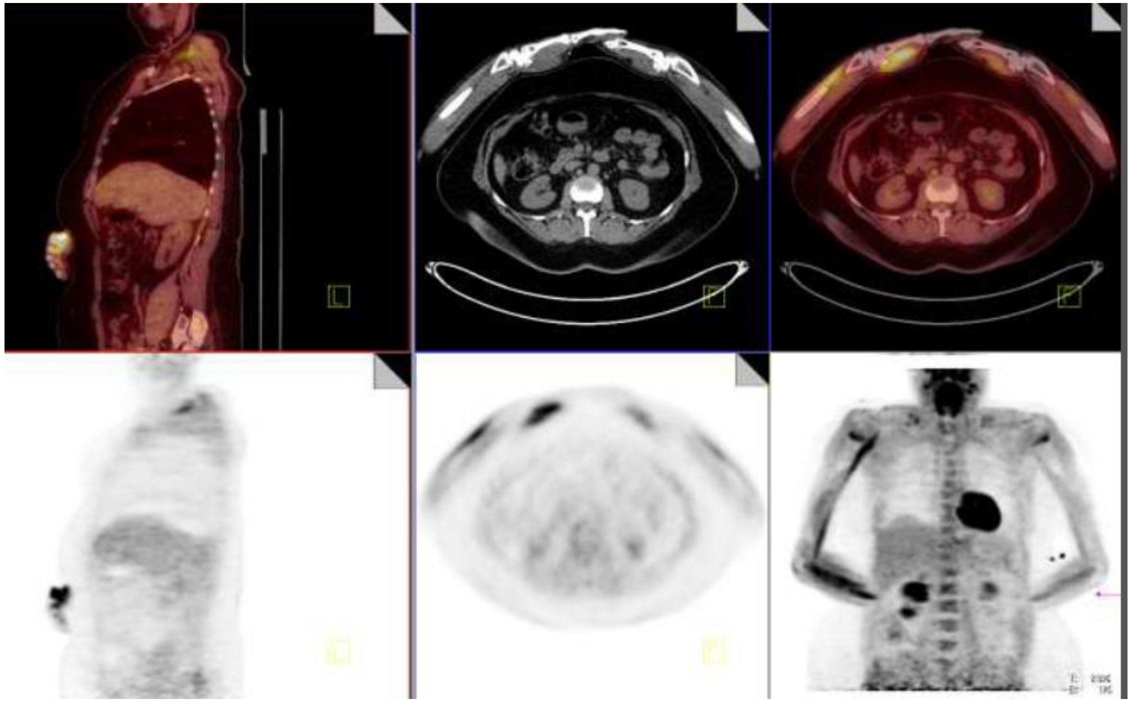


- Hypoxia area is associated with high risk of locoregional failure

Thorwarth BJR 2015

Pitfalls

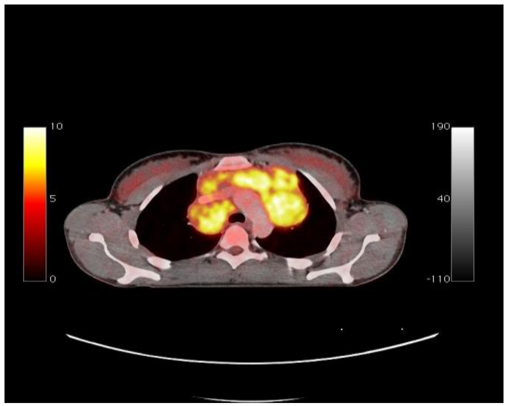
- FDG is not specific
  - ➢ Not all ”hot-spots” are malignant



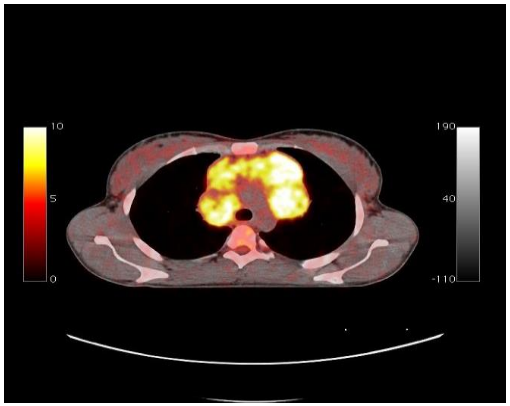
Courtesy of TL Klausen

- Motion blurs the FDG uptake
  - ➢ Is it a small lesion, with high degree of motion and high SUV uptake?
  - ➢ Is it a large lesion, without motion and low SUV uptake?

Free breathing



Breath hold



Courtesy of M Aznar

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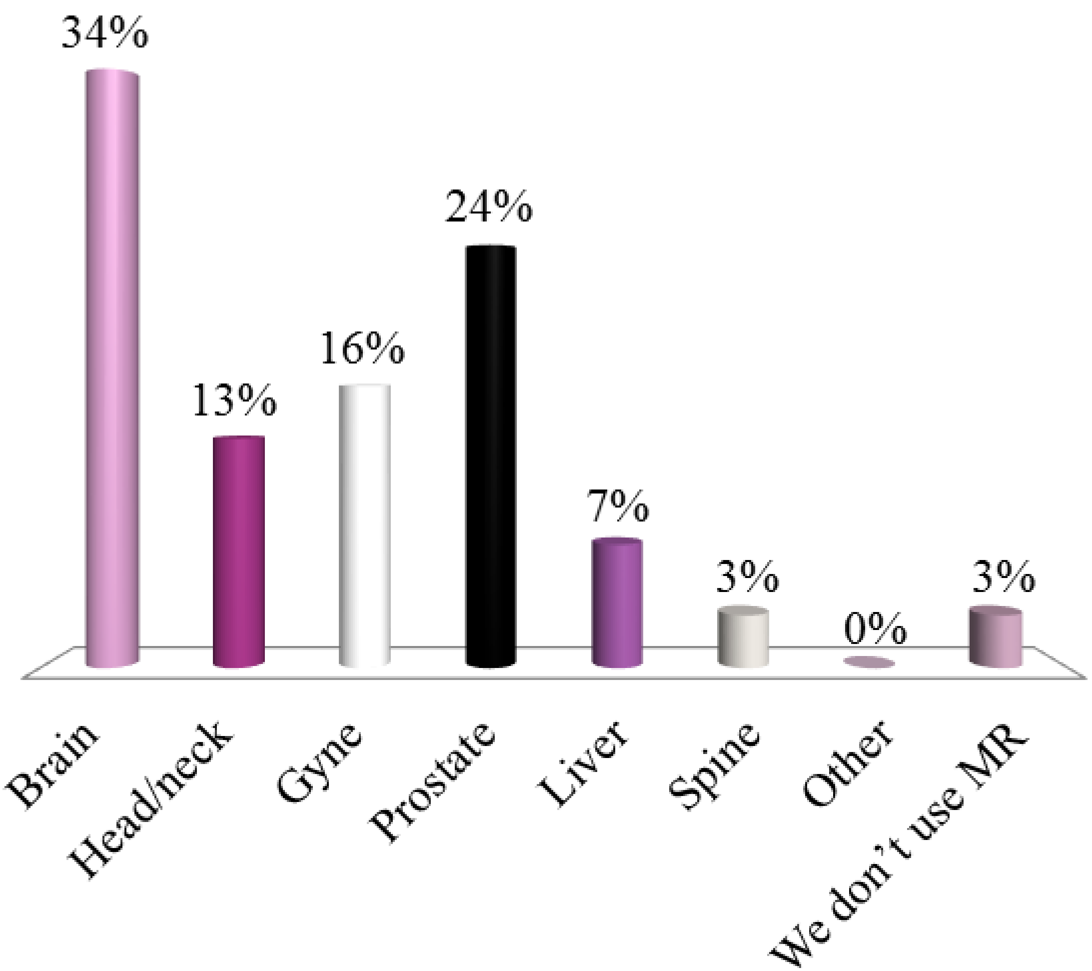
Added value of MR imaging for RT

- Superior soft tissue contrast

Which sites do you plan with MR?

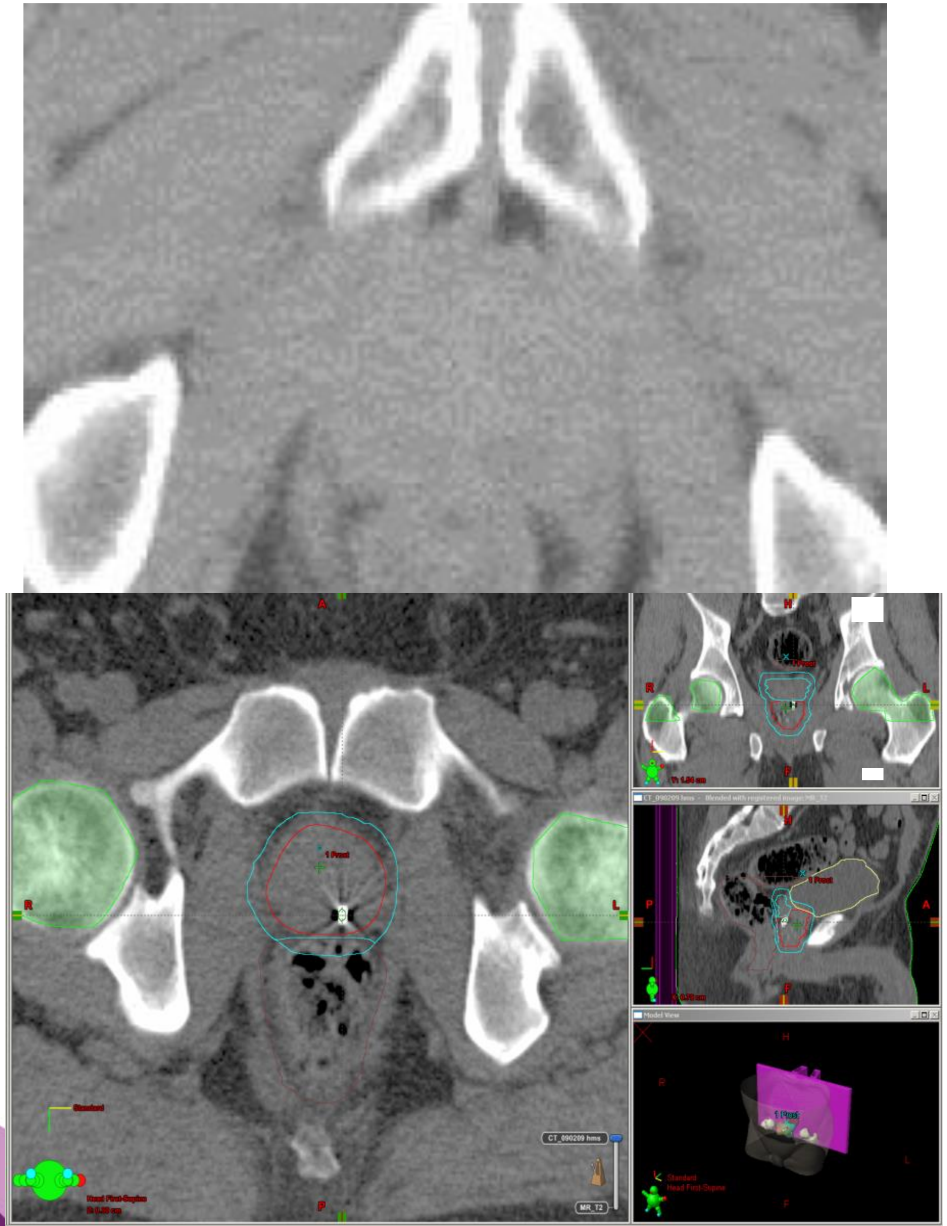
A. Brain
B. Head/neck
C. Gyne
D. Prostate
E. Liver
F. Spine
G. Other
H. We don't use MR



Multiple answers possible!

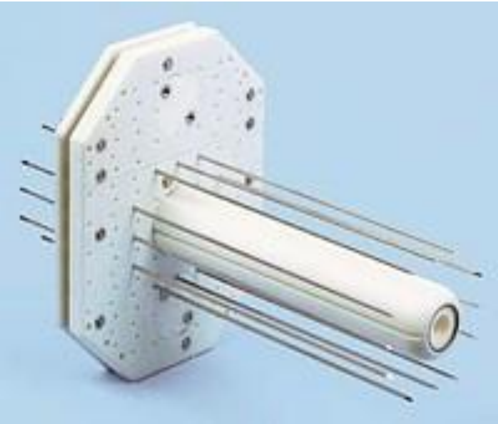
Prostate cancer

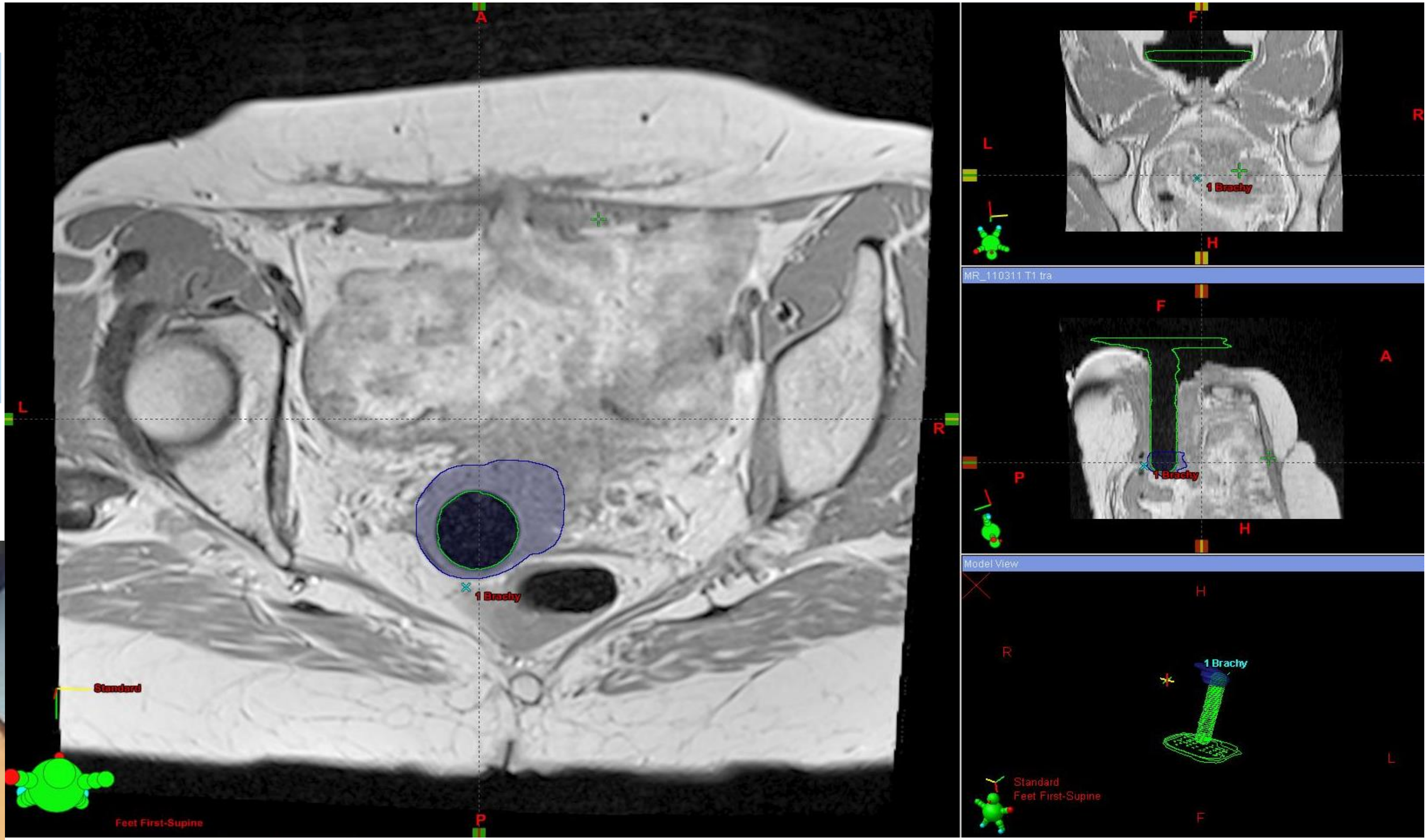
CT



MR

Cervix cancer - brachytherapy





dummy template for interstitial brachytherapy

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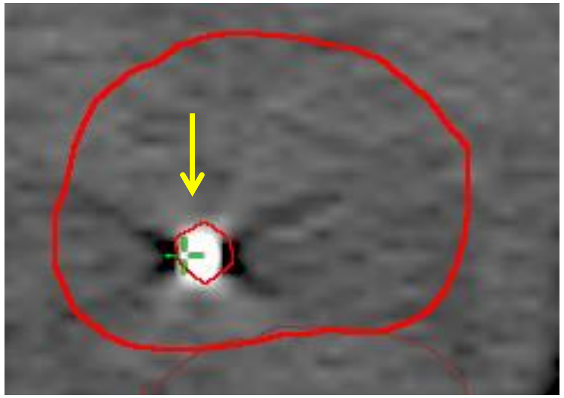
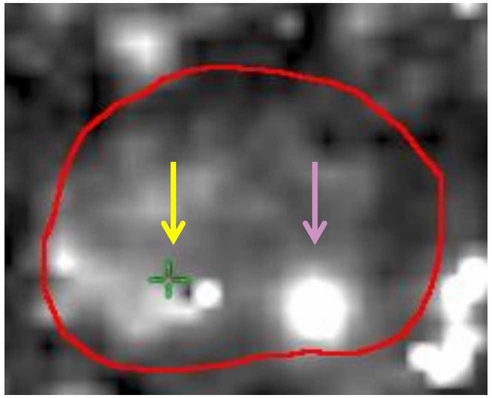
Functional imaging with MR

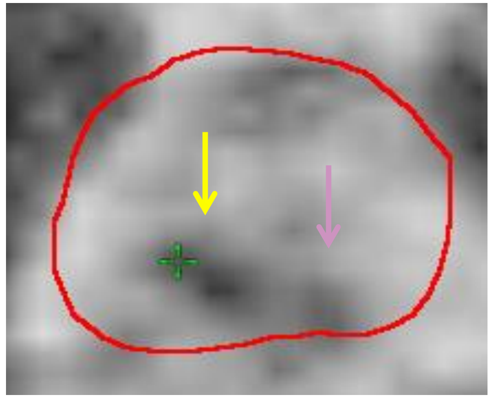


CT

T2



DCE (ktrans)

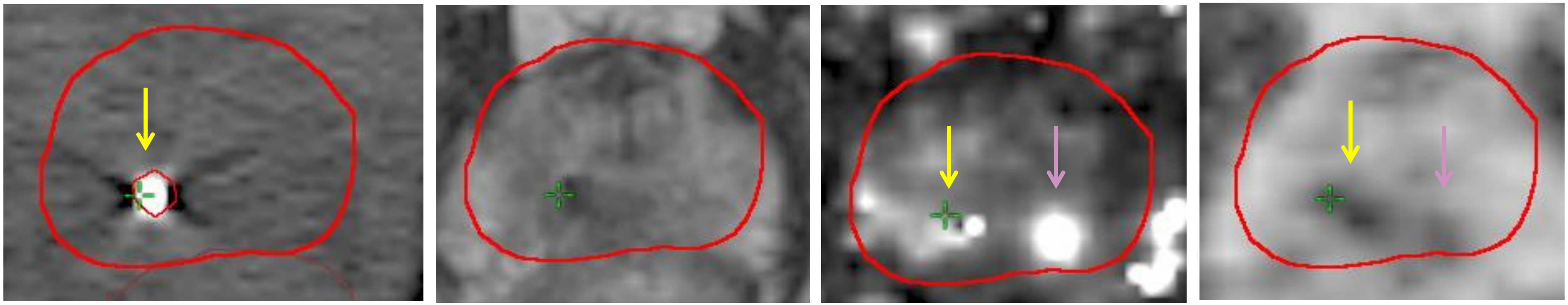


ADC

DCE = dynamic contrast enhanced
- high signal due to increase in capilar permeability

ADC = apparent diffusion coefficient
- lack of signal due to high cell density

Functional imaging with MR



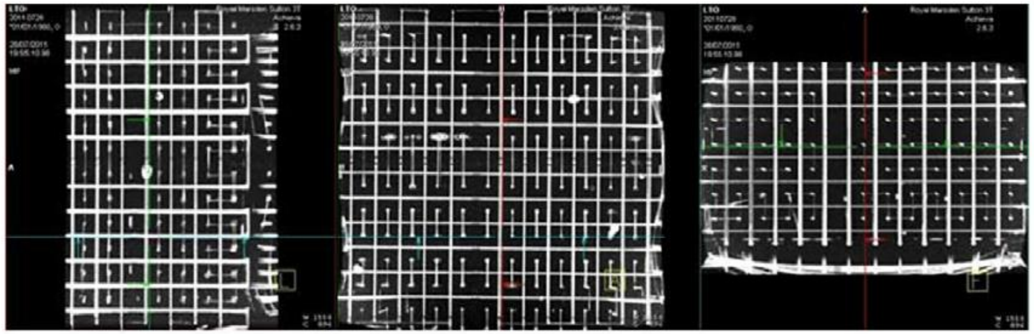
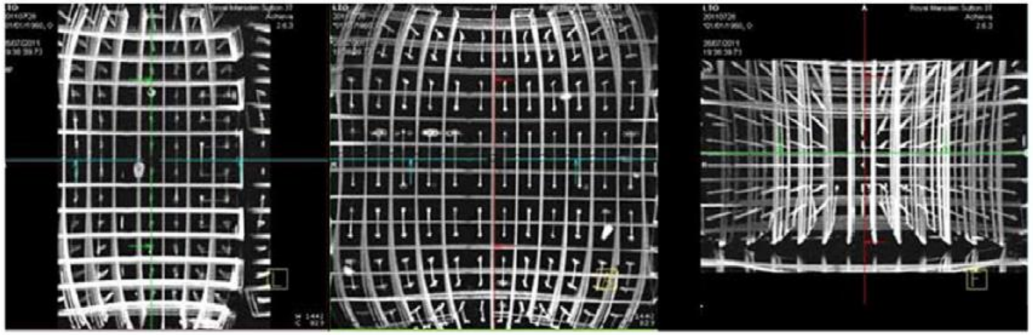
CT T2 DCE (ktrans) ADC

Potential biomarker for prostate cancer progression

- dose escalation
- no compromises in treatment plan

Pitfalls

- Geometric distortion

Schmidt & Payne PMB 2015

- No direct relation with electron density
  - ➢ CT atlas corregistration
  - ➢ MR segmentation

PET/MR for radiotherapy?

European Journal of Radiology 84 (2015) 1285–1292

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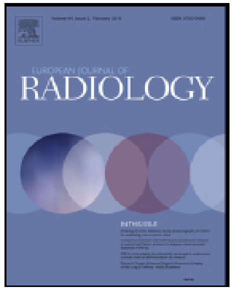
journal homepage: www.elsevier.com/locate/ejrad



Oncological whole-body staging in integrated ^{18}F-FDG PET/MR: Value of different MR sequences for simultaneous PET and MR reading

CrossMark

Benedikt M. Schaarschmidt[a,b], Johannes Grueneisen[b], Philipp Heusch[a,*], Benedikt Gomez[c], Karsten Beiderwellen[b], Verena Ruhlmann[c], Lale Umutlu[b], Harald H. Quick[d,e], Gerald Antoch[a], Christian Buchbender[a]

Conclusion: In conclusion, T2, TIRM, and contrast-enhanced T1 provide a high quality of lesion detectability and anatomical allocation of FDG-avid foci. Their performance is at least comparable to contrast-enhanced PET/CT. Non-enhanced T1 may be omitted and the necessity of DWI should be further investigated for specific questions, such as assessment of the liver.

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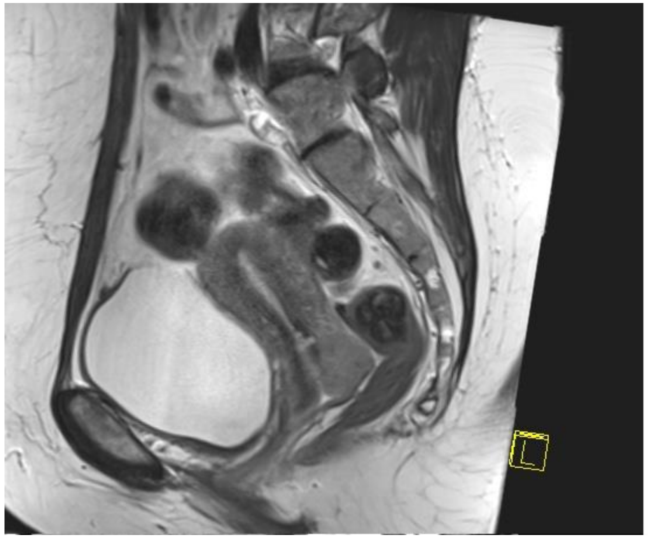
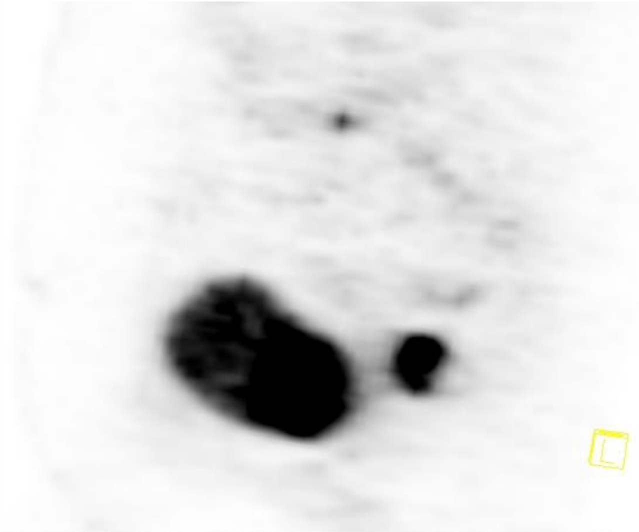
PET/MR

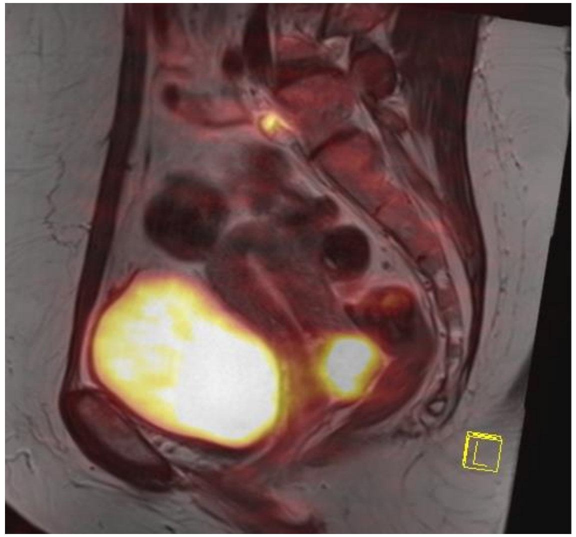
Images courtesy of AK Berthelsen



T2 sag (MR)



FDG-PET



PET/MR

Table 3 Difference in millimeters between the registrations of lesion isocenters measured in three axis with PET/MR

Axis	T2-weighted, PET [mean (SD)] (mm) (25 lesions)	ADC, PET [mean (SD)] (mm) (20 lesions)
x	2.28 (1.36)	4.15 (2.27)
y	2.58 (1.97)	2.08 (1.52)
z	2.95 (2.25)	2.15 (1.78)
Total difference	5.22 (1.97)	5.79 (1.70)

ADC, apparent diffusion coefficient.

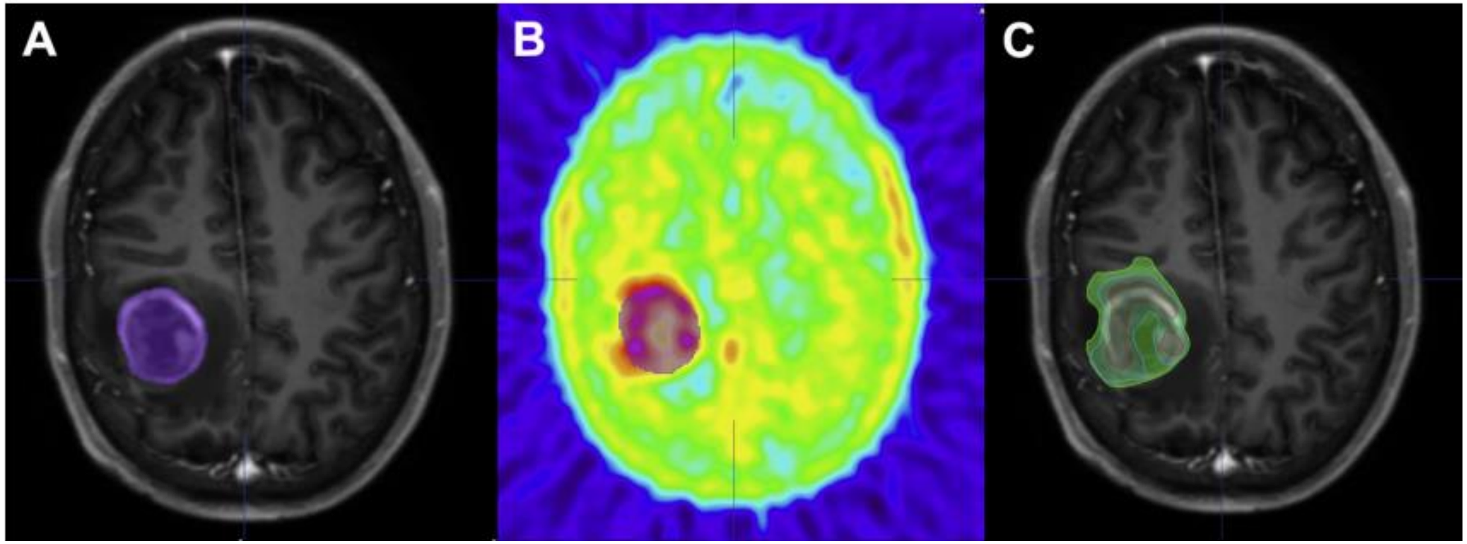
Table 6 Overlap between T2-weighted images and PET, and between ADC and PET

Tumors	T2-weighted, PET [mean (SD)]	ADC, PET [mean (SD)]
All (ml)	0.64 (0.13)	0.56 (0.14)
$<$14 ml	0.51 (0.13)	0.44 (0.14)
14–62 ml	0.63 (0.10)	0.58 (0.11)
$\geq$62 ml	0.76 (0.03)	0.66 (0.04)

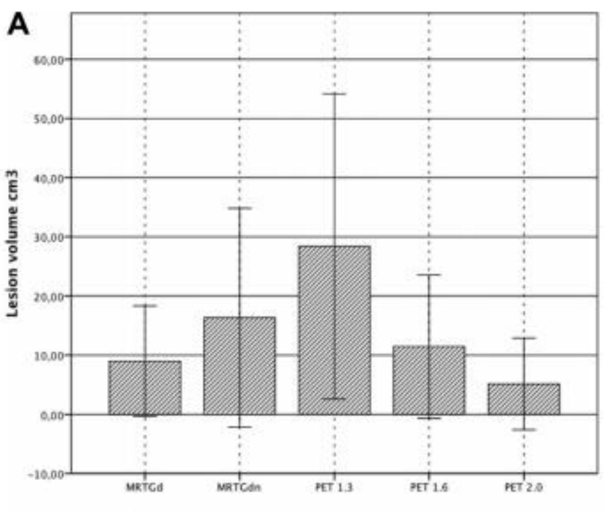
ADC, apparent diffusion coefficient.

Zhang et al. 2016

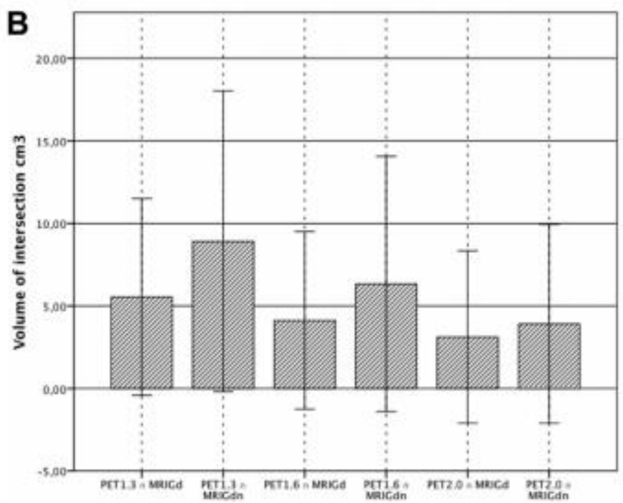
PET/MR imaging of brain tumours



Lesion
volume



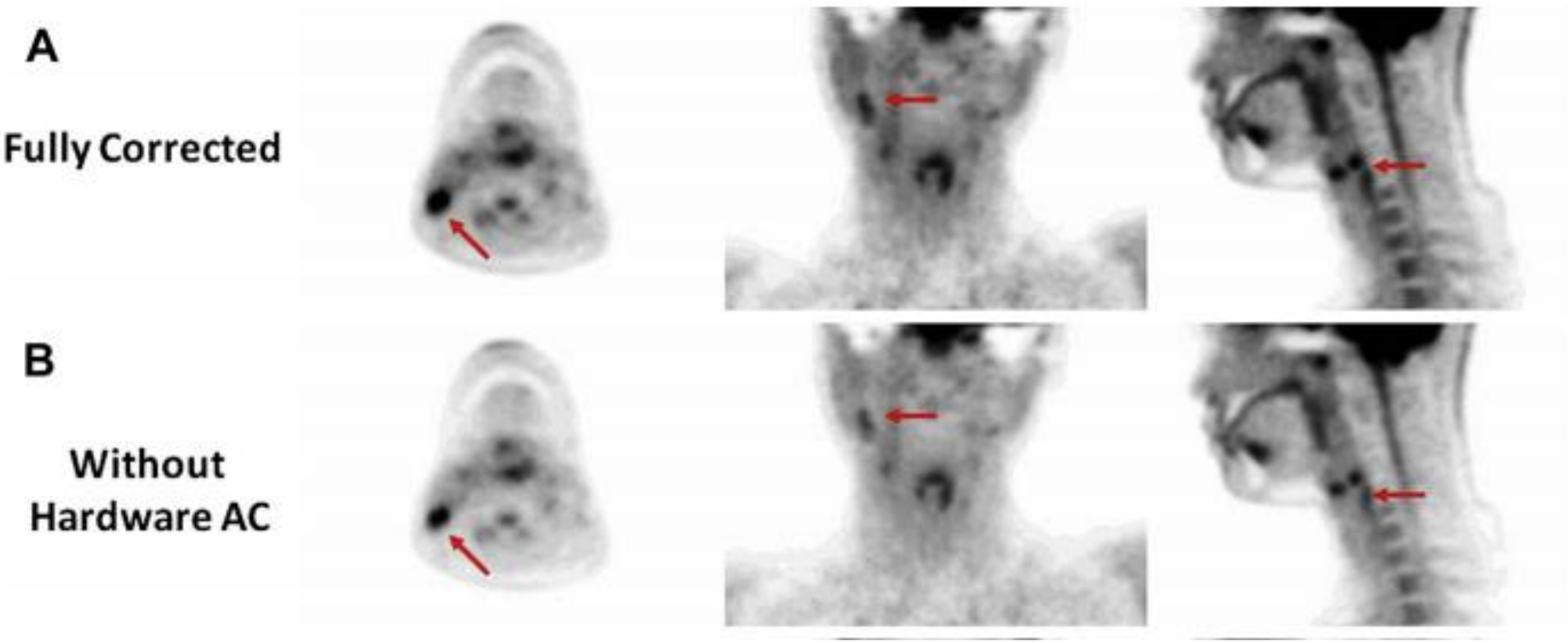
Intersection
volume



Gempt et al. *World Neurosurgery 2015*

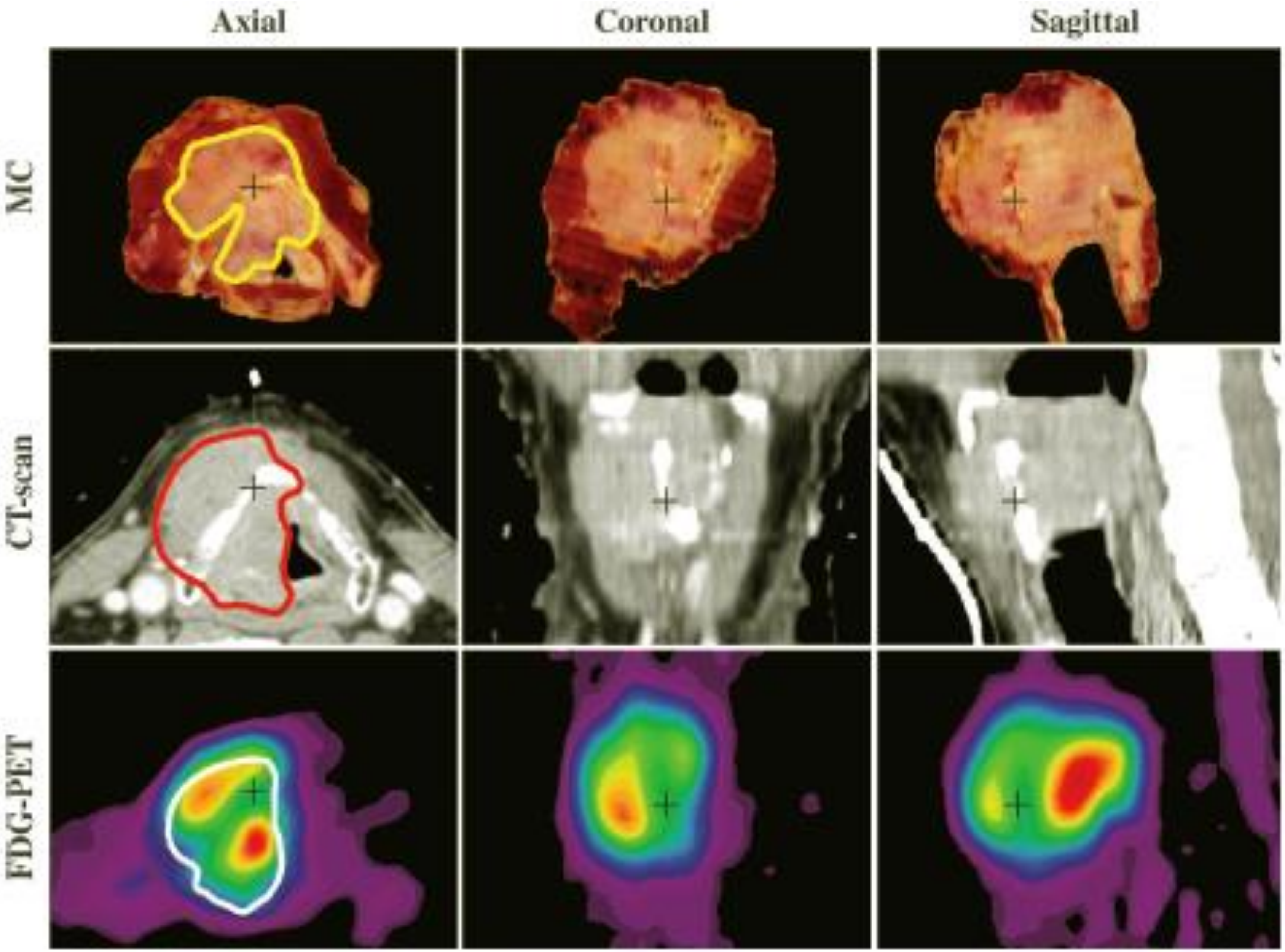
PET/MR pitfall

- MR coils impair PET signal



Eldib et al. PET Clin 2016

Challenge of multi modality imaging

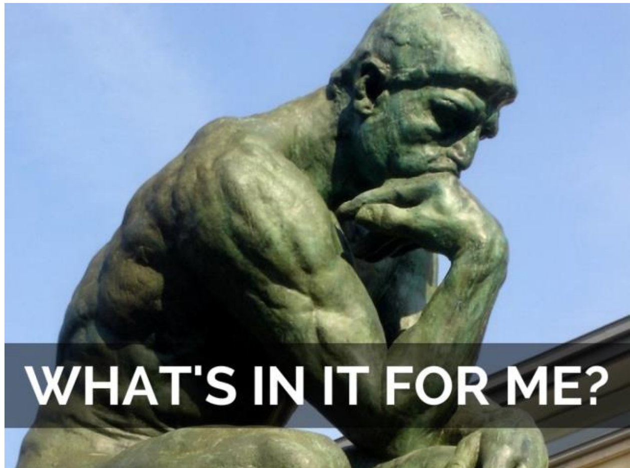


Daisne et al. *Radiology 2004*

Conclusion (1)

- Illustrate the importance of a particular pre-treatment imaging modality for radiotherapy

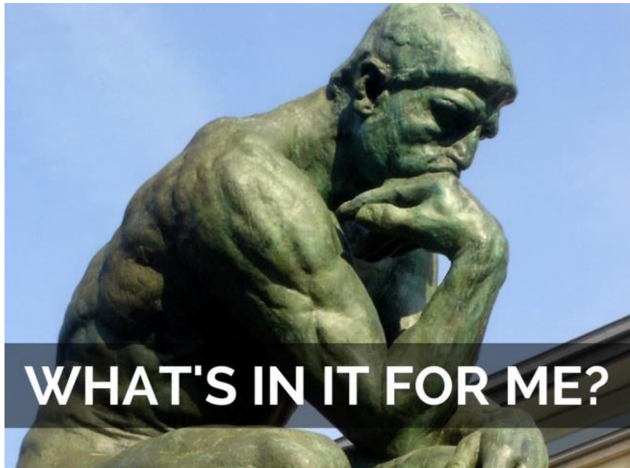
  - ➢ CT is needed for calculation of dose distribution
  - ➢ PET adds value for staging, distinguishing tracer avid areas/volumes
  - ➢ MR increased soft tissue contrast



Conclusion (2)

- Comprehend the additional value of applying combined information from several imaging modalities for radiotherapy planning

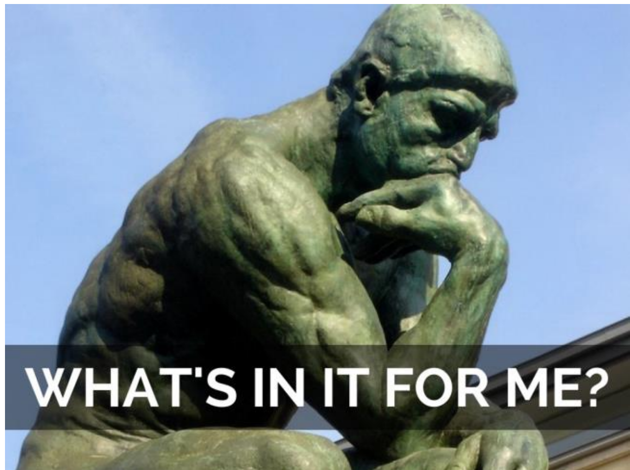
  - ➢ More reproducible target definition
  - ➢ More precise target definition
  - ➢ Optimal treatment strategy



Conclusion (3)

- Identify uncertainties of pre-treatment imaging modalities

  - ➢ Artefacts in images
  - ➢ Differences in (spatial) info on each modality



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TARGET VOLUME DELINEATION

ESTRO School

Sofia Rivera, MD, PhD
Radiation Oncology Department
Gustave Roussy
Villejuif, France

GUSTAVE ROUSSY
CANCER CAMPUS
GRAND PARIS

Advanced skills in modern radiotherapy
June 11, 2017

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Learning outcomes

- Understand why heterogeneity in contouring is a major weak point in modern radiotherapy
- Discuss the challenges in contouring target volumes
- Identify skills required to delineate target volumes
- Identify tools for improving learning in delineation
- Identify adequate imaging modalities according to the target to delineate
- Discuss the impact and consequences of inaccurate delineation of target volumes

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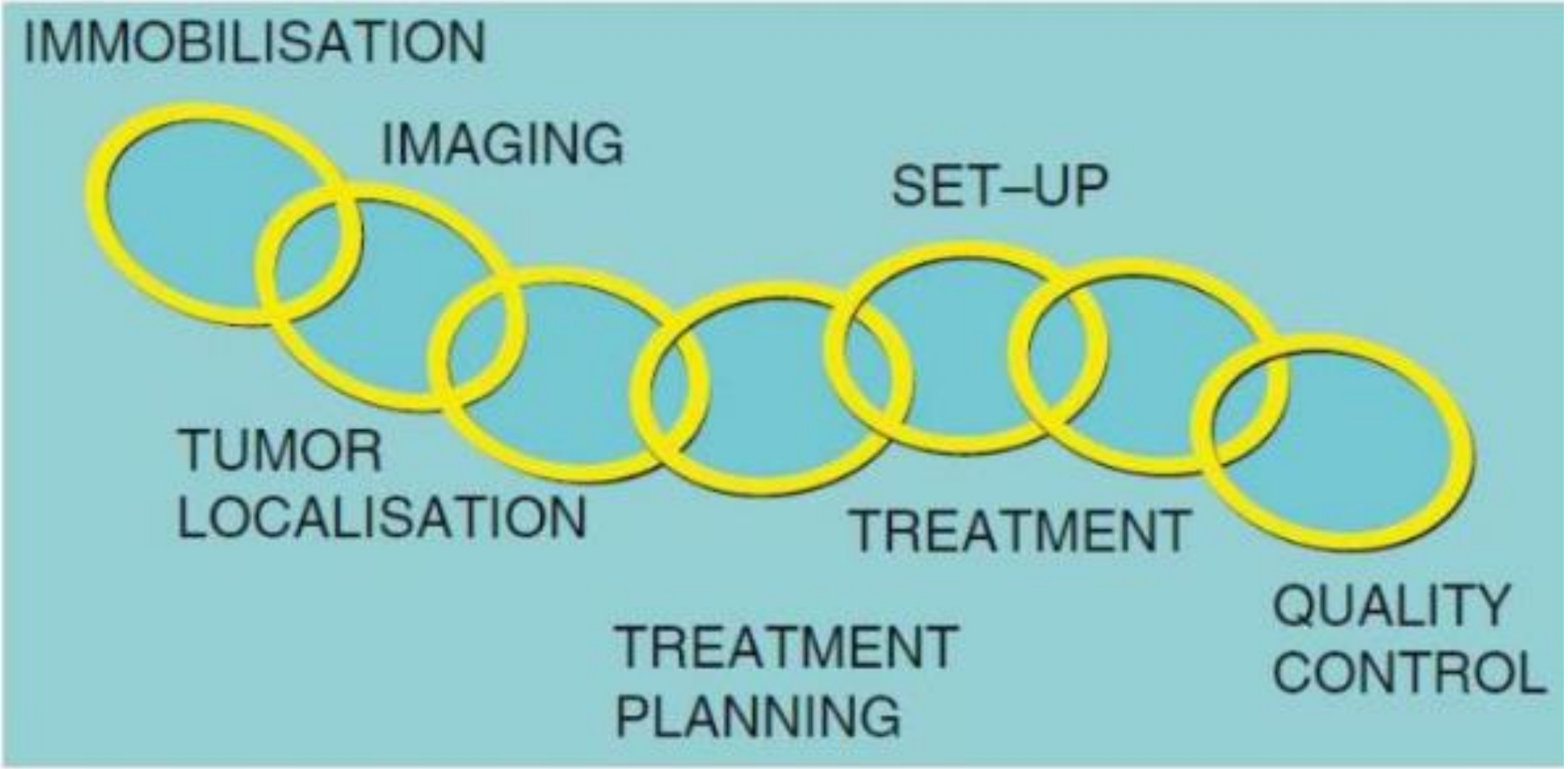
Delineation: one of the links in the treatment chain



Why is delineation important?

- Radiotherapy planning is nowadays mostly based on CT scans
- Constraints for dose distribution are used
- DVH are calculated based on the contours
- Field arrangements are becoming more complex
- An error in contouring will therefore translate in a **systematic error** all along the treatment and may have consequences:
  - ➢ Jeopardizing treatment efficacy
  - ➢ Impacting treatment toxicity

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Do we need to improve?

NIH Public Access
Author Manuscript
Radiother Oncol. Author manuscript; available in PMC 2013 June 27.

Published in final edited form as:
Radiother Oncol. 2012 April ; 103(1): 92–98. doi:10.1016/j.radonc.2012.02.010.

Heterogeneity in head and neck IMRT target design and clinical practice

Theodore S. Hong[a], Wolfgang A. Tomé[b,c,d], and Paul M. Harari[b,*]

Abstract

Purpose—To assess patterns of H&N IMRT practice with particular emphasis on elective target delineation.

Materials and methods—Twenty institutions with established H&N IMRT expertise were solicited to design clinical target volumes for the identical H&N cancer case. To limit contouring variability, a primary tonsil GTV and ipsilateral level II node were pre-contoured. Participants were asked to accept this GTV, and contour their recommended CTV and PTV. Dose prescriptions, contouring time, and recommendations regarding chemotherapy were solicited.

Results—All 20 institutions responded. Remarkable heterogeneity in H&N IMRT design and practice was identified. Seventeen of 20 centers recommended treatment of bilateral necks whereas 3/20 recommended treatment of the ipsilateral neck only. The average CTV volume was 250 cm^3 (range 37–676 cm^3). Although there was high concordance in coverage of ipsilateral neck levels II and III, substantial variation was identified for levels I, V, and the contralateral neck. Average CTV expansion was 4.1 mm (range 0–15 mm). Eight of 20 centers recommended chemotherapy (cisplatin), whereas 12/20 recommended radiation alone. Responders prescribed on average 69 and 68 Gy to the tumor and metastatic node GTV, respectively. Average H&N target volume contouring time was 102.5 min (range 60–210 min).

Conclusion—This study identifies substantial heterogeneity in H&N IMRT target definition, prescription, neck treatment, and use of chemotherapy among practitioners with established H&N IMRT expertise. These data suggest that continued efforts to standardize and simplify the H&N IMRT process are desirable for the safe and effective global advancement of H&N IMRT practice.

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How can we answer that need ?

- Adequate imaging, training and use of contouring guidelines are the main strategies to minimize delineation uncertainties (Petrič et al 2013)

- Establishing and using consensus and guidelines have shown to reduce heterogeneity in contouring

Table III. Mean and ranges of DSC before and after consensus.

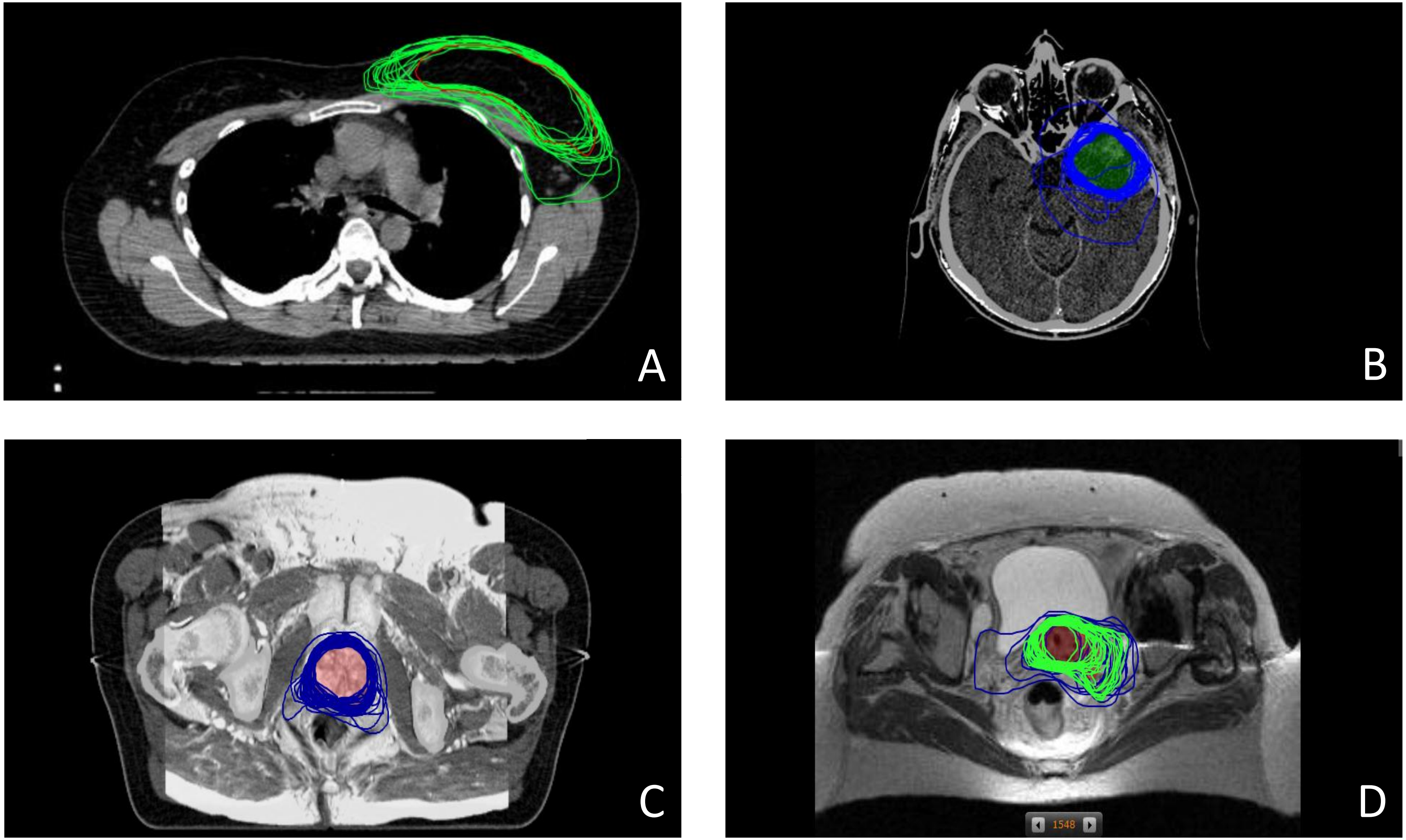
Volume	Consensus volume (ml)	Mean DSC (range) Before consensus	Mean DSC (range) After consensus
Breast	1247	0.93 (0.89–0.96)	0.95 (0.93–0.96)
Boost	40	NA	0.75 (0.60–0.89)
Internal mammary LN	15	0.59 (0.32–0.72)	0.71 (0.63–0.81)
Axillary LN level I	108	0.65 (0.59–0.75)	0.70 (0.60–0.77)
Axillary LN level II	32	0.56 (0.35–0.69)	0.76 (0.67–0.84)
Axillary LN level III	17	0.56 (0.39–0.73)	0.74 (0.66–0.82)
Periclavicular LN	47	0.41 (0.34–0.56)	0.56 (0.43–0.73)
Interpectoral LN	33	0.54 (NA)	0.66 (0.55–0.78)
Heart	731	0.91 (0.88–0.94)	0.94 (0.90–0.96)

DSC, Dice similarity coefficient; NA, not available.

NIELSEN et al 2013

Inter-observer variability in contouring

Examples of participant contours from ESTRO FALCON workshops.
A: CTV breast, B: GTV Brain tumour, C: CTV prostate and D: GTV cervix cancer



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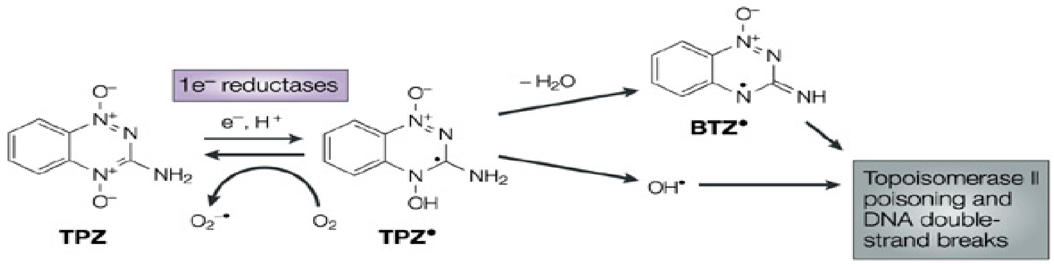
Does heterogeneity in RT matters?

- Bioreductive agent
- Radiosensitizer in hypoxia



Nature Reviews | Cancer

Multicentric international
Randomized phase III
853 locally advanced
H&N patients

RT + CDDP

RT + CDDP
+ Tyrapazamine

Hypoxia radioresistance

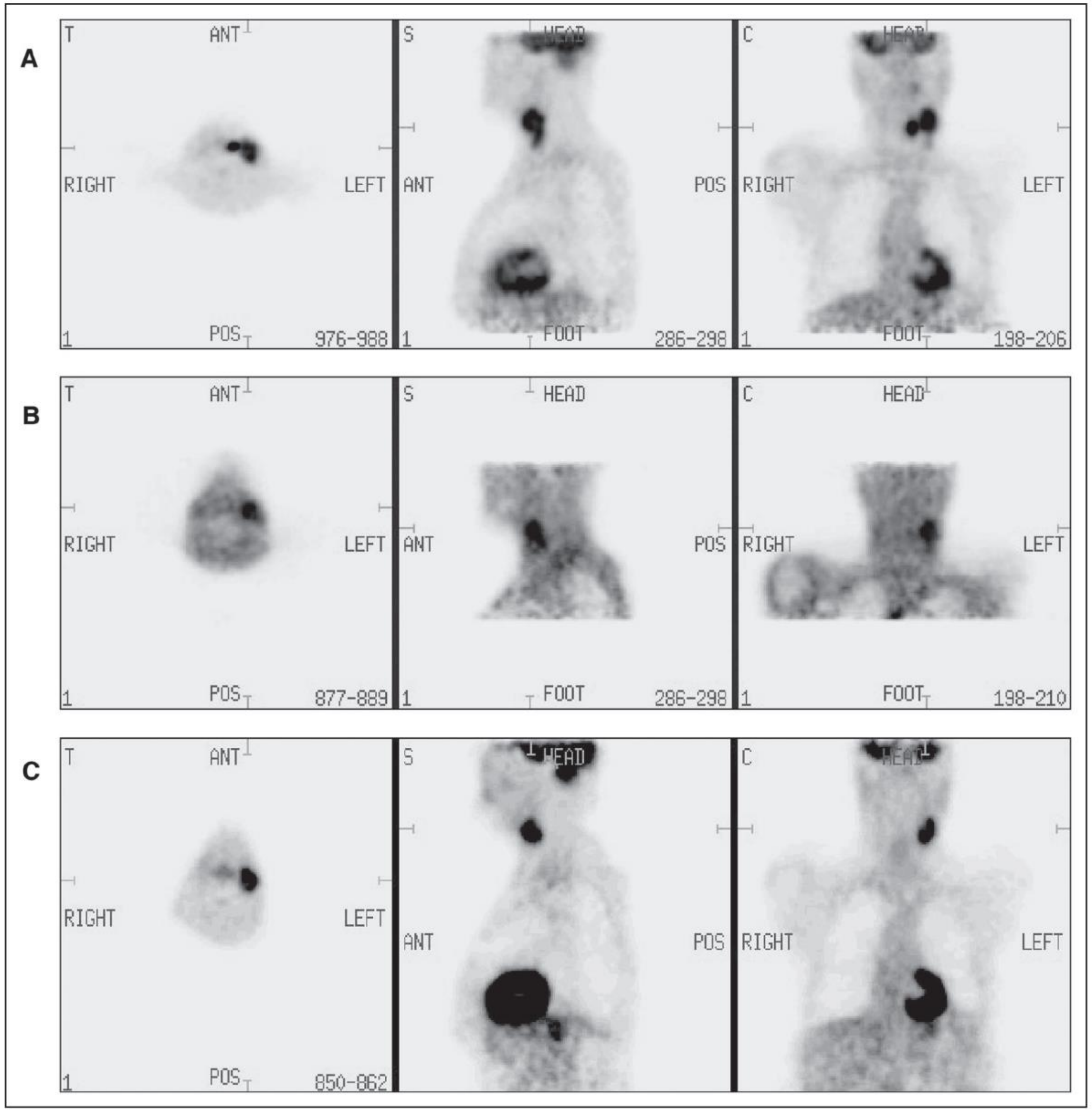
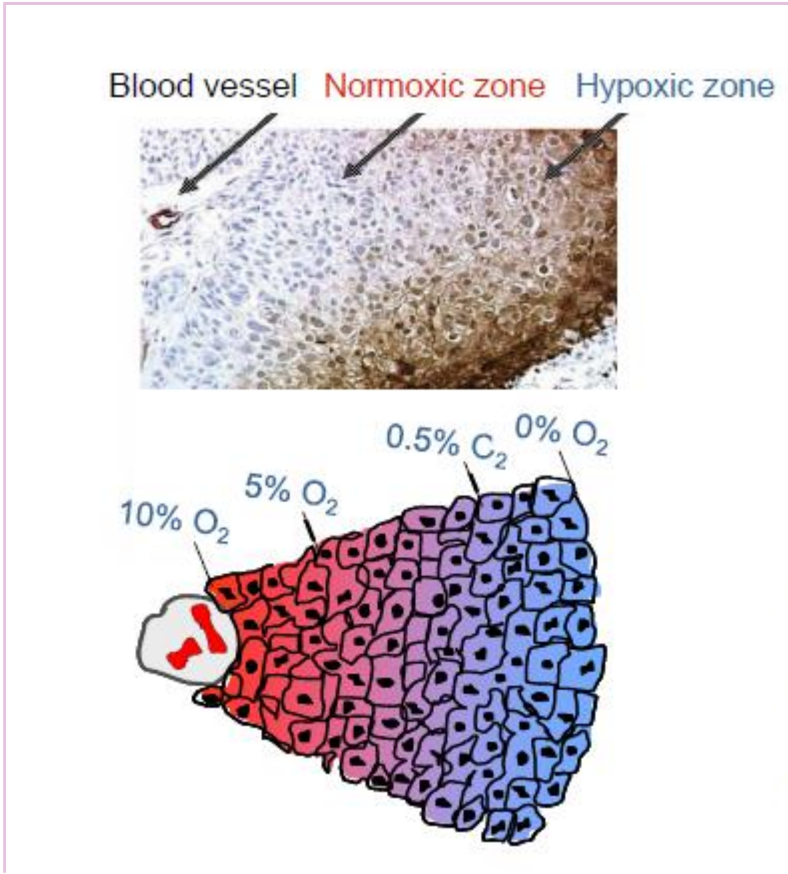


Fig 1. (A) Baseline $[^{18}F]$-fluorodeoxyglucose (FDG) positron emission tomography (PET) of patient with T2N2b squamous cell carcinoma of the pyriform fossa with left nodal mass. (B) $[^{18}F]$-fluoromisonidazole (FMISO) -PET at baseline, nonhypoxic primary tumor, and hypoxic node. (C) FDG-PET 12 weeks after chemoboost, complete response in nonhypoxic primary tumor, and poor response in hypoxic node. Residual tumor in nodal mass was confirmed pathologically after neck dissection.



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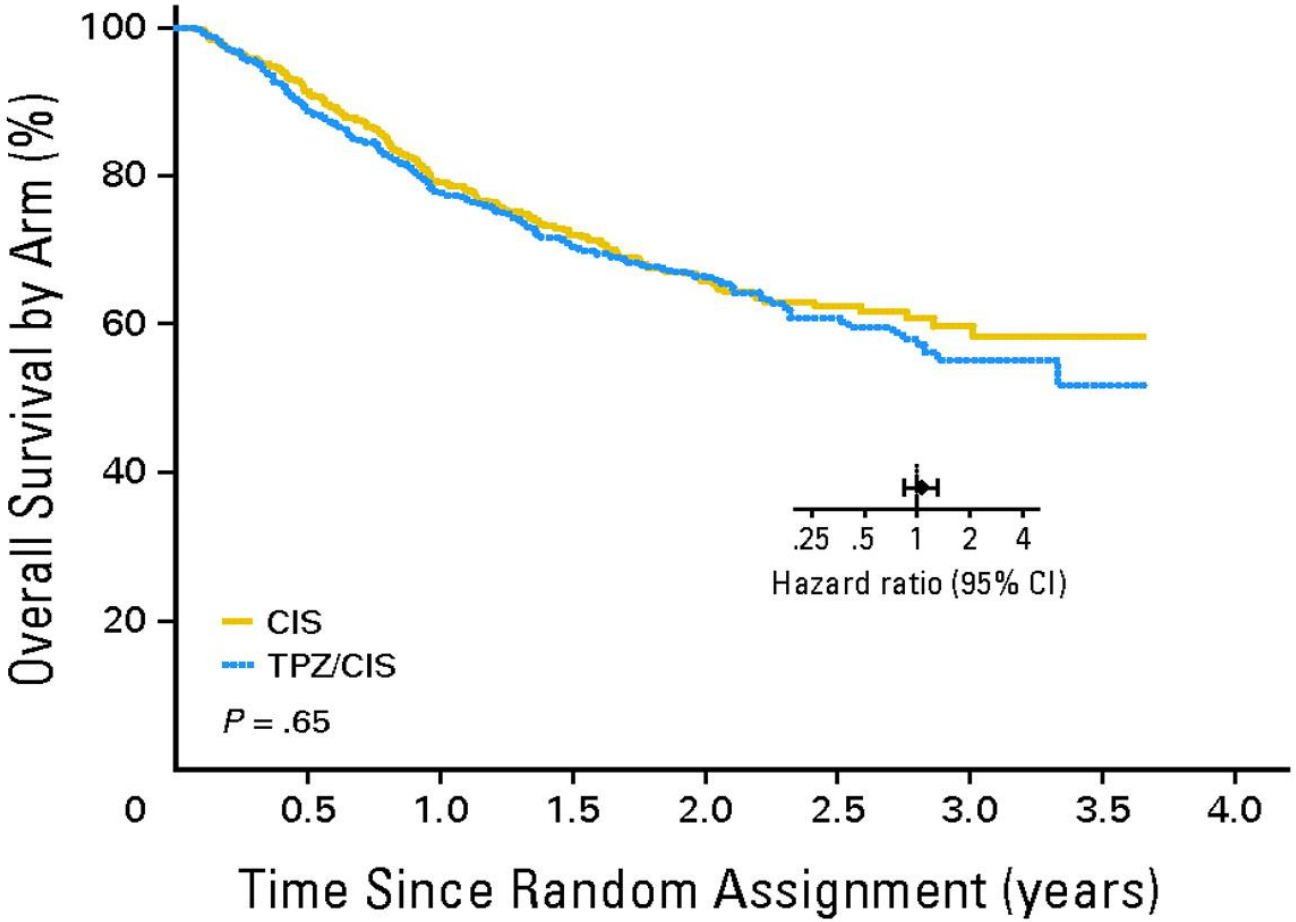
No benefit in overall survival



No. at risk									
CIS	428	389	332	294	248	91	45	6	0
TPZ/CIS	425	374	326	291	252	98	42	7	0

Rischin D et al. JCO 2010;28:2989-2995

JOURNAL OF CLINICAL ONCOLOGY

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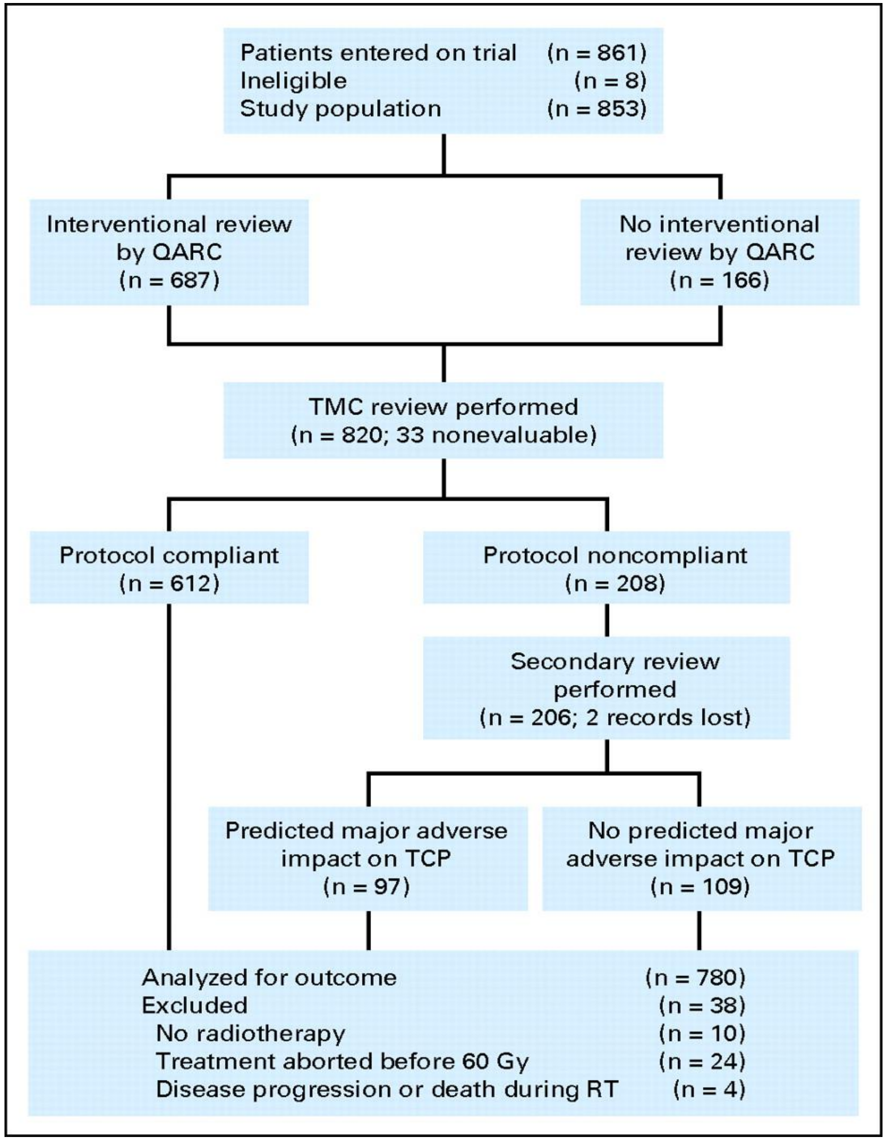
But… Trial quality control



Peters L J et al. JCO 2010;28:2996-3001

JOURNAL OF CLINICAL ONCOLOGY

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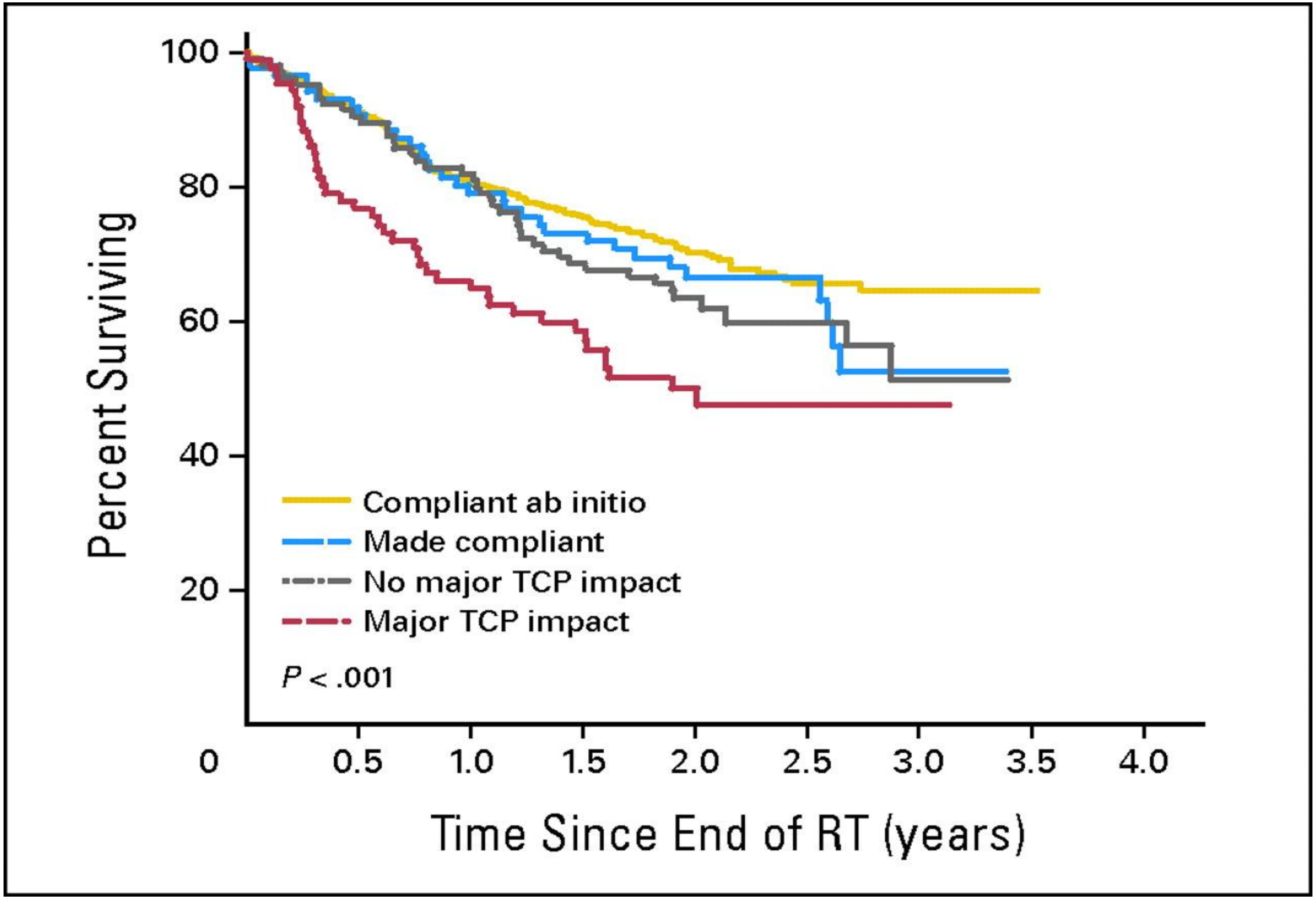
Impact of radiotherapy quality



Peters L J et al. JCO 2010;28:2996-3001

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How to improve?

- Need for a common language: ICRU
- Need for delineation guidelines and anatomical knowledge
- No absolute truth so need to specify according to which guidelines we contour
- Heterogeneity in understanding/interpreting the guidelines
- Need for teaching in contouring
- Need for evaluation in contouring

ICRU Guidelines (ICRU50): volume definition

- Volumes defined prior/ during treatment planning:
  - Gross Tumor Volume (GTV)
  - Clinical Target Volume (CTV)
  - Planning Target Volume (PTV)

  - Organs At Risk (OAR)

  - Treated Volume
  - Irradiated Volume

- Volumes might be redefined during treatment for adaptive RT

Tumor Gross Volume: GTV

- Macroscopic tumor volume visible or palpable

- Includes:
  - Primary tumor
  - Macroscopically involved lymph nodes
  - Metastases

Tumor Gross Volume: GTV

- GTV is defined based on clinical data (inspection, palpation) and imaging (CT, MR, US, PET depending on it's relevance for the tumor site)

- Definition of the GTV allows for TNM classification of the disease

- Definition of the GTV allows for tumor response assessment

- Adequate dose to GTV is therefore crucial for tumor control

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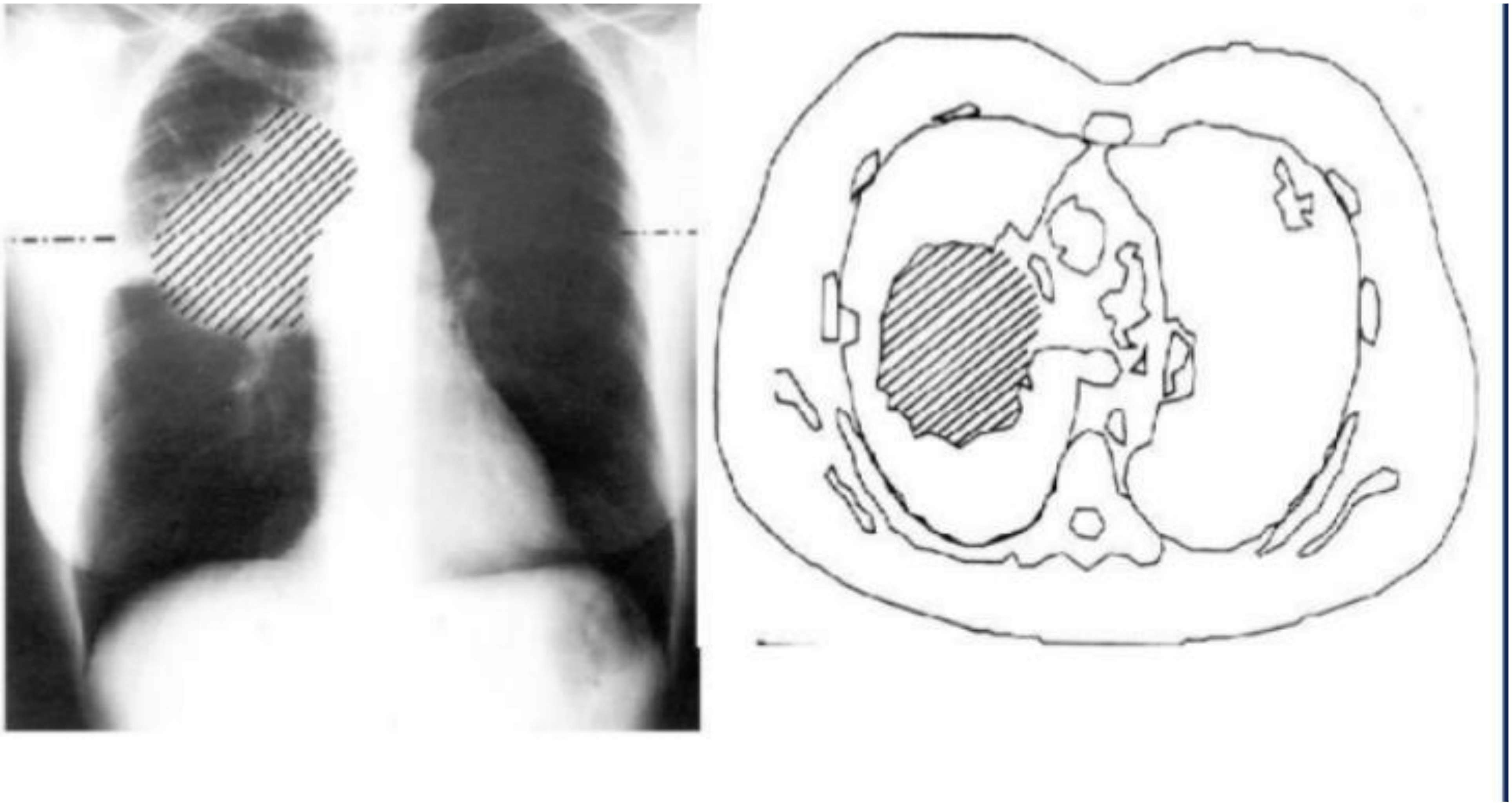
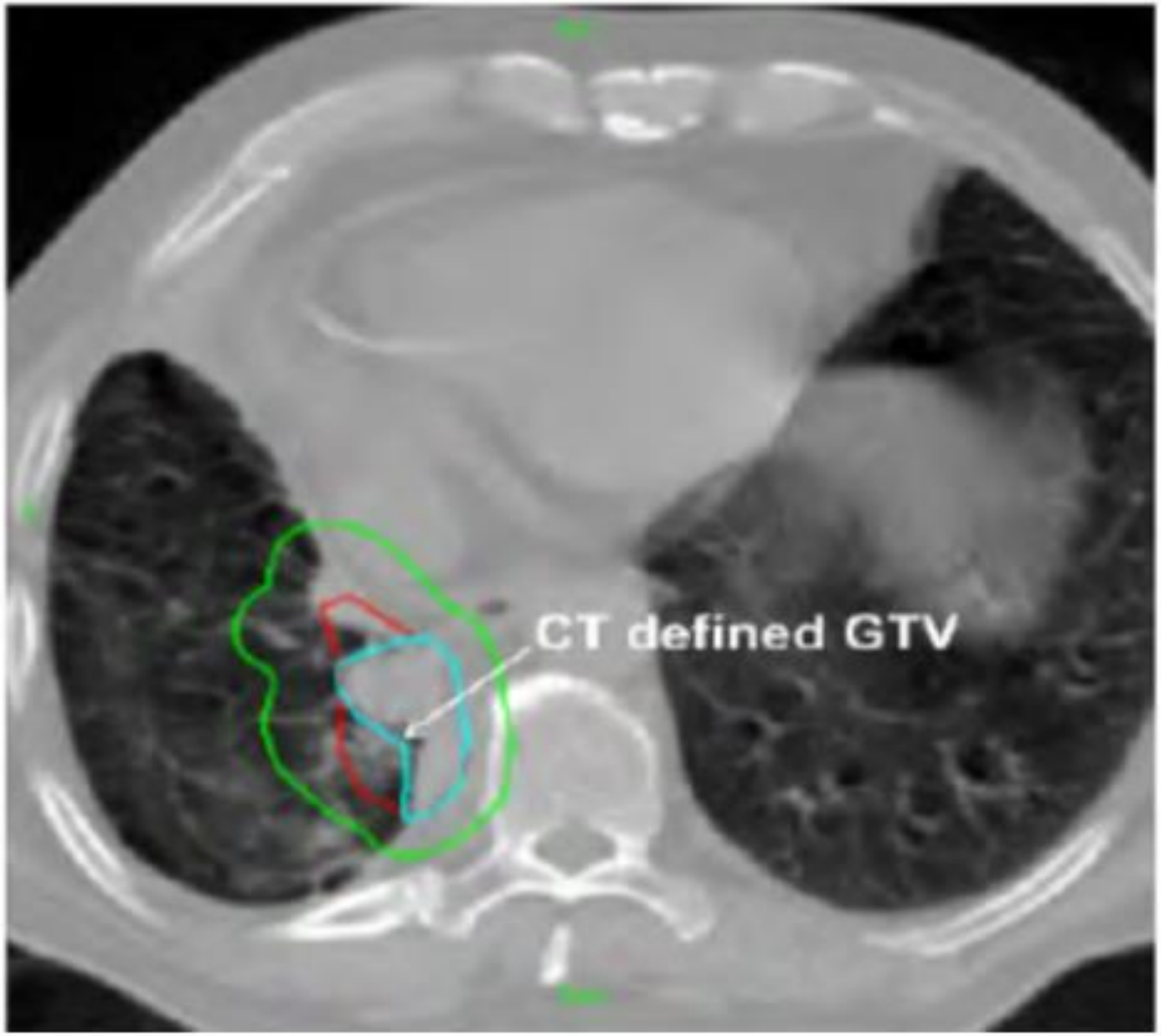
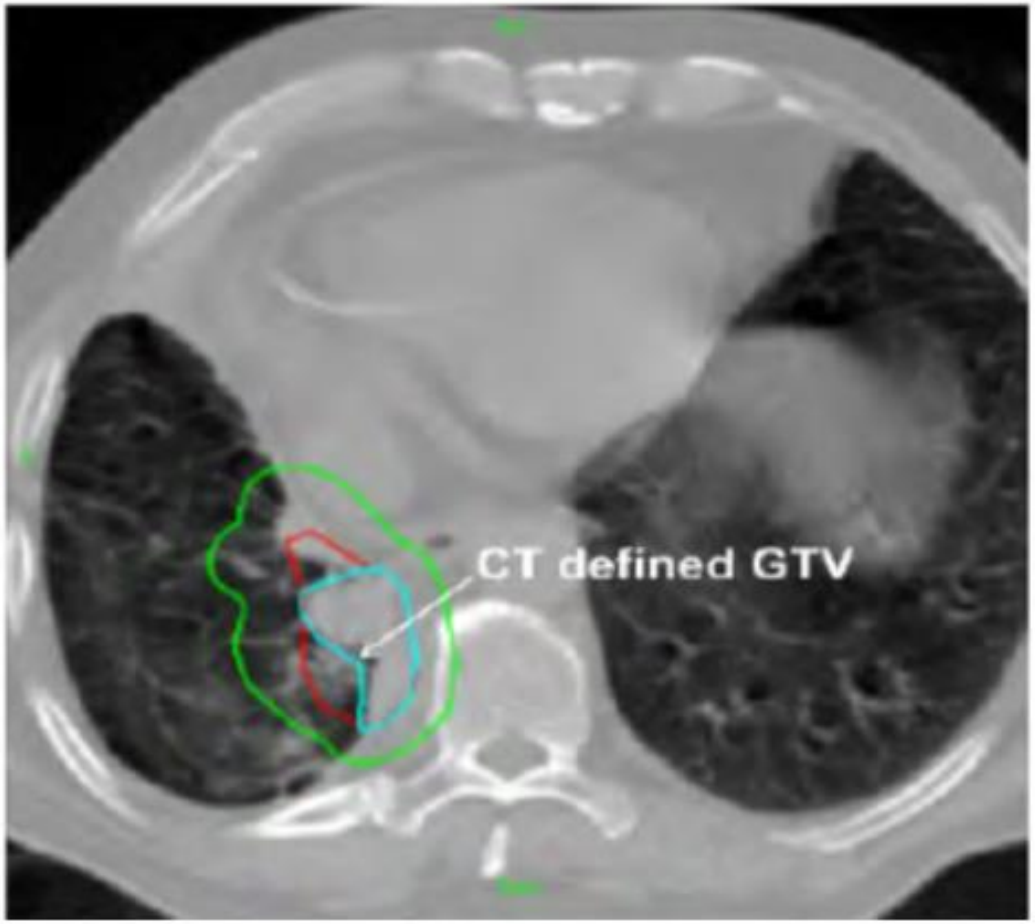
Tumor Gross Volume: GTV

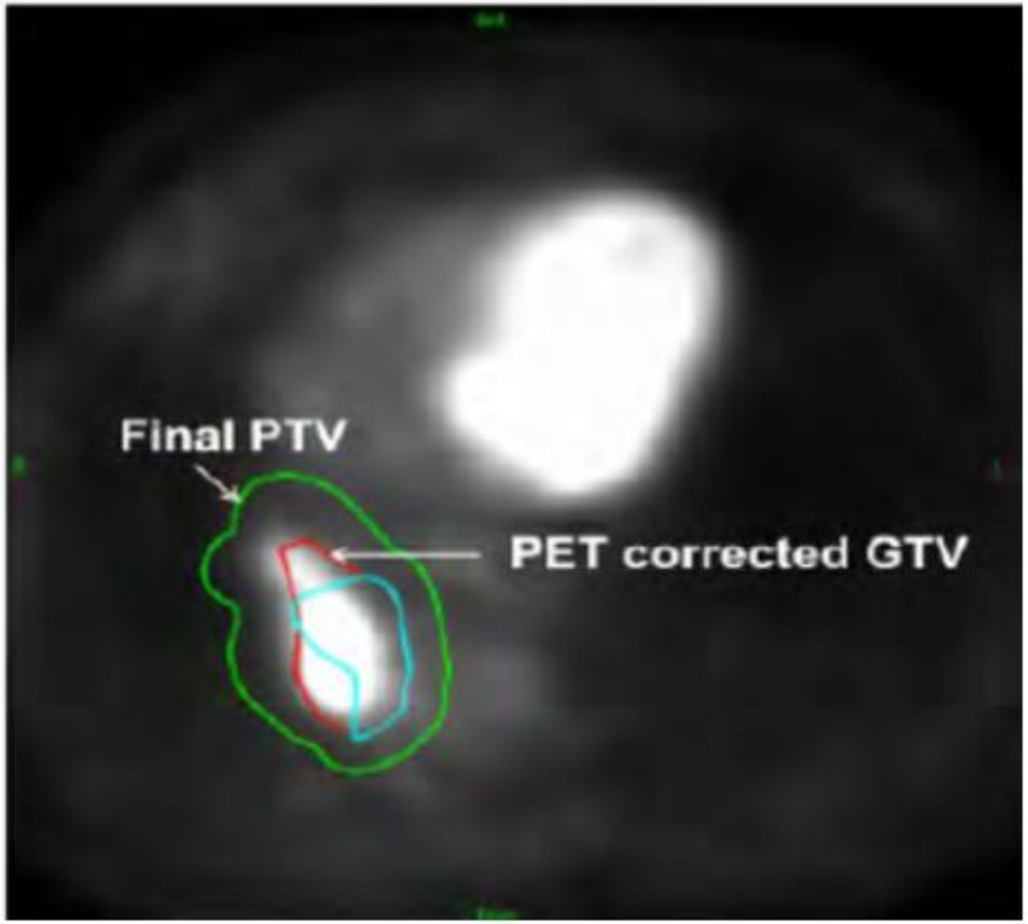


Which one is the GTV?



Are you sure about your GTV????





PET scans in delineation of lung cancer

Contents lists available at ScienceDirect

Radiotherapy and Oncology 101 (2011) 284–290

Contents lists available at ScienceDirect

- FDG-PET has an established role in contouring NSCLC
- Changes the tumor GTV in about 30–60% of patients
- Changes the nodal GTV in 9–39% of patients mainly through detection of occult metastases not seen on CT, lowering the risk of nodal recurrences

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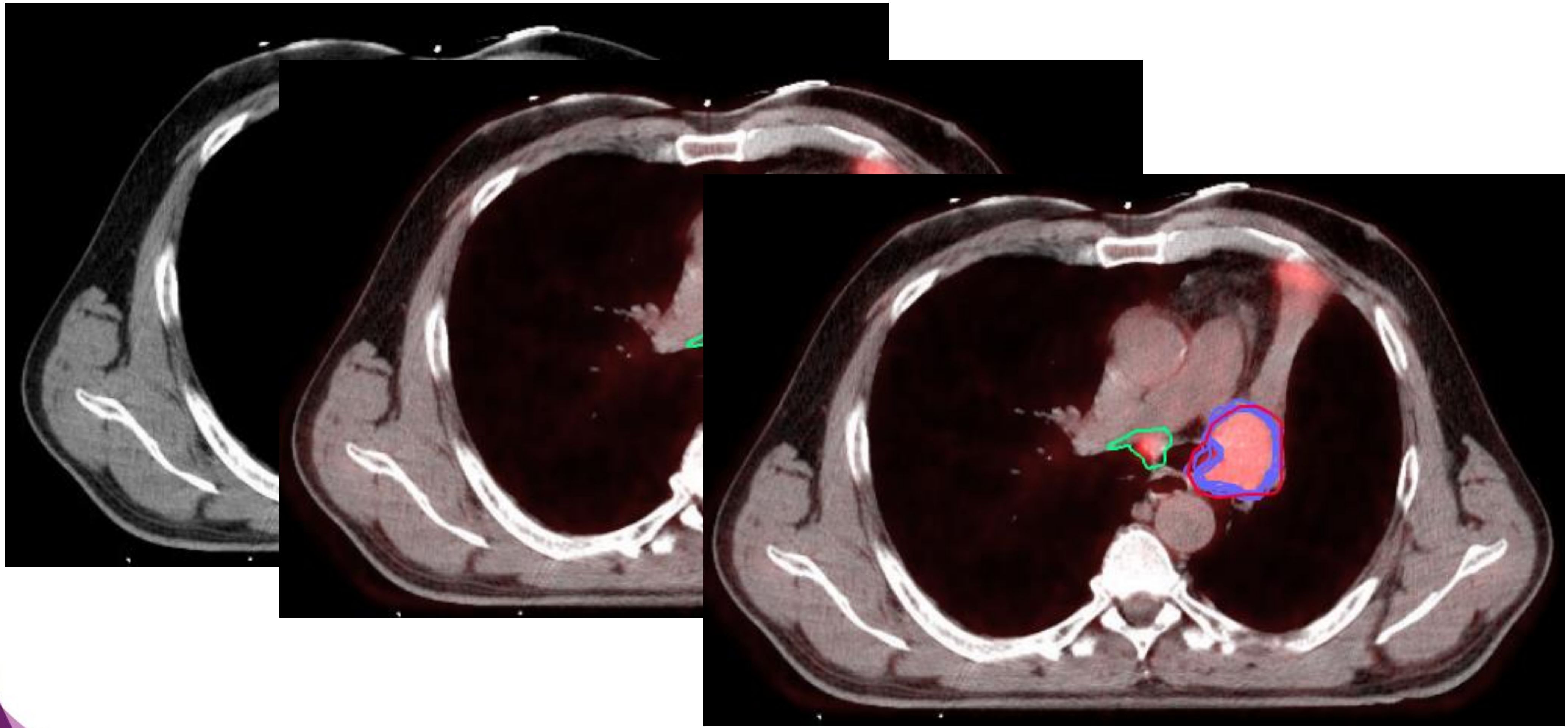
Tumor Gross Volume: GTV

- Adequate high quality imaging is a key point



Images from the FALCON platform; case Lung PET: Vienna 2013

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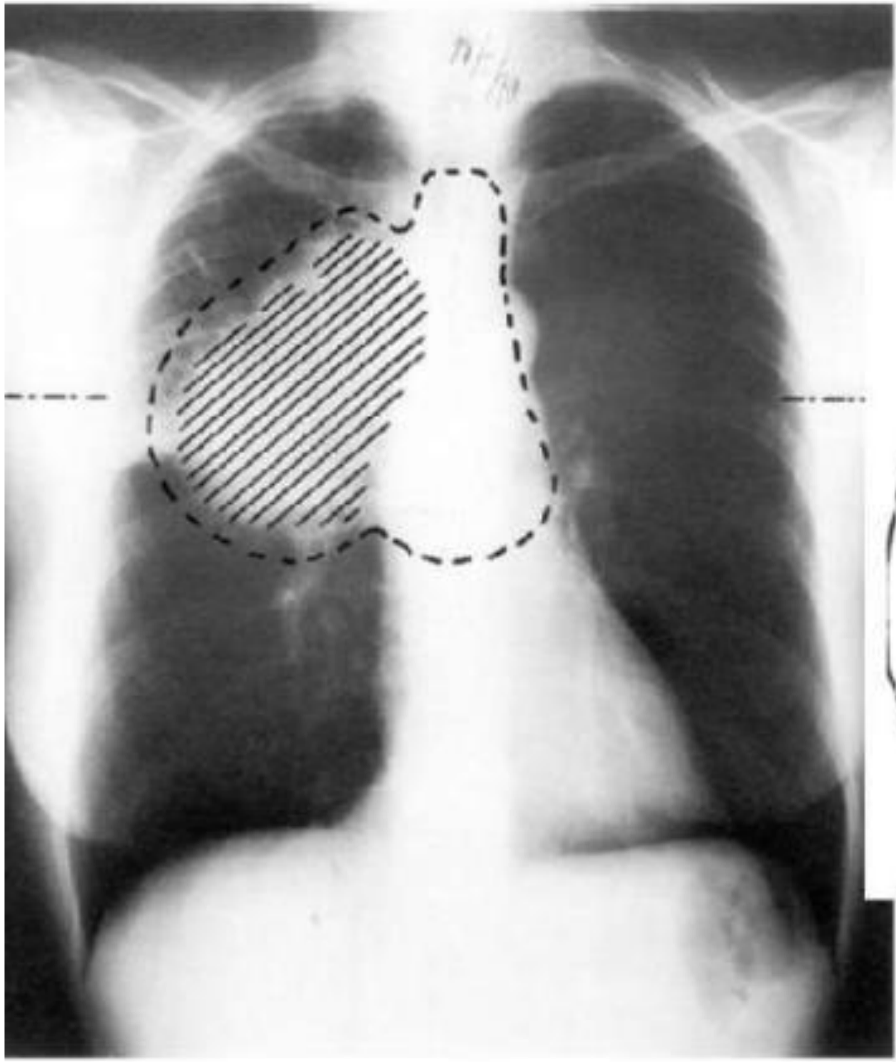
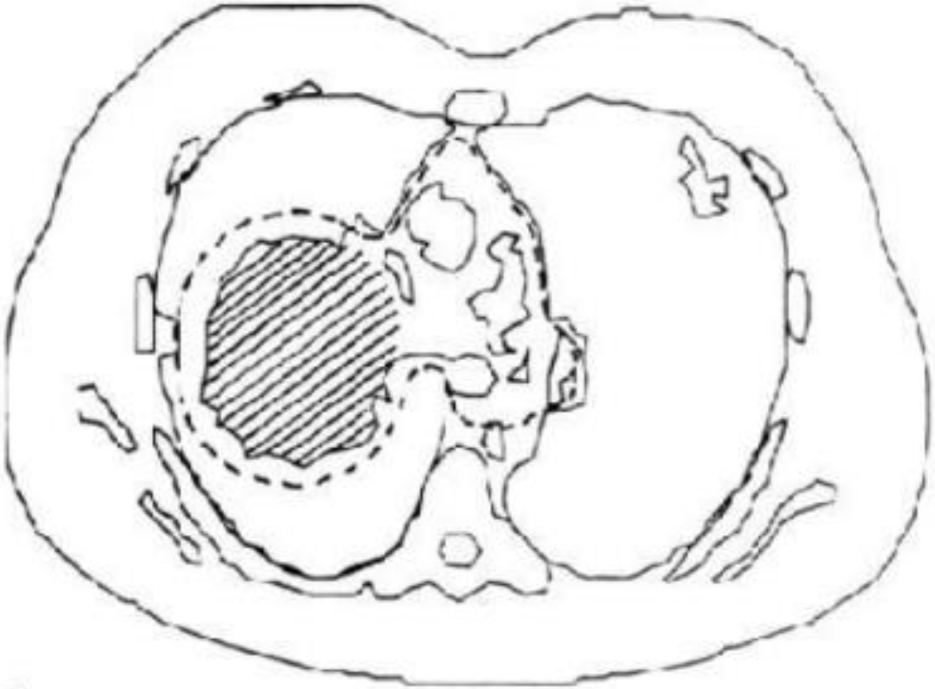
Clinical Target Volume: CTV

- Includes GTV + microscopic extension of the tumor
- Volume to adequately cover to ensure treatment efficacy weather treatment is delivered with a curative or a palliative intent
- CTV delineation is based on local and loco regional capacity/probability of extension of the tumor
- Includes potential micromets surrounding the GTV
- Includes potential micromets in tumor’s drainage territory

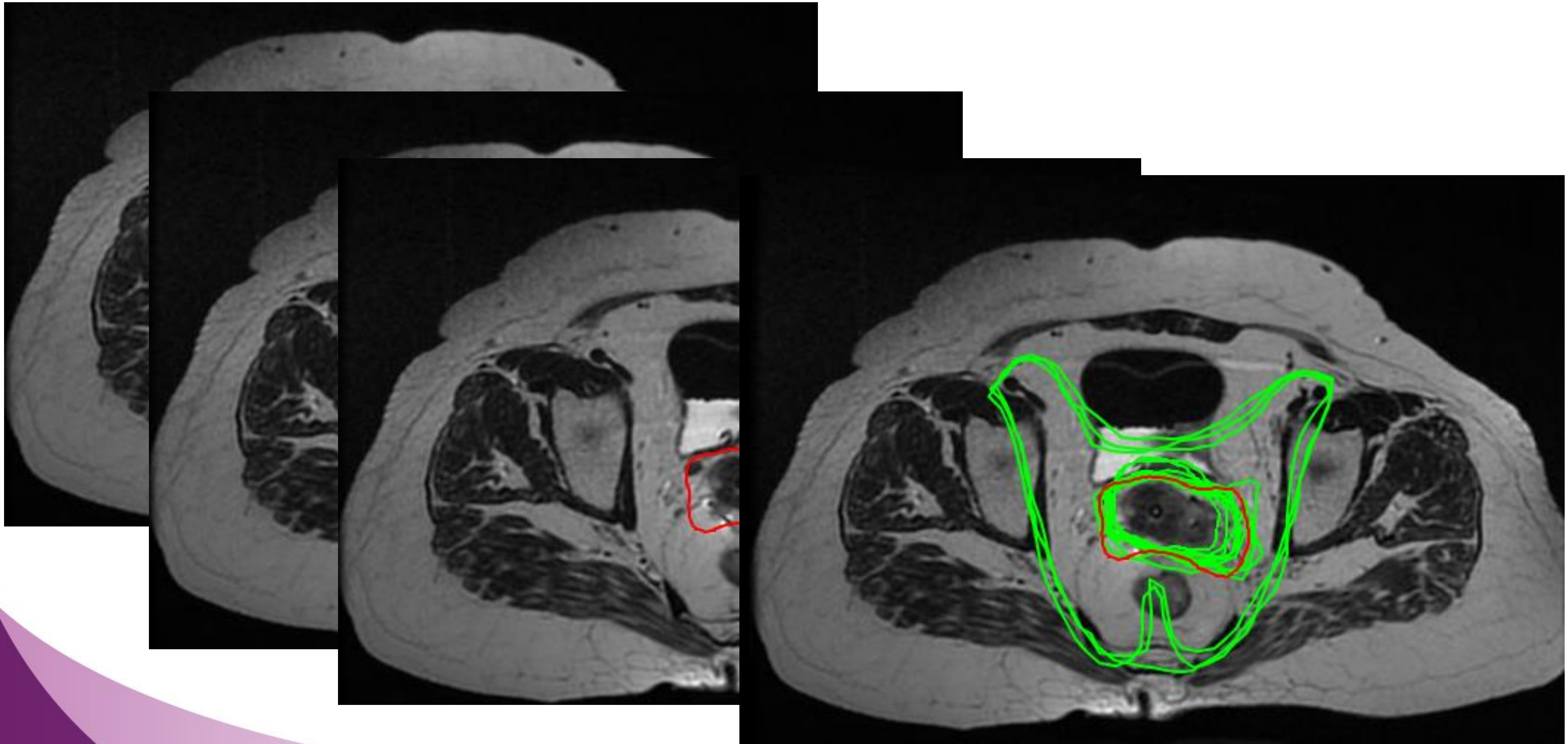
CTV





Clinical Target Volume: CTV

- High quality images are a key point for CTV delineation as well
- Margins adapted to anatomical boundaries



GTV and CTV

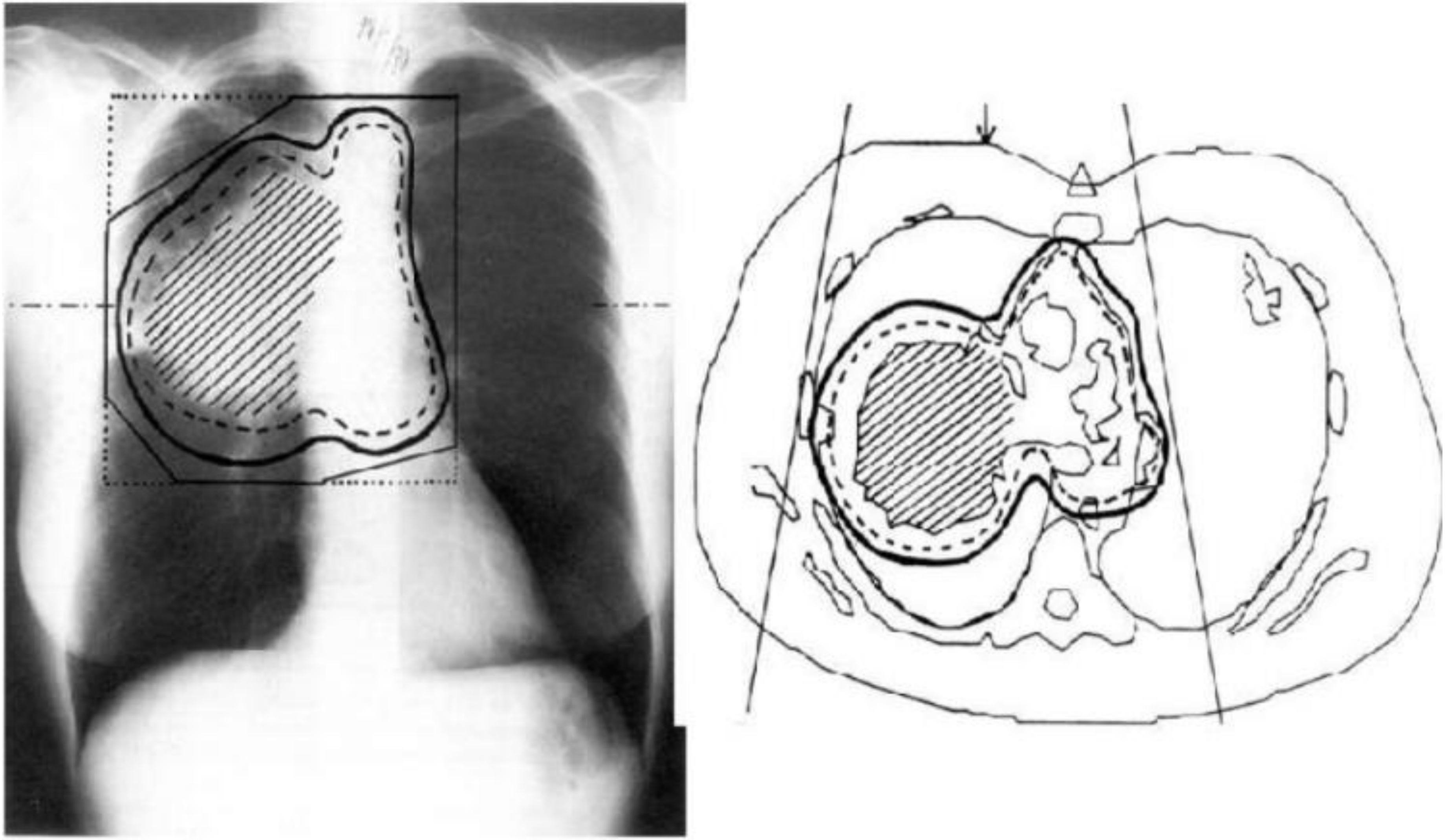
- Definition based on:
  - ➢ Anatomy
  - ➢ Morphology
  - ➢ Imaging
  - ➢ Biology
  - ➢ Natural history of each tumor site

➢ **But GTV and CTV delineation are independent of the technique used**

Planning Target Volume: PTV

- Geometric concept
- Meant to allow for an adequate coverage of the CTV what ever the technique, the movements, the set up uncertainties are
- Volume used for treatment planning
- Volume used for reporting

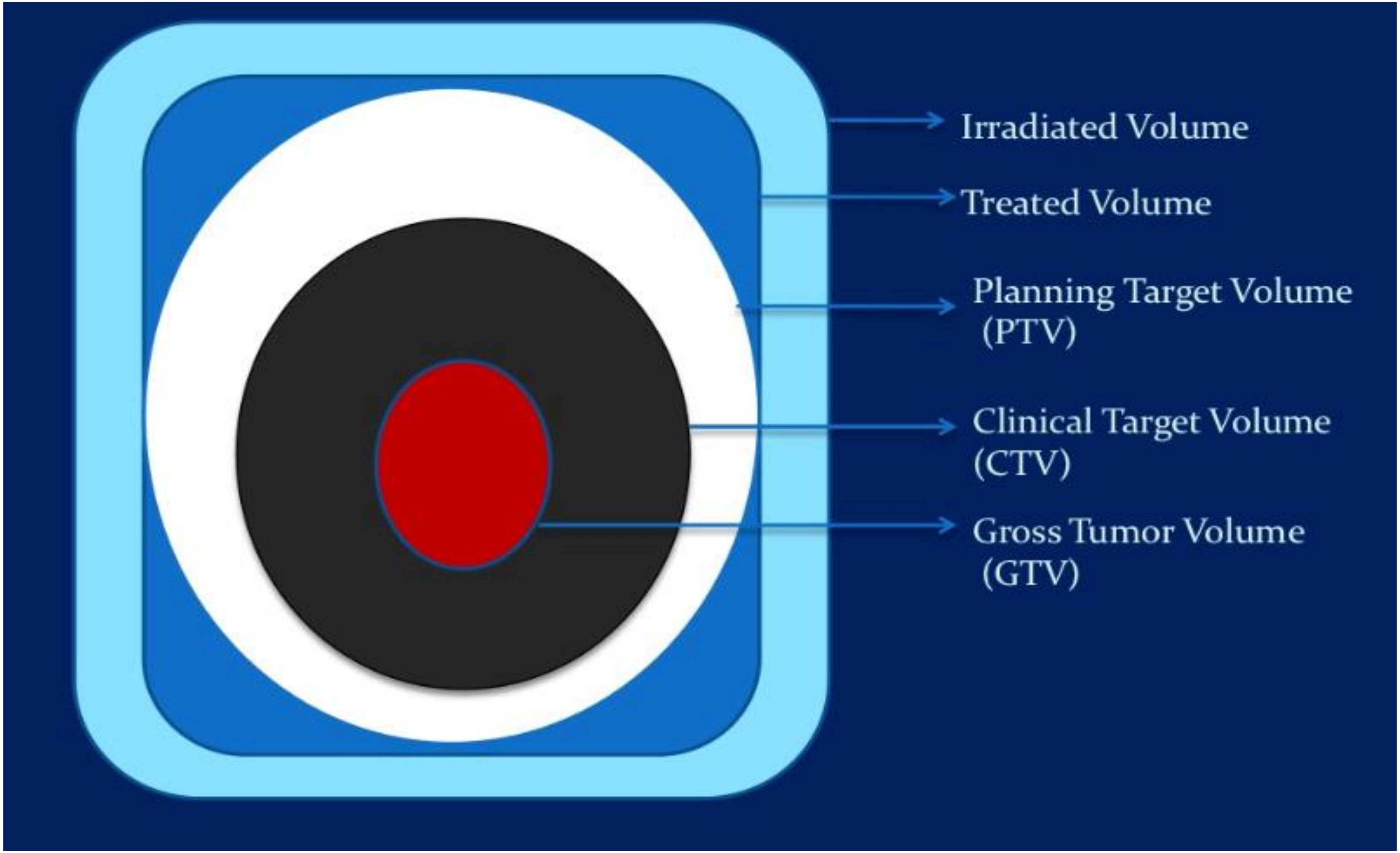
PTV



Irradiated Volume and Treated Volume: IRV and TV

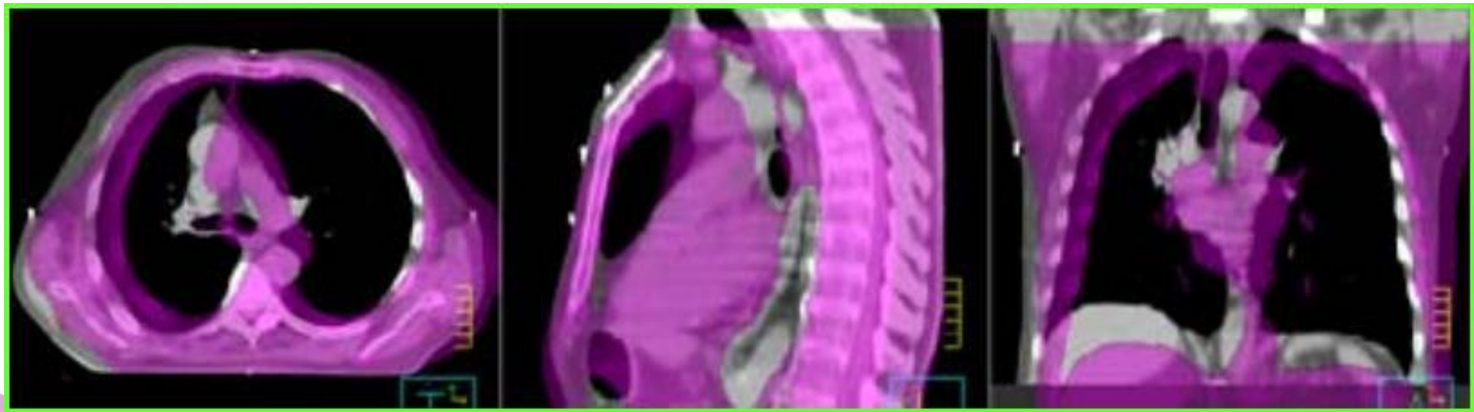
- IRV: Defined as the volume receiving a significant dose on surrounding normal tissues (Organs At Risk)
- Different from the treated volume which is meant to be treated
- Both depend on the technique used
- Both can be evaluated on the dosimetry but IRV evaluation is rather limited by most TPS
  - Ex: dose estimation outside of the treated field when using non coplanar beams

ICRU 50


Irradiated Volume
Treated Volume
Planning Target Volume (PTV)
Clinical Target Volume (CTV)
Gross Tumor Volume (GTV)

ICRU 62 (in addition to ICRU 50)

- Introduces the Conformity Index: **CI= treated volume/ PTV**
- Recommendations on anatomical and geometrical margins
- Internal Margins: **IM** are margins integrating physiological movements (breathing, bowel/ rectum/ bladder repletion, swallowing…)
- Internal Target Volume: **ITV** is defined as the volume taking into account Internal Margins

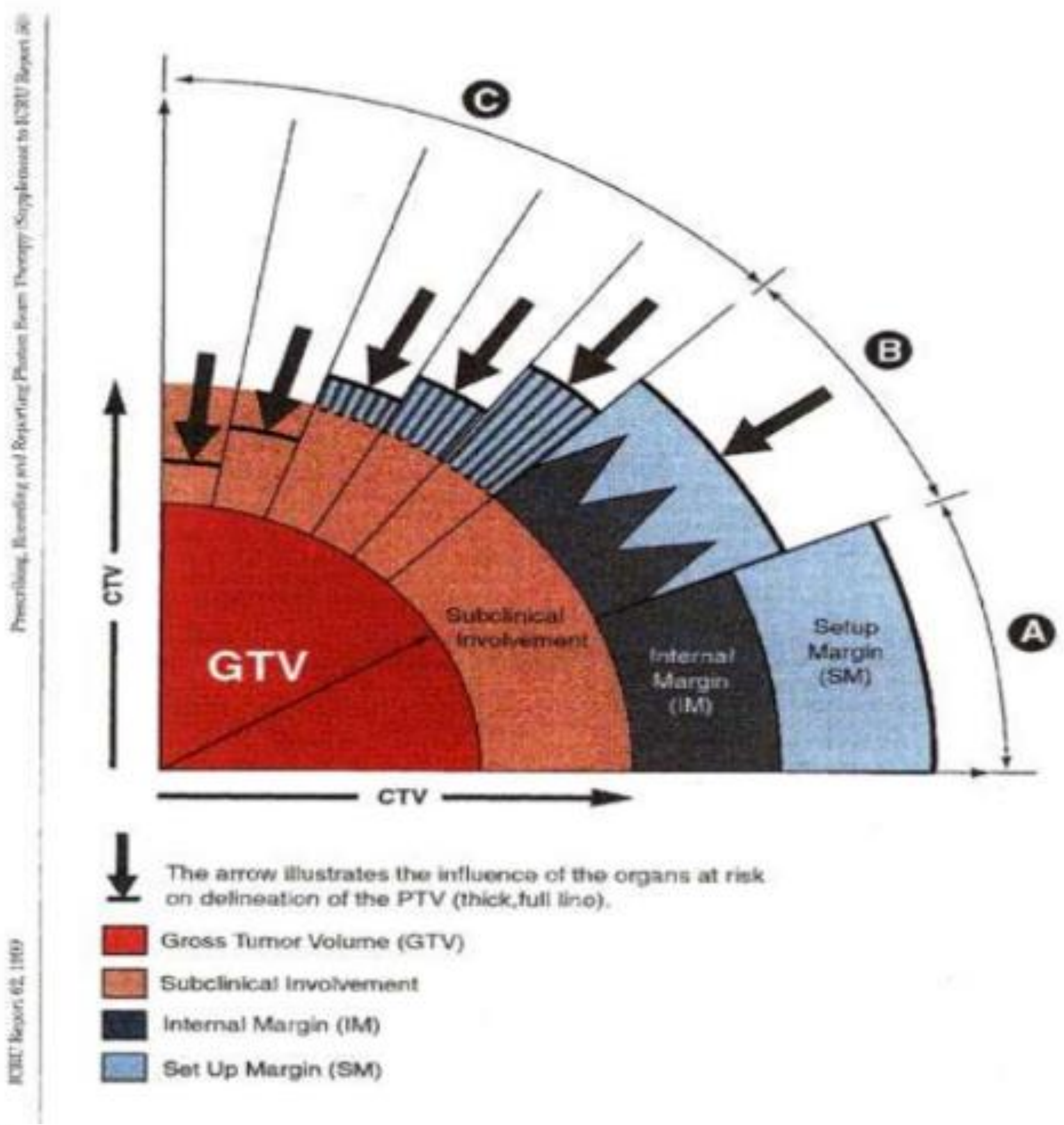


Set up Margin: SM

- Margins related to patient positioning:

  - Positioning uncertainties due to patient external movements
  - Positioning uncertainties due to body markers
  - Mechanical uncertainties due to immobilization device precision

- Depend on the technique (ex: tracking) and immobilization material and protocols (ex: thickness of painting markers or tattoos)



Prescribing, Recording and Reporting Photon Beam Therapy (Supplement to ICRU Report 50)
ICRU Report 62, 1999
C
B
A
GTV
Subclinical Involvement
Internal Margin (IM)
Setup Margin (SM)
CTV
CTV
The arrow illustrates the influence of the organs at risk on delineation of the PTV (thick,full line).
Gross Tumor Volume (GTV)
Subclinical Involvement
Internal Margin (IM)
Set Up Margin (SM)

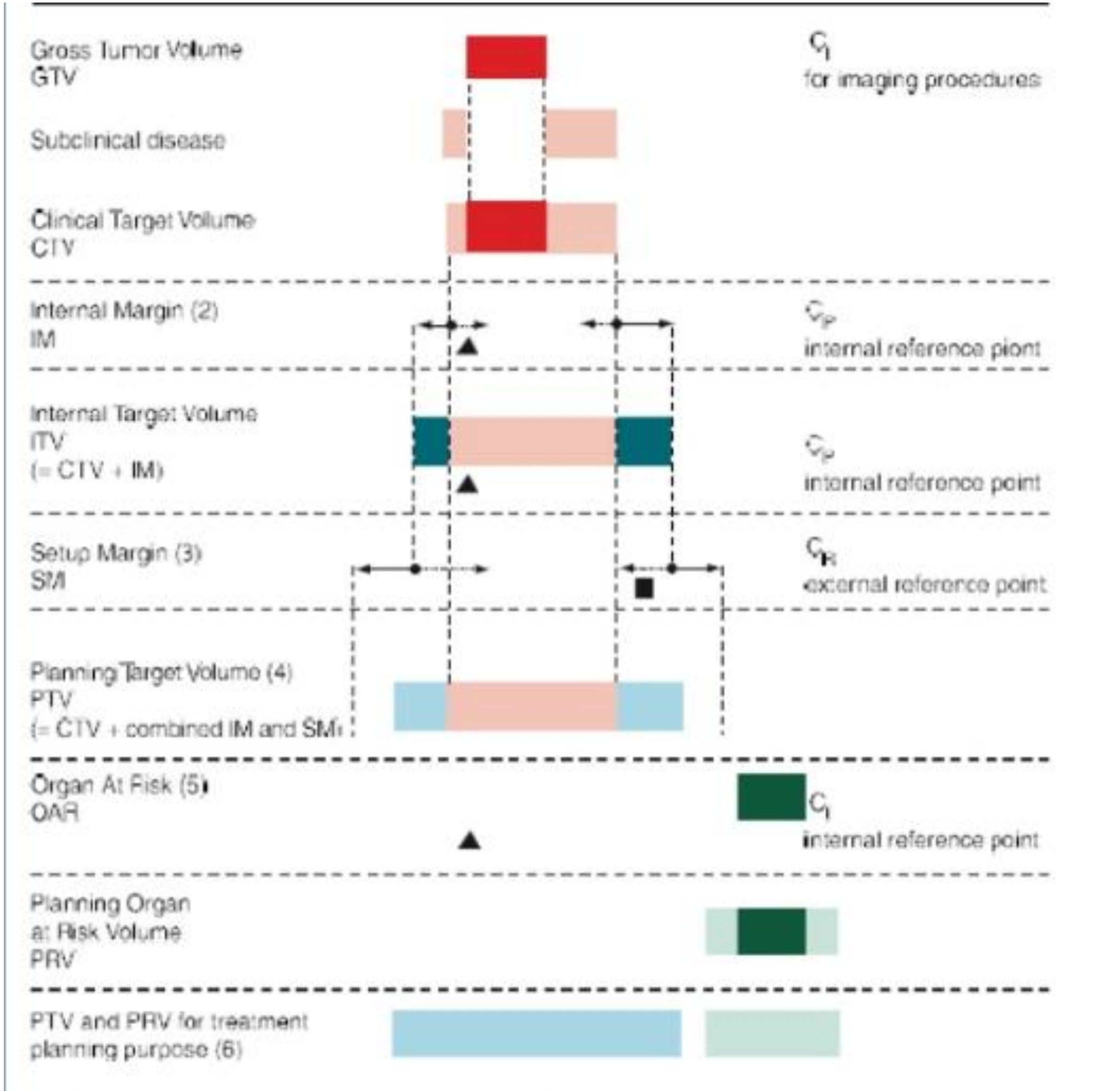


Fig. 3.21 Treatment volumes according to the ICRU-62 report

Contouring Guidelines

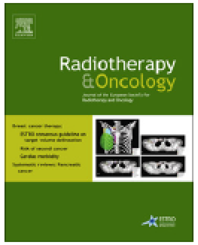
- Ex: ESTRO breast guidelines

Radiotherapy and Oncology 114 (2015) 3–10

Contents lists available at ScienceDirect

Radiotherapy and Oncology

journal homepage: www.thegreenjournal.com



ESTRO consensus guidelines

ESTRO consensus guideline on target volume delineation for elective radiation therapy of early stage breast cancer

Birgitte V. Offersen[a,*], Liesbeth J. Boersma[b], Carine Kirkove[c], Sandra Hol[d], Marianne C. Aznar[e], Albert Biete Sola[f], Youlia M. Kirova[g], Jean-Philippe Pignol[h], Vincent Remouchamps[i], Karolien Verhoeven[j], Caroline Weltens[j], Meritxell Arenas[k], Dorota Gabrys[l], Neil Kopek[m], Mechthild Krause[n], Dan Lundstedt[o], Tanja Marinko[p], Angel Montero[q], John Yarnold[r], Philip Poortmans[s]

Contouring Guidelines

Table 1
ESTRO delineation guidelines for the CTV of lymph node regions, breast and postmastectomy thoracic wall for elective irradiation in breast cancer (see figures).

Borders per region	Axilla level 1 CTVn_L1	Axilla level 2 CTVn_L2	Axilla level 3 CTVn_L3	Lymph node level 4 CTVn_L4	Internal mammary chain CTVn_IMN	Interpectoral nodes CTVn_interpectoralis	Residual breast CTVp_breast	Thoracic wall CTVp_thoracic wall
Cranial	Medial: 5 mm cranial to the axillary vein Lateral: max up to 1 cm below the edge of the humeral head, 5 mm around the axillary vein	Includes the cranial extent of the axillary artery (i.e. 5 mm cranial of axillary vein)	Includes the cranial extent of the subclavian artery (i.e. 5 mm cranial of subclavian vein)	Includes the cranial extent of the subclavian artery (i.e. 5 mm cranial of subclavian vein)	Caudal limit of CTVn_L4	Includes the cranial extent of the axillary artery (i.e. 5 mm cranial of axillary vein)	Upper border of palpable/ visible breast tissue; maximally up to the inferior edge of the sterno-clavicular joint	Guided by palpable/visible signs; if appropriate guided by the contralateral breast; maximally up to the inferior edge of the sterno-clavicular joint
Caudal	To the level of rib 4 – 5, taking also into account the visible effects of the sentinel lymph node biopsy	The caudal border of the minor pectoral muscle. If appropriate: top of surgical ALND	5 mm caudal to the subclavian vein. If appropriate: top of surgical ALND	Includes the subclavian vein with 5 mm margin, thus connecting to the cranial border of CTVn_IMN	Cranial side of the 4th rib (in selected cases 5th rib, see text)	Level 2's caudal limit	Most caudal CT slice with visible breast	Guided by palpable/visible signs; if appropriate guided by the contralateral breast

B.Offersen et al radiother oncol 2015

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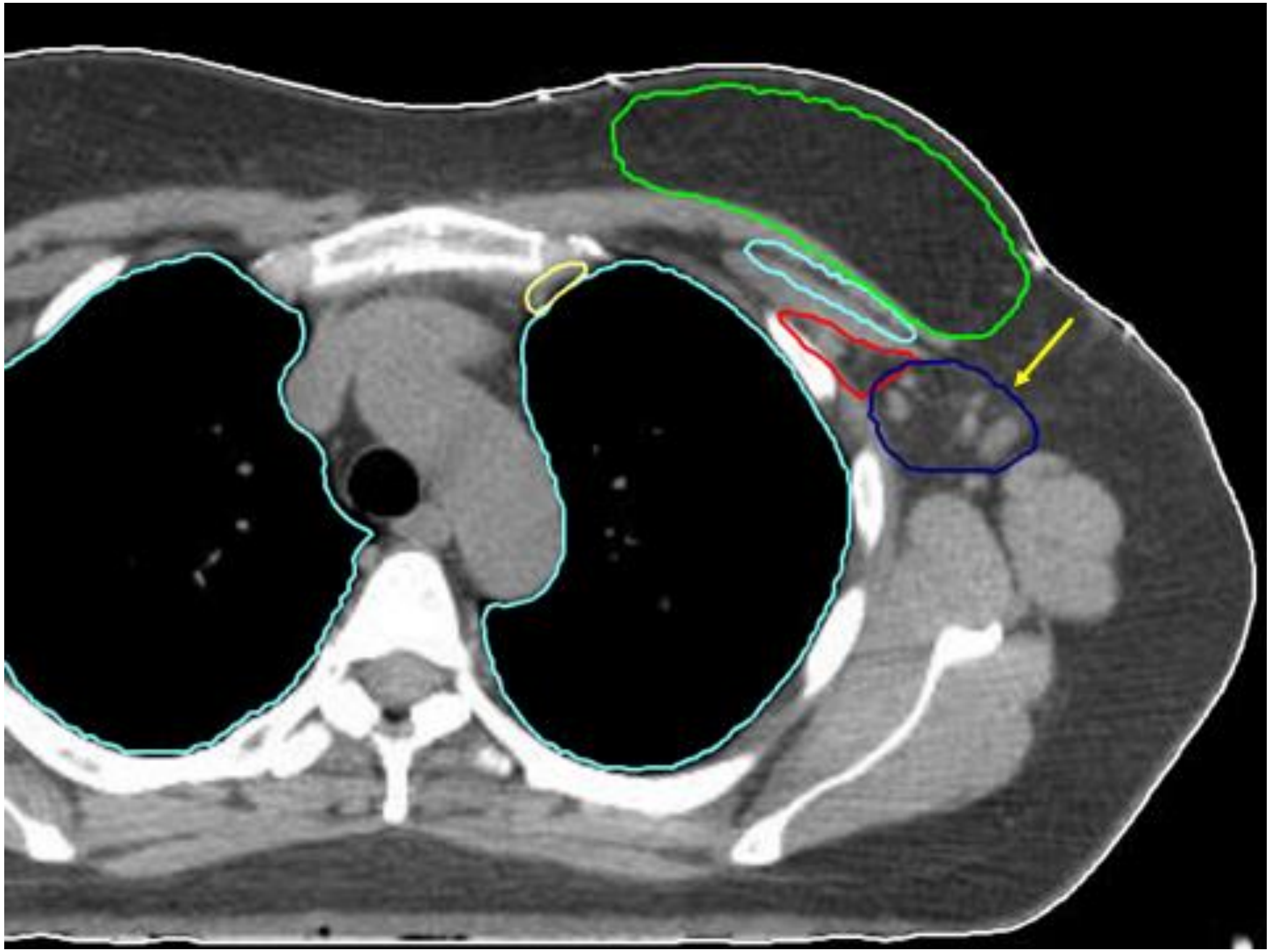
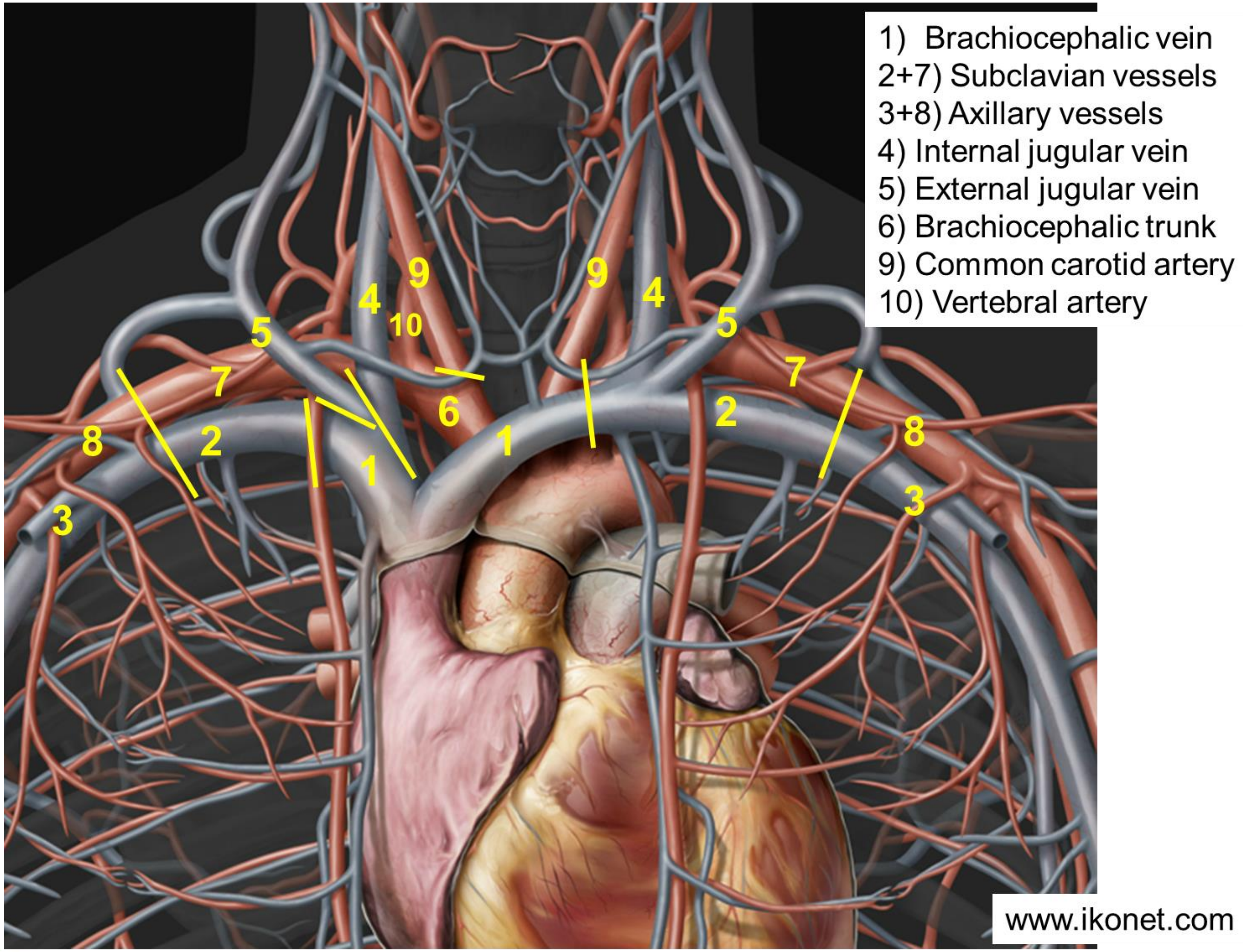
Contouring Guidelines

- Ex: ESTRO breast guidelines



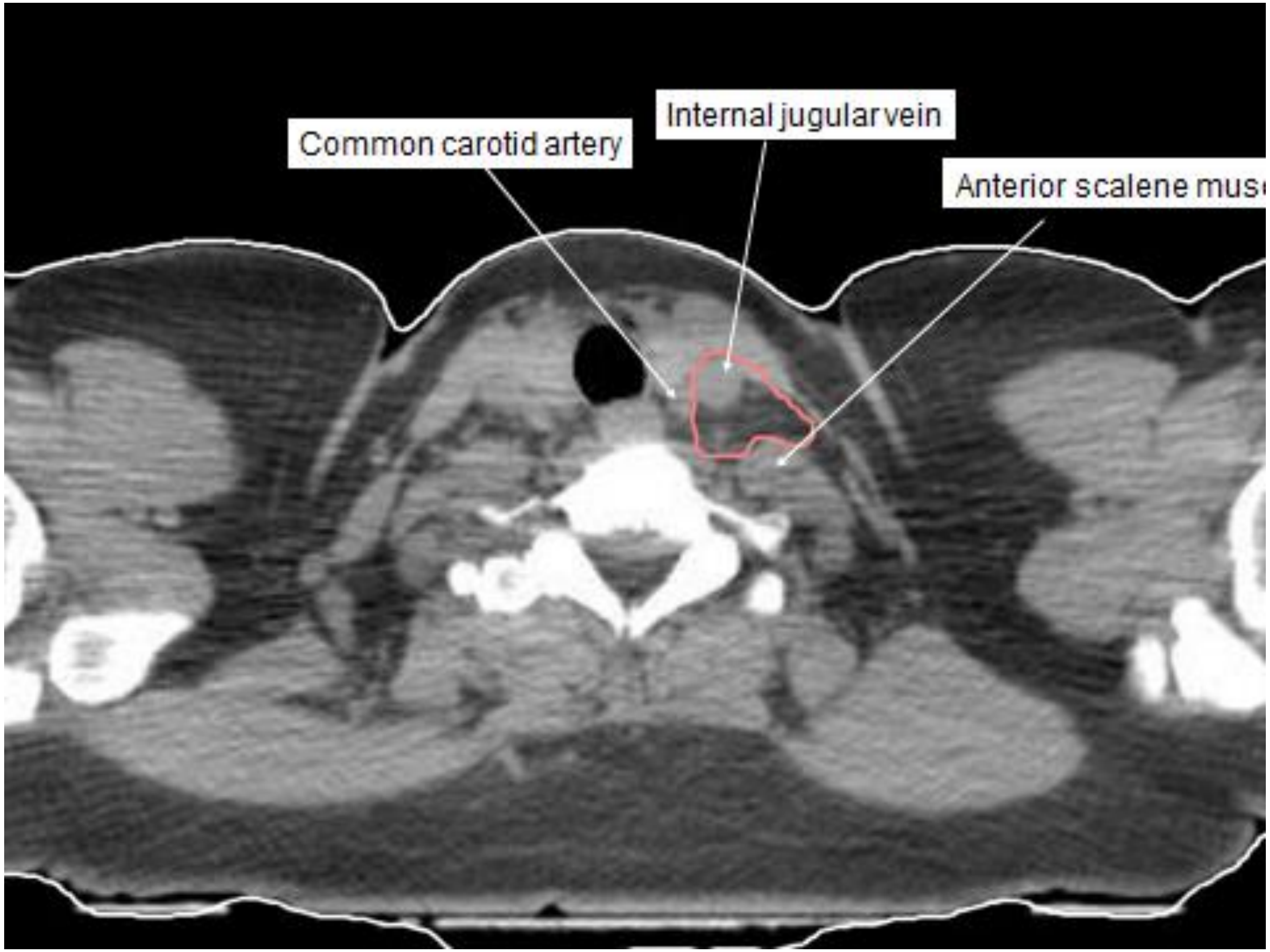
Contouring guidelines

- Anatomical basis are the key!



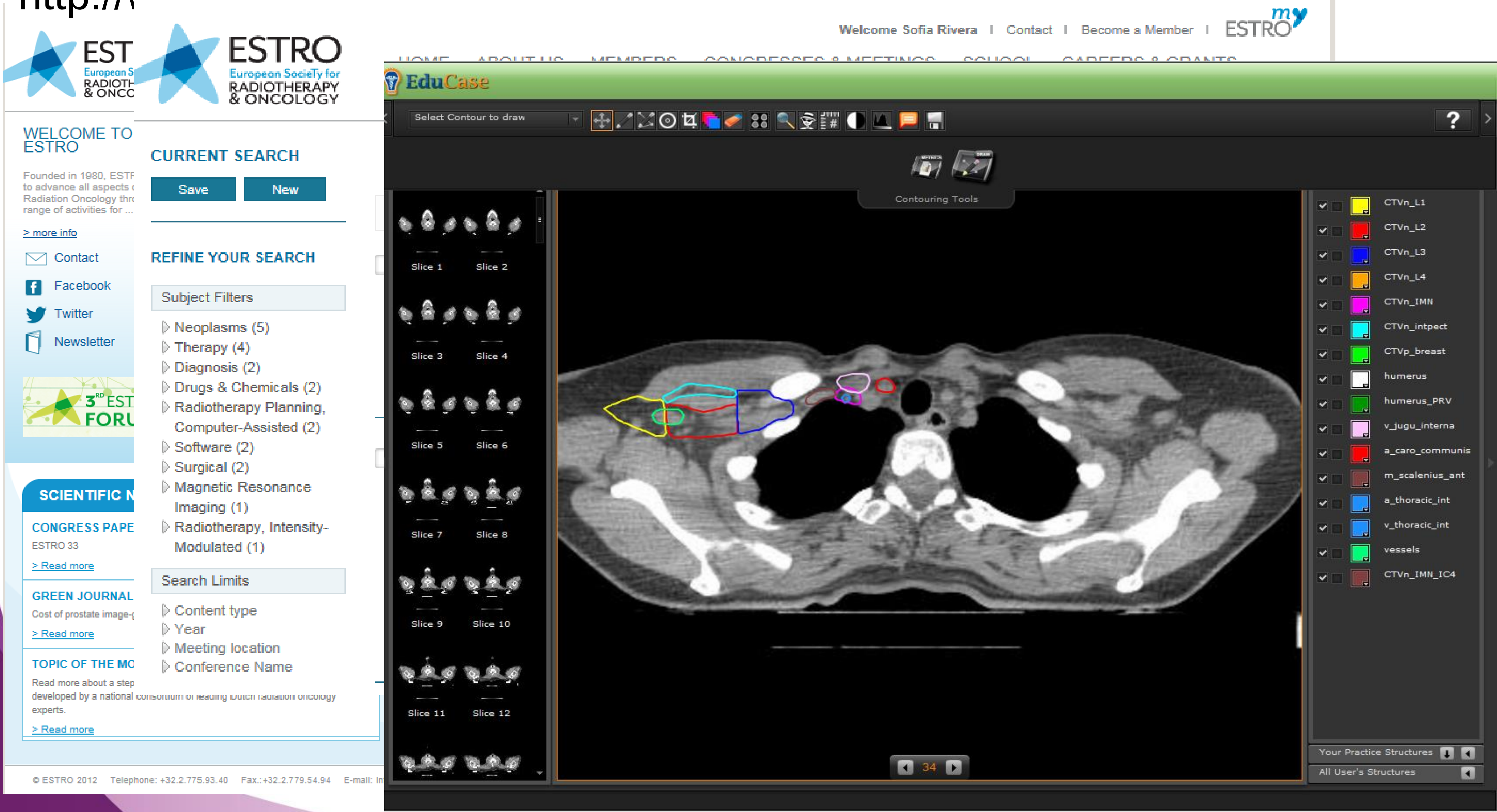
Contouring guidelines

- Anatomical basis are the key!



ESTRO guidelines

http://



Take home messages:

- Inter observer variability in contouring can translate in a systematic error

- Need for a common language: ICRU

- Need for delineation guidelines

- Need for teaching in contouring

Thank you for you attention

Any question?

ORGANS AT RISK DELINEATION

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Liz Forde, MSc (RTT)
Assistant Professor
Discipline of Radiation Therapy
Trinity College Dublin

ARTT
Applied Radiation Therapy
Trinity Research Group

Trinity College Dublin
Coláiste na Tríonóide, Baile Átha Cliath
The University of Dublin

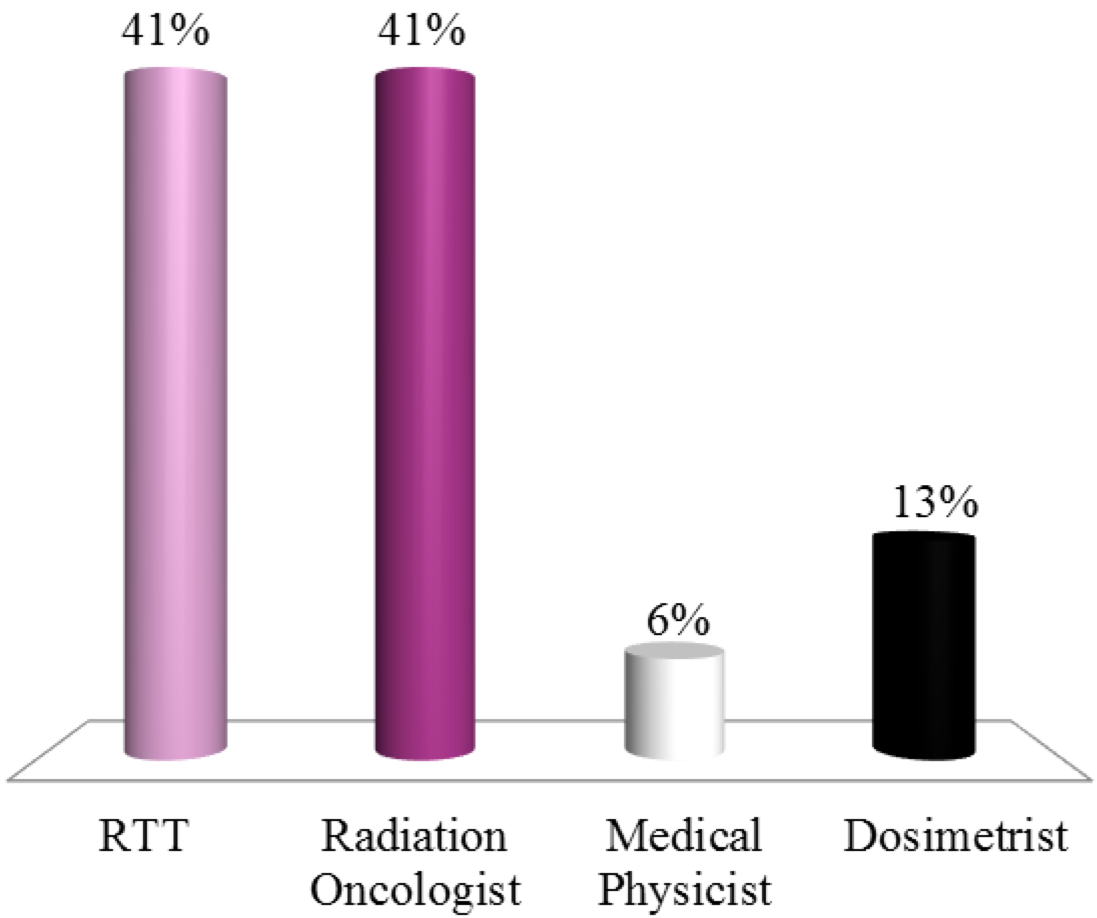
Learning Outcomes

- Discuss the changing roles and responsibilities of RTTs for Organ at Risk (OAR) delineation
- Identify skills required to delineate OARs
- Indentify tools for implementing RTT OAR delineation into your department
- Identify common OARs based on current clinical trials and evidence based consensus guidelines
- Discuss the impact of inaccurate OAR delineation on the evaluation of plan quality

Question Time!

In my current practice organs at risk are contoured by the:

A. RTT
B. Radiation Oncologist
C. Medical Physicist
D. Dosimetrist



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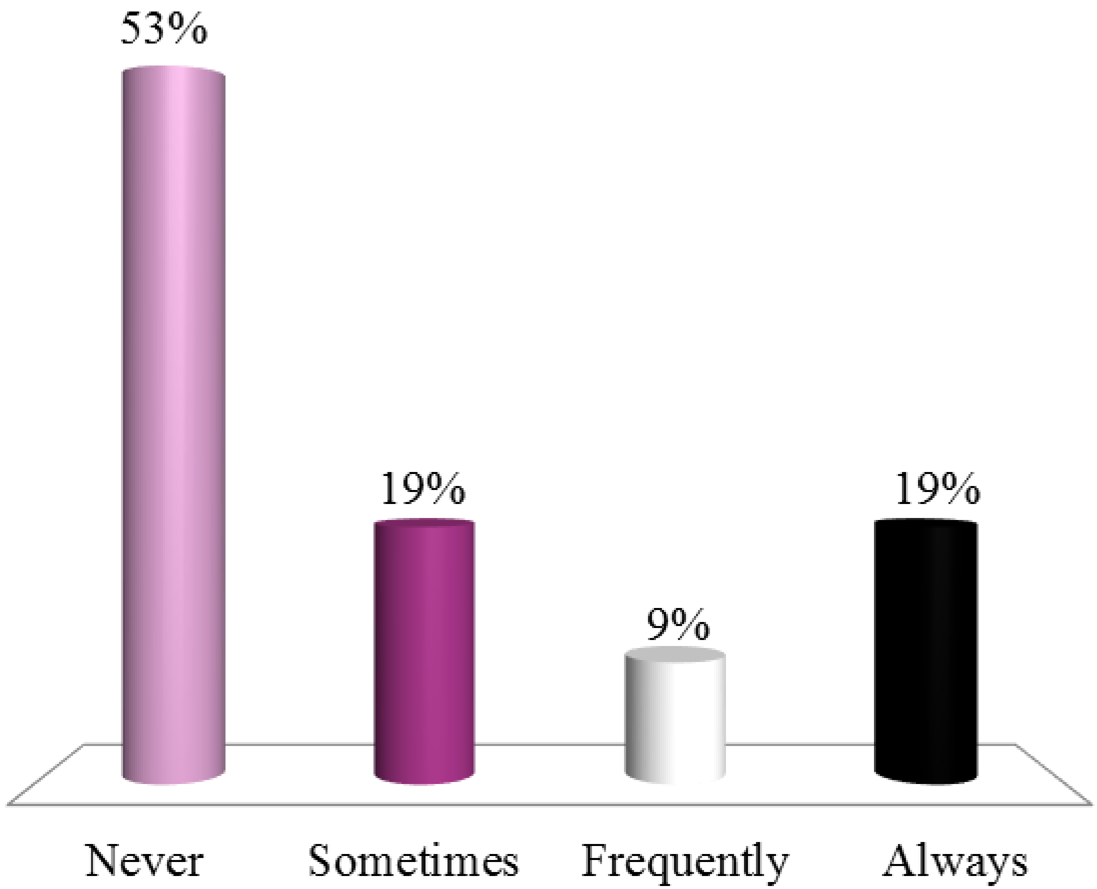
I personally am involved in OAR delineation:

A. Never
B. Sometimes
C. Frequently
D. Always



The New RTT!



“flexible inter professional boundaries” *Schick et al., 2011*



“The goal of a radiation therapist undertaking OAR delineation is logical role expansion.” *(Schick et al 2011)*

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The New RTT

ELSEVIER

Journal of Medical Imaging and Radiation Sciences xx (2014) 1-8

Journal of Medical Imaging and Radiation Sciences

Journal de l'imagerie médicale et des sciences de la radiation

www.elsevier.com/locate/jmir

Role Development for Radiation Therapists: An Examination of the Computed Tomographic Simulation Procedure for Patients Receiving Radiation Therapy for Breast Cancer

Bonnie Bristow, MRT(T), BSc*, Saffiyya Saloojee, MRT(T), Michele Silveira, MRT(T), Shila Vakani, MRT(T) and Angela Turner, MRT(T), BA(Hons)

Department of Radiation Therapy, Odette Cancer Centre, Sunnybrook Health Sciences Centre, Toronto, Ontario, Canada

- Comparison of practice and confidence
- Identified tasks performed at CT Simulation
- Results: 84% no change made by RO

Table 4

Responses for Confidence Levels (n = 9 ROs, n = 21 RTs)

I have confidence in RTs performing the following tasks:	Agree (%)		Neutral (%)		Disagree (%)	
	RO	RT	RO	RT	RO	RT
Placement of baseline	75	100	0	0	25	0
Contouring of cardiac volume	87	95	0	5	13	0
Lung volume	76	100	12	0	12	0
Scar/seroma delineation	50	95	25	5	25	0
Cardiac contour	88	72	12	23	0	5
Spinal contour	75	90	13	10	12	0
Placement of field junction	75	80	13	10	12	10
Humeral shielding	63	62	25	24	12	14
Selection of immobilization	75	90	25	5	0	5

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RTT Lead OAR Delineation – Conclusions from Literature

- Potential for site specialisation of RTs
  - Provide mentorship
  - “train the trainers” approach

- Confidence and accuracy would improve with:
  - Standard protocols or “supporting documentation”
    - Consensus
  - Exposure to a high number of cases and “non standard” cases
  - Enhanced communication between ROs and RTs

- Training model that includes case based education package and is competency based

Tools for Implementation and Facilitating Change

- Education
  - ➢ Online courses
  - ➢ Support from national and international bodies

- Culture of the department
  - ➢ Clinical mentorship
  - ➢ Commitment to evidence based practice
  - ➢ Commitment to role development
  - ➢ Shared goals within the MDT
  - ➢ Open communication

↓ Intra and interobserver variability

Why Are OARs So Important?

- Do no harm culture of medicine
  - ➢ Decrease impact of radiation to our patients

- Requirement for inverse planning optimisation process
  - ➢ IMRT
  - ➢ VMAT

- Generates DVH information and assists in prediction of toxicity
  - ➢ Serial and Parallel structures
  - ➢ Assessment of clinical impact and disturbance on daily activities

Why Is ***Accuracy*** So Important?

- Consistency and uniformity
  - Within the department
    - Prospective data collection
    - Analysis of local practice and impact on patients
  - Within the context of clinical trials
    - Compliance with trial specifications
    - Allows for collections of data and comparison of outcomes and toxicity at a larger international scale
  - "reduction in inter- and intra-observer variability and therefore unambiguous reporting of possible dose-volume effect relationships" *(van der Water, 2009)*

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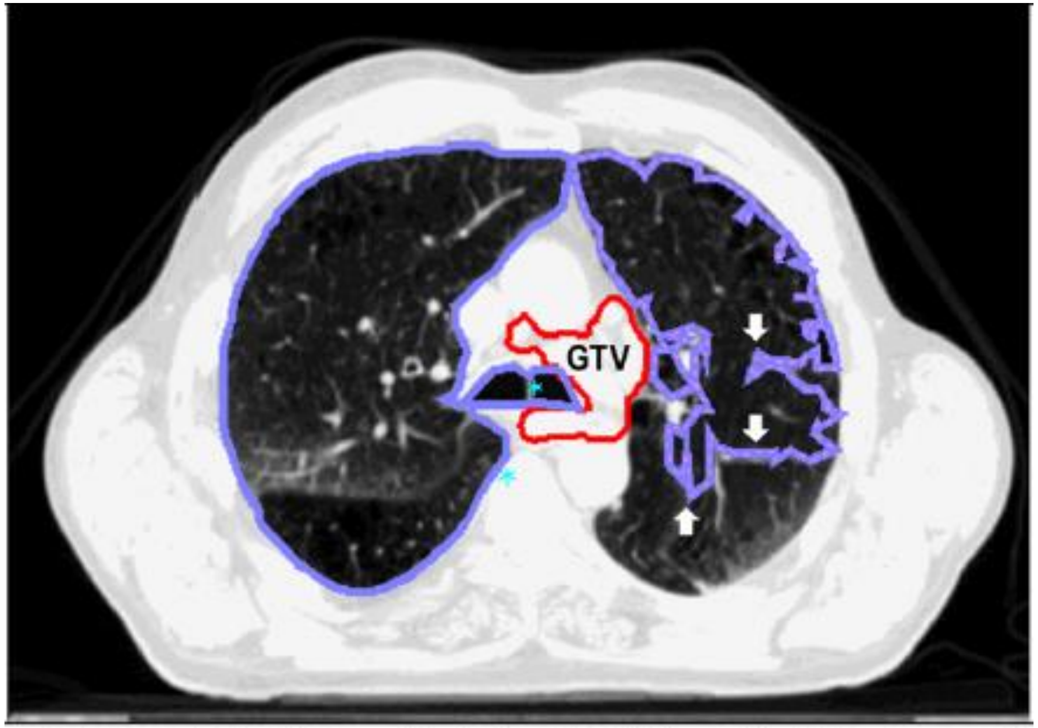
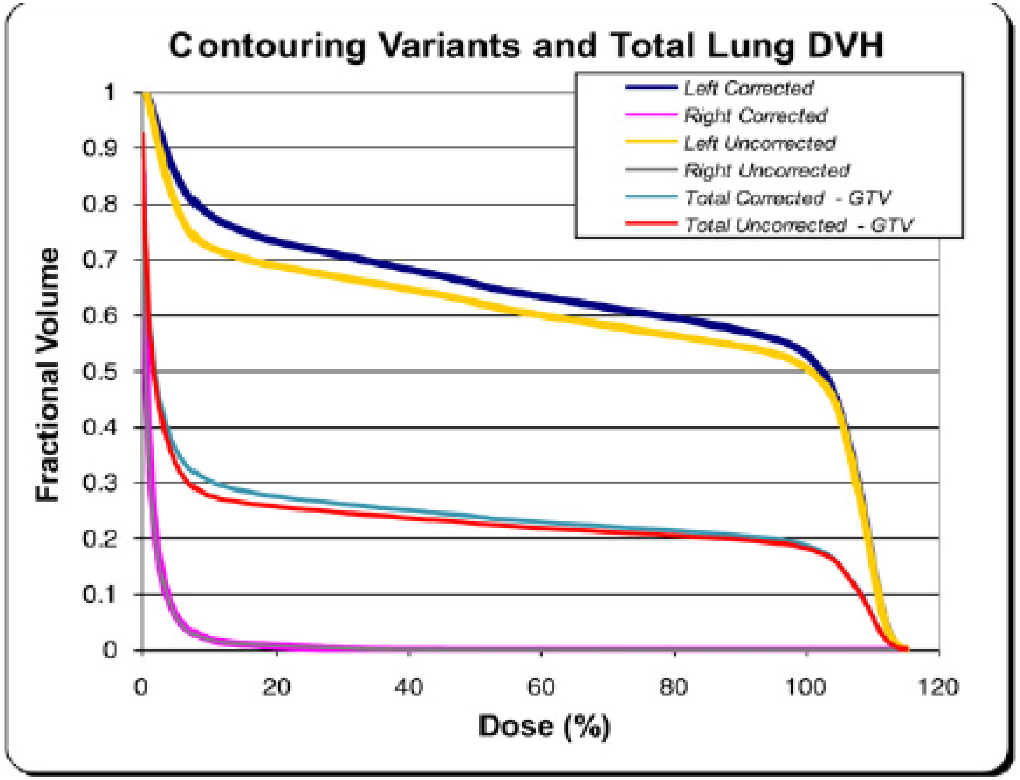
Why is ***Accuracy*** So Important?



A: Lung Contour - Autotrack Failure (white arrows)

What is wrong in this picture?
What has caused this?
What impact would this have?

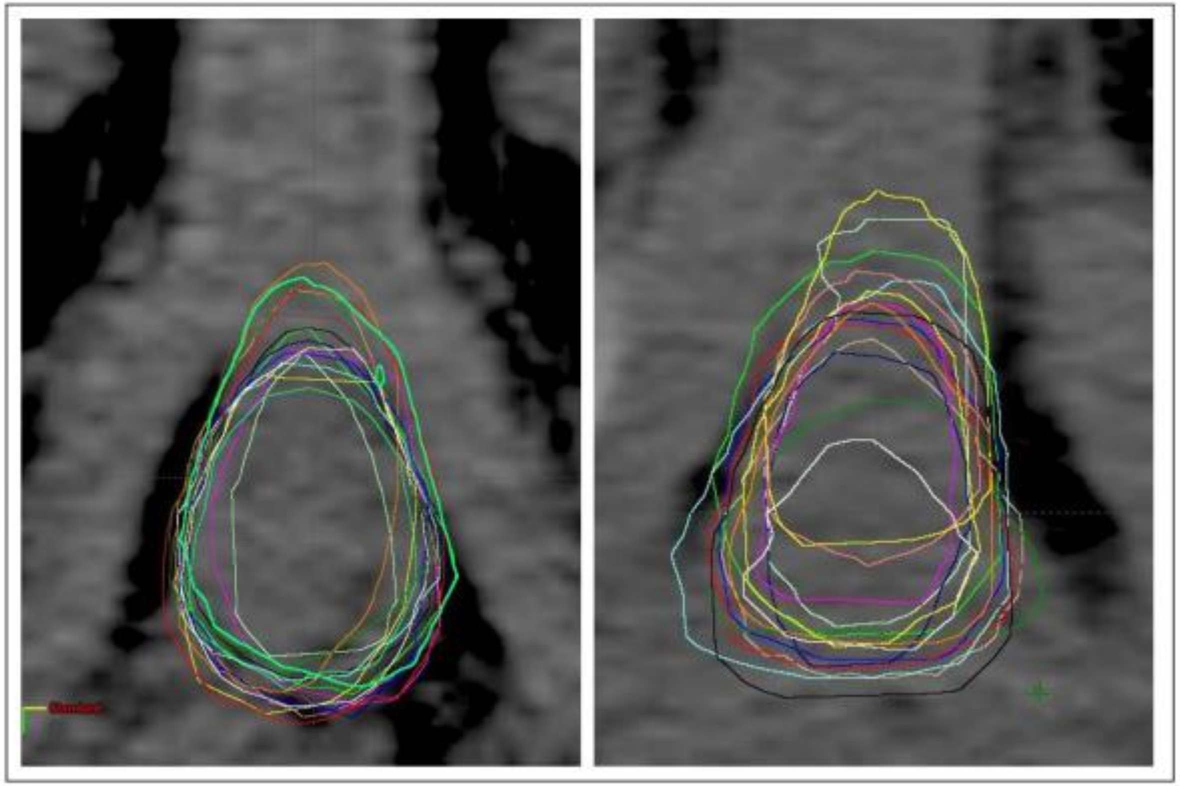


C: Lung DVH differences of contouring variants

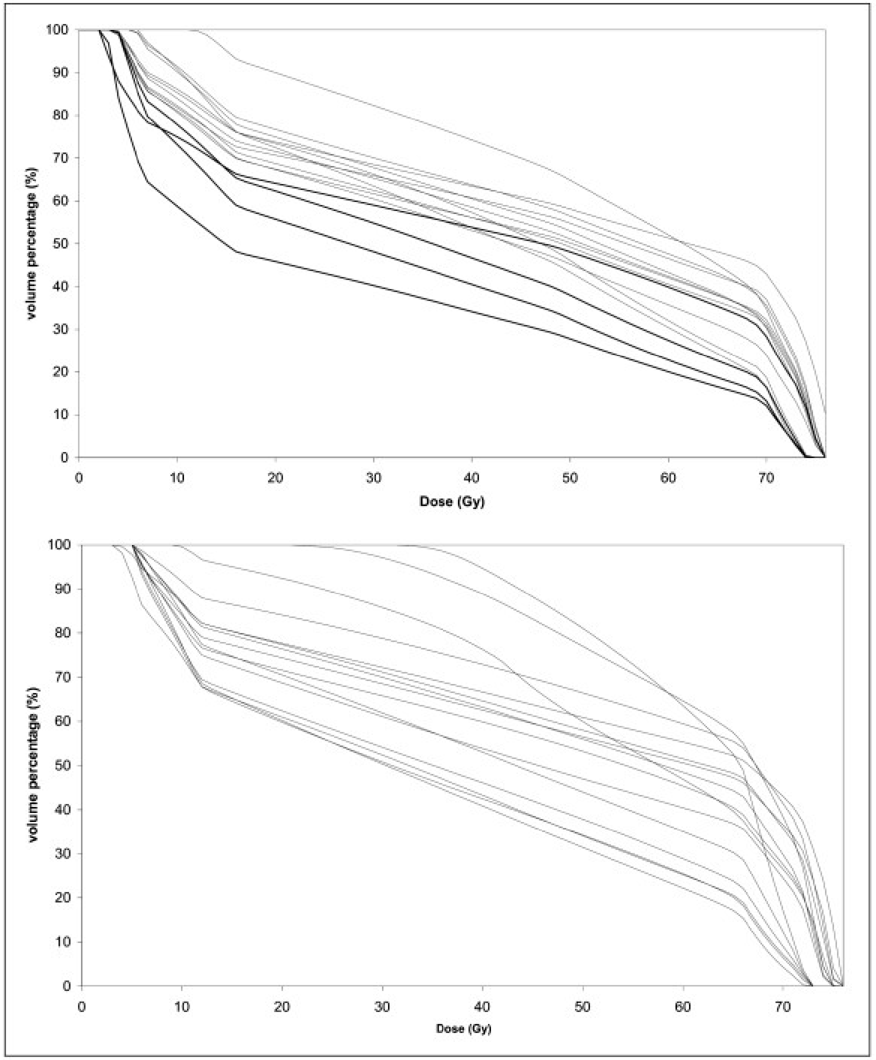
Research — Open Access

Inter-observer variability in contouring the penile bulb on CT images for prostate cancer treatment planning

Lucia Perna[1]*, Cesare Cozzarini[2], Eleonora Maggiulli[1], Gianni Fellin[3], Tiziana Rancati[4], Riccardo Valdagni[4], Vittorio Vavassori[5], Sergio Villa[6] and Claudio Fiorino[1]



A plot of the central slice of PB contours drawn by all observers of two patients: one with the lowest inter-observer volume variation (left side) and one with the largest inter-observer volume variation (right side).



Graphs showing PB dose-volume histograms relative to the two patients in figure 5: the first (top of figure) with the lowest impact of inter-observer variation on DVH parameters, and the second (bottom of the figure) with the largest impact of inter-observer variation on DVH parameters.

Perna *et al. Radiation Oncology* 2011 **6**:123 doi:10.1186/1748-717X-6-123

Possible recommendations put forward by the authors:

- Contouring by a single user
- Introduction of MRI into practice
- Improving the agreement between observers (consensus)

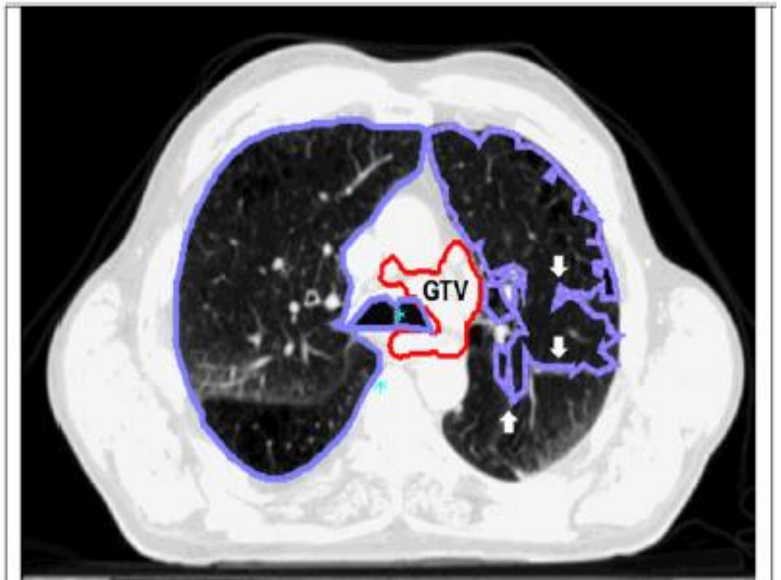
What Are Some of the Challenges in Delineation

- Windowing
- Length to contour
- Over reliance on auto-contouring
- Contrast
- Motion
- Exclusion of disease
- Patient positioning

Tools Available – Auto-segmentation

- Auto segmentation based on **tools in the TPS**
  - ➢ Widely available
  - ➢ Spindle snake, Flood fill…

  - ➢ "Common errors include…using the auto-threshold contouring tools in the TPS and not editing the resulting errors" *(Gay et al., 2012)*



A: Lung Contour - Autotrack Failure (white arrows)

Trachea included and portion of lung missing

Tools Available – Auto-segmentation

- **Atlas based** Auto segmentation

- Propagation of segmented structures from an atlas onto the patient image using deformable registration *(Lim and Leech, 2017)*

- Atlas can be based on:
  - Single patient dataset
  - Multiple patient data (based on an average of a range of patients from multiple libraries)
  - Model based (using library of previously manually contoured patients)

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Tools Available – Auto-segmentation

- Attractive due to time saving aspects and support of adaptive RT, but…

- Beware of automaticity!

  - “Even with the implementation of AS software in the future, it should be reinforced that manual editing is still a necessity for patient safety.” *(Lim and Leech, 2017)*

  - “atlas-based automatic segmentation tool … is timesaving but still necessitates review and corrections by an expert” *(Daisne and Blumhofer, 2013)*

You still need the anatomical knowledge of what is correct!

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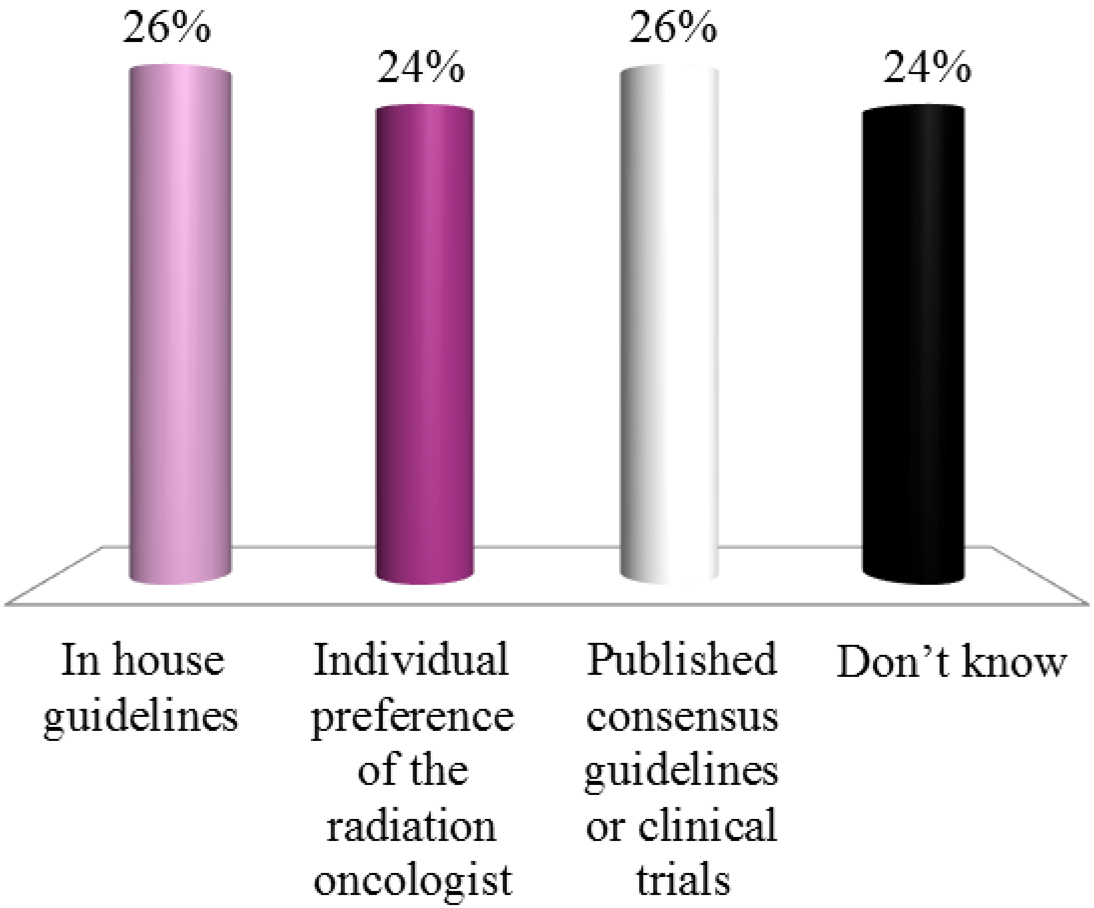
Question Time!

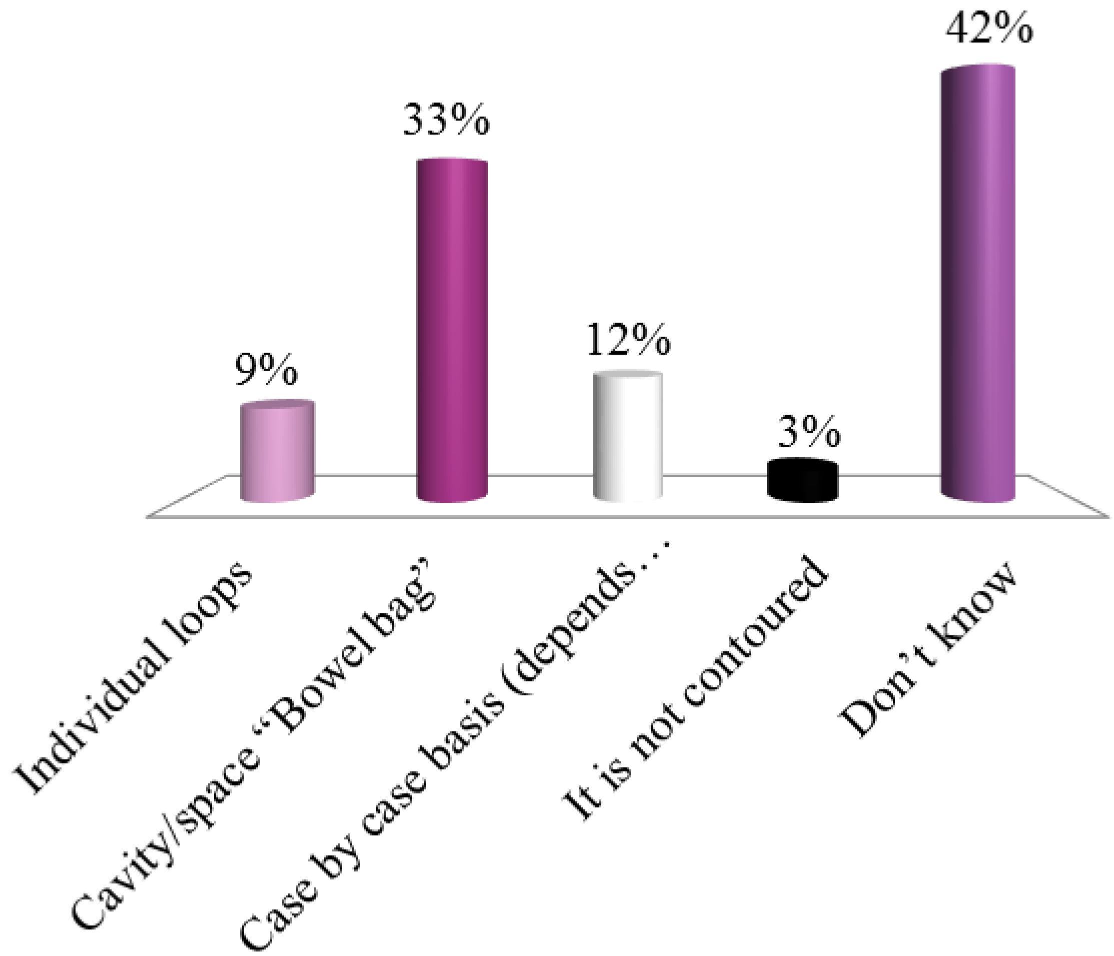
In your current practice what defines how organs at risk are contoured?

A. In house guidelines
B. Individual preference of the radiation oncologist
C. Published consensus guidelines or clinical trials
D. Don’t know



In your current practice how is the small bowel contoured?

A. Individual loops
B. Cavity/space "Bowel bag"
C. Case by case basis (depends on treatment site)
D. It is not contoured
E. Don't know



Is there Consensus?

eLearning Modules by Experts

QUANTEC

Contouring Atlases

Clinical Trials

Let's Look at Some Common OARs in the *Pelvis*

Rectum

Small Bowel

Urethra

Bladder

Sigmoid

Femoral heads

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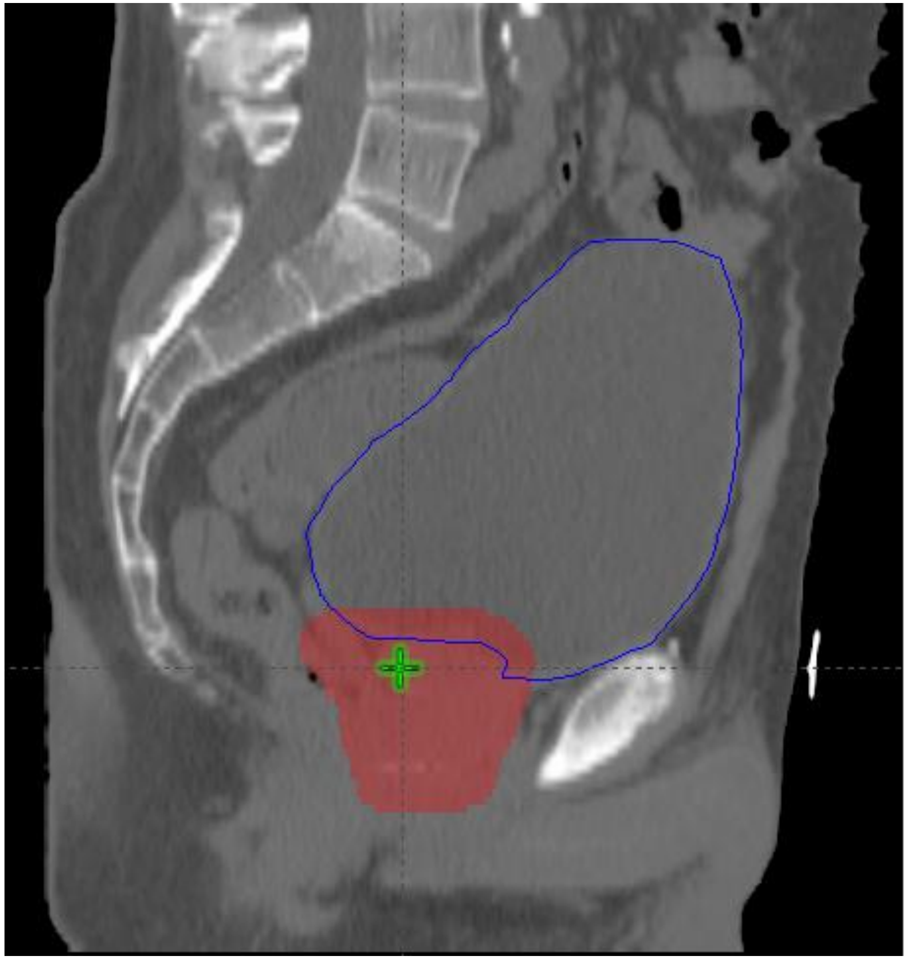
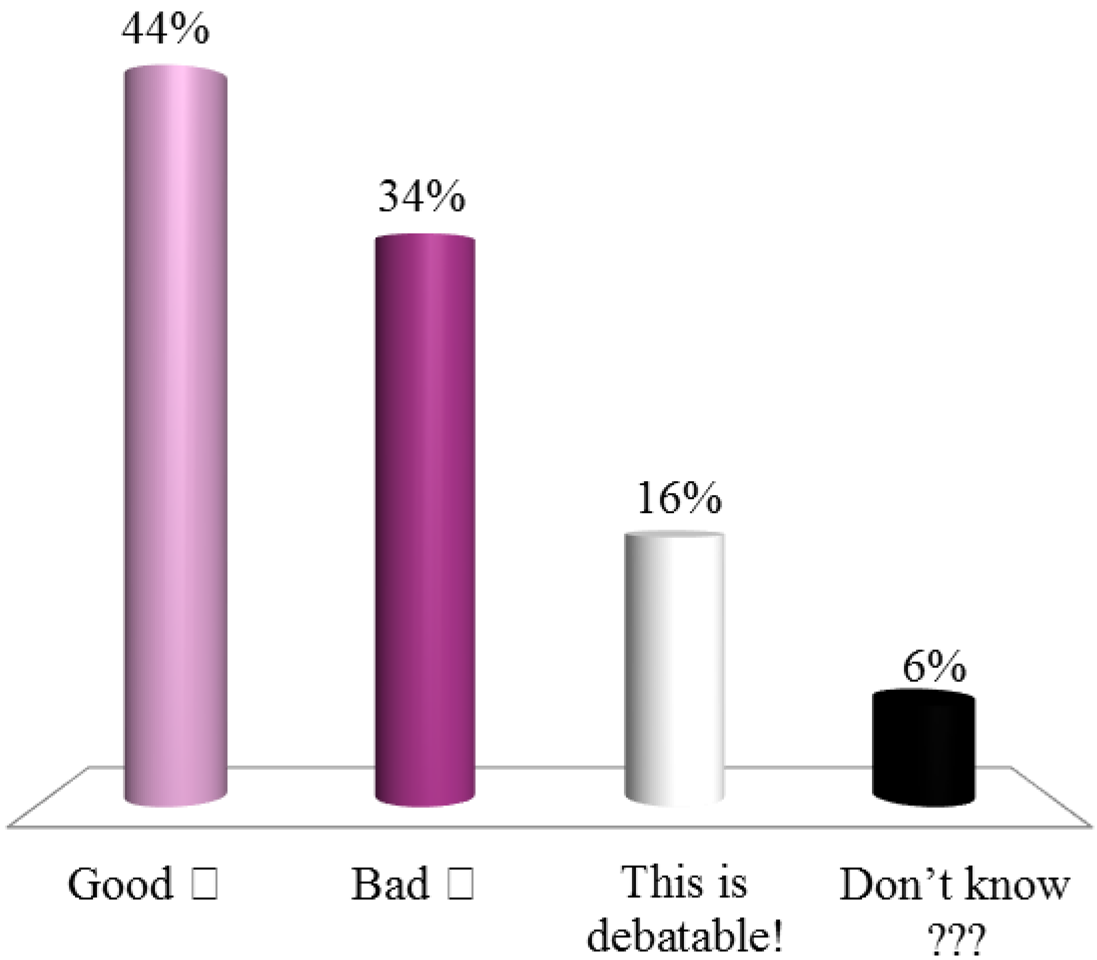
Bladder - Good or Bad?

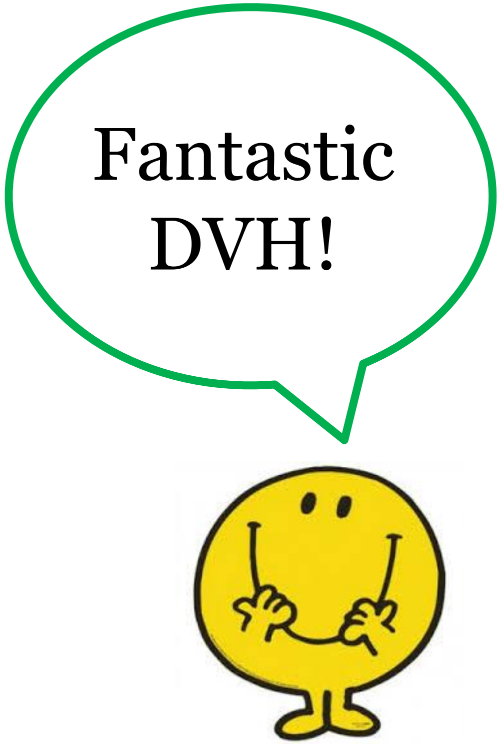


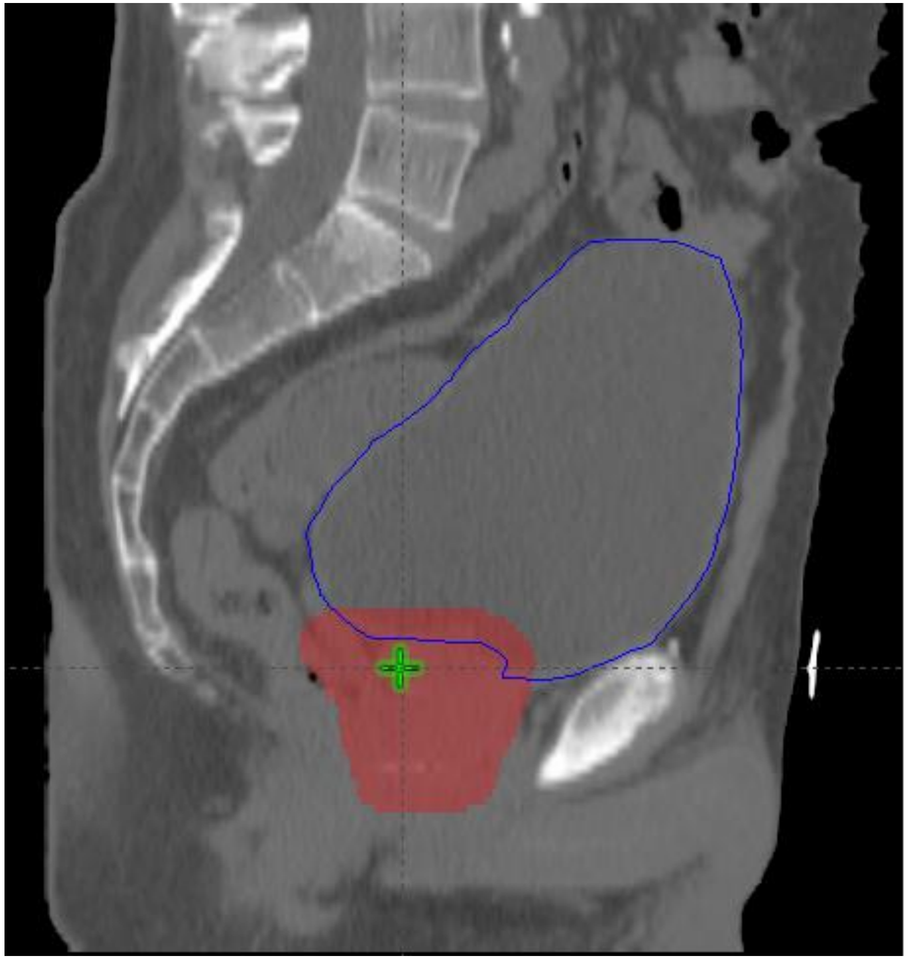
This bladder size is:

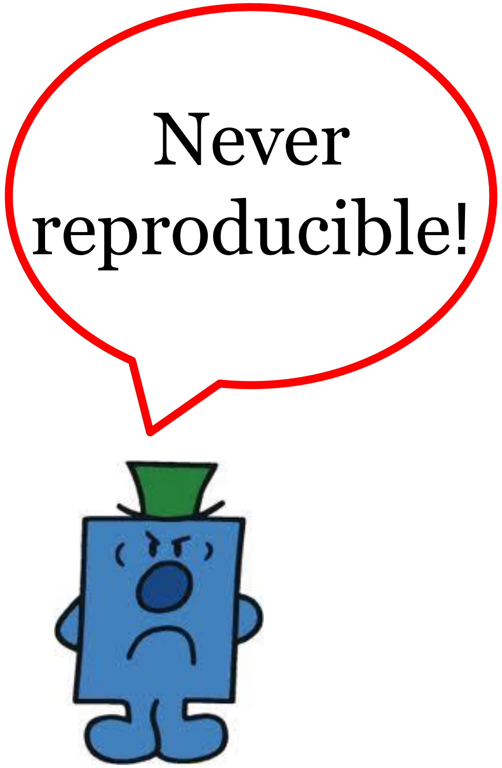
A. Good ☺
B. Bad ☹
C. This is debatable!
D. Don’t know ???



Bladder - Good or Bad?







What Do the Experts Say? - ***Bladder***

- Uncertainties or variations in practice:
  - Bladder wall or solid contour including urine?
  - Whole structure or set length from PTV?
  - Contrast from post prostatectomy (defining the SUA)

  - Easy to define on planning CT but potential of high variation
    - Unrealistic DVH
    - Consider CBCT review and generate bladder DVH of the day

  - Does it impact on target position?

    - **What are you treating?**
    - Prostate
    - Prostate bed
    - Endometrial cancer

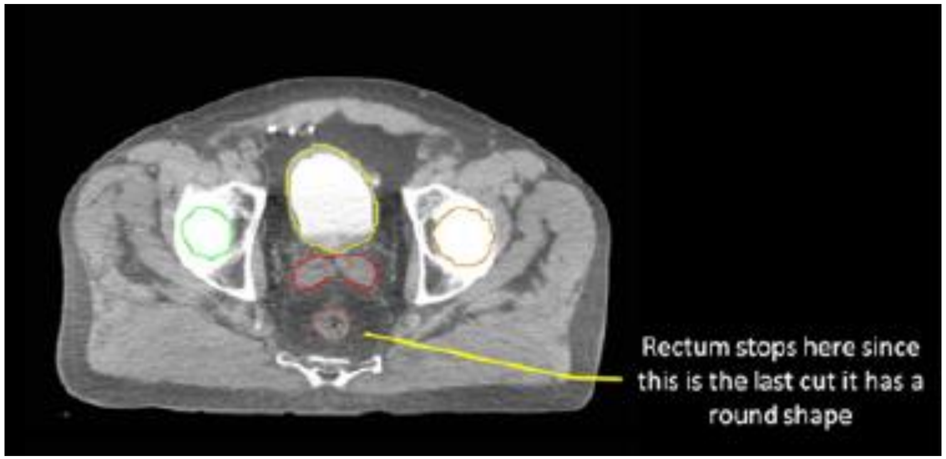
What Do the Experts Say? - ***Rectum***

- Uncertainties or variations in practice:
  - ➢ Inferior limit – Anal verge or ischial tuberosities?
  - ➢ Rectal wall or solid including contents?
  - ➢ Set length defined by the PTV volume?

- Recommendations:

Organ segmentation

The rectum should be segmented from above the anal verge to the turn into the sigmoid colon, including the rectal contents. Although there can be variation in defining these landmarks, the superior limit is where the bowel moves anteriorly, close to the inferior level of the sacroiliac joints, and the inferior limit is commonly at the bottom of the ischial tuberosities. In prostate cancer therapy, an empty rectum at



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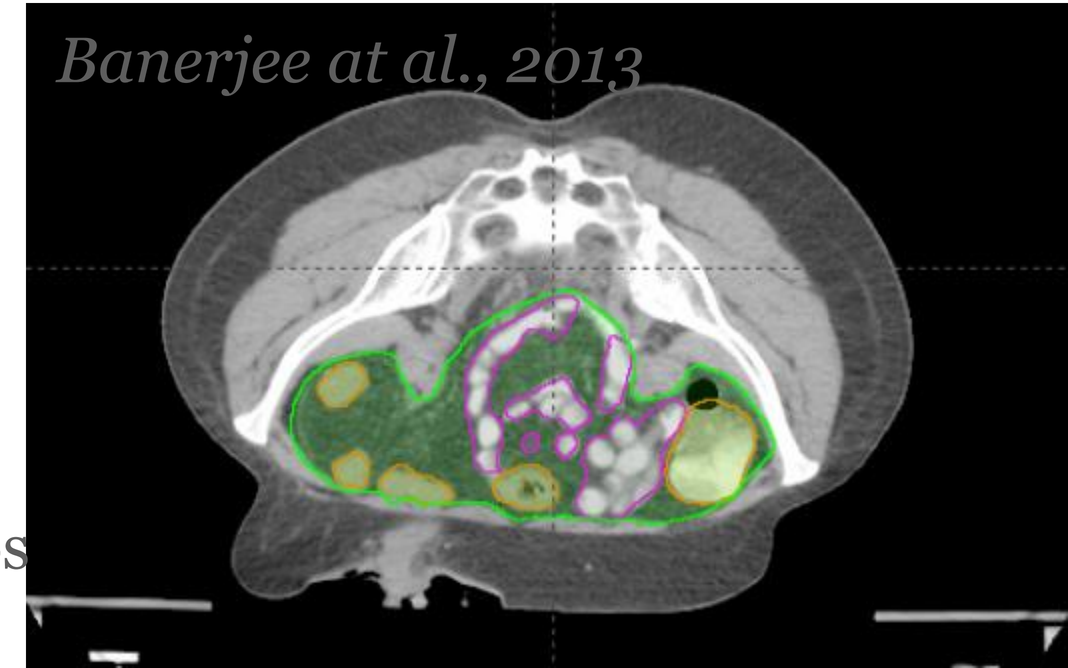
What Do the Experts Say? – *Small Bowel*

- Uncertainties or variations in practice
  - What is large bowel/vessels/nodes
  - Oral contrast results in artefact on planning scan and inappropriate HU
  - Small bowel position is variable during treatment
  - Individual loops vs. "Bowel bag"

- Recommendations:

The absolute volume of small bowel receiving ≥15 Gy should be held to <120 cc when possible to minimize severe acute toxicity, if delineating the contours of bowel loops themselves. Alternatively, if the entire volume of peritoneal space in which the small bowel can move is delineated, the volume receiving >45 Gy should be <195 cc when possible.

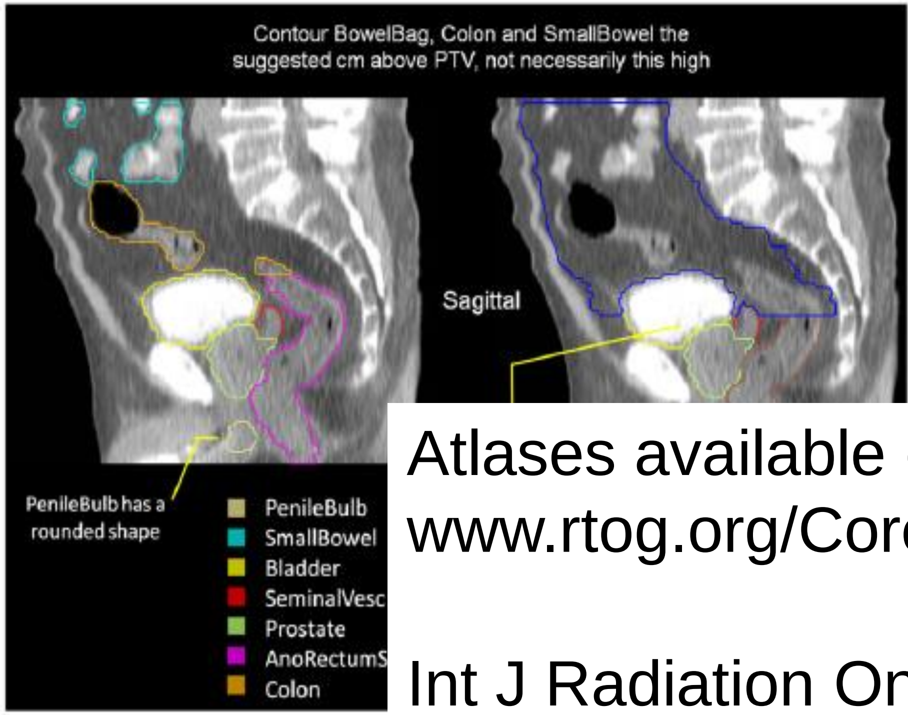


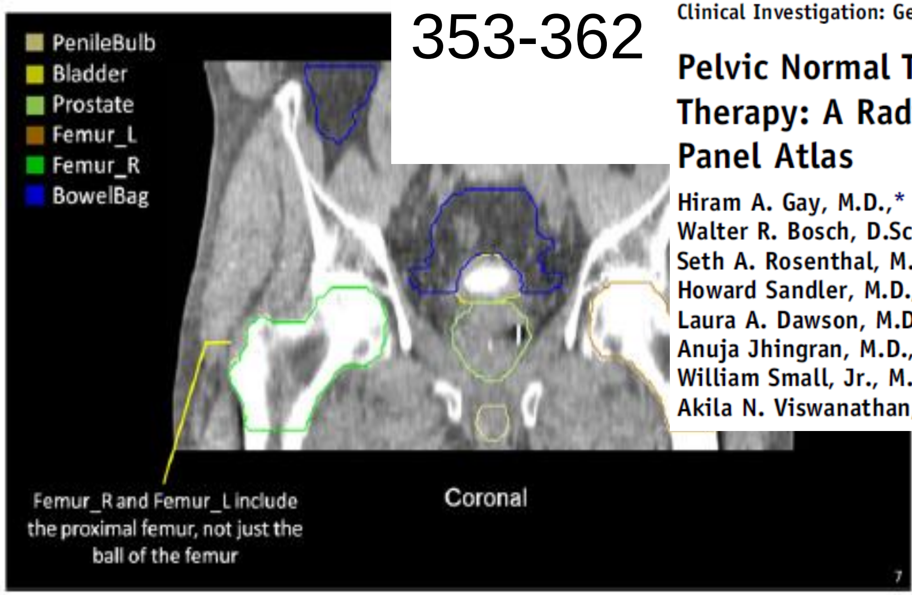
Orange = Large bowel

Pink = Small bowel loops

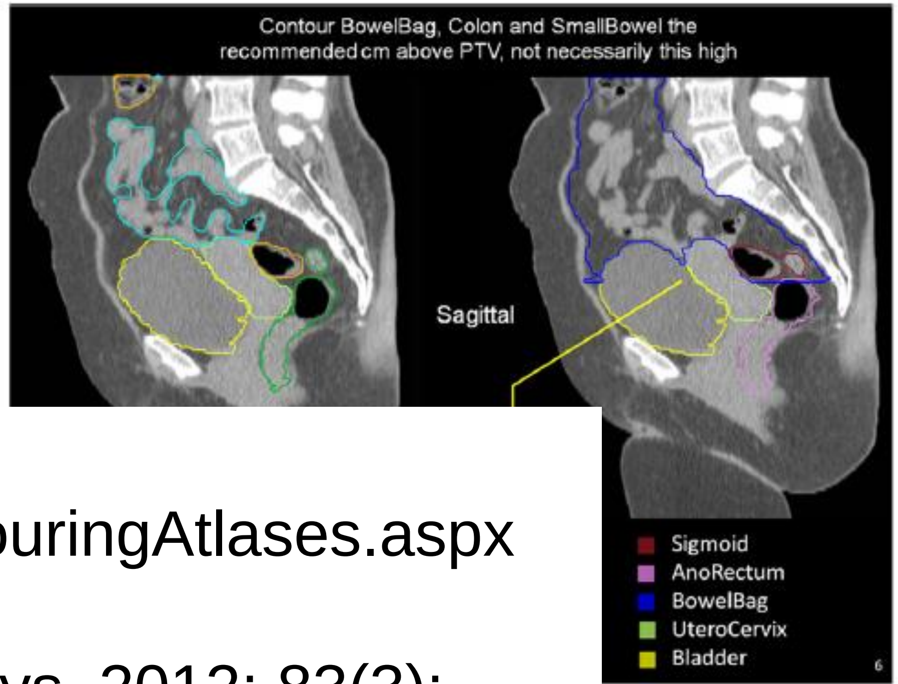
Green = Bowel bag

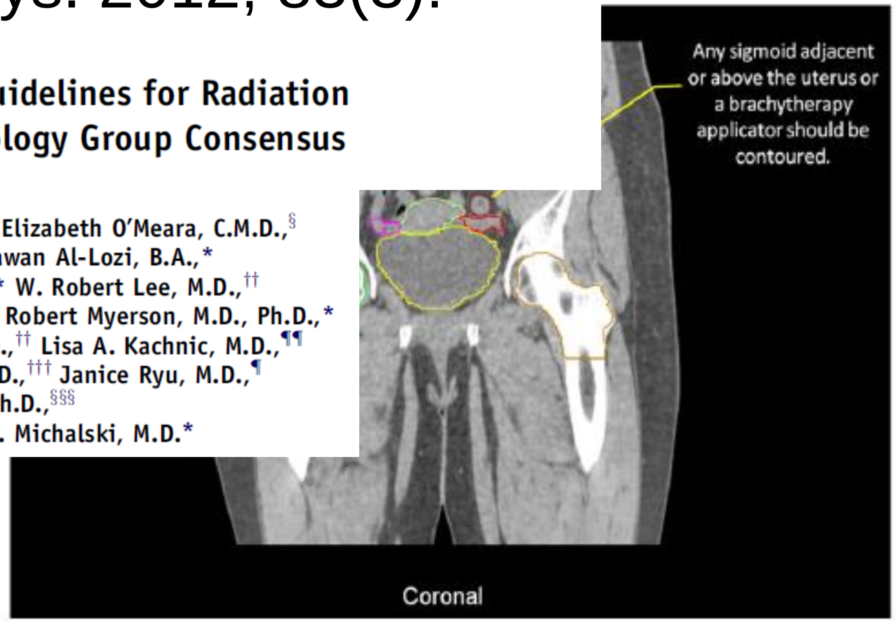
Male pelvis





Female Pelvis





Atlases available online at:
www.rtog.org/CoreLab/ContouringAtlases.aspx

Int J Radiation Oncol Biol Phys. 2012; 83(3): 353-362

Clinical Investigation: Genitourinary Cancer

Pelvic Normal Tissue Contouring Guidelines for Radiation Therapy: A Radiation Therapy Oncology Group Consensus Panel Atlas

Hiram A. Gay, M.D.,* H. Joseph Barthold, M.D.,[†,‡] Elizabeth O'Meara, C.M.D.,[§] Walter R. Bosch, D.Sc.,* Issam El Naqa, Ph.D.,[‖] Rawan Al-Lozi, B.A.,* Seth A. Rosenthal, M.D.,[¶] Colleen Lawton, M.D.,** W. Robert Lee, M.D.,[††] Howard Sandler, M.D.,[‡‡] Anthony Zietman, M.D.,[§§] Robert Myerson, M.D., Ph.D.,* Laura A. Dawson, M.D.,[‖‖] Christopher Willett, M.D.,[††] Lisa A. Kachnic, M.D.,[¶¶] Anuja Jhingran, M.D.,*** Lorraine Portelance, M.D.,[†††] Janice Ryu, M.D.,[¶] William Small, Jr., M.D.,[‡‡‡] David Gaffney, M.D., Ph.D.,[§§§] Akila N. Viswanathan, M.D., M.P.H.,[‖‖‖] and Jeff M. Michalski, M.D.*

Let's Look at Some Common OARs in the ***Thorax***

Heart

Ribs

Lungs

Spinal Cord

Oesophagus

Main Bronchus

Brachial Plexus

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RTOG Thoracic Atlas available from:

http://www.rtog.org/CoreLab/ContouringAtlases/LungAtlas.aspx

RTOG
RADIATION THERAPY ONCOLOGY GROUP

Atlases for Organs at Risk (OARs) in Thoracic Radiation Therapy

Feng-Ming (Spring) K
Leslie Quint
Mitchell Macht
Jeffrey Bradl

Int. J. Radiation Oncology Biol. Phys., Vol. 81, No. 5, pp. 1442–1457, 2011

0360-3016/$ - see front matter

ELSEVIER

doi:10.1016/j.ijrobp.2010.07.1977

CLINICAL INVESTIGATION — **Normal Tissue**

CONSIDERATION OF DOSE LIMITS FOR ORGANS AT RISK OF THORACIC RADIOTHERAPY: ATLAS FOR LUNG, PROXIMAL BRONCHIAL TREE, ESOPHAGUS, SPINAL CORD, RIBS, AND BRACHIAL PLEXUS

Feng-Ming (Spring) Kong, M.D., Ph.D.,* Timothy Ritter, Ph.D.,* Douglas J. Quint, M.D.,†
Suresh Senan, M.D.,‡ Laurie E. Gaspar, M.D.,§ Ritsuko U. Komaki, M.D.,¶
Coen
Jeffrey D. Bra

Int. J. Radiation Oncology Biol. Phys., Vol. 79, No. 1, pp. 10–18, 2011

0360-3016/$–see front matter

ELSEVIER

doi:10.1016/j.ijrobp.2009.10.058

CLINICAL INVESTIGATION — **Breast**

DEVELOPMENT AND VALIDATION OF A HEART ATLAS TO STUDY CARDIAC EXPOSURE TO RADIATION FOLLOWING TREATMENT FOR BREAST CANCER

Mary Feng, M.D.,* Jean M. Moran, Ph.D.,* Todd Koelling, M.D.,† Aamer Chughtai, M.D.,‡
June L. Chan, M.D.,* Laura Freedman, M.D.,* James A. Hayman, M.D.,*
Reshma Jagsi, M.D., D. Phil.,* Shruti Jolly, M.D.,* Janice Larouere, M.D.,*
Julie Soriano, M.D.,* Robin Marsh, C.M.D.,* and Lori J. Pierce, M.D.*

What Do the Experts Say? - ***Lung***

Challenges

- Inappropriate window settings!
- Exclusion of disease from healthy lung?
- Inclusion of vessels?

Recommendations

- Air inflated lung only
  - Do not include fluid
- Contoured as single or combined structures
- Exclude lung GTV
- Exclude trachea/bronchus
- Exclude vessels <1cm
- Auto-segmentation is allowed combined with manual inspection
- Ensure appropriate windowing

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What Do the Experts Say? – *Spinal Cord*

Challenges

- Difficult to see true cord on CT
- Often not specifically covered in atlases
- Circumferential extend?
  - Contour cord or canal?
- Superior/Inferior extent
  - Entire length visible on planning scan or set distance from PTV?

Recommendations

- Use MRI fusion, if available
- Contour to the bony limits of the canal
- For lung cases, superior limit is the same as oesophagus (cricoid cartilage)
- Inferior limit is L2/L3 junction

What Do the Experts Say? – ***Heart***

Challenges

- Contour specific structures within the heart?
- Superior limit

Recommendations

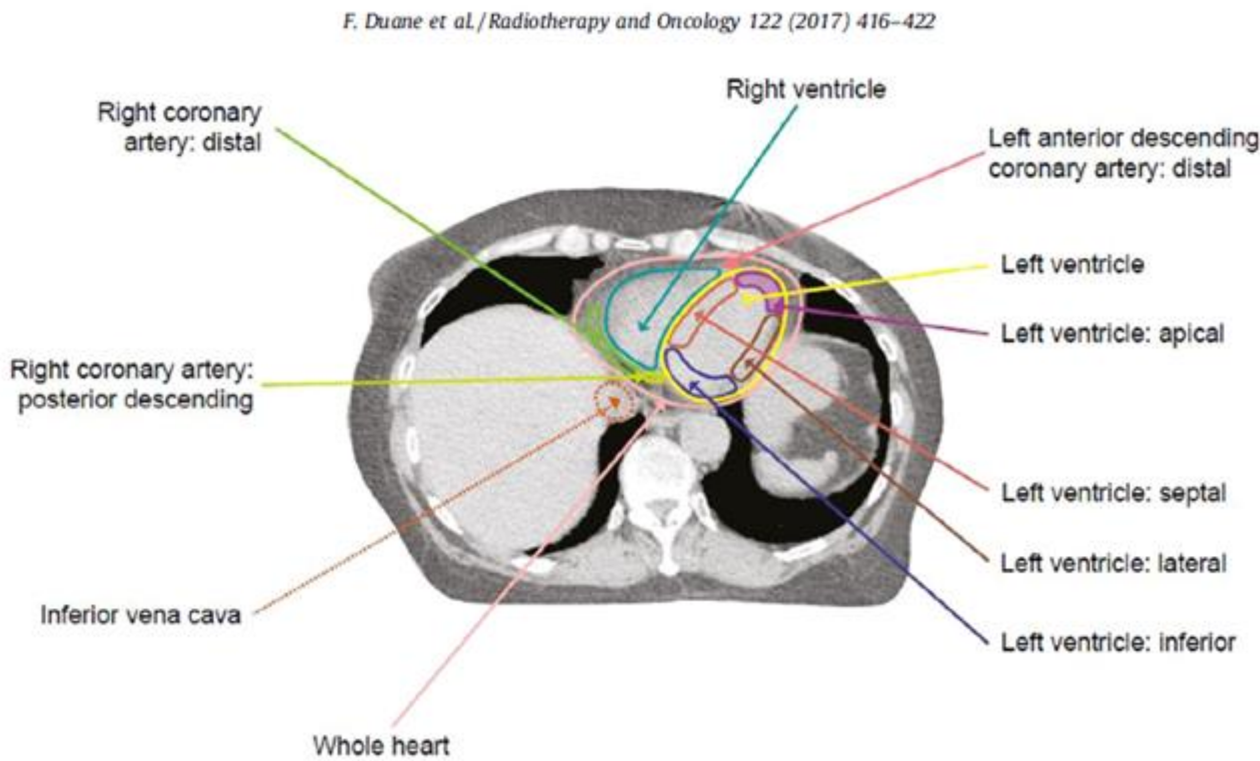
- Superiorly: Just inferior to the left pulmonary artery, include the great vessels in a rounded contour
- Inferiorly: to diaphragm, include pericardium
- If contrast is used, contour SVC separately

What Do the Experts Say? – *Heart (Substructures)*

2017 Atlas in Green Journal

- Whole heart dose may not be the best predictor for the different types of radiation induced cardiac toxicity

- Focus on left ventricle and coronary arteries



Dunane et al., 2017

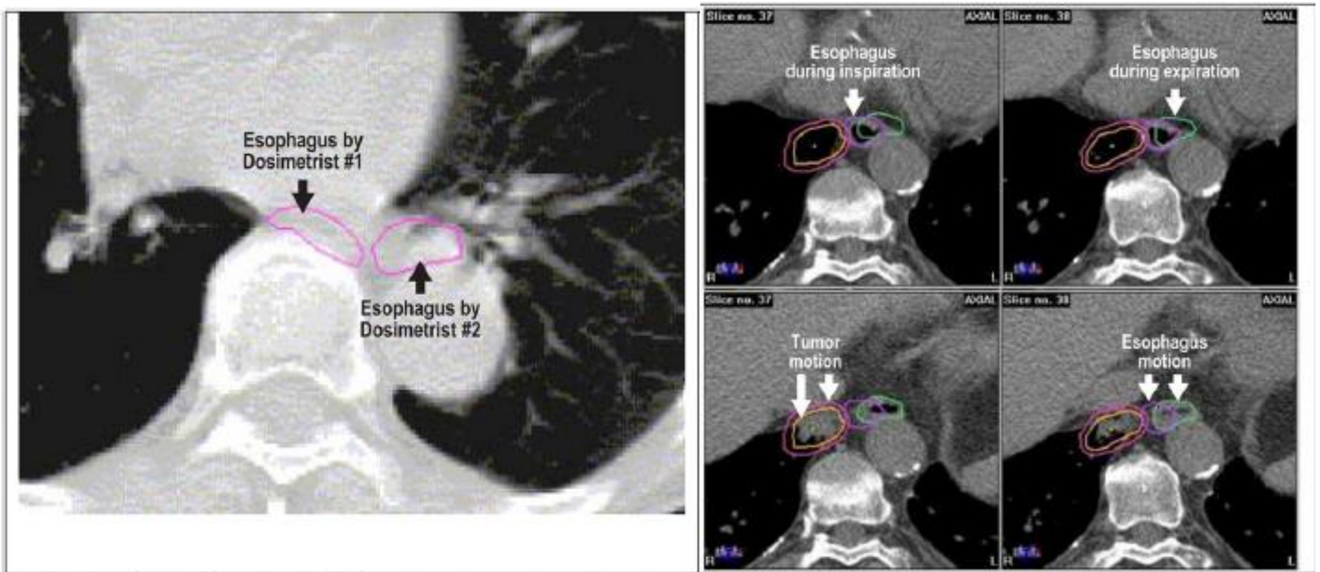
What Do the Experts Say? – ***Oesophagus***

Challenges

- Impact of windowing
- Impact of oral contrast
- Motion
- Inclusion of the muscular wall
- Length of contour

Recommendations

- Use mediastinal windowing level
- Contour from cricoid cartilage to gastro oesophageal junction
- Avoid oral contrast
  - Distorts shape and density



A: Esophagus Contour Variants
B: Esophagus Motion

What about clinical trials?

RADIATION THERAPY ONCOLOGY GROUP

RTOG 0529

A Phase II Evaluation of Dose-Painted IMRT in Combination with 5-Fluorouracil and Mitomycin-C for Reduction of Acute Morbidity in Carcinoma of the Anal Canal

Critical Normal Structures: In addition, surrounding critical normal structures, including the femoral heads (right and left), bladder, external genitalia, iliac crest, small bowel, large bowel outside the CTVs, and perianal skin should be outlined. The normal tissues will be contoured and considered as solid organs. The tissue within the skin surface and outside all other critical normal structures and PTVs is designated as unspecified tissue.

Critical normal structures: DVHs must be generated for all critical normal structures.
NOTE: Effort should be made to achieve the listed dose constraints to normal tissues below. Failure to meet the 6.5.1.1 and 6.5.1.2 dose constraints will result in minor deviation. The dose constraints are listed in order from most to least important.

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AGITG – For Anus

International Journal of Radiation Oncology biology • physics

www.redjournal.org

Clinical Investigation: Gastrointestinal Cancer

Australasian Gastrointestinal Trials Group (AGITG) Contouring Atlas and Planning Guidelines for Intensity-Modulated Radiotherapy in Anal Cancer

Michael Ng, M.B.B.S.(Hons), F.R.A.N.Z.C.R.,*
Trevor Leong, M.B.B.S., M.D., F.R.A.N.Z.C.R.,[†,||]
Sarat Chander, M.B.B.S., F.R.A.N.Z.C.R.,[†] Julie Chu, M.B.B.S., F.R.A.N.Z.C.R.,[†]
Andrew Kneebone, M.B.B.S., F.R.A.N.Z.C.R.,[‡,**]
Susan Carroll, M.B.B.S., F.R.A.N.Z.C.R.,[§,**] Kirsty Wiltshire, M.B.B.S., F.R.A.N.Z.C.R.,[†]
Samuel Ngan, M.B.B.S., F.R.C.S.Ed., F.R.A.N.Z.C.R.,[†,||] and Lisa Kachnic, M.D.[¶]

**Radiation Oncology Victoria, Victoria, Australia; [†]Department of Radiation Oncology, Peter MacCallum Cancer Centre, Victoria, Australia; [‡]Department of Radiation Oncology, Northern Sydney Cancer Centre, Royal North Shore Hospital, NSW, Australia; [§]Department of Radiation Oncology, Sydney Cancer Centre, Royal Prince Alfred Hospital, NSW, Australia; [¶]Department of Radiation Oncology, Boston Medical Center, Boston University School of Medicine, Boston, MA; [||]University of Melbourne, Australia; and **University of Sydney, Australia*

Received Jun 19, 2011, and in revised form Dec 13, 2011. Accepted for publication Dec 18, 2011

- Bladder
  - Entire outer wall
- Femoral Heads
  - Inferior – Cranial edge of the lesser trochanter
- Bowel
  - Small and large bowel
  - 15mm superior of PTV down to the rectosigmoid junction
- External Genitalia
  - Male – penis, scrotum, skin and fat anterior to the pubic symphysis
  - Female - clitoris, labia majora and minora, skin and fat anterior to pubic symphysis
- Bone Marrow
  - Iliac crests, both contoured and combined
  - Superior - top of the iliac crests
  - Inferior - superior part of the acetabulum

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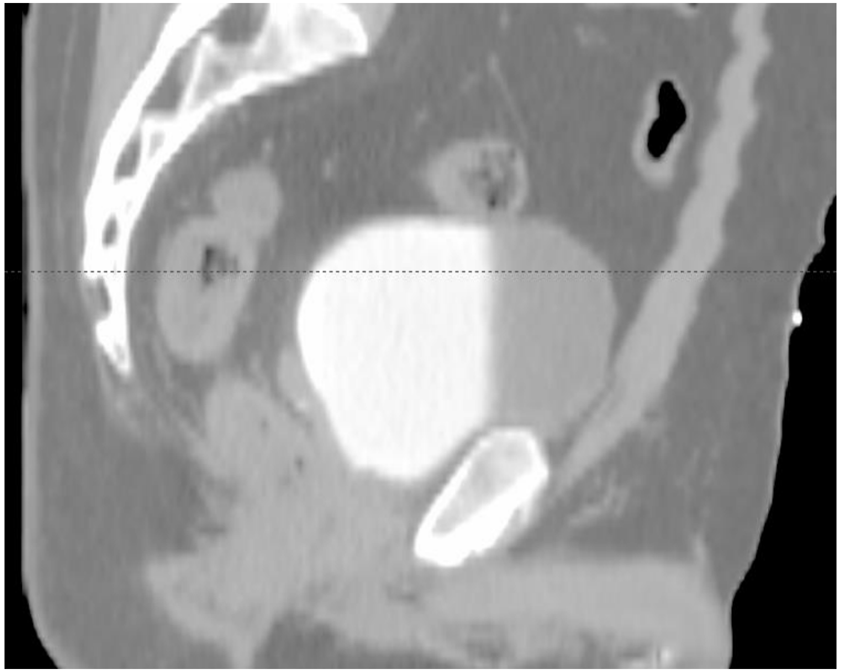
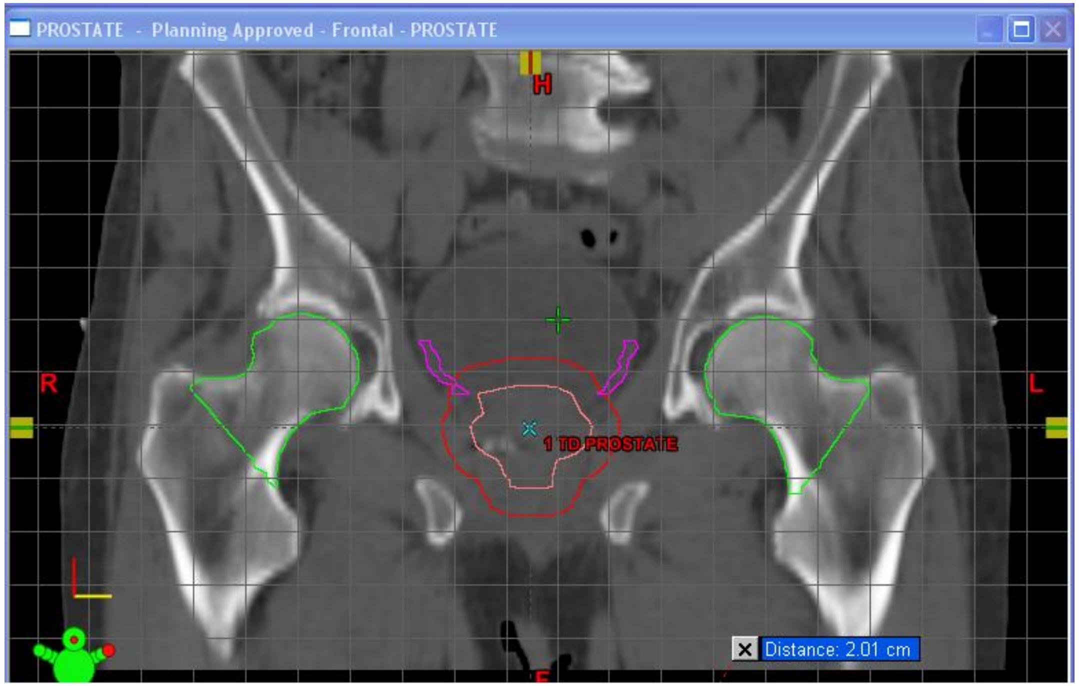
RAVES

- Femoral head:
  - ➢ Superior – acetabulum
  - ➢ Inferior – inferior edge of the treatment field
- Bladder:
  - ➢ Whole structure with bulk homogeneity correction for contrast
- Rectum:
  - ➢ Superior – rectosigmoid junction
  - ➢ Interior – 15mm inferior to the CTV



PROFIT Trial

- Rectal Wall
- Bladder Wall
- Femoral Head and Neck



Head and Neck

RADIATION THERAPY ONCOLOGY GROUP

RTOG 0615

A PHASE II STUDY OF CONCURRENT CHEMORADIOTHERAPY USING THREE-DIMENSIONAL CONFORMAL RADIOTHERAPY (3D-CRT) or INTENSITY-MODULATED RADIATION THERAPY (IMRT) + BEVACIZUMAB (BV) FOR LOCALLY OR REGIONALLY ADVANCED NASOPHARYNGEAL CANCER

NCI-supplied agent: Bevacizumab (NSC 704865; IND 79211)

A lot of contouring!

Critical Normal Structures

Surrounding critical normal structures, including the brainstem, spinal cord, optic nerves, chiasm, parotid glands, pituitary, temporo-mandibular (T-M) joints and middle and inner ears, skin (in the region of the target volumes), oral cavity, mandible, eyes, lens, temporal lobes, brachial plexus, esophagus (including postcricoid pharynx) and glottic larynx should be outlined.

Critical structures are ***critical***!

Planning Priorities

Critical normal structure constraints followed by the prescription goals are the most important planning priorities. The priorities in addressing the protocol aims and constraints will be in the following order:

1) Critical Normal Structure Constraints (Section 6.5);
2) Dose Specifications (Section 6.1);
3) Planning Goals: Salivary glands (Section 6.5.3);
4) Planning Goals: Other normal structures (Section 6.5.3).

Head and Neck

- RTOG Atlases for H&N do not cover OARs!!!

- Where to turn to?
  - Published literature
  - Expert consensus

Head and Neck

Radiotherapy and Oncology 117 (2015) 83–90

Contents lists available at ScienceDirect

Radiotherapy and Oncology

journal homepage: www.thegreenjournal.com

Head and neck guidelines

CT-based delineation of organs at risk in the head and neck region: DAHANCA, EORTC, GORTEC, HKNPCSG, NCIC CTG, NCRI, NRG Oncology and TROG consensus guidelines

CrossMark

Charlotte L. Brouwer [a,*,1], Roel J.H.M. Steenbakkers [a,1], Jean Bourhis [b], Wilfried Budach [c], Cai Grau [d], Vincent Grégoire [e], Marcel van Herk [f], Anne Lee [g], Philippe Maingon [h], Chris Nutting [i], Brian O'Sullivan [j], Sandro V. Porceddu [k], David I. Rosenthal [l], Nanna M. Sijtsema [a], Johannes A. Langendijk [a]

Consensus panel of Radiation Oncologists from Europe, North America, Asia and Australia

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Head and Neck

- Don't worry – even the "experts" have significant inter-observer variability

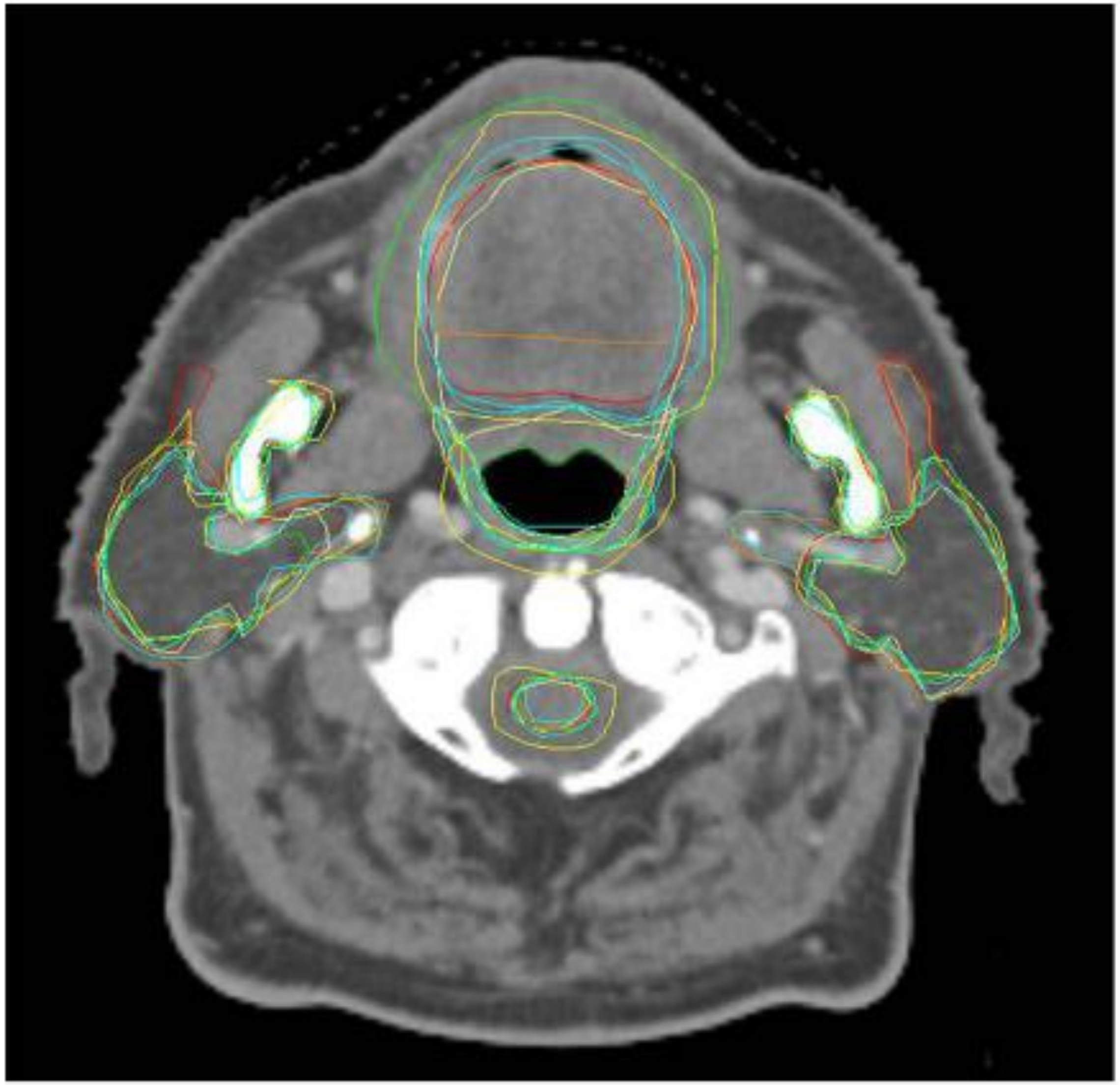


Fig. 1. Delineation results of 7 members of the panel for the parotid glands, spinal cord, pharyngeal constrictor muscles and the oral cavity, projected on an axial CT slice.

Head and Neck

- But still worth a read!
- Text and table description of anatomy with multimodality images to show

Supraglottic larynx

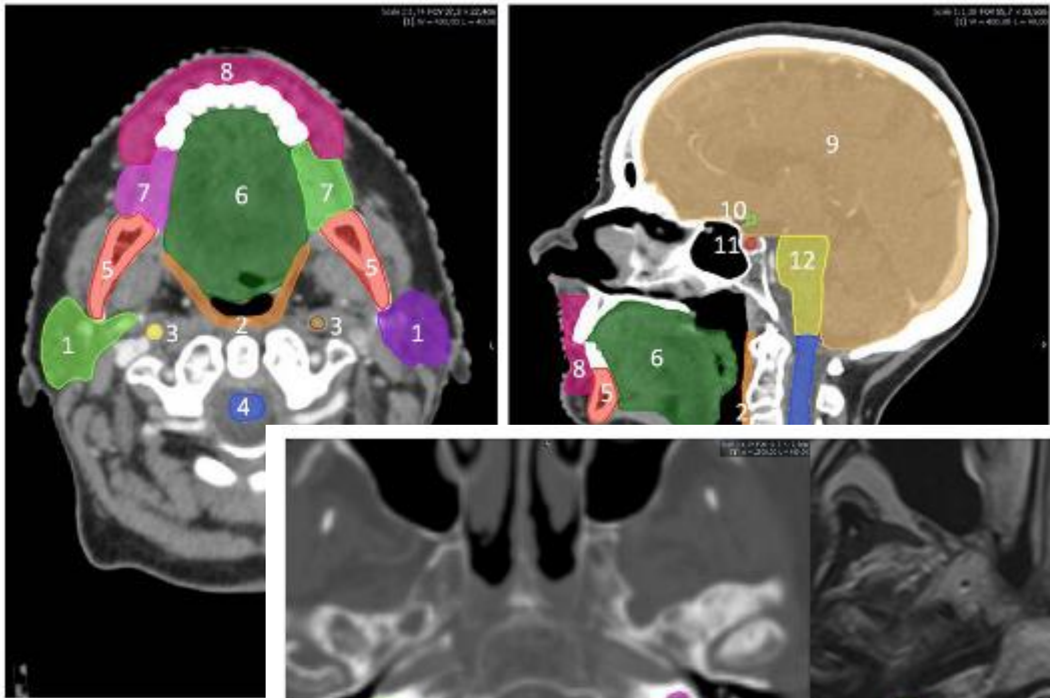
The supraglottic larynx is delineated according to Christianen et al. [7]. Anatomic borders are listed in Table 1. An axial slice of the supraglottic larynx is depicted in Fig. 4a.

Glottic area

We decided to define the glottic area structure, including the vocal cords and paraglottic fat. Air should be excluded from the contour. Cranial, caudal and posterior borders can be found in Table 1. An axial slice of the glottic area is depicted in Fig. 4b.

Arytenoids

The arytenoids (or arytenoids cartilage) are defined as a separate structure. The base (caudal edge) of each arytenoid is broad for articulation with the cricoid cartilage. The apex (cranial edge) is pointed.



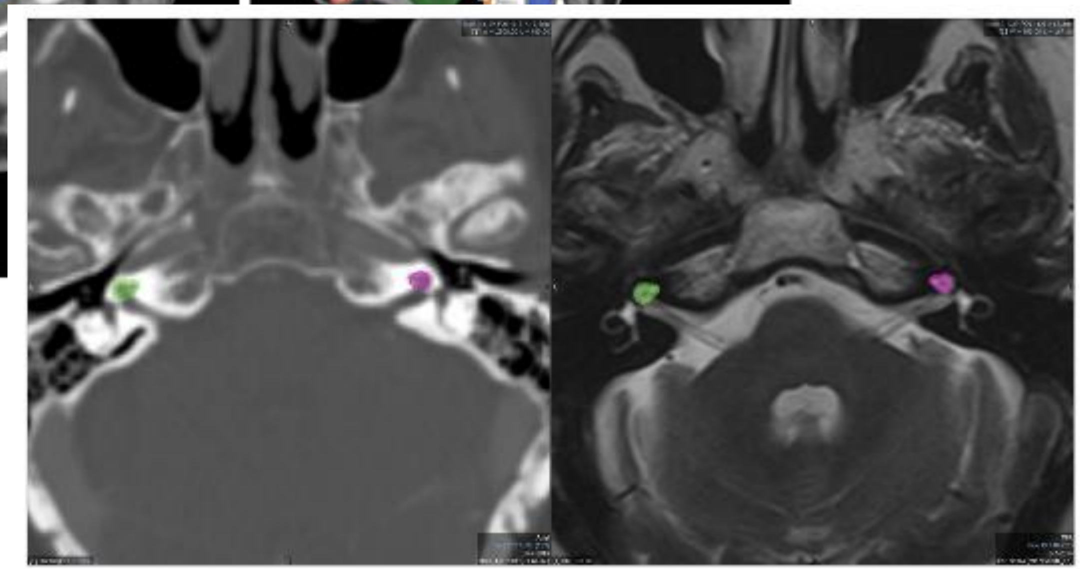
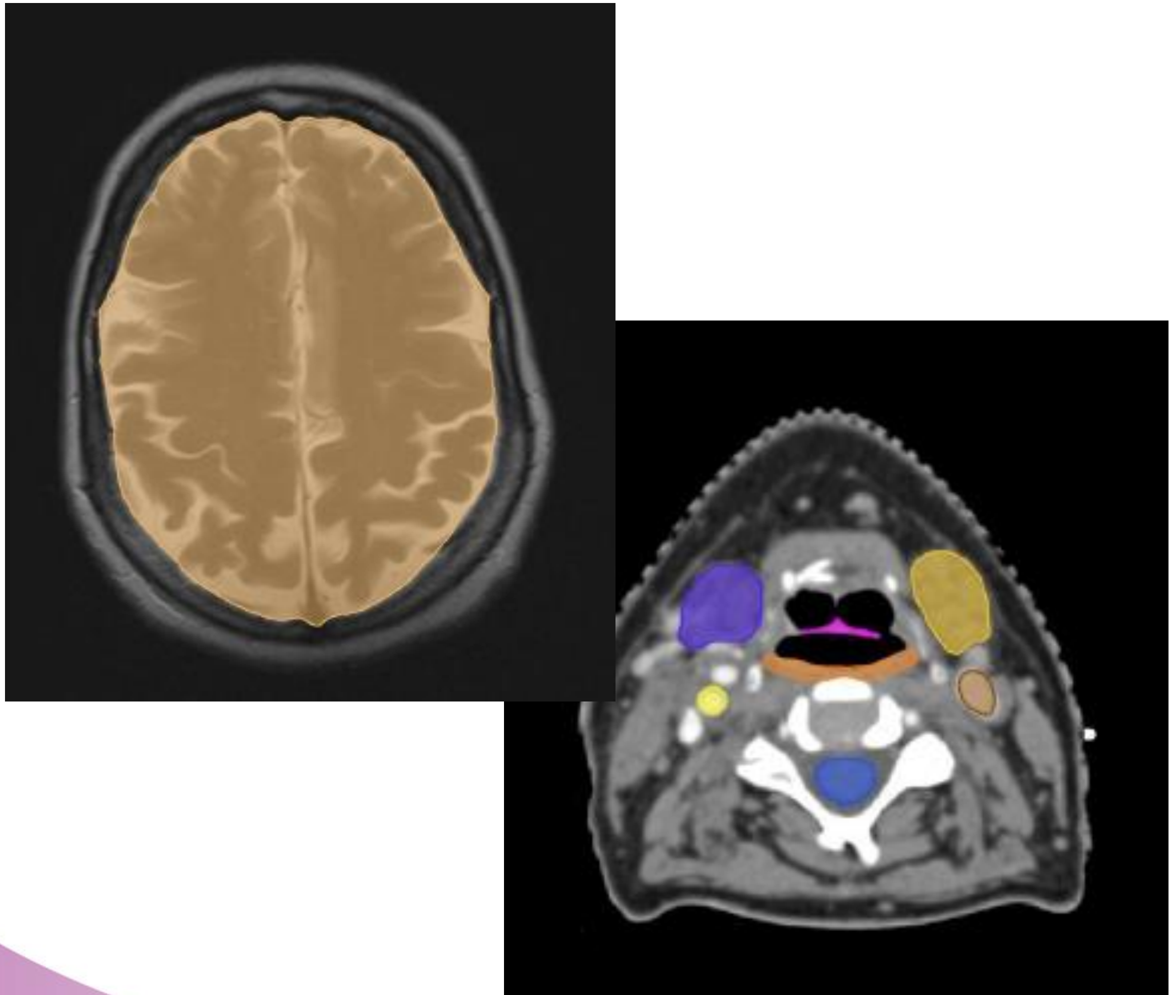


Fig. 2. Delineation of the cochlea in CT bone settings (left), matched to MRI-T2 (right).

Head and Neck

- Thank you – they have an atlas published as supplementary material



Head and Neck

Radiation Oncology, Head and Neck, Organs at Risk (OAR)

ID: 001523 Approved:08 Aug 2013 Last Modified: 02 Oct 2013 Review Due:08 Se

Head and Neck Organs At Risk (OAR)

- Doses listed in the table below are based on radiation doses of 2Gy per fraction

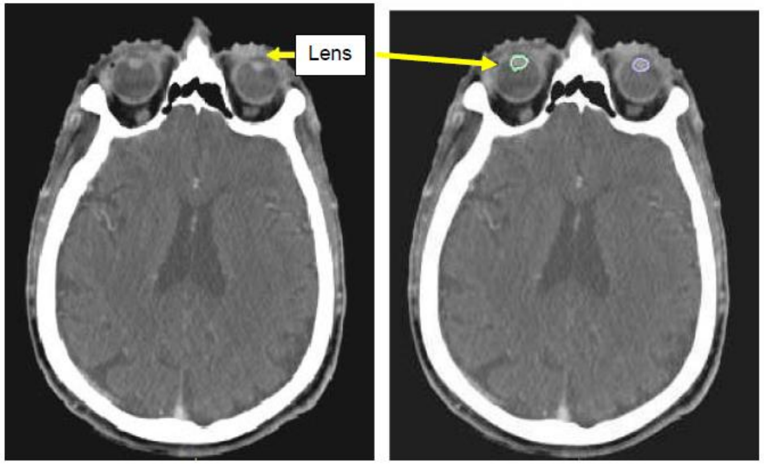
OAR Structure	Description based on RTOG 0920	True structure constraint (ideal)	Notes (Aim to keep doses as low as possible)
Brainstem	The inferior most portion of the brainstem is at the cranial-cervical junction where it meets the spinal cord. The superior most portion of the brainstem is approximately at the level of the top of the posterior clinoid. The brainstem shall be defined based on the treatment planning CT scan.	▪ Max dose ≤ 54Gy	Additional goals may include: ▪ ≤ 1% of PRV to exceed 60Gy ▪ small volumes (1-10cc) max dose ≤ 59Gy for fraction doses ≤ 2Gy [1]
Optic nerves		▪ Max dose ≤ 50Gy	Additional goals may include: ▪ ≤ 1% of PRV to exceed 60Gy ▪ To keep the risk of radiation induced optic neuropathy (RION) ≤ 3-7%, max dose 55-60Gy ▪ The risk of RION increases to 7-20% for doses > 60Gy in 1.8-2Gy fractions [2]
Optic Chiasm		▪ Max dose ≤ 54Gy	Additional goals may include: ▪ ≤ 1% of PRV to exceed 60Gy ▪ To keep risk of radiation induced optic neuropathy (RION) < 3-7%, max dose 55-60Gy ▪ The risk of RION increase to 7-20% for doses > 60Gy in 1.8-2Gy fractions [2]

Available from www.eviq.org.au

eviQ Head and Neck Critical Structures Atlas

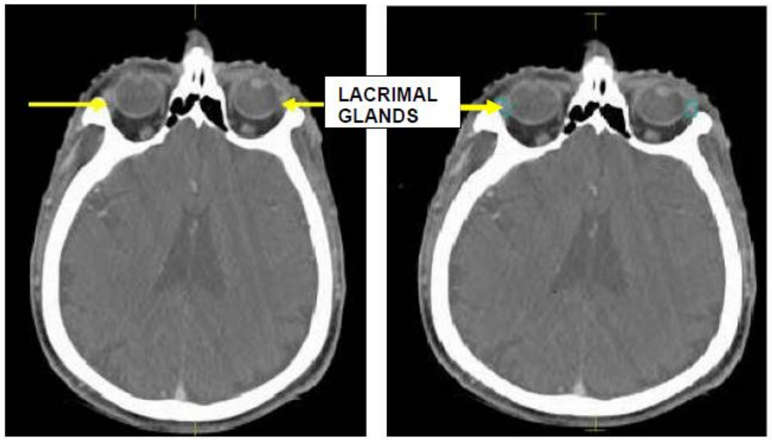
LENSES

Description: The lens is an anterior structure 5-8mm in length
Window level: W600/L40
Typical tolerance dose: 5Gy maximum



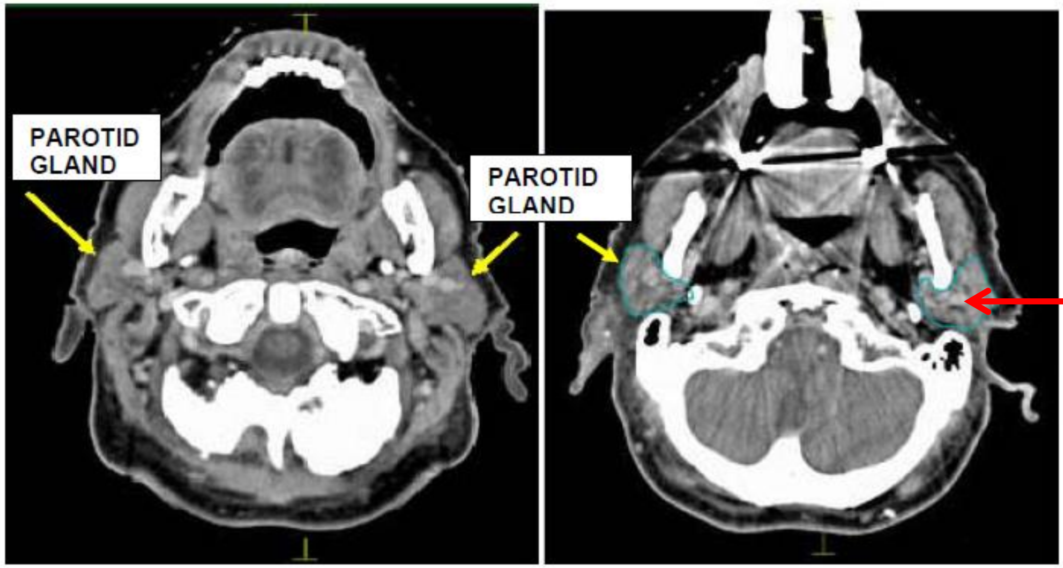
LACRIMAL GLAND

Location: Bilateral structure located supero-laterally to the orbits.
Length: Contoured extends approximately 10-15mm
Scroll through the images first to distinguish between muscle and the gland itself.
Window level: use approximately W270/L40 or W500/L60.
Typical Tolerance dose: <40Gy



- Shows adjacent images with and without contour
- Provides anatomical location, description, suggested window level and tolerance dose

eviQ Head and Neck Critical Structures Atlas



Note: degradation of image quality due to dental artefact

PAROTID GLAND

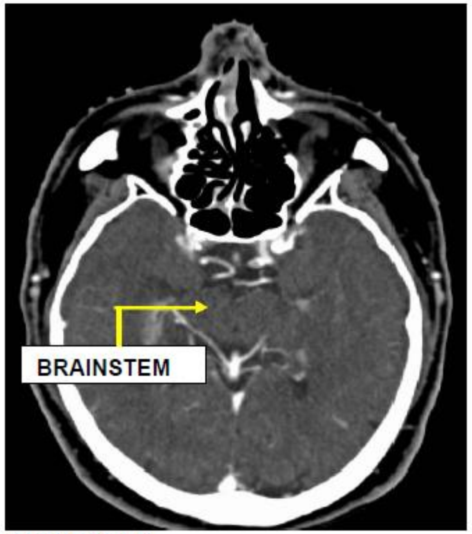
Location: The parotid gland is a bilateral glandular tissue lying anterior to the ear between the masseter muscle and the skin. It lies inferior to the zygomatic arch beneath the skin that covers the lateral and posterior surface of the mandible.
Length: approximately 50-60mm.
Borders: Medial Border is at the styloid process. Anteriorly hooks around the posterior aspect of anterior ramus of mandible.
Window level: use approximate window levels W290/L40 or W400/L80.
Typical tolerance doses: Mean parotid dose <26Gy (in at least one gland) or at least 50 % of one gland should receive <30Gy mean. (Doses to the parotid should be kept as low as reasonably achievable)

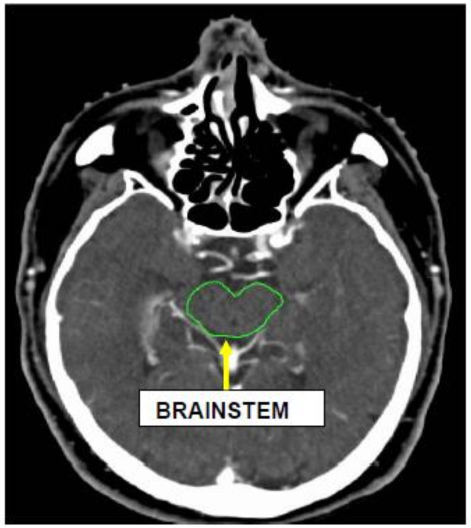
eviQ Head and Neck Critical Structures Atlas

BRAINSTEM

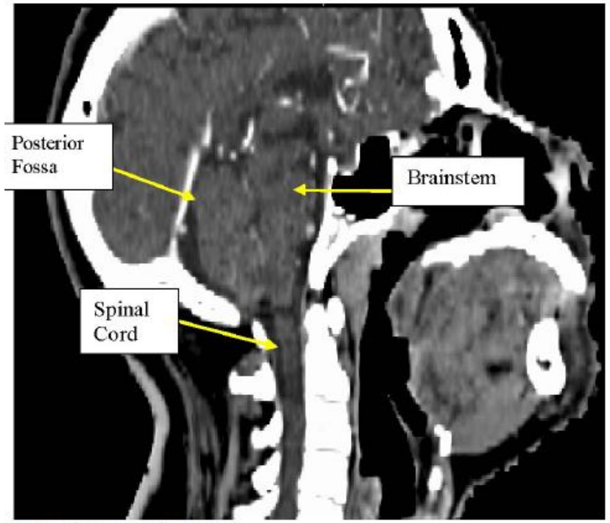
Location: Superior to as well as a continuous structure from the proximal spinal cord, the brain stem is characterised by a sudden increase in width compared to the spinal cord above the level of the foramen magnum. The brain stem sits inferior to the optic chiasm. The brainstem is composed of the medulla, the pons and midbrain. It lies posterior to the bony clivus. Use sagittal view for ant/post definition; inferiorly it may be over contoured as spinal cord, due to tighter dose constraints.
Window level: Approximate window level of W200/L80.
Typical tolerance doses: <54Gy maximum.

Remember to view structures in all planes





Superior level



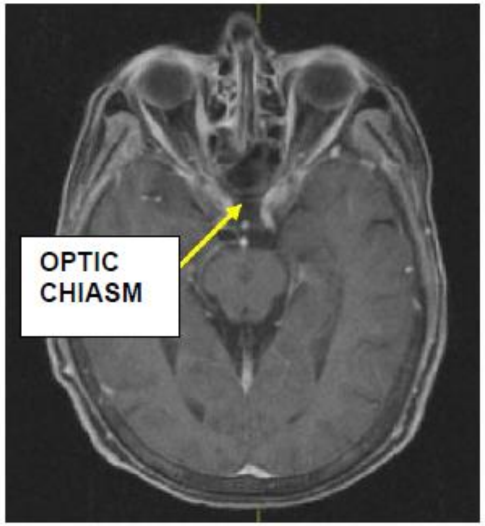
Brainstem sagittal view

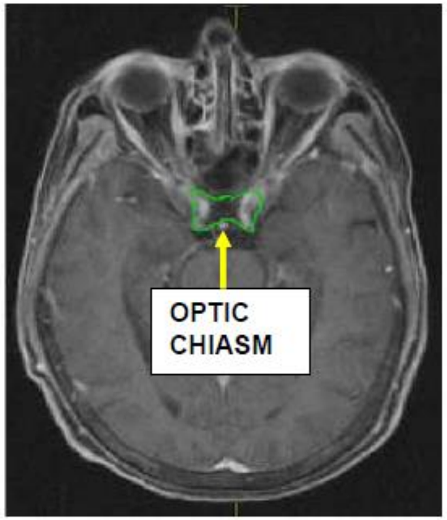
Note: It is important to avoid a gap between the brainstem and spinal cord contours as the emetic centre which controls nausea is located in this space. To avoid dose dumping in this region it is advised to overlap the contours by 1 CT slice to avoid a gap between these structures. (Monroe et al 2008 Radiother Oncol 87(2):188-194).

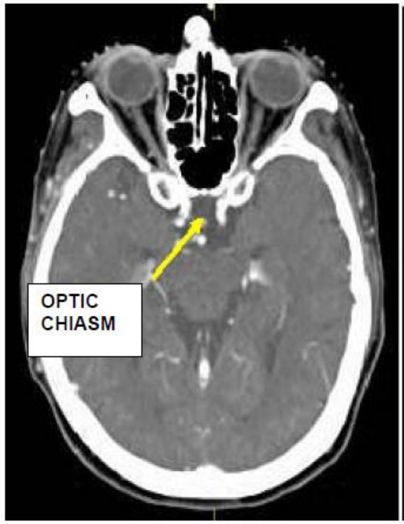
OPTIC CHIASM

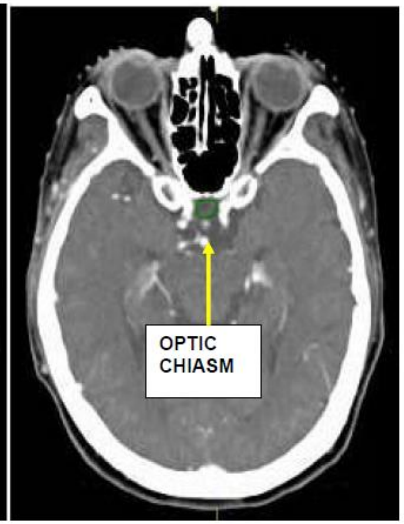
Location: A butterfly-shaped structure which sits directly above the pituitary fossa. To aid in contouring trace the optic nerves to the point of posterior intersection to help with identifying the optic chiasm.
Course: Anterior it begins directly posterior to the optic canal. Begin contouring at this position. At this area it lies medial to the carotid arteries (which enhance with contrast) but anterior to the pituitary stalk. The optic chiasm joins in front of the pituitary stalk and then divides again posteriorly to travel to the most superior/anterior part of the brainstem (ie gives position of the most superior limit of the brainstem). It should look butterfly shaped.
Length: Approximately 5-8mm, consider using an MRI study set if it is available for easier visualisation of the optic chiasm.
Window level: use approximate window level of W220/L70.
Typical Tolerance dose: Ideally <50Gy with a maximum of <54Gy

Remember to use all imaging available for that patient





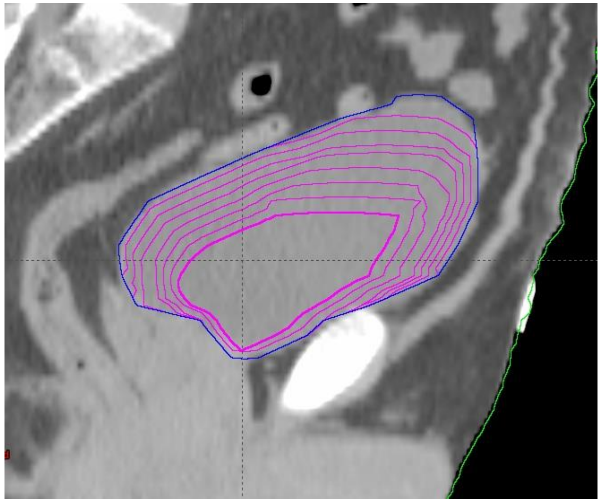




Other Points to Consider

- Planning Risk Volume
  - ➢ Margin added to true structure
  - ➢ ICRU 83
  - ➢ RTOG H&N Trials

- Additional structures to assist in decision making at the linac



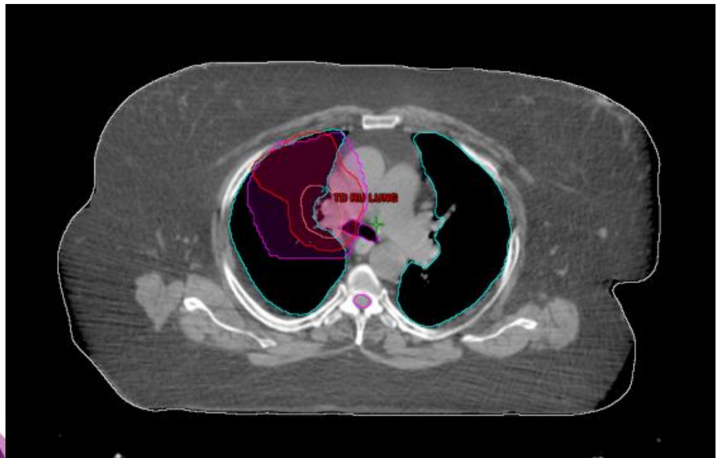
Moore and Forde, JMIRS 2017

Minimum allowable bladder volume

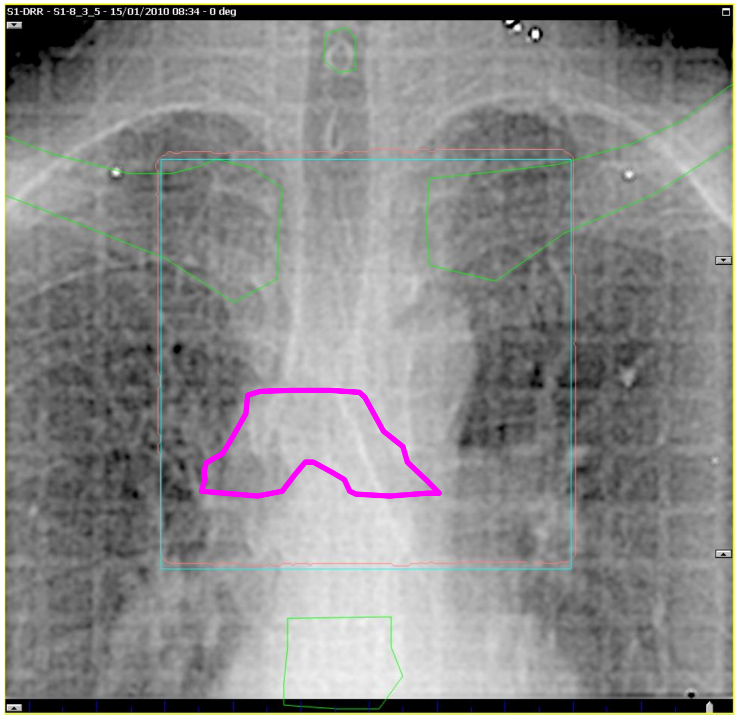
Other Structures for IGRT at the Linac

- What is the best surrogate for the target?
- What else can you see that might help you match?

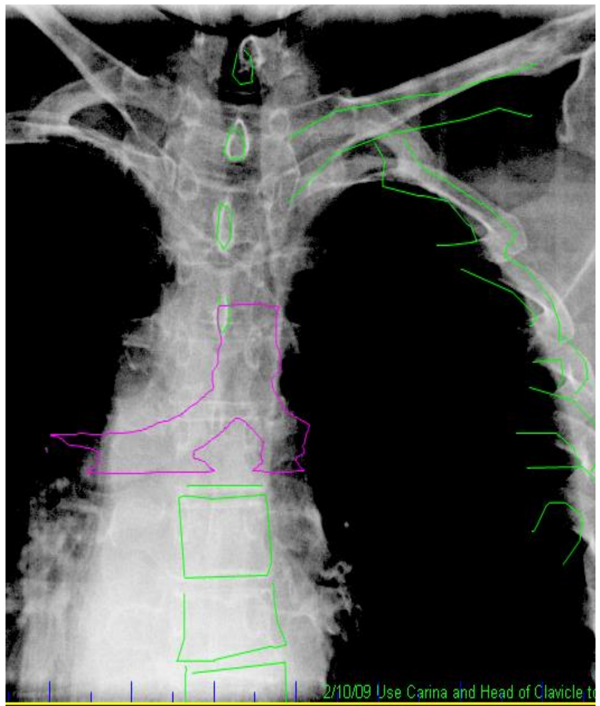
Planning CT



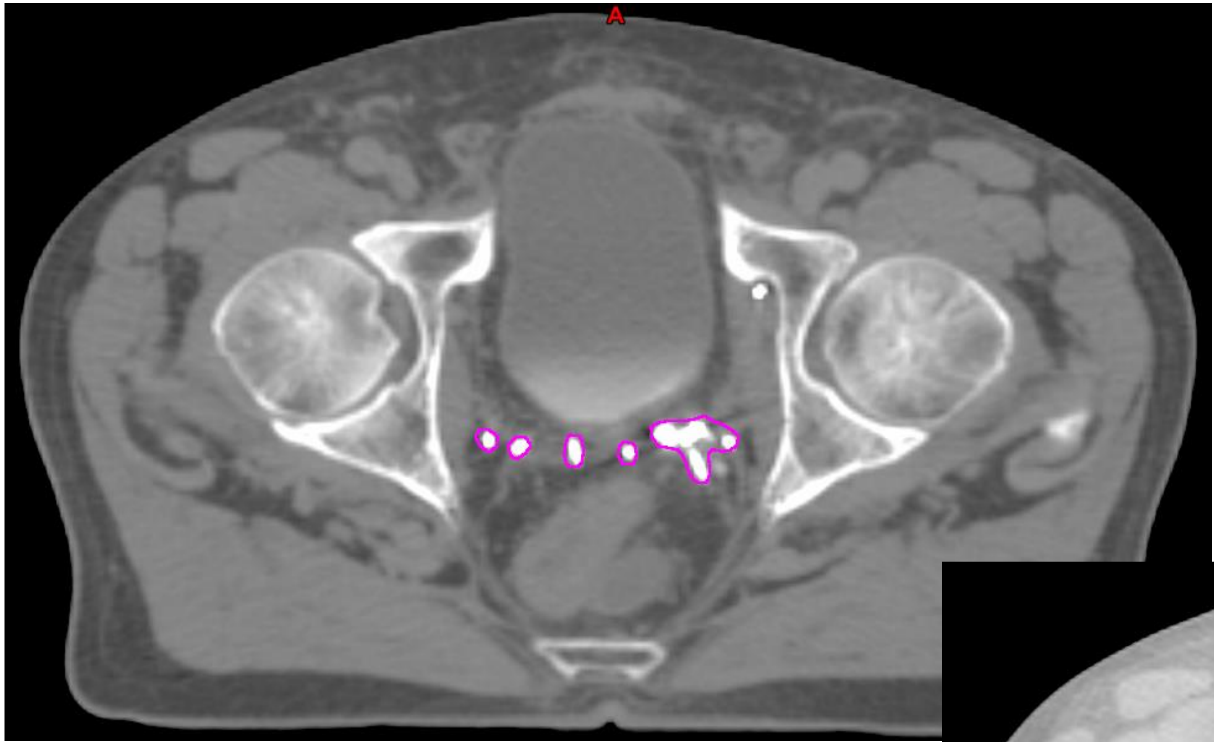
2D MV EPI

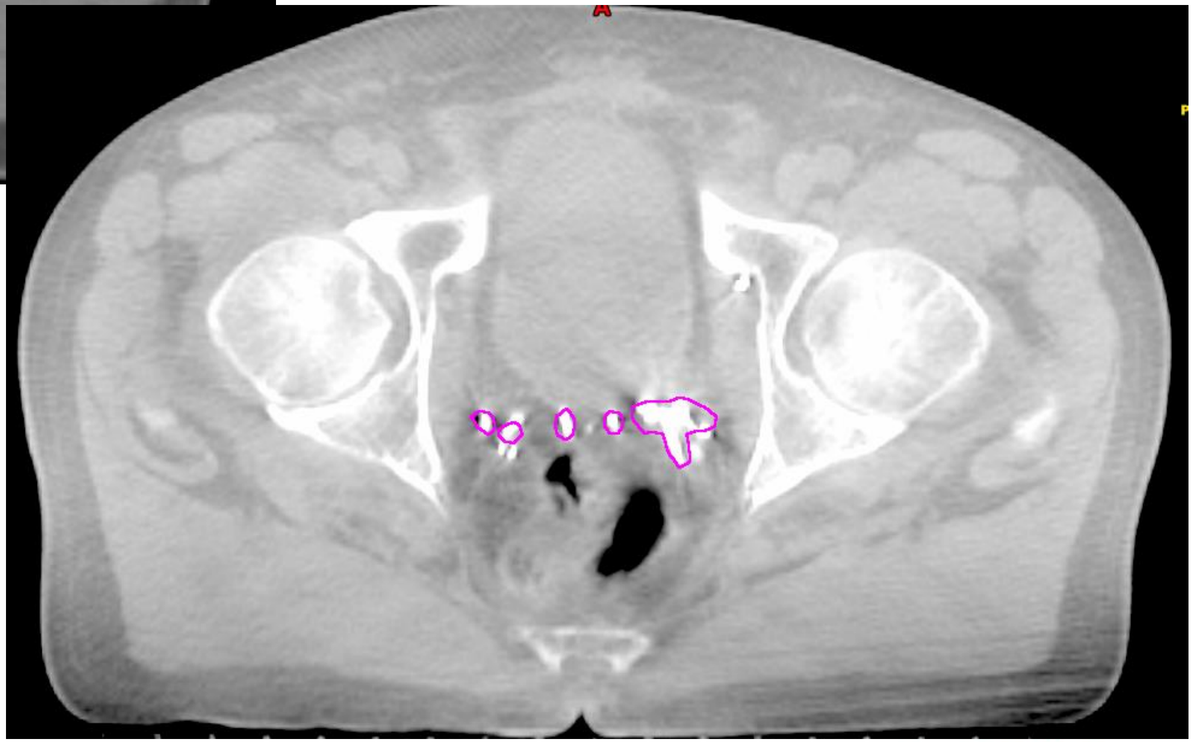


2D kV OBI



Other Structures for IGRT at the Linac





Take Home Message

- Quality assurance of organ delineation is vital regardless of who is responsible for OAR delineation
- "The accuracy of any autosegmenting tools should be carefully assessed" *(Marks et al., 2010)*
- Use all imaging modalities and viewing planes that you have available for that patient
- Think about the whole patient pathway
  - ➢ What will these contours impact on?
- Be consistent!
  - ➢ Preferably with international recommendations/consensus
  - ➢ At least at a local level

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"Inaccuracy and variation in defining critical volumes will affect everything downstream: treatment planning, dose–volume histogram analysis, and contour based visual guidance used in image-guided radiation therapy"

(Nelms et al., 2012)

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OAR delineation **workshop**

ESTRO School

Sofia Rivera, M.D.
Radiation Oncology Department
Gustave Roussy
Villejuif, France

GUSTAVE ROUSSY
CANCER CAMPUS GRAND PARIS

Advanced skills in modern radiotherapy
June 2017

WWW.ESTRO.ORG/SCHOOL

ESTRO VISION 2020

Every cancer patient in Europe will have access to state of the art radiation therapy, as part of a multidisciplinary approach where treatment is individualized for the specific patient's cancer, taking into account the patient's personal circumstances

Radiotherapy & Oncology 103(2012) 99-101

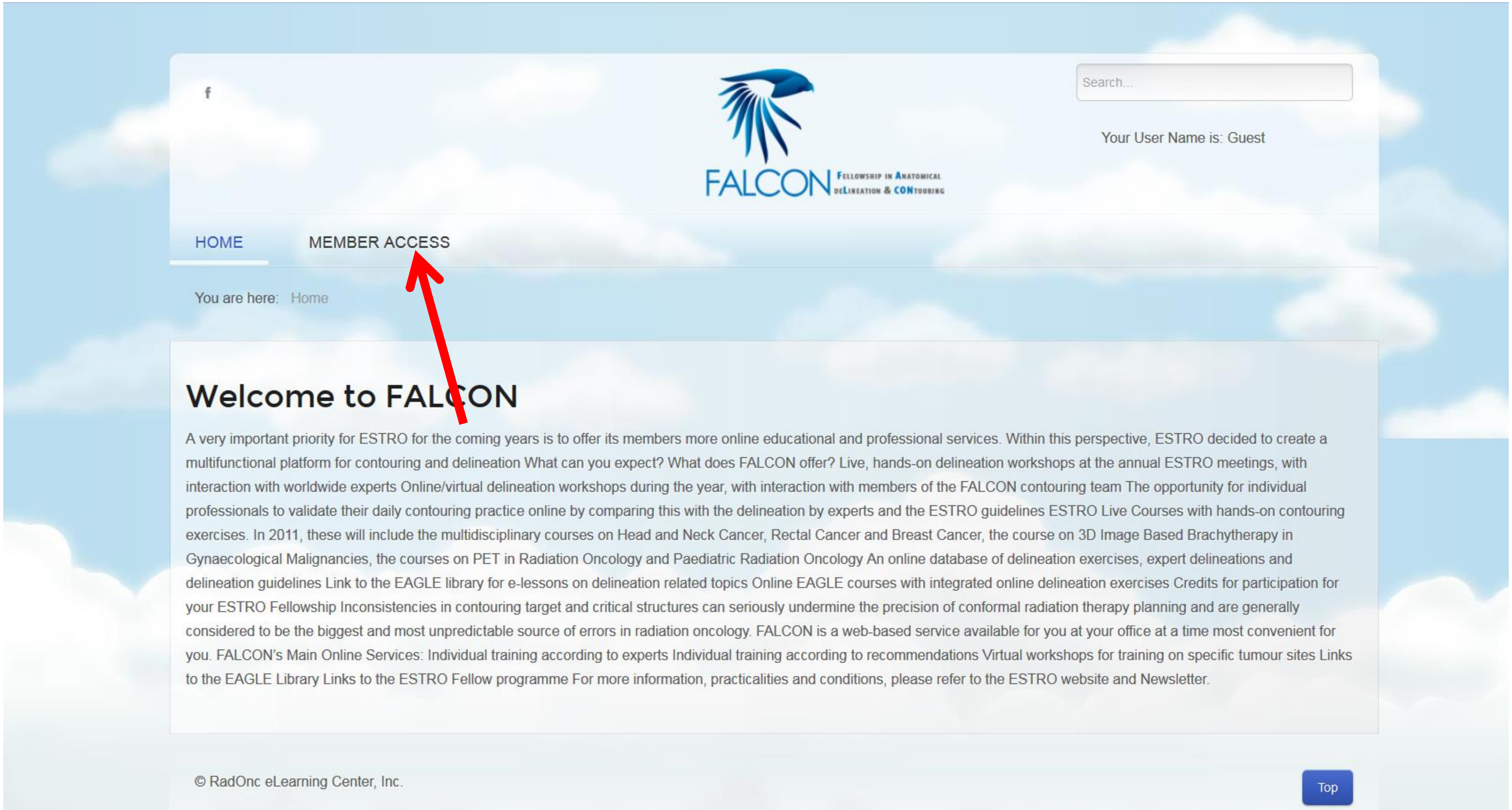
FALCON Vison

- Falcon provides valuable global educational training for radiotherapy professionals on delineation.
- It is a dynamic and evolving pedagogical programme that answers educational needs of current and future clinical practice using live, online and blended format.
- It facilitates and serves research projects and development of guidelines.
- It is fully integrated into the ESTRO School's programme and strategy.

FACON activities

- ESTRO courses
- On site Workshops
- Online Workshops
- Supporting guidelines
- Research projects
  - In pedagogics
  - In clinical research (Dummy run…)

How to use FALCON?



Go to **http://estro.educase.com/**
Login with your user name and password

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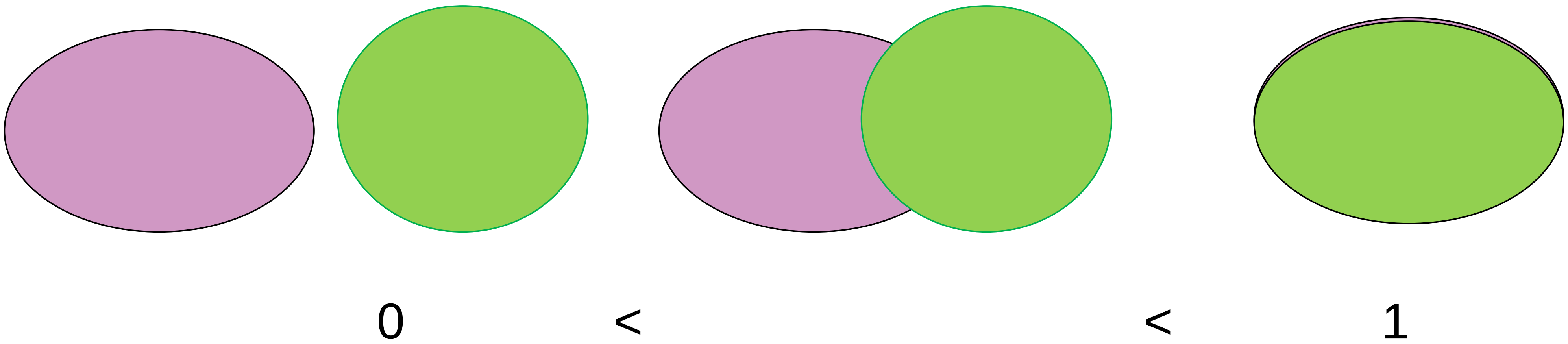
Homework results

- 29 participants over 34 did their homework

- DICE index: $$QS = \frac{2|X \cap Y|}{|X| + |Y|}$$



- Excellent results with DICE index : 0,7 to 0,89!
  - ➢ CONGRATULATIONS!!!!

So let’s use it again!!!

- OAR contouring in the thoracic region:
  - Spinal canal
  - Lung
  - Heart
  - Esophagus

Ready to improve your contours?

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Image registration

Mirjana Josipovic

Dept. of Oncology, Rigshospitalet
Niels Bohr Institute, Uni. of Copenhagen
Denmark

Peter Remeijer

NKI-AVL
Amsterdam
The Netherlands

Advanced skills in modern radiotherapy
June 2017

Intended learning outcomes

- Describe basic principles of image registration process

- Identify limitations in image registration process

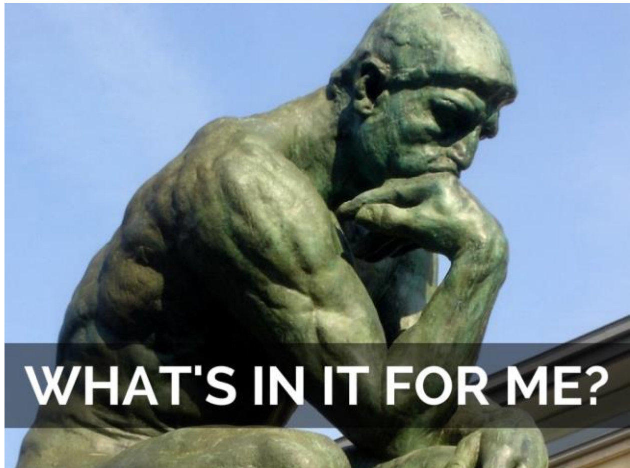


Image registration

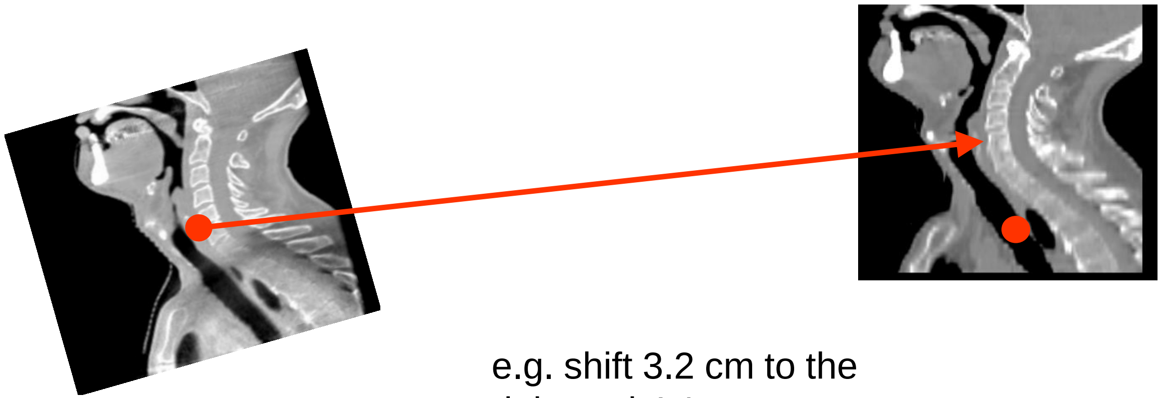
You may also call it

- Image fusion
- Image matching
- Image warping

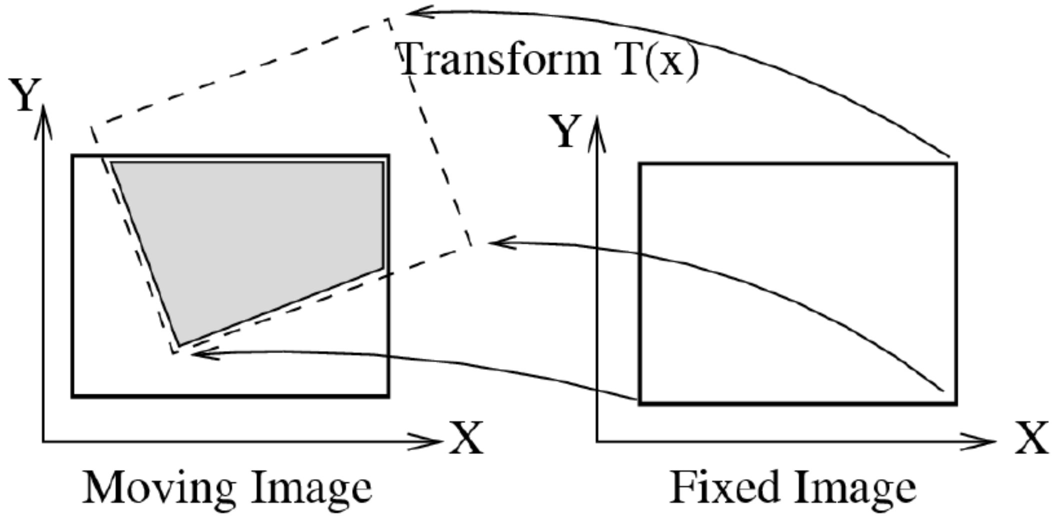
= process of aligning two (or more) images

Definition: Image registration

- Determine **rigid transformation** between two scans

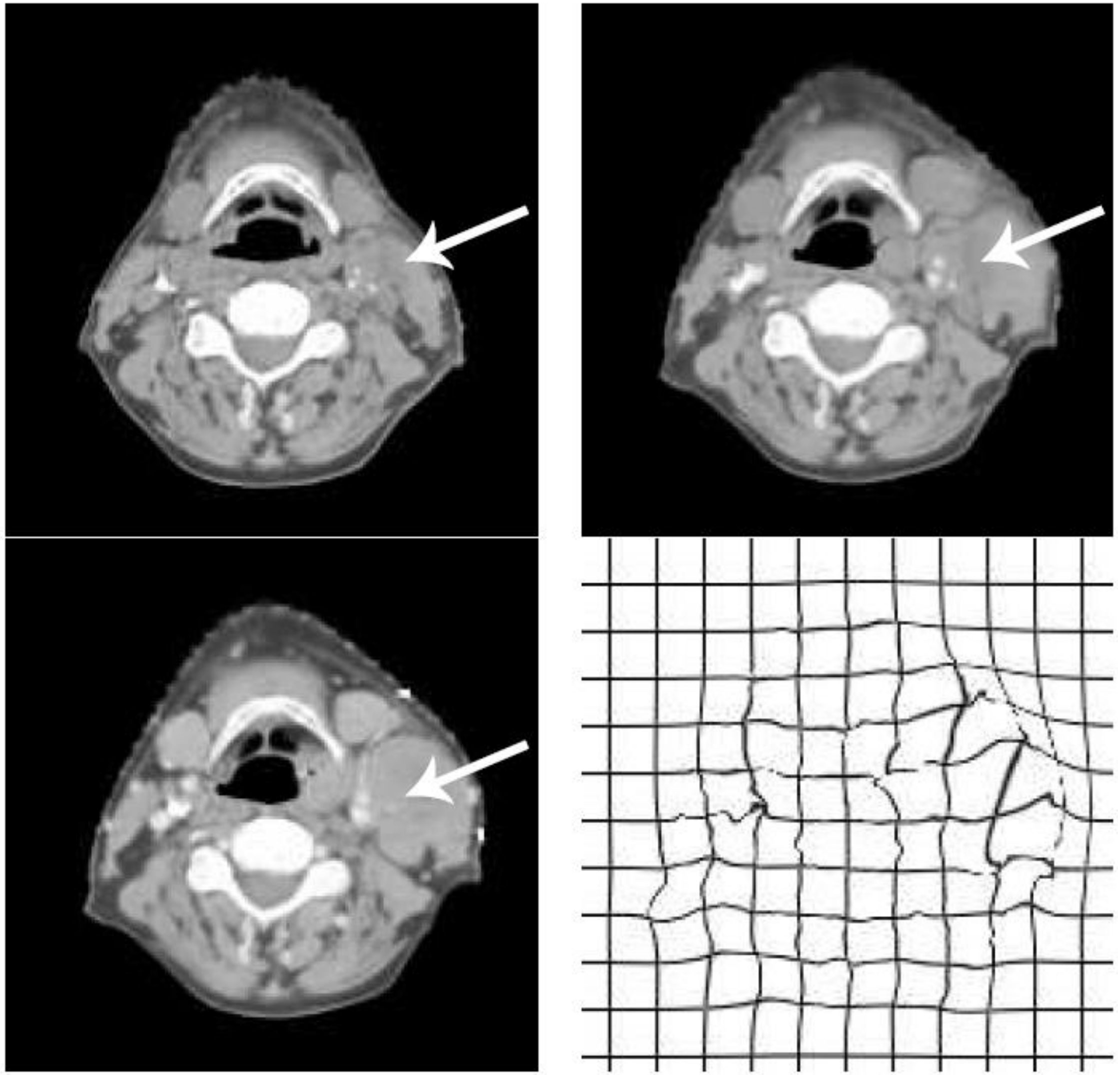


e.g. shift 3.2 cm to the right and 4.1 cm up and rotate



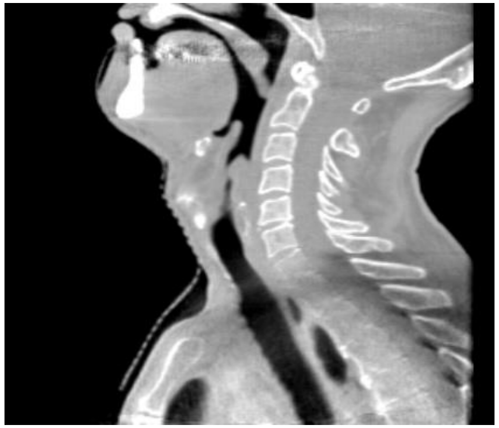
Definition: Image registration

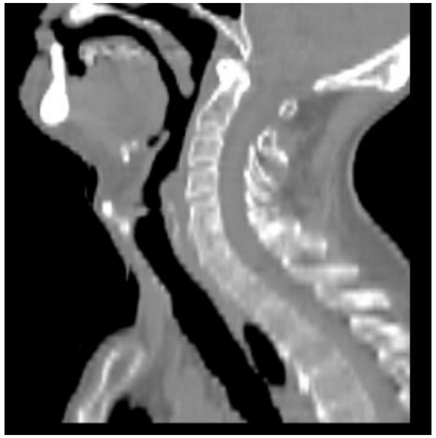
- Determine **deformable transformation** between two scans

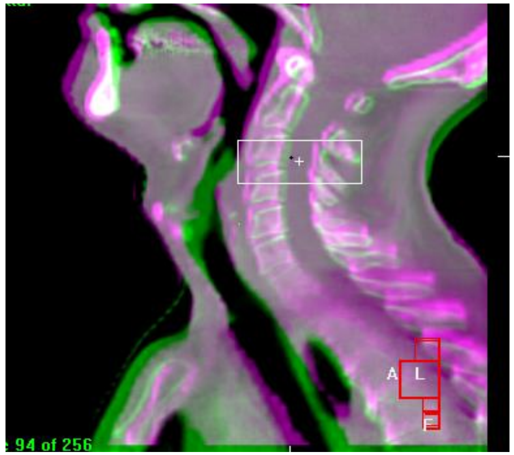


Definition: Image fusion

- Combine the information of two images







- **Viewing and validation** of registration result

Image registration in radiotherapy

- In the RT planning process
  - ➢ Inclusion of PET/MRI
  - ➢ Pre-chemo CT scans
- During RT delivery - IGRT
  - ➢ Reduction of setup uncertainty
  - ➢ Detect patient anatomy changes during treatment
    - ▪ Daily dose assesement / plan adaptation
- After RT
  - ➢ Follow up (tumour response, normal tissue damage)
  - ➢ Re-irraditaion

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Image registration in radiotherapy

- Algorithms
- Validation
- Challenges

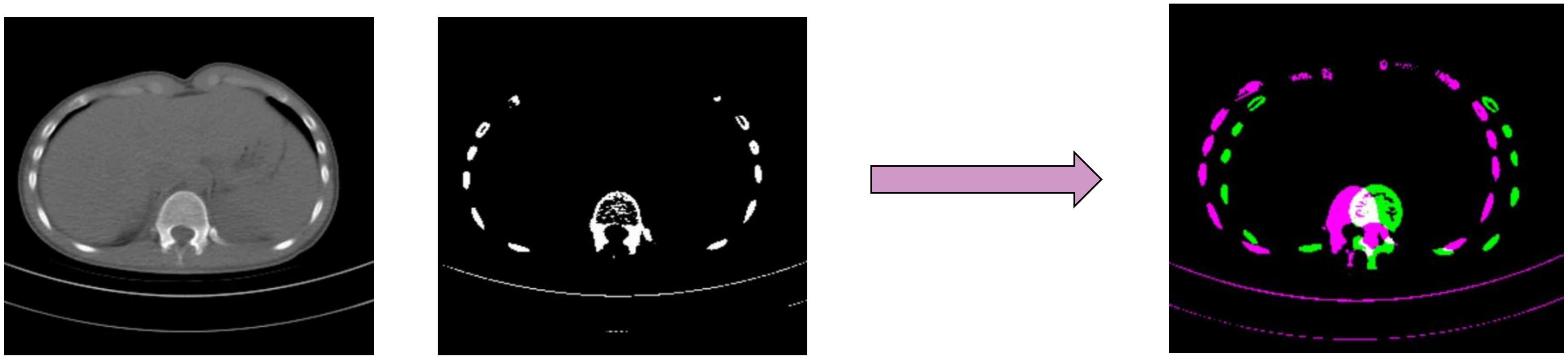
Manual image registration

- Simple ‘algorithm’
- Good for gross alignment

- Difficult in 3-D
- Not very precise

Automatic image registration

- Geometry based
  - ➢ Point matching (anatomic landmarks, implanted fiducial markers)
  - ➢ Surface matching (skull surface, pelvic bones)
    - ▪ Fx Chamfer matching



Automatic image registration

- Feature based
  - ➢ Numerical gray scale

- Uses gray values in all pixel values
  - ➢ Inside the regions of interest

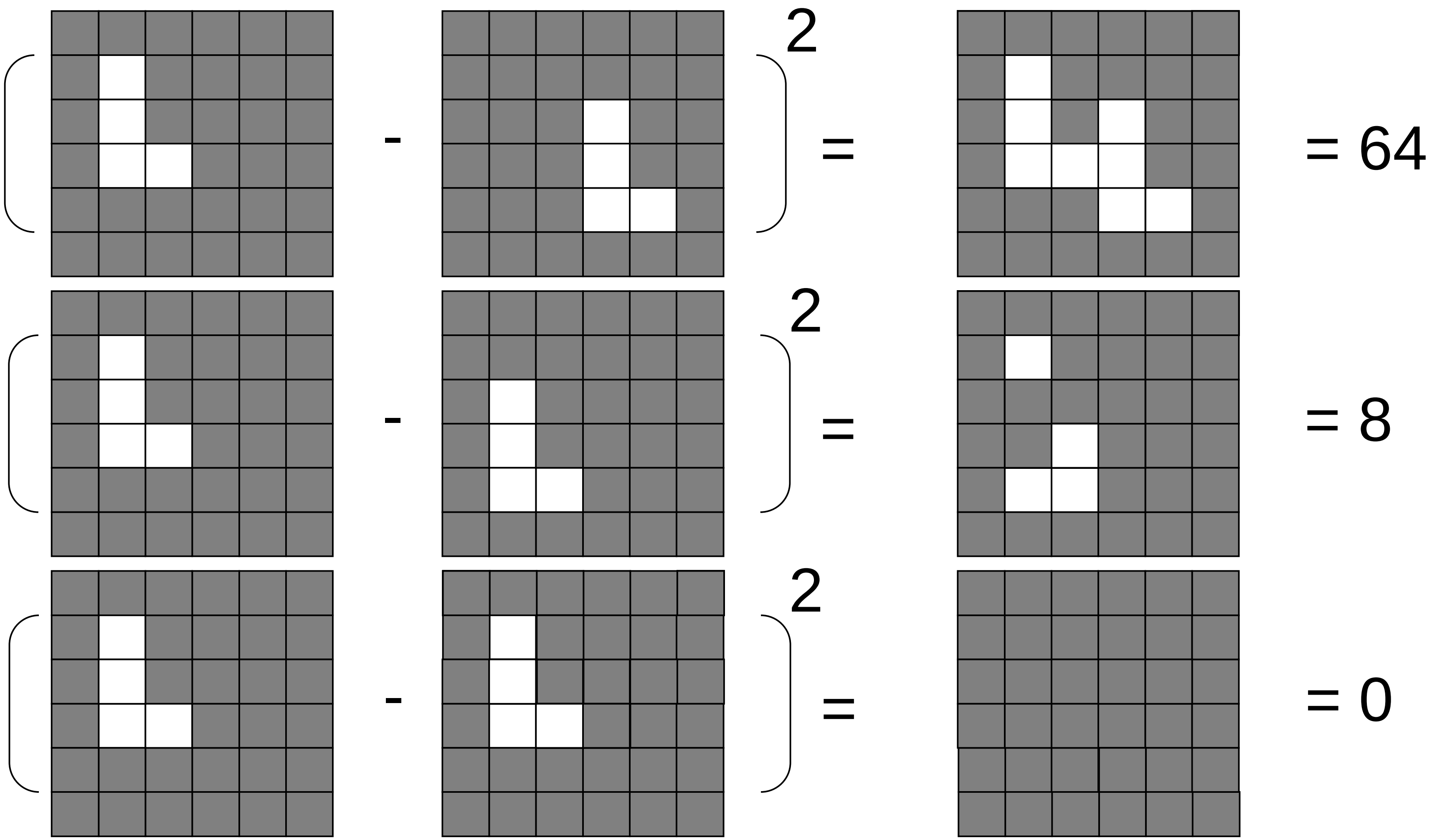
- Slower than chamfer matching
  - ➢ not really an issue today due to more computing power ☺

Similarity assessment

- How good is the resulting image registration?

- Similarity metrics / cost functions
  - Root mean square
  - Correlation ratio
  - Mutual information
  - …

Grey value registration example



Mutual information cost function

Understand your registration algorithm

- You see:

The computer sees:

$$R = \begin{bmatrix} \cos\theta_z & -\sin\theta_z & 0 \\ \sin\theta_z & \cos\theta_z & 0 \\ 0 & 0 & 1 \end{bmatrix} \begin{bmatrix} \cos\theta_y & 0 & \sin\theta_y \\ 0 & 1 & 0 \\ -\sin\theta_y & 0 & \cos\theta_y \end{bmatrix} \begin{bmatrix} 1 & 0 & 0 \\ 0 & \cos\theta_x & -\sin\theta_x \\ 0 & \sin\theta_x & \cos\theta_x \end{bmatrix}$$

$$= \begin{bmatrix} \cos\theta_y\cos\theta_z & -\cos\theta_x\sin\theta_z + \sin\theta_x\sin\theta_y\cos\theta_z & \sin\theta_x\sin\theta_z + \cos\theta_x\sin\theta_y\cos\theta_z \\ \cos\theta_y\sin\theta_z & \cos\theta_x\cos\theta_z + \sin\theta_x\sin\theta_y\sin\theta_z & -\sin\theta_x\cos\theta_z + \cos\theta_x\sin\theta_y\sin\theta_z \\ -\sin\theta_y & \sin\theta_x\cos\theta_y & \cos\theta_x\cos\theta_y \end{bmatrix}$$

Specify how the algorithm should handle image registration:

- Define region of interest
- Choose the appropriate algorithm

Check the result!

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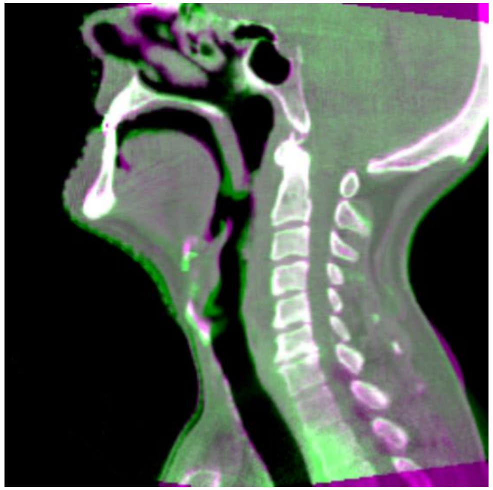
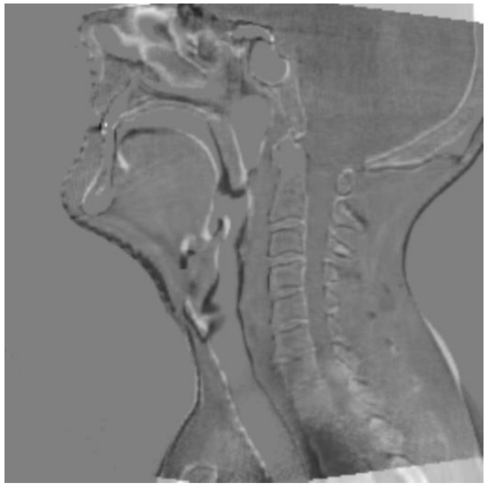
Image fusion

- Viewing & validation of the image registration



Overlay

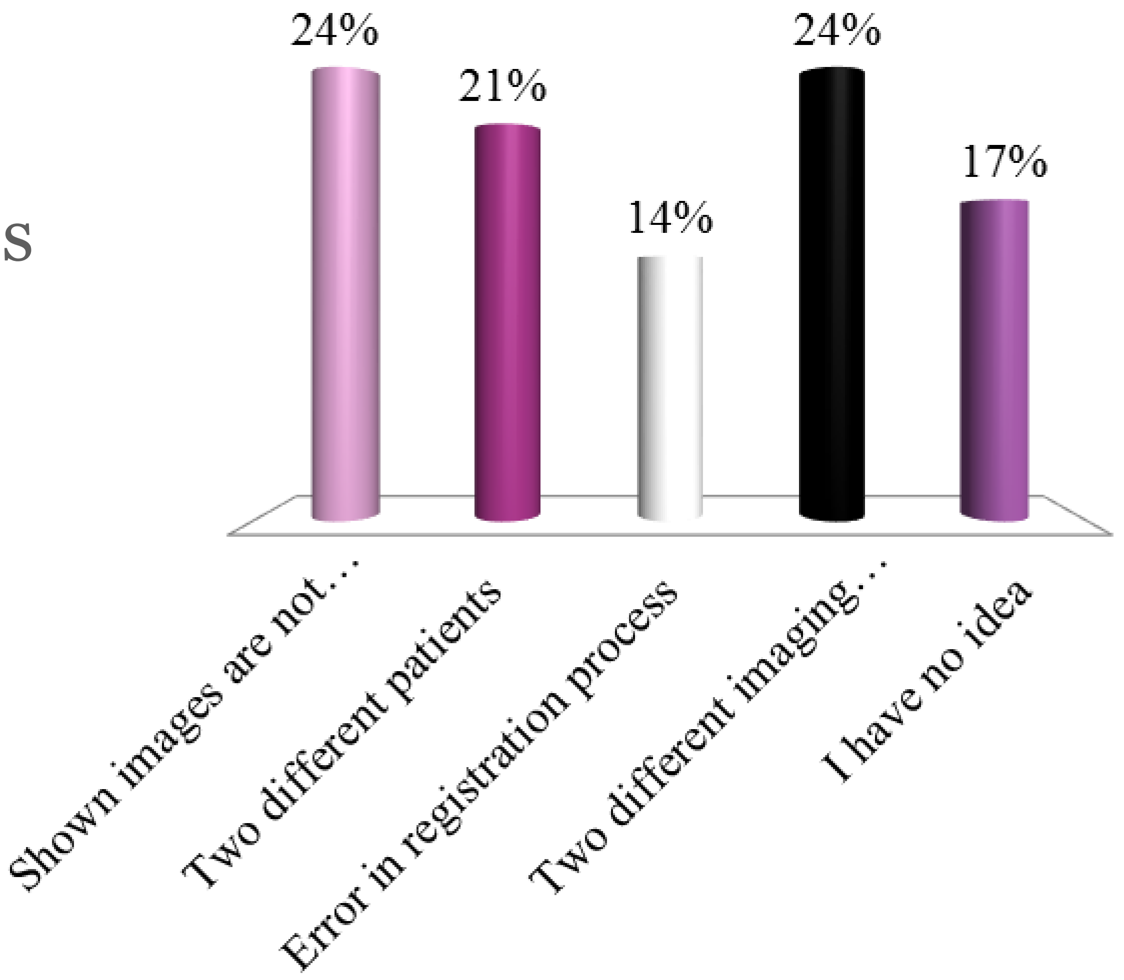


Substract

Checker

Why does this overlay look so purple?

A. Shown images are not weighted equally
B. Two different patients
C. Error in registration process
D. Two different imaging modalities
E. I have no idea



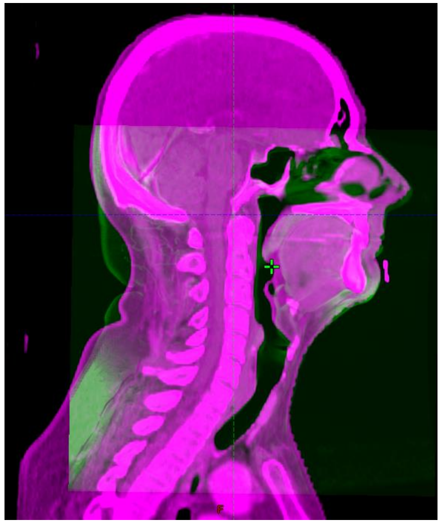
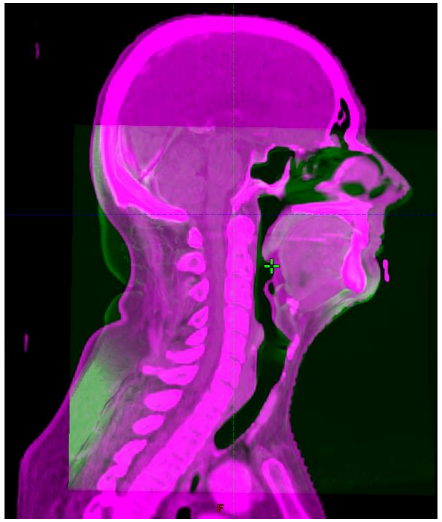
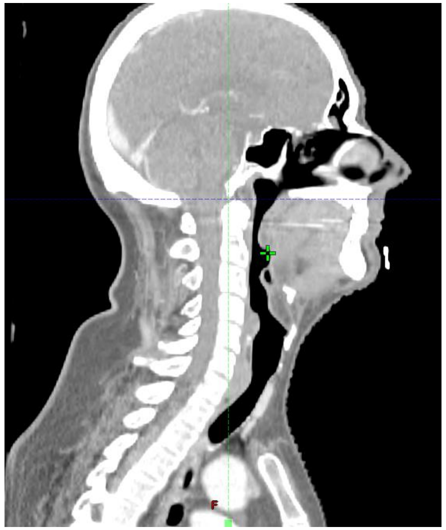


Image fusion

- Viewing & validation of the image registration





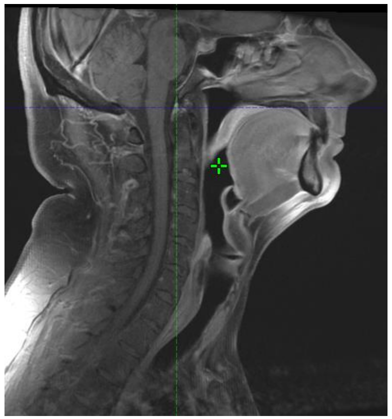
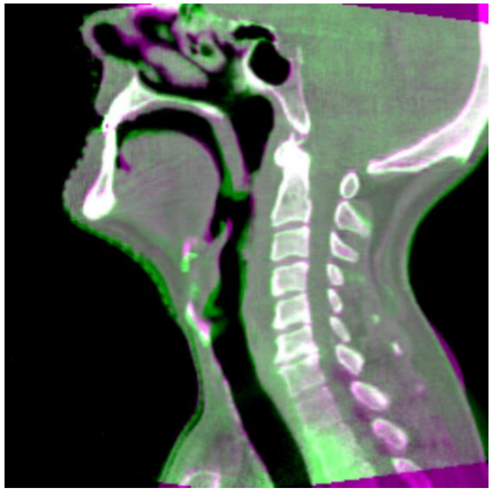
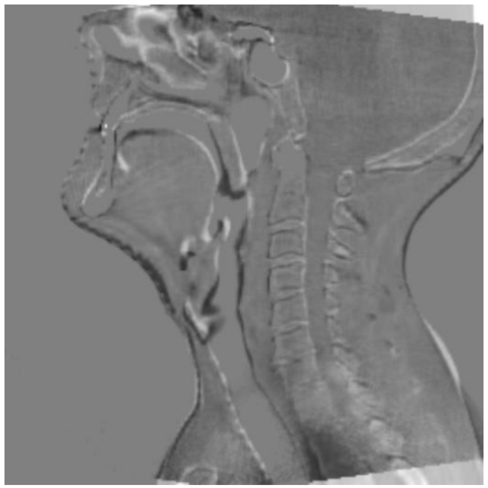


Image fusion

- Viewing & validation of the image registration



Overlay



Substract

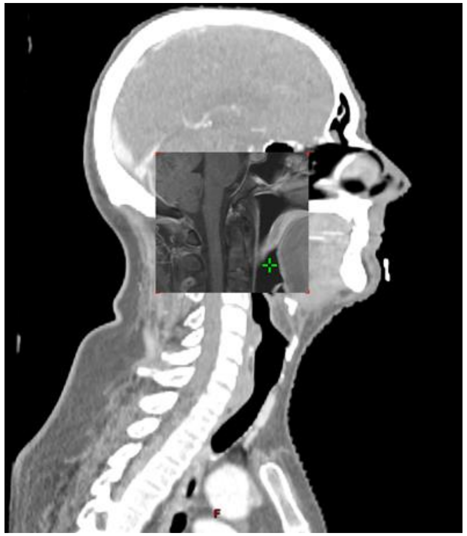
Checker

Same modality

Image fusion

- Viewing & validation of the image registration

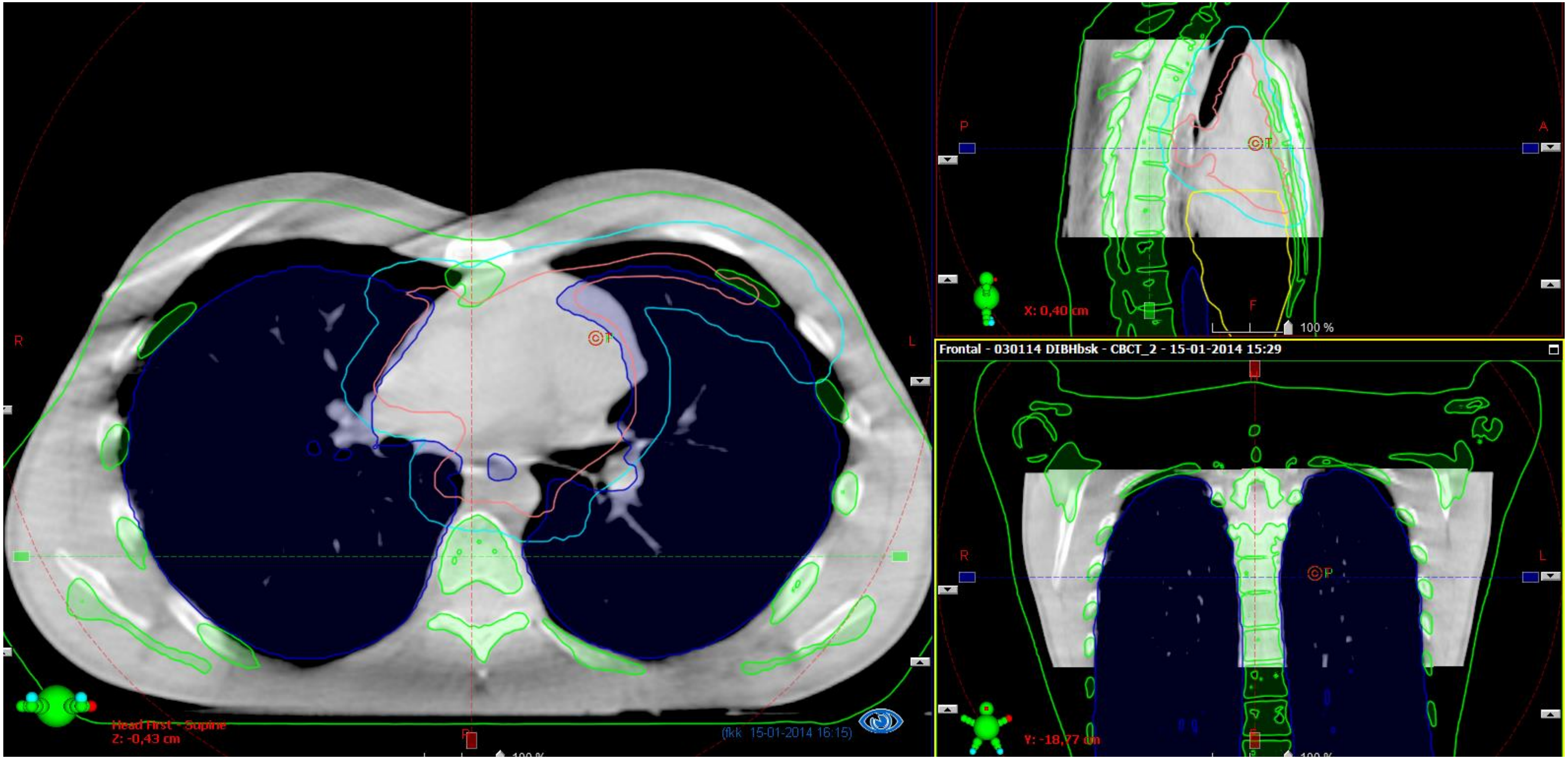
Split window



Spy glass

Different modalities

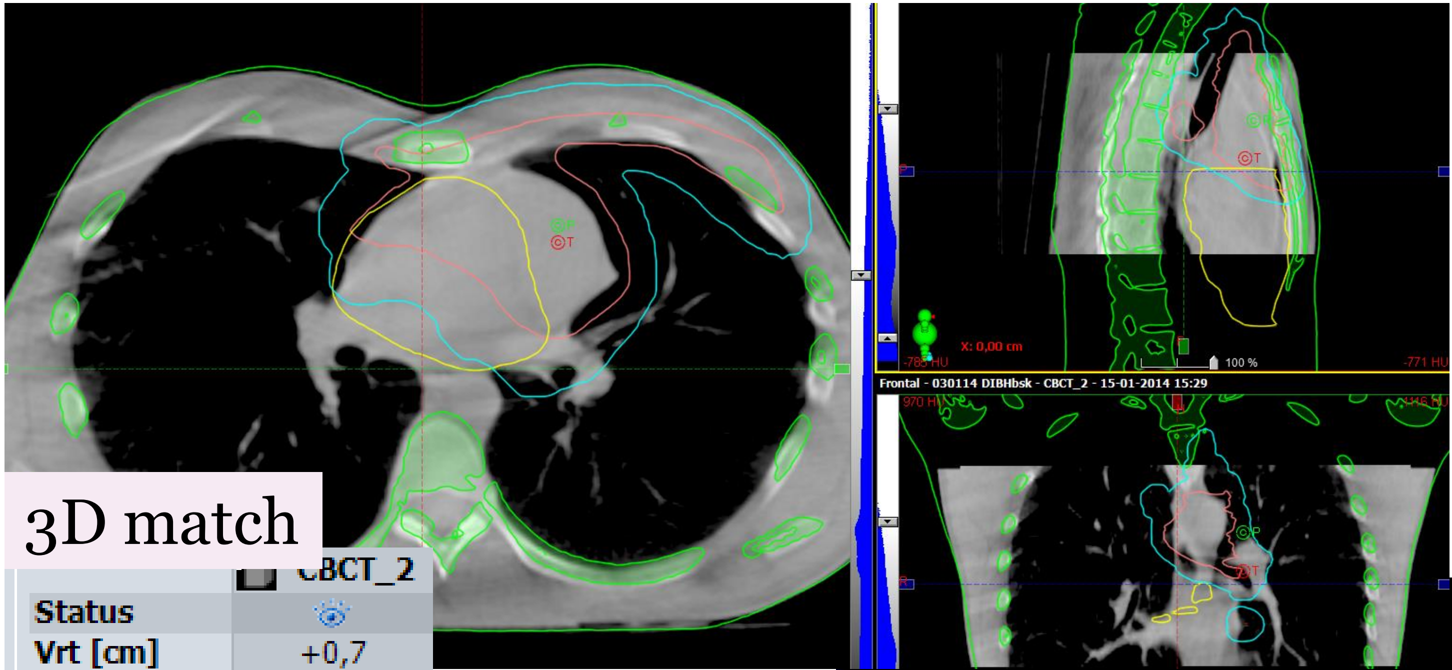
Case: error in automatic image registration



Automatic image registration has to be evaluated!

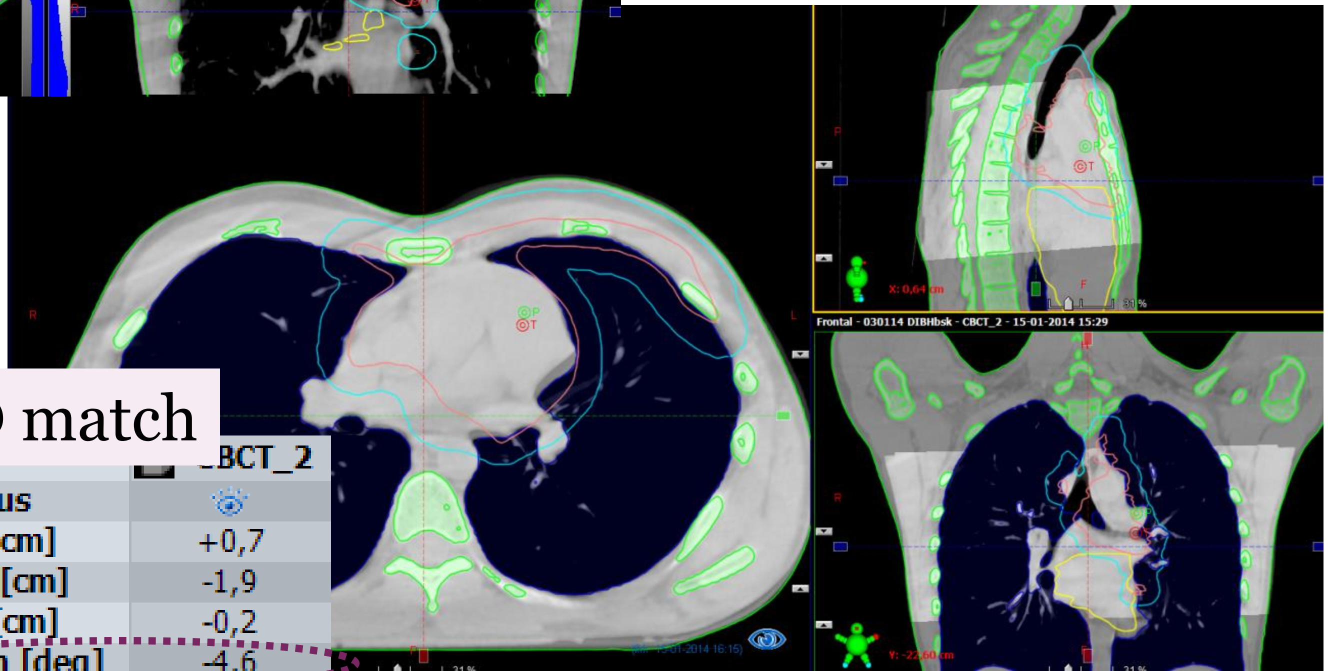
Focus not only on the primary structures of interest, but on the whole image!

Case: error in automatic image registration



3D match

	CBCT_2
Status	
Vrt [cm]	+0,7
Lng [cm]	-3,0
Lat [cm]	0,0
Pitch [deg]	0,0
Roll [deg]	0,0
Rtn [deg]	0,0

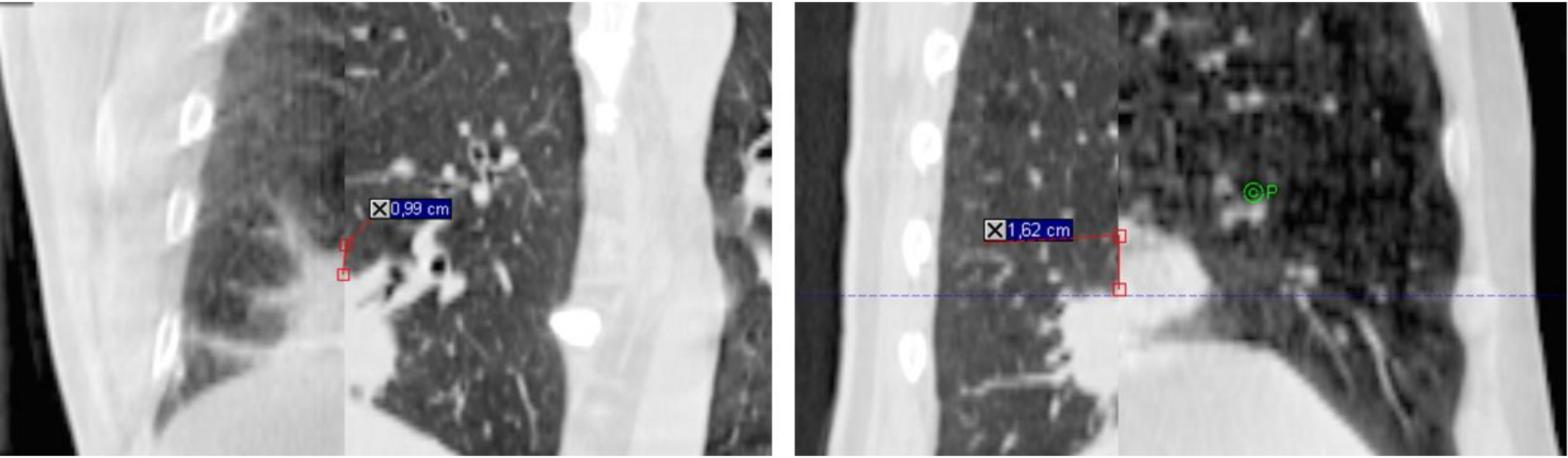


6D match

	CBCT_2
Status	
Vrt [cm]	+0,7
Lng [cm]	-1,9
Lat [cm]	-0,2
Pitch [deg]	-4,6
Roll [deg]	-1,4
Rtn [deg]	-1,1

Focus on the patient set-up!

Lung tumour baseline shift



… misalignment of the peripheral tumour after registration on vertebrae

Challenges in image registration

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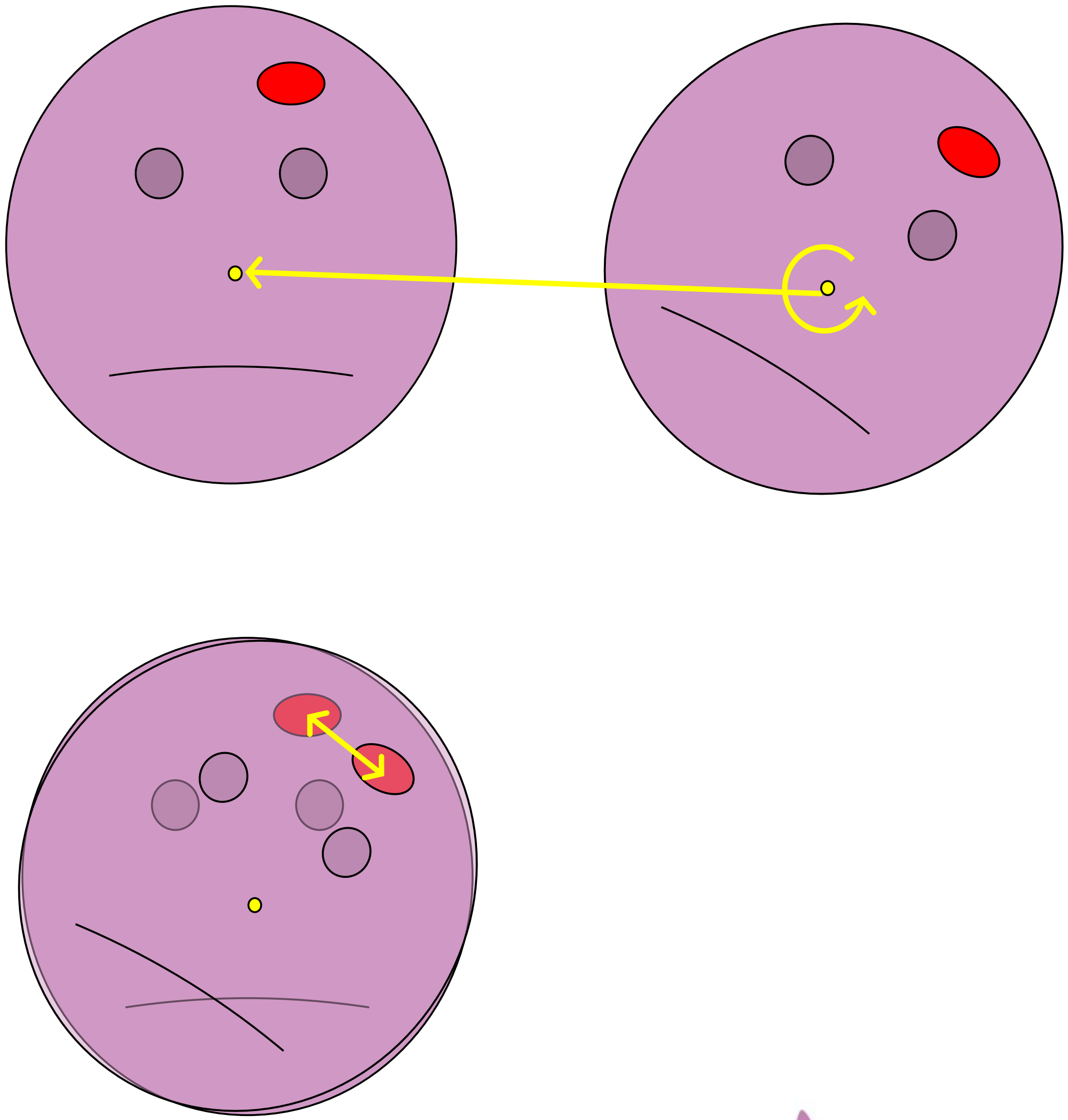
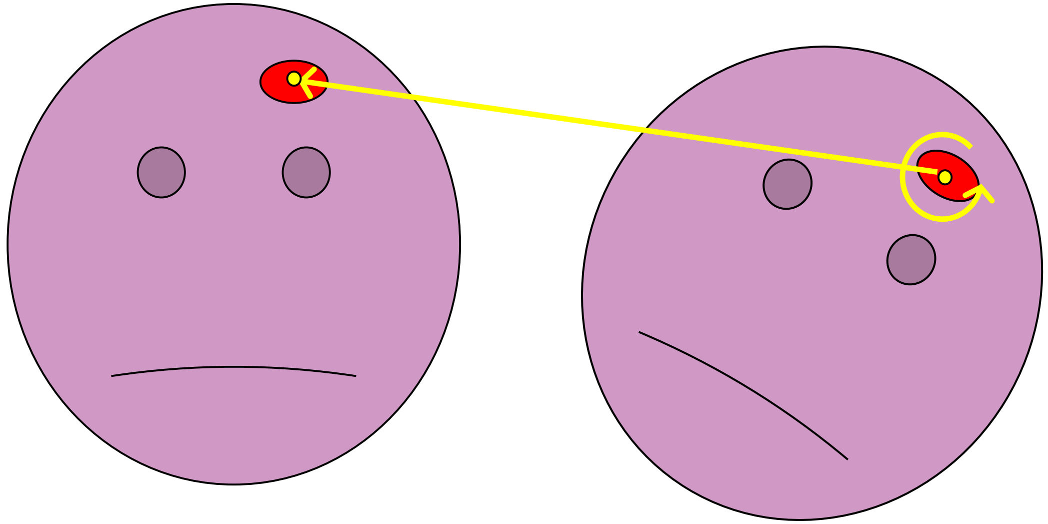
Impact of rotations on image registration

- Registration
  - Bony anatomy
  - Translations and rotations
  - Very accurate
- Correction
  - Only translations
  - Potentially large errors

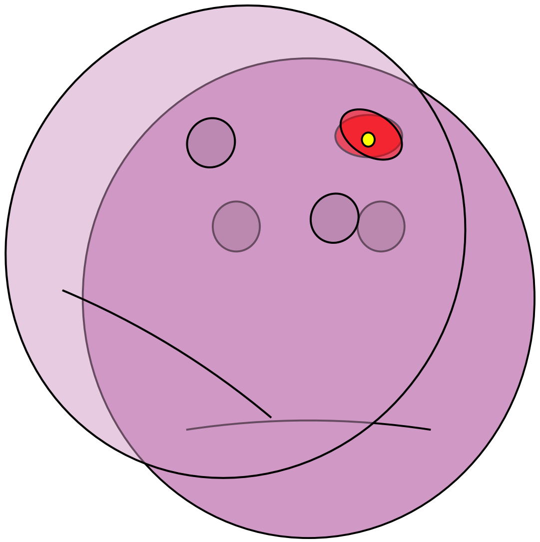


Impact of rotations on image registration

- Registration
  - Redefine match volume
  - Isocenter position



- Correction
  - Only translations
  - Rotational errors are small close to rotation center



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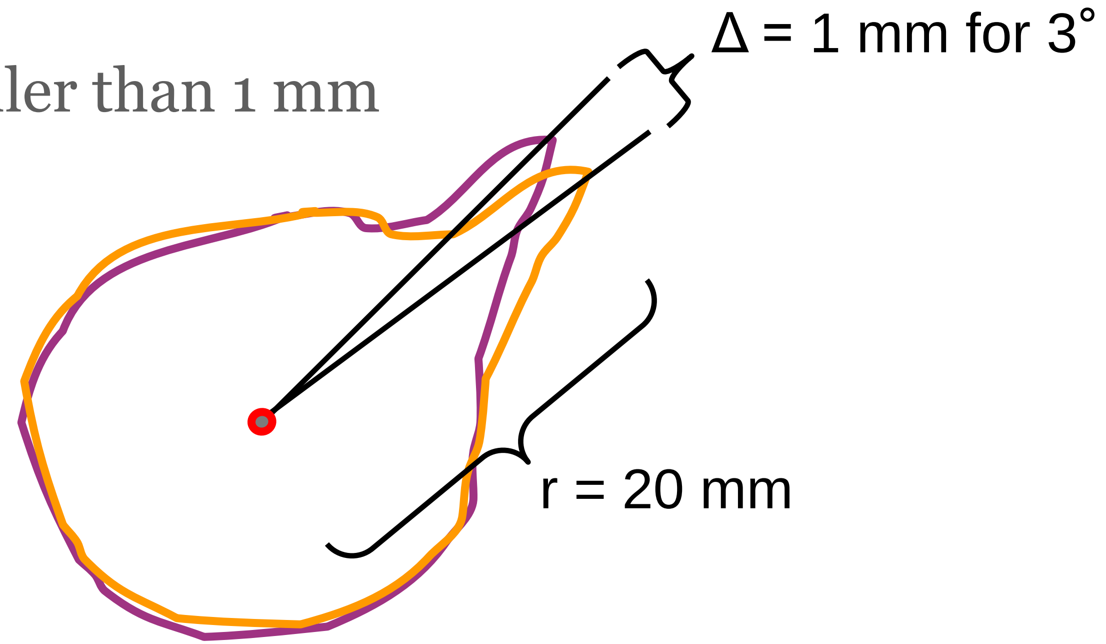
Corrections without rotations

Rule of thumb: $\Delta = 0.02 \times \varphi \times r$ (mm)

- 3° rotation
- CTV diameter is 40 mm (r = 20 mm)
- Rotation centre is in CTV

  →Errors to CTV will be smaller than 1 mm



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Corrections without rotations

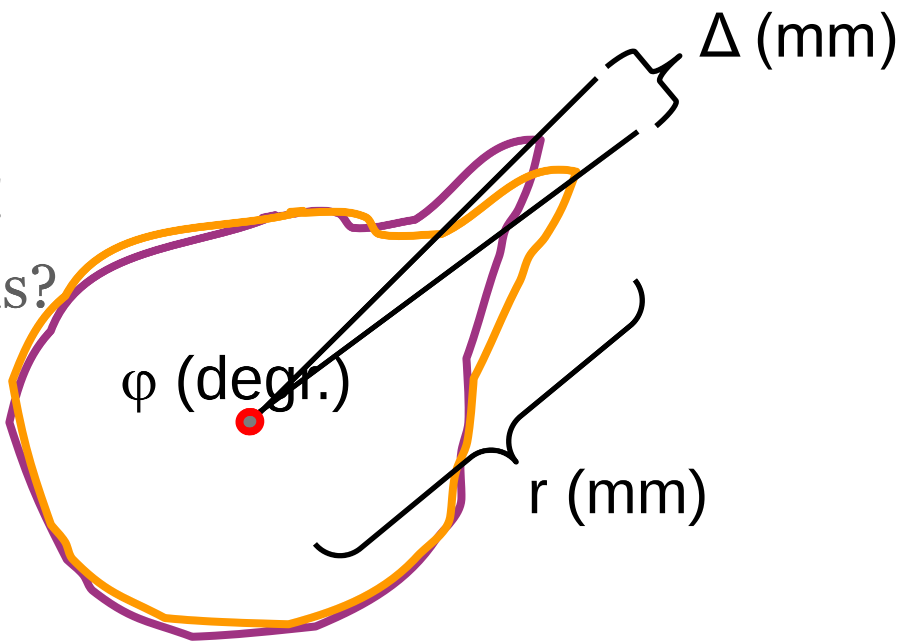
Rule of thumb: $\Delta = 0.02 \times \varphi \times r$ (mm)

Problem for structures far from rotation center

- 3° rotation
- Rotation centre is in CTV

→ 6 mm shift at 10 cm distance!

→ does treatment plan allow this?



Lung stereotactic body radiotherapy

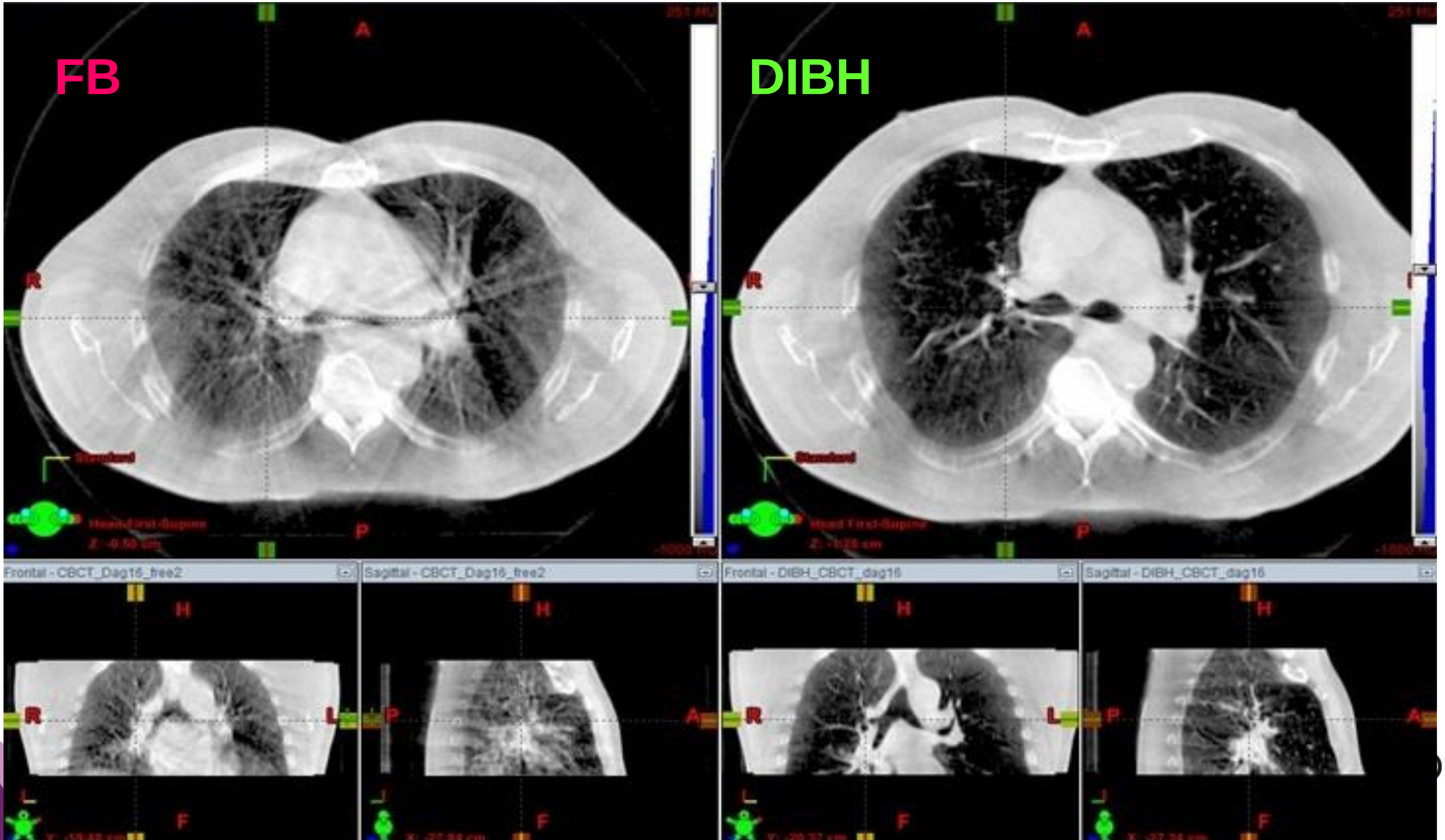
- Residual positional error when only translations were used for image registration

	AP [mm]	CC [mm]	LR [mm]	pitch [°]	roll [°]	rot [°]
M	−0.1	0.1	−0.1	0.31	−0.06	−0.56
Σ	1.3	1.0	0.8	1.20	1.23	1.42
σ	1.5	1.0	1.1	0.79	1.33	0.85

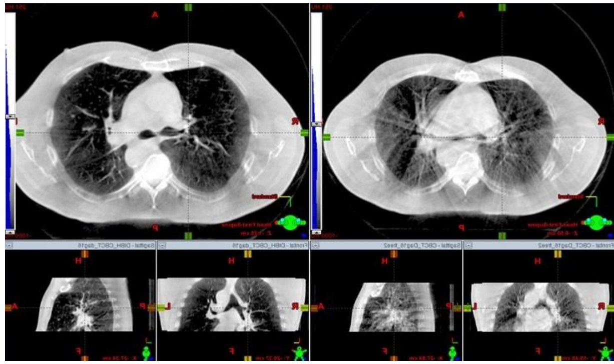
AP, anterior-posterior; CC, cranio-caudal; LR, left-right.

Josipovic et al, Acta Oncol 2012

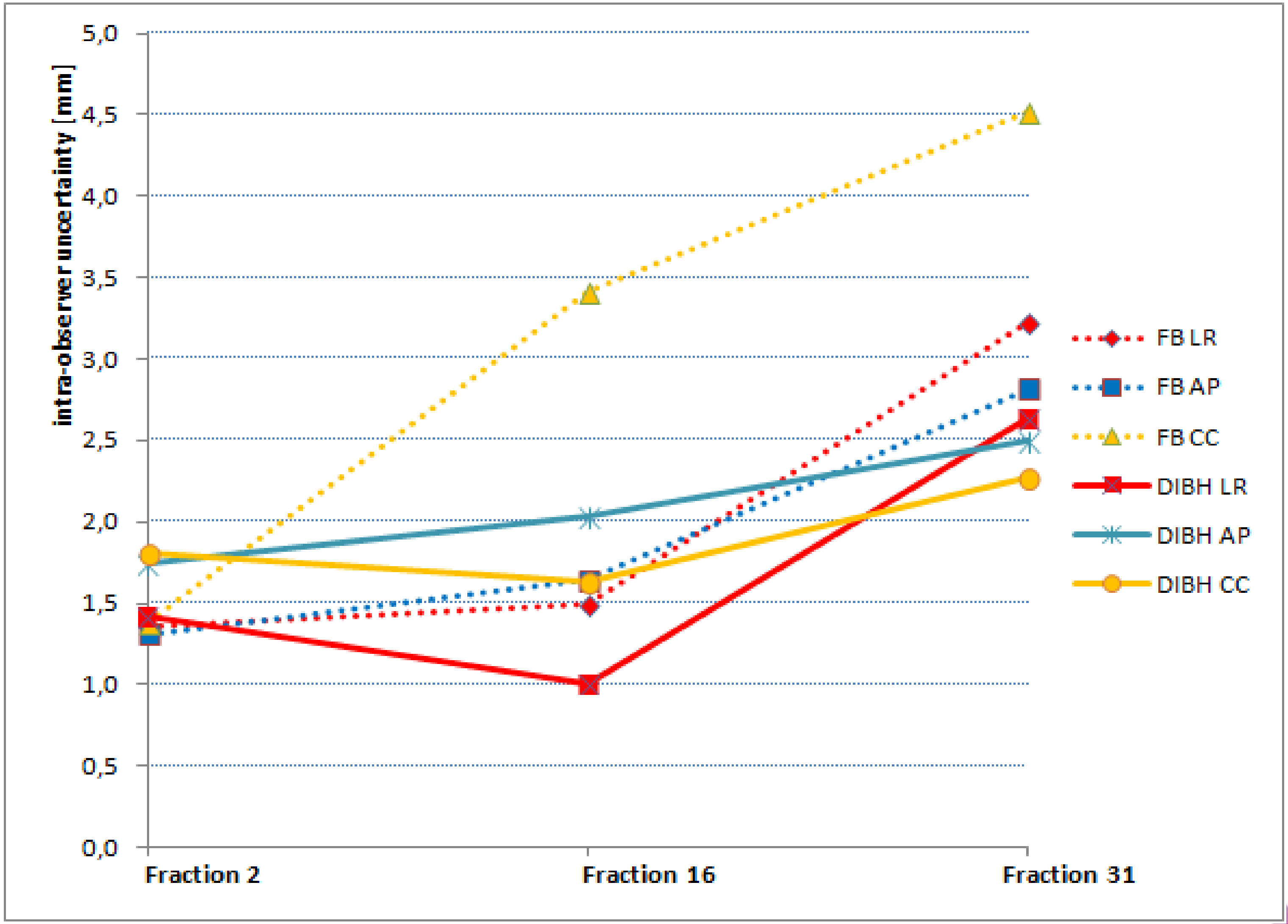
Impact of image quality



Impact of image quality



Observer uncertainties in CBCT registration



Josipovic et al. *BJR 2016*

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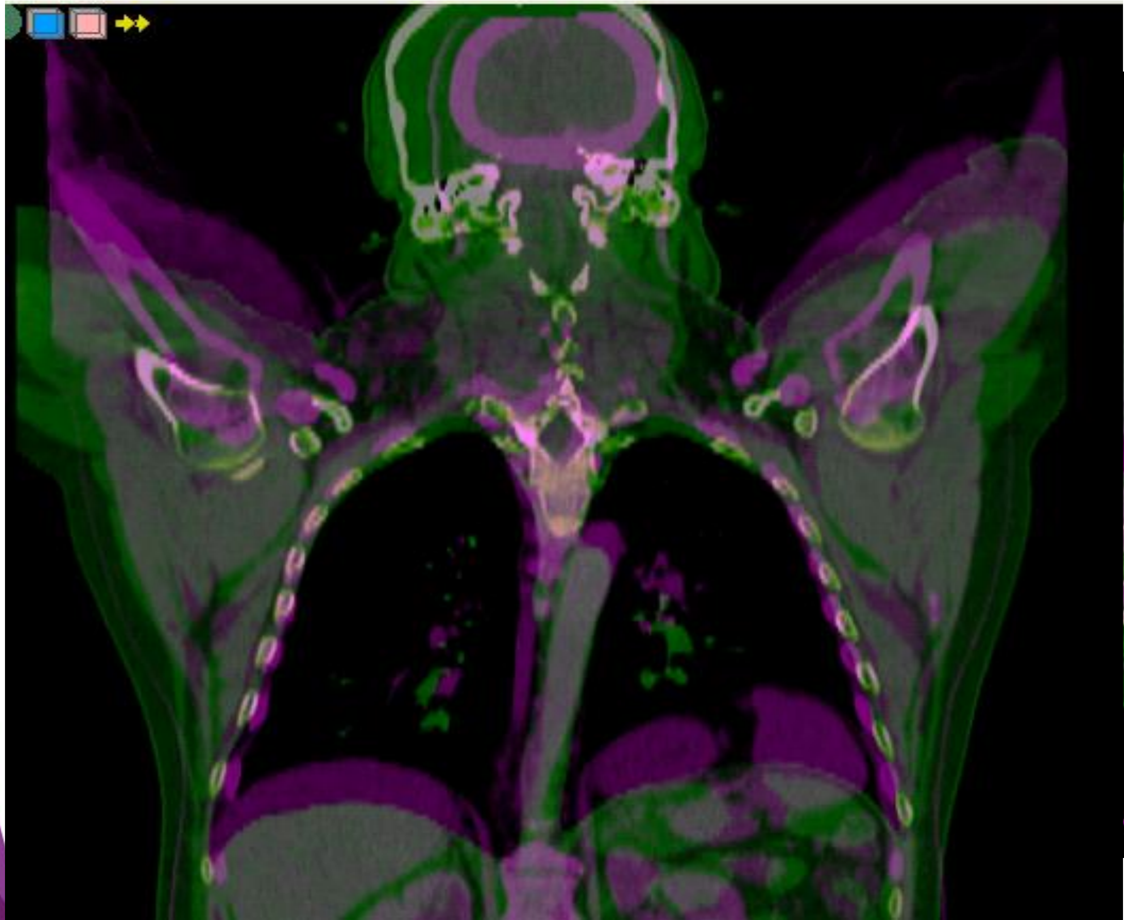
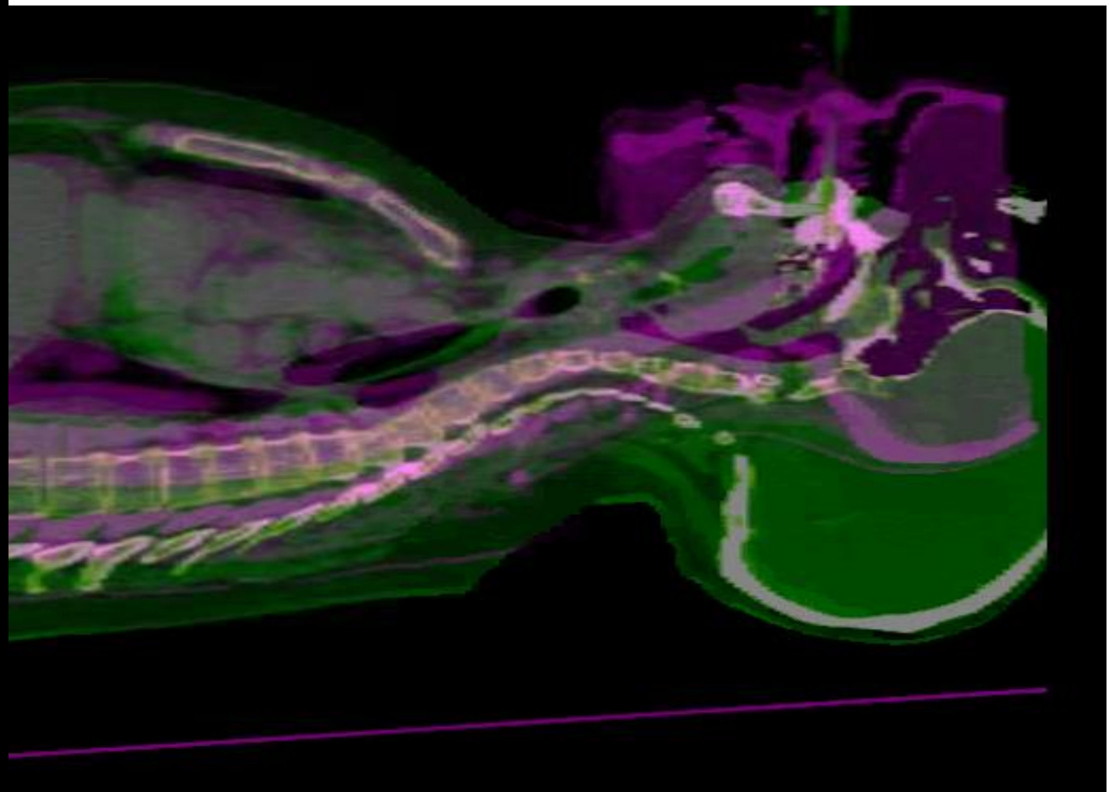
Case: fusion of pre- and post-chemo scan





Courtesy M. Aznar

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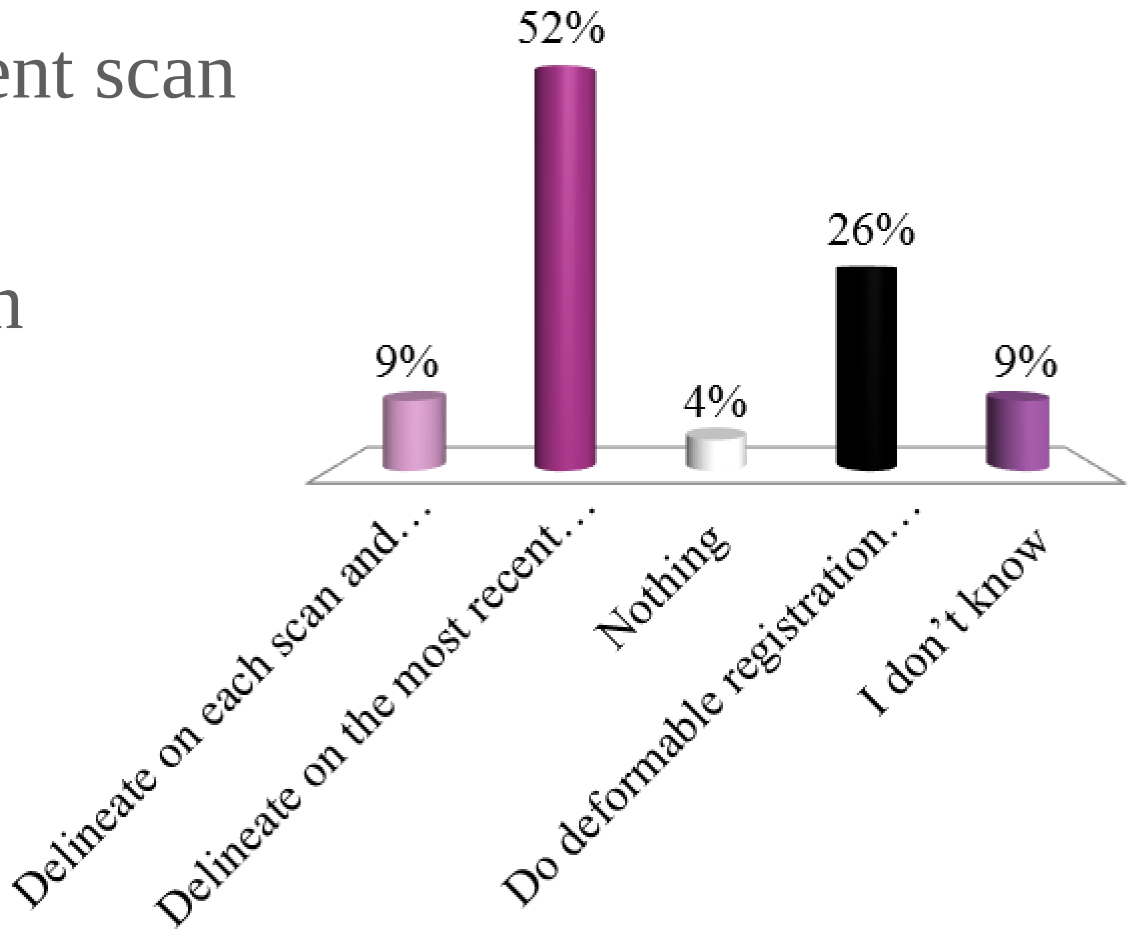
What would you do (or your radiation oncologist)?

A. Delineate on each scan and combine contours
B. Delineate on the most recent scan
C. Nothing
D. Do deformable registration before delineation
E. I don’t know



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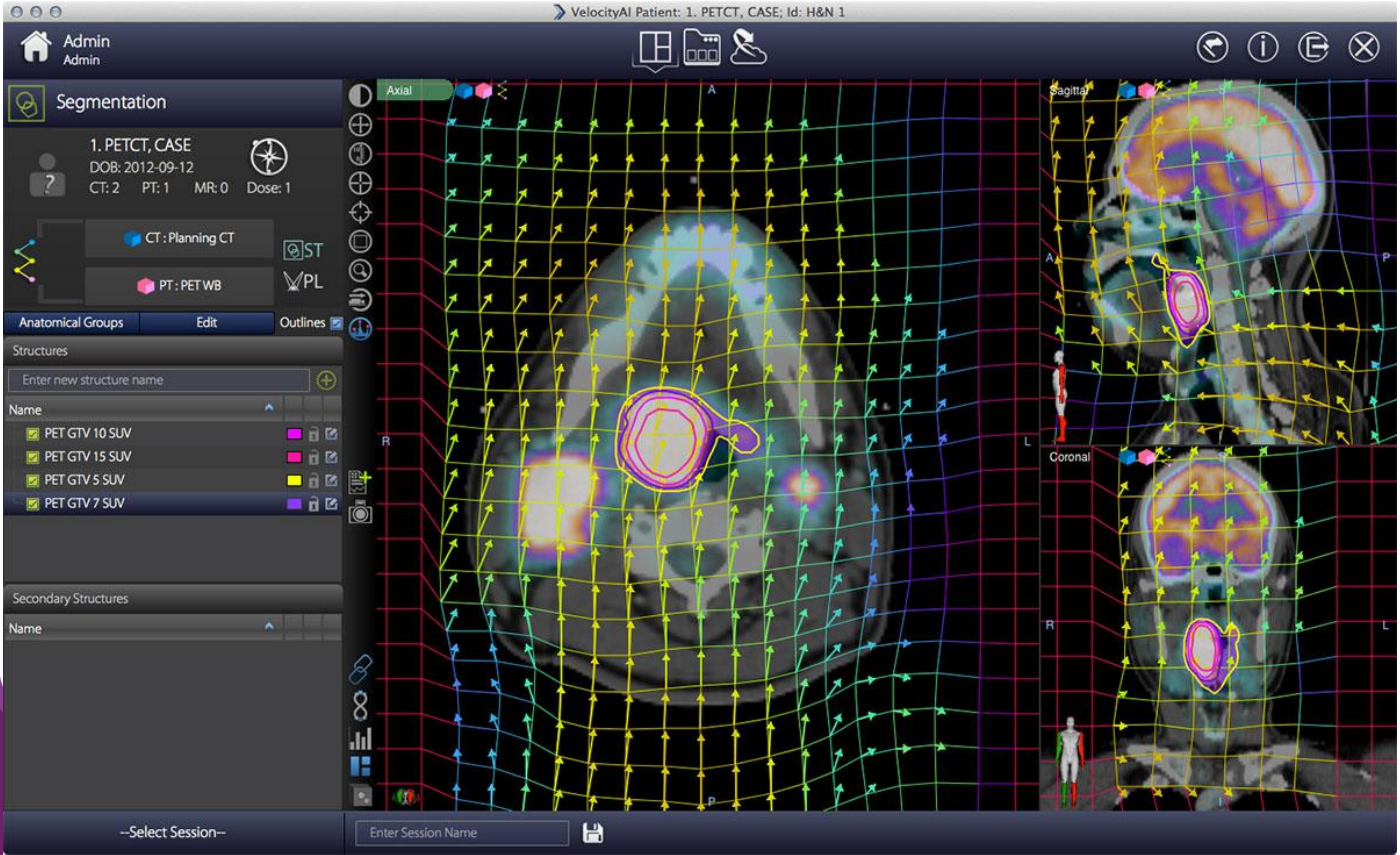
How to handle registration uncertainties ?

- Ensure a treatment-like position already at staging
  - ➢ Flat table top
  - ➢ Arms up
  - ➢ Chest board
  - ➢ Motion management

- Good collaboration with the PET / MR department!

Deformable image registration - DIR



Deformable image registration

- How do you know the result is good?
  - ➢ It looks ok ☺
- Getting the contours / outlines of organs right
  - ➢ Ok for IGRT
- Getting the heterogeniety/tissue cells inside the organs right
  - ➢ Necessary for dose accumulation
- Different challenges with different organs
- DIR needs to be evaluated for each clinical problem

Take home messages

- Image registration plays an important role for:
  - routine treatment planning
  - routing treatment delivery
  - Follow up, clinical studies, re-irradiation

- Consider the effect of rotations and anatomical changes

- There is no perfect solution:
  - use best registration algorithm for each problem
  - **<u>always</u>** include a visual inspection step in the process

Additional reading: **AAPM TG 132 report**

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Management of respiratory motion in radiation therapy

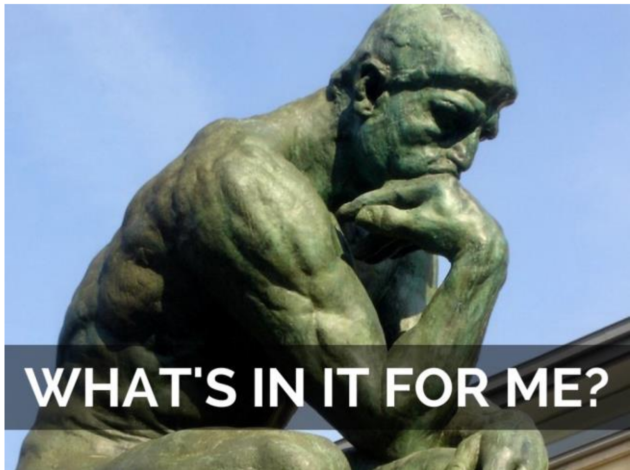
Mirjana Josipovic

Dept. of Oncology, Rigshospitalet
& Niels Bohr Institute, University of Copenhagen
Denmark

Advanced skills in modern radiotherapy
June 2017

Intended learning outcomes

- Differentiate between different motion management strategies in RT
- Interpret the purpose of motion management for different patient groups
- Identify the limitations in motion management



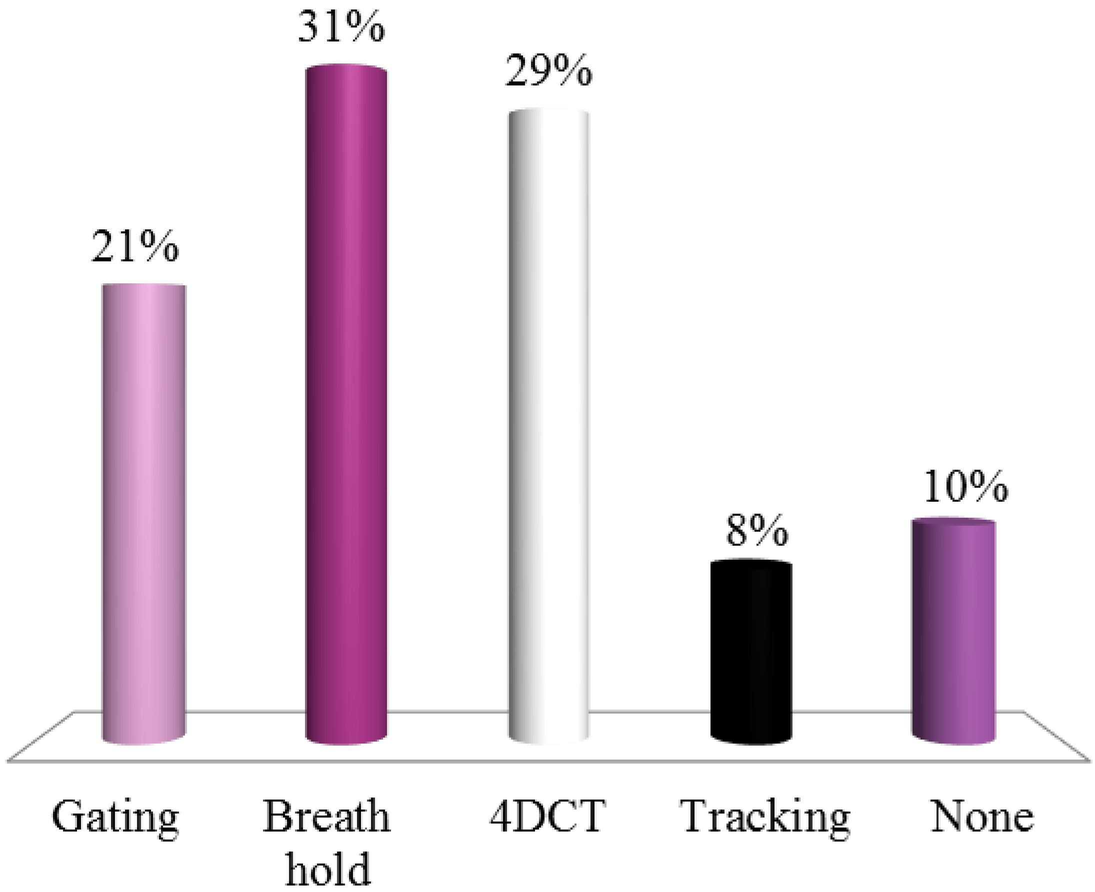
Management of respiratory motion in RT

- Respiratory gating technique
- Breath hold methods
- Motion encompassing methods
- Respiration synchronized techniques

AAPM TG 76 definition

Which motion management do you use?

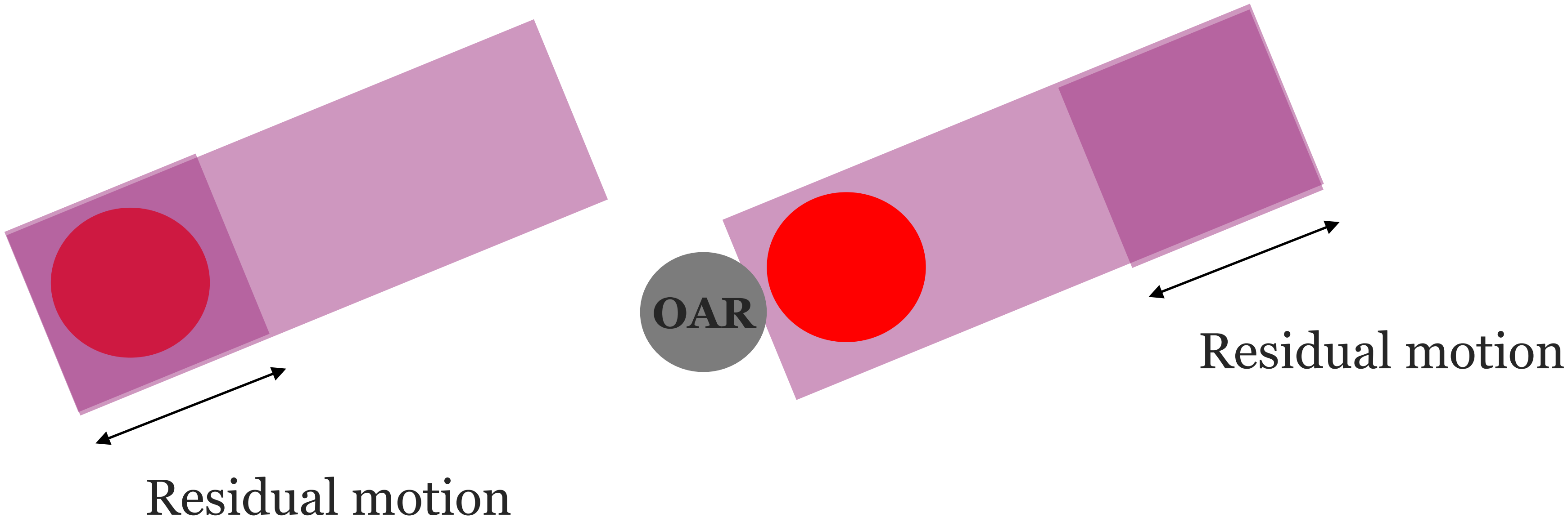
A. Gating
B. Breath hold
C. 4DCT
D. Tracking
E. None



Multiple answers allowed

What is respiratory gating?

- Applying radiation within a particular part of the patient's breathing cycle



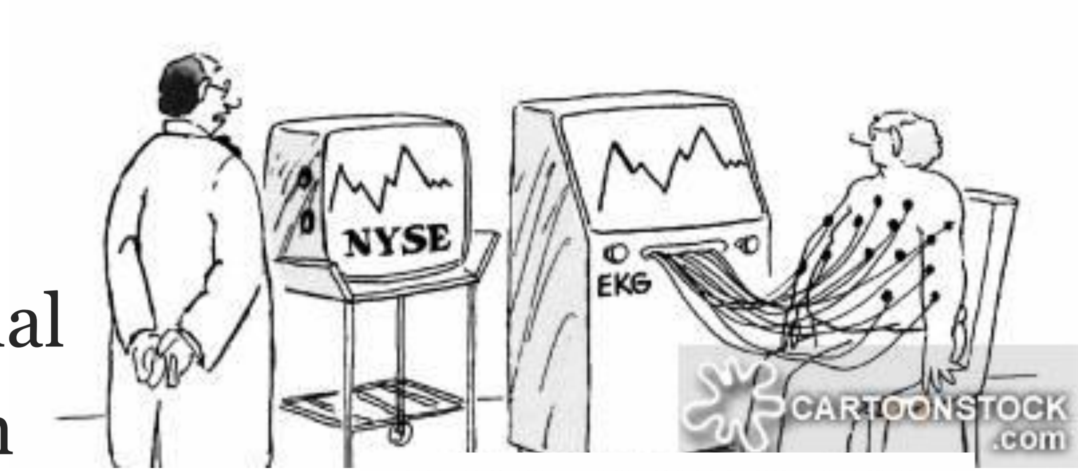
→ Reduce motion during treatment
→ Move target away from OAR

Condition for success with gating

Strong correlation

Internal organ motion - External chest motion

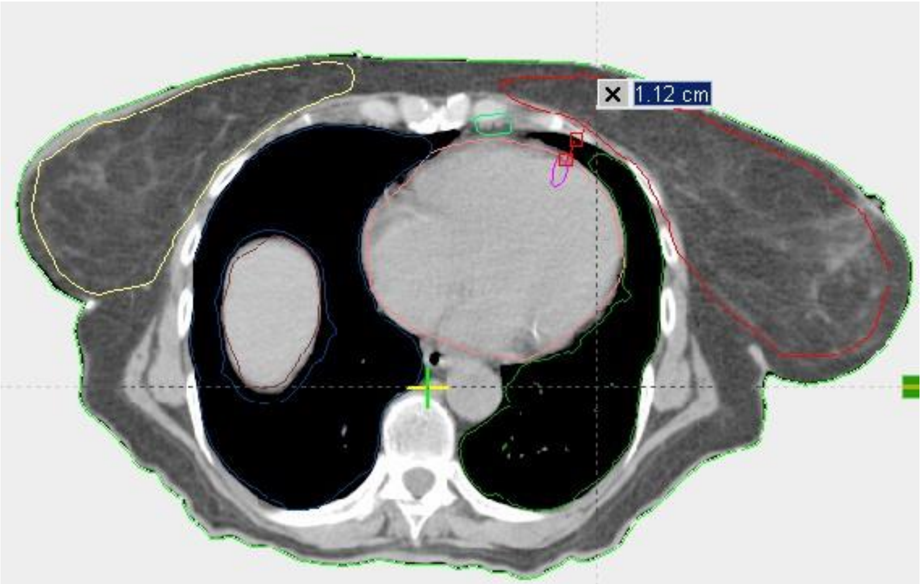
- Tumour type and location
- Source of the respiratory signal
- Reproducibility of respiration



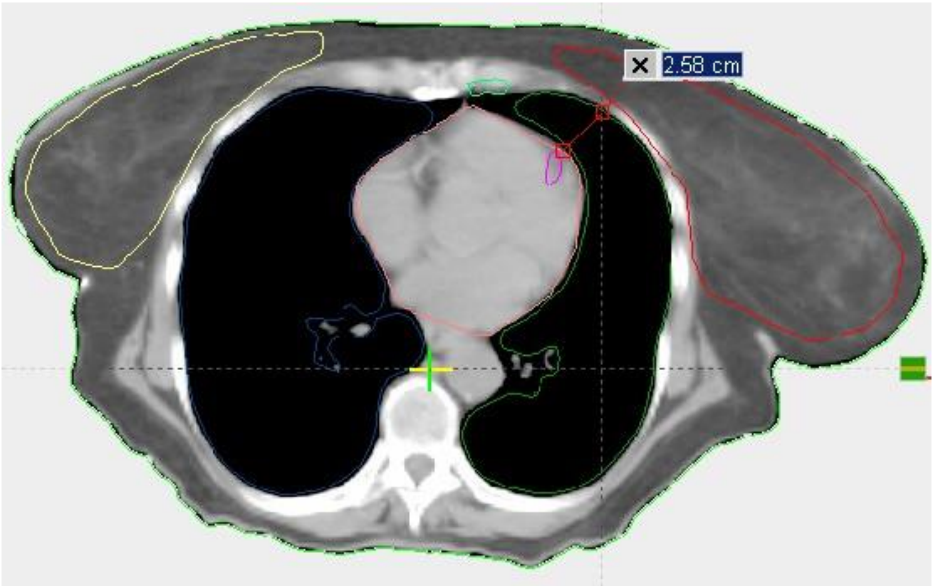
" Amazing . . the patterns are the same ! "

External vs. “internal” motion - breast

- Good correlation



Spontaneous breathing



Enhanced inspiration gating

External vs. internal motion - lung

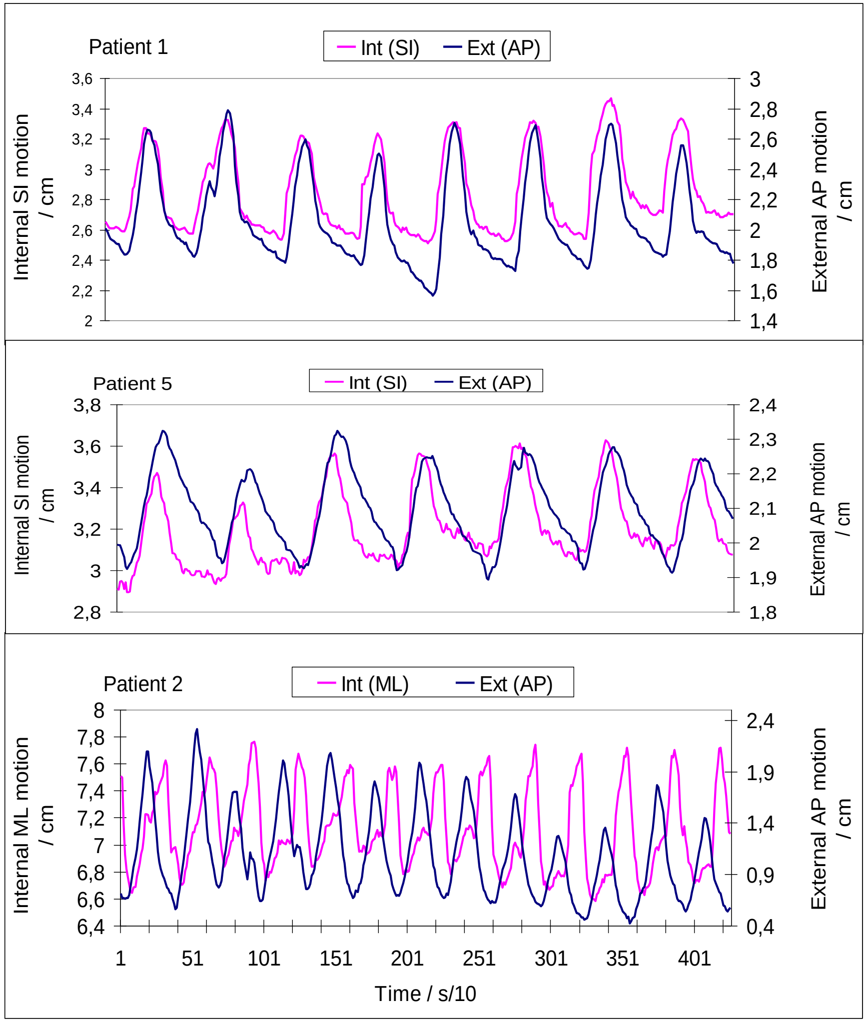


Image courtesy of S Korreman

Correlation can be established

Phase difference

Phase drift

- No correlation

No external vs. internal motion correlation

Simple approach:

- Don't do gating

Complicated approach:

- Monitor the target position during (gated) treatment

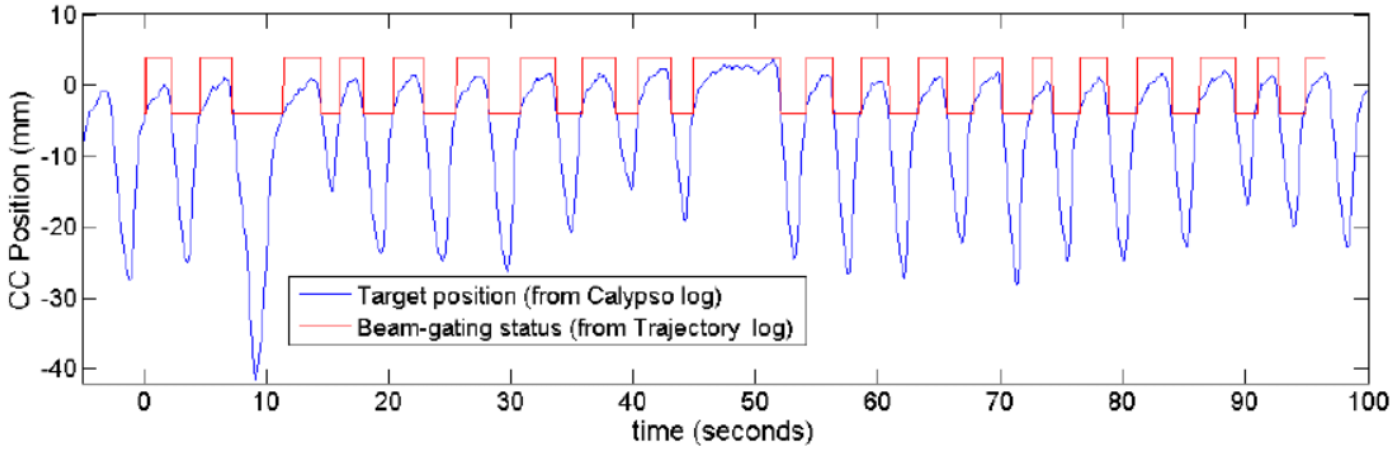


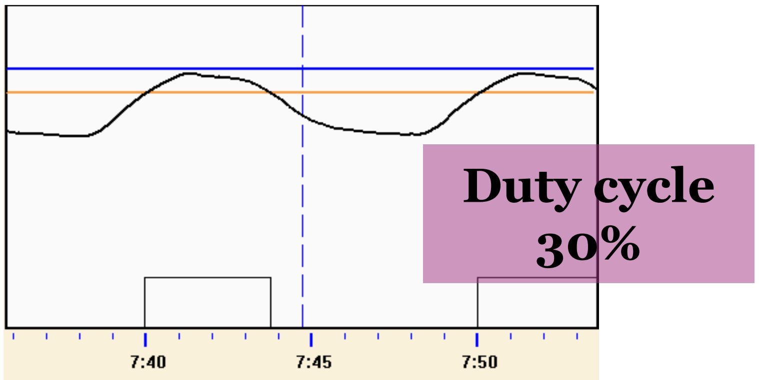
Image courtesy of PR Poulsen

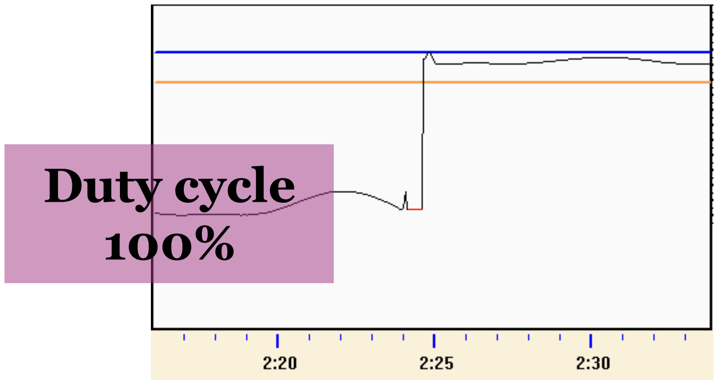
- Free breathing respiratory gating can be applied if there is a good correlation between the respiratory signal and the tumour motion

The choice of breathing technique

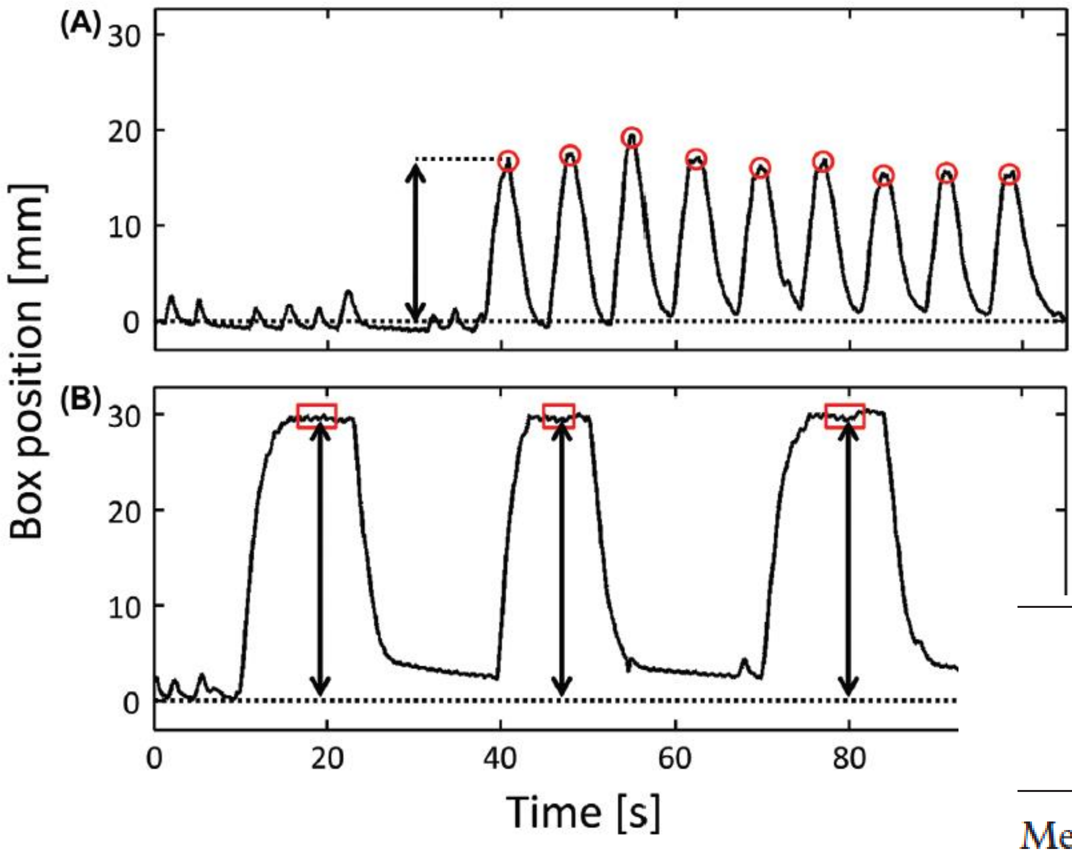
Inspiration gating

Deep inspiration breath hold (DIBH)





Respiration reprodicibility



← audio coaching + insp.gating

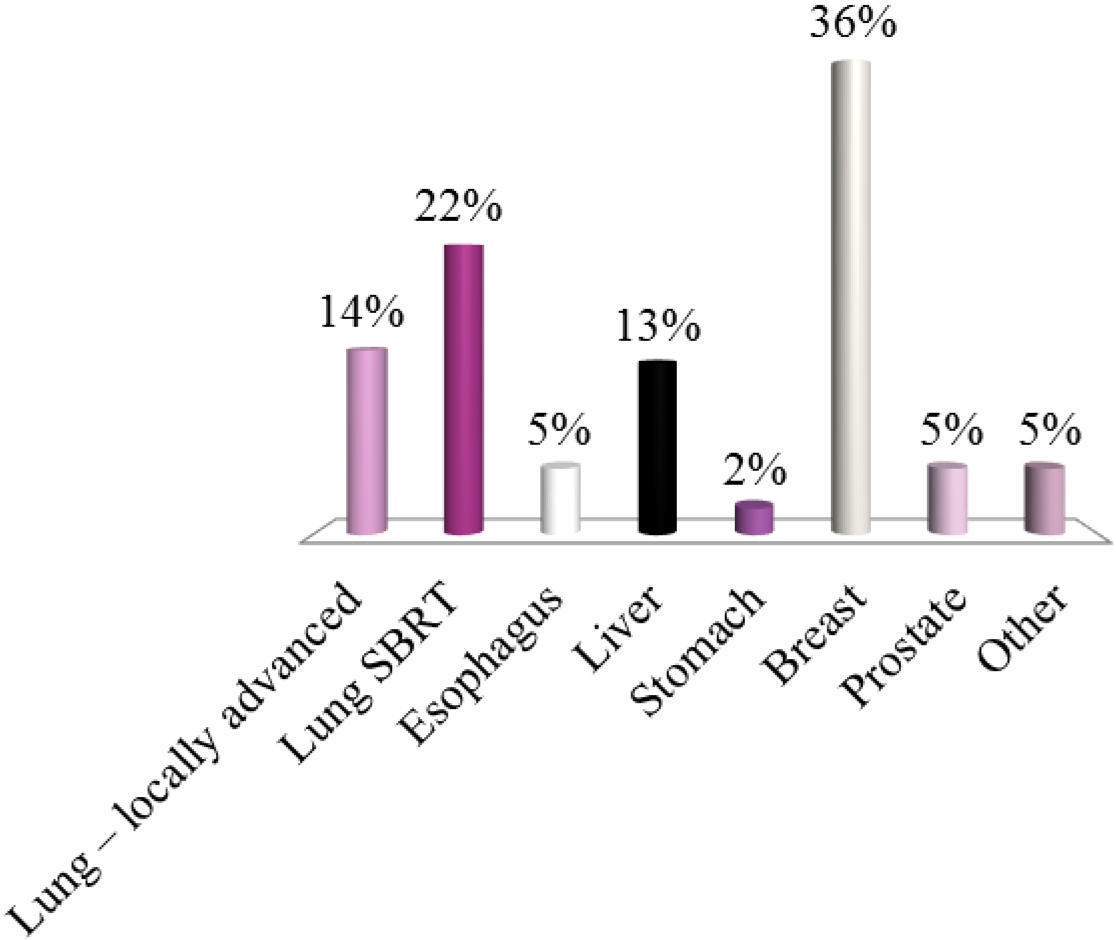
← visual guidance + DIBH

	Audio-coached EIG mean (range)	Visually guided DIBH mean (range)
Mean inspiration level [mm]	16.6 (5–35)	20.5 (5–34)
Mean standard deviation [mm]	1.66 (0.5–3.5)	0.38 (0.2–0.6)

Damkjær et al. Acta Oncologica, 2013

In which sites do you use gating / DIBH?

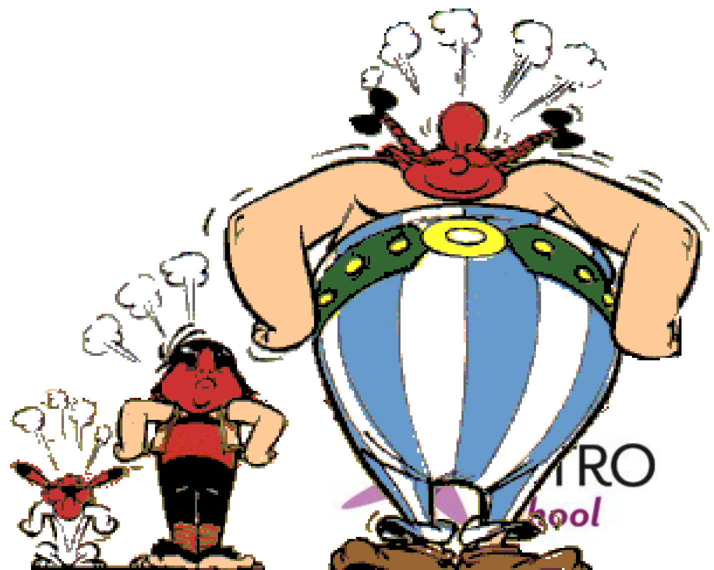
A. Lung – locally advanced
B. Lung SBRT
C. Esophagus
D. Liver
E. Stomach
F. Breast
G. Prostate
H. Other



How to DIBH?

- Free DIBH 

- Computer-controlled
  - ➢ Breathing volume based
  - ➢ Optical surface tracking

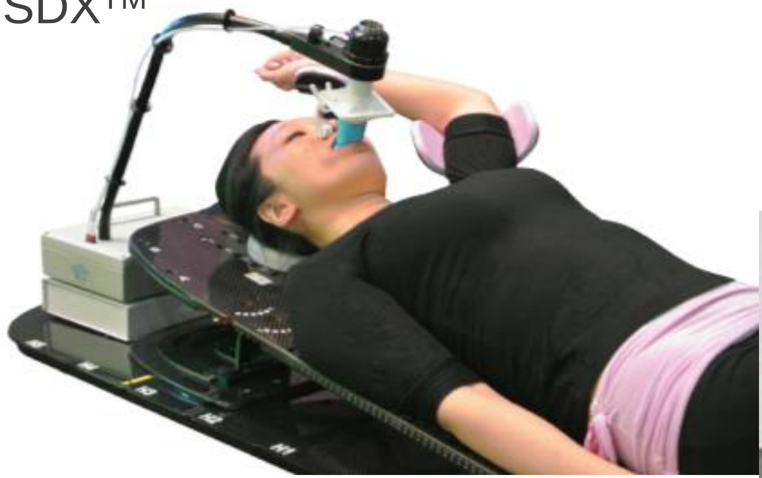


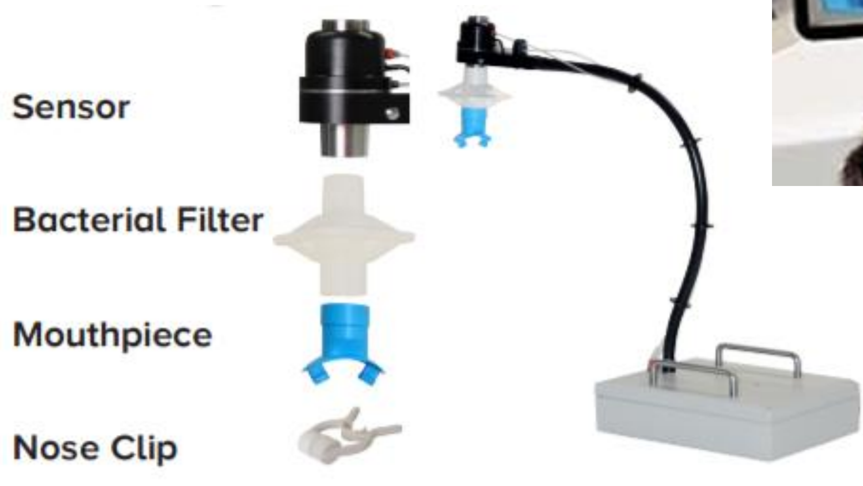
Boda-Heggemann IJROBP 2016

Breathing volume based DIBH

- Spirometry

SDX™





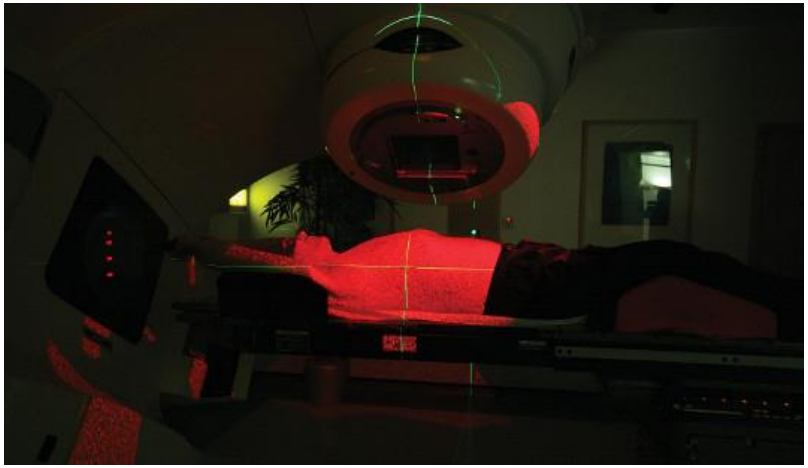
ABC™

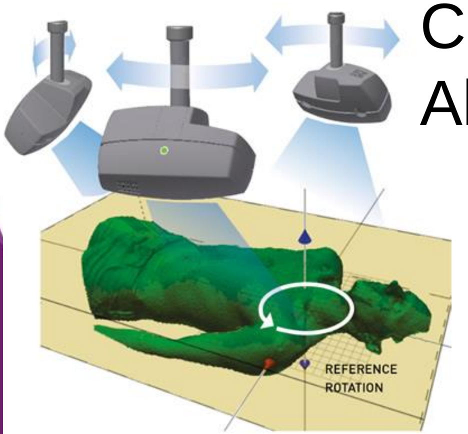
Optical surface tracking based voluntary DIBH

Surface tracking

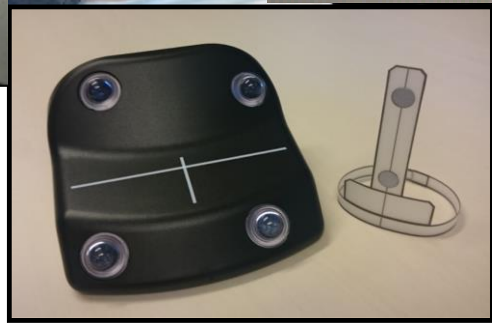
(Surface Guided RT)

Marker tracking





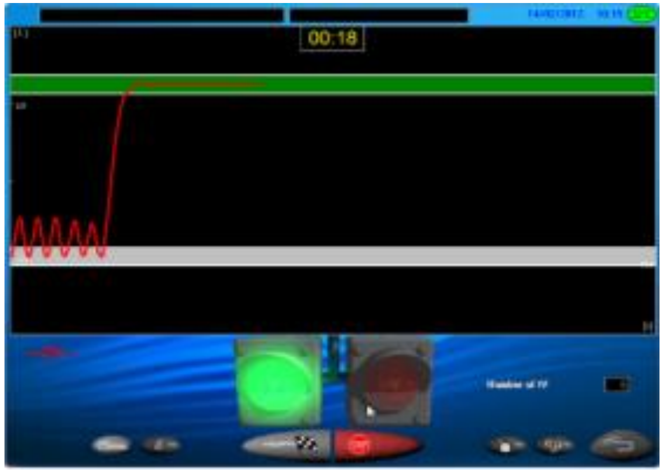
C-RAD Sentinel™
Align RT®



Varian RPM™

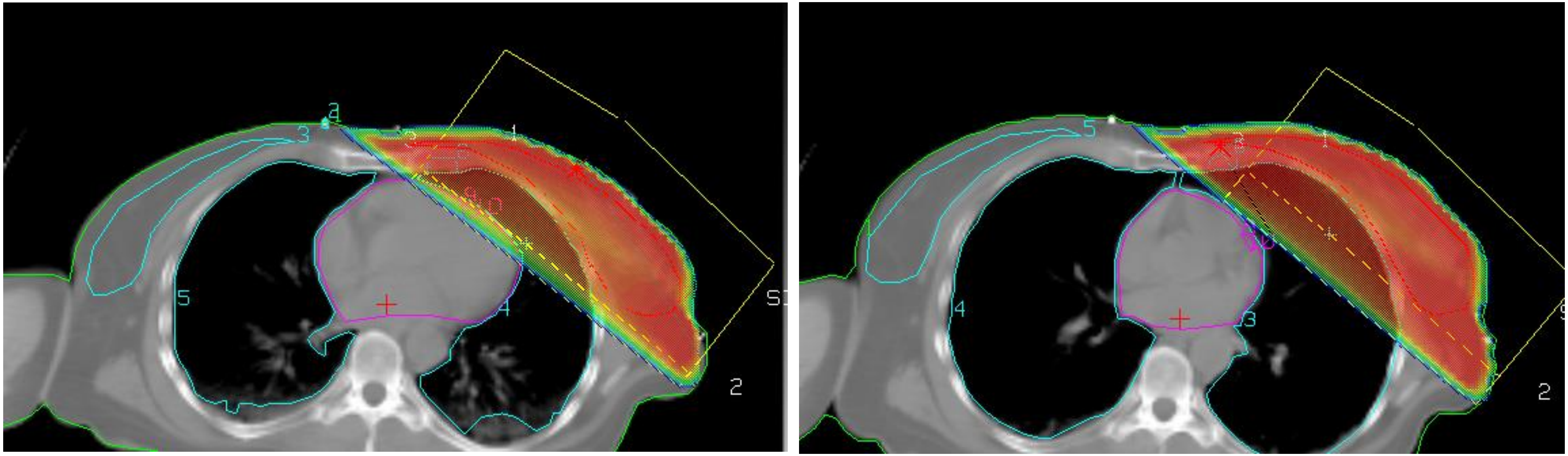
Patient training & QA

- Patient information
- Patient coaching



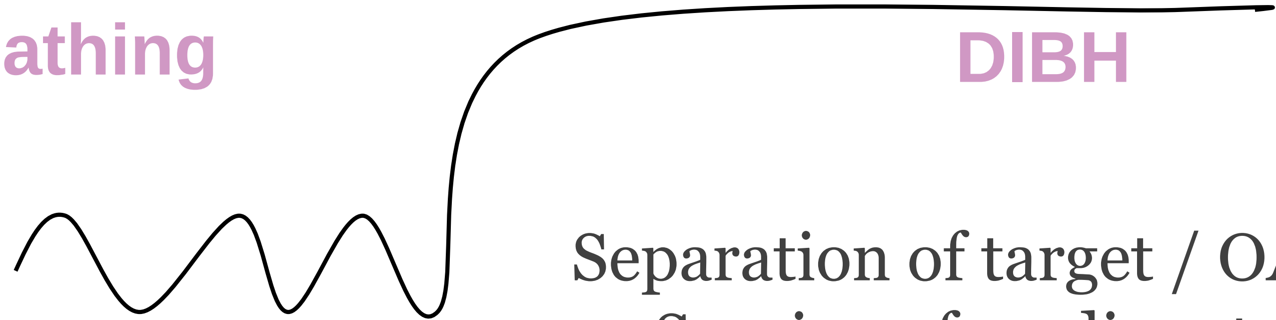
- DIBH level / volume individually adjusted!
- DIBH duration 15-30 s
  - If the patient doesn't comply – exclude!

Dosimetric potential of DIBH – breast



Free breathing

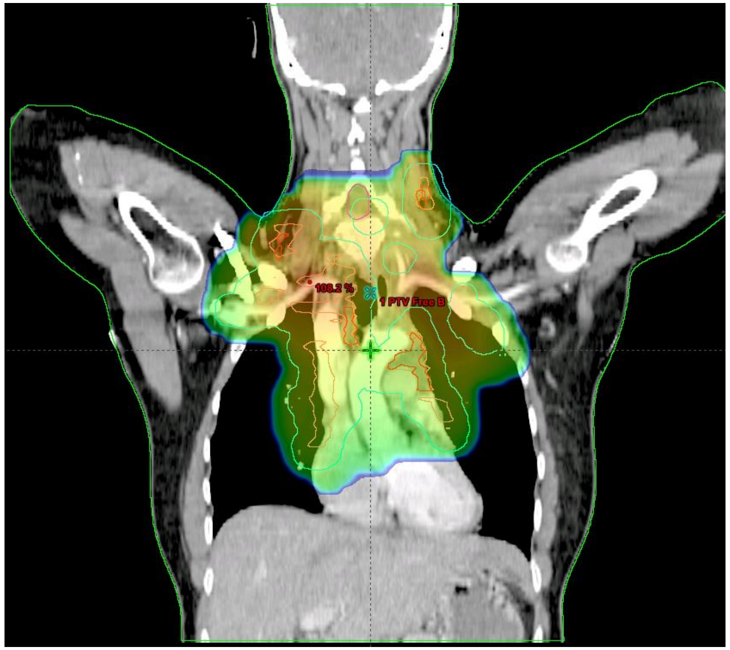
DIBH



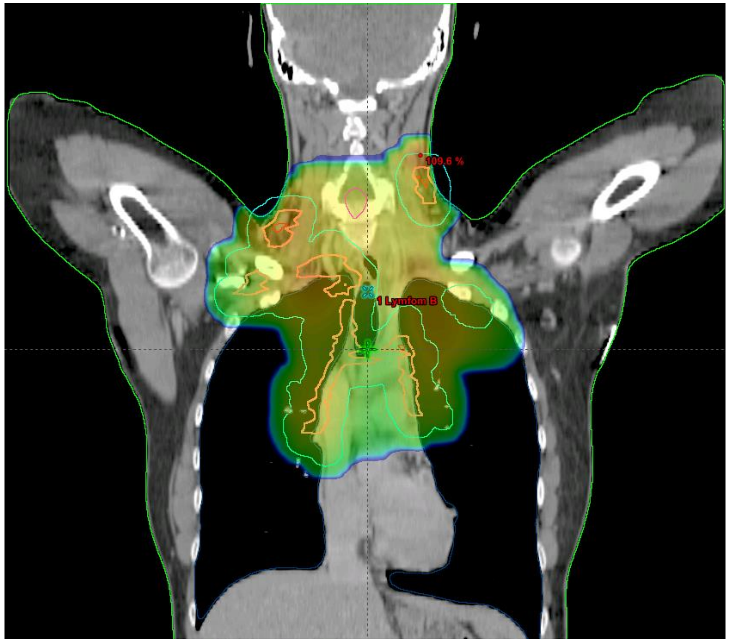
Separation of target / OAR

- Sparing of cardiac structures
- IMN coverage not compromised

Dosimetric potential of DIBH – lymphoma



Free breathing

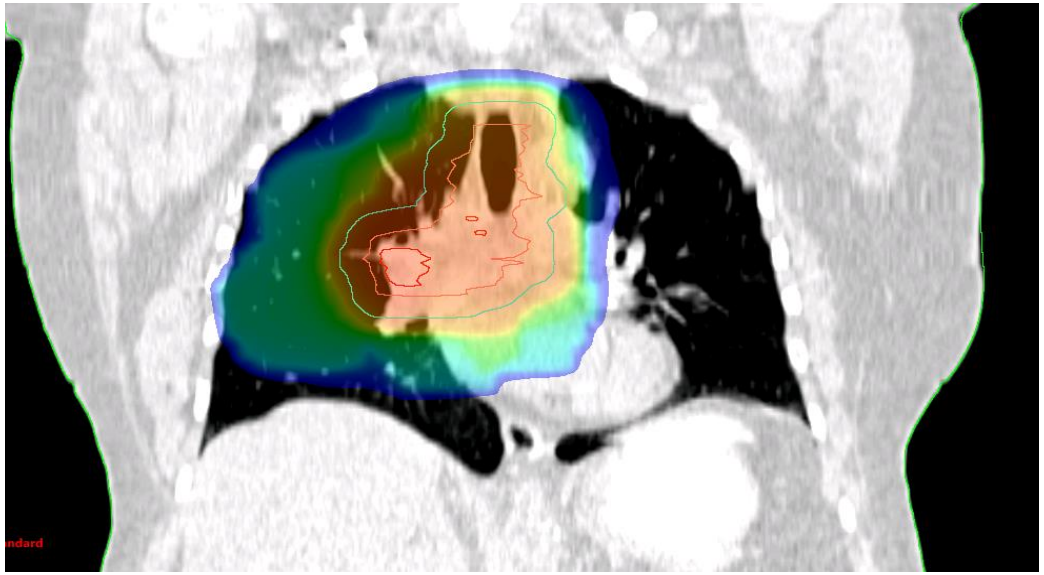


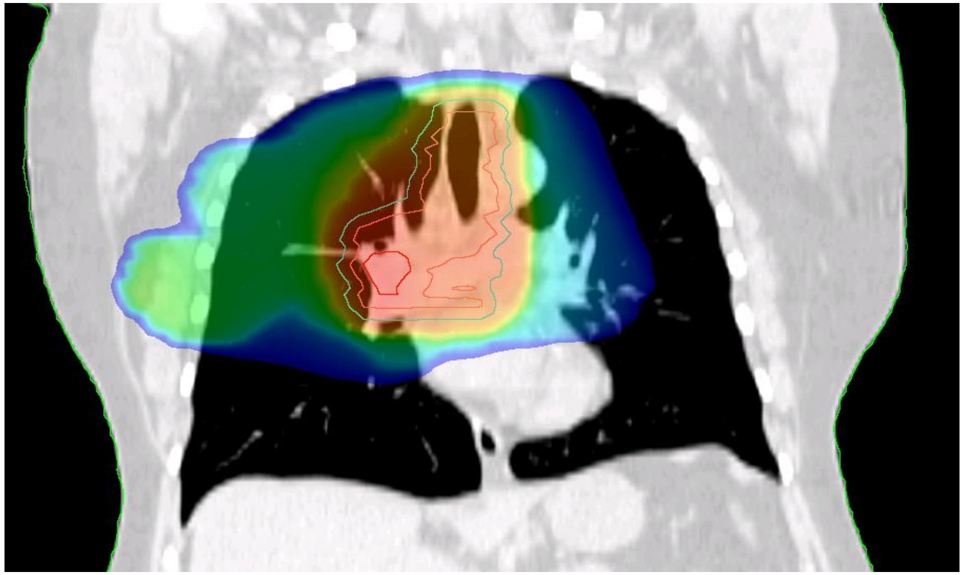
DIBH

- Sparing of heart & lung
- Separation of target & OAR

Images courtesy of Marianne Aznar

Dosimetric potential of DIBH – lung





Free breathing

DIBH

- Sparing of heart & lung
- Maintain curative treatment intent
- Tumour motion reduction

Josipovic et al, Acta Oncologica 2013 & 2014

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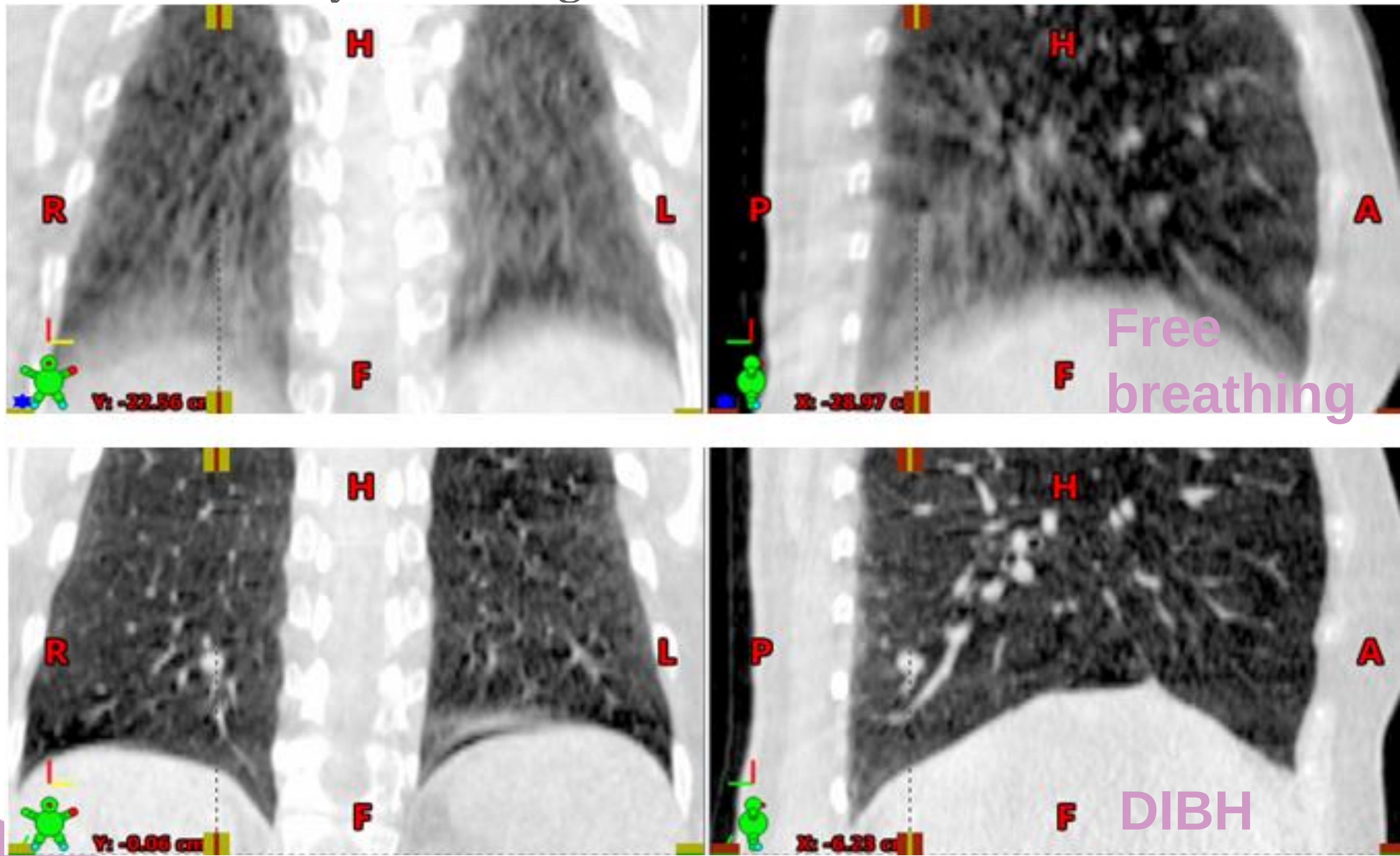
Special case: lung SBRT

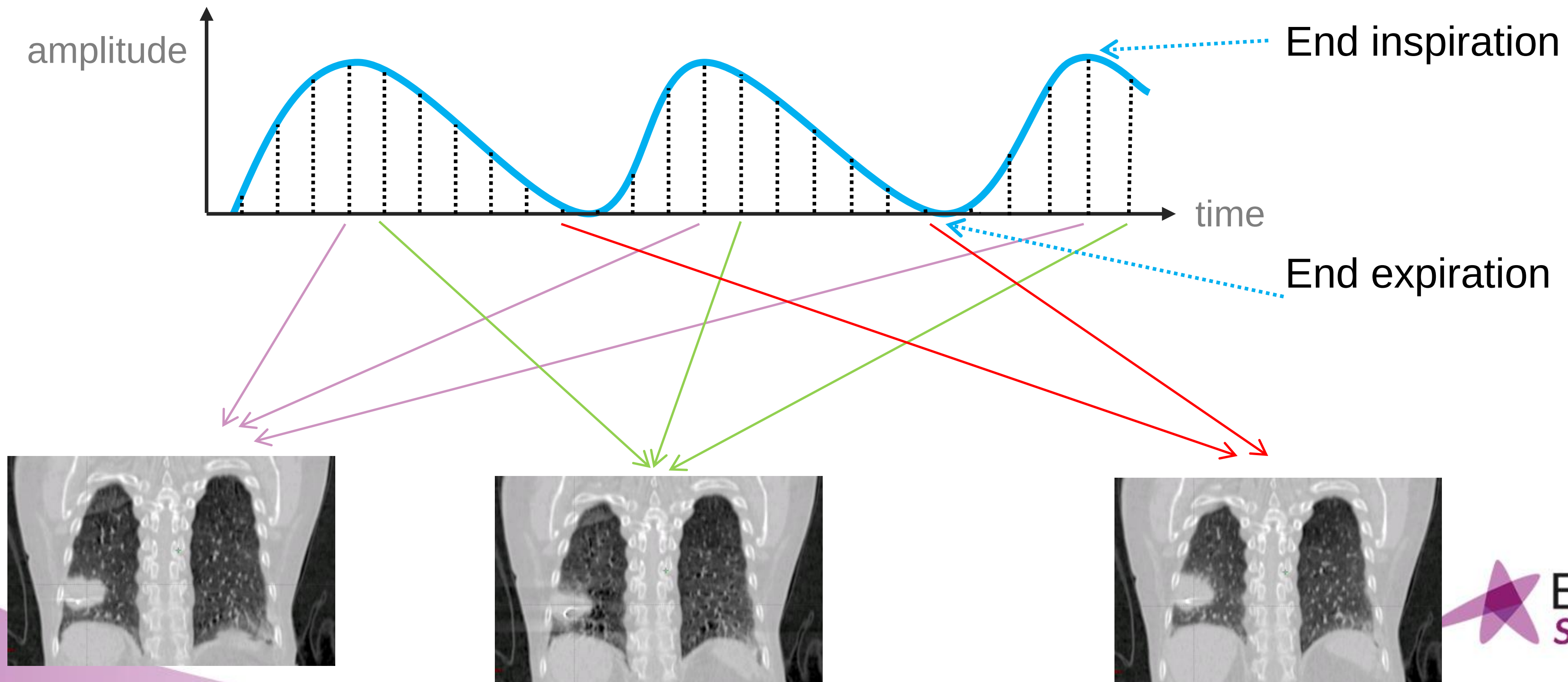
SBRT – very small targets



- DIBH gating is more reproducible than inspiration gating
- DIBH facilitates anatomical separation of target & OAR
- DIBH mitigates target motion

4DCT – a motion encompassing method

- A very slow CT
- Sorting of images acc. to respiration
  - Resp. phase
  - Resp. amplitude



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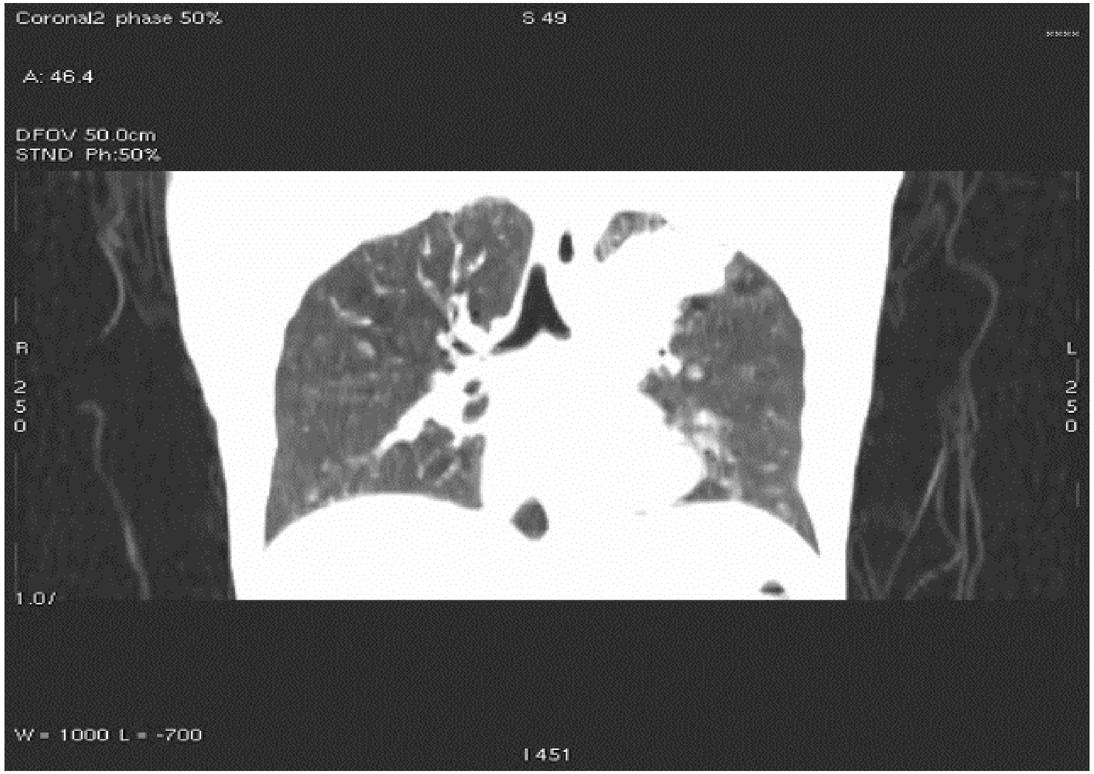
4DCT – a motion encompassing method



Gitte Persson, RH

4DCT facilitates

- Tumour motion evaluation

- Delineation of ITV

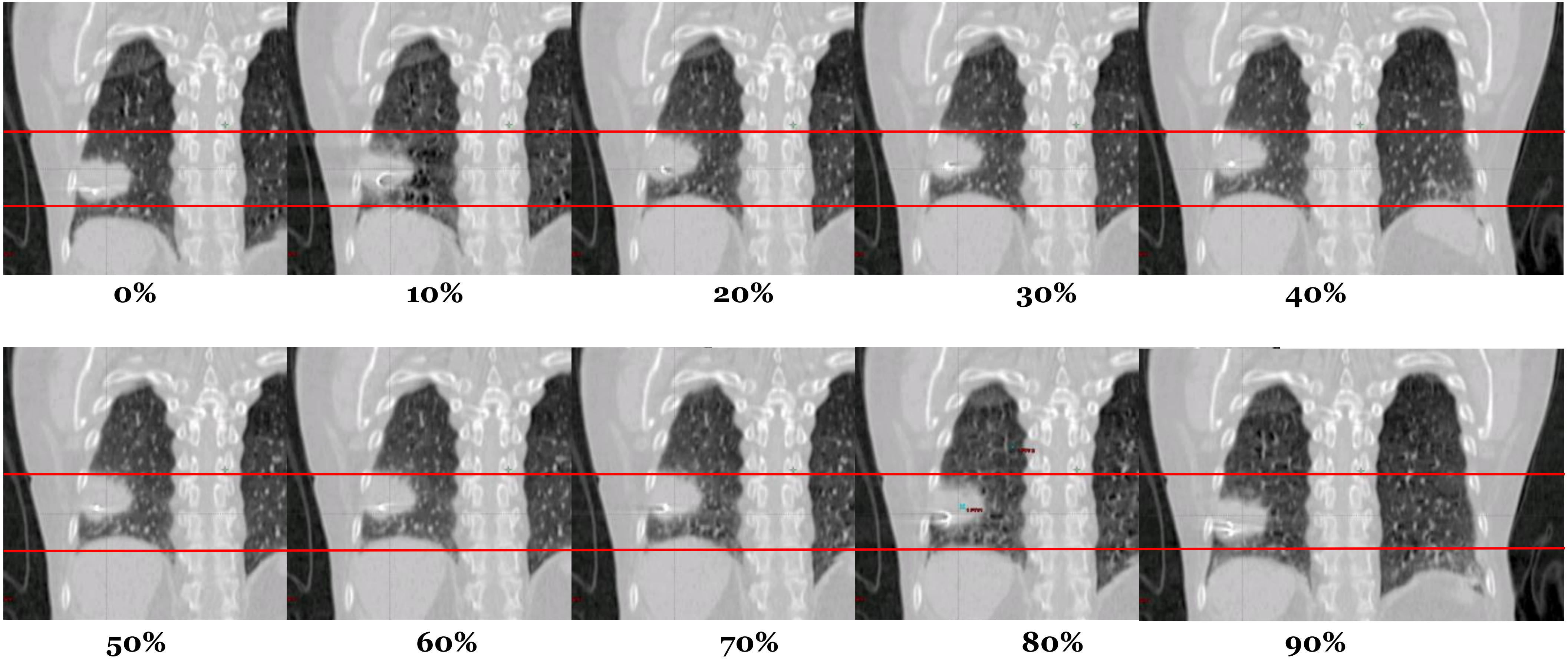
  or

- Selection of midventilation phase

- Correlation of tumour position respiratory phase

- 4DCT is only a snapshot!

4DCT = 10 3D CTs from 10 respiratory phases



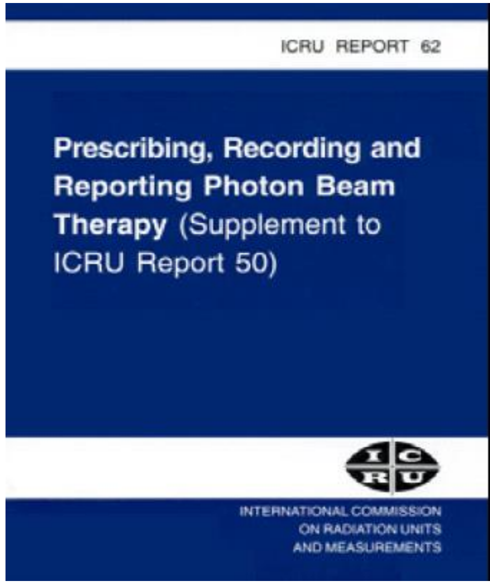
Gitte Persson, Rigshospitalet

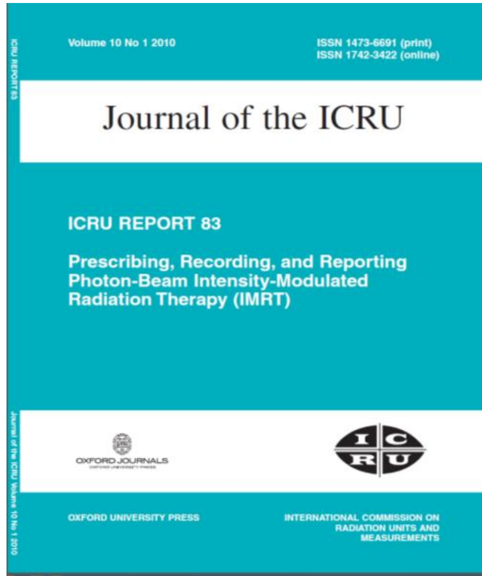
ITV = internal target volume

- ITV = margin for tumor motion added to CTV
- *ICRU 62: ”ITV = CTV + margin for uncertainties in size, shape & position of CTV <u>within</u> the patient”*

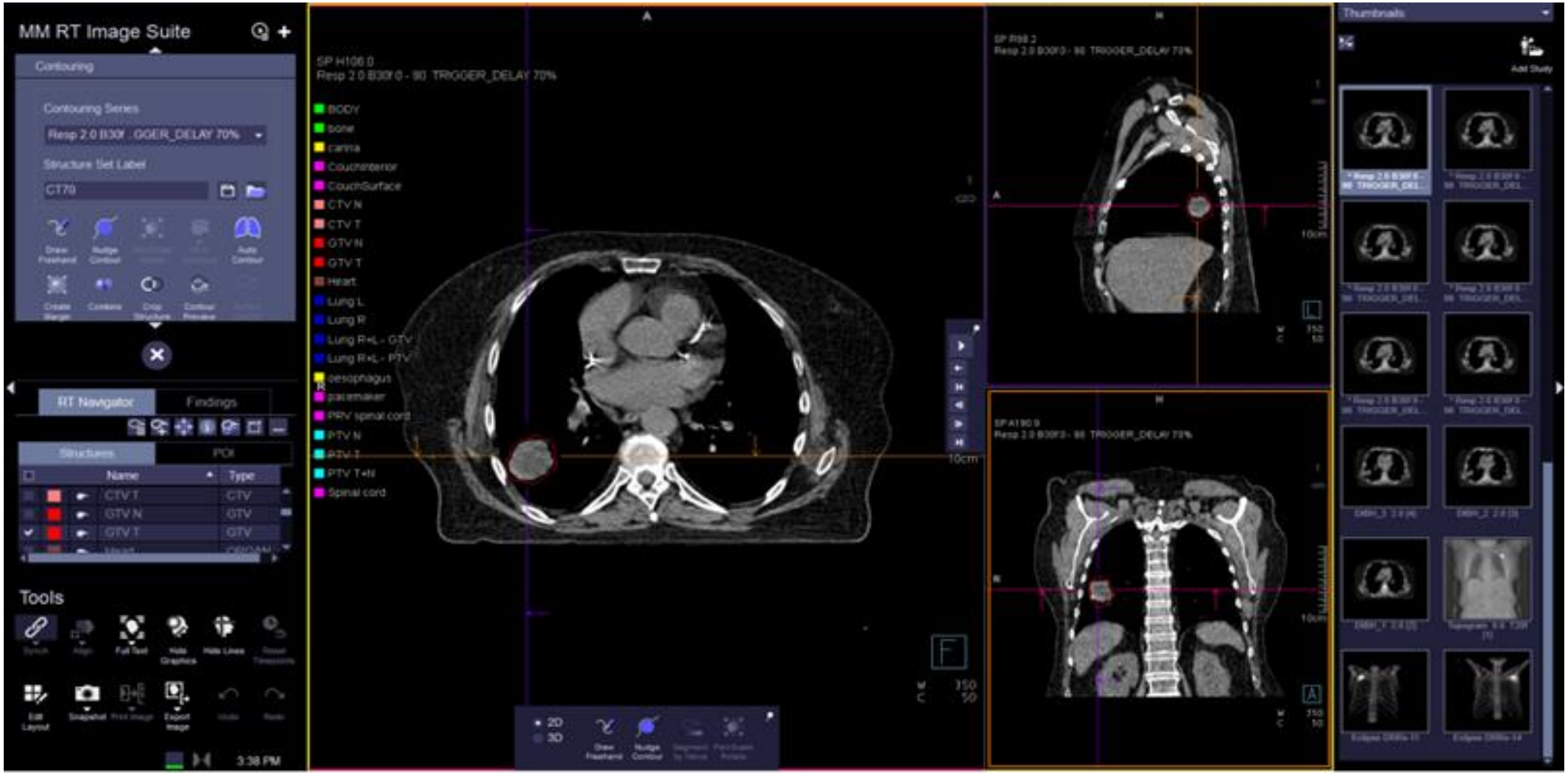
- iGTV = sum of GTVs in al phases of 4DCT

- ICRU 83: *”resulting PTVs were too big”*



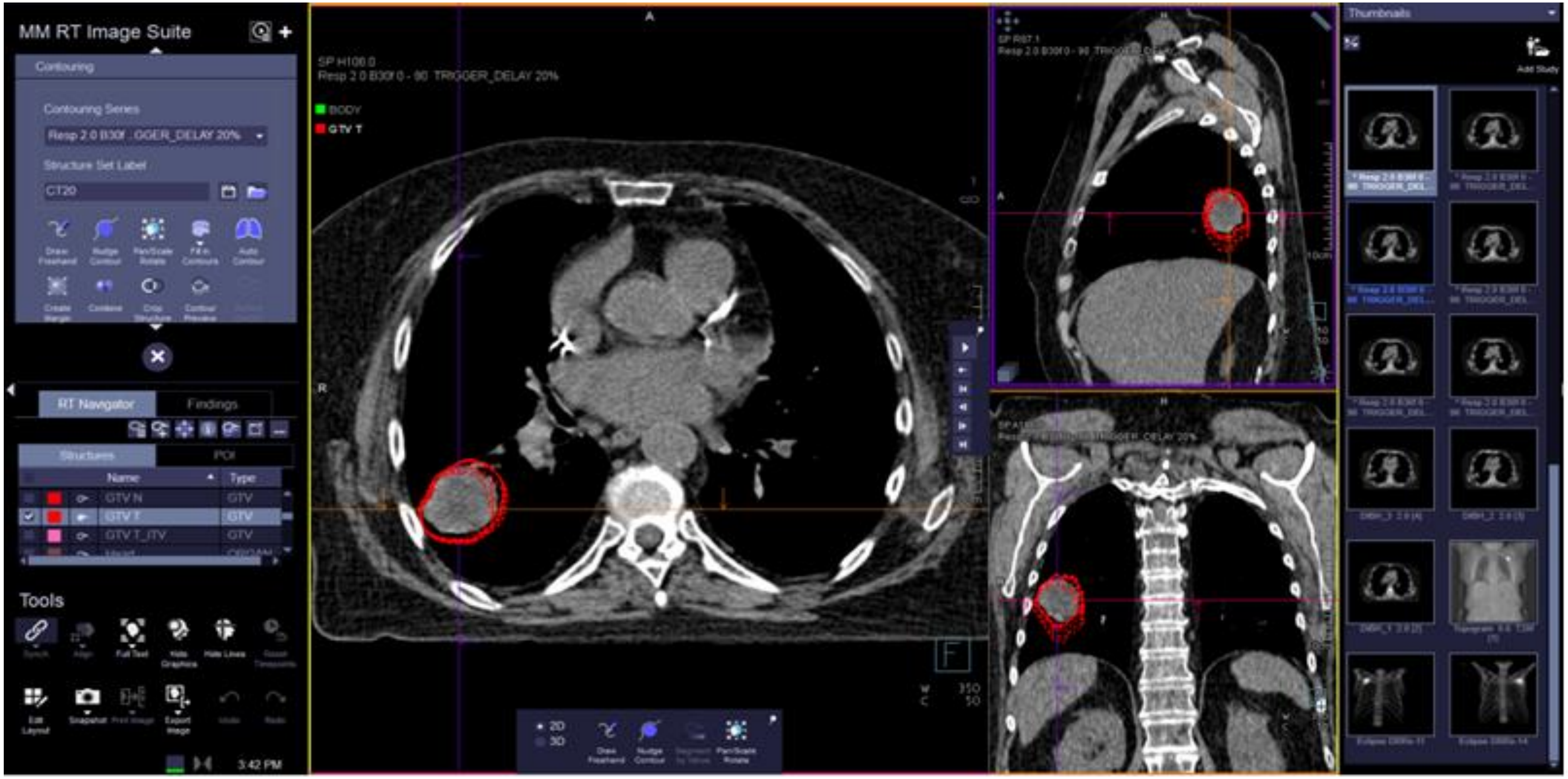


4DCT: ITV-like approach

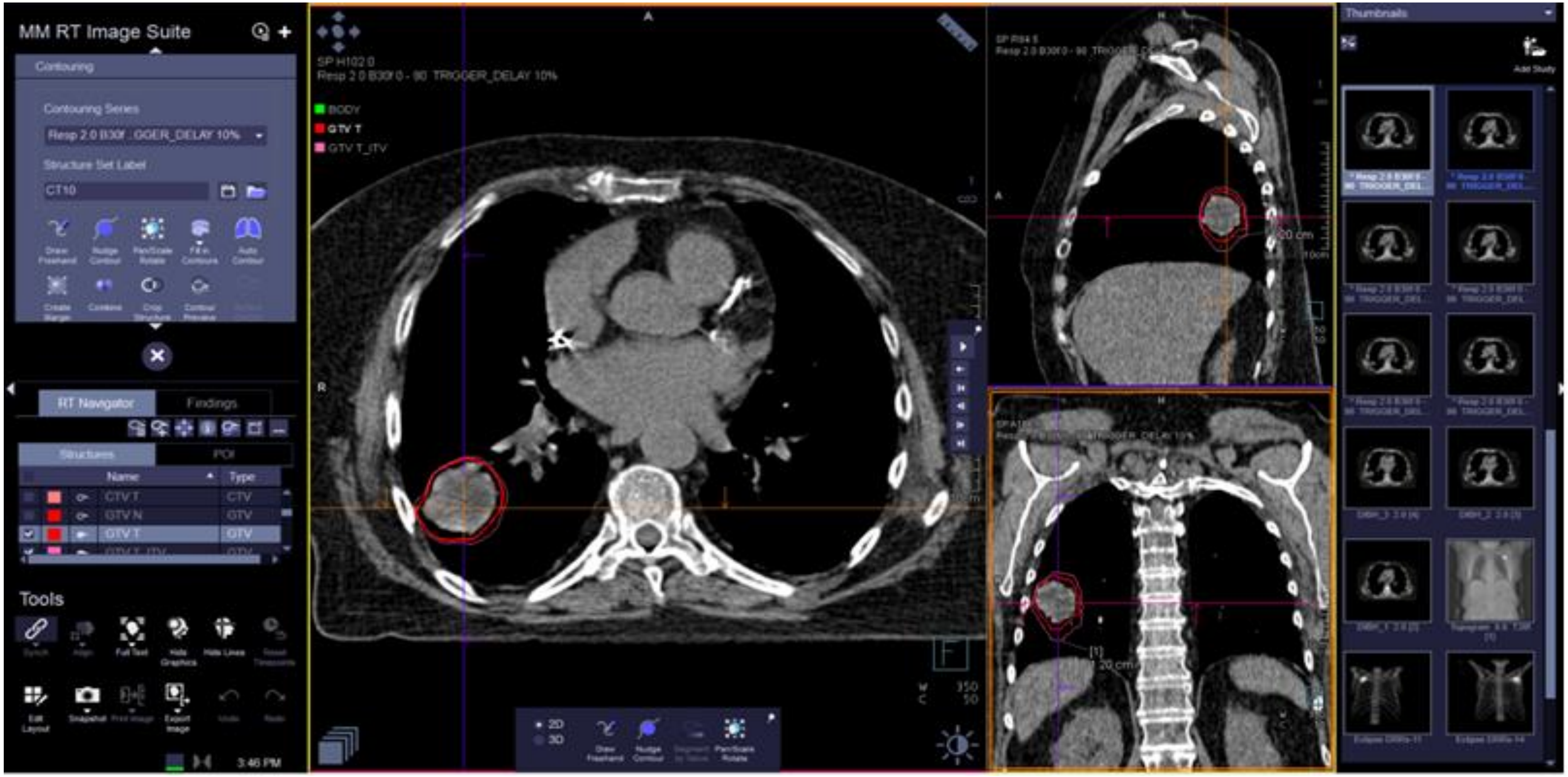


4DCT: ITV-like approach

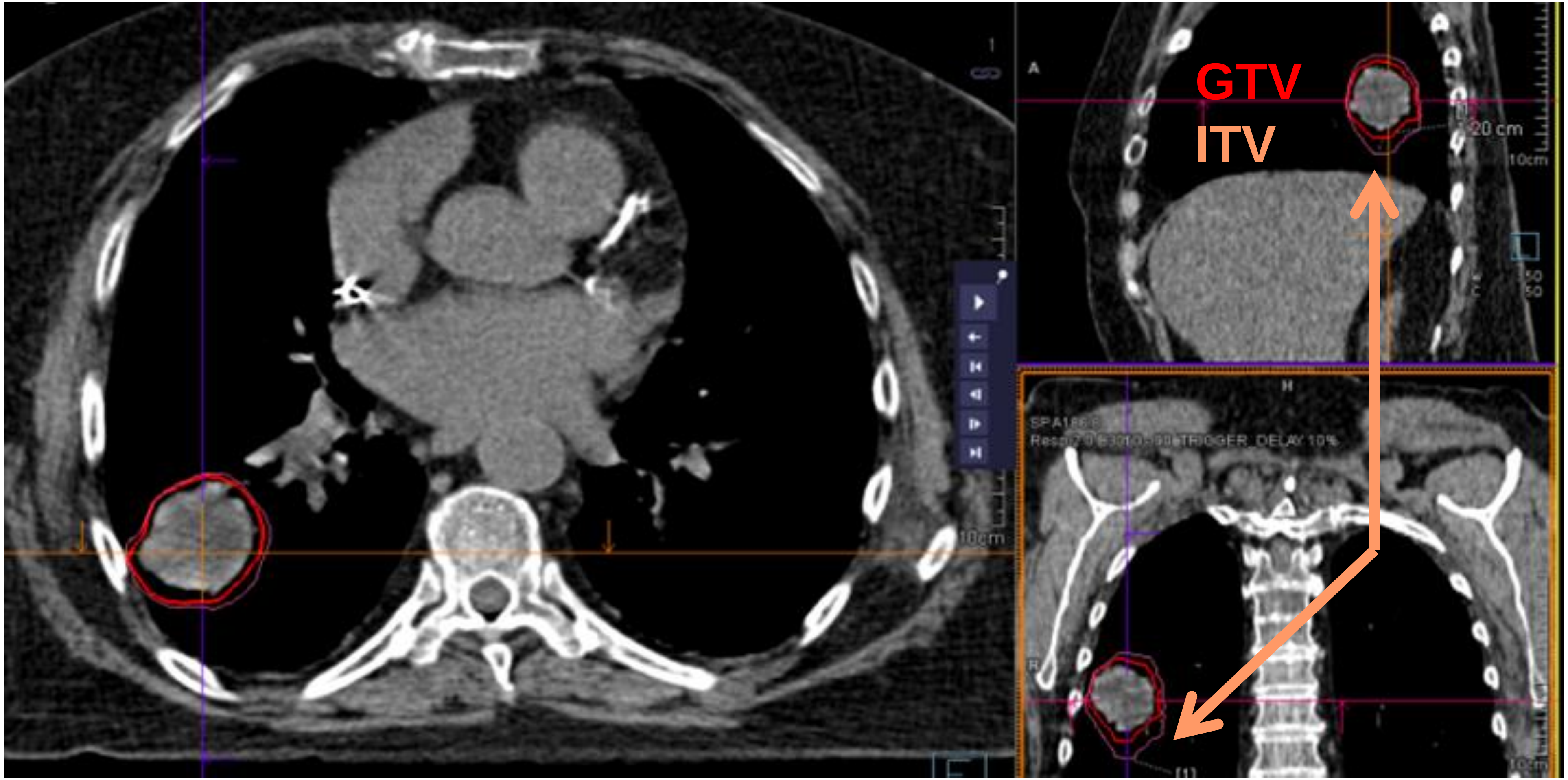
4DCT: ITV-like approach



4DCT: ITV-like approach



4DCT: ITV-like approach



4DCT: Midventilation

ELSEVIER

Int. J. Radiation Oncology Biol. Phys., Vol. 65, No. 5, pp. 1560–1571, 2006

0360-3016/06/$–see front matter

doi:10.1016/j.ijrobp.2006.04.031

PHYSICS CONTRIBUTION

MID-VENTILATION CT SCAN CONSTRUCTION FROM FOUR-DIMENSIONAL RESPIRATION-CORRELATED CT SCANS FOR RADIOTHERAPY PLANNING OF LUNG CANCER PATIENTS

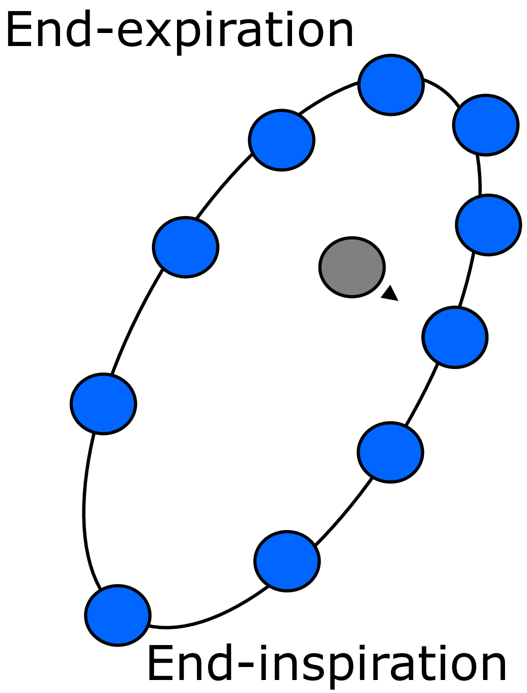
Jochem W. H. Wolthaus, M.Sc., Christoph Schneider, Ph.D., Jan-Jakob Sonke, Ph.D., Marcel van Herk, Ph.D., José S. A. Belderbos, M.D., Maddalena M. G. Rossi, D.C.R.(R), R.T.T., Joos V. Lebesque, M.D., Ph.D., and Eugène M. F. Damen, Ph.D.

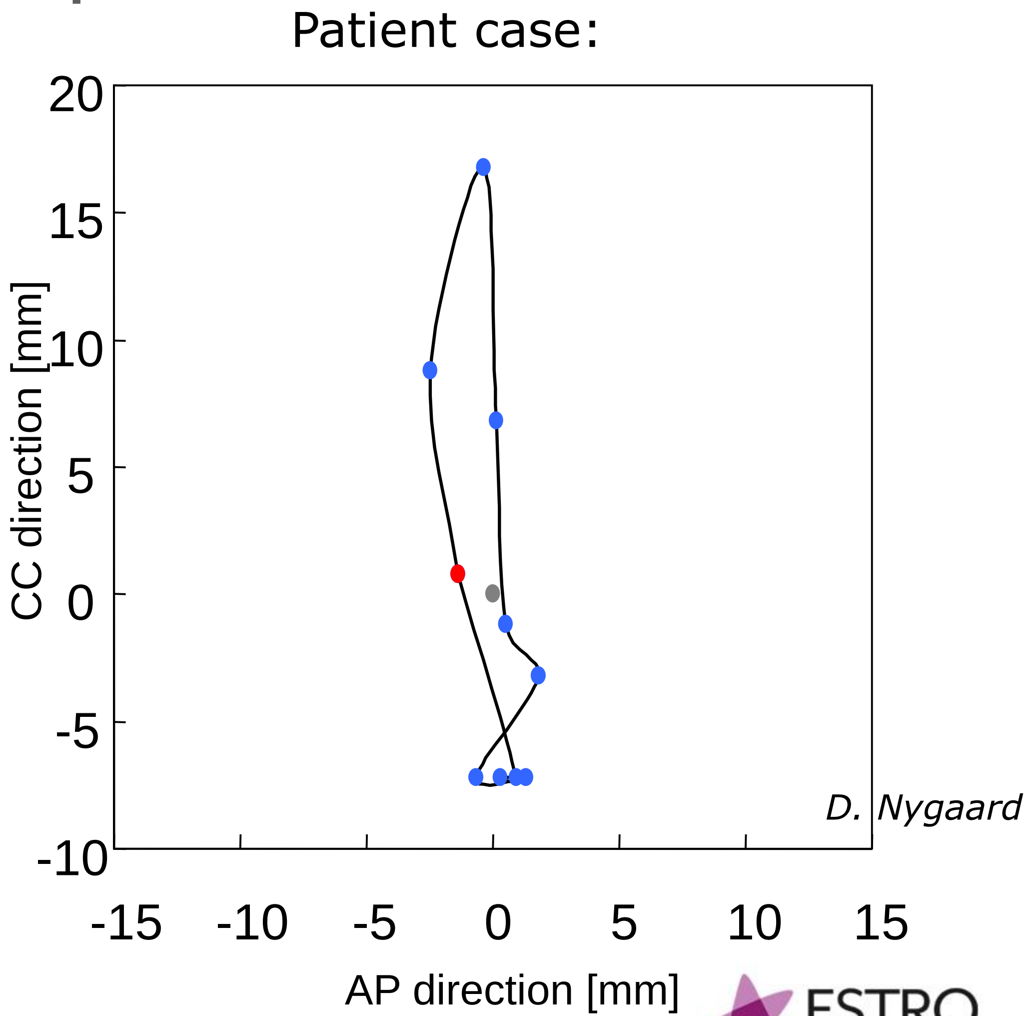
Department of Radiation Oncology, The Netherlands Cancer Institute, Antoni van Leeuwenhoek Hospital, Amsterdam, The Netherlands

Purpose: Four-dimensional (4D) respiration-correlated imaging techniques can be used to obtain (respiration) artifact-free computed tomography (CT) images of the thorax. Current radiotherapy planning systems, however, do not accommodate 4D-CT data. The purpose of this study was to develop a simple, new concept to incorporate patient-specific motion information, using 4D-CT scans, in the radiotherapy planning process of lung cancer patients to enable smaller error margins.

4DCT: Midventilation

= time weighted average position of tumour

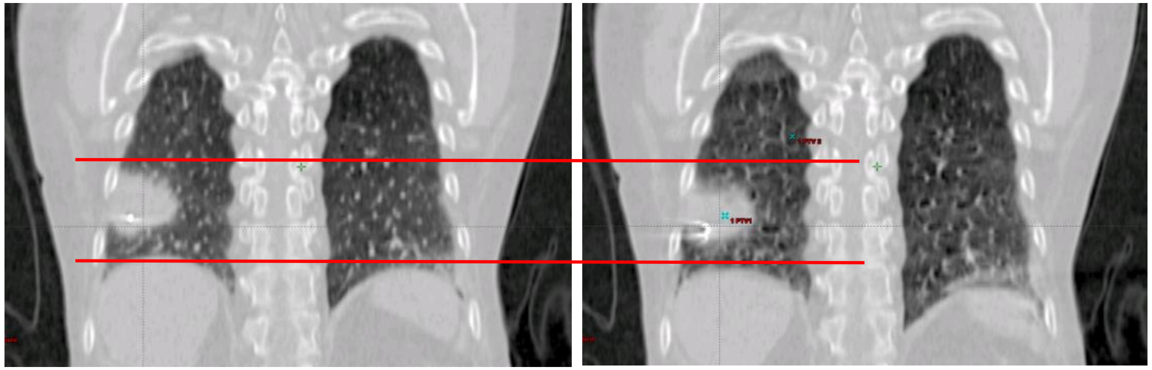




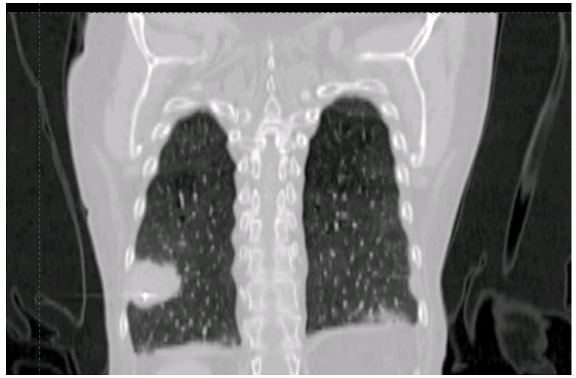
- Tumour position in phases 1-10
- Time weighted average tumor position
- Midventilation

Midventilation

- choice of the correct phase



50% 80%



Breath Hold scan

- Comparisson of tumour size & shape with the breath hold scan

Midventilation vs. midposition

MIDVENTILATION =

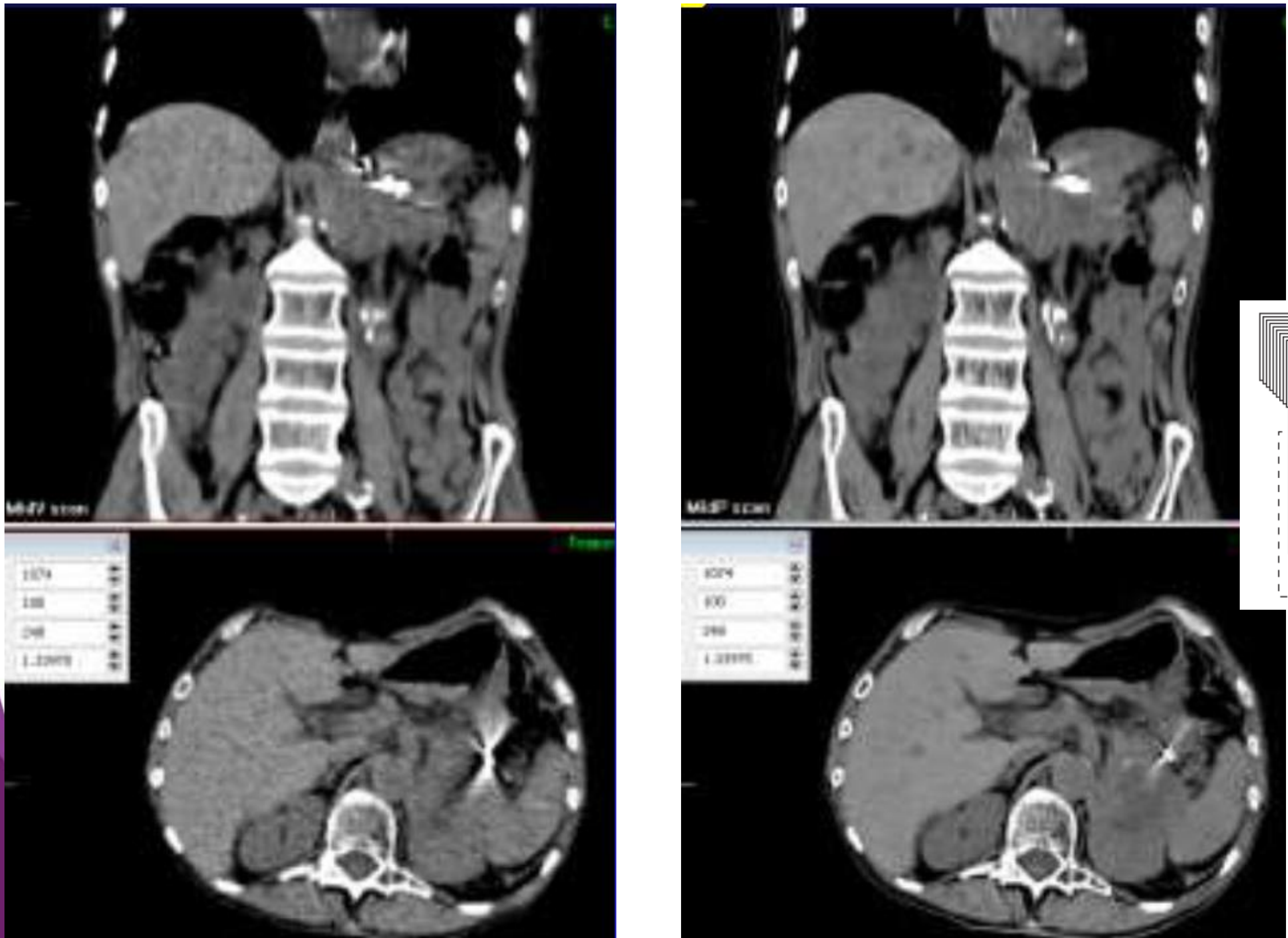
1 phase of the 4DCT

MIDPOSITION =

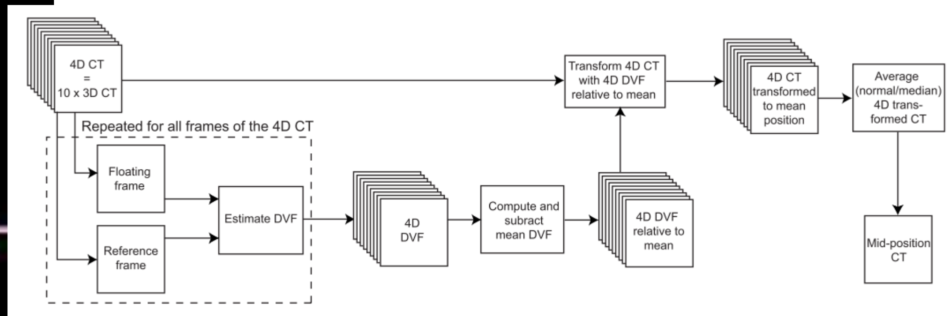
Deformable registration

Deforming phases to time-weighted midposition

Averaging (median)

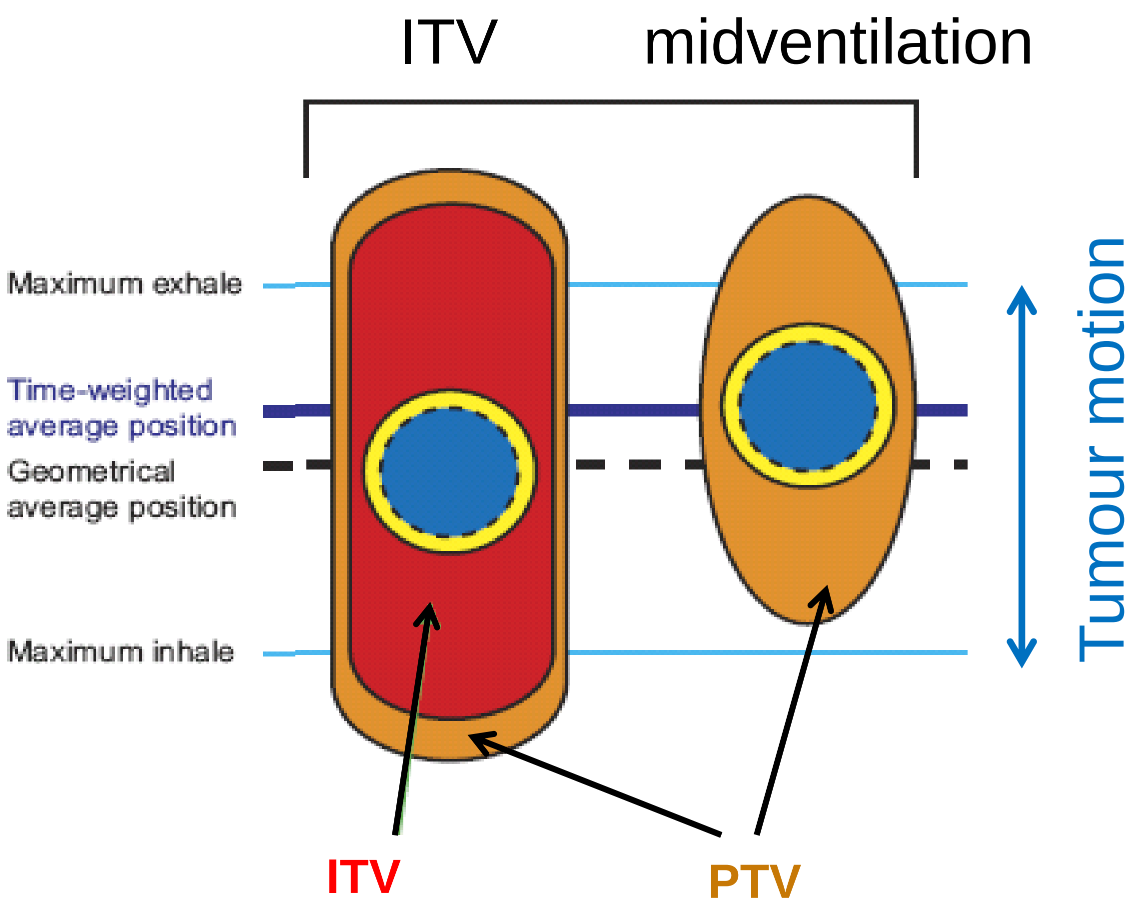


Images courtesy of Marcel van Herk

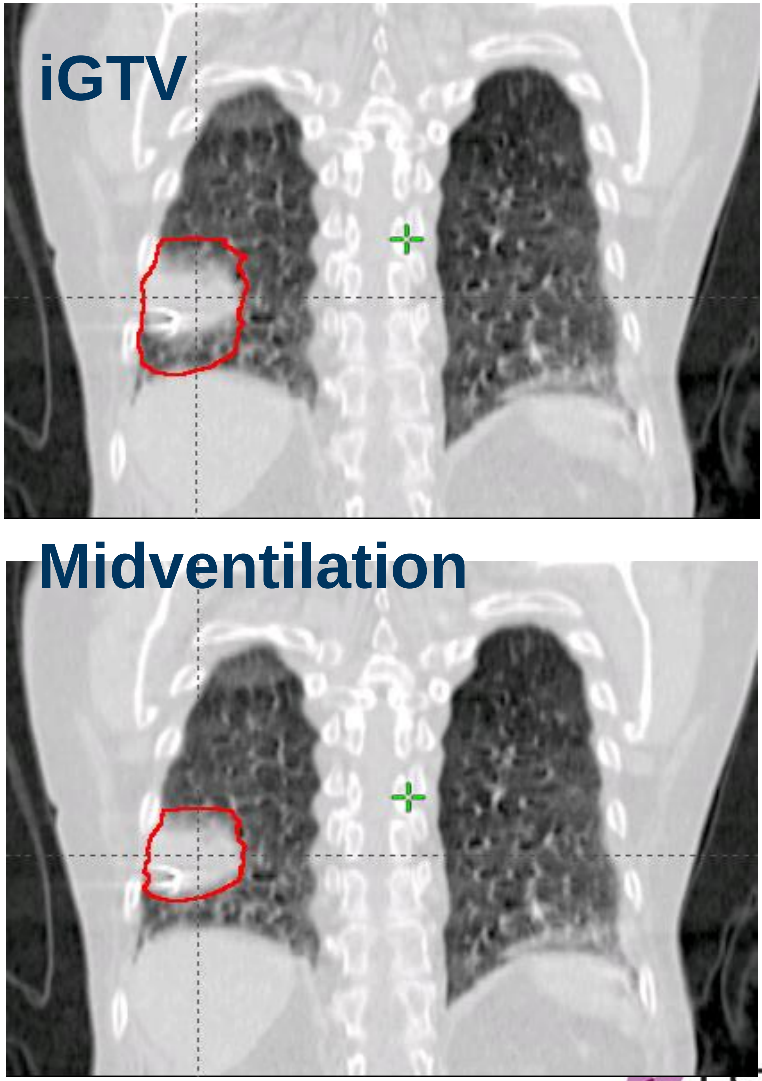


Wolthaus 2008

ITV or midventilation – impact on PTV



adapted from J Wolthaus IJROBP 2008



ITV-like approach

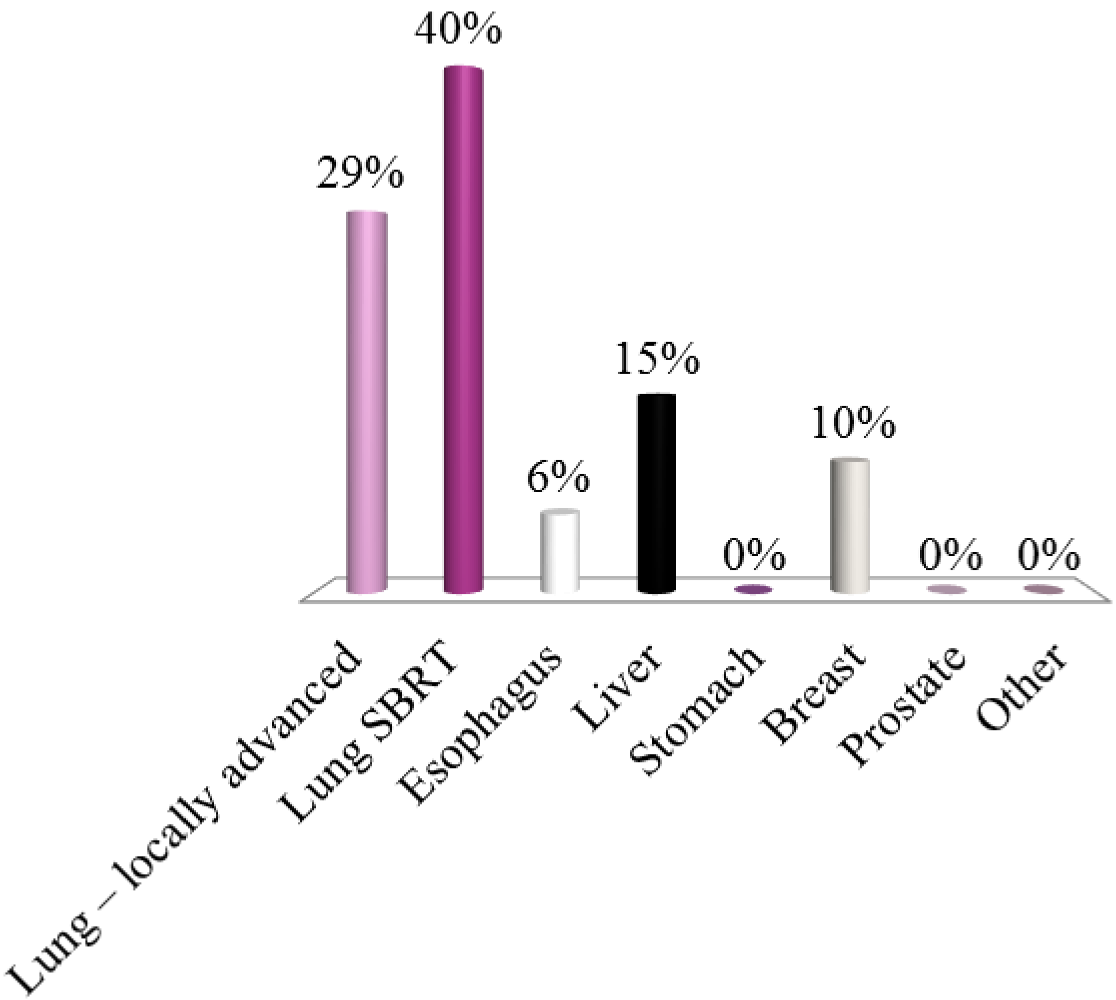
- Larger GTV
- Smaller GTV-PTV margin
- Larger PTV
- Beneficial if hysteresis in tumour motion

Midventilation

- Smaller GTV
- Larger GTV-PTV margin
- Smaller PTV
- Problem if hysteresis in tumour motion

In which sites do you use 4DCT ?

A. Lung – locally advanced
B. Lung SBRT
C. Esophagus
D. Liver
E. Stomach
F. Breast
G. Prostate
H. Other



Respiration synchronised techniques

Rationale of motion tracking…

Letting the beam move with the target

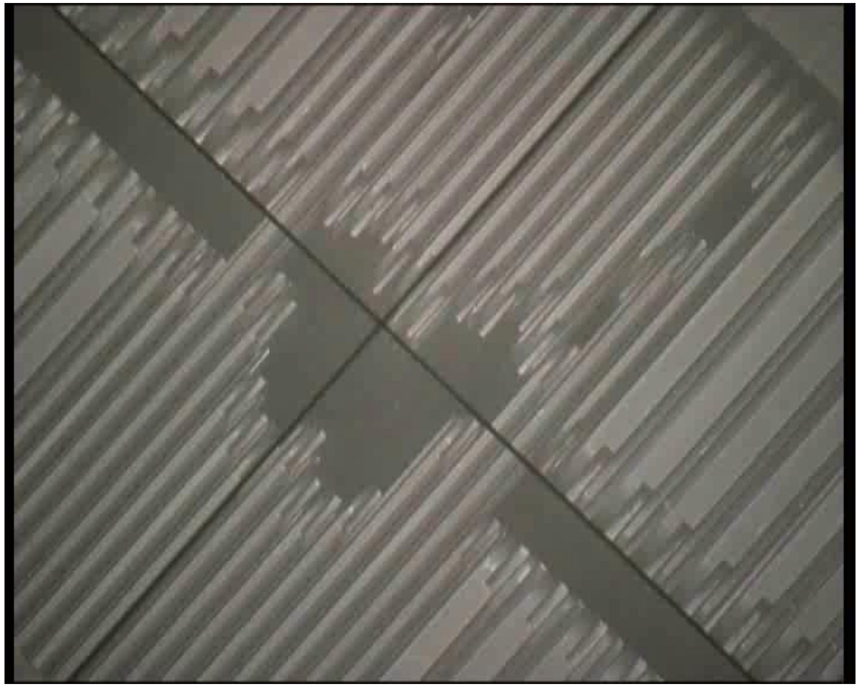
How

- By using surrogate for tumor motion:
  - external or internal
- Prediction algorithms

Respiration synchronised techniques

Tracking on linac

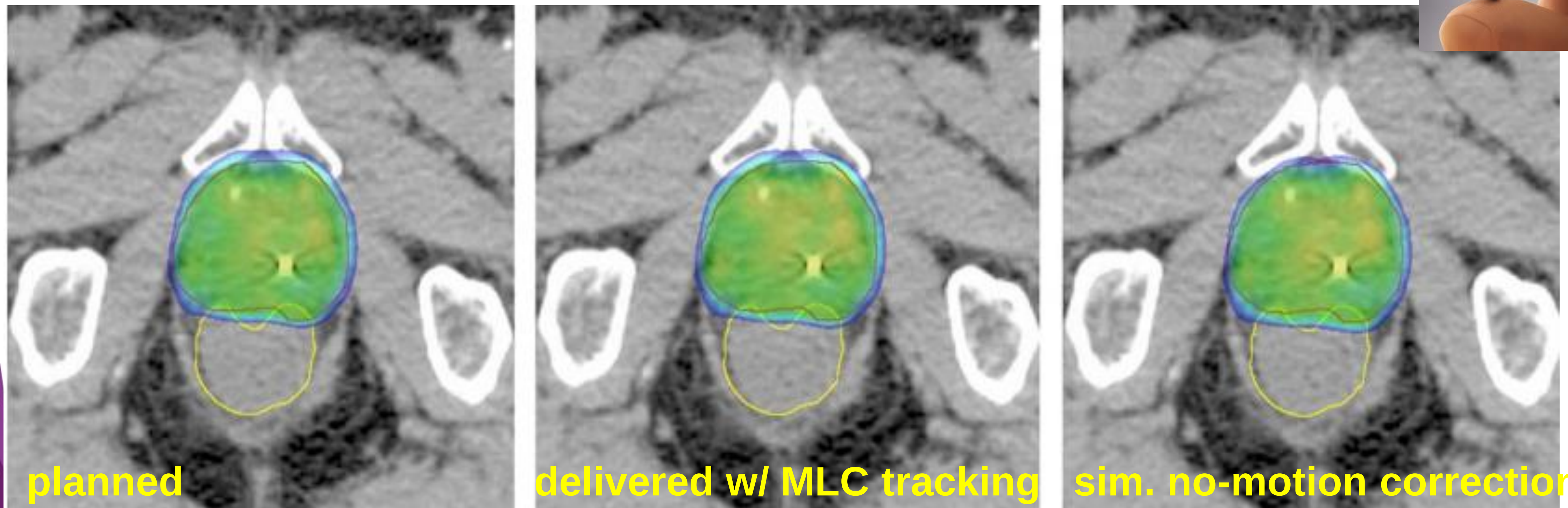
- MLC shape adjusted to compensate for target motion in real-time



You need to KNOW the target motion!

Motion synchronised techniques

First patient treated with electromagnetic transponder MLC tracking



Keall Med Phys 2014

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Take home messages

- Different motion management strategies
  - Gating
  - Breath hold
  - Tracking

  } Dosimetric benefit!
  - 4D imaging
- Good correlation between respiration surrogate & target motion
- Patient training improves reproducibility

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Treatment Planning

Liz Forde, MSc (RTT)
Assistant Professor
Discipline of Radiation Therapy
Trinity College Dublin

ARTT Applied Radiation Therapy Trinity Research Group

Trinity College Dublin
Coláiste na Tríonóide, Baile Átha Cliath
The University of Dublin

Learning Outcomes

- Discuss the role of the RTT in the treatment planning process
- Discuss key concepts of ICRU 50, 62 and 83
- Identify key features of inverse planning techniques
  - IMRT
  - VMAT
- Identify evidence for the use of inverse planning
- Describe the inverse planning process for IMRT and VMAT
- Describe the importance of target and organ definition and it's impact on the inverse planning process
- Review the benefits of inverse planning to "non standard" sites

RTT Lead Planning

- Scope of practice may vary significantly
- Often seen as a "Specialist role"
  - Rotations may be limited
- Regardless of level of involvement in planning, a basic understanding of key principles increase your ***"clinical intelligence"***

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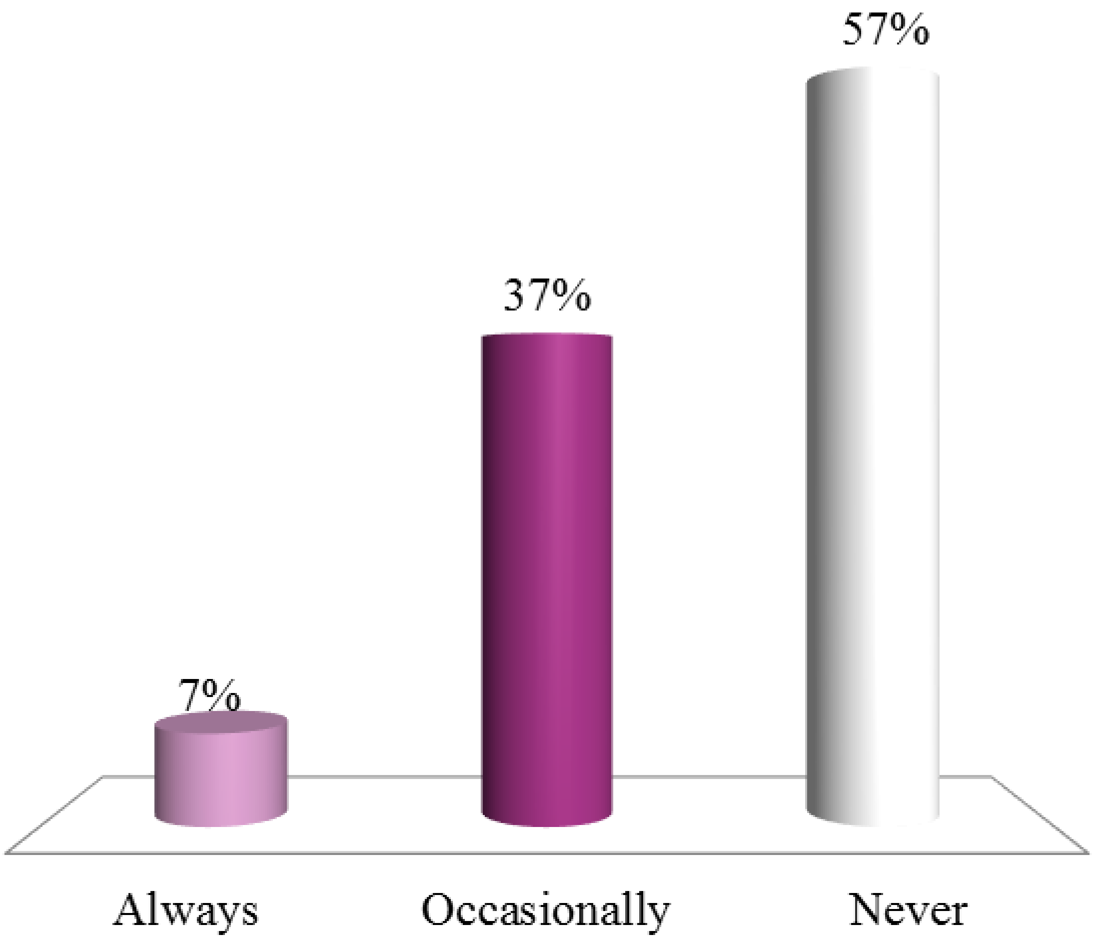
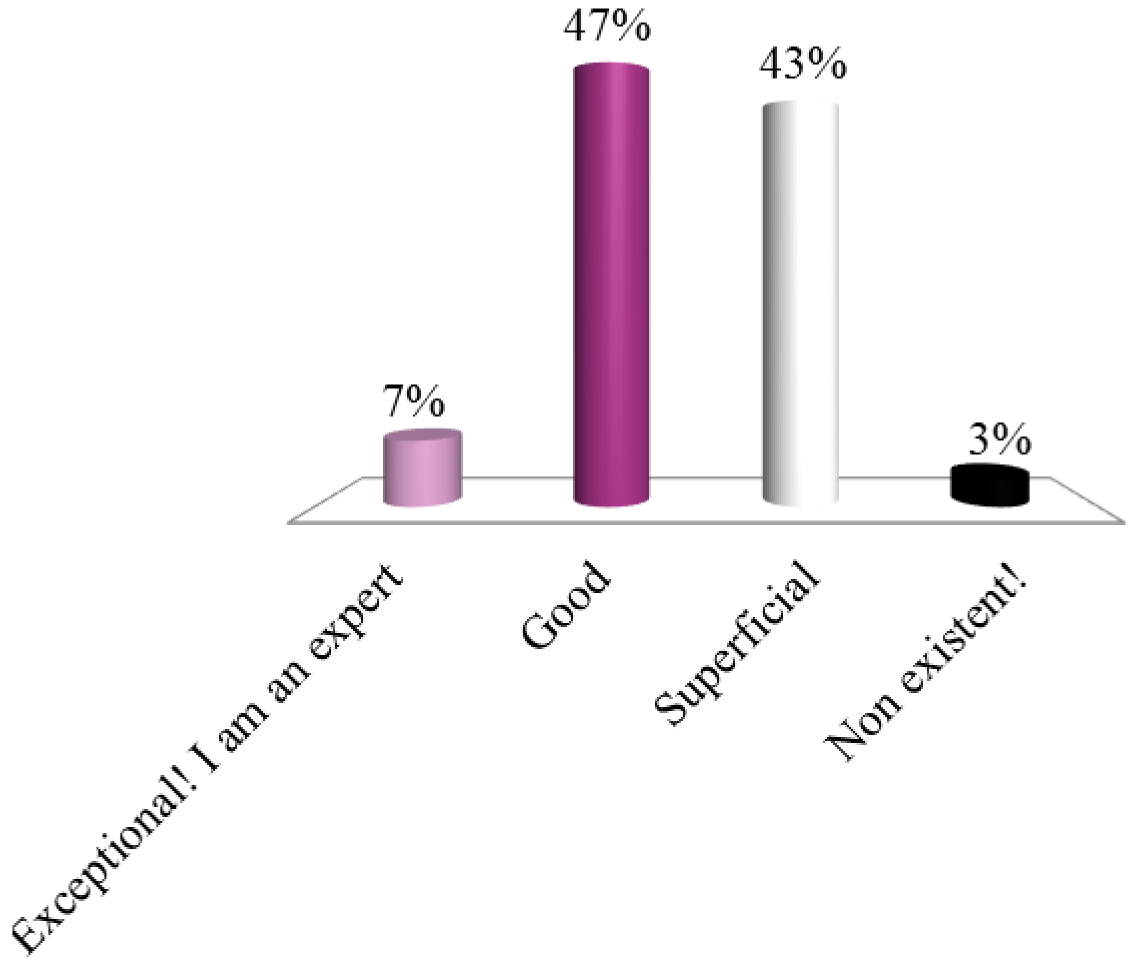
In my work, I am involved in treatment planning:

A. Always
B. Occasionally
C. Never



My knowledge and understanding of treatment planning and theoretical concepts is:

A. Exceptional! I am an expert
B. Good
C. Superficial
D. Non existent!



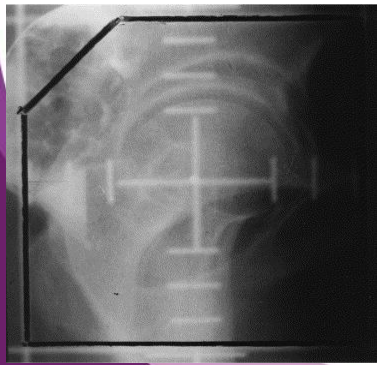
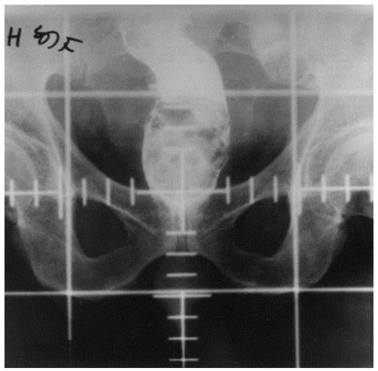
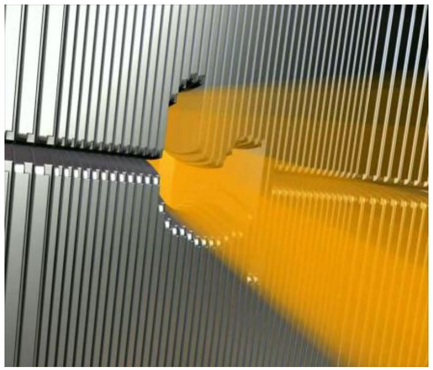
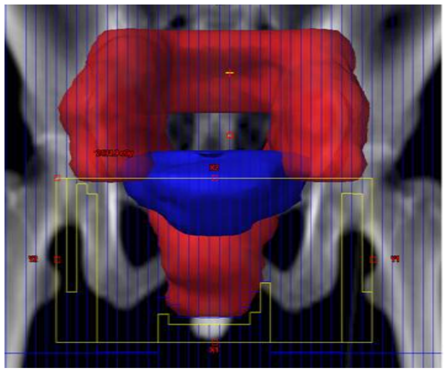
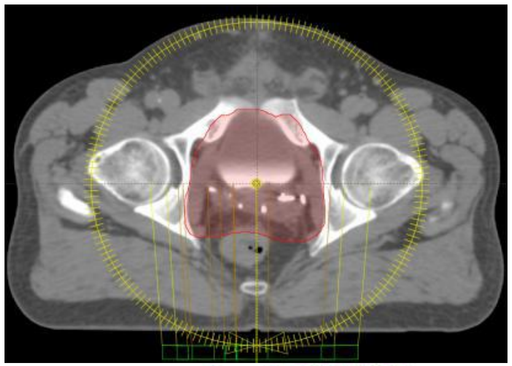
Planning: Where are we now?

- Technology boom

- From 2D to 3D
- From 3D to 4D, ART and tumour tracking

- From block shielding to conformal shielding
- From conformal shielding to dynamic shielding

- Inverse planning allows for greater control

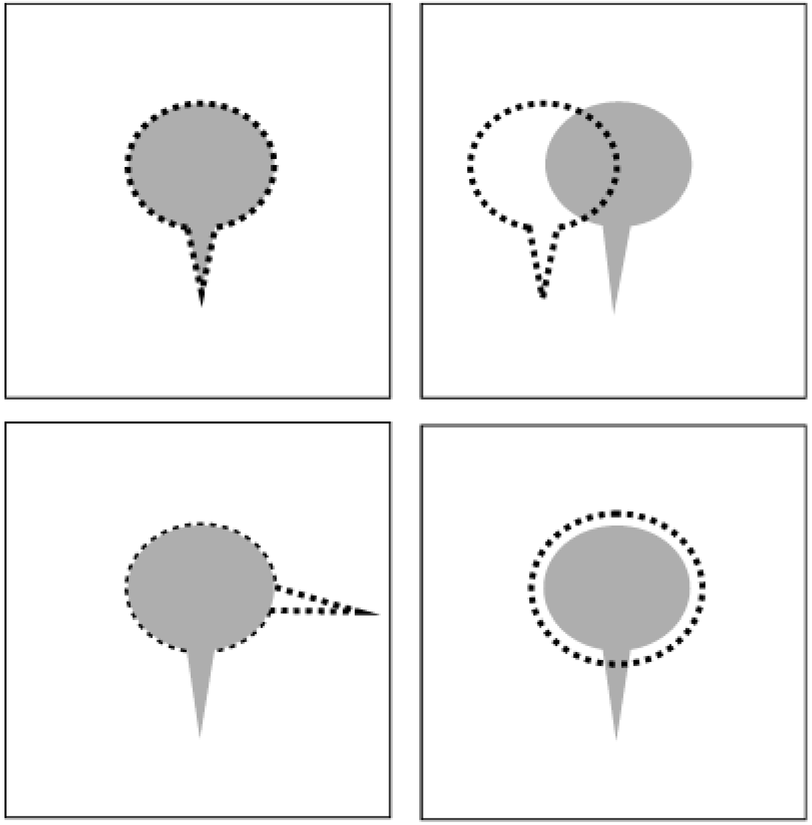






Inverse Planning: Is the "Evidence" There?

- Understanding the Literature and the Evidence
- Caution!
  - Small patient numbers
  - Retrospective in nature
  - Important to recognise fundamental differences in planning techniques between centres
    - Target dose and coverage stipulated
      - ICRU Pt or Volumetric
    - OAR constraints (protocol or department specific)
    - Beam energy
    - Number of fields/arcs
    - Planning system used
      - Sliding window vs. step and shoot IMRT

"it is important that clear well defined unambiguous, and universally accepted concepts and terminology are used to ensure a common understanding" *(ICRU 62)*

ICRU 50	ICRU 62
• GTV • CTV • PTV • Irradiated Volume • Treated Volume • OAR • ICRU reference point • Dose heterogeneity • (>95%, <107%)	• Reference points • Coordinate Systems • PRV • ITV • CI



Feuvret et al., 2006

ICRU 50	ICRU 62	ICRU 83
• GTV • CTV • PTV • Irradiated Volume • Treated Volume • OAR • ICRU reference point • Dose heterogeneity • (>95%, <107%)	• Reference points • Coordinate Systems • PRV • ITV • CI	• Detailed labelling of structures • Volumetric prescription • Median dose (D50%) • Near min (D98%) • Near max (D2%) • CI (again) • HI

The Need for Standardised Reporting

- Green Journal Editorial, 2013 *(Yartsev, Muren and Thwaites)*

- Planning papers are interesting to everyone (RO, MP and RTTs)

- Pick up practical tips and share outcome data ***BUT…***

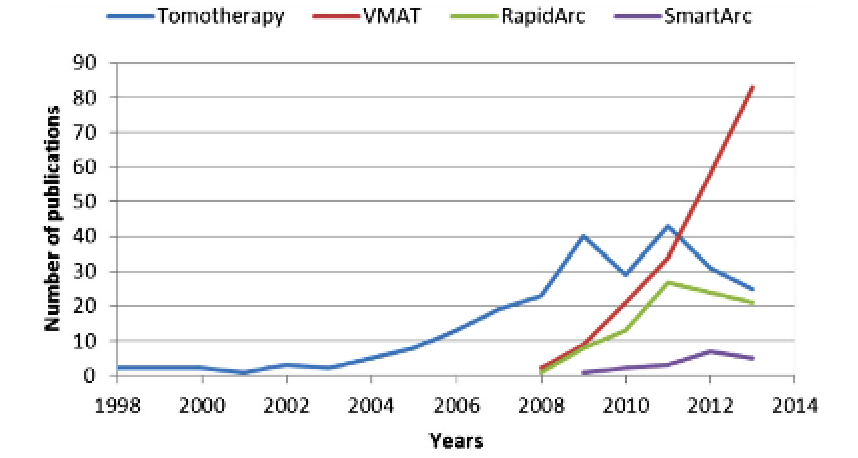


Fig. 1. Number of publications per year for rotational IMRT planning studies. (The data for 2013 is limited to 11 months.)

A third group of readers includes treatment planners who need solid information about the details of the planning procedure applicable to the current case. Unfortunately, there is a variety of definitions and a confusion in terminology that makes it difficult to compare publications of plans performed by different groups. For example, we have found nine different definitions used to describe conformity of the prescribed dose to the target, and seventeen (!) for the homogeneity of dose distribution within the target. The included DVHs should be reproduced in high-quality, allowing for exact numerical values to be derived. It is also essen-

Adherence to ICRU 83 Reporting

- 48 IMRT or VMAT papers published from 2010 – 2015 were analysed *(A Mohan and E Forde, 2017 - Publication currently under review)*

- 22.9% reported PTV D2%
- 18.8% reported PTV D98%
- 8.3% reported PTV D50%

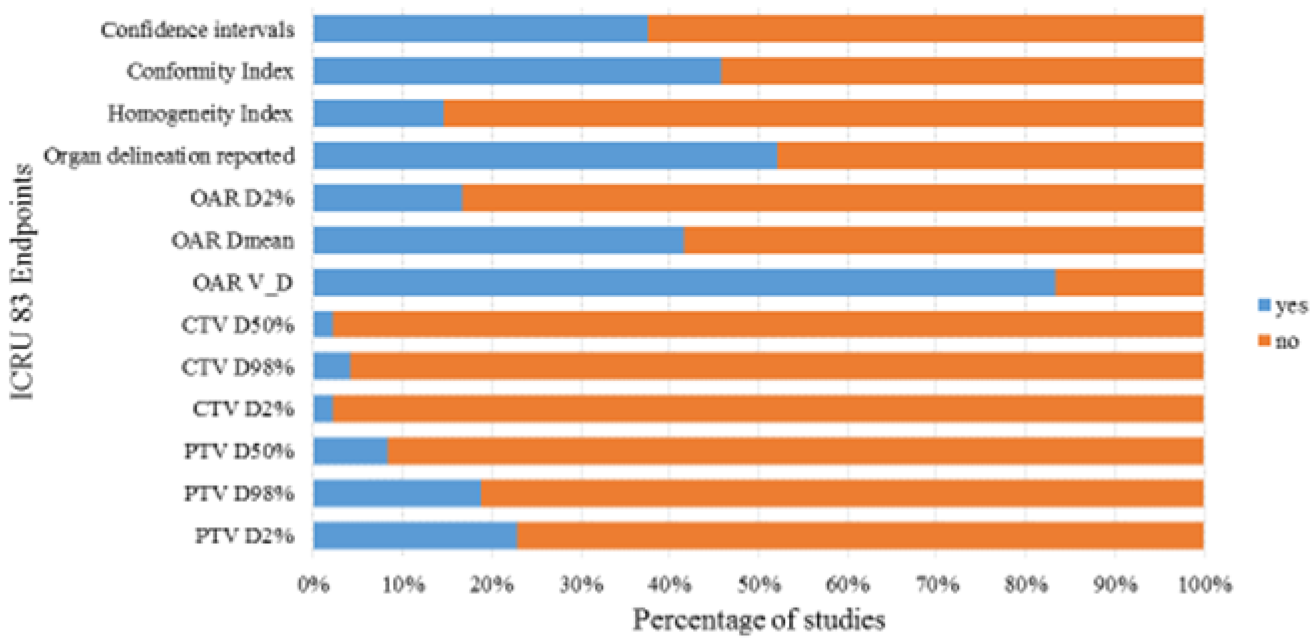


Figure 1 shows the proportion of studies which followed the ICRU 83 Report recommendations for modulated plans.

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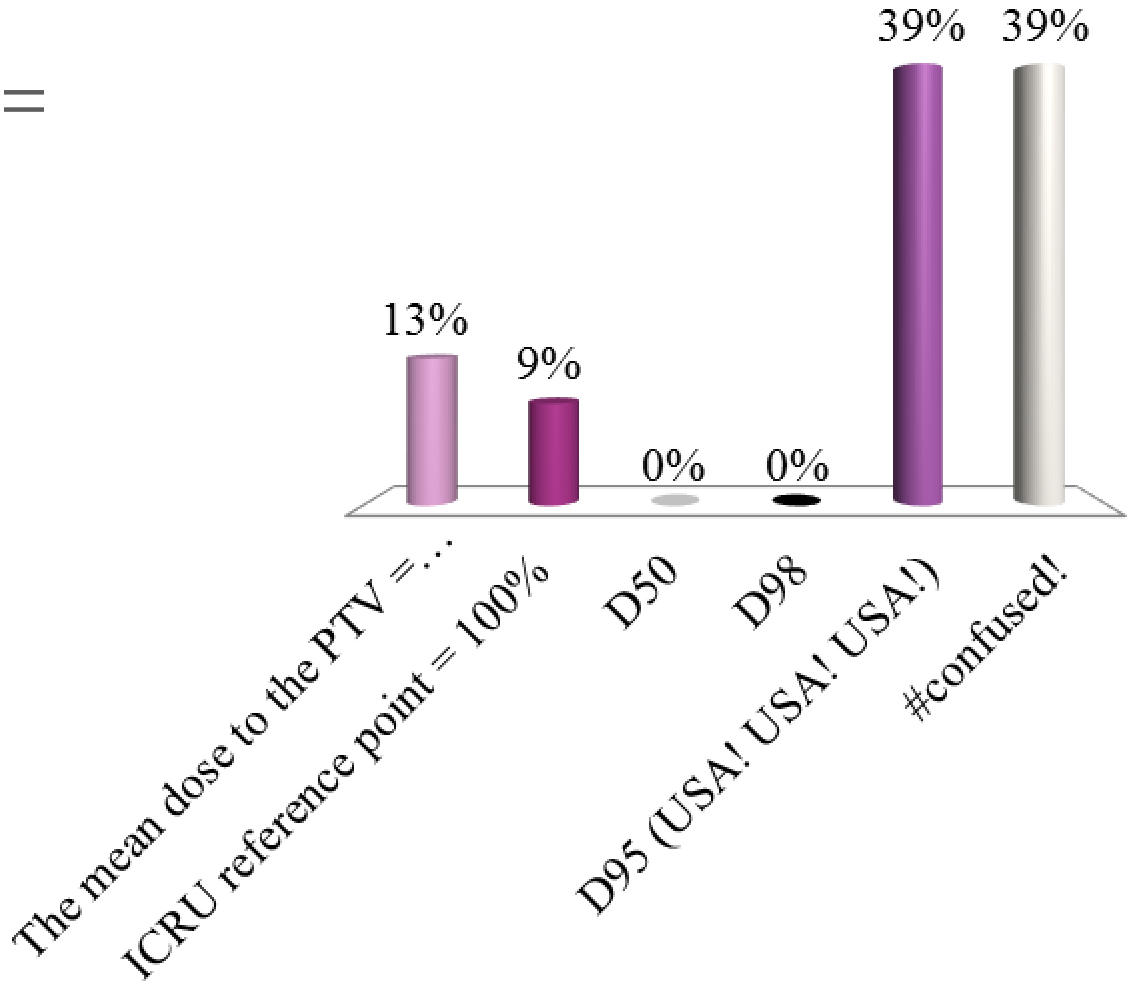
Fine, But What is Happening in Clinical Practice?

- Survey of 10 Academic Institutions in The US (Das et al., **2017**)
- *"Nearly 95% of patient treatments deviated from the ICRU-83 recommended D50 prescription dose delivery."*
- The majority of institutions appear to be prescribing to D95

In my department we prescribe our IMRT/VMAT prostate plans to:

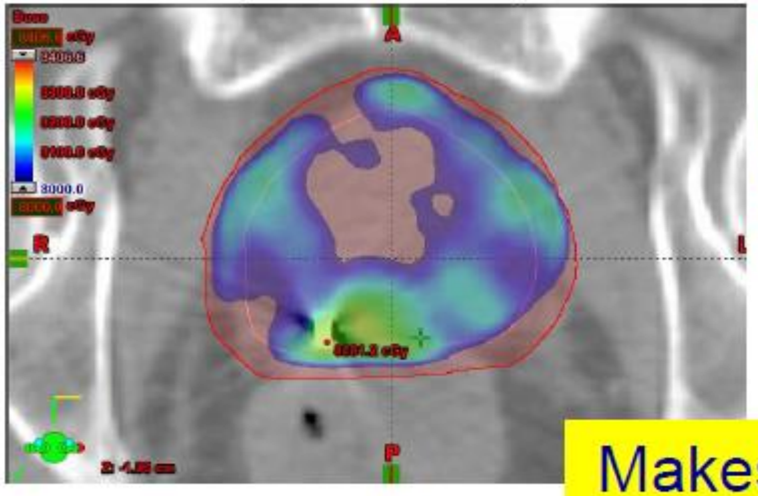
A. The mean dose to the PTV = 100%
B. ICRU reference point = 100%
C. D50
D. D98
E. D95 (USA! USA! USA!)
F. #confused!



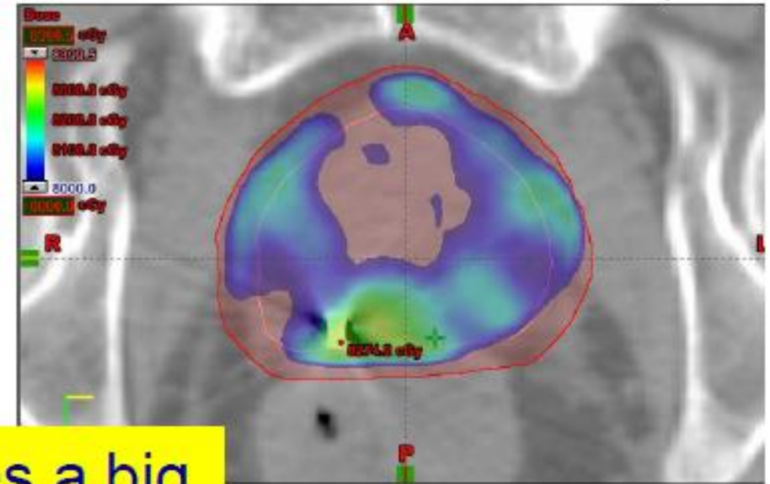
Plan Normalisation

What happened to ICRU 83?

ICRU point = 80Gy

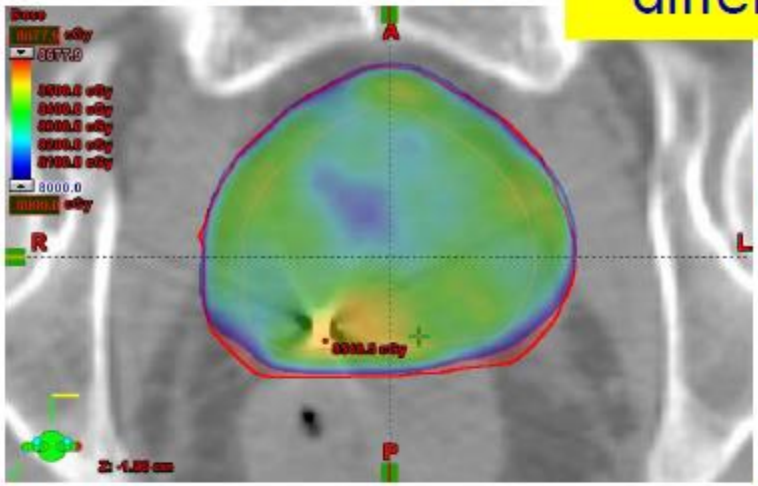


Mean dose = 80Gy

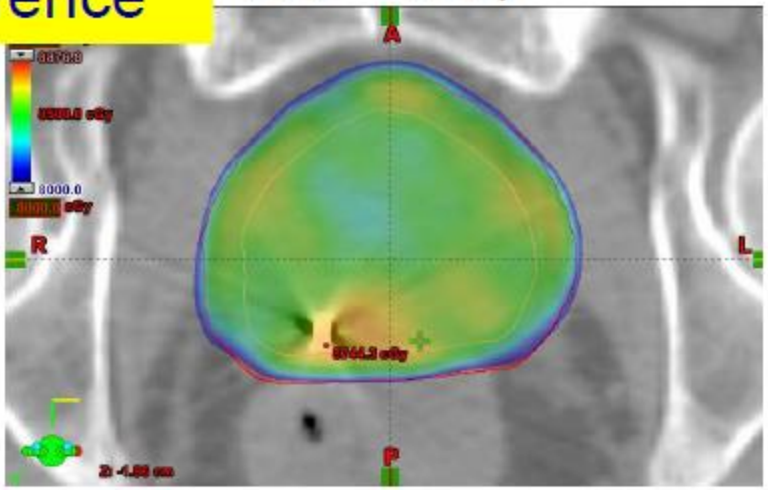


Makes a big difference

D95 = 80Gy



D98 = 80Gy



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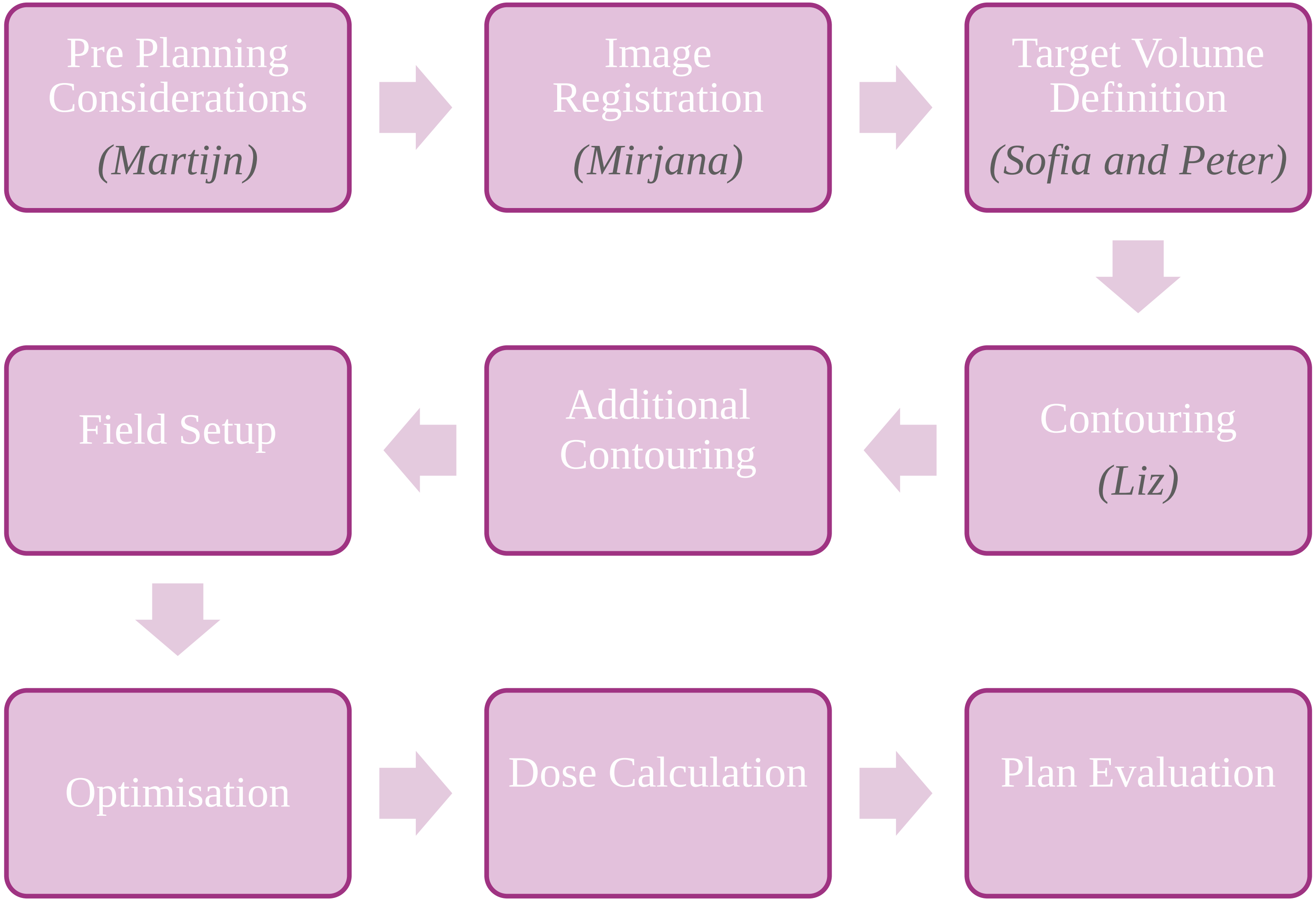
The Planning Process

What do you think is missing from this flowchart?

Field Setup

Optimisation → Dose Calculation → Plan Evaluation

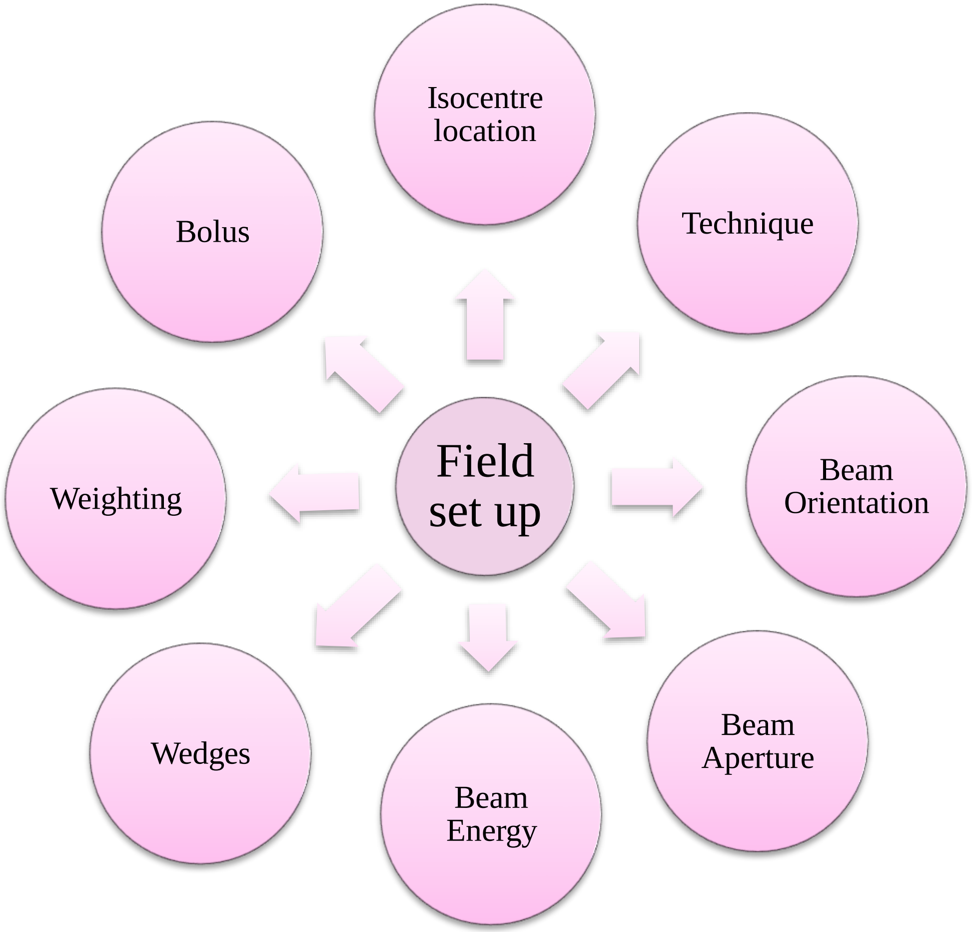
This is a dynamic process


Pre Planning Considerations
(Martijn)
Image Registration
(Mirjana)
Target Volume Definition
(Sofia and Peter)
Contouring
(Liz)
Additional Contouring
Field Setup
Optimisation
Dose Calculation
Plan Evaluation

Key Concepts of 3DCRT

- Field set up… *“Finally we get to put some beams on!”*

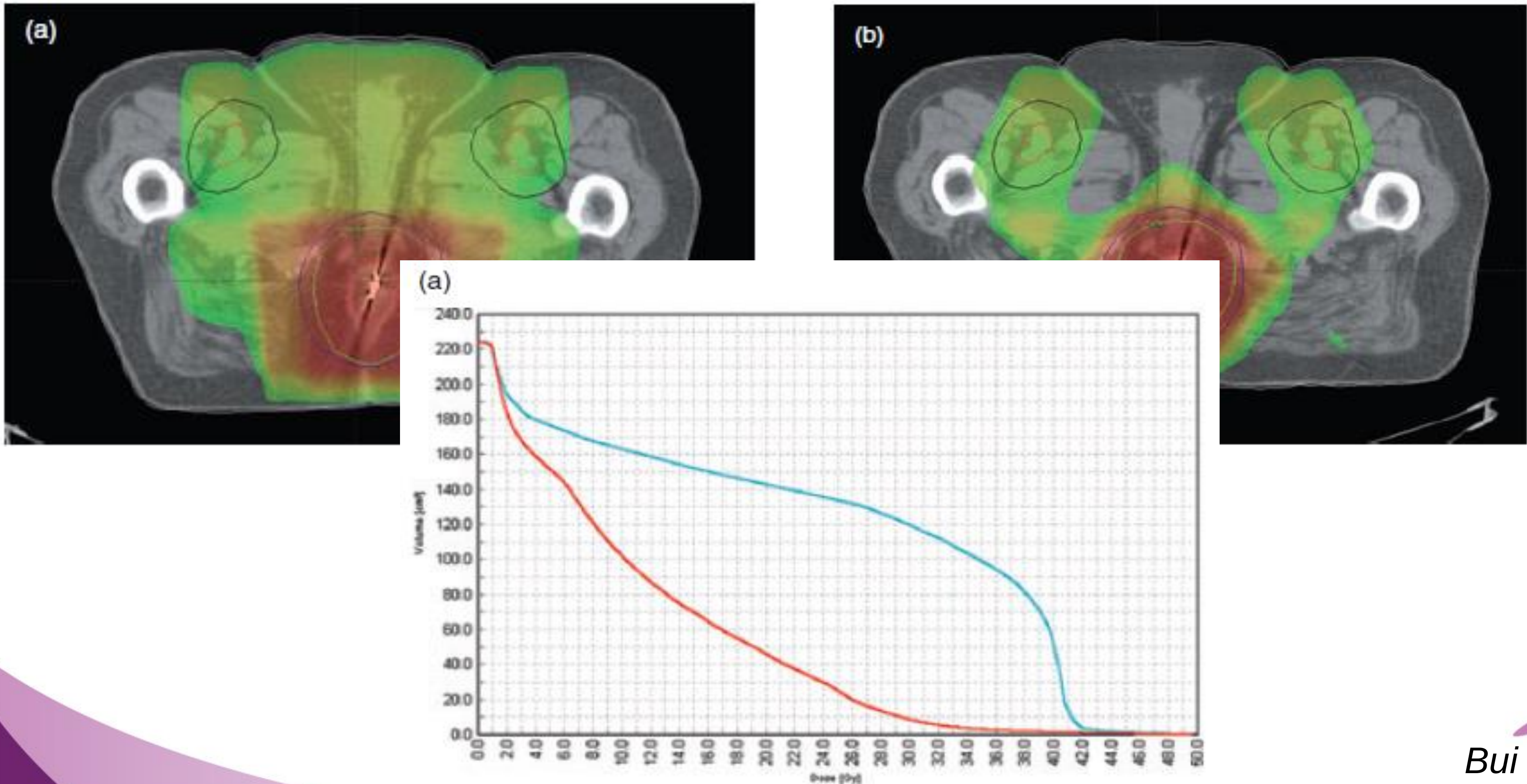
- User defines:



Planning Techniques Explored...

- With 3D targets now being delineated, 3DCRT techniques have become more complex

- “Genital sparing” technique



Bui et al., 2009

Key Concepts of 3DCRT

- But…
- How many fields are we up to now?
- ***Enter IMRT…***

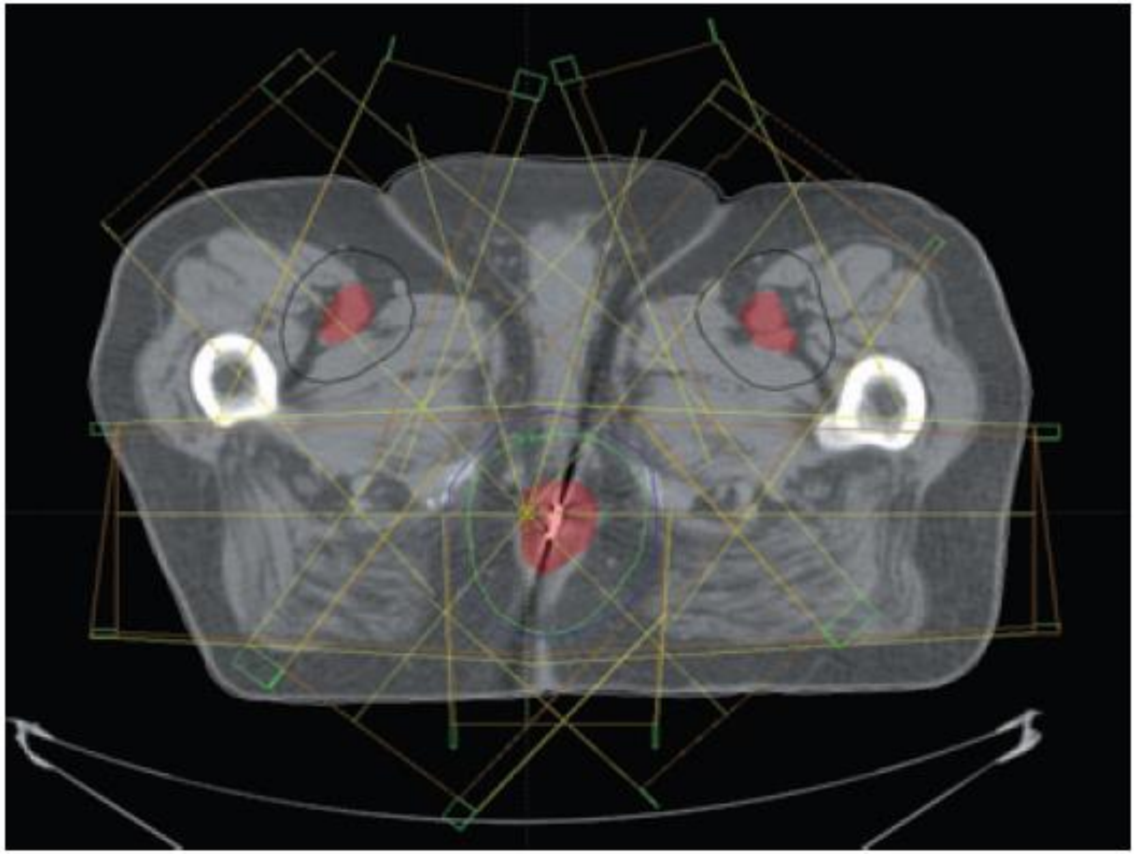


Fig. 2. Example of three-dimensional conformal radiotherapy technique field arrangement. Gross tumour anus and inguinal, red; planning target volume (PTV) anus, green; PTV inguinal, black; PTV pelvis, dark blue.

Bui et al., 2009

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Key Concepts of IMRT

- The multiple-static-field MLC technique
  - ➢ Step and Shoot
- The dynamic MLC technique
  - ➢ Sliding Window
- Intensity modulated arc therapy
  - ➢ IMAT
- Intensity modulated proton therapy
  - ➢ IMPT

- *“IMRT requires expertise and careful target design to avoid reduction in local control by marginal miss”* *(NCCN 2013)*

Key Concepts of IMRT

- IMRT is the delivery of radiation to the patient via fields that have a non-uniform radiation distribution across a field.
- Progression from geometric to **fluence** shaping of a field

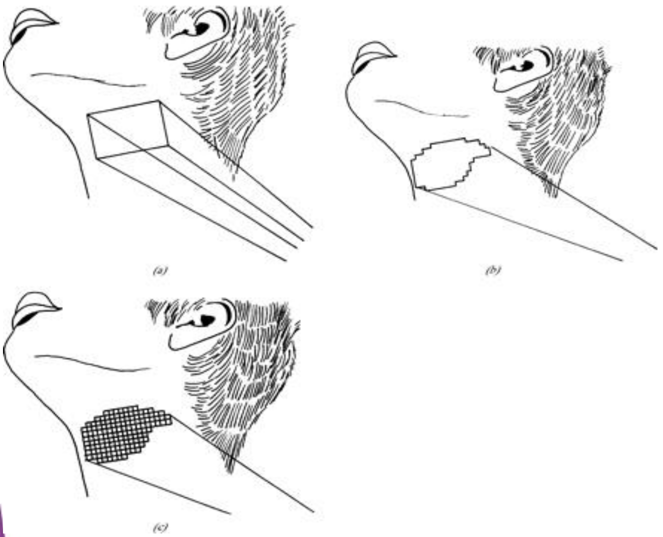
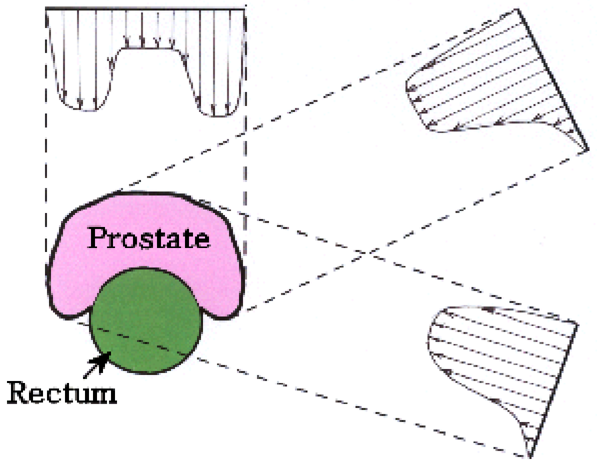
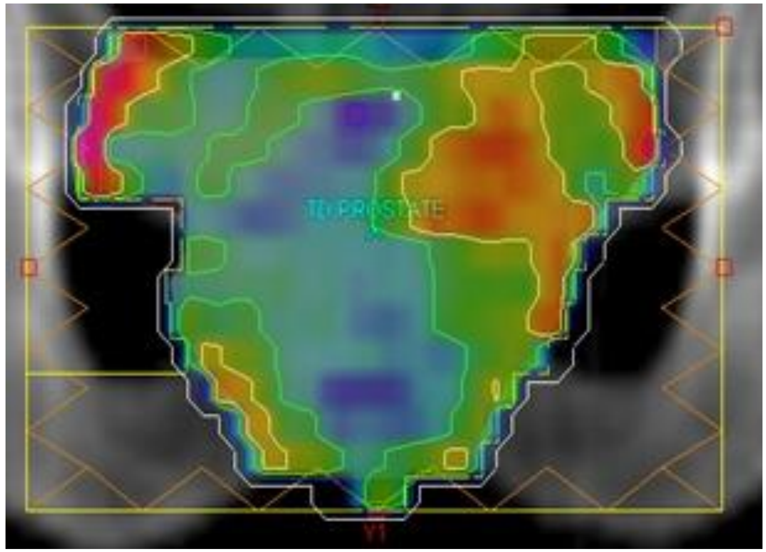


Image taken from: S Webb (2003) The physical basis of IMRT and inverse planning British Journal of Radiology 76: 678-689



Sketch illustrating intensity modulated beams of radiation.



Key Concepts of IMRT

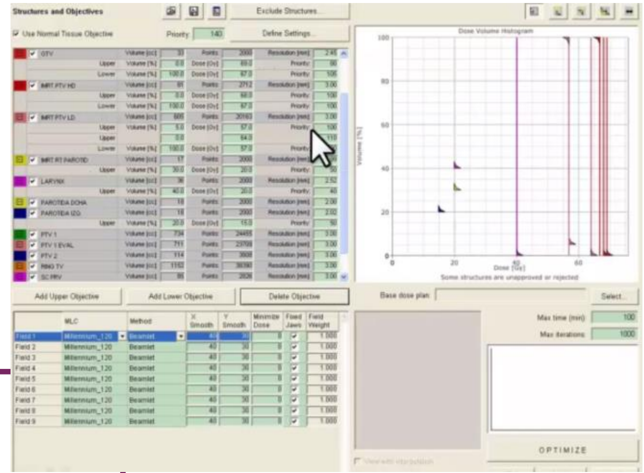
- This fluence is **modulated**
- The intensity of the fluence changes across the beam
- This changing intensity is based on the required dose to be delivered across a field
- This modulated fluence will determine the dMLC leaf motion

Key Concepts of IMRT

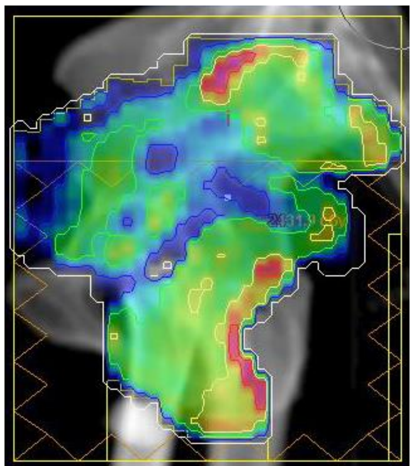
- Limitations of IMRT…

1. Multiple PTVs
2. Complex PTVs (close to skin edge)
3. Multiple OARs with multiple DVCs

Sophisticated optimisation parameters



Complex fluence patterns



High MUs

Key Concepts of IMRT

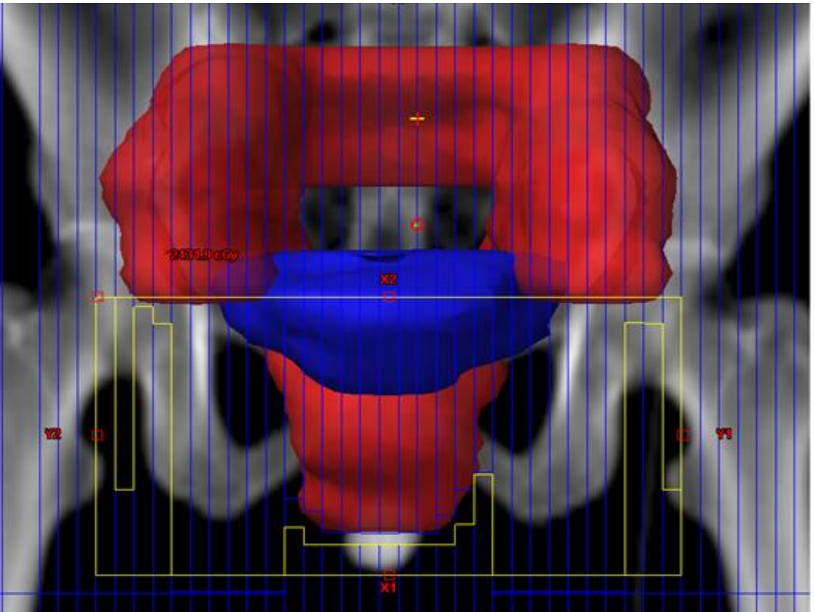
- Limitatio f IMRT…

Large PTVs

Enter VMAT…

Increased number of planning fields

Due to restrictions r motion for SW IMRT, even more treatment fields (for some Varian machines)



NB: this image demonstrates the concept of split carriages

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Key Concepts of VMAT

- Simultaneously changing 3 main features
  - ➢ MLC leaf motion
  - ➢ Gantry speed
  - ➢ Variably dose rate

- Inverse planning based on Progressive Resolution Optimisation Algorithm (PRO)

- PRO 3
  - ➢ 4 multi resolution levels
  - ➢ All 178 control points are included in each level
  - ➢ Internal logic
  - ➢ Intermediate dose calculation

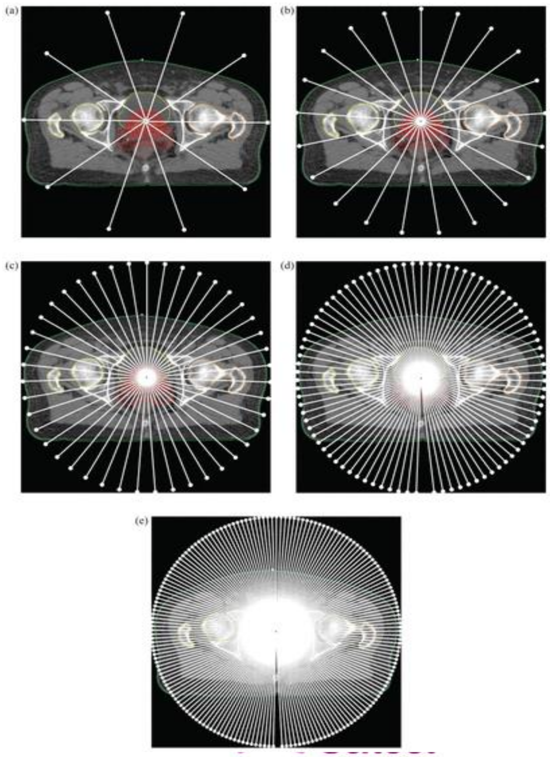


Image taken from: Jolly D, Alahakone D and Meyer J A RapidArc planning strategy for prostate with integrated boost. J Appl Clin Med Phys 2010

Clinical Applications of VMAT

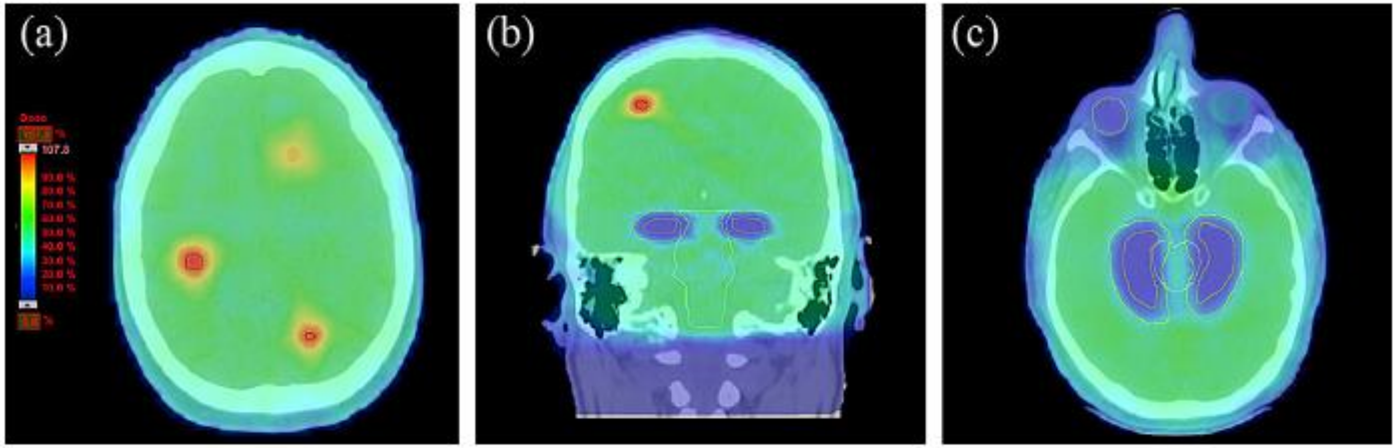
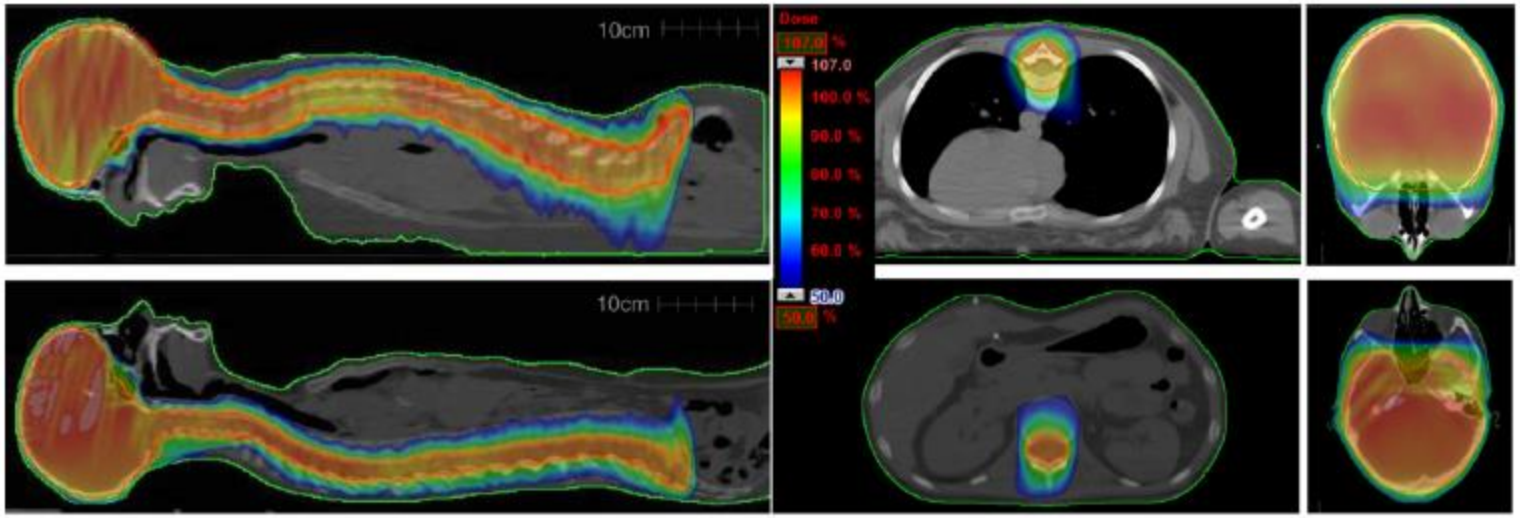


Fig. 1. Examples of isodose distributions for whole brain radiotherapy with hippocampal avoidance and simultaneous integrated boost for three brain metastases using volumetric modulated arc therapy. The whole brain clinical target volume was prescribed to 32.25 Gy in 15 fractions. Three metastases were prescribed 70.8 Gy in 15 fractions. (a) Axial image with three metastases. (b) Coronal image with one metastasis and the hippocampi. (c) Axial image with the hippocampi and eyes.

Hsu et al., 2010



Fogliata et al., 2011

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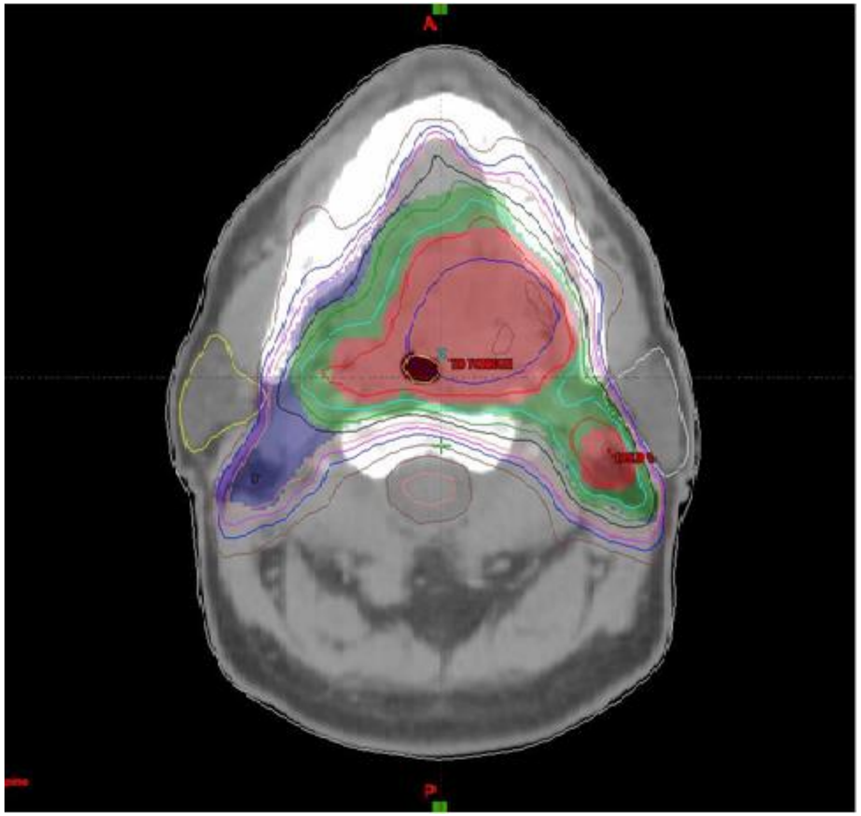
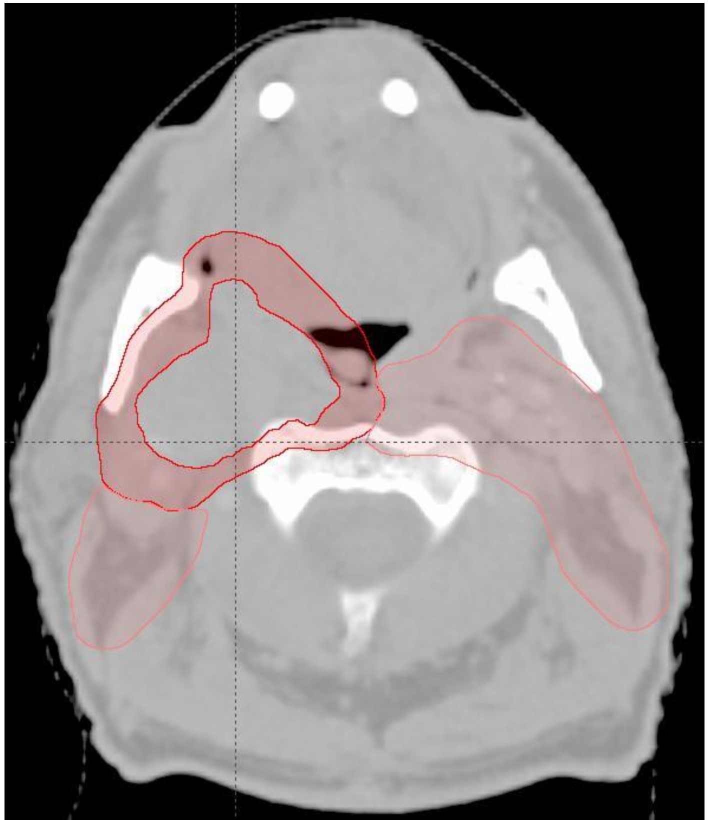
The Benefits of Inverse Planning



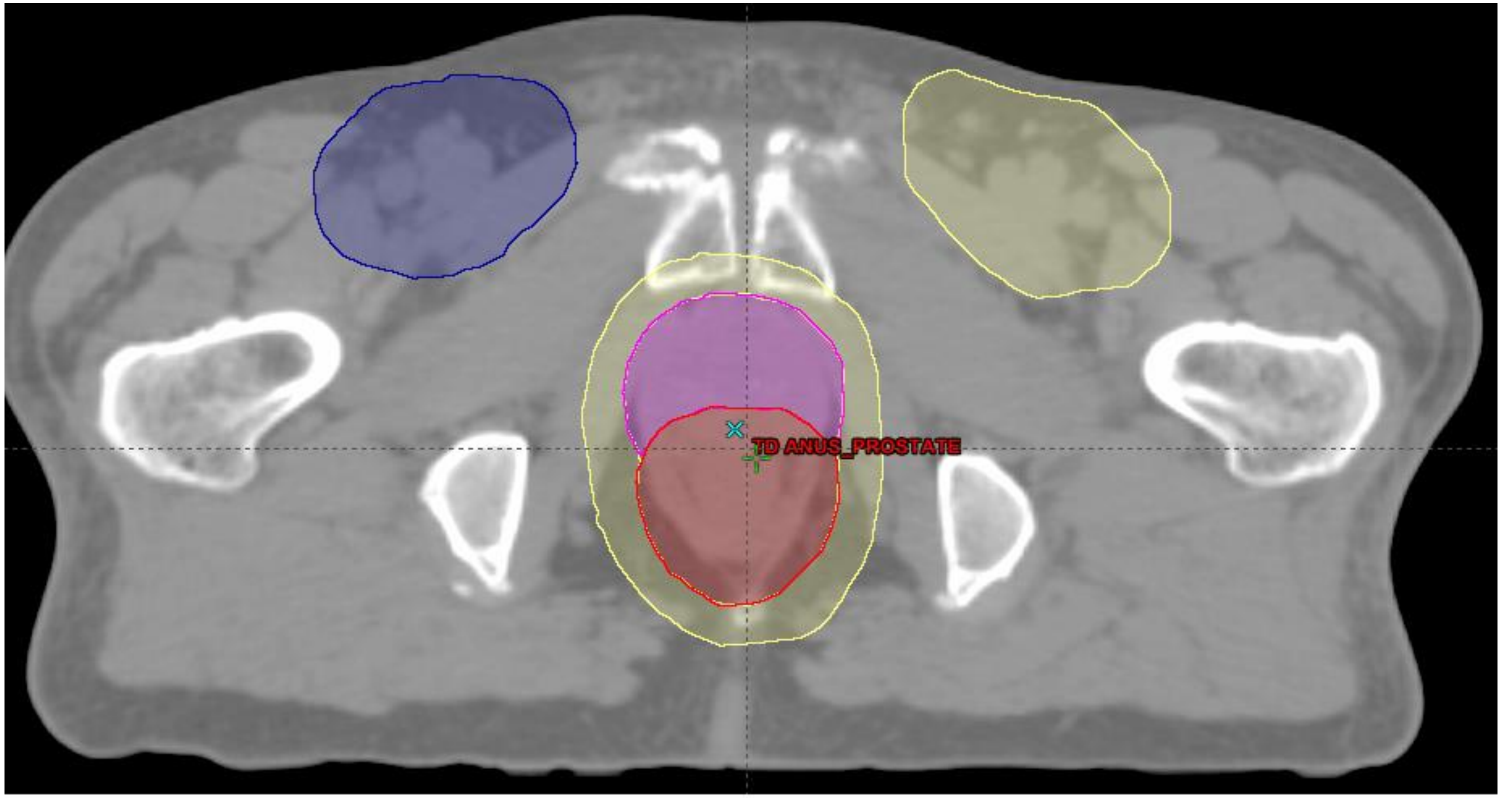
Complex concave volumes



Increased control over distribution

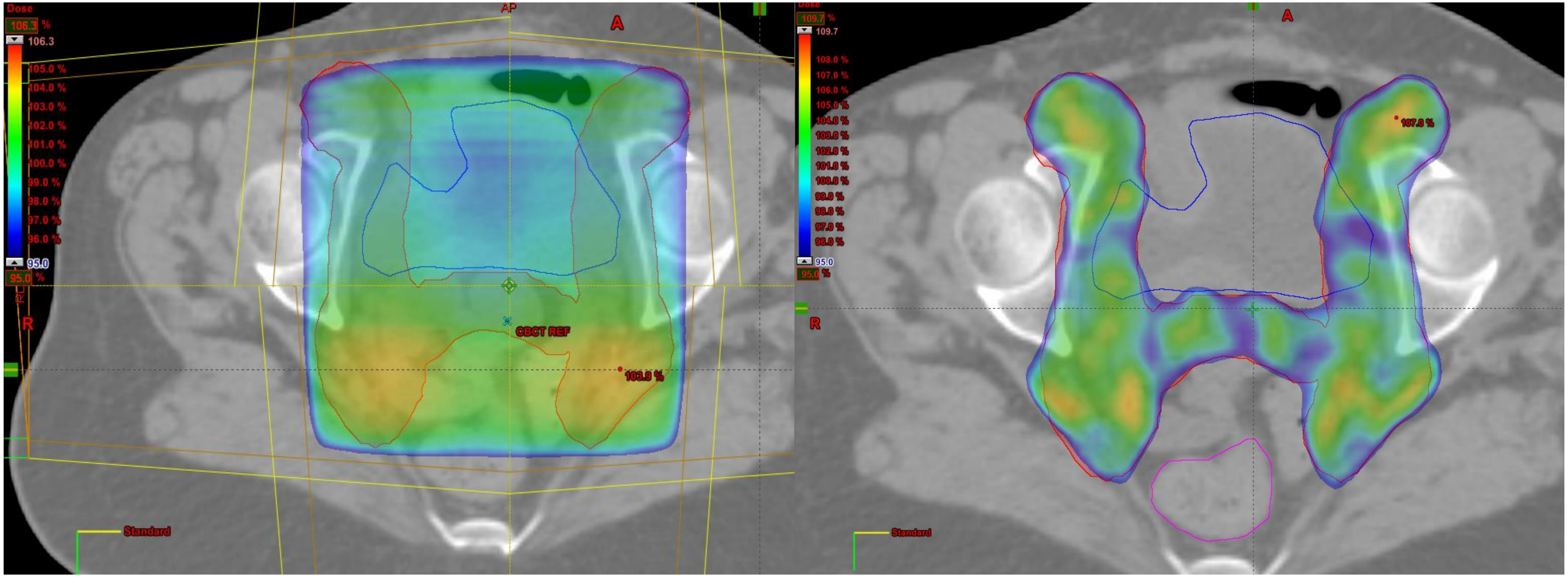
Boosting targets within targets

The Benefits of Inverse Planning



Multiple targets
Simultaneous integrated boost

The Benefits of Inverse Planning

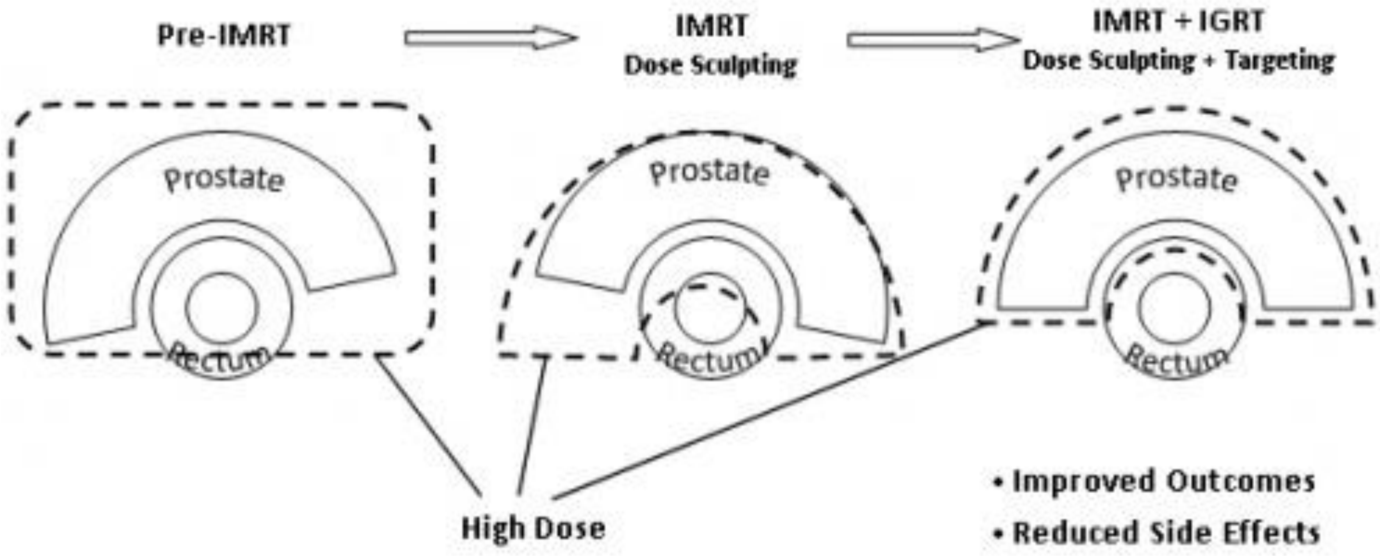


Sharp dose fall off
Improved OAR sparing

Need robust IGRT!

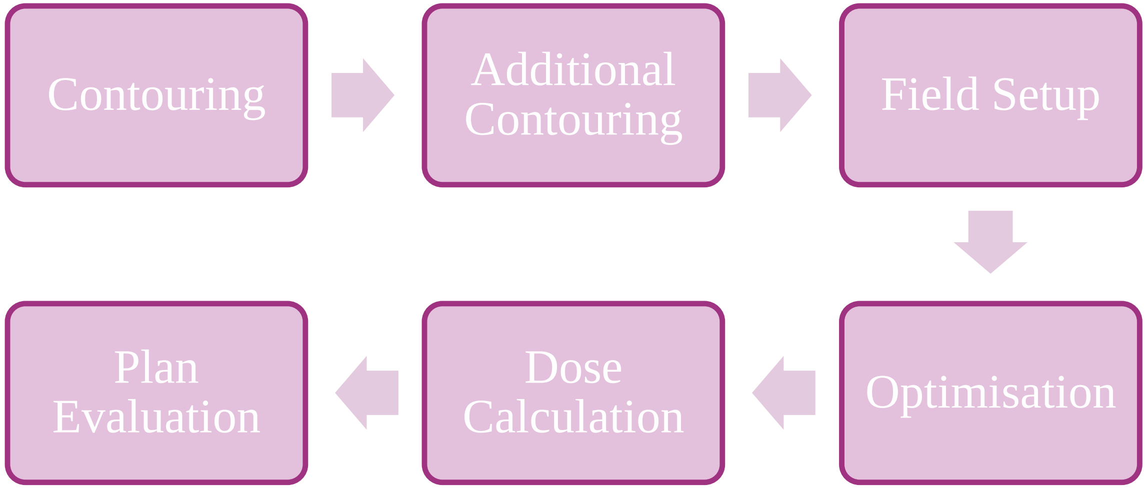
The Benefits of ***IG***-IMRT

- Jose will cover this in more detail this afternoon!



http://radiotherapy.blog.co.uk

Let's Look at the Inverse Planning Process in Closer Detail...

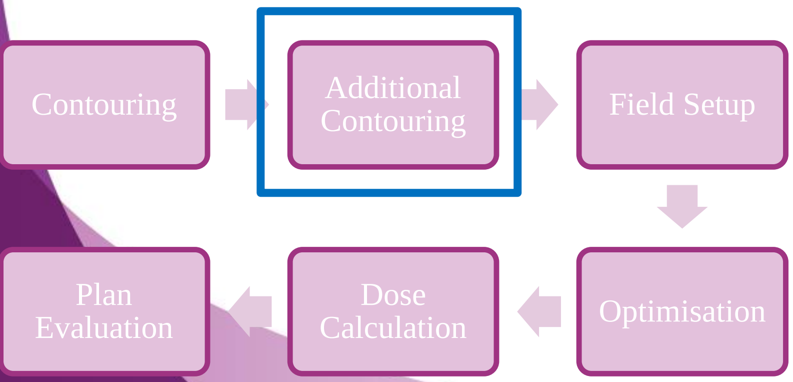


Additional Contouring

- Virtual contours used only in optimisation but ***not*** plan evaluation

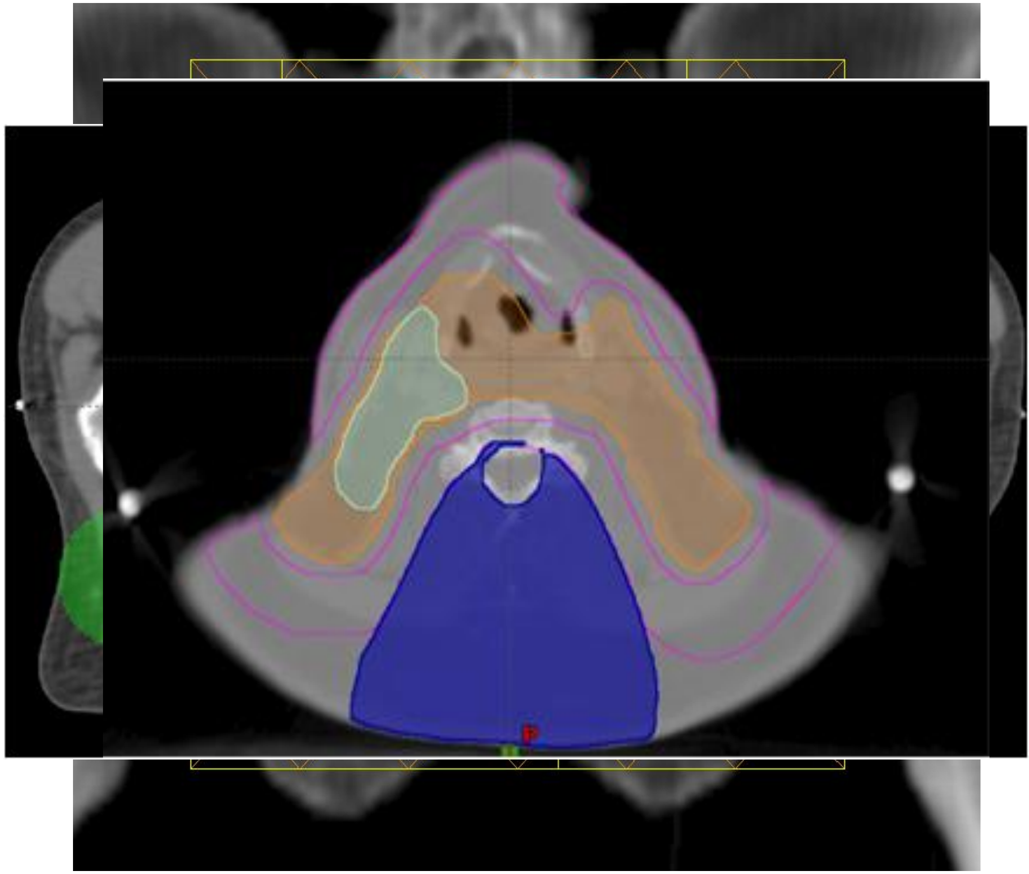
- Ease the optimisation process/algorithm

- How and when you use them will depend on the case and also on your experience as a planner
  - ➢ Also what point of the optimisation process you are at for VMAT



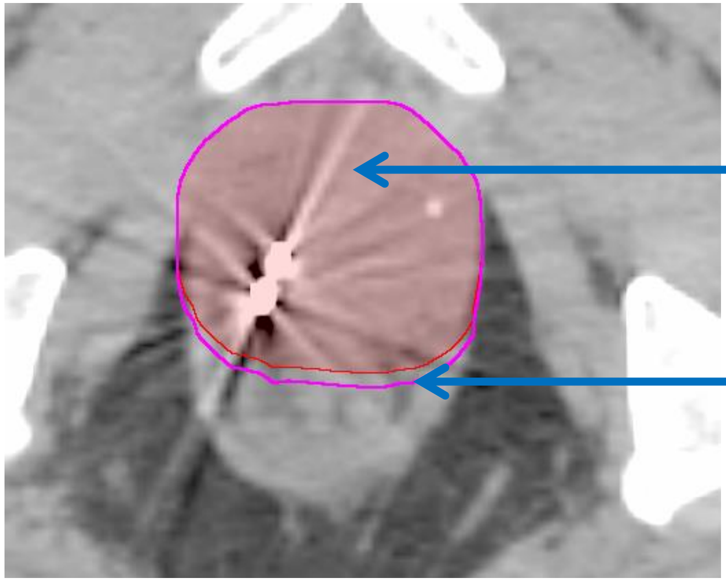
Additional Contouring

- Increase control over dose distribution
  - Dose escalate within a PTV
  - Dose fall off across a structure
  - Dose directly surrounding PTV
  - Dose dumping in healthy tissue



Additional Contouring

- Improve coverage of whole or partial target
  - ➢ We can't manually adjust the MLC
  - ➢ Inverse planning is volume based planning
  - ➢ Can be "cold" on superior or inferior slices
  - ➢ Can be "cold" where there is a competition between structures
  - ➢ "IMRT PTV"



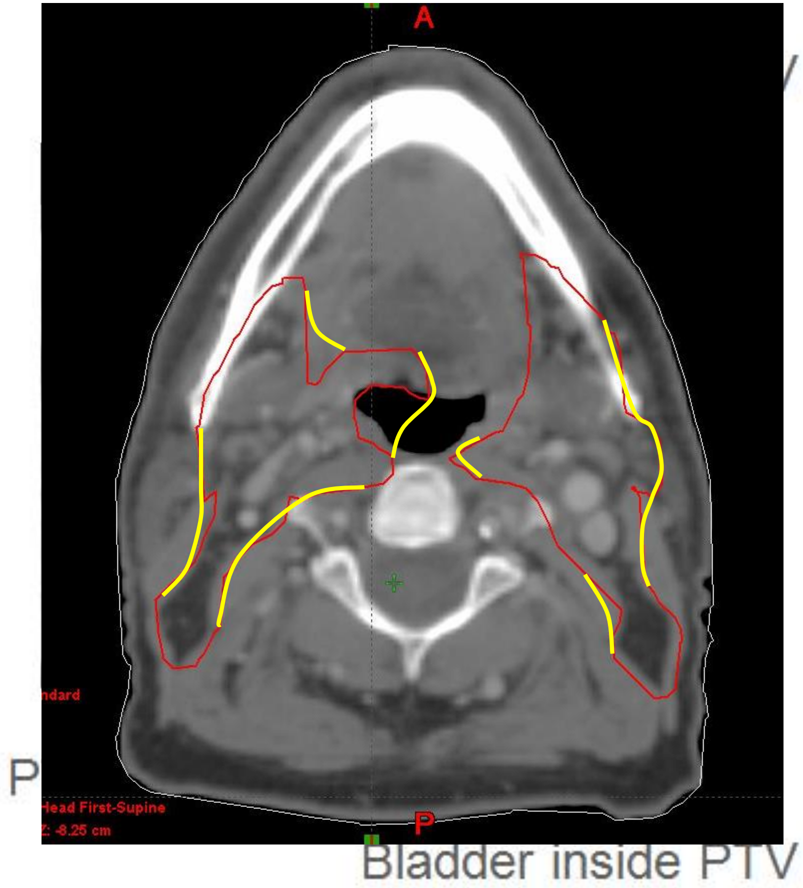
"True" PTV
Used for plan evaluation

"IMRT" PTV
Used for optimisation

Additional Contouring

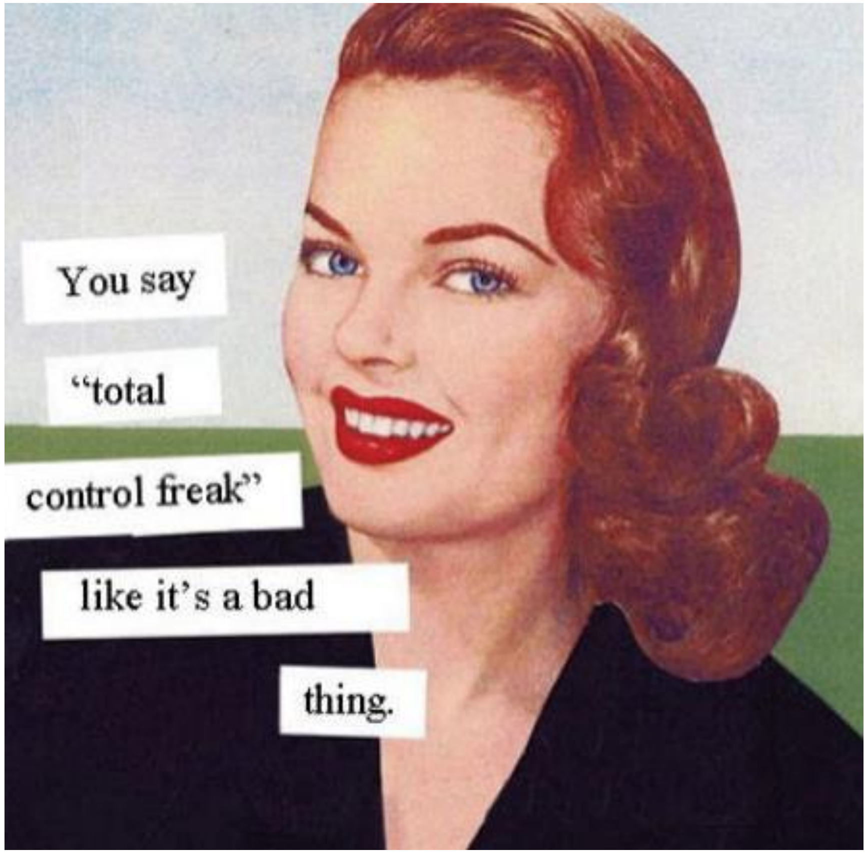
- Lessen the competition between structures
  - OAR and target

- Smoother contours and gradients between slices of target structure

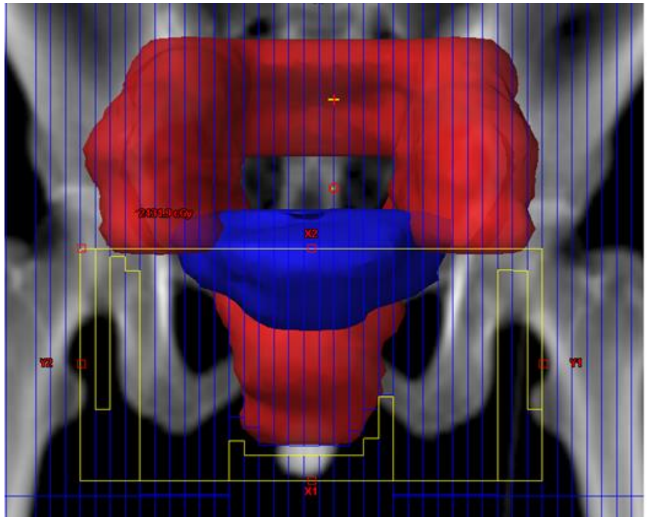


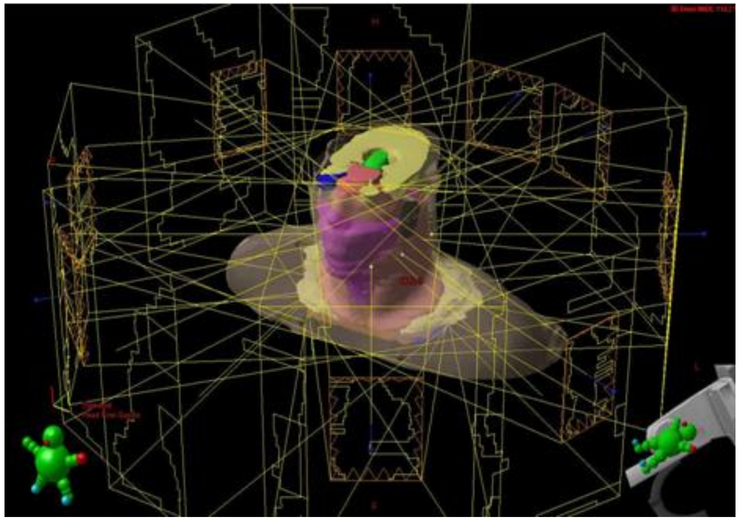
Field Setup

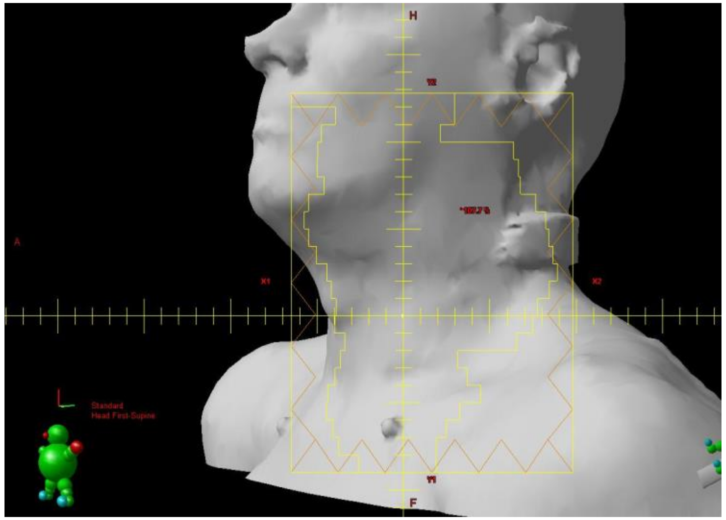
- Isocentre placement
- Beam arrangement
- Field size
- Collimator angle
- Dose rate



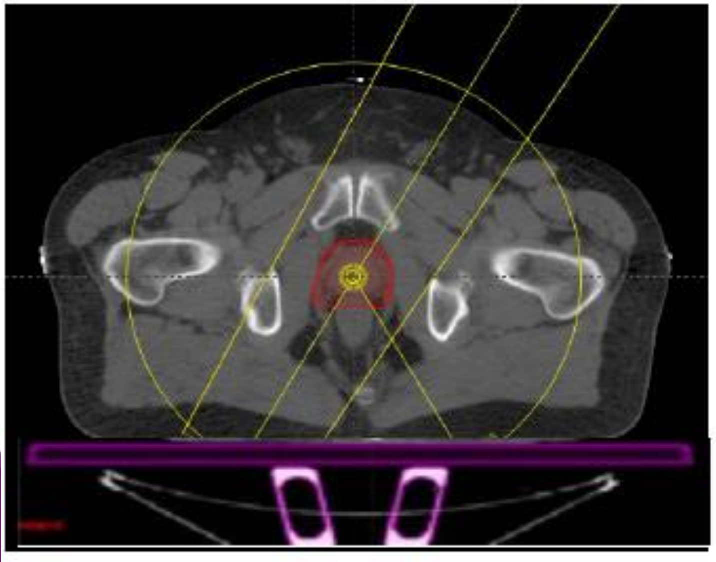
IMRT

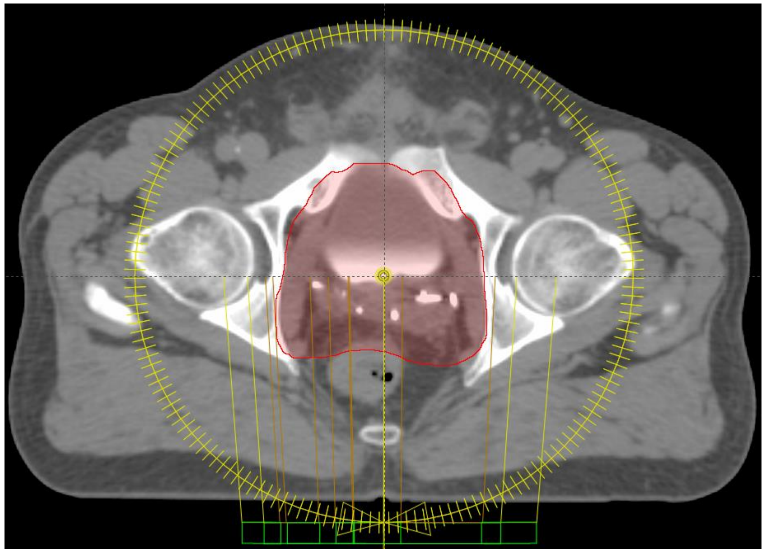






VMAT





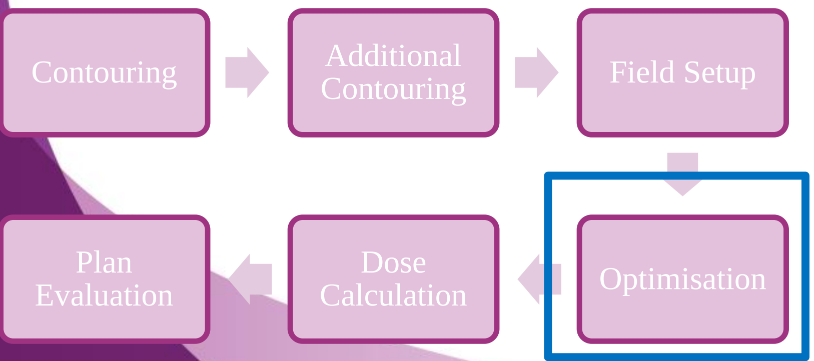
Shoulders:
Angle gantry to avoid
Angle couch to avoid
Fix jaw to avoid
(sup or ant/post)

Inverse Planning Optimisation

- Planner decides on required dose coverage with dose constraints for surrounding structures
  - ➢ Cost function algorithm

- Upper and lower dose limits are to be nominated
  - ➢ Target structures have both

- Planning systems allow for dose constraints to be specified
  - ➢ Either as a dose max, mean dose or as a %volume to receive a specified dose
  - ➢ Can have either a single point, a series of points or a line



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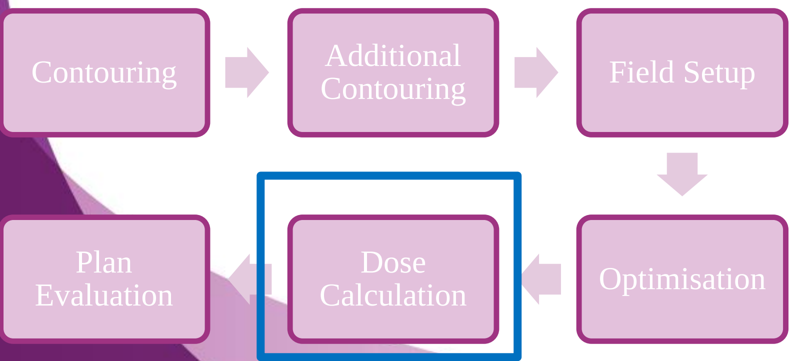
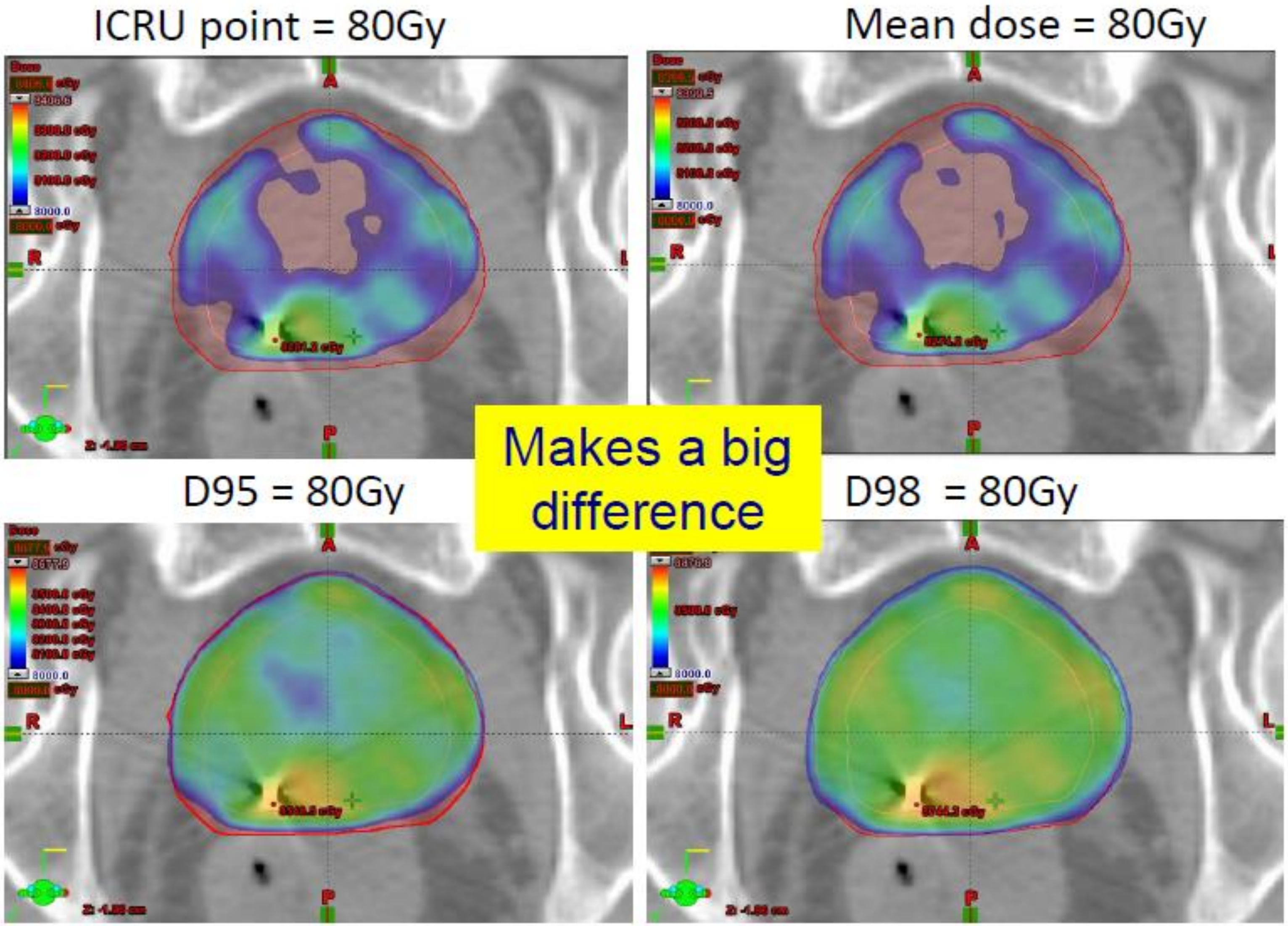
IMRT Dose Calculation

- The fluence maps are generated at the time of optimisation
- The leaf motion is then calculated to enable the delivery of this
- The 3D dose calculation is then carried out generating a dose distribution
- Note the subtle changes:
  - ➢ Fluence now reflected the deliverable values
  - ➢ The DVH is now based on AAA as opposed to PBC



Plan Normalisation

What happened to ICRU 83?



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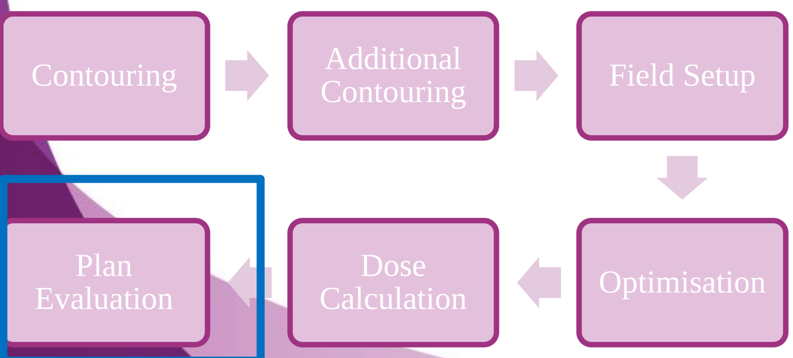
Plan Evaluation

- This is a crucial component of the planning process and should not be rushed or undervalued

- Target Coverage
- Target Conformity
- Target Homogeneity
- OAR doses
- Integral Dose
- Field arrangement used
- Fluence maps or segments for IMRT
- Monitor Units
- Treatment time



Plan Evaluation

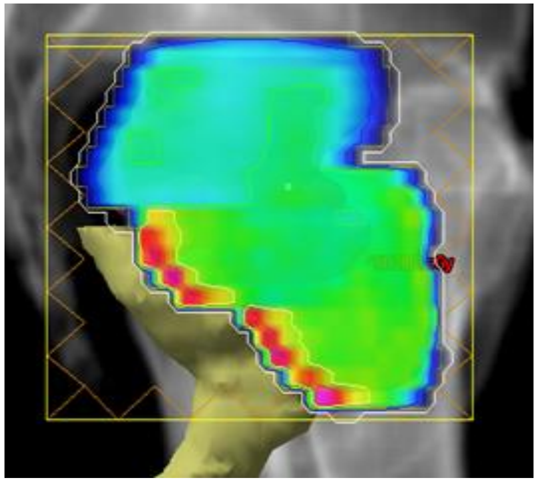
- Select appropriate tools
  - ➢ Modern TPS are developed to make our life easier but are only as good as the user who is interpreting the information
- Qualitative
  - ➢ Visual inspection is vital
  - ➢ Clinical judgement
- Quantitative
  - ➢ ICRU 56, 62, 83
  - ➢ DVH
  - ➢ Conformity and homogeneity indices

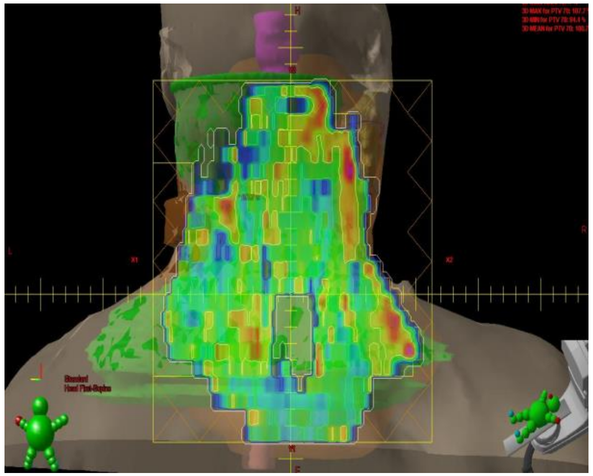
Revise ICRU!
You must know and use the correct terminology
You must know the main recommendations

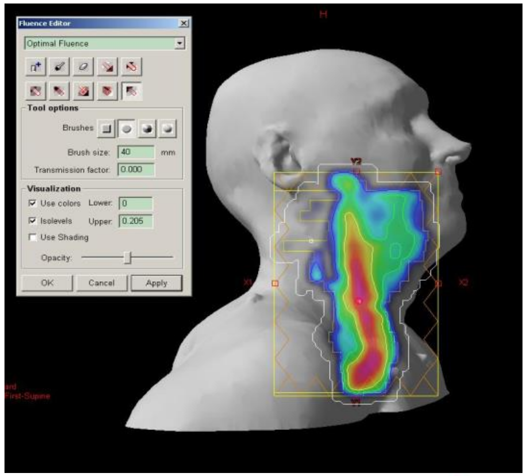
Plan Evaluation

- RTTs care about fluence maps too!

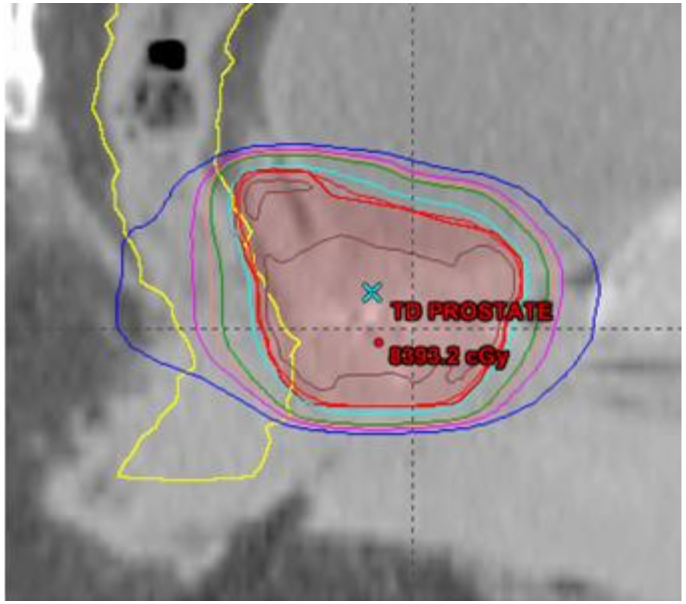
- What is level of modulation
- Is this necessary
- What impact does this have on the dose distribution
- What impact does this have on treatment delivery

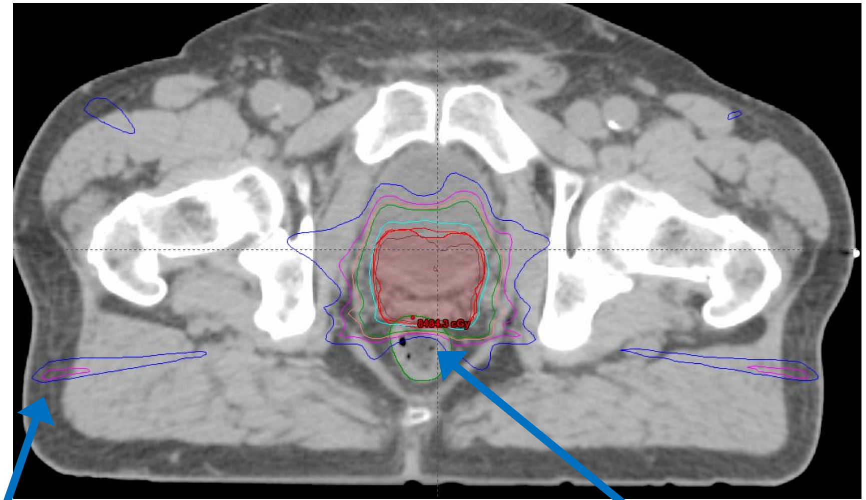






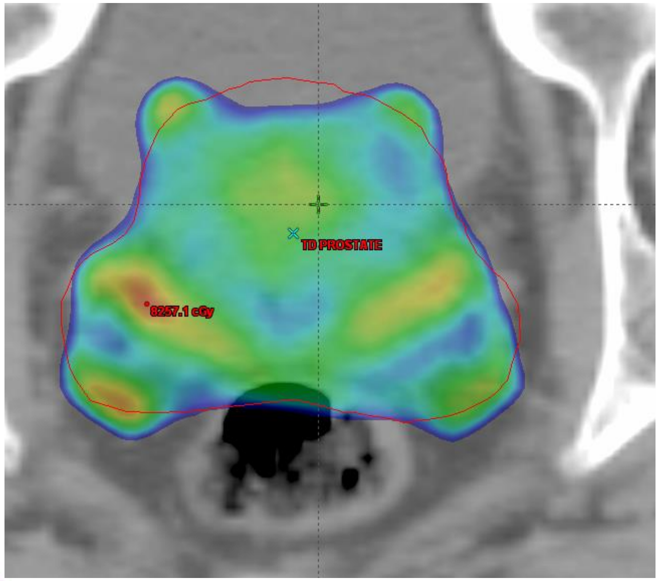
Plan Evaluation

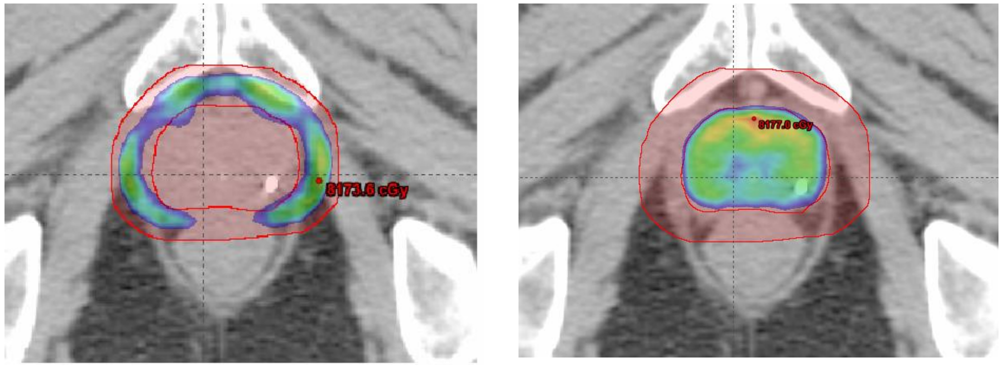




Lateral Hot Spot 50Gy

Max in Rectum





How To Improve a Bad Plan

- Beam Angles
  - Number and position
  - Bare in mind length of treatment

- Plan normalisation
  - Heat up or cool down the whole plan
  - Quick, does not require re calc

- Reoptimise
  - Think about what you are trying to achieve
  - Relax constraints if possible
  - Try to keep it simple

Just Remember...

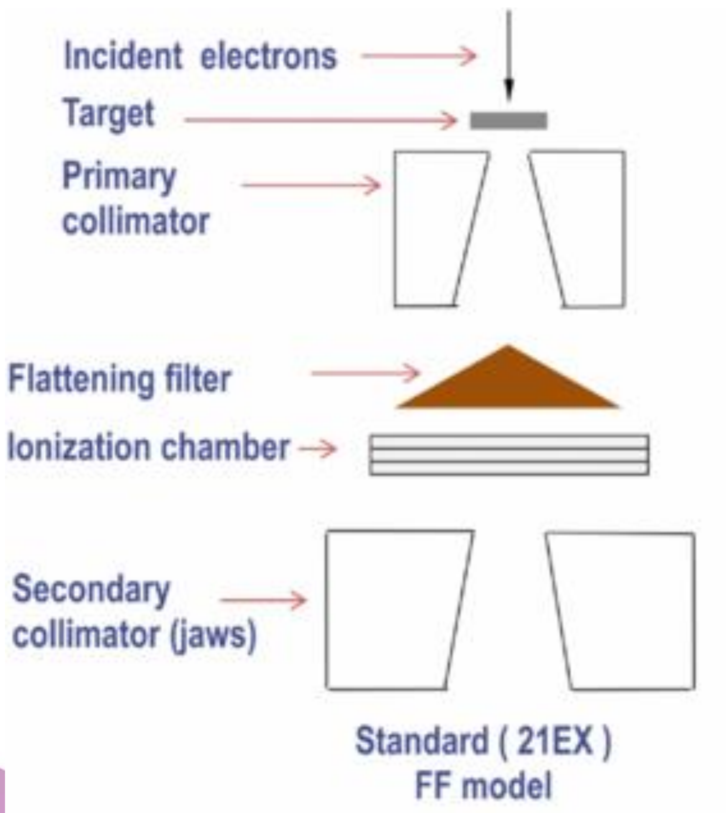
Planning is a collaborative and dynamic process

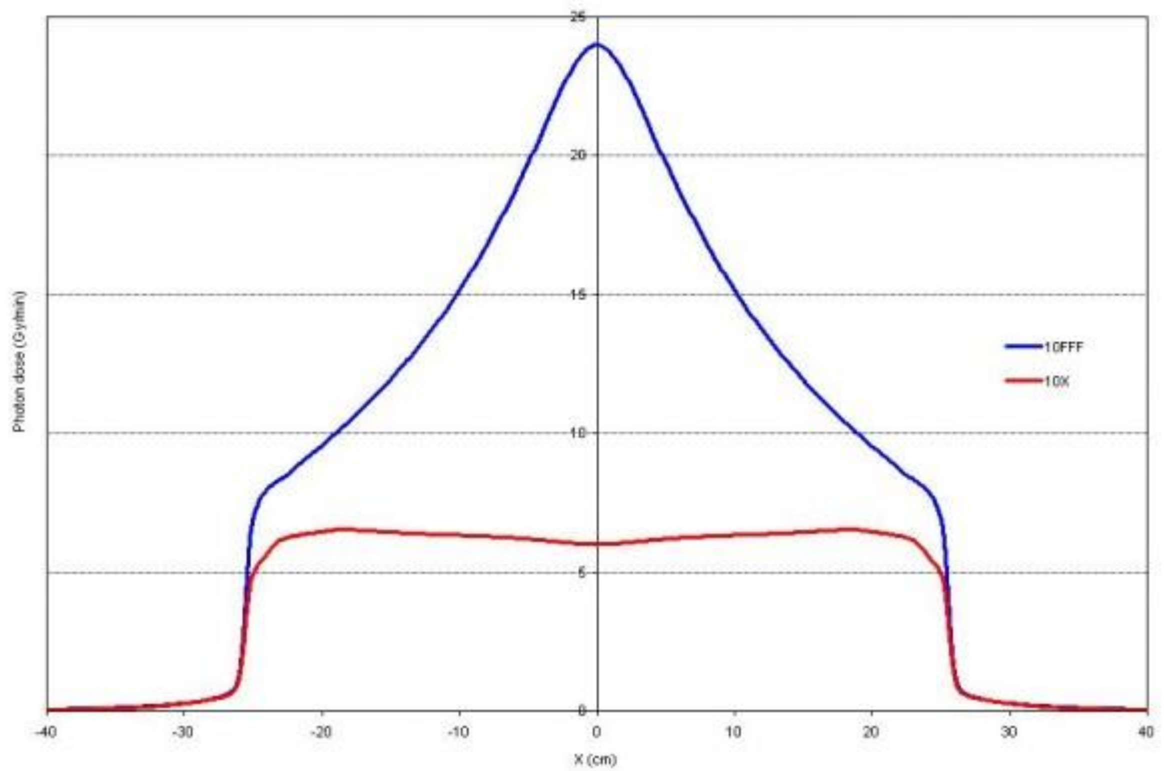
I want a better plan!

This is the best plan!

What Has Changed in the World of Planning?

- Flattening Filter Free (FFF)
- Characterized by high dose rate, cone-like fluence profile, increased superficial dose, reduced out-of-field dose





Flattening Filter Free (FFF)

- Not a new concept (1990s) but gained momentum with SRS and SBRT increasing in clinical use

- Rationale and ***Theoretical*** Benefits
  - Increase dose rate (300-600) to 1400-2400
  - Decreased beam on time (consider even more when combined with VMAT)
  - Improve efficiency
  - Patient comfort and stability
  - Intrafraction motion
  - Particularly attractive for treatments with high dose per fraction or respiratory motion management (eg DIBH)
  - Lower leaf leakage and out of field dose
    - Possibly offset by an increase in MUs compared to FF beams

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What Has Changed in the World of Planning?

- SBRT Planning

- The goal SBRT is to deliver *very* high doses/fx to the target to induce maximum damage
  - "ablative" doses

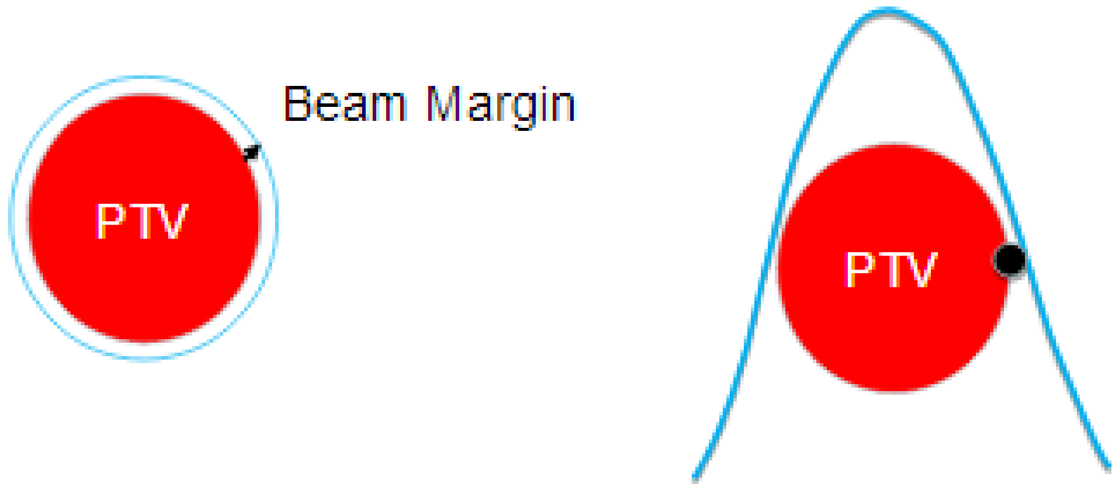
- Aim to minimise the volume of healthy tissue receiving a high dose per fraction
  - Dose to OARs is very important due to high dose/fx and increased risk of toxicity

- Traditional dose homogeneity is less of a concern
  - Up to 160% dose maximum is not uncommon

SBRT Planning

Standard approach

SBRT approach



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What Has Changed in the World of Planning?

- "**Isotoxic**" Treatment Planning
- Pioneered by MAASTRO
- Most data for this approach comes from lung cancer with Spinal Cord and MLD as the toxic endpoints
- Moves away from the "one size fits all" approach for dose prescription
  - ➢ Dose escalation is based on patient specific OAR DVH results
- Dose escalate the PTV until the OARs reach their tolerance

What Has Changed in the World of Planning?

- Adaptive Radiotherapy

- Definition: "Adaptive radiotherapy involves changes to the radiotherapy plan during treatment on the basis of patient specific observations that were not taken into account during initial planning" *(Gregoire et al., 2012)*

- Incorporates systematic measurements of treatment variations into a closed-loop RT treatment process

- Provides feedback to re-optimise the treatment plan early on during the fractionated course of RT

- Delivers treatment that is customised to the **daily** patient target volumes

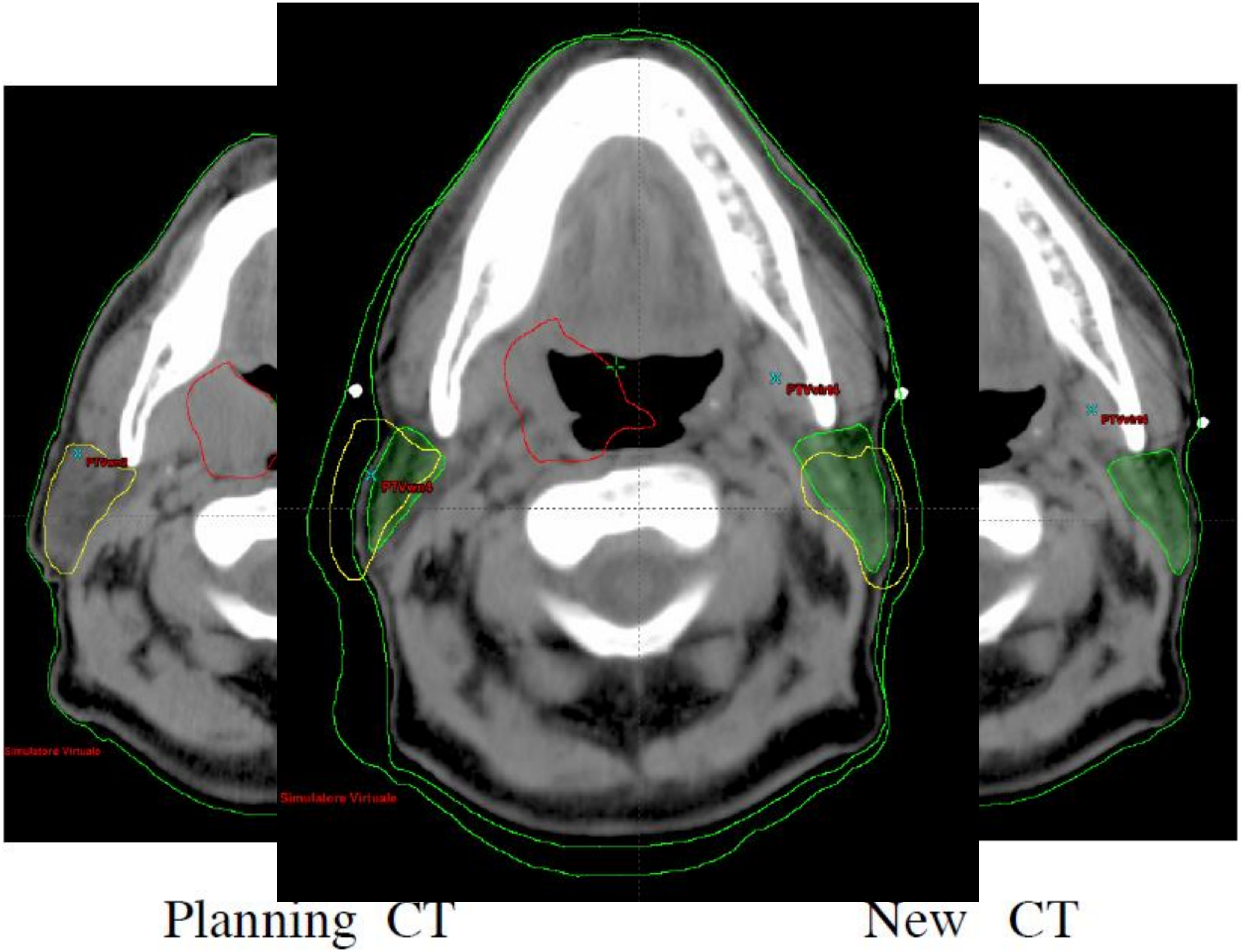
Principles of ART

- Can be adapting to changing geometry or changing geometry and delivered dose

- Approaches:
  - Completely Online
  - Library of Plans
  - Offline
    - Composite CTV at treatment initiation
    - Scheduled replan
    - Unsceduled replan

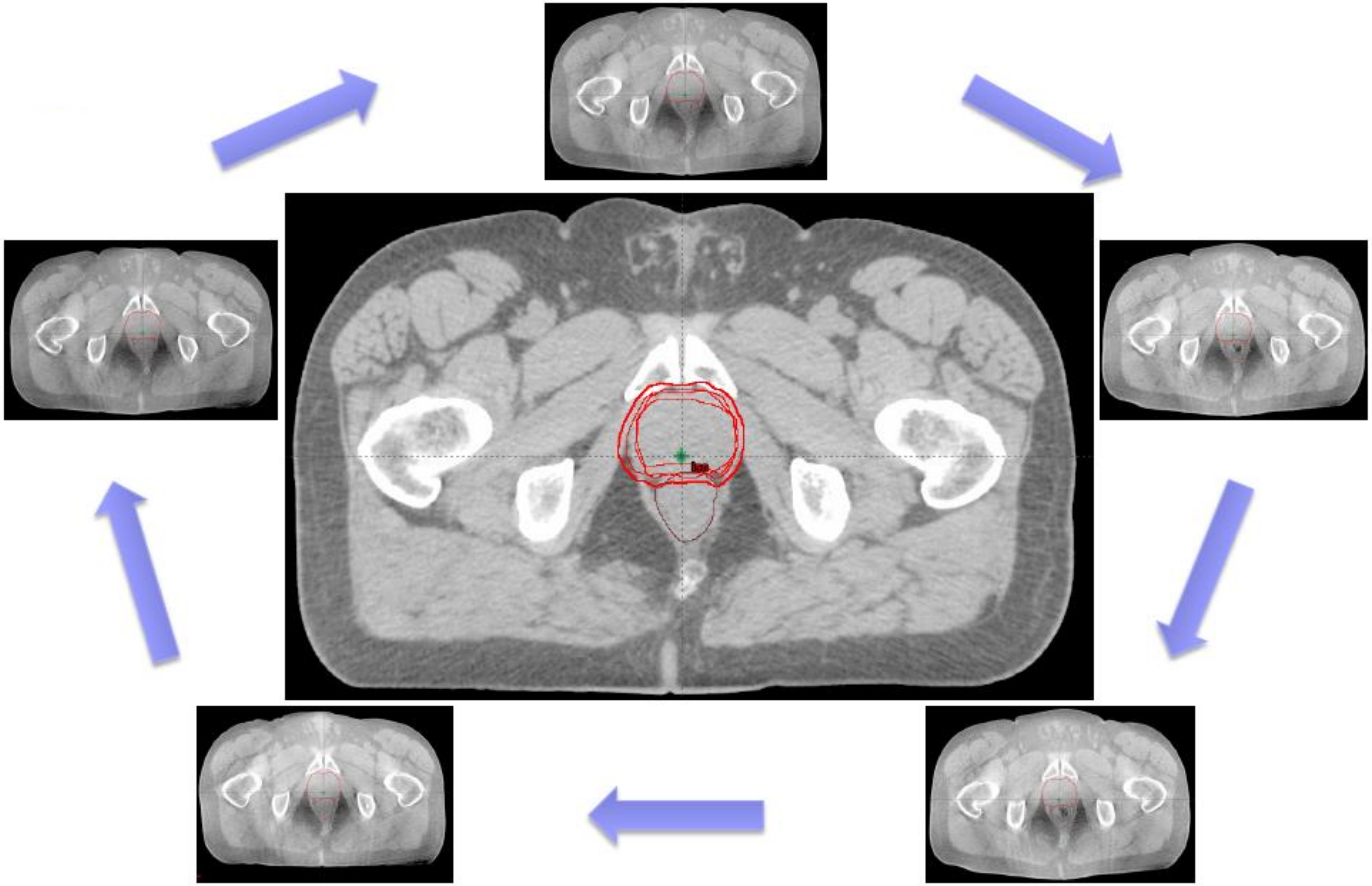
Slide courtesy of Michelle Leech

Adapting Planning on CT



Slide courtesy of Michelle Leech

Adaptive Planning Based on CBCT 1



Adaptive Planning Based on CBCT 2

- Recalculation of planned dose using CBCT

- Are HU on CBCTs accurate?
  - Some conflicting evidence in the literature
  - Depends on the quality of your CBCT

- Options to overcome these uncertainties:
  - Pixel correction technique
    - CT numbers from conventional CT are applied to CBCT
  - Deformable registration
    - Deform planning CT to the CBCT to calculate "dose of the day"
    - This is a move towards "online" ART

Be Careful of Potential Limitations!

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Slide courtesy of Michelle Leech

Geometric accuracy of bladder plan libraries

- A plan library strategy does not necessarily **guarantee** geometric accuracy
  - Risk of geographical miss due to intra-fractional bladder filling in 6 directions (Murthy, 2011)
  - No suitable plan in plan libraries (Foroudi, 2011, Lalondrelle 2011, Tuomikoski 2011, Gronborg 2015, Vestergaard 2014)
  - Confusion in plan selection (Tuomikoski 2011, Meijer 2012)
  - Inappropriate plan selection (Foroudi 2014, Meijer 2012)

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Slide courtesy of Michelle Leech

Logistics of implementation of plan libraries

- ART is not currently feasible for **all** clinical departments
  - Interobserver variability in plan choice post-education (Kuyumcian et al 2012, Hutton et al 2013)
  - Availability of technology may hinder ART implementation (Hutton et al 2013, Murthy et al 2011, Meijer et al 2012)
  - Additional education: Cost and Time (MacDonald et al 2013, Lalondrelle 2013, Meijer et al 2012, Wright et al 2008)
  - Resource implications on daily workflow (Burridge et al 2006, Hutton et al 2013, Wright et al 2008)

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What Has Changed in the World of Planning?

- **Automated Planning**

- From basic class solution to "Knowledge Based Planning"

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What Will Planning Look Like in the Future?

- Will continue to increase in complexity
  - ➢ Biological optimisation
  - ➢ ART and personalised approach based on Radiomics based analysis of pre treatment and during treatment imaging

- ***Radiomics*** is the extraction of quantitative imaging features that can be combined with clinical data

- Will move from a separate planning room to the linac
  - ➢ MRI linac
  - ➢ Online reoptimisation
  - ➢ *Online* ART

Take Home Message

- Have an awareness of what to expect from your plan
- If you don't get that, always ask ***why***?
  - Having an understanding of why the dose has behaved that way will help you find a solution to the problem
- Be guided by the literature
  - Almost all dosimetry papers will outline their planning process
    - Beam arrangement
    - Energy
    - Prescription method used
  - Critical analysis is needed!

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Take Home Message

- When reading the literature, ***read carefully!***

Good, that sounds like ICRU 50

- Methodology:

  "The radiation dose was prescribed to the PTV, such that 100% of the PTV received >95% of the prescribed dose and that no region in the field received greater than 107% of the prescribed dose"

Hang on a minute?!

- Results:

  "All treatment plans showed adequate coverage of the target volume, with more than 95% of volume of PTV1 and PTV2 receiving greater than 95% of the prescribed dose."

Menkarios et al

In-room imaging modalities

Martijn Kamphuis MSc MBA
Research Radiation Therapist IGRT

Department of Radiotherapy
Amsterdam, the Netherlands

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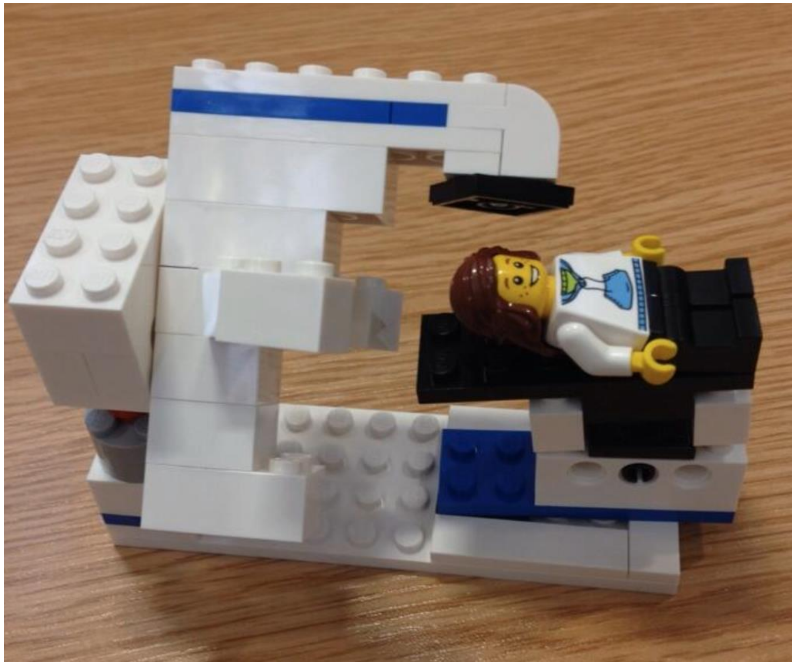
Content of the presentation

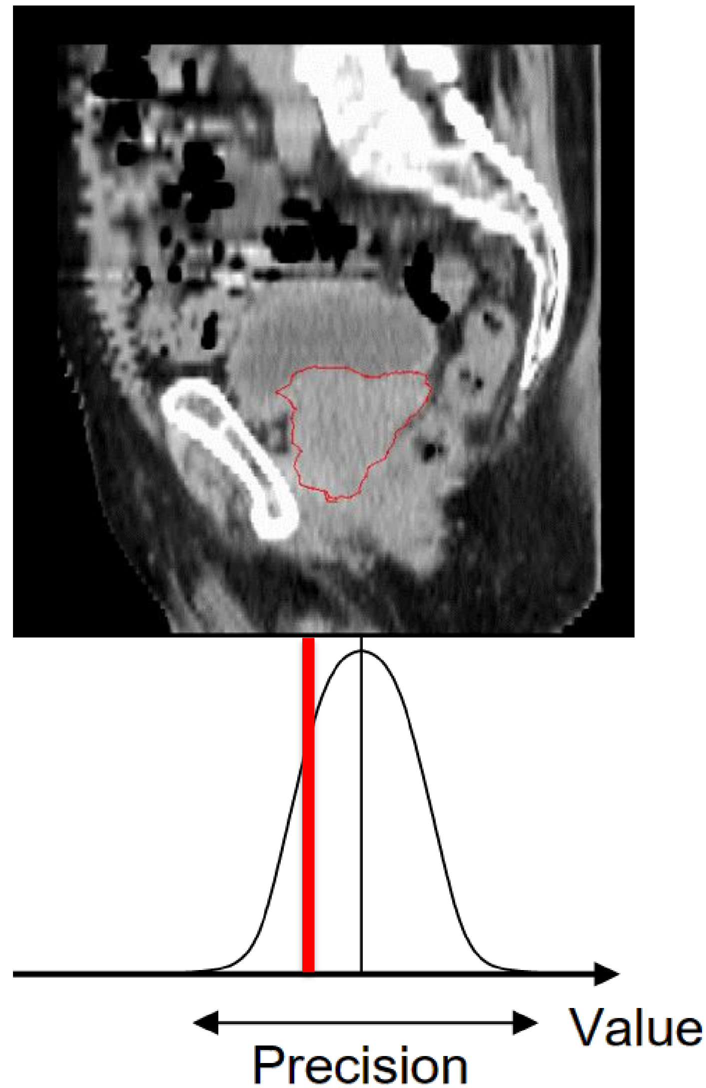
- Why do we need imaging on the linac?

- Imaging modalities
  - How do the work?
  - What can we do with them?
  - Pros and cons



At the start of treatment

- Single CT introduces systematic errors*:
    - Delineation errors
    - Organ position and shape at time of localization
    - Phantom transfer errors
        - Geometric imaging error
        - Treatment planning system error
        - Linear accelerator geometry error
        - Set-up error at time of localization
    - TPS beam algorithm error
    - Breathing positional error



*McKenzie et al., BIR 2003
Image courtesy: Marcel van Herk

In fact…it's just a snapshot

Why do we need imaging on the linac?

- To reduce systematic and random geometrical errors

- Monitor/adapt to patient anatomy/pathology
  - ➢ Plan of the day
  - ➢ (Ad hoc) replanning

- To document the treatment accuracy
  - ➢ Margin calculation
  - ➢ Incident analyses

Imaging modalities

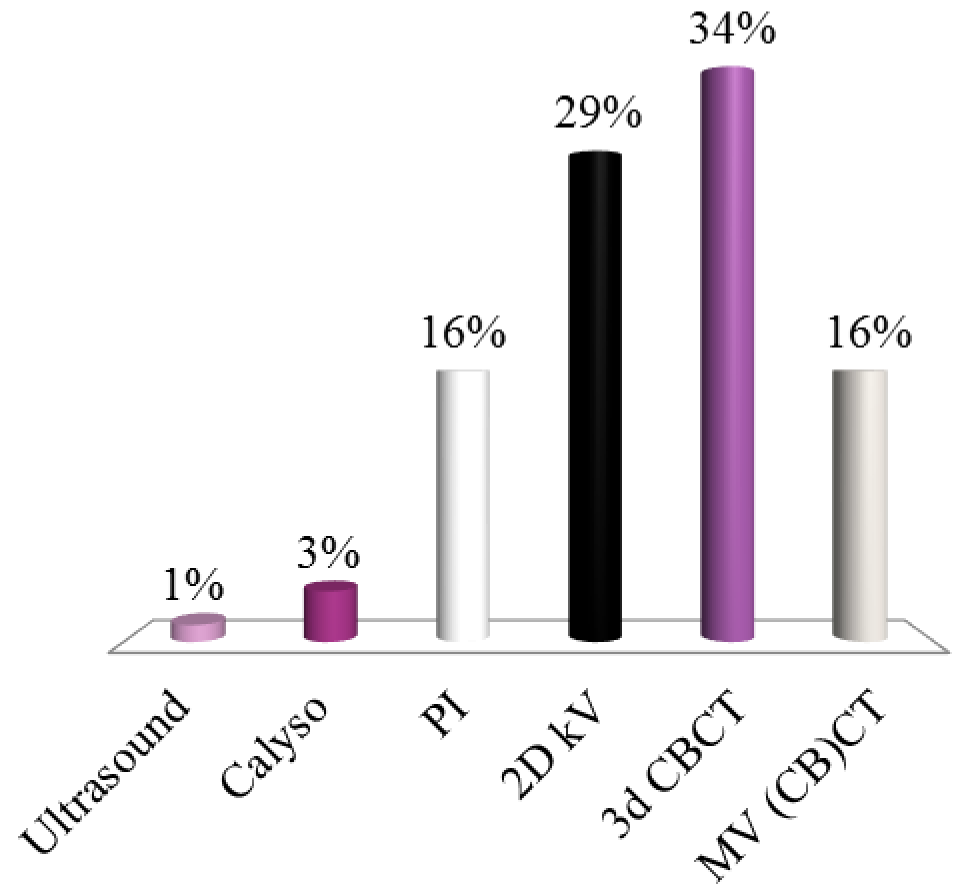
- Ultrasound systems
- Electromagnetic tracking

- Portal Imaging (EPID)
- kV cone beam CT
- 3D CBCT
- MV (CB)CT

- Surface scanning
- MR linac

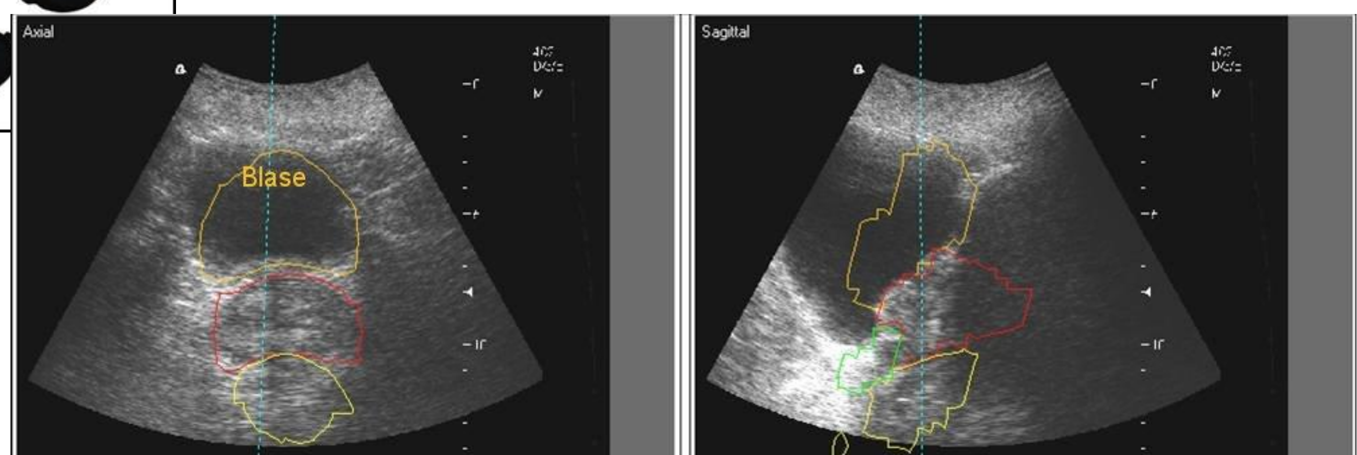
Polling: Who is using what?

A. Ultrasound
B. Calyso
C. PI
D. 2D kV
E. 3d CBCT
F. MV (CB)CT

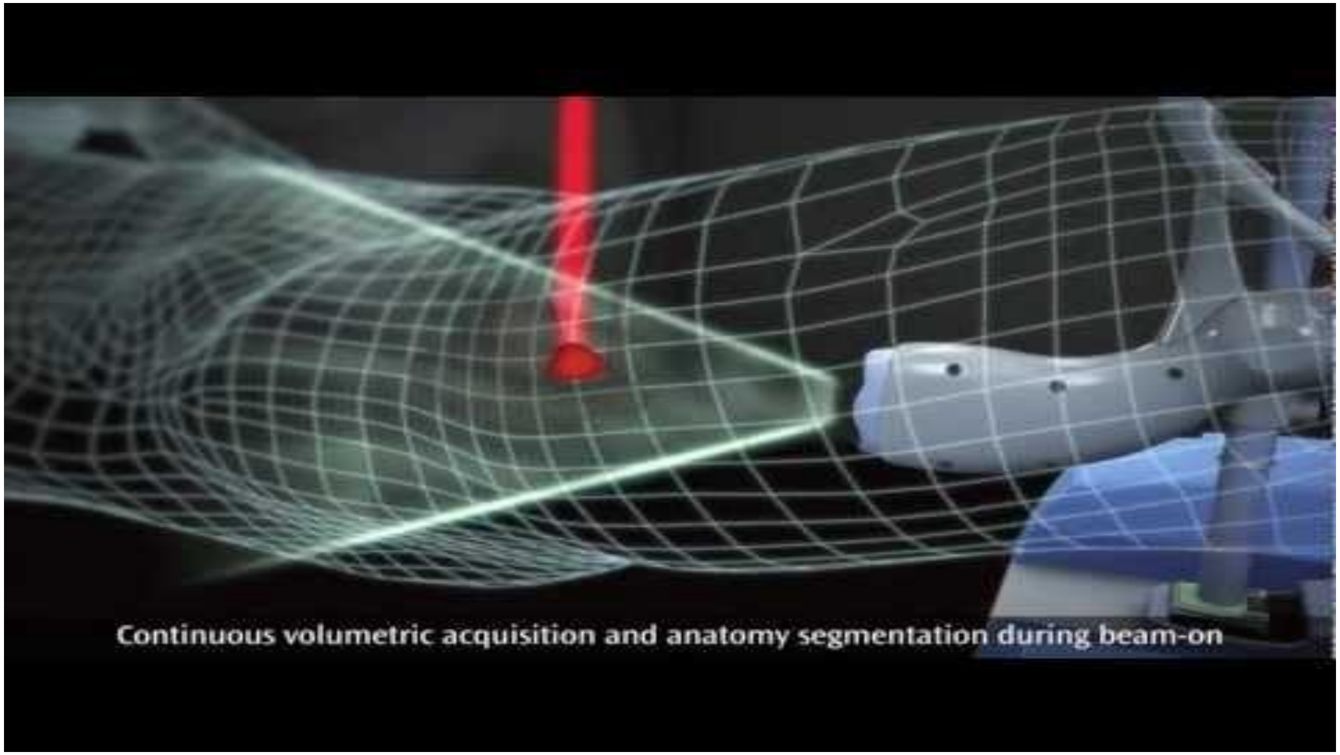


Ultrasound systems

- With probe define position target
- Infrared enables correlation with linac



More recent developments



https://www.elekta.com/software-solutions/treatment-management/imaging/clarity/?utm_source=clarity&utm_medium=redirect&utm_campaign=redirects

Ultrasound system

Pros:

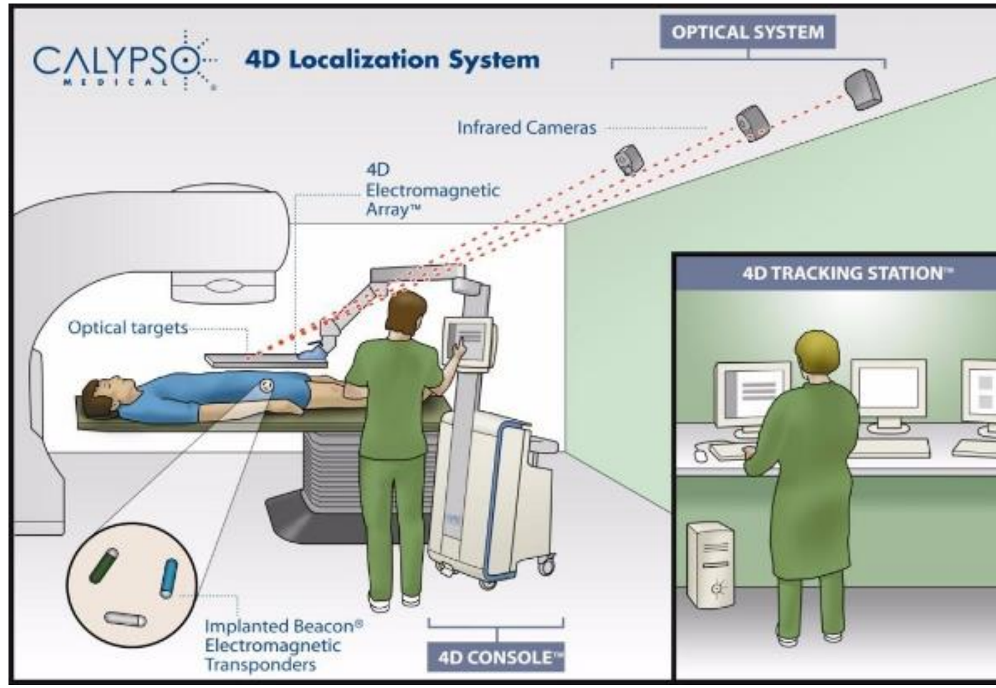
- Non invasive
- No imaging dose
- (Intra fraction imaging)

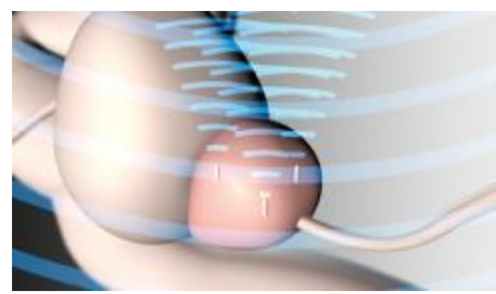
Cons:

- (User dependent accuracy)
- (No intra fraction information)
- Limited number of indications
  - Prostate
  - Upper abdominals
- (Probes influences position target)
  - Systematic error

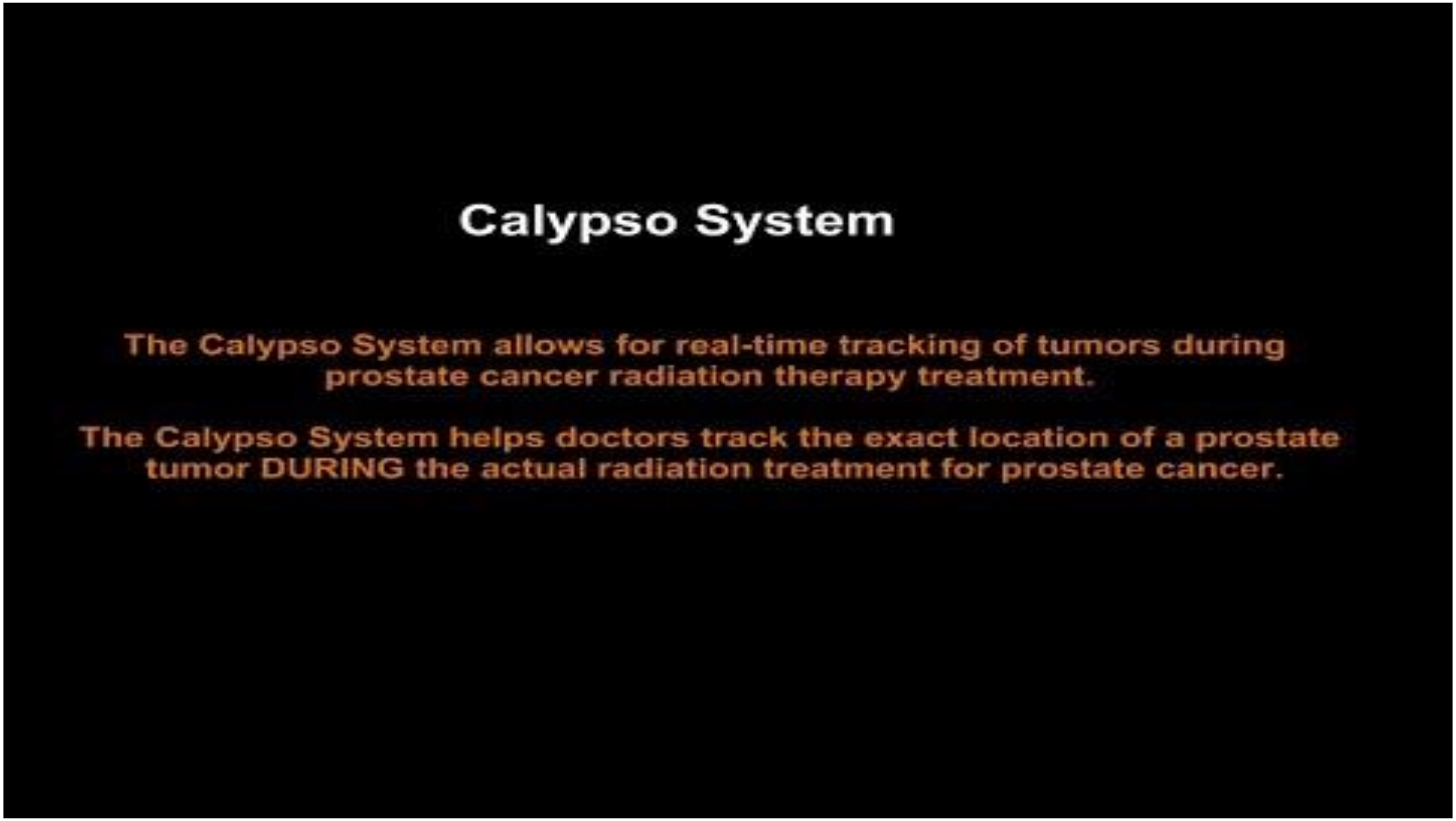
Electromagnetic tracking

- Uses implanted fiducials
- Lower magnetic field
- Transponder emits RF





Electromagnetic tracking



Electromagnetic tracking (GPS)

Pros:

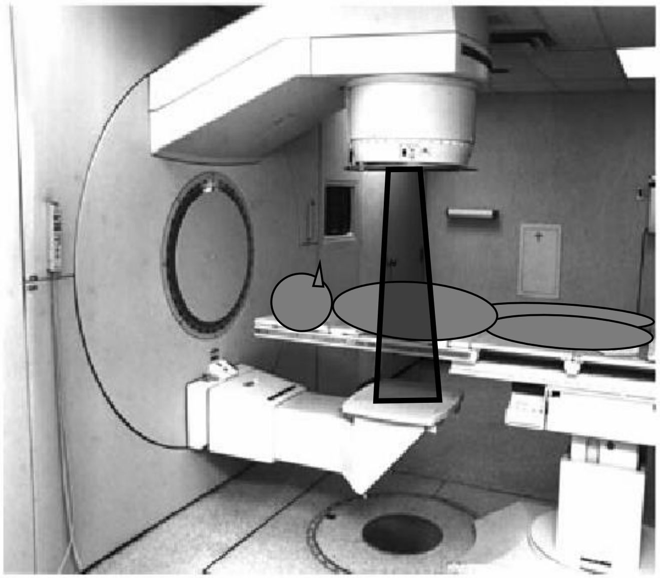
- Continuous real time measurements (10Hz)
  - ➢ Intra fraction monitoring is used for others sites as well
- Non ionizing

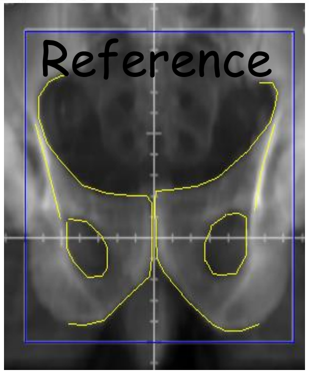
Cons:

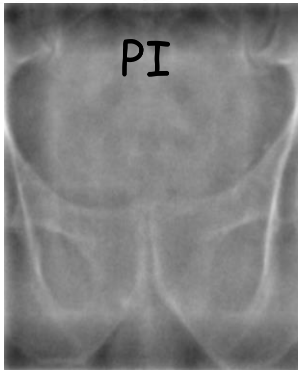
- Limited number of indications
  - ➢ Mostly prostate
  - ➢ Lung
  - ➢ Breast (PBI)
  - ➢ Pancreas
- No anatomical information
- Invasive pre imaging procedure

Portal Imaging - physics

- An imager used to detects the photons that cross the patient
- The portal image is compared to a reference image







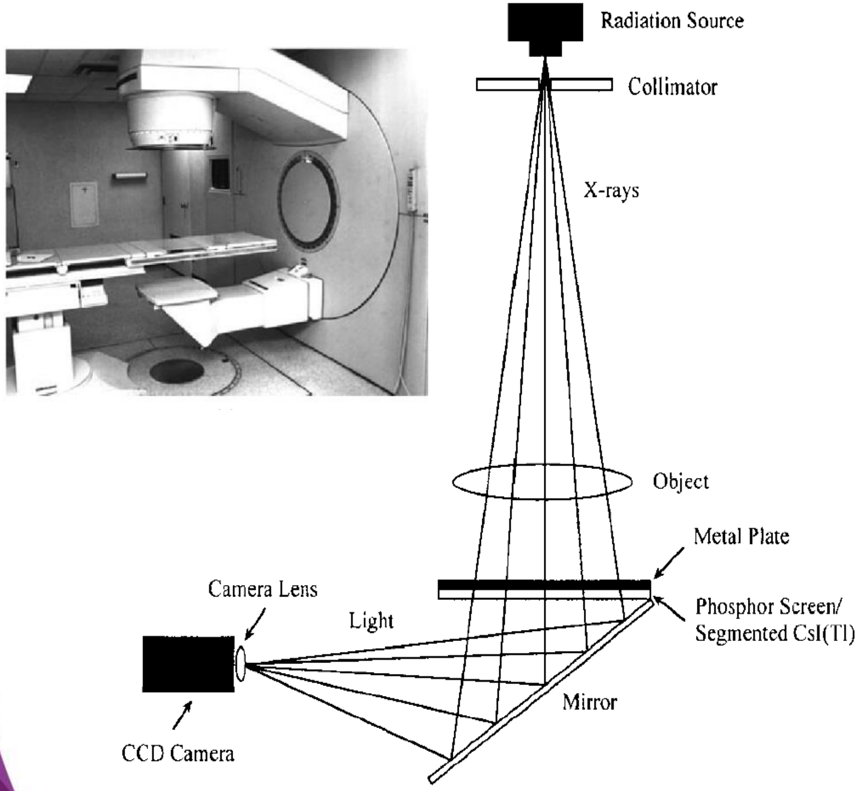
Goals of Portal Imaging

- Position verification

- Documentation of treatment
- Portal dosimetry (in-vivo)
- QA (MLC adjustment)

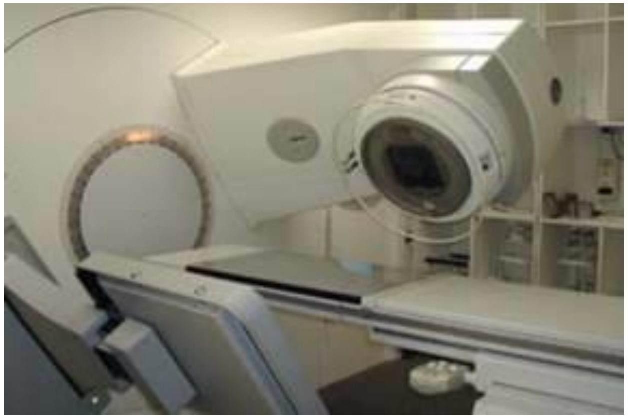
Technical aspects of EPIDs

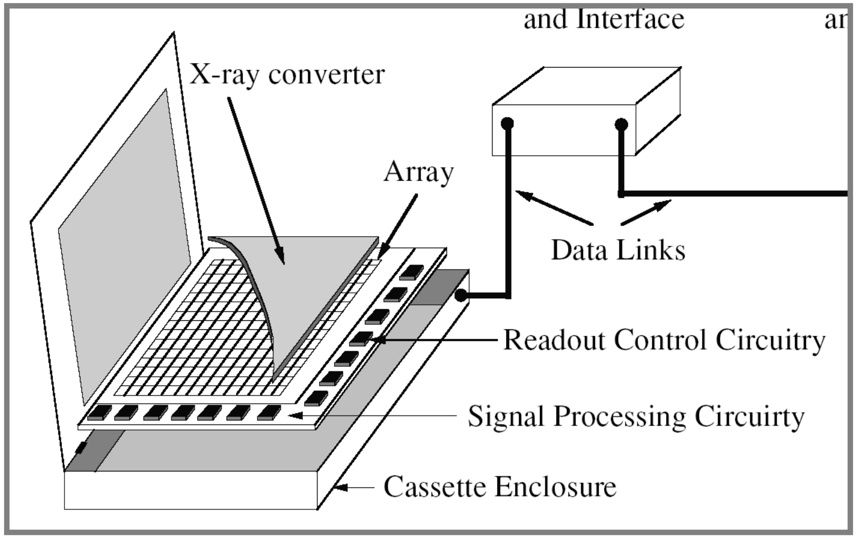
Camera-mirror based systems



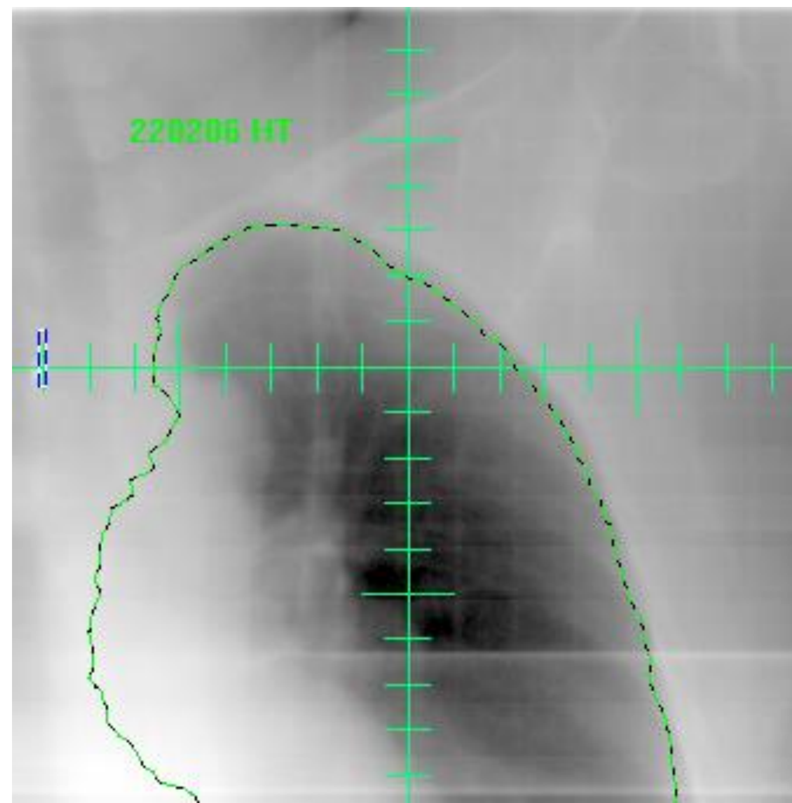
Active matrix flat panel imagers (AMFPI)

- also called amorphous silicon imagers



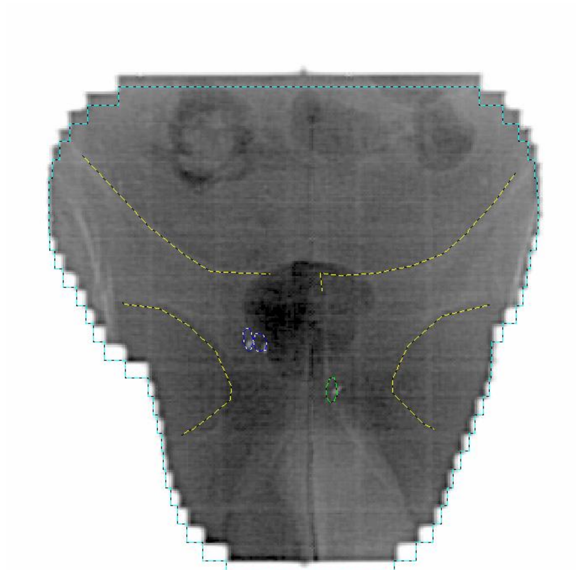


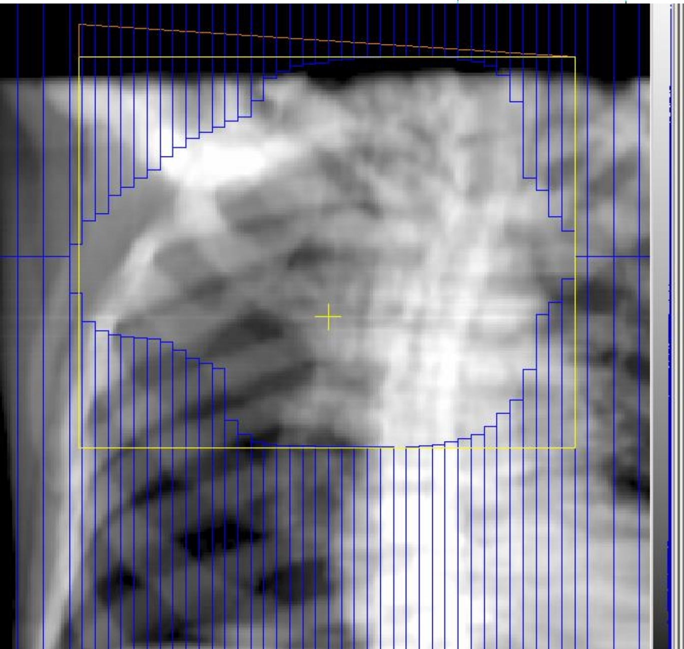
Examples of portal images (open field)

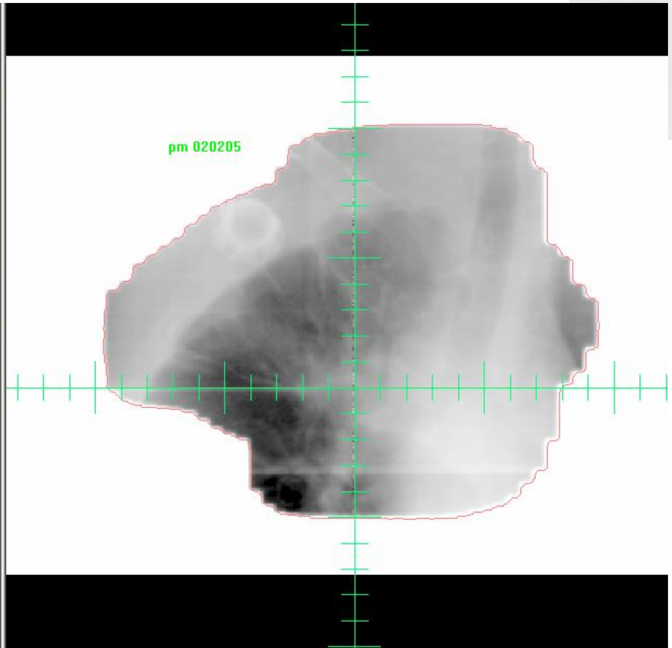


Images: M. Josipovic

EPID – field images







Images: M. Josipovic

Electronic Portal Imaging

Pros

- Image made with treatment beam
- Imaging during treatment
- Possible to perform dosimetry

Cons

- Surrogate imaging
  - ➢ Additional margins
- Imaging dose
  - ➢ Although it is possible to compensate for
- Imaging quality

2D kV imaging

kV source & detector panel

Different approaches:

- kV source moutend on linac
- kV sources on fixed position in room

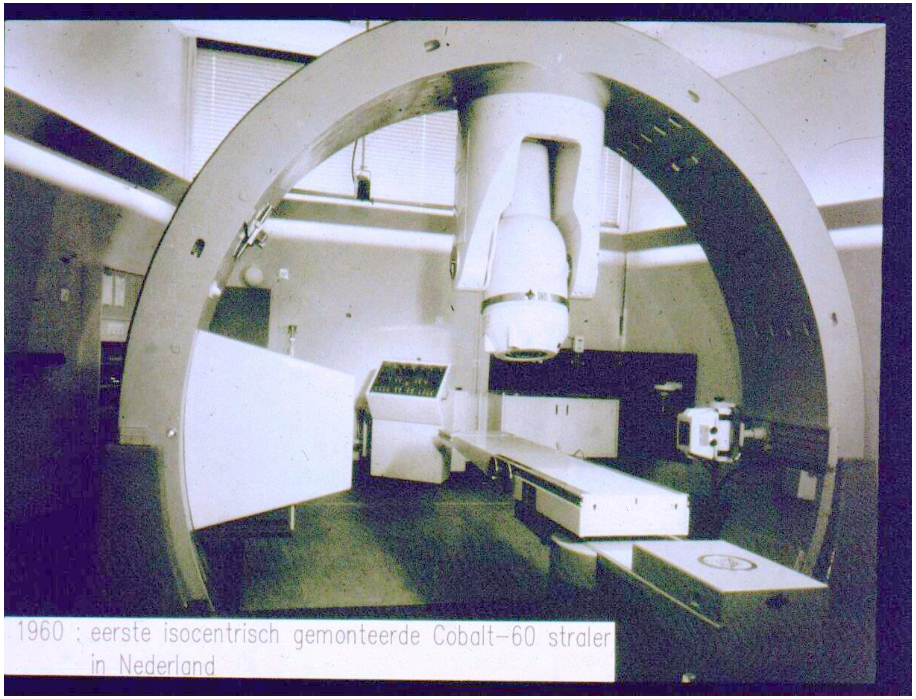
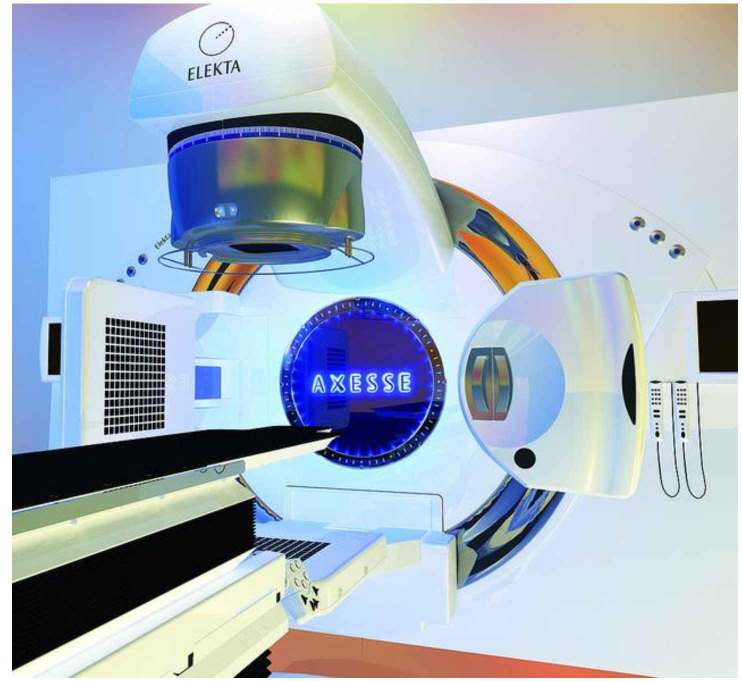


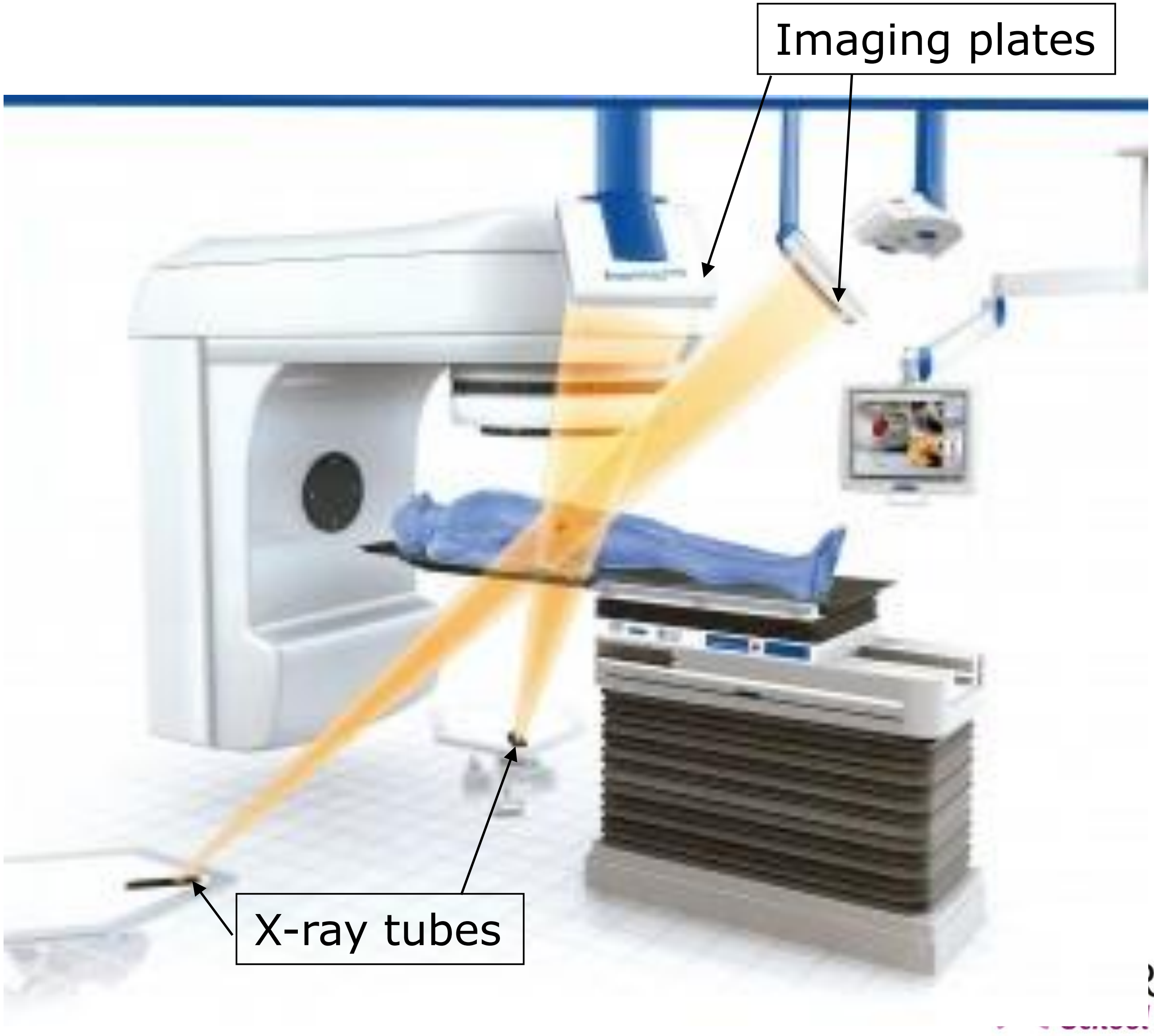
Image: Ben Mijnheer (NKI)

kV source moutend on linac

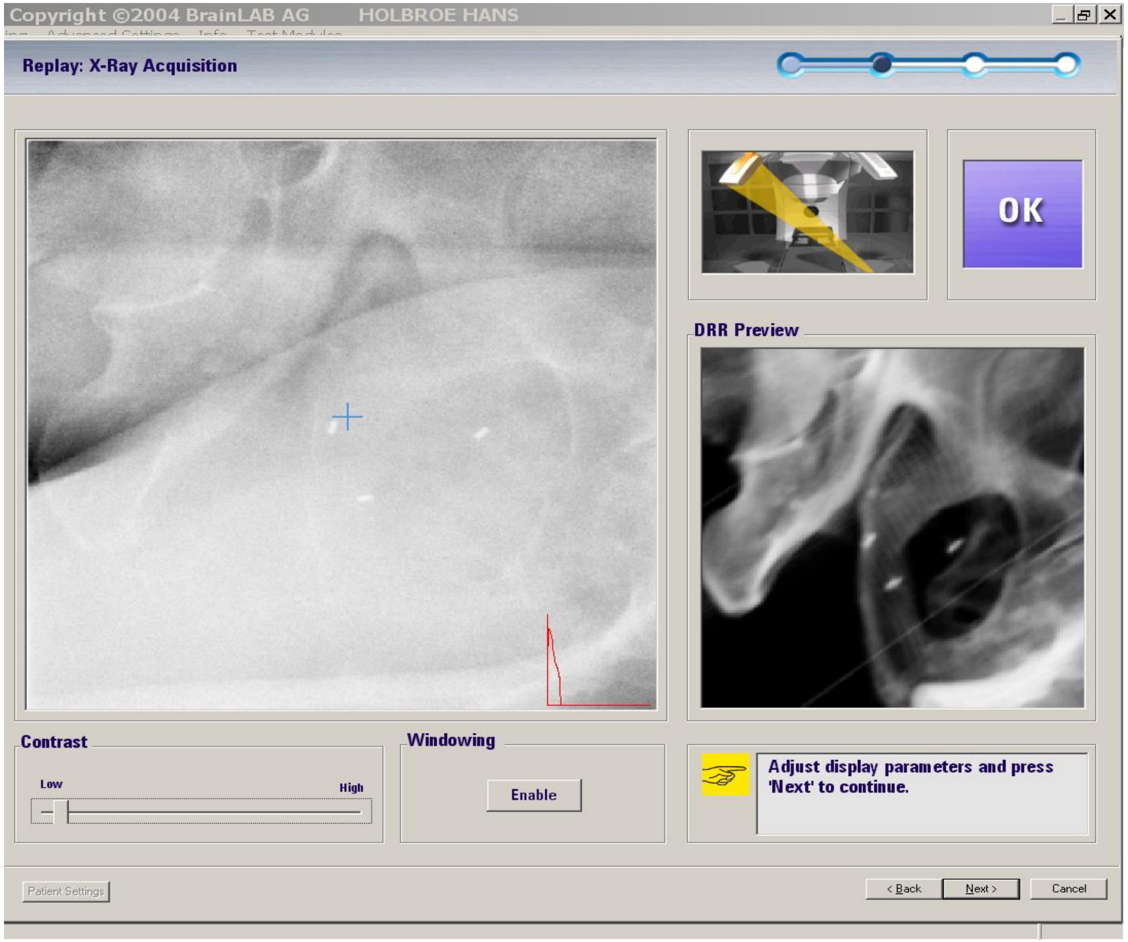


kV imaging: Cyberknife

Exac Trac® IGRT system



Exac Trac® IGRT system



Images: M.Josipovic

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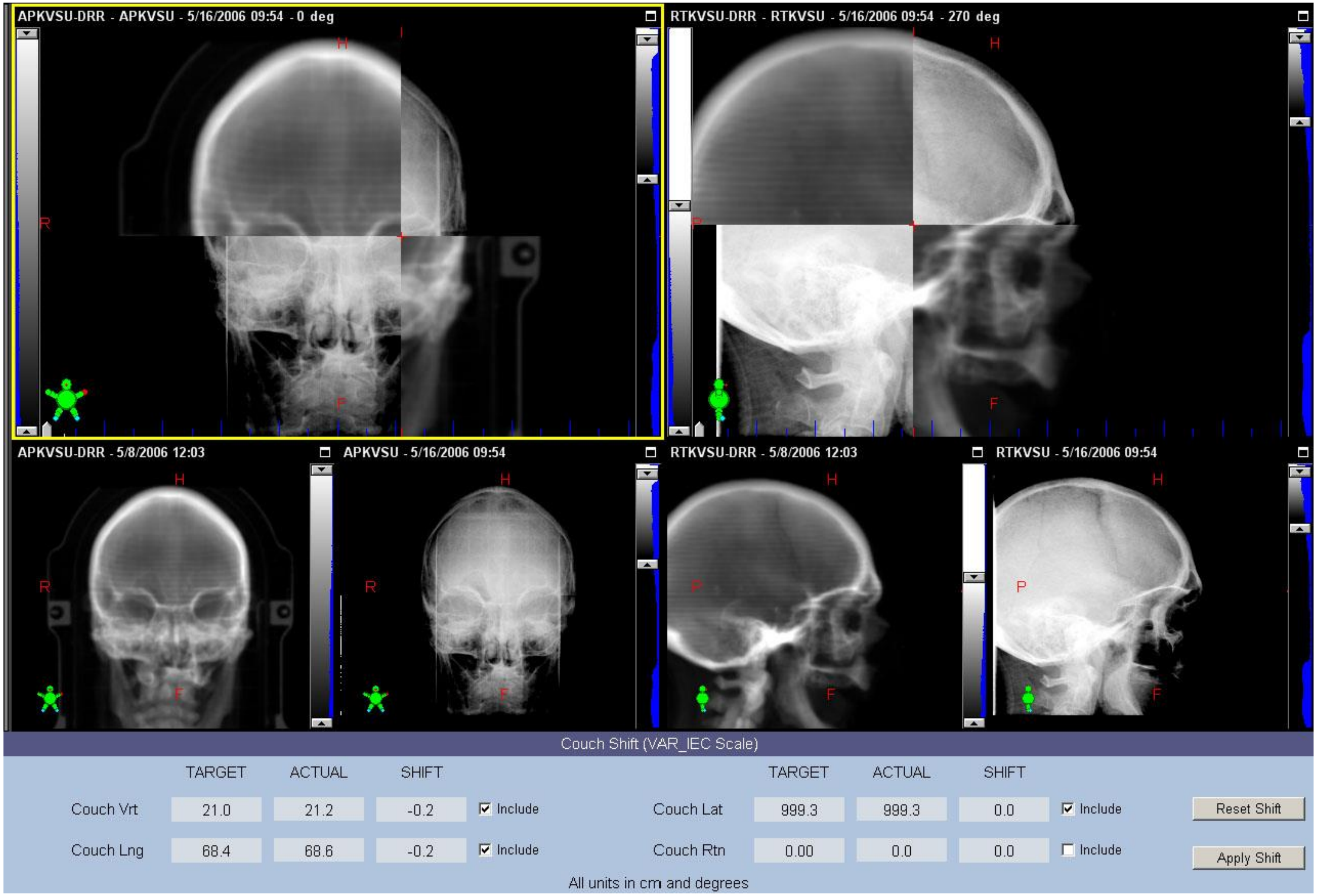
OBI kV imaging



Images: M.Josipovic

kV imaging

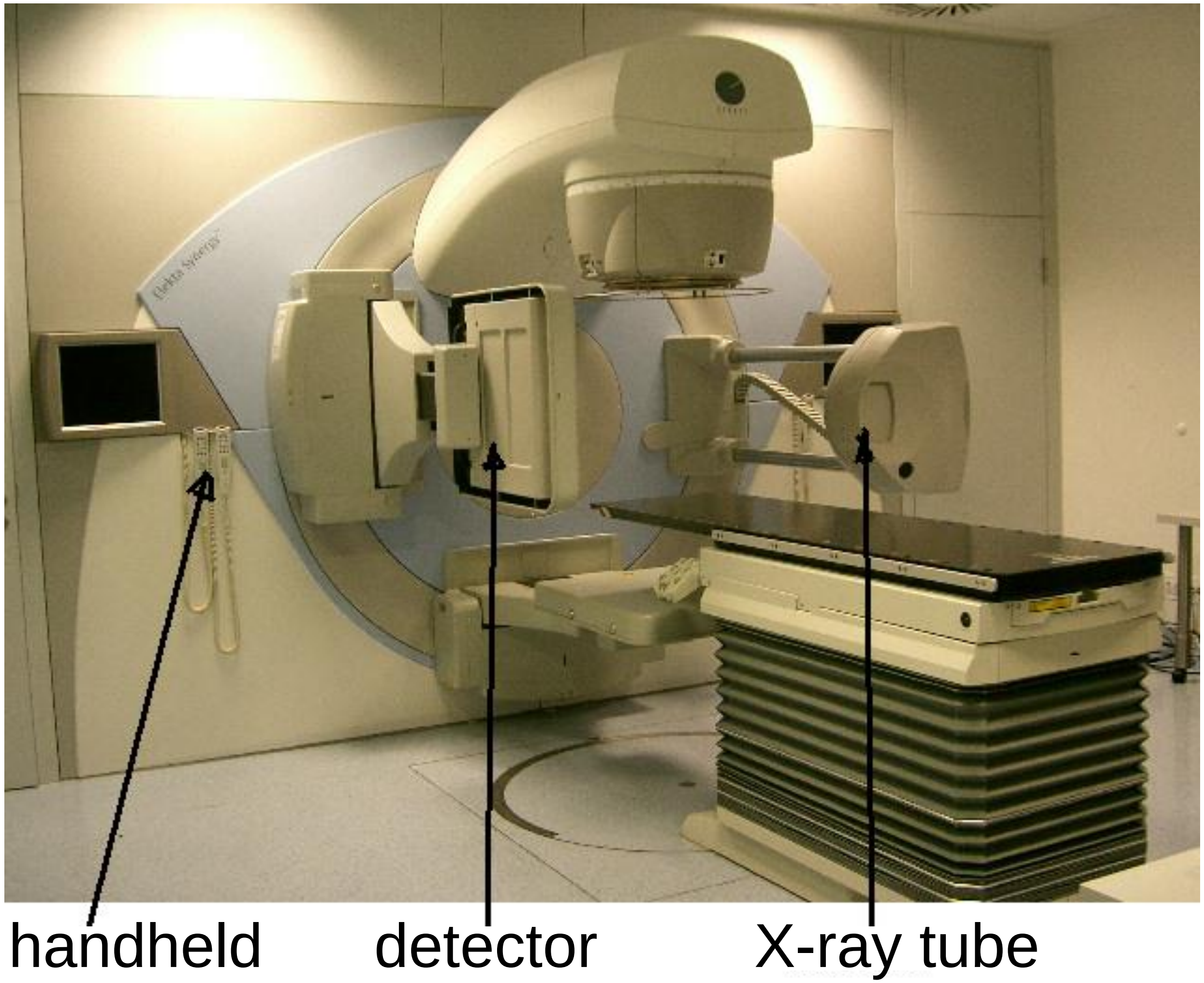
Pros:

- Imaging dose is low
- High 2D imaging quality
- Real time imaging in some systems (all angles)

Cons

- Limited anatomical information
- In most times it is a surrogate
- Oblique images are difficult to interpret.

Cone beam CT



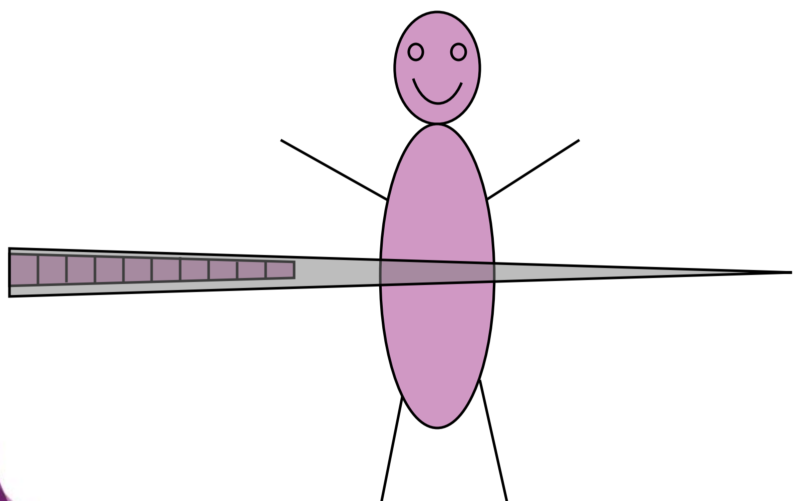
CBCT Acquisition

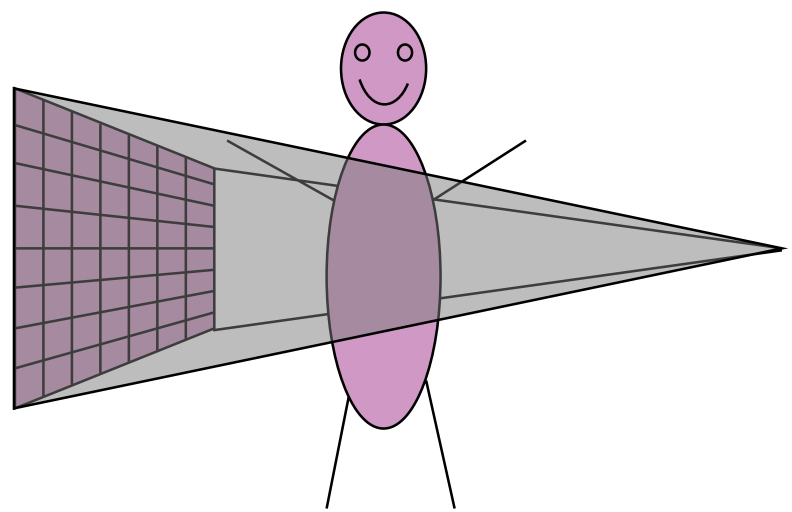
Conventional CT

- ‘Fan’ beam
- 1D detector
- 1 rotation = 1 slice

Cone-beam CT

- ‘Cone’ beam
- 2D detector
- 1 rotation = volume (many slices)

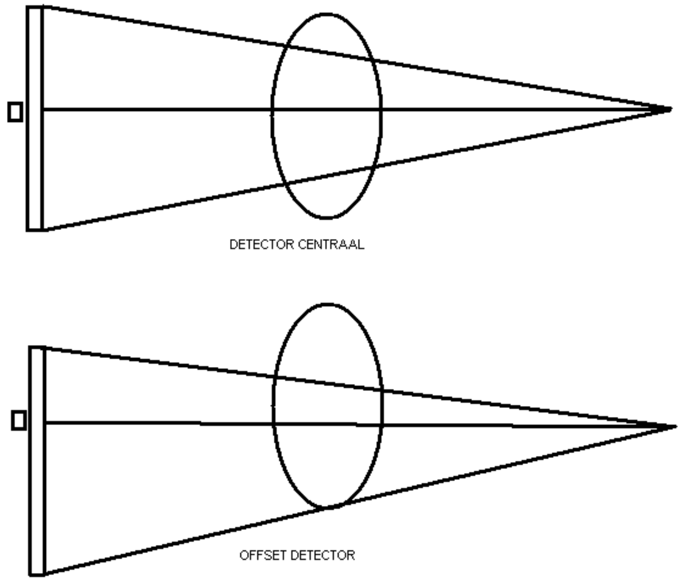




Courtesy: Peter Remeijer

How does it work?

Variable detector position



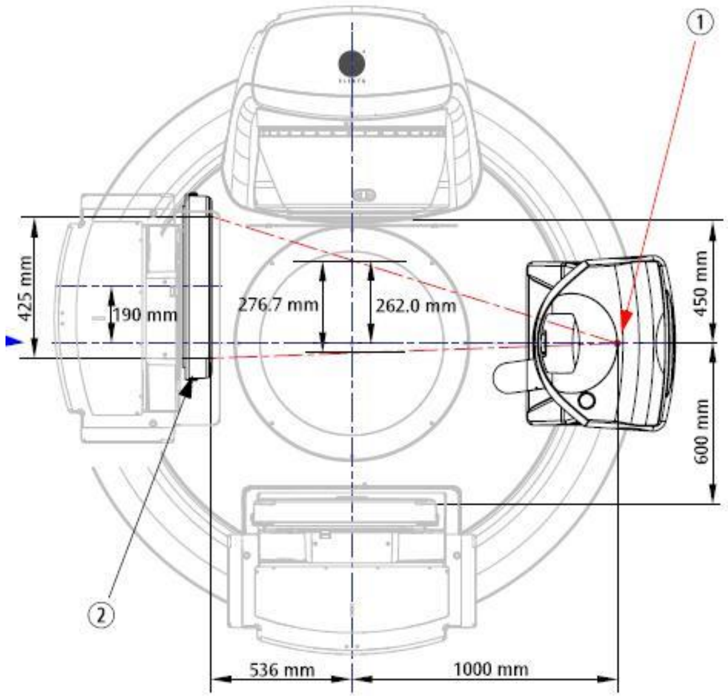


Image registration: Defining the ROI

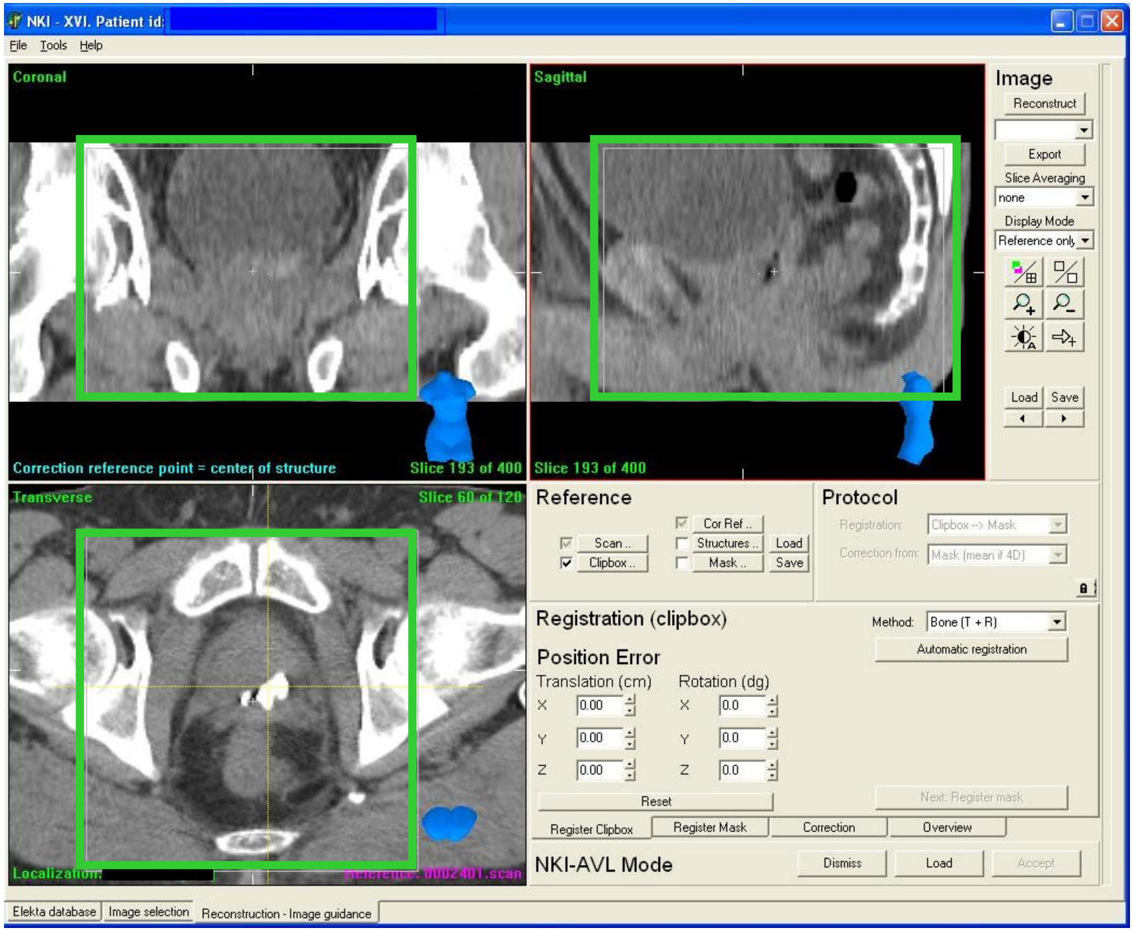


Image registration: Defining the ROI

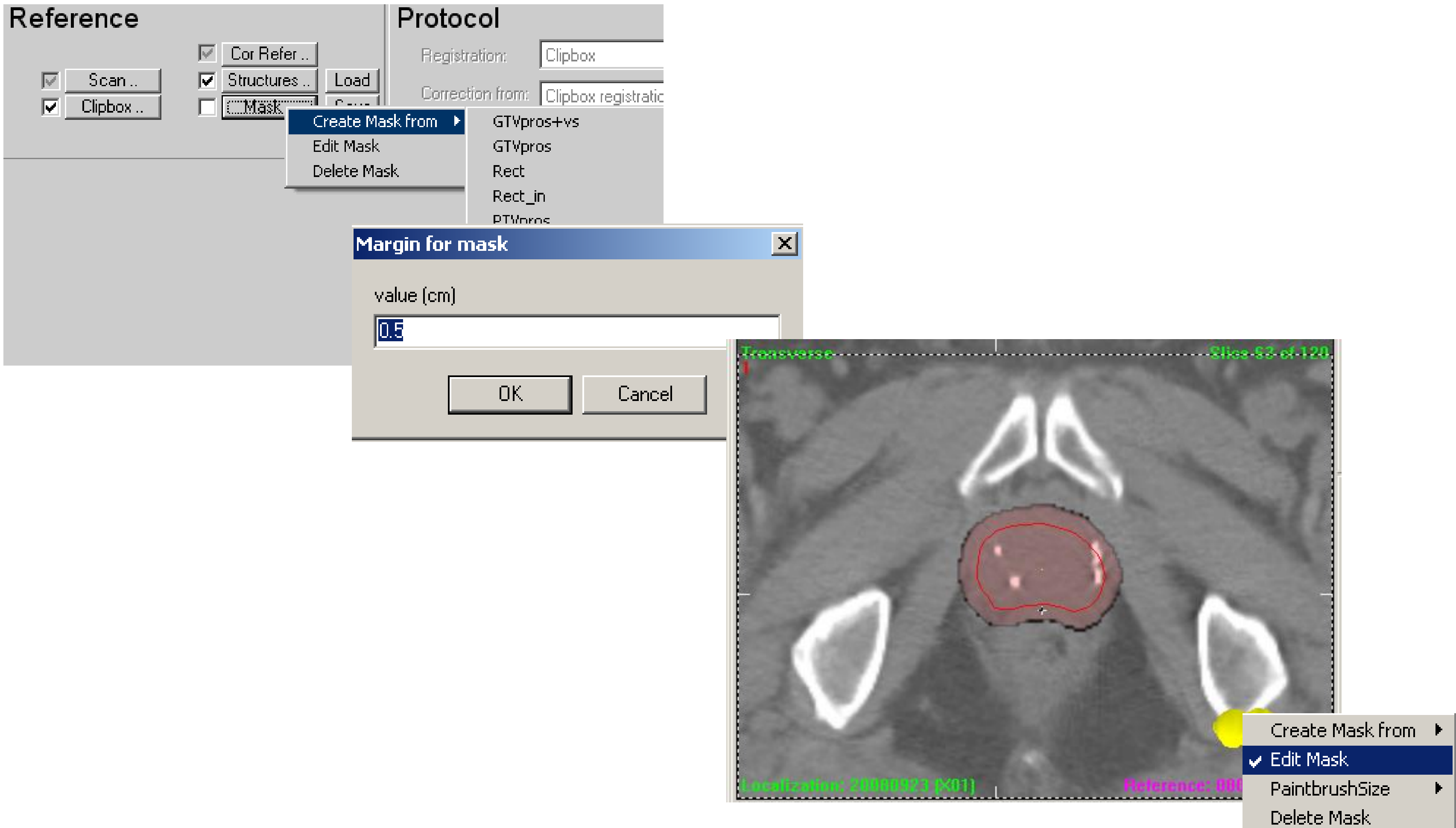


Image registration

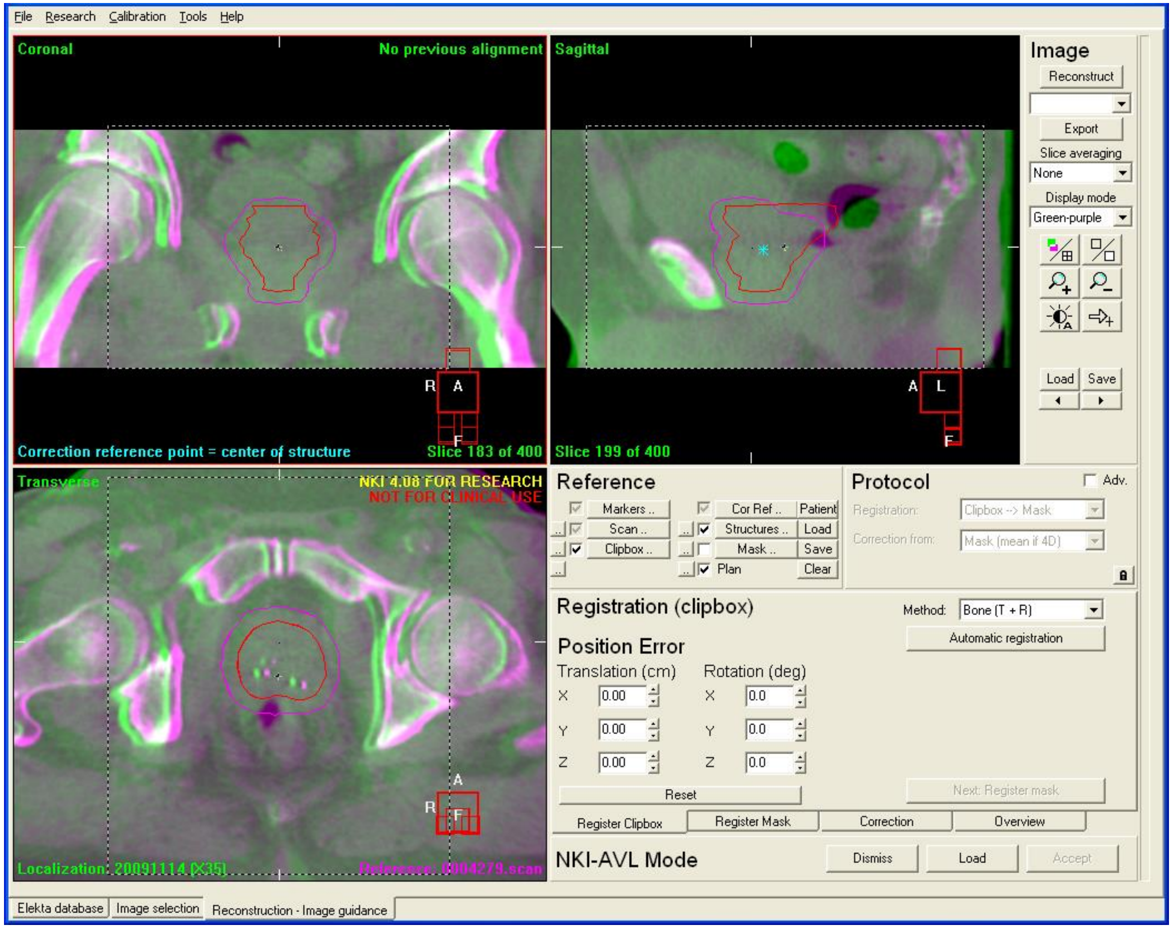


Image registration: bony anatomy

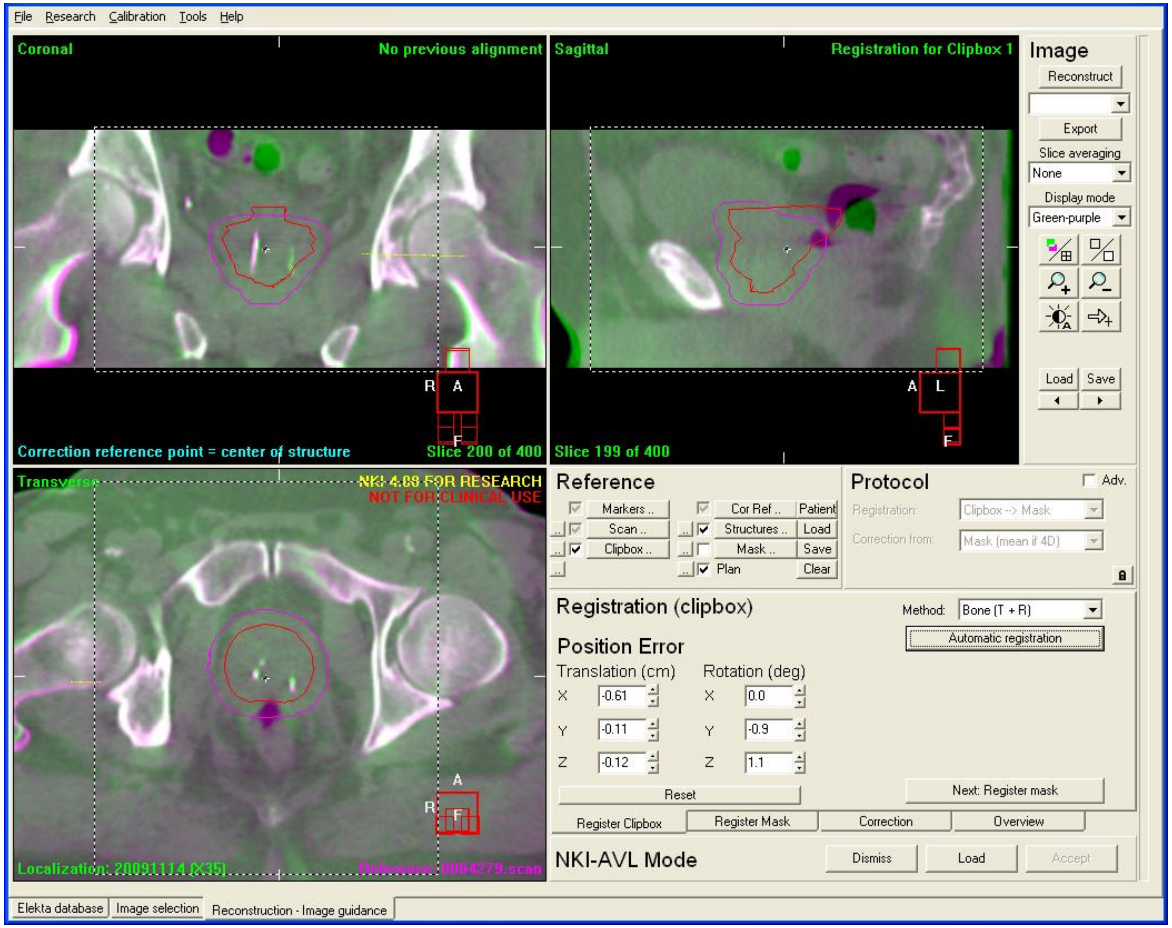
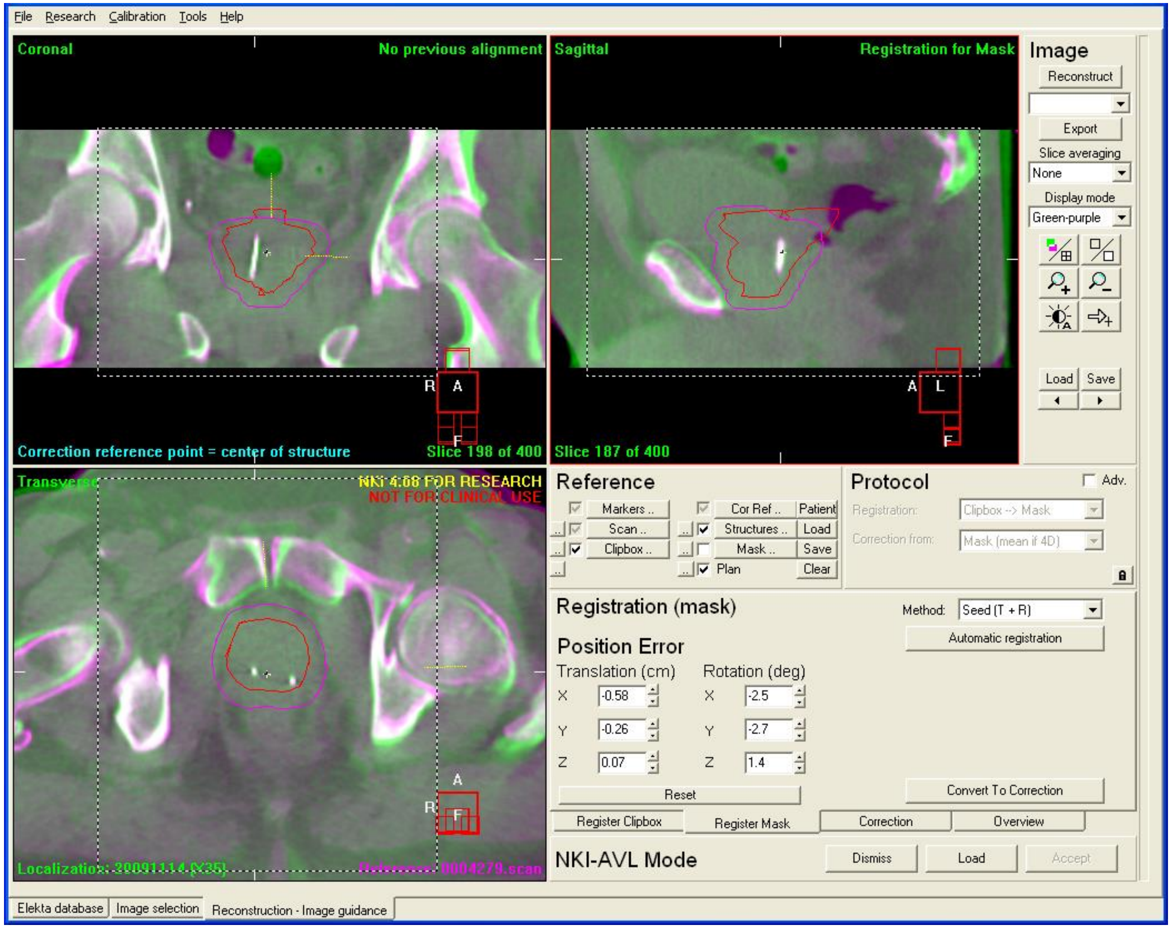


Image registration: fiducial markers



CBCT imaging

Pros:

- Anatomical information
- Imaging dose can be low
- Relatively high imaging quality
- Good to excellent registration algoritms

Cons

- Imaging dose can be substantial
- No real time imaging in some systems
  - Inline scanning still leads to retrospective analyses

MV-(CB)CT

Using:

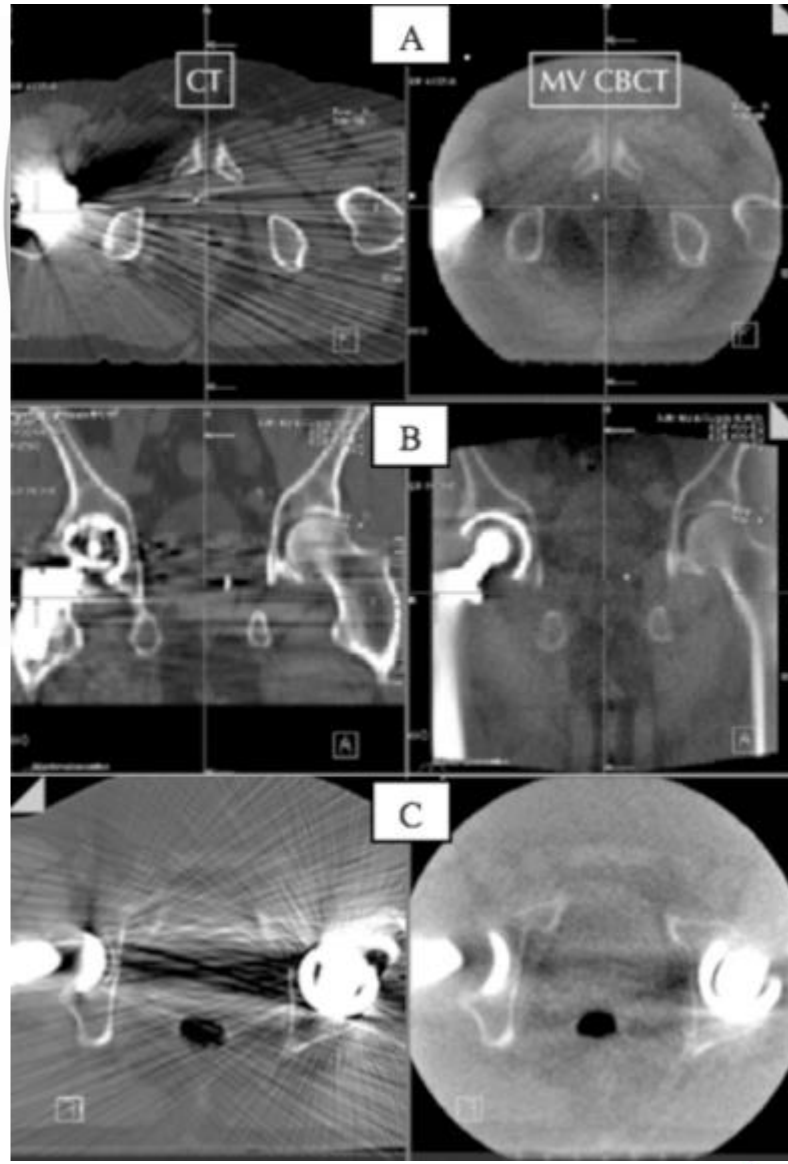
- ➢ Treatment beam
- ➢ Flat panel
- ➢ 3D acquisition

MV-CT:

- ➢ Helical acquisition
- ➢ TomoTherapy

MV-CBCT:

- ➢ 360 degrees acq.
- ➢ Siemens Oncor



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MV-CT

Pros:

- Anatomical information
- Limited influence of high densities (prostheses)
- Image of the actual absorbed dose

Cons

- Image quality not as good as kV CBCT
- Imaging dose
- Only available as Siemens

Videosystems

Different approaches:

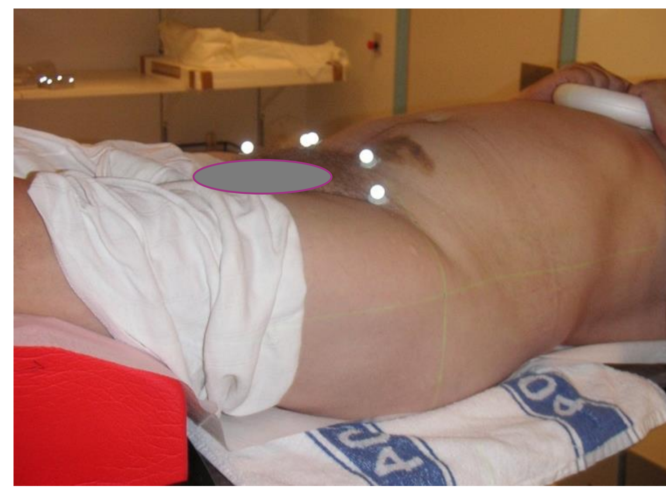
- Infrared tracking of external markers
- Surface scanning

What can you do with these systems?

- Set-up aid
- More important: monitor the patient during treatment:
    1. Passive: monitoring set-up accuracy
    2. Active: correlate motion with treatment (e.g. gating or DIBH)

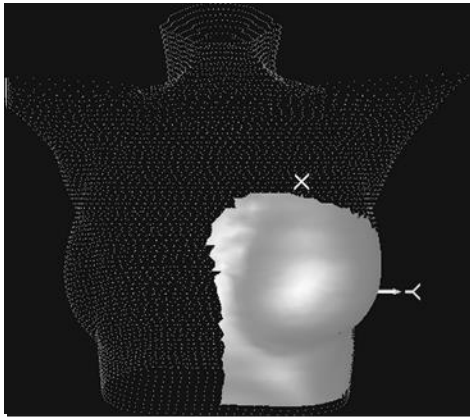
Exac trac infrared

- Infrared marker,
  - placed on fixed spots
- Tracking of the markers during RT
  - Correlate with respiration (tracking/gating)

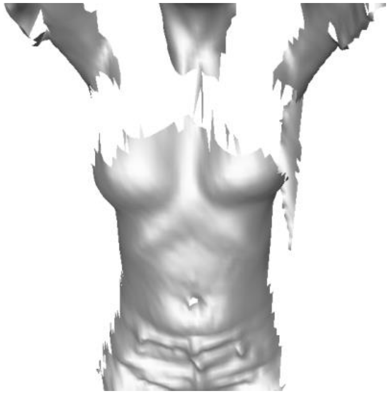


Images: M.Josipovic

Surface scanning



Left side



Images: T.Alderliesten

Infra red systems

Pros

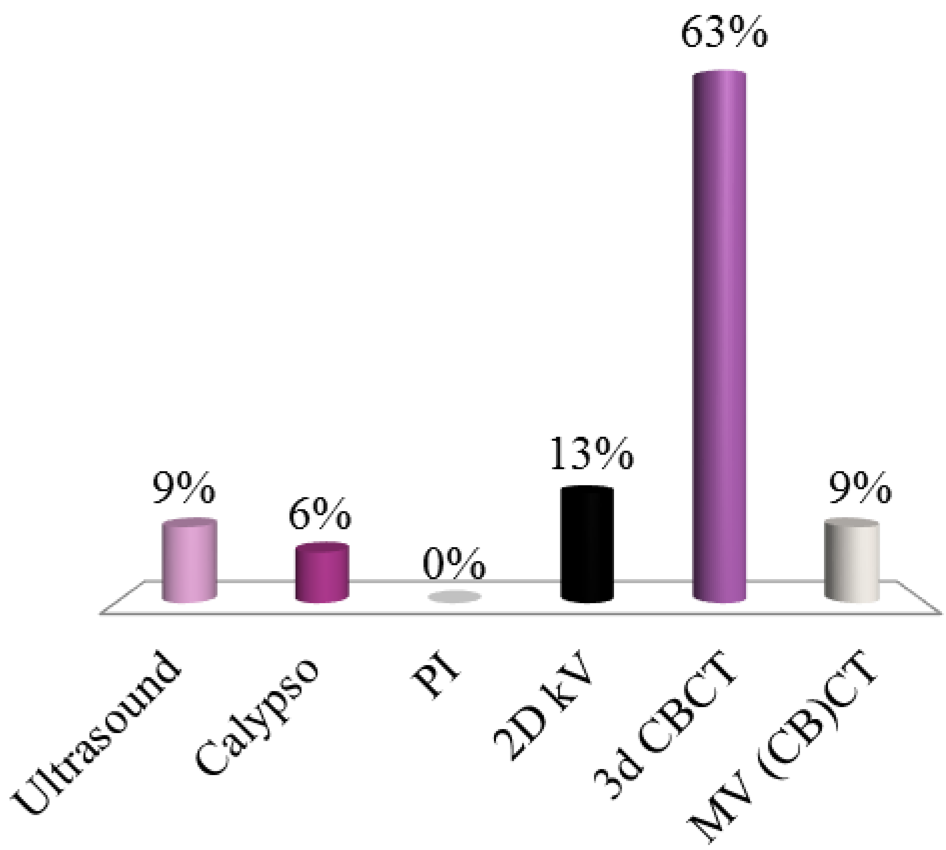
- No imaging dose
- Enables tracking and gating
- Real time measurements
- Surface scanning:
  - ➢ Pre treatment set-up check

Cons

- It’s an aid
  - ➢ Can never be a stand alone system
- Surrogate

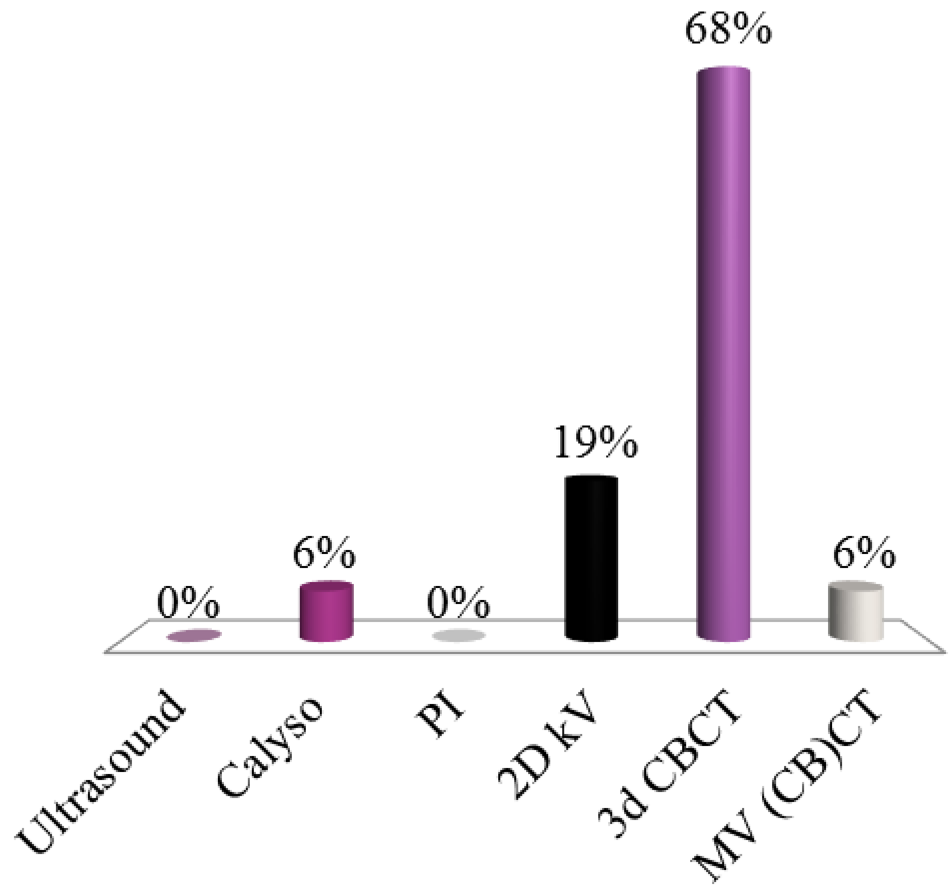
Which one do you prefer most in prostate?

A. Ultrasound
B. Calypso
C. PI
D. 2D kV
E. 3d CBCT
F. MV (CB)CT



Which one do you prefer most in lung?

A. Ultrasound
B. Calyso
C. PI
D. 2D kV
E. 3d CBCT
F. MV (CB)CT



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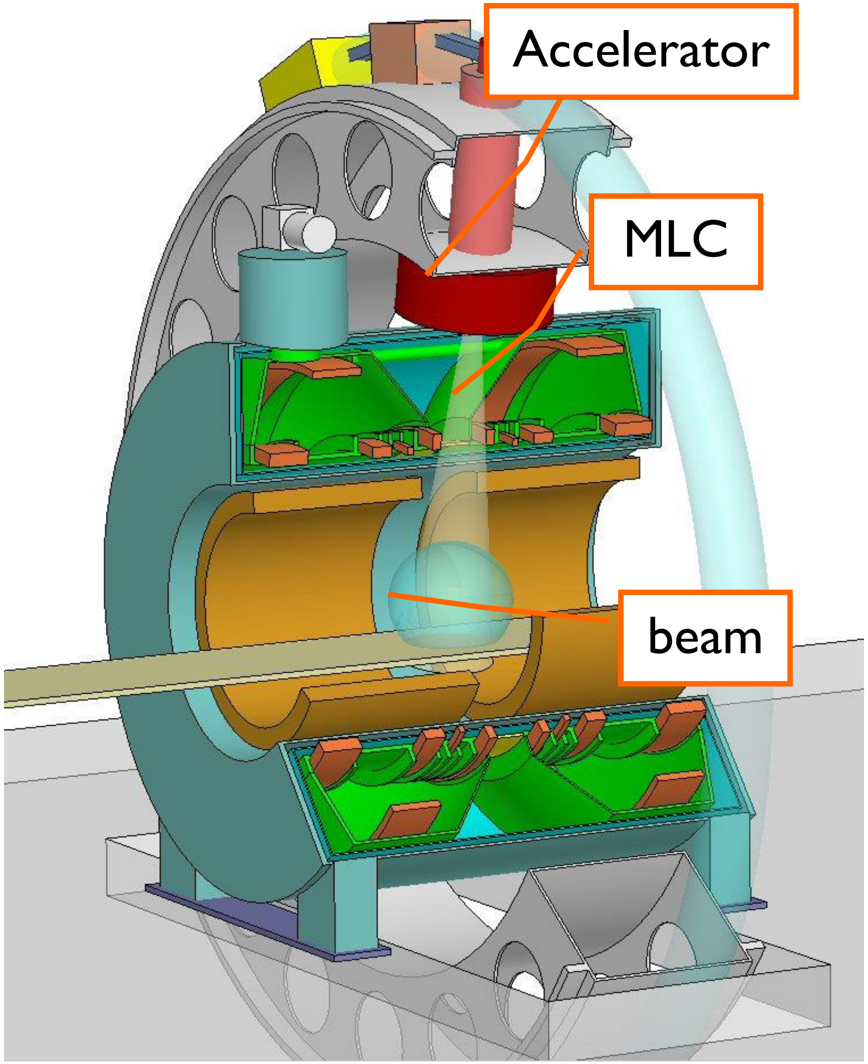
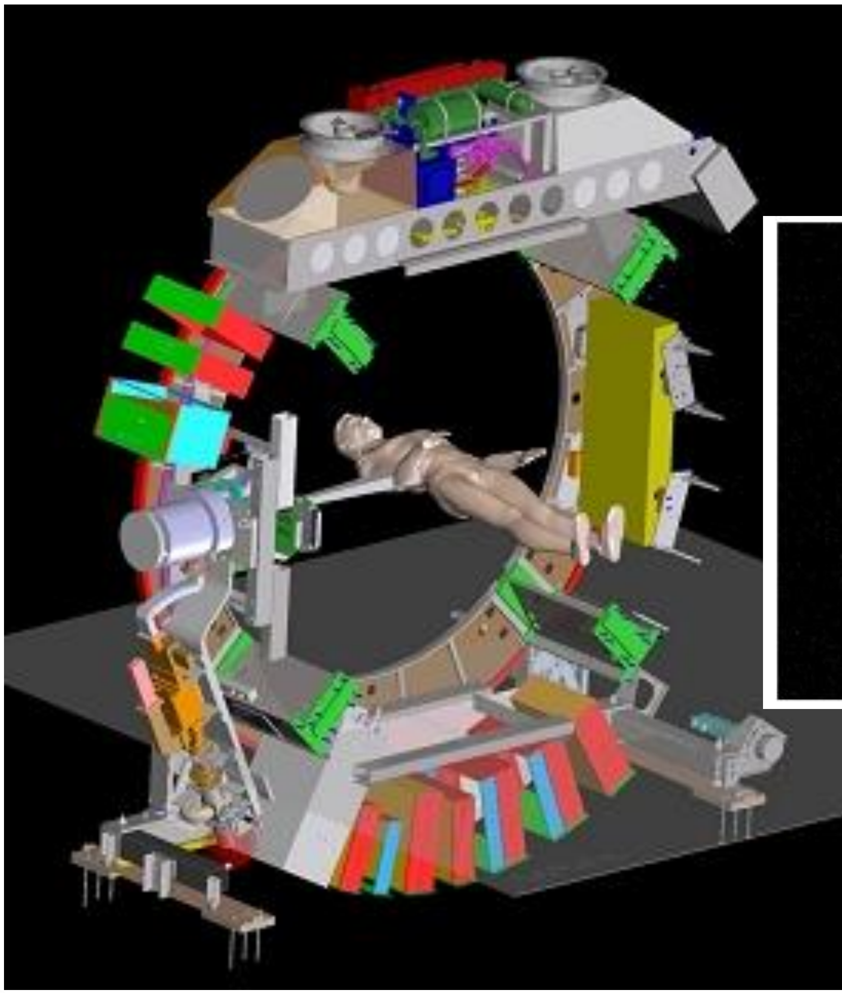
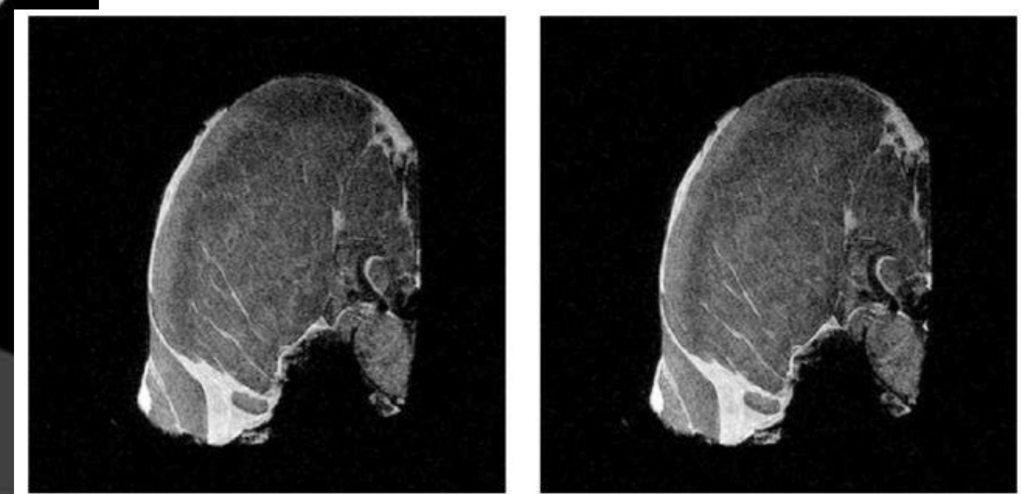
Integrating MRI functionality with external beam radiotherapy



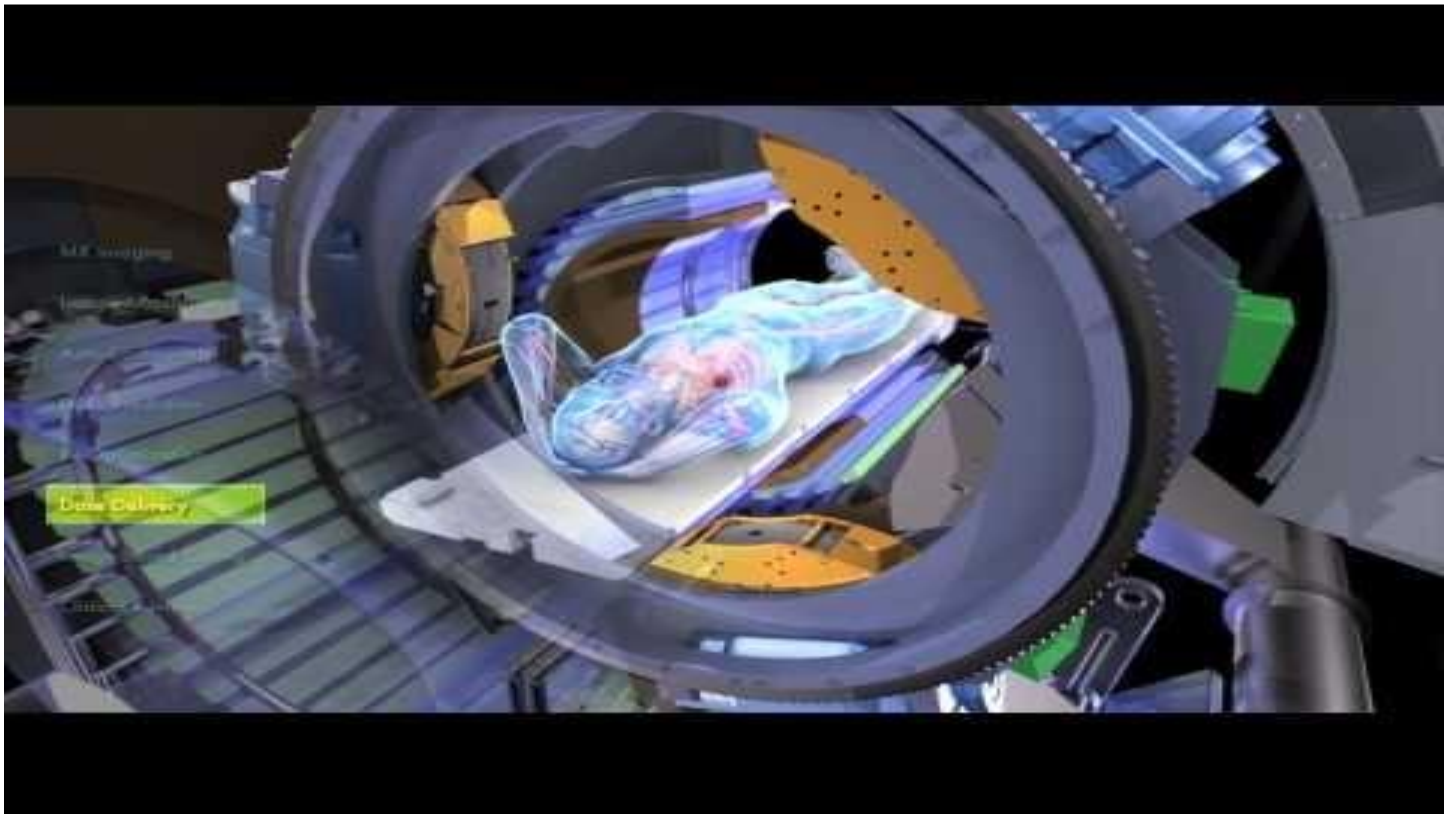
Integrating MRI functionality with external beam radiotherapy

Gantry design MRL: (MRI-Linac)





MRIdian: MR Cobalt



MR linac

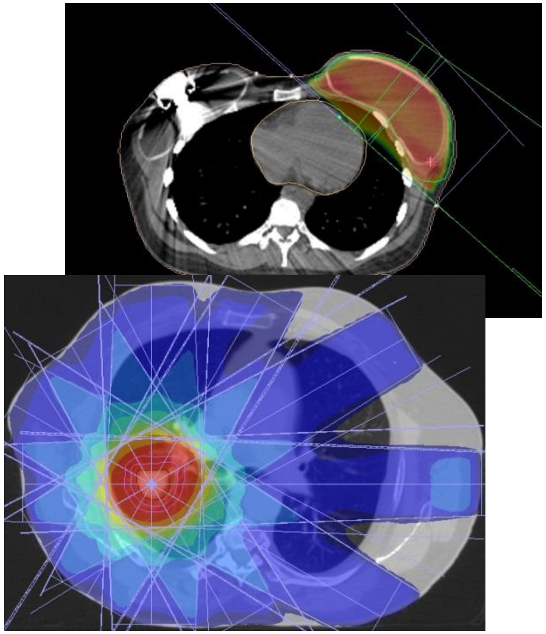
Pros

- Optimal image quality
- Intra fraction imaging

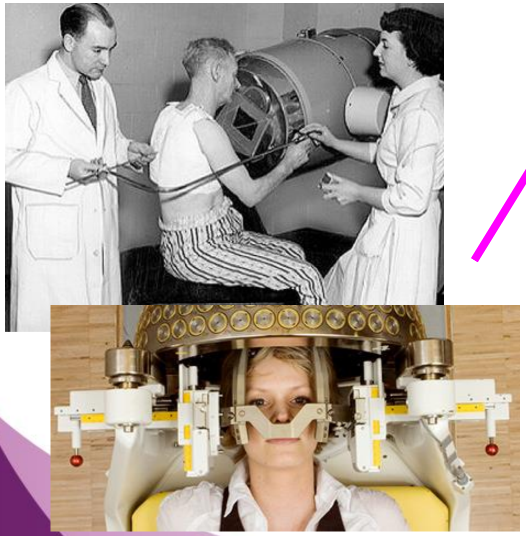
Cons

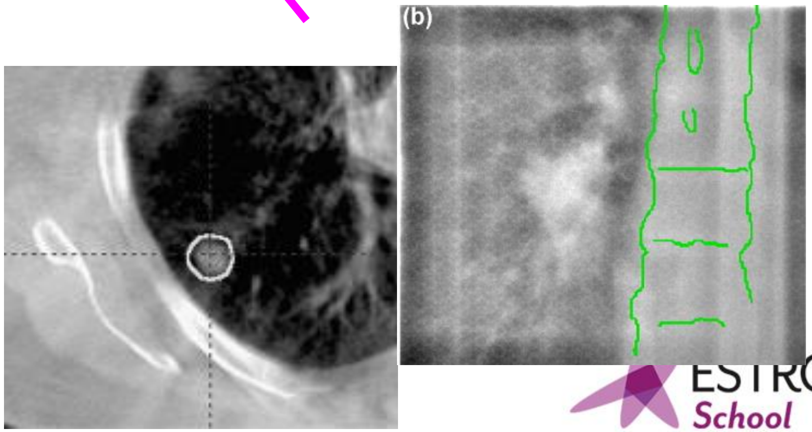
- MR-Linac:
  - ➢ quite expensive
  - ➢ Under development, mainly research
- Cobalt treatment: linac upcoming
- Challenging Treatment planning (1,5 Tesla)
  - ➢ Secondary electrons are influenced by the magnetic field

How accurate should the delivery be?



Balance!





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Clinical rationale for image-guided radiation therapy (IGRT)

Jose Lopez, M.D., Ph.D
Radiation Oncology
University Hospital Virgen del Rocio
Seville, Spain

Advanced skills in modern radiotherapy
Prague, Czech Republic –11-15 June 2016

Learning Objectives (IGRT)

- Learn the **clinical rationale** for IGRT
  Why we should do it

- Learn the challenges in achieving **precision and accuracy**

- Understand the **benefits and limitations** of IGRT

- Learn the **evidence** that supports the use of IGRT

Peterpedia

Wikipedia

- IGRT is the process of frequent **two and three-dimensional imaging**, during a course of RT, **utilizing the imaging coordinates**.

- The patient is localized in the treatment room in the **same position as planned** from the reference imaging dataset.

- An example of IGRT would include:

 - localization of a **CBCT** dataset with the planning **CT** dataset
 - matching planar **kV** or **MV** images with **DRRs**

Why do we need IGRT?

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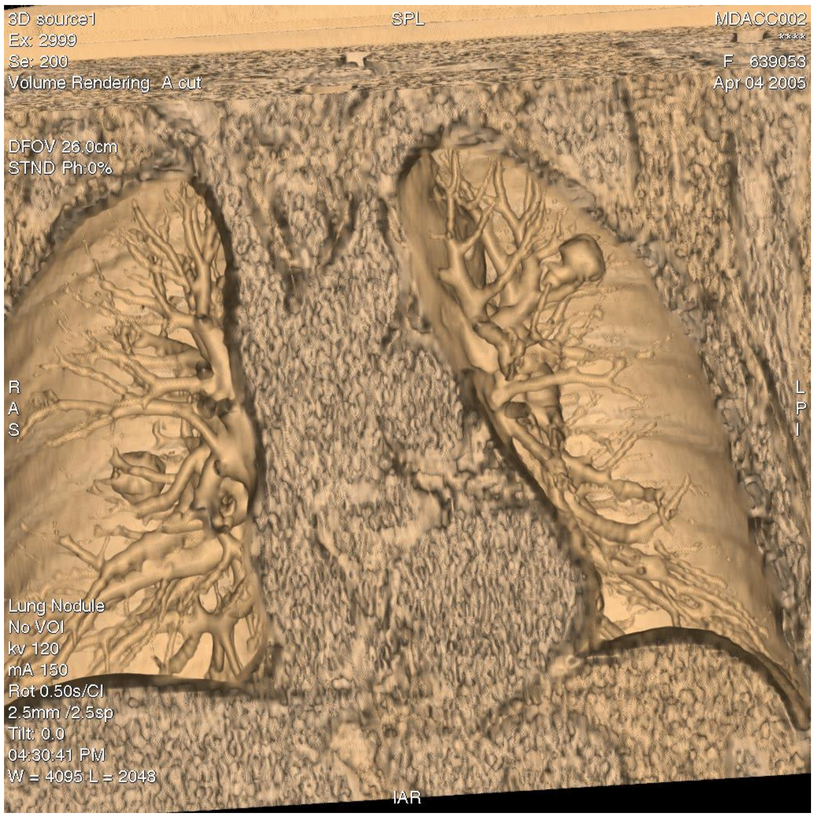
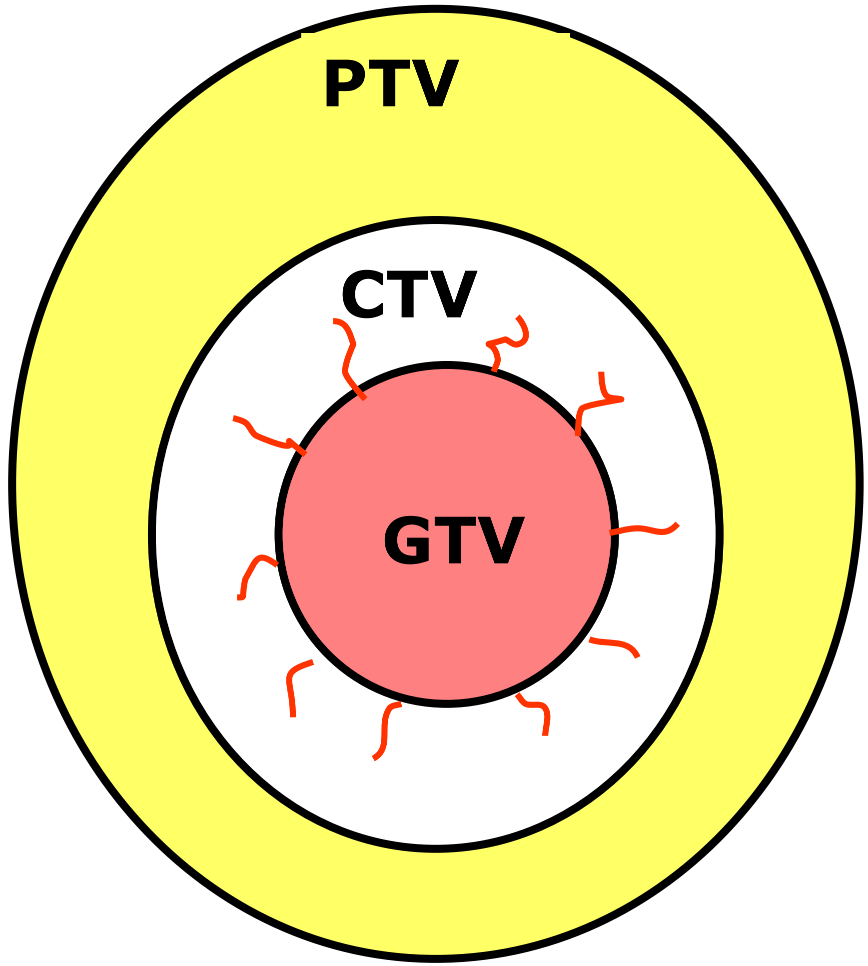
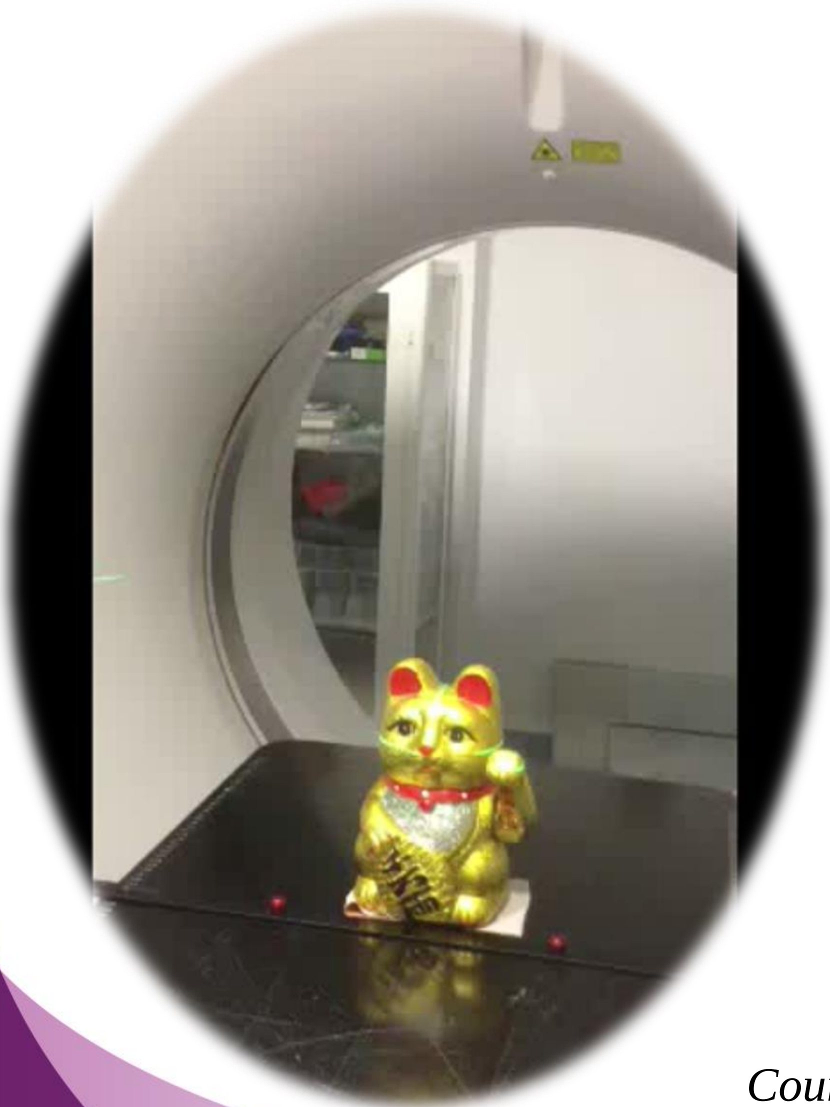
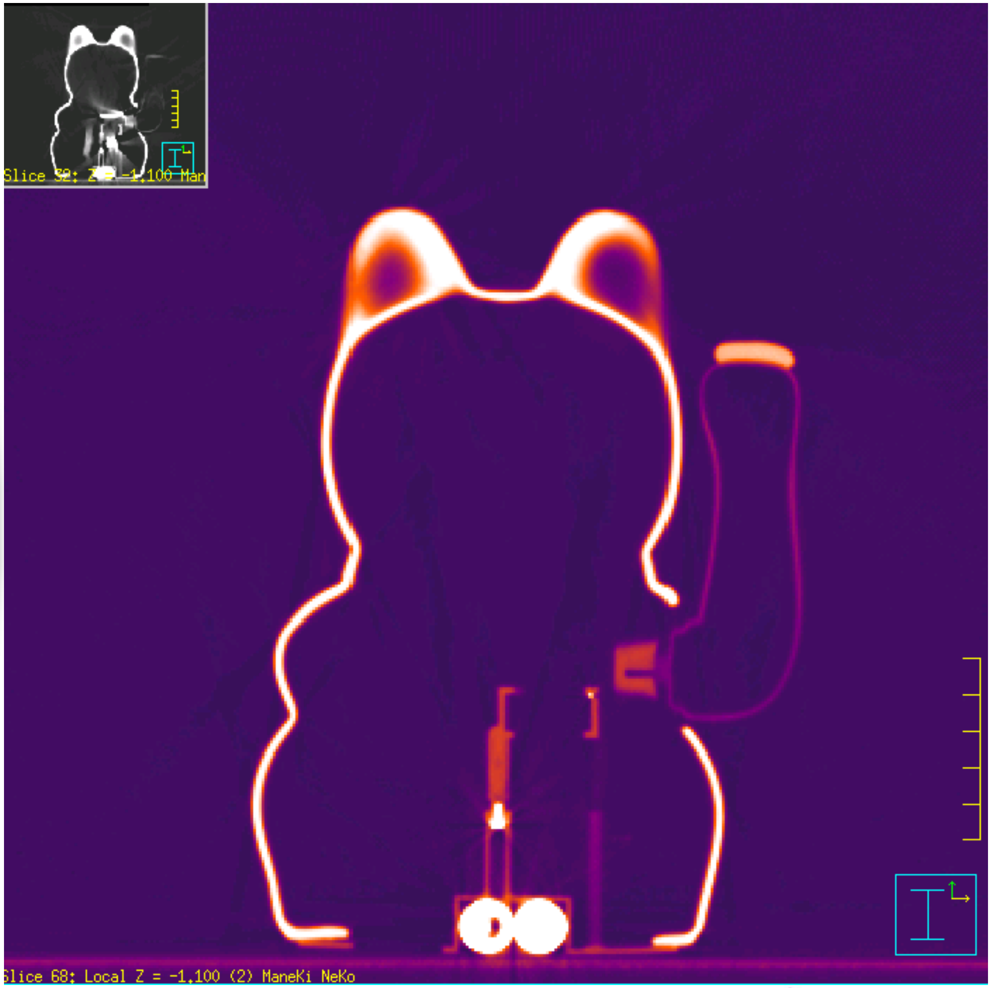
Tumor motion

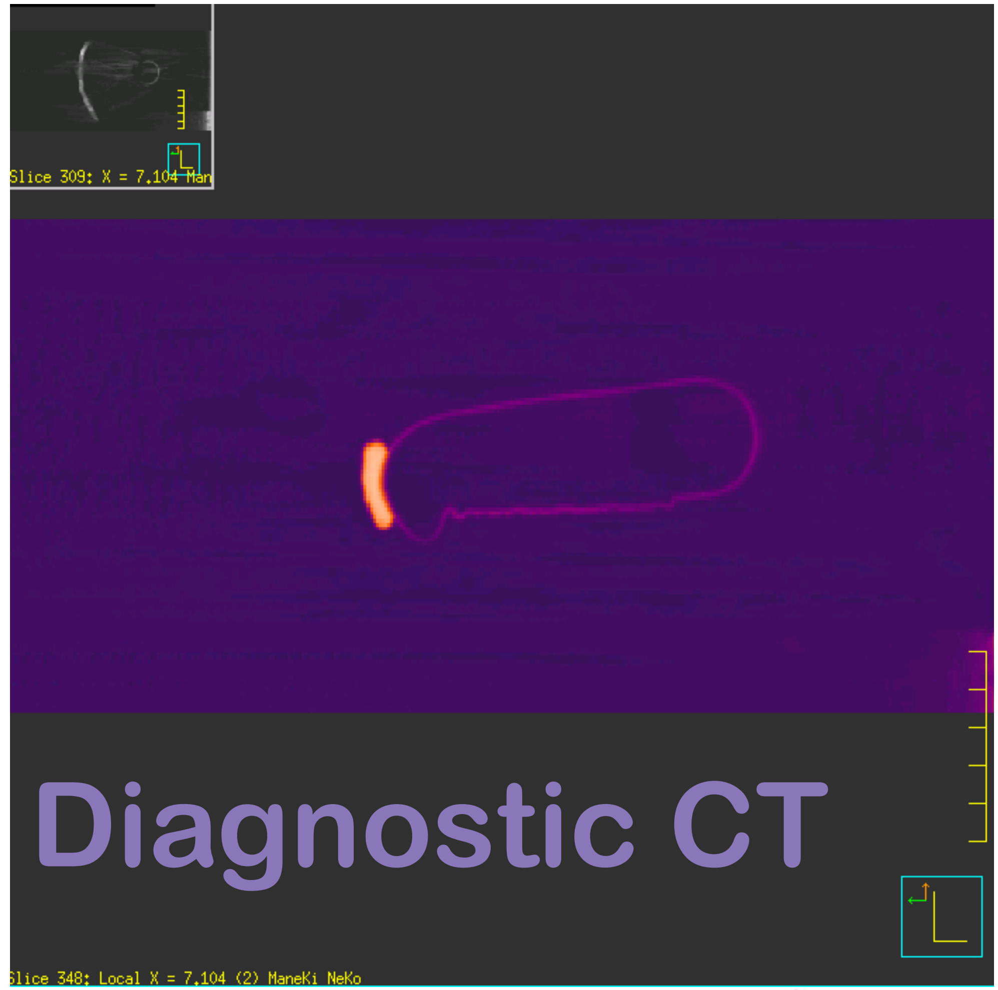




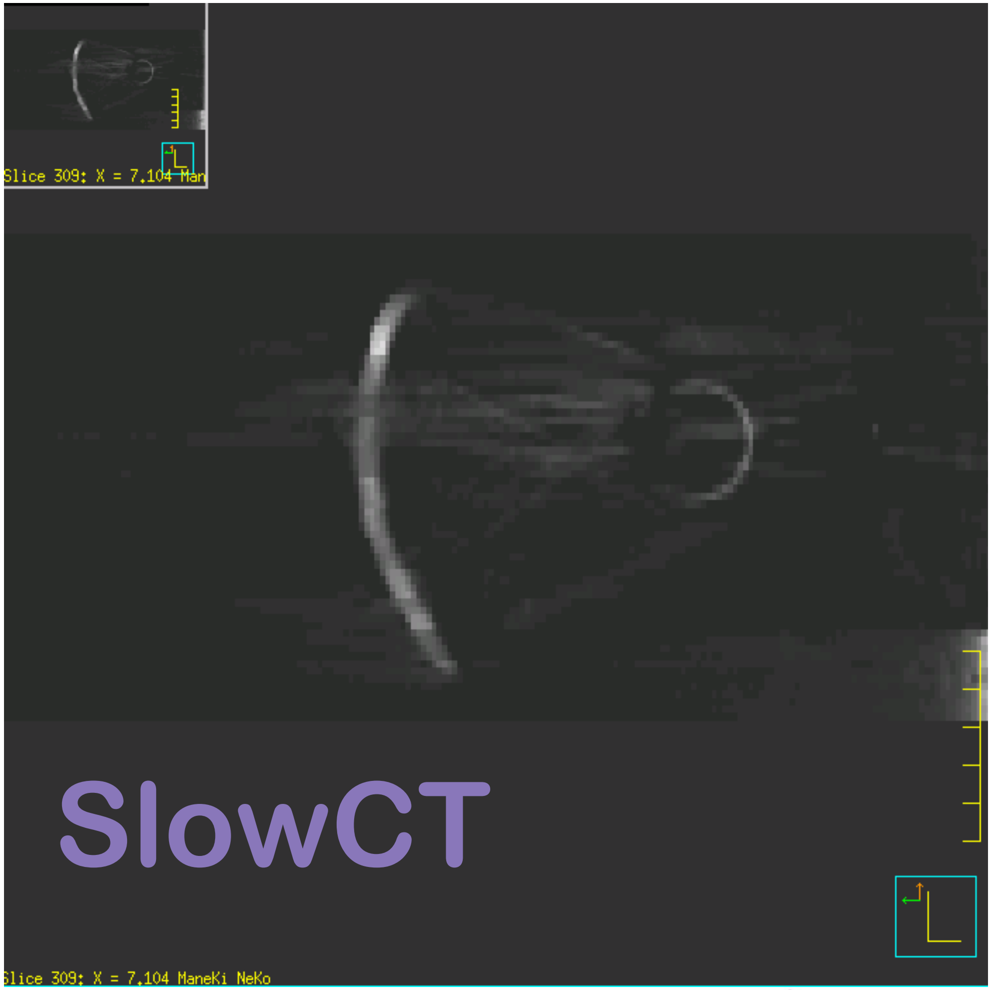




Courtesy Santiago Velazquez

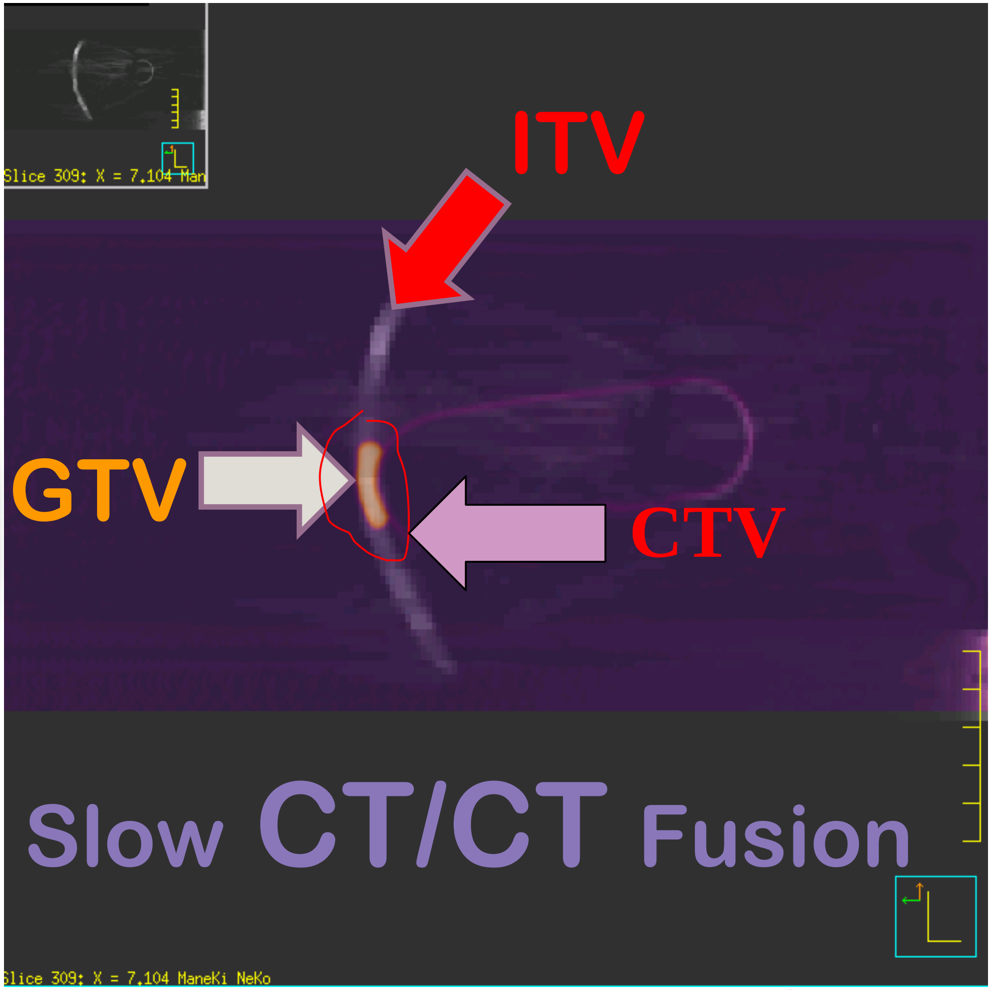


Courtesy Santiago Velazquez



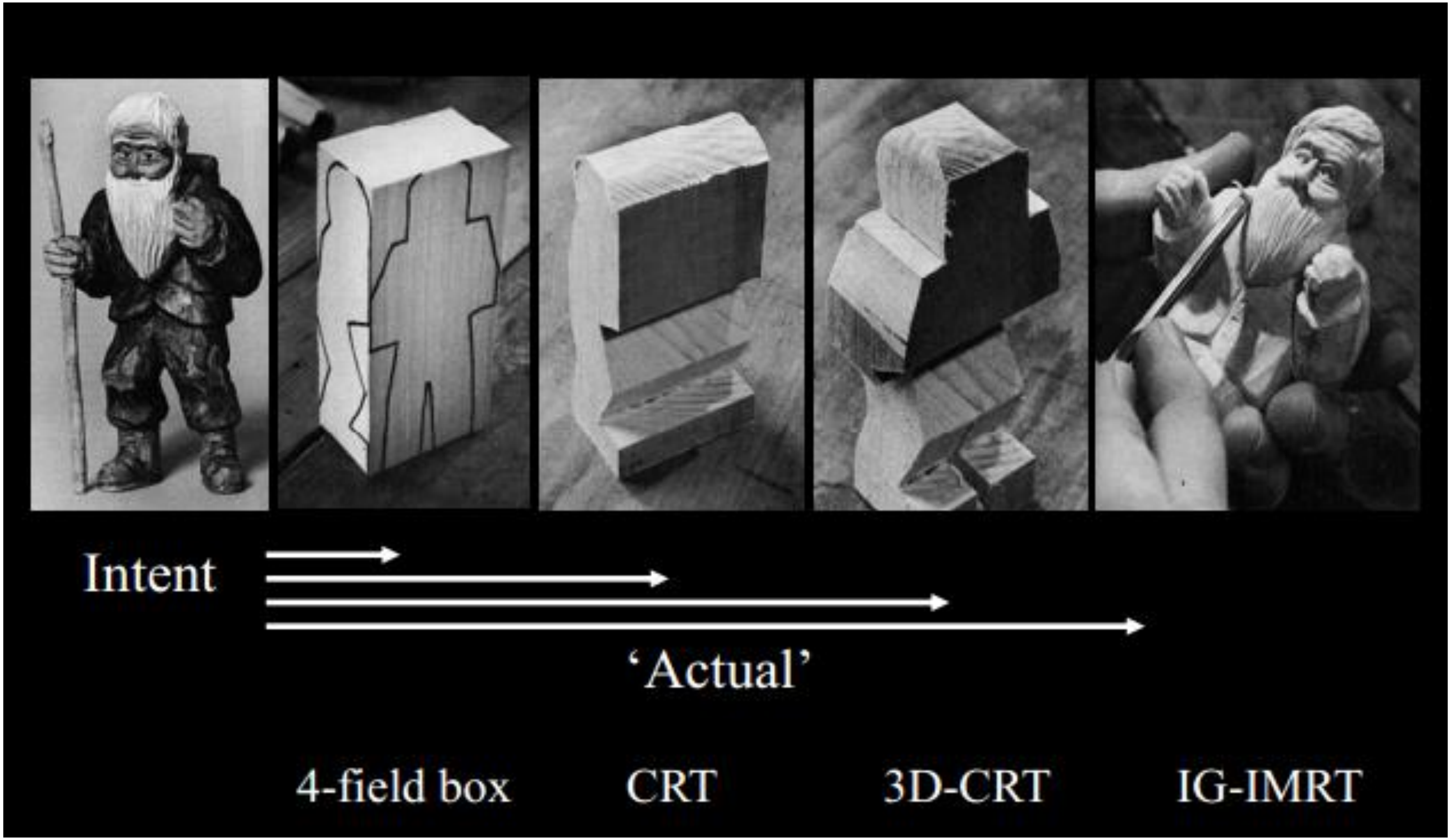
Courtesy Santiago Velazquez

SlowCT/CT Fusion

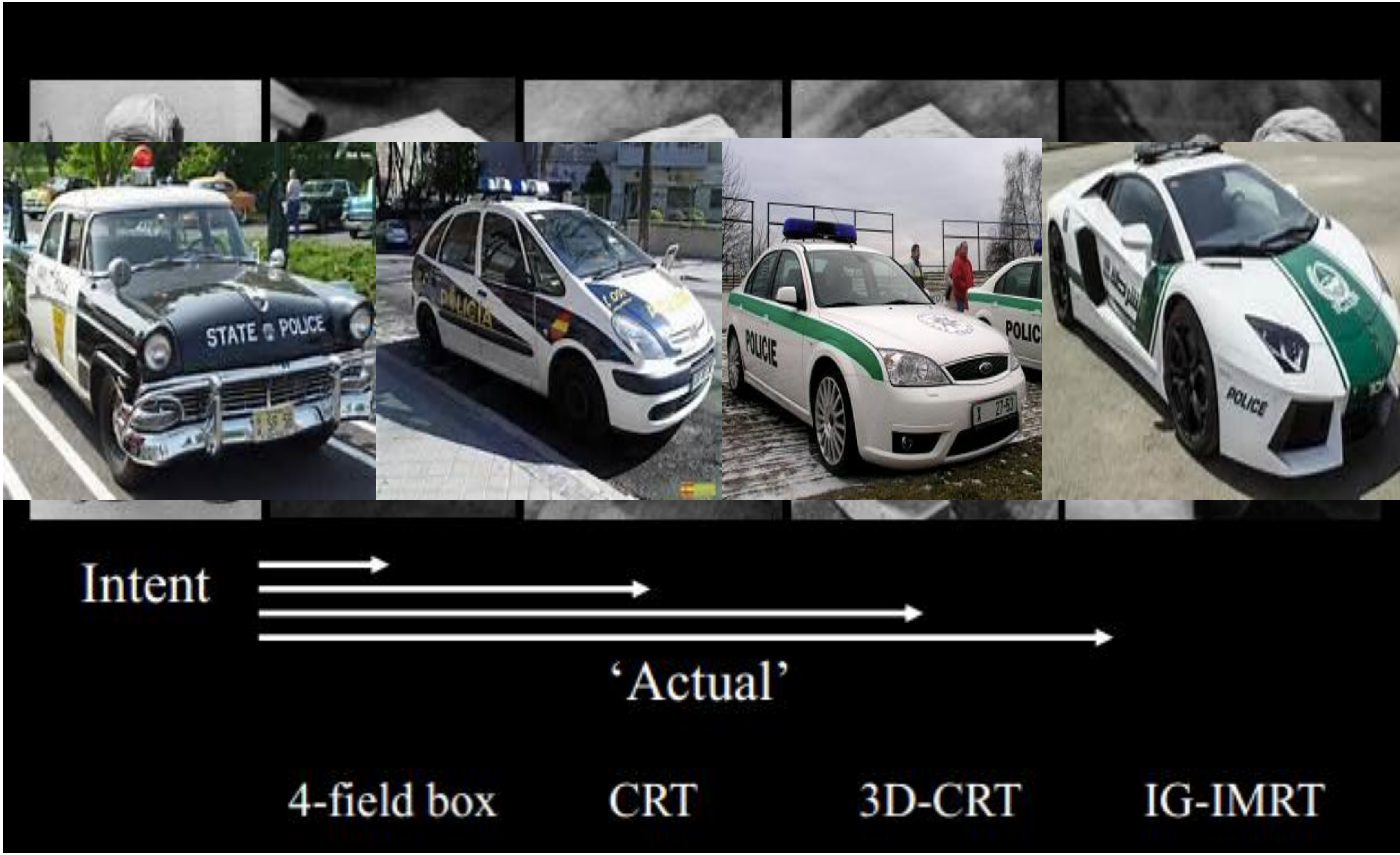


Courtesy Santiago Velazquez

IGRT



http://www.astro.org/uploadedFiles/Main_Site/Meetings_and_Events/Spring_Refresher_Course/Meeting_Program/Jaffray%20Physics.pdf



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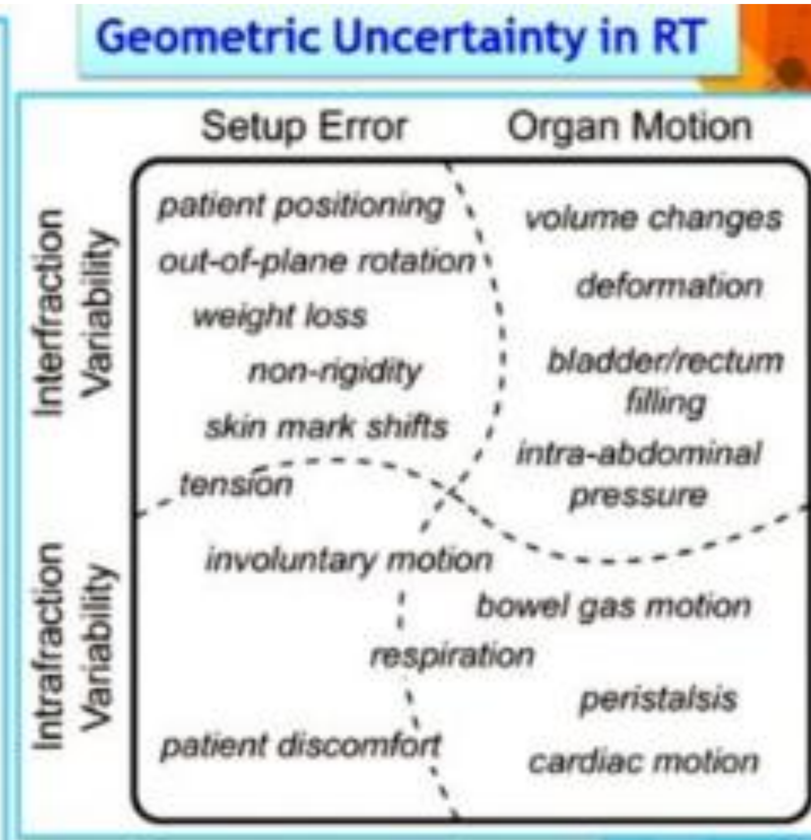
Rationale for IGRT

Quality of Radiotherapy Delivery

- Quality of radiotherapy (RT) delivery is one of the important determinants of patient outcomes
- Efforts to improve the quality of RT delivery include:
  - Accurate target delineation
  - Robust plan optimization
  - Minimizing day-to-day setup variation
  - Tracking intra-fractional organ motion
  - Monitoring & adapting to inter-fractional tumor and normal tissue changes
  - Enhance deliverability (spatial access)

IGRT



Jaffray – ASTRO 2012

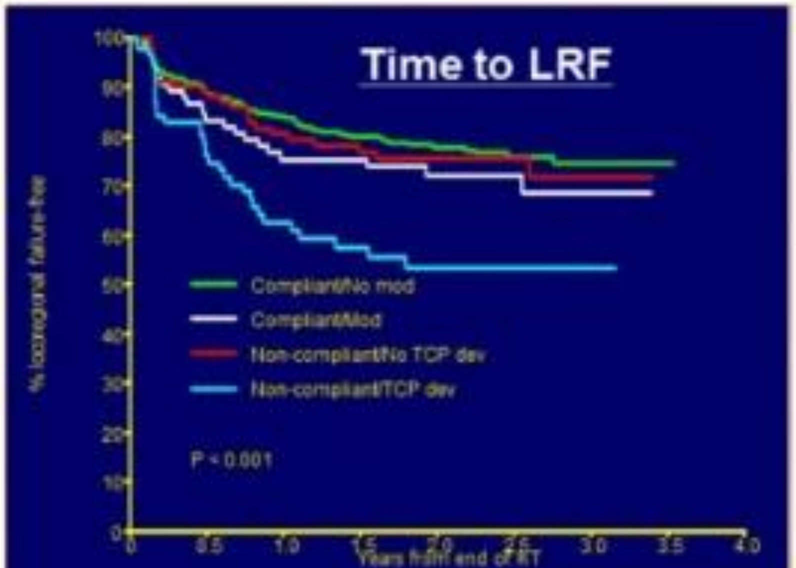
VOLUME 28 · NUMBER 18 · JUNE 20 2010
JOURNAL OF CLINICAL ONCOLOGY
ORIGINAL REPORT

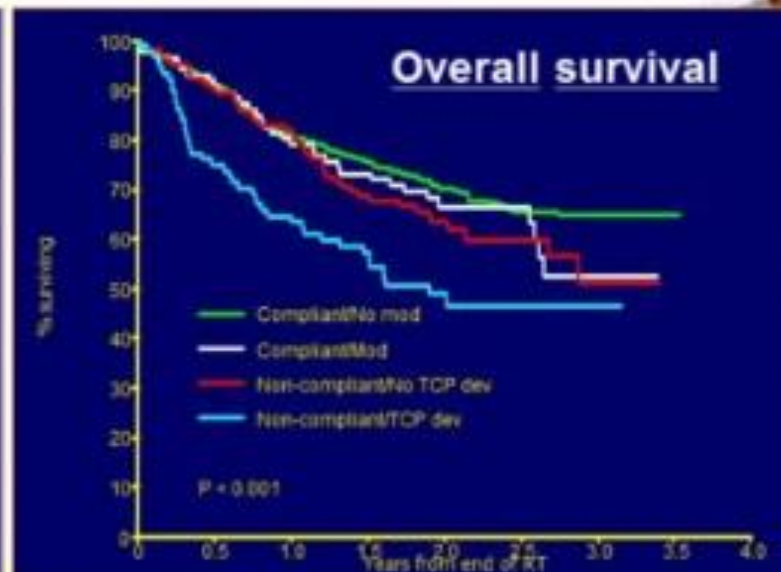
- >800 patients across four Continents
- Influence by accrual numbers

Critical Impact of Radiotherapy Protocol Compliance and Quality in the Treatment of Advanced Head and Neck Cancer: Results From TROG 02.02

Lester J. Peters, Brian O'Sullivan, Jordi Giralt, Thomas J. Fitzgerald, Andy Trotti, Jacques Bernier, Jean Bourhis, Kally Yuen, Richard Fisher, and Danny Rischin

Radiation Quality Matters: Results by deviation status





Patients who had received at least 60 Gy to PTV2

Imaging for treatment verification

1980's – port films	
1990's -	emergence of MV portal imagers
	in-room ultrasound localization
	marker-based localization
	Fluoroscopic tracking
2000's –	flat panel imaging
	KV digital imaging
	CBCT
	MV CBCT
	CT "on rails"
Emerging -	Electromagnetic localization and tracking
	surface tracking
	in-room MRI

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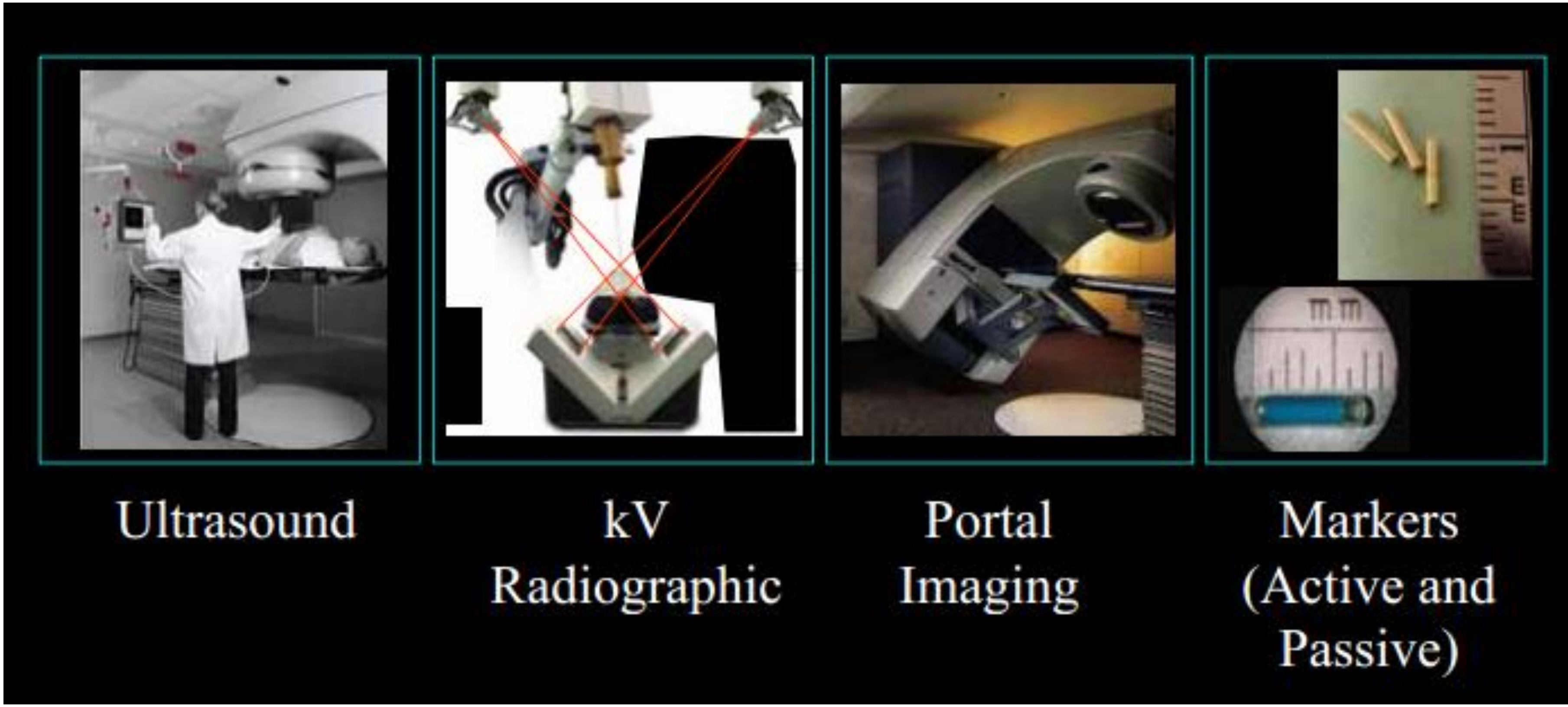
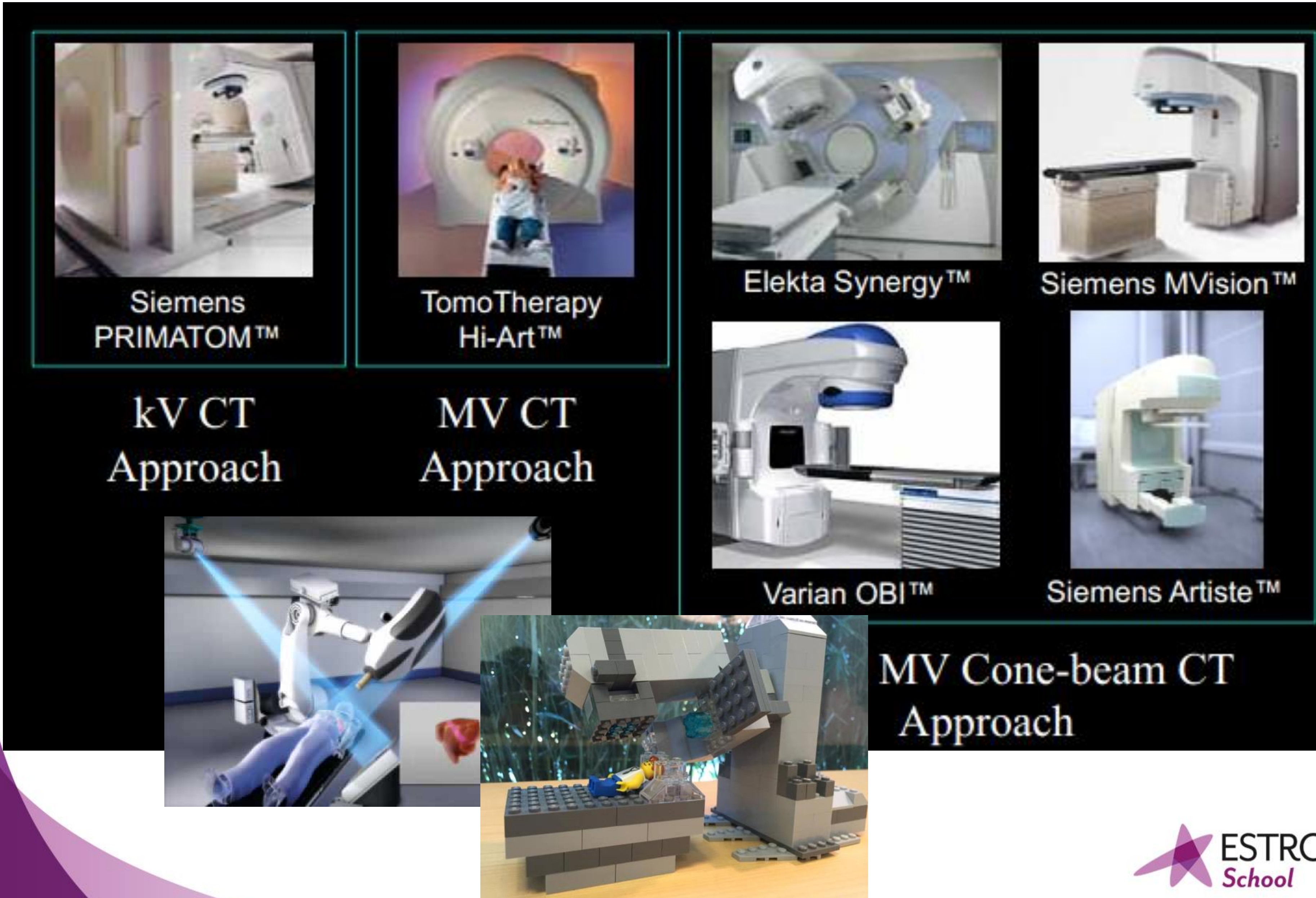
Technologies available for IGRT



Technologies available for IGRT



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Adoption of new RT Technology

- Vendor and developer motivation
- Healthcare provider´s incentive
- Patient and their family´s perception
- Public health provider and Policy maker´s concern
- Adoption of these techniques is often hasty

Mainly focus on **technological capacity** rather than **evidence-based** sptepwise approach

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Rising Cost of Radiotherapy

Radiotherapy and Oncology

The cost of radiotherapy in a decade of technology evolution

Evelyn Van de Werf, Jan Verstraete, Yolande Lievens

Table 2
Comparison of the costs at the activity-group level for respectively 2000 and 2009.

	2000 (€)	%	2009 (€)	%
Treatment preparation	839,247	31	1,480,112	27
First patient contact	137,066	5	197,612	4
Simulation	423,162	16	667,324	12
Delineation	25,540	1	114,611	2
Dose calculation	253,479	9	500,565	9
Treatment delivery	1,872,695	69	4,059,947	73
Quality assurance (QA)	283,192	10	1,252,789	23
General at start	40,561	1	102,459	2
Patient specific		0	48,678	1
Supervision plan	69,606	3	68,519	1
Portal imaging	60,324	2	791,248	14
In vivo dosimetry	32,423	1	76,064	1
Chart round	80,278	3	165,821	3
Daily radiotherapy delivery	1,508,306	56	2,501,649	45
Clinical follow up	44,820	2	116,816	2
Discharge	36,377	1	188,693	3
Total	2,711,942	100	5,540,059	100

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Rationale for IGRT

Adoption of new IGRT techniques should be based on clinical rationale/evidence and clinical needs:

- **What is the clinical evidence for the claims**
  - ➢ It is better/lower cost than current standard
  - ➢ It can tackle a currently unsolvable clinical problem
  - ➢ It is any purported benefit
- **What is the clinical indication**
- **What are the limitations/risks**
- **Do we have resources and demand**

- **CLAIM IS NOT EVIDENCE!!**

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Challenges in RT delivery:

- Day-to-day setup variation
- Intra-fractional organ motion
- Inter-fractional tumor and normal tissue deformation

IGRT Claims: (compared to conventional 3D Conformal)

- IGRT improves the precision and accuracy of RT delivery
  - Minimizes day-to-day setup variation with daily image-guidance using appropriate matching surrogate
  - Tracks intra-fractional organ motion
  - Tracks inter-fractional tissue deformation (adaptive)

- ***Does it translate into better clinical outcomes?***

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IGRT

Radiotherapy and Oncology 78 (2006) 119-122
www.thegreenjournal.com

Special commentary

From IMRT to IGRT: Frontierland or Neverland?

C. Clifton Ling[a,*], Ellen Yorke[a], Zvi Fuks[b]

[a]*Department of Medical Physics, and* [b]*Department of Radiation Oncology, Memorial Sloan Kettering Cancer Center, New York, NY, USA*

Abstract

The recent enthusiasm for real-time image guidance in radiotherapy (IGRT) is in part due to the commercial availability of advanced on-line imaging technologies. Perhaps more important than its potential to improve conventional radiotherapy, IGRT may lead to a paradigm shift in facilitating hypo-fractionated or single-dose treatment. However, there are uncertainty regarding features and approaches of competing IGRT systems and as to whether a sub-set of the features of an ideal IGRT system would suffice for specific disease sites and clinical applications. Clinical studies are necessary for the quantification of benefit needed for evidence-based medicine (Bentzen, SM. Radiation therapy: intensity modulated, image guided, biologically optimized and evidence based. Radiat Oncol 2005;77:227-230).

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IGRT

Acta Oncologica, 2008; 47: 1186–1187

informa
healthcare

EDITORIAL

Will IGRT live up to its promise?

MARCEL VAN HERK

The Netherlands Cancer Institute/Antoni van Leeuwenhoek Hospital, Amsterdam, the Netherlands

Evidence levels

Levels		Type of Evidence
I	1A	Systemic review (with homogeneity) of RCTs
	1B	Individual RCT (with narrow confidence intervals)
	1C	All or none study
II	2A	Systematic review (with homogeneity) of cohort studies
	2B	Individual cohort study (including low quality RCT, e.g. <80% follow-up)
	2C	"Outcomes" research: Ecological studies
III	3A	Systematic review (with homogeneity) of case-control study
	3B	Individual Case-control study
IV	4	Case series (and poor quality cohort and case-control study)
V	5	Expert opinion without explicit critical appraisal or based on physiology bench research or "first principles"

Guyatt et al. JAMA 2000

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Improved Clinical Outcomes With High-Dose Image Guided Radiotherapy Compared With Non-IGRT for the Treatment of Clinically Localized Prostate Cancer

Michael J. Zelefsky, M.D.,* Marisa Kollmeier, M.D.,* Brett Cox, M.D.,* Anthony Fidaleo, B.A.,* Dahlia Sperling, B.A.,* Xin Pei, Ph.D.,* Brett Carver, M.D., Ph.D.,† Jonathan Coleman, M.D.,† Michael Lovelock, Ph.D.,† and Margie Hunt, B.S.†

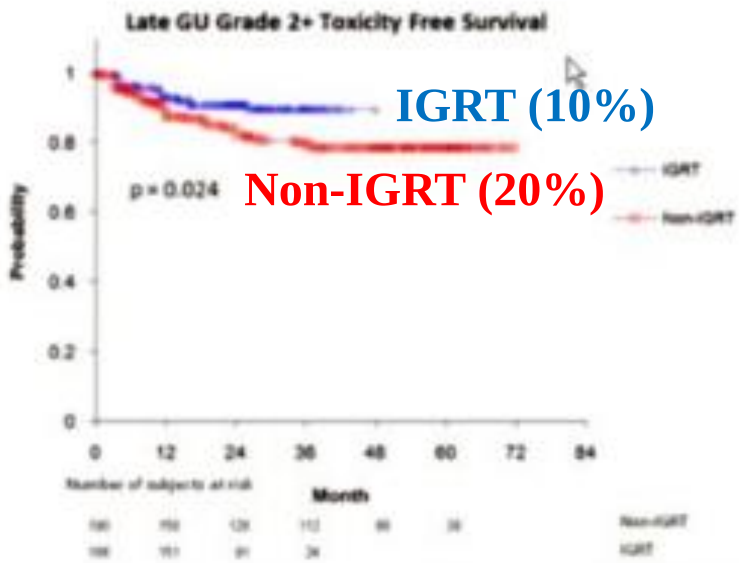

Fig. 1. Comparison of actuarial likelihood of grade 2 or higher late urinary toxicity for patients treated with image-guided radiotherapy (IGRT) to 86.4 Gy vs. intensity-modulated radiotherapy.

IGRT (daily imaging with fiducial marker) vs. non-IGRT (weekly imaging without marker):

- ✓ Same Rx dose: 86.4 Gy
- ✓ Same PTV margin
- ✓ Similar delivery technique: IMRT

IGRT vs non-IGRT

- Lower G2+ GU toxicity (3-y: 10 vs 20%)
- Higher biochemical tumor control in high-risk cohort
- Limitation:
  - ✓ Retrospective review
  - ✓ Slightly different study period
    - Non-IGRT: 2006-2008
    - IGRT: 2007-2009
  - ✓ Short follow-up: median 2.8 years, esp. IGRT cohort

IGRT reduced daily setup variation ⇒ better clinical outcomes **(level 3B evidence)**

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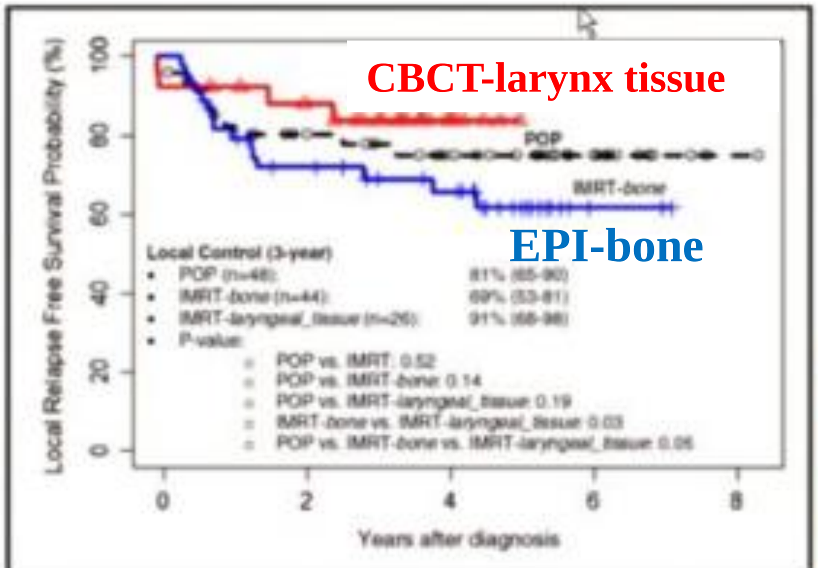
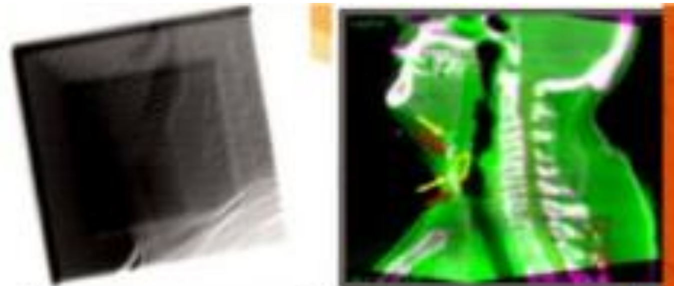
CBCT (vs. MV-EPID): better soft tissue visualization

Outcome following IMRT for T2 glottic cancer: the potential impact of image-guidance protocols on local control

Albert Tiong · Shao Hui Huang · Brian O'Sullivan · Indrajit Mallick · John Kim · Laura A. Dawson · John Cho · Jolie Ringash · Andrew Bayley · Andrew Hope · Eugene Yu · Stephen Breen · Andrea McNiven · Ralph Gilbert · Wei Xu · John Waldron





IMRT (CBCT to laryngeal tissue) vs IMRT (MV-EPID to bone)

- Higher LC (97 vs 69% at 3-yr)
- Limitations:
  - ✓Retrospective review
  - ✓Different study period
    - Non-IGRT: 2006-2008
    - IGRT: 2008-2010
- Smaller sample size (44 vs 26 patients)

- IMRT with MV-EPID matching to bone could result in geographic miss
- IGRT with CBCT allows selecting appropriate matching surrogate (laryngeal soft tissue) ⇒ improved setup accuracy ⇒ improved clinical outcomes

Level 4 evidence

Sources for Clinical Rationale

- Premarketing research work:
  - Randomized trial is ideal but often lacking
    - Difficult to conduct (small "*window of opportunity*")
- Published literature
  - Various quality: high level of evidence is scant
  - Be aware of publication bias, reporting bias, reviewers' bias, omission bias
- Official and unofficial communication
  - Conference, courses, symposium, expert narration
    - Subject to bias, especially vendor sponsored symposium
- Own institutional experience following implementation
  - Cumulative, prospective, and reflective
    - Requires close monitoring and timely feedback

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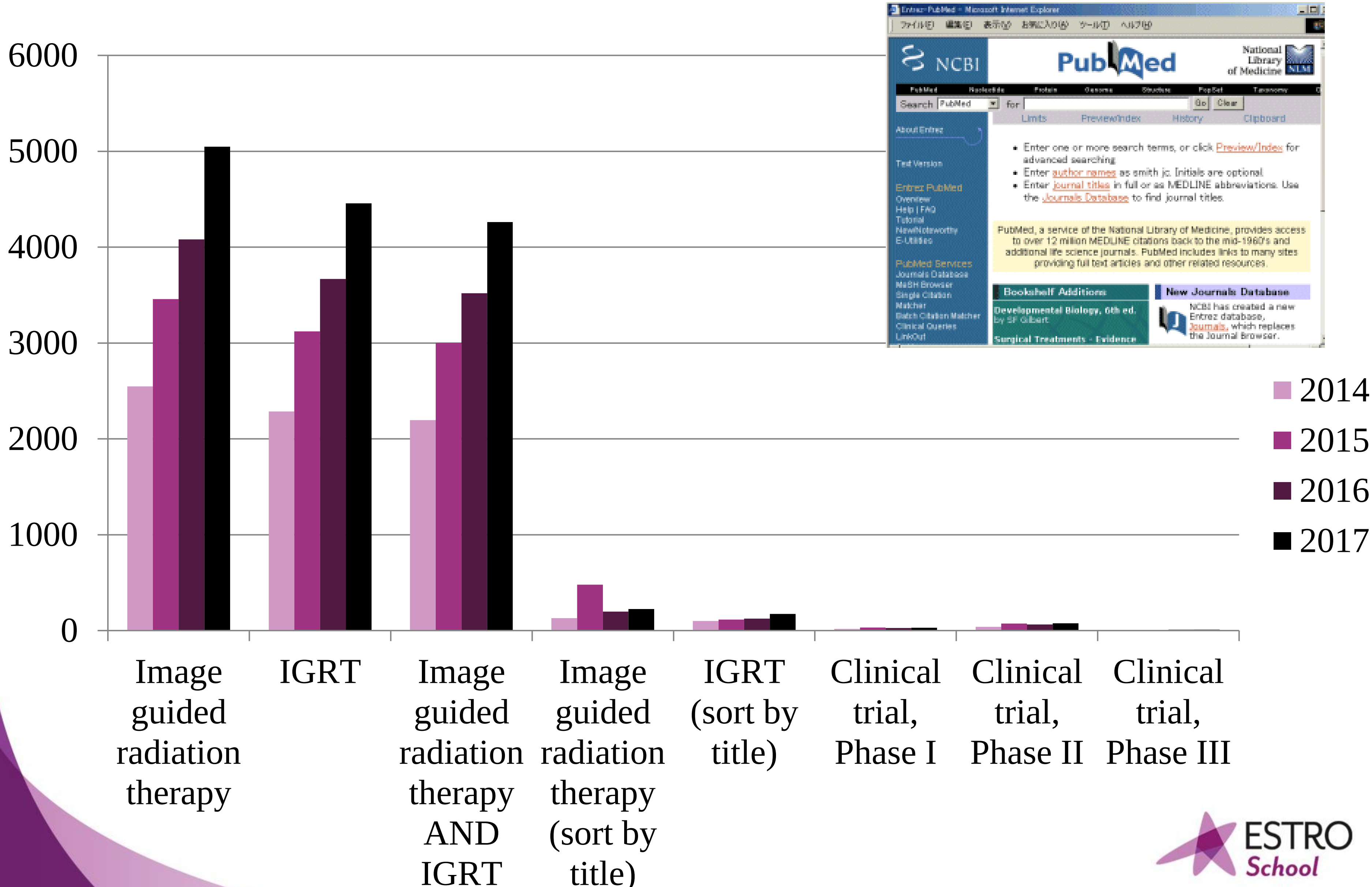
Cites in Pubmed (2014-2017)



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Clinical trial, Phase III
(compare new treatments with the standard)

- **Standard-dose (60Gy) vs high-dose RT (74Gy) for NSCLC patients (RTOG 0617): negative results**

➢ RT planning was more likely to be noncompliant in the high-dose group (26% vs 17%, *P* = .02)

➢ They used both 3D and IMRT

➢ No details about IGRT

- **RTOG 0631 phase 2/3 study of image guided stereotactic radiosurgery for localized (1-3) <u>spine</u> metastases: <u>phase 2 results</u>.**

- **A randomized hypofractionation <u>dose escalation</u> trial for high risk <u>prostate</u> cancer patients: interim analysis of acute toxicity and quality of life in 124 patients.**

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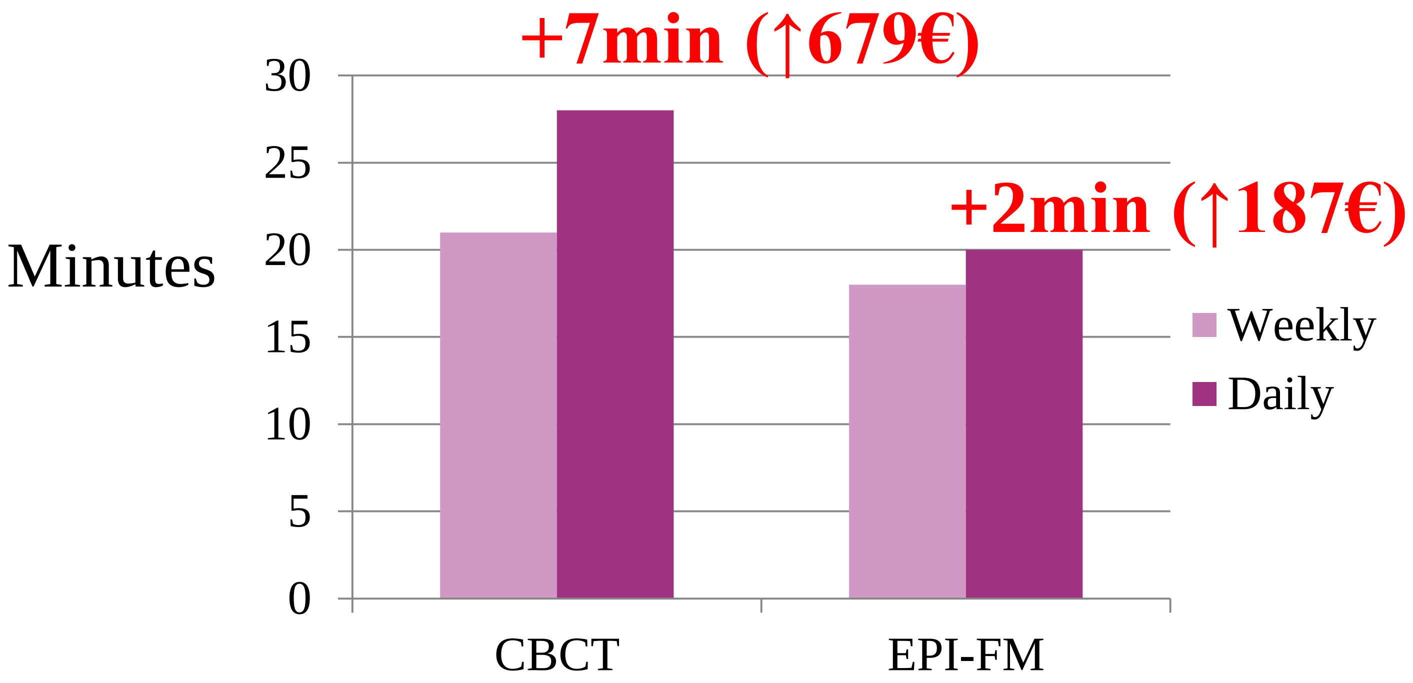
Clinical trial, Phase III

- **Cost** of prostate IGRT: results of a randomized trial.
- Prognostic **impact of abdominal adiposity** in prostate patients.
- **Recommendations** for implementing **SBRT** in peripheral stage IA NSCLC: phase III ROSEL study.
- **Dosimetric experience** with accelerated partial breast irradiation using image-guided interstitial brachytherapy.

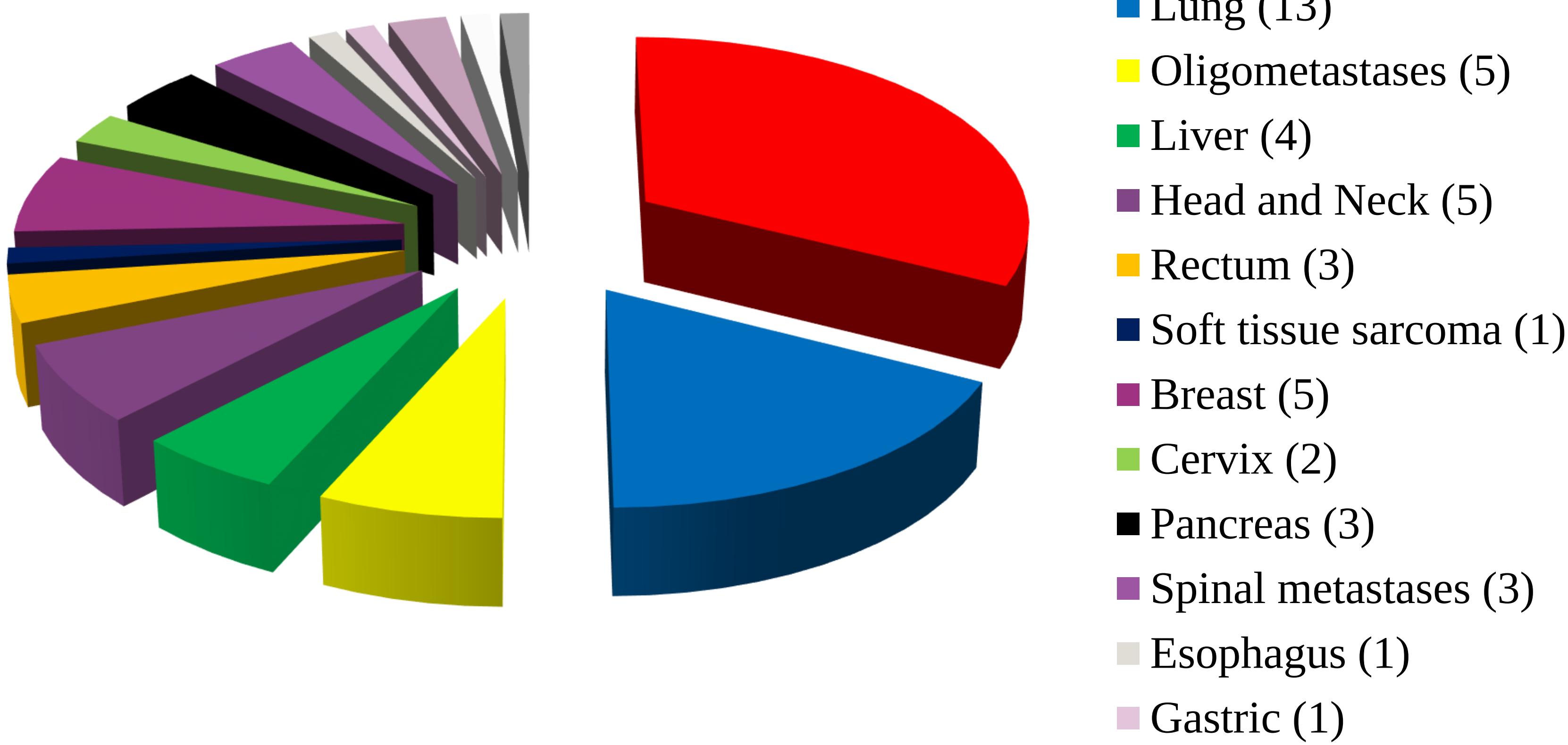
COST and TIME

- N=208 patients (France)



- The incremental costs due to different IGRT strategies are relatively **moderate**.

Clinical trial, Phase II (N = 74)
(if a new treatment works well)



Toxicity

Grade 0	None
Grade 1	Mild
Grade 2	Moderete
Grade 3	Severe
Grade 4	Intensive care
Grade 5	Fatal

Phase II (Prostate)

Table 1 Patient and treatment characteristics

Variable	3D-CRT (n=215)	IG-IMRT (n=260)
Mean (±SD), y	68.9 (±6.3%)	70.5 (±6.0%)
T category		
1	36 (16.7%)	40 (15.4%)
2	97 (45.1%)	89 (34.2%)
3a	53 (24.7%)	102 (39.2%)
3b	29 (13.5%)	28 (10.8%)
4	0	1 (0.4%)
Gleason score		
2-6	106 (49.3%)	75 (28.8%)
7	81 (37.7%)	119 (45.8%)
8-10	28 (13.0%)	66 (25.4%)
Median prehormone PSA concentration, Indeed "Median initial PSA concentration" μg/L (range)	11.3 (0.4-57.0)	15.0 (1.8-59.6)

SIMILAR GROUPS

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Int J Radiation Oncol Biol Phys, Vol. 91, No. 4, pp. 737–744, 2015

Treatment

	3D	IG-IMRT
Risk category		
Low	34 (15.8%)	0
Intermediate	72 (33.5%)	75 (28.8%)
High	109 (50.7%)	185 (71.2%)
Seminal vesicle dose (Gy)		
0	43 (20.0%)	50 (19.2%)
50	35 (16.3%)	0
68	101 (47.0%)	0
70	0	125 (48.1%)
78	36 (16.7%)	85 (32.7%)
Planning margins (mm)		
5	0	107 (41.3%)
6-8	0	151 (58.3%)
10	215 (100%)	1 (0.4%)
Hormone therapy	42 (19.5%)	174 (66.9%)
TURP	24 (11.2%)	28 (10.8%)
Diabetes mellitus	12 (5.6%)	29 (11.2%)
Abdominal surgery	57 (26.5%)	65 (25.0%)
Smoking	34 (15.8%)	28 (15.0%)

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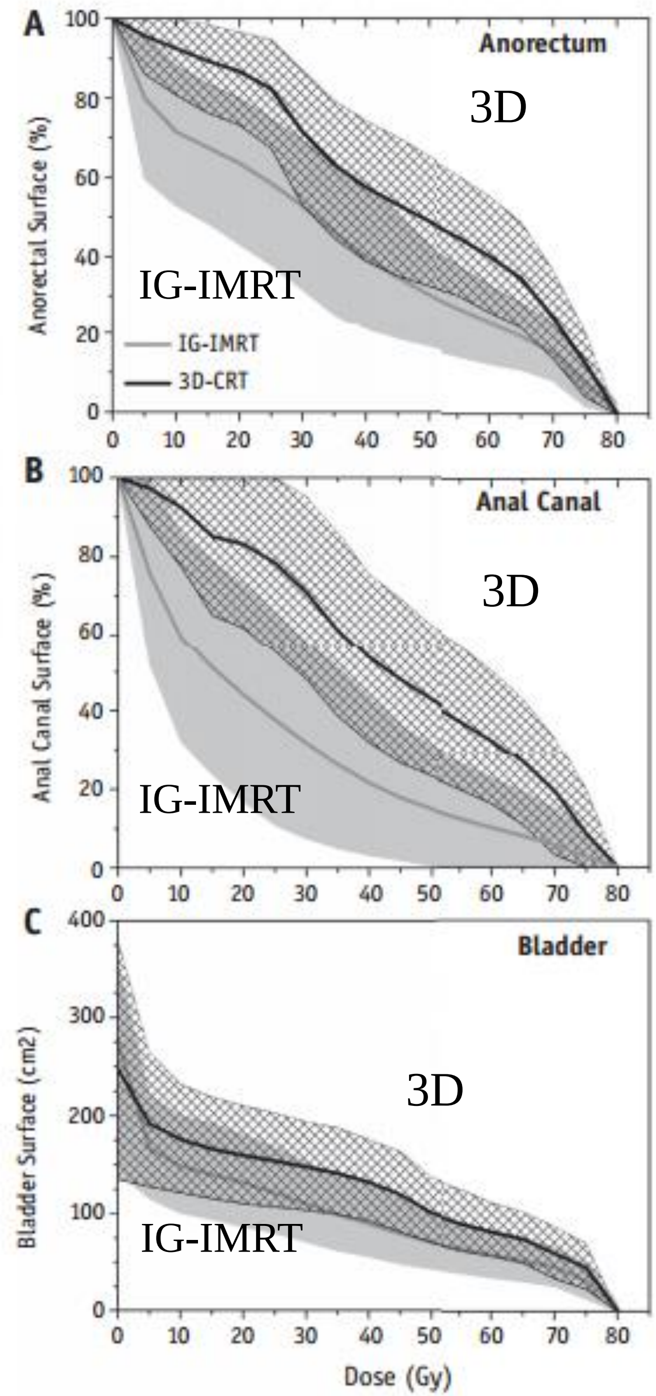
Int J Radiation Oncol Biol Phys, Vol. 91, No. 4, pp. 737–744, 2015



Mean dose and 10th to 90th percentiles are shown

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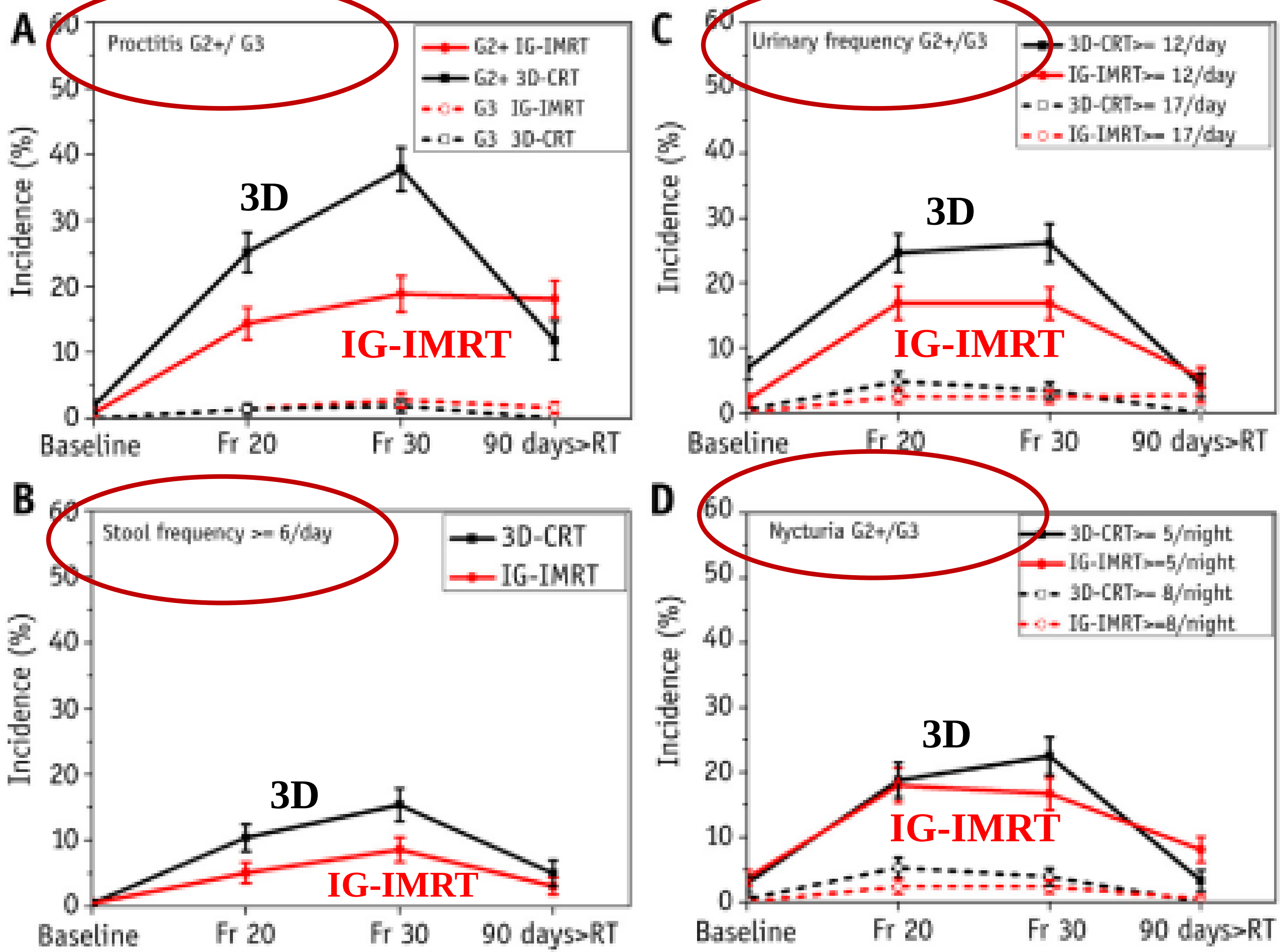
Int J Radiation Oncol Biol Phys, Vol. 91, No. 4, pp. 737–744, 2015

TOXICITY



Int J Radiation Oncol Biol Phys, Vol. 91, No. 4, pp. 737–744, 2015

Prostate IGRT

ARTICLE IN PRESS

Radiotherapy and Oncology xxx (2014) xxx–xxx

ELSEVIER

Contents lists available at ScienceDirect

Radiotherapy and Oncology

journal homepage: www.thegreenjournal.com

Original article

Is "pelvic radiation disease" always the cause of bowel symptoms following prostate cancer intensity-modulated radiotherapy?

Myo Min [a,*], Benjamin Chua [a], Yvonne Guttner [d], Ned Abraham [d], Noel J. Aherne [a], Matthew Hoffmann [b], Michael J. McKay [c,*,1], Thomas P. Shakespeare [a,1]

[a] North Coast Cancer Institute, Coffs Harbour; [b] North Coast Cancer Institute, Port Macquarie; [c] North Coast Cancer Institute, Lismore; [d] Coffs Harbour Hospital, Australia

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Prostate IGRT

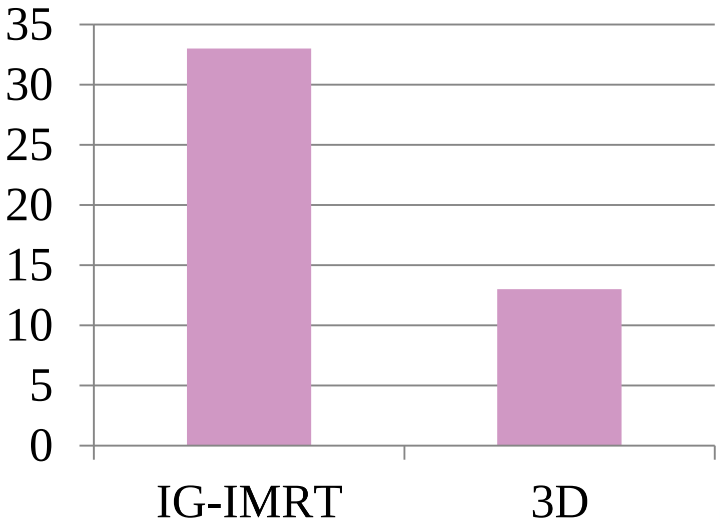
- Multicenter study
- N=102
- Prostate cancer
- Bowel symptoms persisting >90 days post-RT
- IMRT-IGRT
- Dose: 74-78 Gy at 1,8-2 Gy/fx
- Bowel symptoms + **ENDOSCOPIC EXAMINATION**
- Endoscopy findings:
  - 56% Polyps
  - 49% Diverticular disease
  - 38% Haemorrhoids
  - 29% radiation proctopathy with associated pathology
  - **4% radiation proctopathy alone**

M Min et al. Radiother Oncol 110 (2), 278-283. 2014

Clinical trial, Phase II (hepatocellular carcinoma)

- IG-IMRT (N=65) vs 3D (N=122)
- Stage III-IV
- Period: 2006-2011
- Retrospective
- Dose: 62 Gy for IG-IMRT and 53 Gy for 3D

- **No differences in toxicity**
- **Survival at 3 years:**



J Cancer Res Clin Oncol. 2014 Sep;140(9):1595-605

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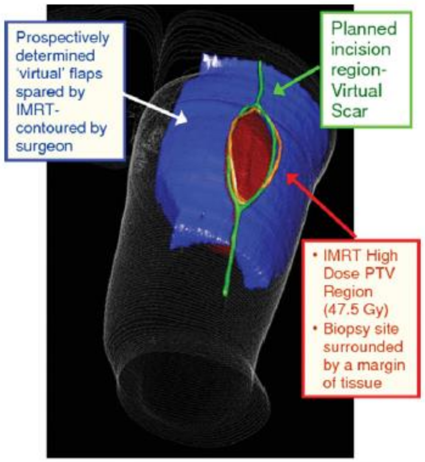
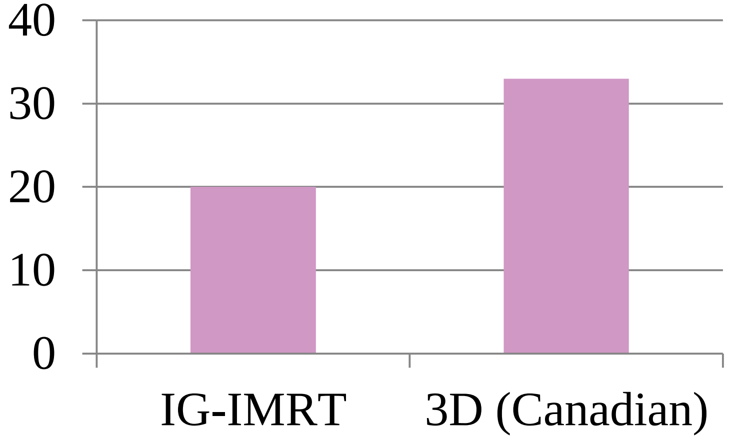
Clinical trial, Phase II (Sarcoma)

- Single Institution study
- Lower extremity soft tissue sarcoma
- N=56
- Period: 2005-2009
- IG-IMRT
- Dose: 50 Gy at 2 Gy/fx



Multi-disciplinary STS phase II study protocol investigating high precision pre-operative IMRT to spare tissues from surgery and RT morbidity

- **Acute wound complication:**
- Local control 88%
- OS: 74%



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O'Sullivan B, et al. Cancer. 2013 May 15;119(10):1878-84.

Clinical trial, Phase II (Lung)

- Multicenter study
- Prospective
- Inoperable T1/T2 NSCLC
- N=60
- Period: 2003-2005
- SBRT
- Dose: 45 Gy at 15 Gy/fx

- **Grade 3 toxicity: 21%**
- Local control 96%
- OS: 65%

Table 3
Lung-related toxicity maximum grade per patient number of affected patients

Toxicity	CVD (17 patients)		COPD (40 patients)	
	Gr 1–2	Gr 3	Gr 1–2	Gr 3
Cough	4	–	11	1
Dyspnoea	2	2	8	2
Pneumonia	–	–	1	1
Pneumonitis	3	–	7	–
Fibrosis	8	1	12	1
Atelectasis	3	1	3	–
Pleural effusion	6	2	5	–
Heart disorder	1	–	–	1
Esophagitis	1	–	1	–

Toxicity grading was done according to CTC v2. Radiation-related pulmonary fibrosis >90 days post-treatment was graded according to RTOG/EORTC Late Radiation Morbidity Scoring Scheme.
Maximum grade refers to the highest degree of toxicity recorded during follow-up. CVD, cardiovascular disease; COPD, chronic obstructive pulmonary disease.

Baumann et al. Radiotherapy and Oncology 88 (2008) 359–367

Clinical trial, Phase II (oligometastases)

- Single Institution study
- Oligometastases
- N=25
- Period: 2004-2006
- SBRT
- Dose: 50 Gy at 5 Gy/fx + sunitinib

- **Grade 3 toxicity: 28%**
- Local control 75%
- OS: 71%; PFS: 56%

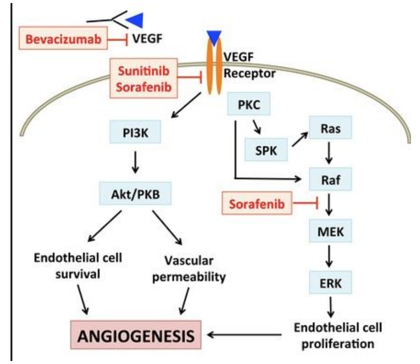

Table 2. Adverse Events.

Adverse Event	All grades	Grade 3	Grade 4	Grade 5
Anemia	18	2	0	0
Neutropenia	14	2	0	0
Fatigue	18	0	0	0
LFT abnormalities	15	1	0	0
Thrombocytopenia	15	4	0	0
Mucositis/stomatitis	8	0	0	0
Nausea/vomiting	7	0	0	0
Skin changes	4	0	0	0
Diarrhea	5	0	0	0
Hypertension	3	0	0	0
Bleeding	4	1	0	1*
Metabolic abnormalities	2	1 (PO_4)	0	0
Increased creatinine	5	0	0	0

*One case occurred after sunitinib treatment and was likely related to reirradiation performed prior to protocol therapy.

doi:10.1371/journal.pone.0036979.t002

Tong CC, et al. PLoS One. 2012;7(6):e36979.

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Clinical trial, Phase II (head and neck)

- Multicenter study
- Reirradiation
- N=60
- Period: 2007-2010
- SBRT

- Dose: 36 Gy at 6 Gy/fx + cetuximab
- **Grade 3 toxicity: 18%**
- OS: 47,5%

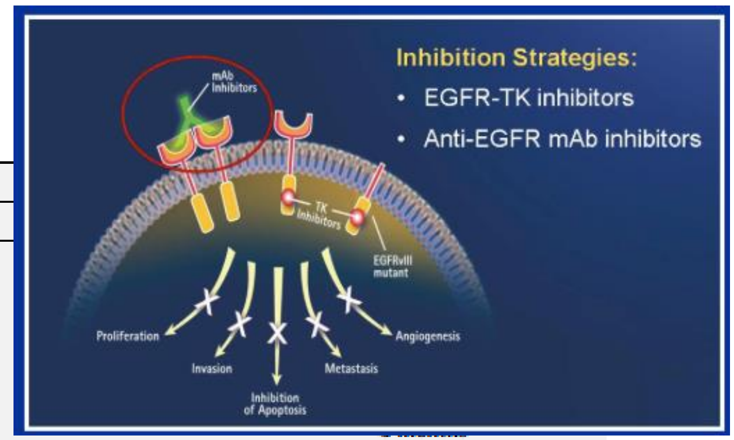

Table 1
Grade 3 toxicities and cutaneous toxicity.

Grade ≥ 3 AE related to study treatment		
(N = 56)	n	
Cutaneous		
Rash	4	
Cutaneous toxicity	1	
Fibrosis	1	
Gastrointestinal		
Mucositis	4	
Dysphagia	3	
Xerostomia	2	3–6 months
Fistula (oral cavity)	1	>6 months
Dysgeusia	1	<3 months
Cutaneous toxicity (N = 56)	Related to cetuximab and/or radiotherapy	Related to cetuximab
Cutaneous toxicity, n (%)	47 (84)	41 (73)
NK	1 (2)	1 (2)
Grade 1	14 (25)	14 (25)
Grade 2	27 (48)	22 (39)
Grade 3	[illegible] (9)	[illegible] (7)

Lartigau et al. Radiotherapy and Oncology 109 (2013) 281–285

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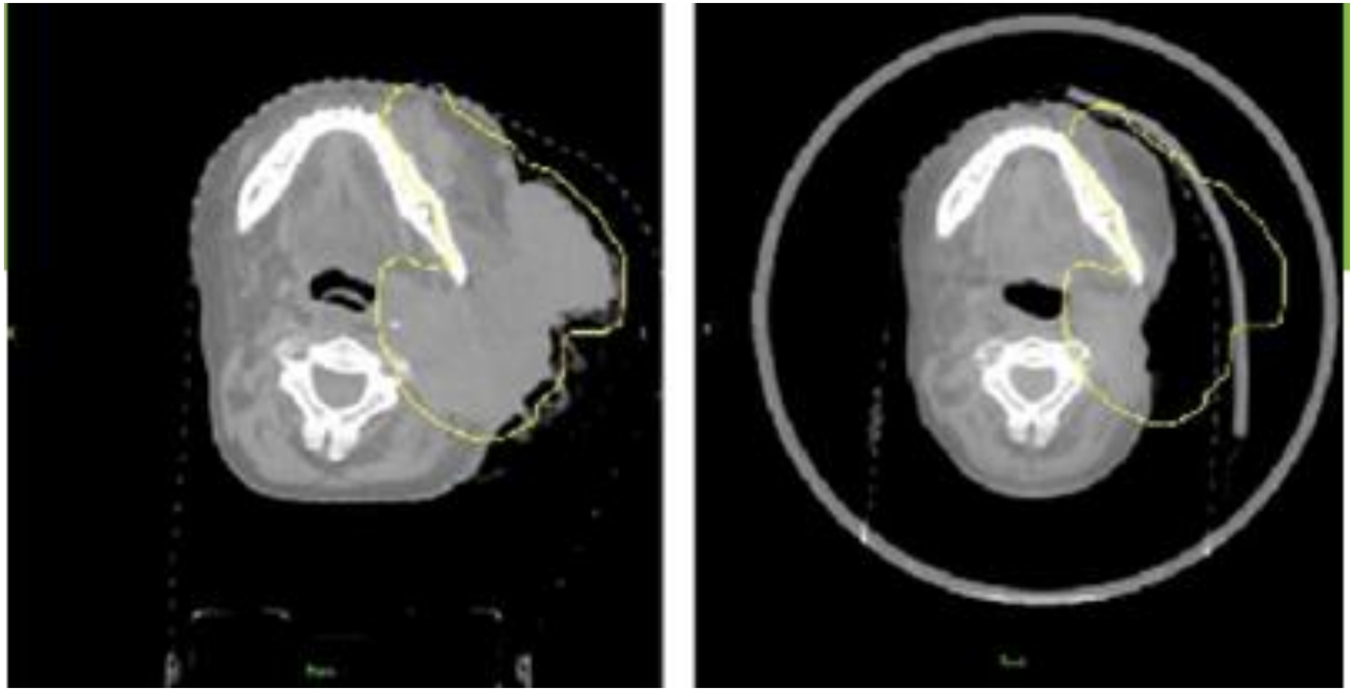


Corresponding axial CT slices from the beginning and the end of treatment.

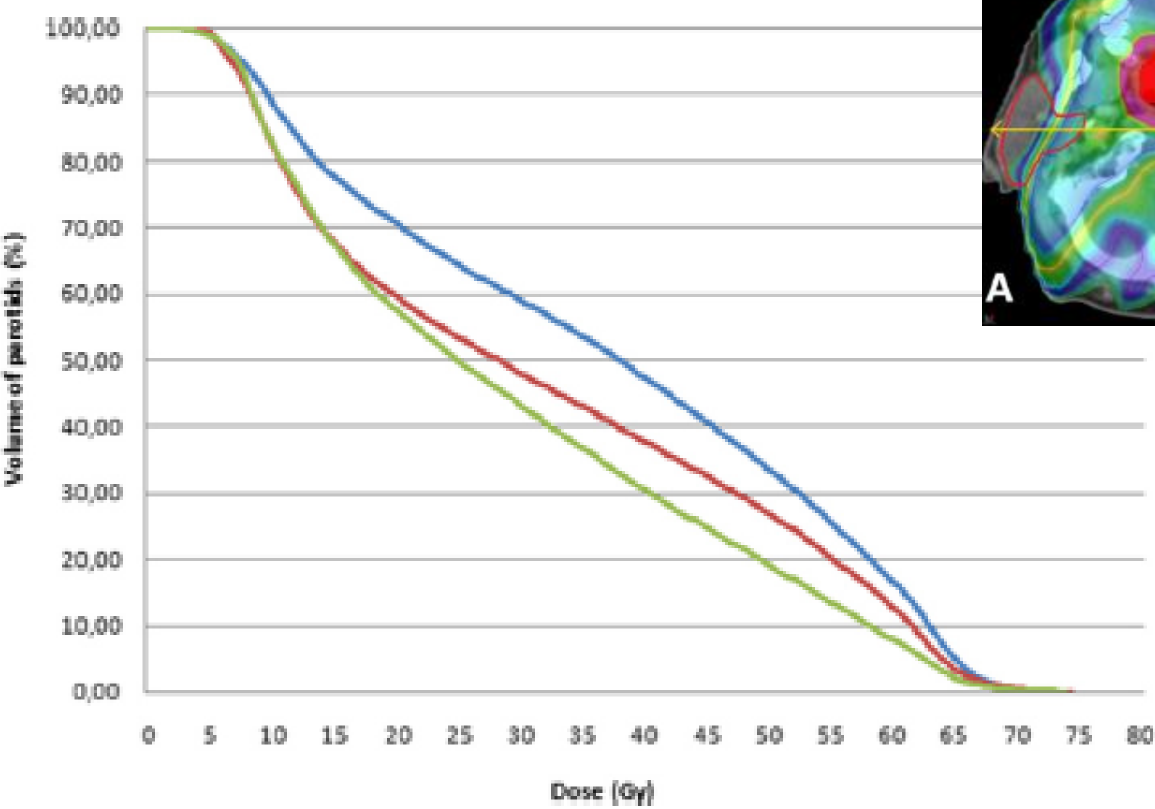
The volume of the PTV changed from 606 to 336 cm3 over treatment, a decrease of 45%.

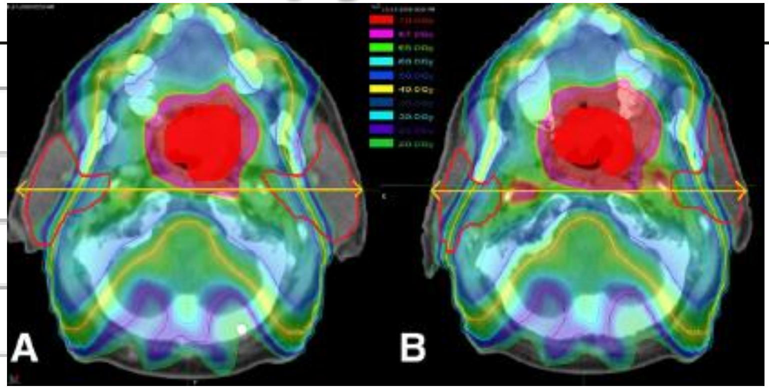
Spinal cord D05 differed from the planned value by:

3.5% (average) +/- 9.8% (standard desviation)

Mechalakos J et al. Med Dosim. 2009 Fall;34(3):250-5.

Adaptive radiotherapy





Head and Neck
N=15
IG-IMRT

•

Replanning decreased the PG mean dose by 5 Gy, and 11% the xerostomia

LEVEL 2B: INDIVIDUAL COHORT STUDY

Castelli et al. Radiation Oncology (2015) 10:6

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FUTURE DIRECTIONS (phase III studies on-going)

- A Randomised, Two Centre Trial on Daily Cone-beam vs Standard Weekly Orthogonal IGRT for **Prostate**
- Hypofractionated IGRT in Patients With Stage II-III Non-Small Cell **Lung Cancer**
- Biological Image Guided Antialgic SBRT of **Bone Metastases**: a Randomized Phase II/III Trial
- Evaluation of 3DCRT Versus IGRT and Analysis of Early Response in **Head and Neck Cancer**.
- Tomotherapy vs Conventional Radiation for Adjuvant Pelvic RT in **Ca Cervix.**
- Can 3D Ultrasound Be Used Reproducibly by RTTs in Partial **Breast** IGRT?

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BEYOND IGRT:

Daily real time planning (RTP)—Treatment of prostate cancer, clinical implementation, and technique

- 60 RTP's were delivered (10 daily RTP/patient) in 6 consecutive patients.
- In 20% of the cases, the CTV-DVH by RTP improved by >10%.

Plans	V40 (%)	V50 (%)	V60 (%)	V70 (%)
RTP	47.1	29.9	18.6	7.8
IGRT	63.8	49.3	38.0	26.5

↓ 20%

Journal of Clinical Oncology 2013;31:191.

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FUTURE DIRECTIONS

Radiotherapy and Oncology 109 (2013) 165–169

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Radiotherapy and Oncology

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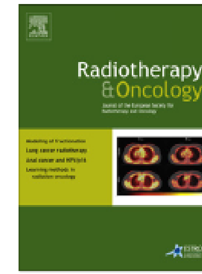

Learning methods in radiation oncology

The utility of e-Learning to support training for a multicentre bladder online adaptive radiotherapy trial (TROG 10.01-BOLART)

Farshad Foroudi [a,*], Daniel Pham [a], Mathias Bressel [b], David Tongs [a], Aldo Rolfo [a,1], Colin Styles [a], Suki Gill [a], Tomas Kron [a]

[a] *Division of Radiation Oncology and Cancer Imaging, Peter MacCallum Cancer Centre, Melbourne, Australia;* [b] *Centre for Biostatistics and Clinical Trials, Peter MacCallum Cancer Centre, Melbourne, Australia*

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IGRT confidence and knowledge

- To demonstrate the utility of an e-Learning programme for providing training regarding a multi-centre **IGRT** trial.
- Participants : **185 RTTs** from 12 centres.
- There was **an increase confidence after** modules ($p < 0.001$).
- The pre **scores increased** from 67 ± 11 ⇨ 79 ± 8 ($p < 0.001$)

IGRT confidence and knowledge

Confidence questions	Pre e-Learning		Post e-Learning		p-Value
	n	Percentage	n	Percentage	
Identifying bladder on CT					<0.001
Not confident	0	0.0	0	0.0	
A little confident	20	10.8	4	2.2	
Somewhat confident	60	32.4	31	16.8	
Quite confident	69	37.3	102	55.1	
Very confident	36	19.5	48	25.9	
Identifying soft tissue anatomies on pelvic CBCT					<0.001
Not confident	13	7.0	0	0	
A little confident	49	26.5	7	3.8	
Somewhat confident	80	43.2	71	38.4	
Quite confident	39	21.1	91	49.2	
Very confident	4	2.2	16	8.6	
Implementing the BOLART at your centre					<0.001
Not confident	28	15.1	1	0.5	
A little confident	40	21.6	9	4.9	
Somewhat confident	58	31.4	48	25.9	
Quite confident	45	24.3	86	46.5	
Very confident	14	7.6	41	22.2	

57% → 81%

23% → 56%

32% → 69%

E-LEARNING WAS FEASIBLE AND IMPROVED CONFIDENCE AND KNOWLEDGE

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CONCLUSIONS: Why IGRT?

- Security
- Precision
- Accuracy (dose escalation)
- Homogeneity
- Potentially, less toxicity: **clinical trials needed!!**
- Reliability
- Adapt to changes in antomy
- Shortening RT


Thank you!
Triana Bridge (Sevilla, Spain)

Case report: **Cervix**

Sofia Rivera, Gustave Roussy, Villejuif, France

Case from the Gyn GEC ESTRO Network / FALCON WS
Courtesy of Pr Pötter

Advanced skills in modern radiotherapy
June 2017

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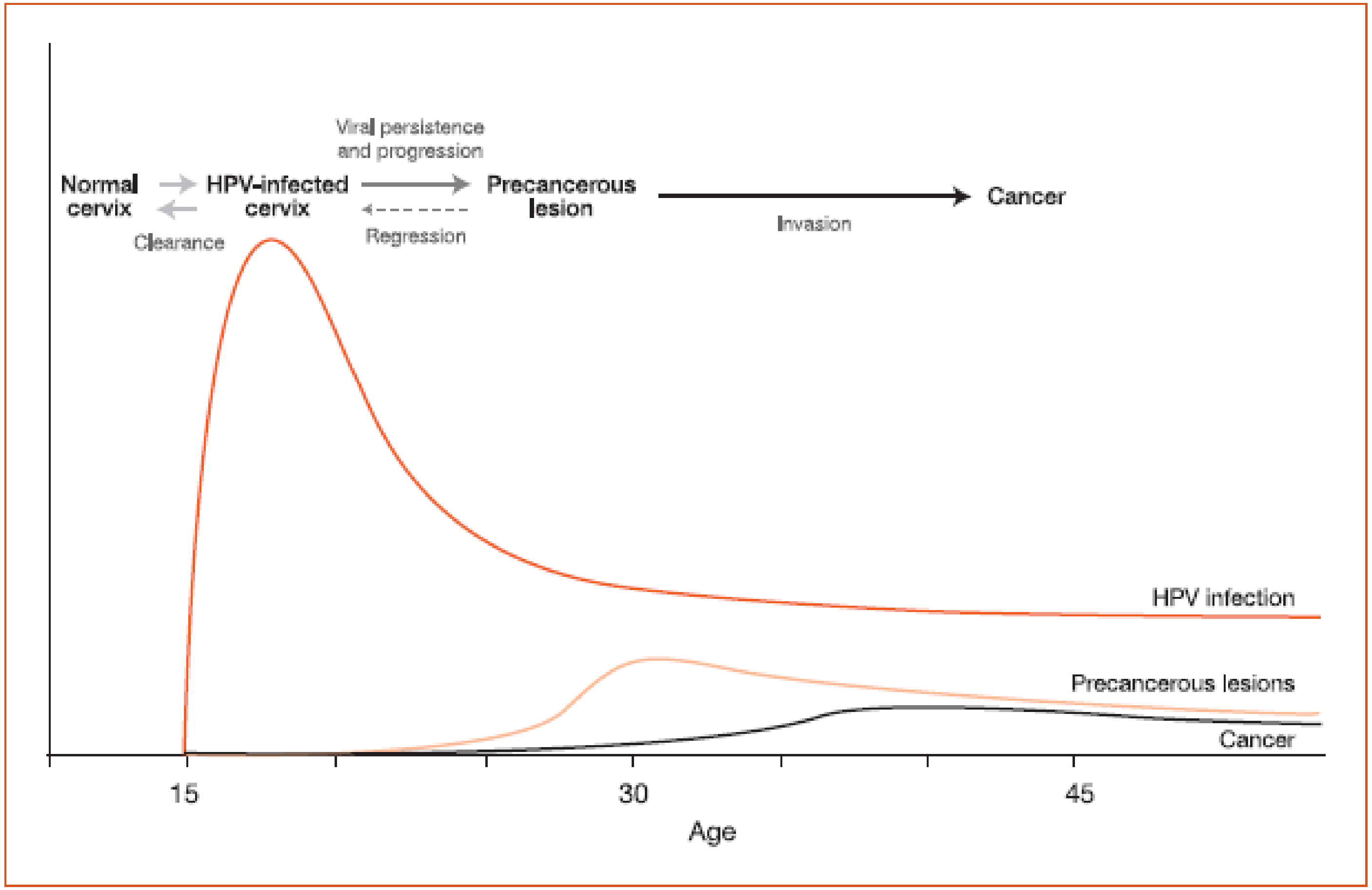
HPV infection natural history

Figure 1. Prevalence of HPV infection, precancerous lesions and cervical cancer by age of women



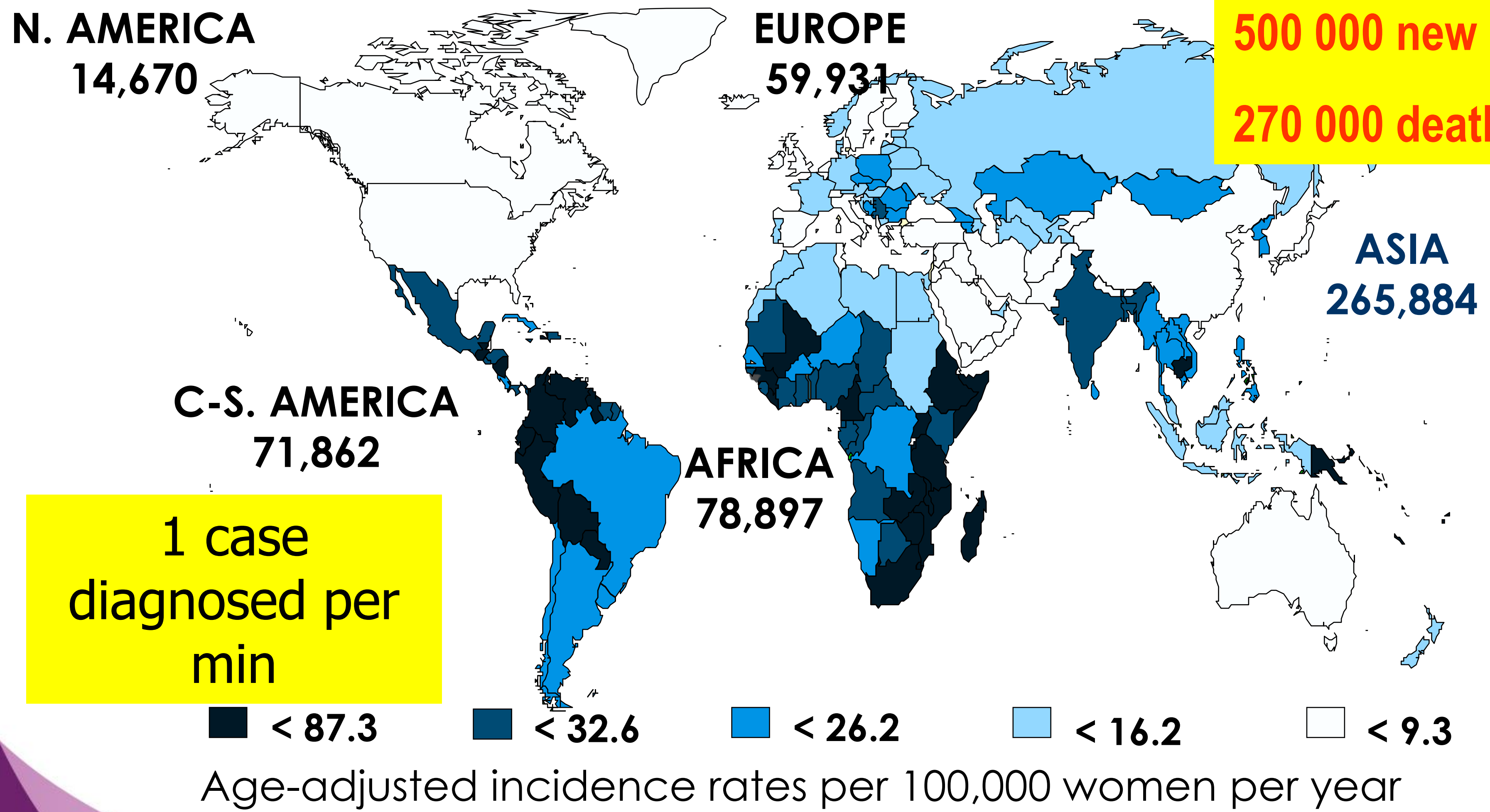
Source: Schiffman M, Castle PE. The promise of global cervical-cancer prevention. *New England Journal of Medicine*, 2005, 353(20): 2101–2103. (© 2005 Massachusetts Medical Society. Adapted with permission.)

Cervix cancer diagnosis OMS (2002)

1,4 Million cases

500 000 new cases/ year

270 000 death / year



1 case diagnosed per min

Whosis Statistical Database, 2012.

Patient History

- 42-year old woman.
- WHO performance status=0
- No clinical symptom
- No palpable node
- Squamous cell carcinoma, grade 3
- TNM: T3b N1 M0

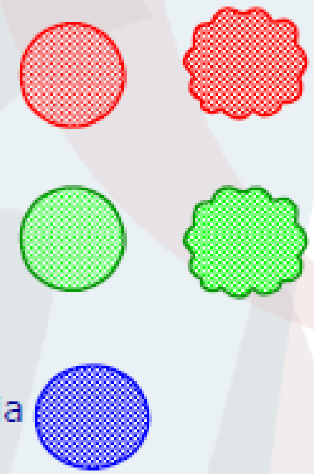
Clinical findings of gyn. examination: at DIAGNOSIS

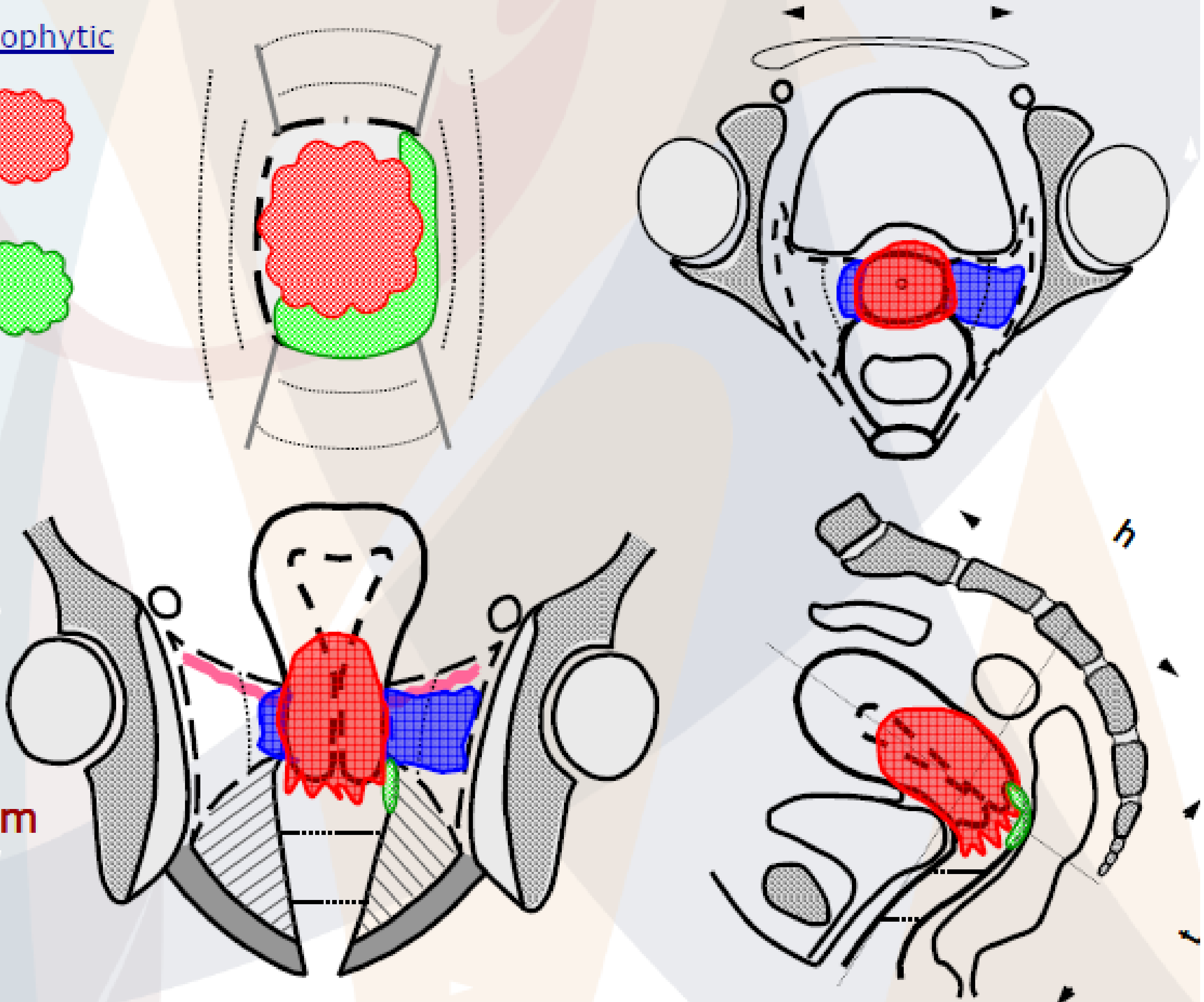
Infiltrative Exophytic

Cervix

Vagina

Parametria





Dimensions:

Width: 90 mm

Thickness: 50 mm

Height: 60 mm

Vaginal inv.: 20 mm

ESTRO
Gyn contouring workshop
Barcelona, May 2012

*Radiological findings integrated on the drawing

Clinical findings of gyn. examination: SUMMARY

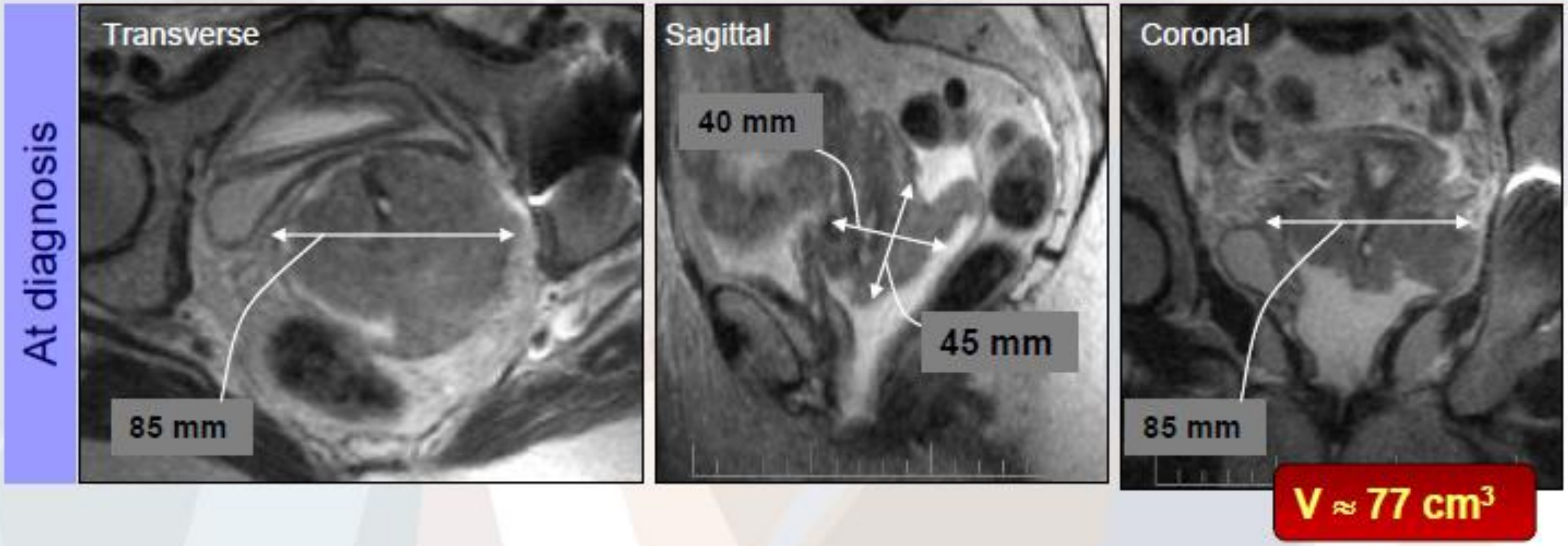
FIGO stage: IIIB

	At diagnosis	At brachytherapy
Width	90 mm	
Thickness	50 mm	
Height*	60 mm	
Left parametrium	Infiltration to pelvic wall	
Right parametrium	Proximal infiltration	
Vagina	20 mm: left & posterior wall	
Bladder**	Not infiltrated	
Rectum**	Not infiltrated	

*Some uncertainty in assessment of height

**Endoscopy at diagnosis

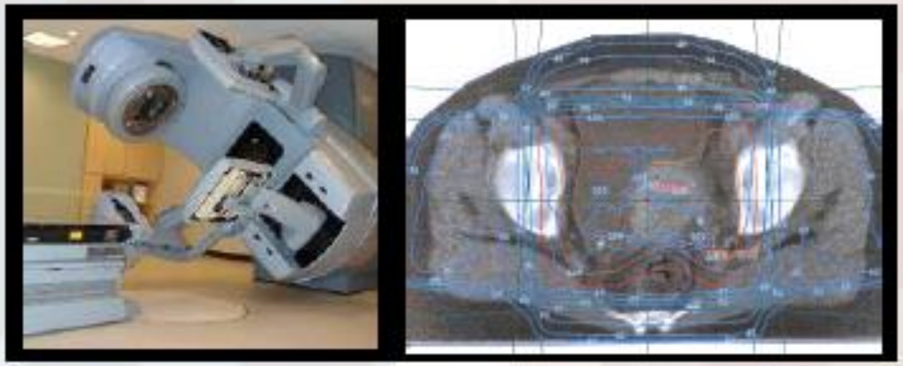
MRI findings

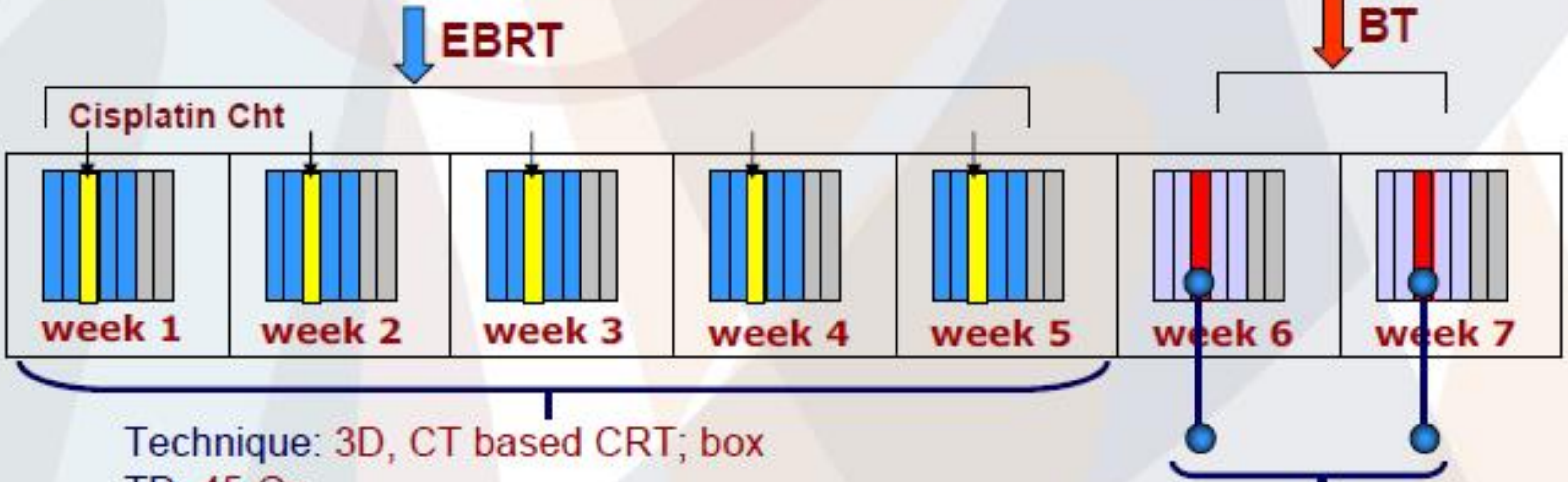


Comment:

Only the representative slices are shown here. Use the information from complete initial MRI data set to fully understand the extent and topography of the tumour.

EBRT, Chemotherapy & timing of BT





Technique: 3D, CT based CRT; box
TD: 45 Gy
Dose per fraction: 1,8 Gy

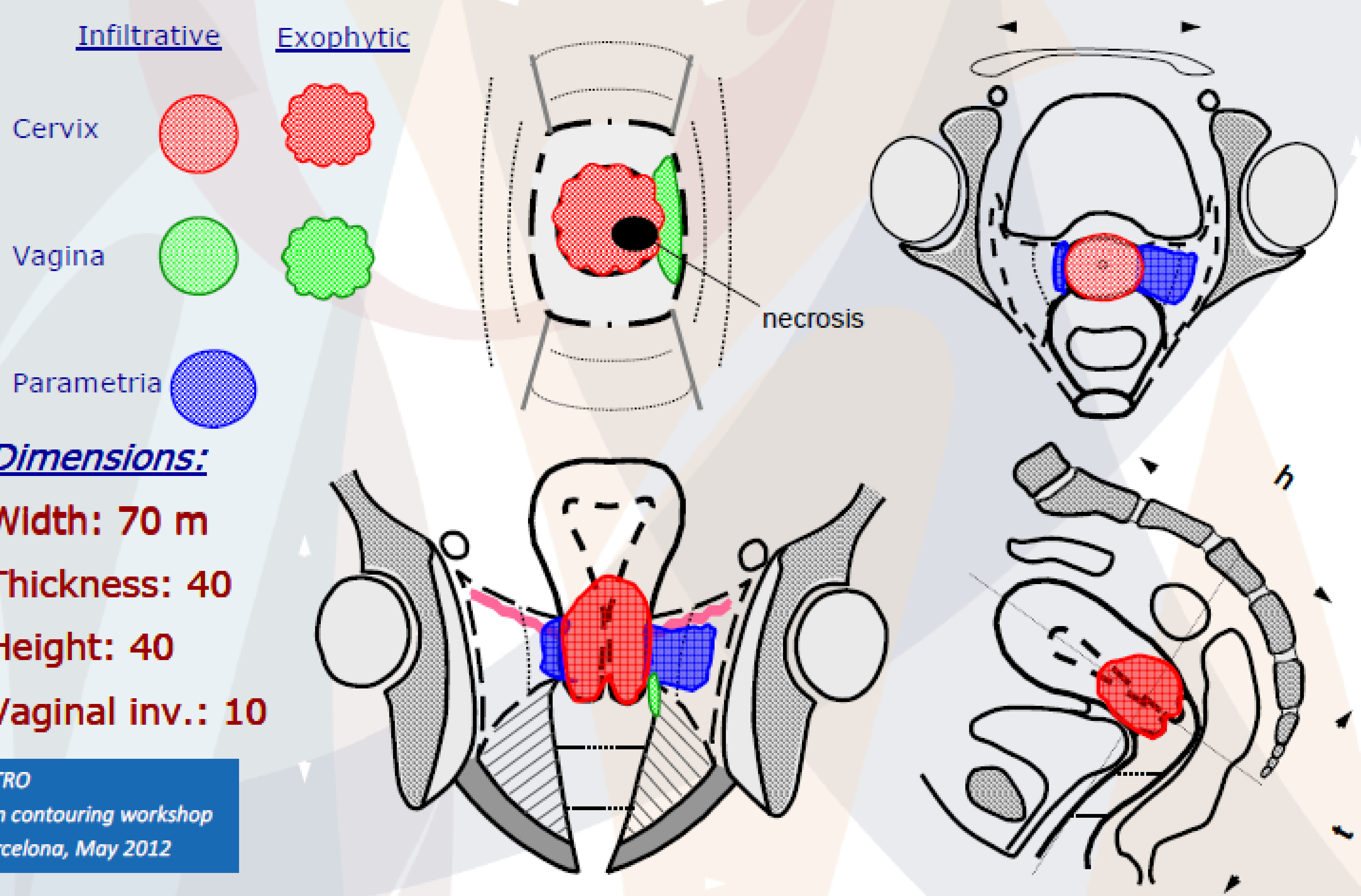
Concomitant chemotherapy:
Cisplatin 40 mg/m2 weekly, 5 cycles

2 x 7 Gy 2 x 7 Gy

Prescribed to HR CTV

High Dose Rate

Clinical findings of gyn. examination: at Brachytherapy



Dimensions:

Width: 70 m

Thickness: 40

Height: 40

Vaginal inv.: 10

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Gyn contouring workshop
Barcelona, May 2012

Clinical findings of gyn. examination: SUMMARY

FIGO stage: IIIB

	At diagnosis	At brachytherapy
Width	90 mm	70 mm
Thickness	50 mm	40 mm
Height*	60 mm	40 mm
Left parametrium	Infiltration to pelvic wall	Distal infiltration (≈ 30 mm)
Right parametrium	Proximal infiltration	Proximal infiltration (≈ 10 mm)
Vagina	20 mm: left & posterior wall	10 mm: left fornix
Bladder**	Not infiltrated	NA
Rectum**	Not infiltrated	NA

*Some uncertainty in assessment of height

**Endoscopy at diagnosis

Brachytherapy application

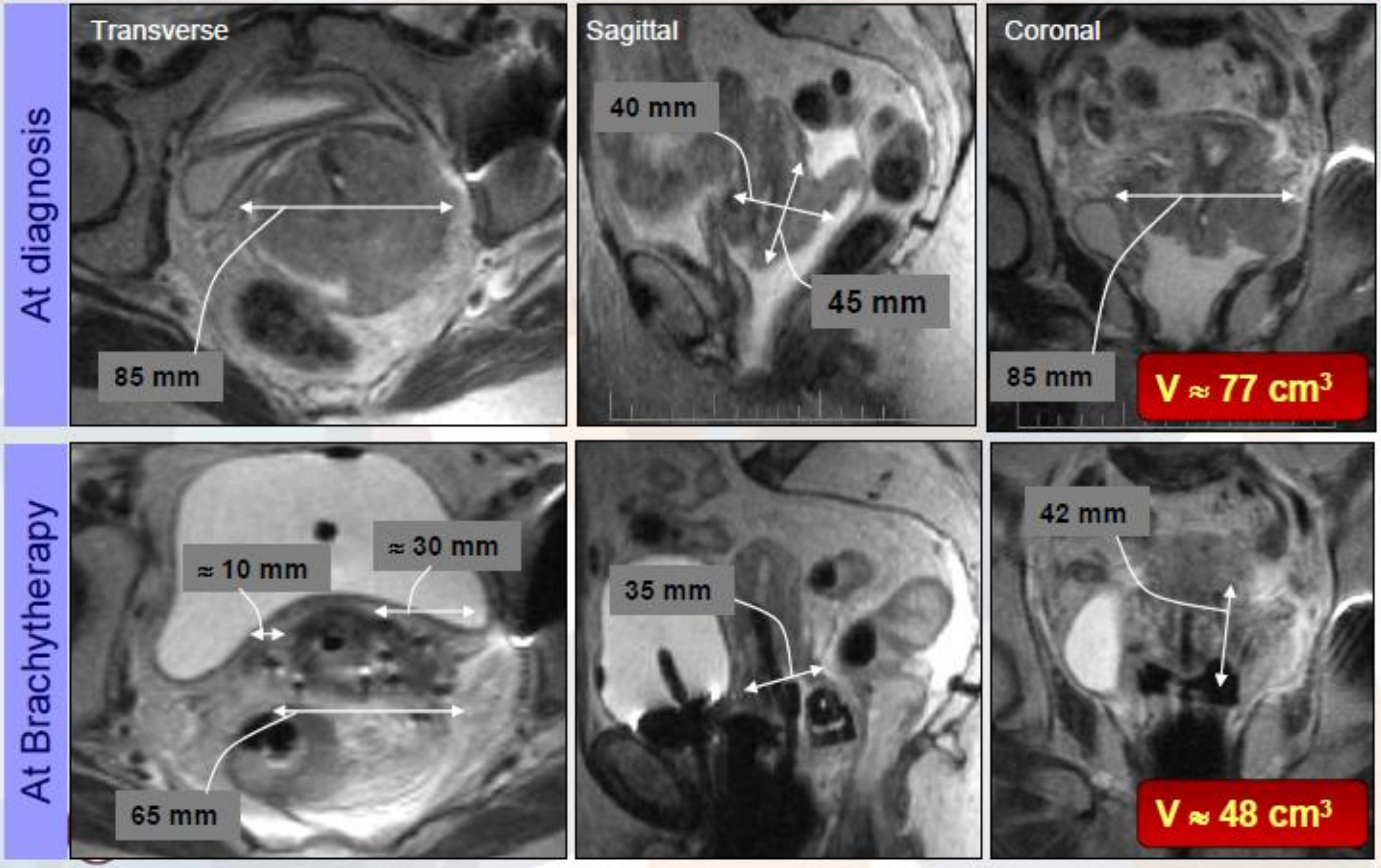
Tandem & Ring

Interstitial parametrial needles according to tumour spread

↳ Following applicator insertion:

pelvic MRI with the applicator in place

MRI findings



Radiotherapy and Oncology 78 (2006) 67–77
www.thegreenjournal.com

ESTRO project

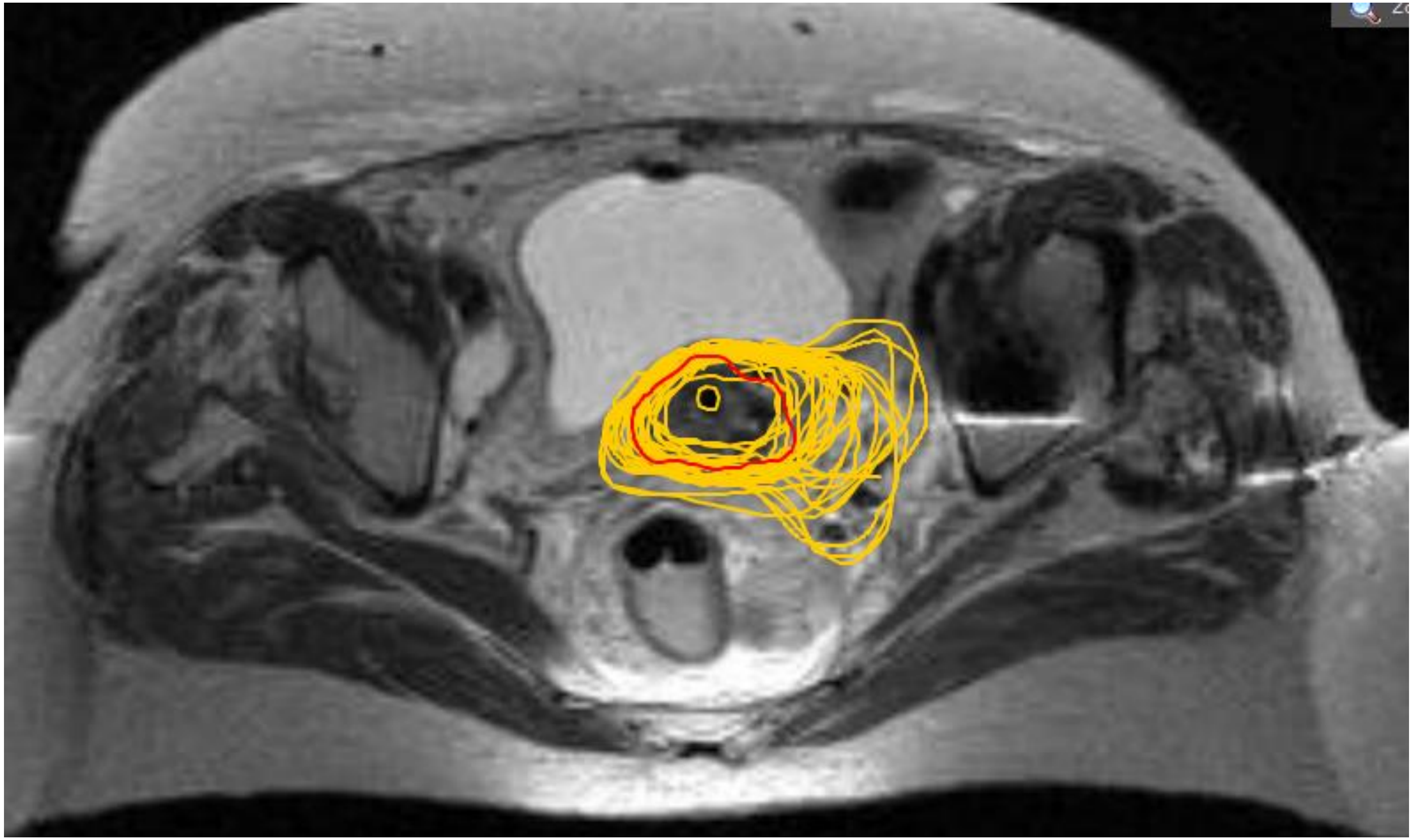
Recommendations from gynaecological (GYN) GEC ESTRO working group (II): Concepts and terms in 3D image-based treatment planning in cervix cancer brachytherapy—3D dose volume parameters and aspects of 3D image-based anatomy, radiation physics, radiobiology

Richard Pötter[a,*], Christine Haie-Meder[b], Erik Van Limbergen[c], Isabelle Barillot[d], Marisol De Brabandere[c], Johannes Dimopoulos[a], Isabelle Dumas[b], Beth Erickson[e], Stefan Lang[a], An Nulens[c], Peter Petrow[f], Jason Rownd[e], Christian Kirisits[a]

[a]*Department of Radiotherapy and Radiobiology, Medical University of Vienna, Austria,* [b]*Department of Radiotherapy, Brachytherapy Unit, Institut Gustave Roussy, Villejuif, France,* [c]*Department of Radiotherapy, University Hospital Gasthuisberg, Leuven, Belgium,* [d]*Department of Radiation Oncology, Centre George-Francois Leclerc, Dijon, France,* [e]*Department of Radiation Oncology, Medical College of Wisconsin, Milwaukee, WI, USA,* [f]*Service de Radiodiagnostic, Institut Curie, Paris, France*

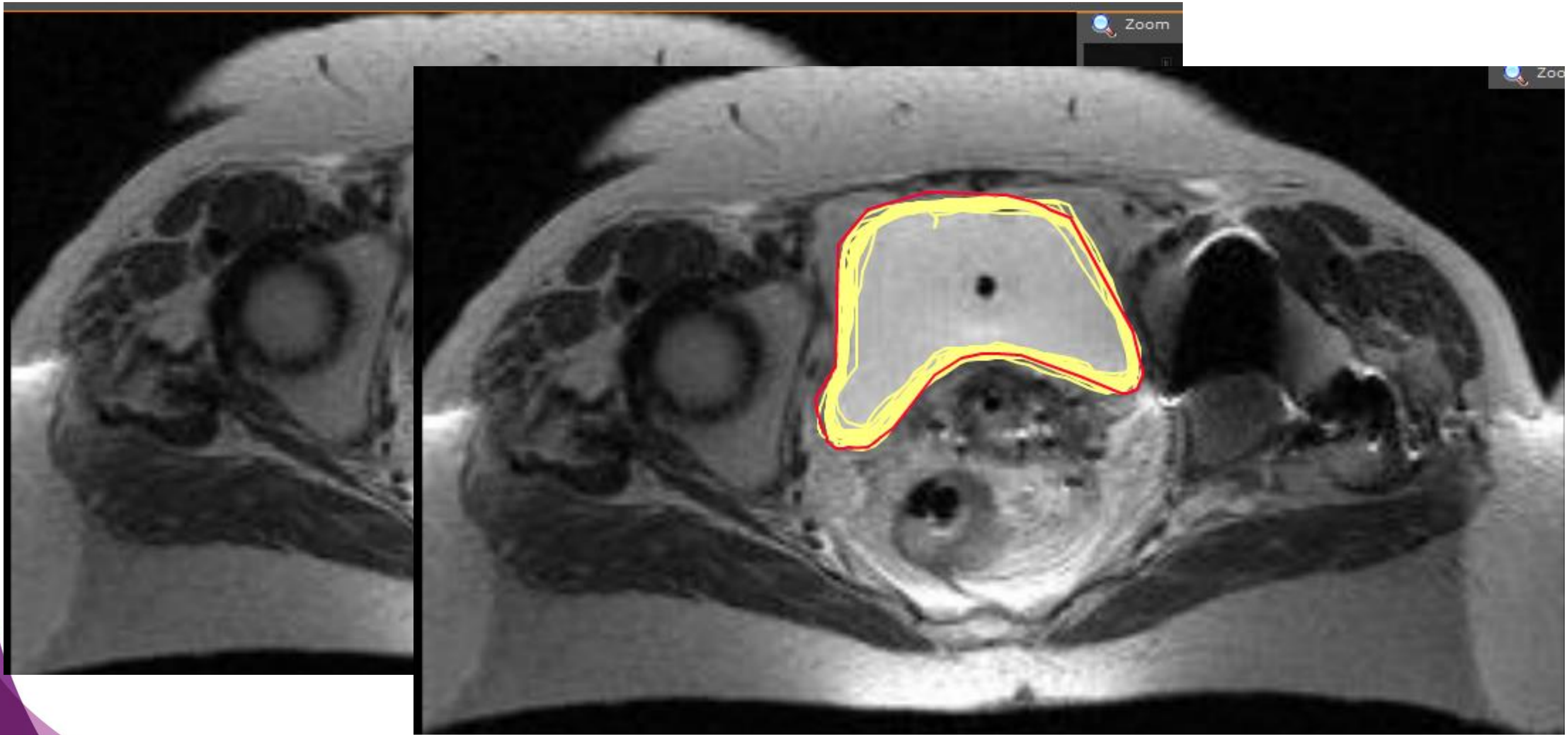
Heterogeneity in contouring target volumes besides the use of guidelines

- High Risk CTV

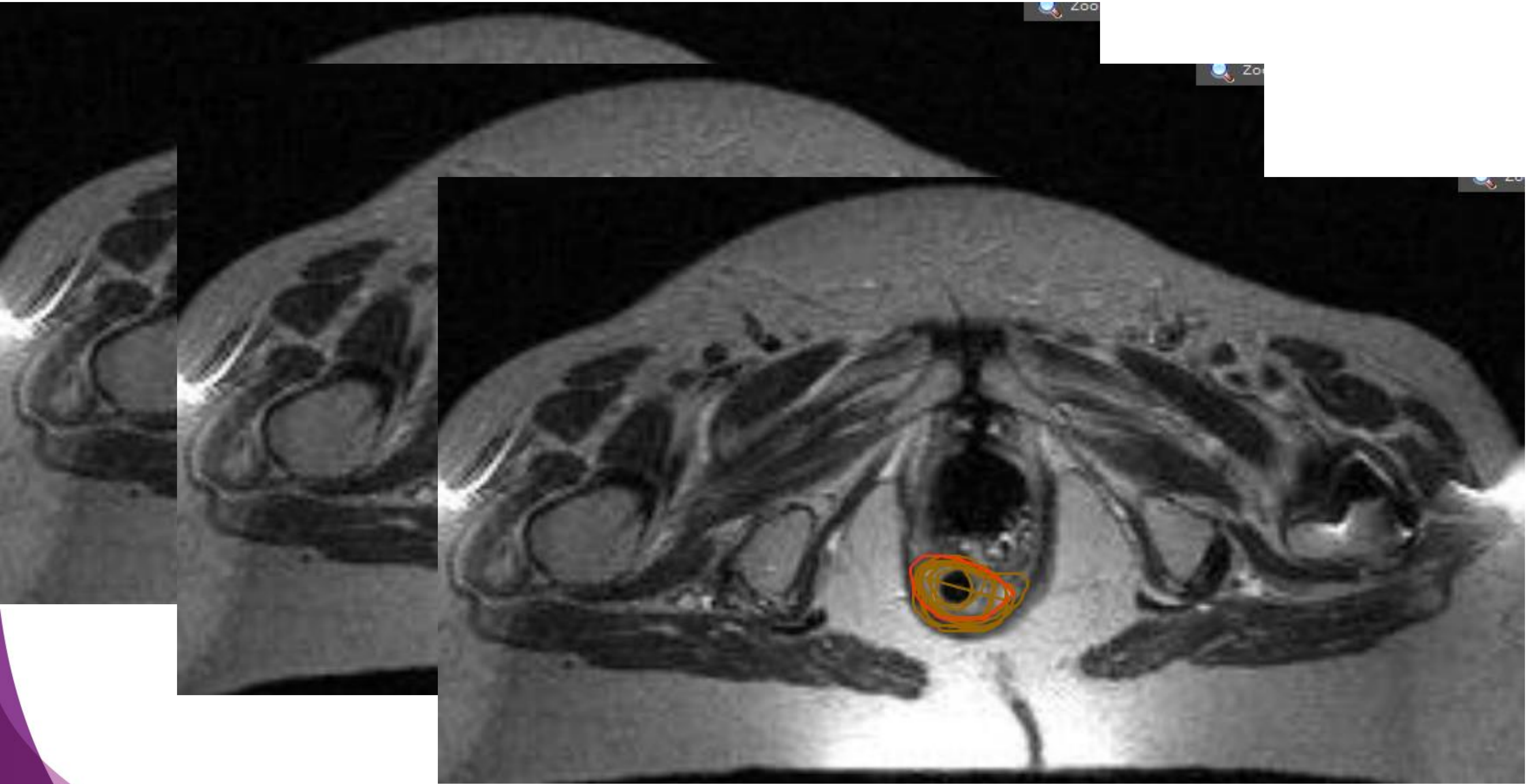


Quite good homogeneity in some OAR contouring

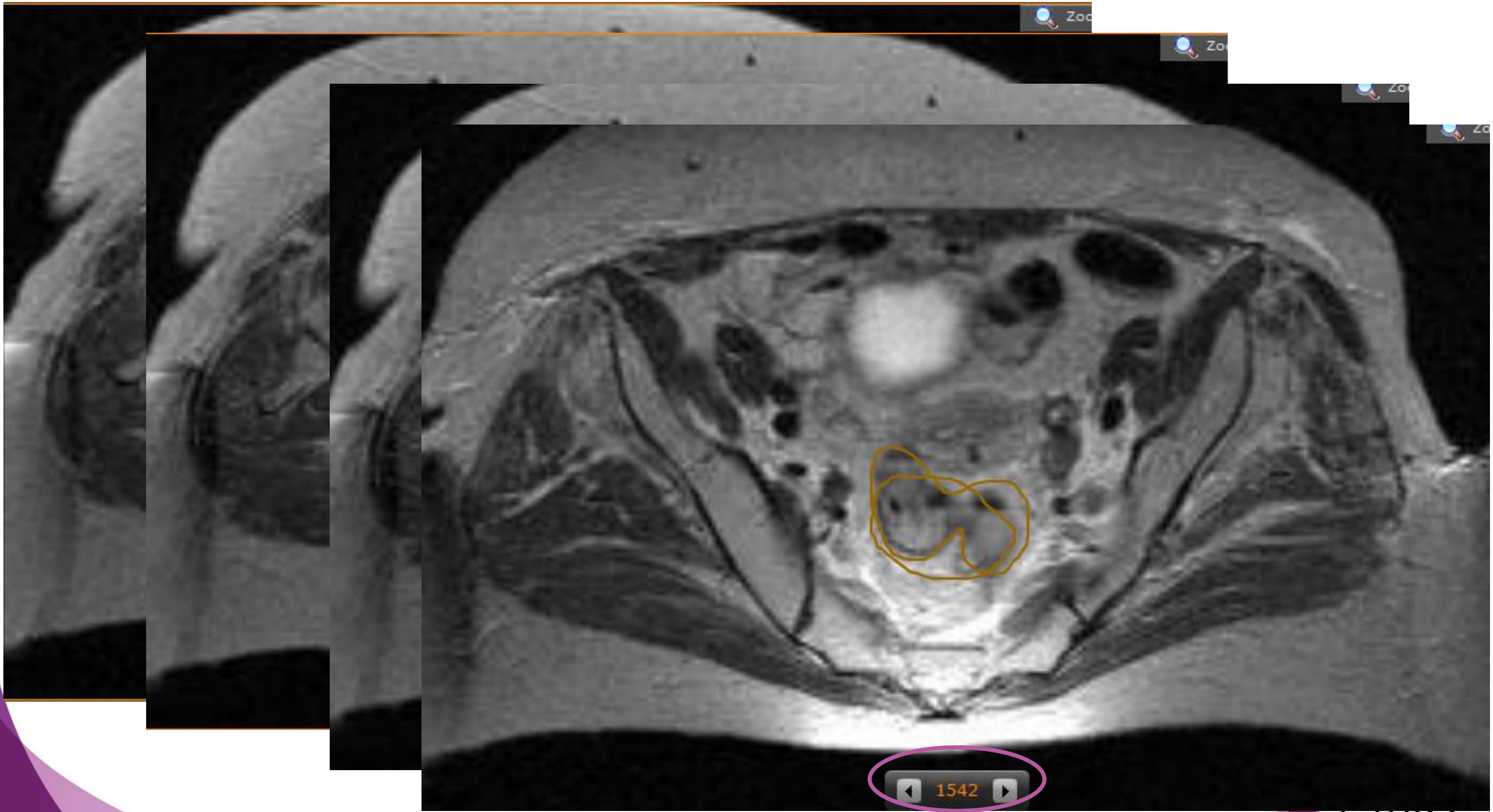
- Where anatomical bundaries are well visible



But it's not always the case!



Upper and lower limits are a source of heterogeneity in contouring as well



5 slices = 1,5cm difference in the upper limit of the rectum

Take home messages:

- High quality CT, MR imaging and clinical examination are crucial for contouring targets and OAR in the pelvic region

- High quality re-imaging and clinical examination are key points in cervical cancer to adapt contours for brachytherapy dosimetry

- MR is a key imaging modality in gynecology

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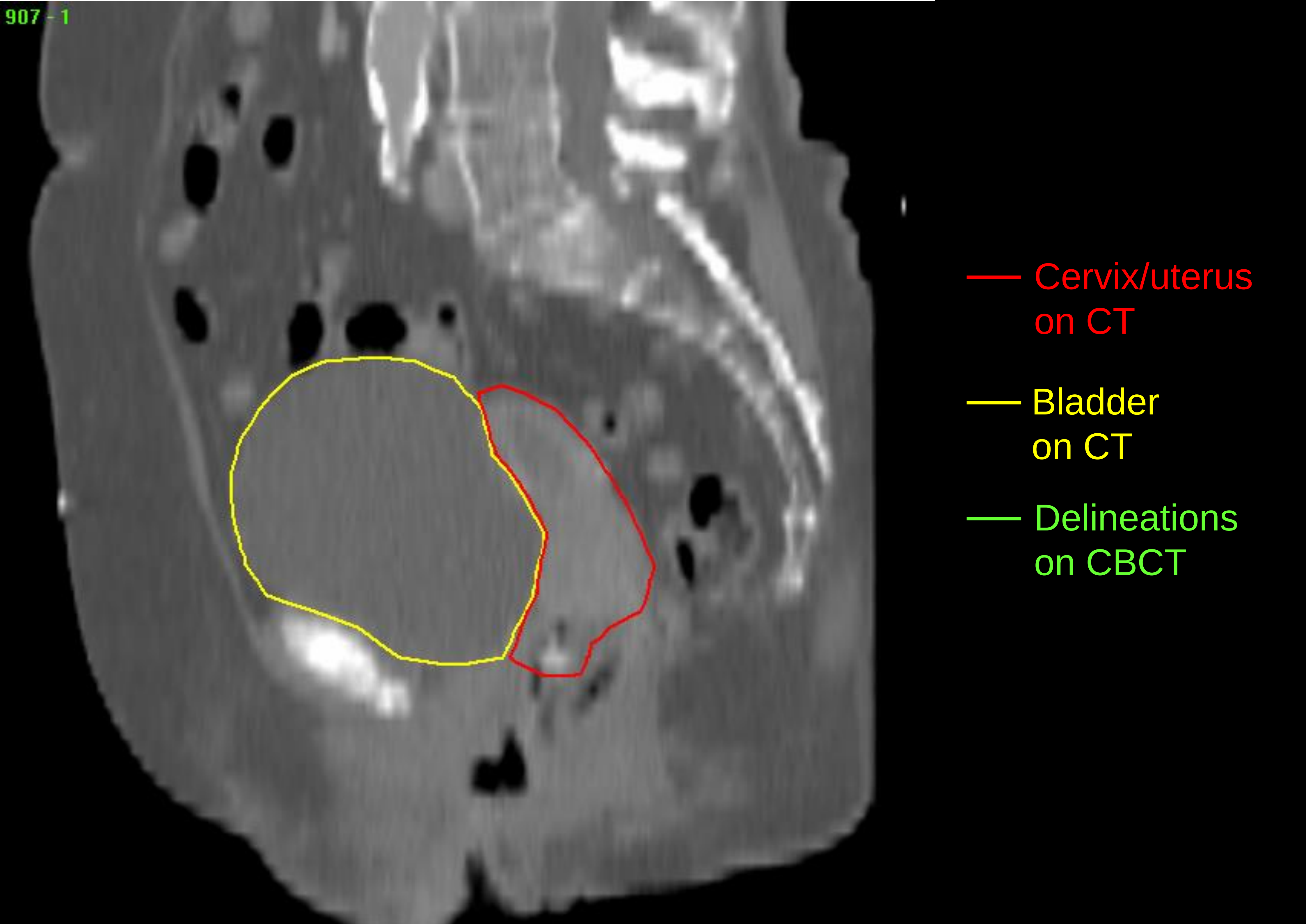
Cervix case – Physics aspects

Peter Remeijer


907 - 1
Cervix/uterus on CT
Bladder on CT
Delineations on CBCT

The main issue

- Very large movement
- Clinically a margin of 2 cm is used
- Probably too small

Options

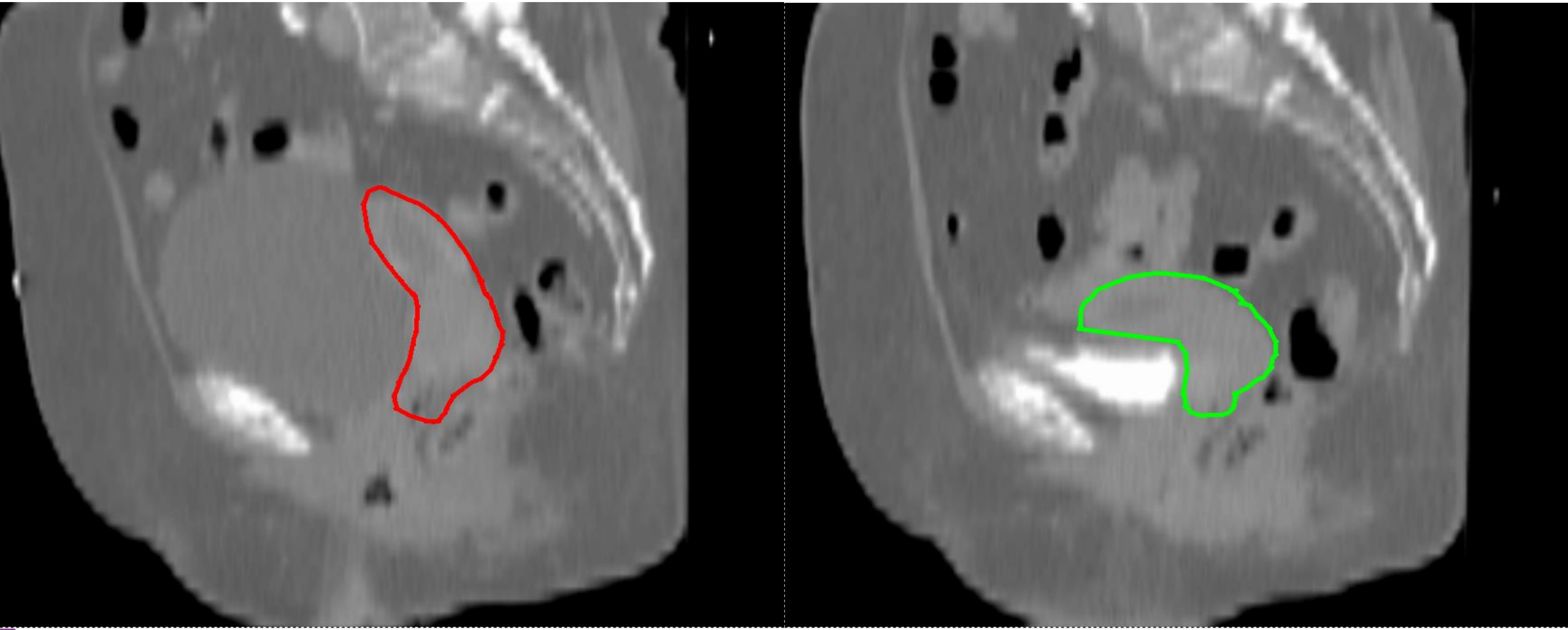
- Drinking protocol
  - ➢ Does it work?
- Scan and postpone treatment if not ok
  - ➢ Ask patient to empty bladder or drink and wait
  - ➢ Not very efficient
- Adapt the plan
  - ➢ Fast planning and delineation not readily available
  - ➢ A-priori plans – select the right one at treatment


hey, i had a full bladder

Options

- Drinking protocol
  - ➢ Does it work?
- Scan and postpone treatment if not ok
  - ➢ Ask patient to empty bladder or drink and wait
  - ➢ Not very efficient
- Adapt the plan
  - ➢ Fast planning and delineation not readily available
  - ➢ A-priori plans – select the right one at treatment

Full/empty bladder CT



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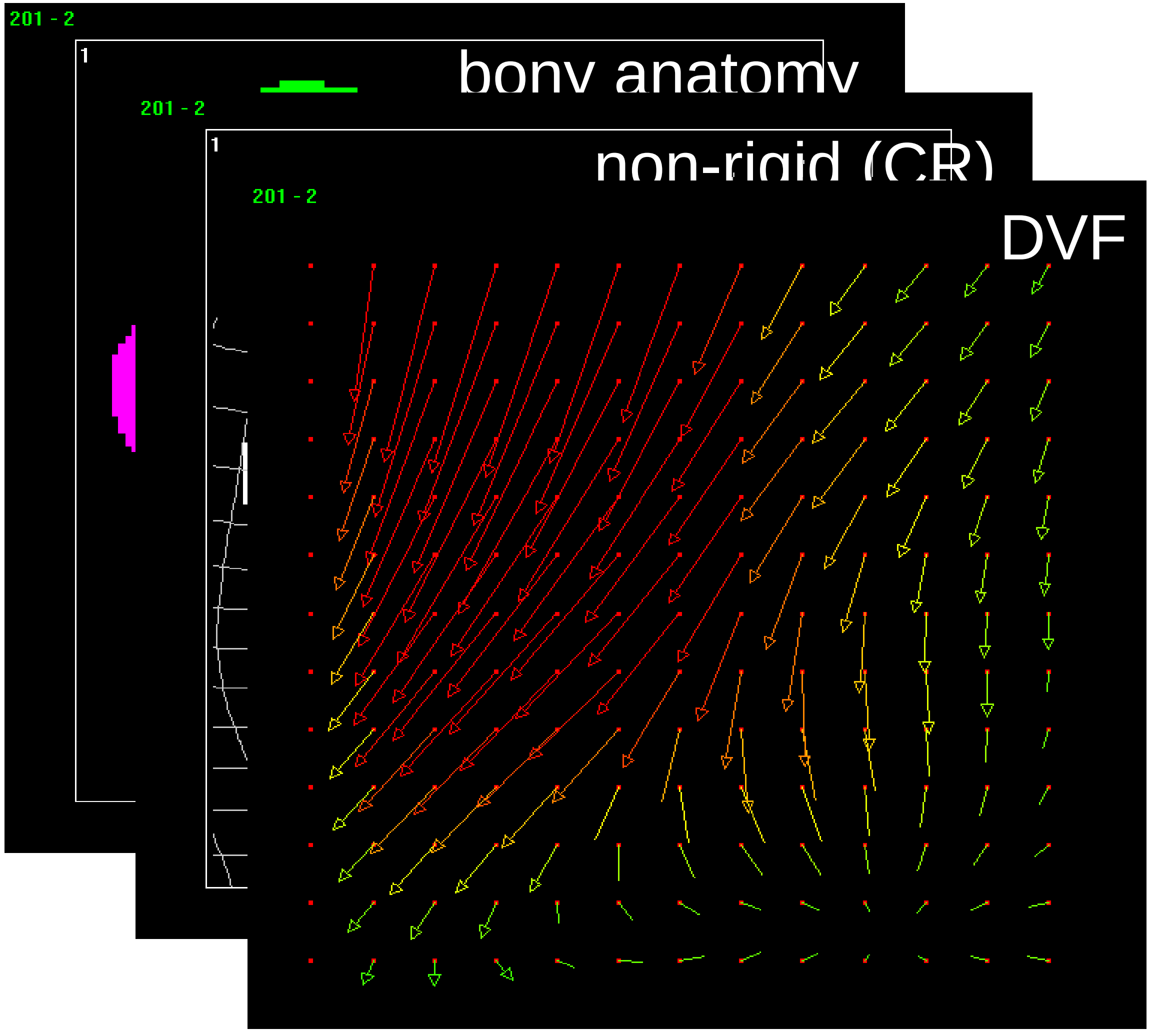
Generate uterus motion model

Delineate on full and empty bladder CT

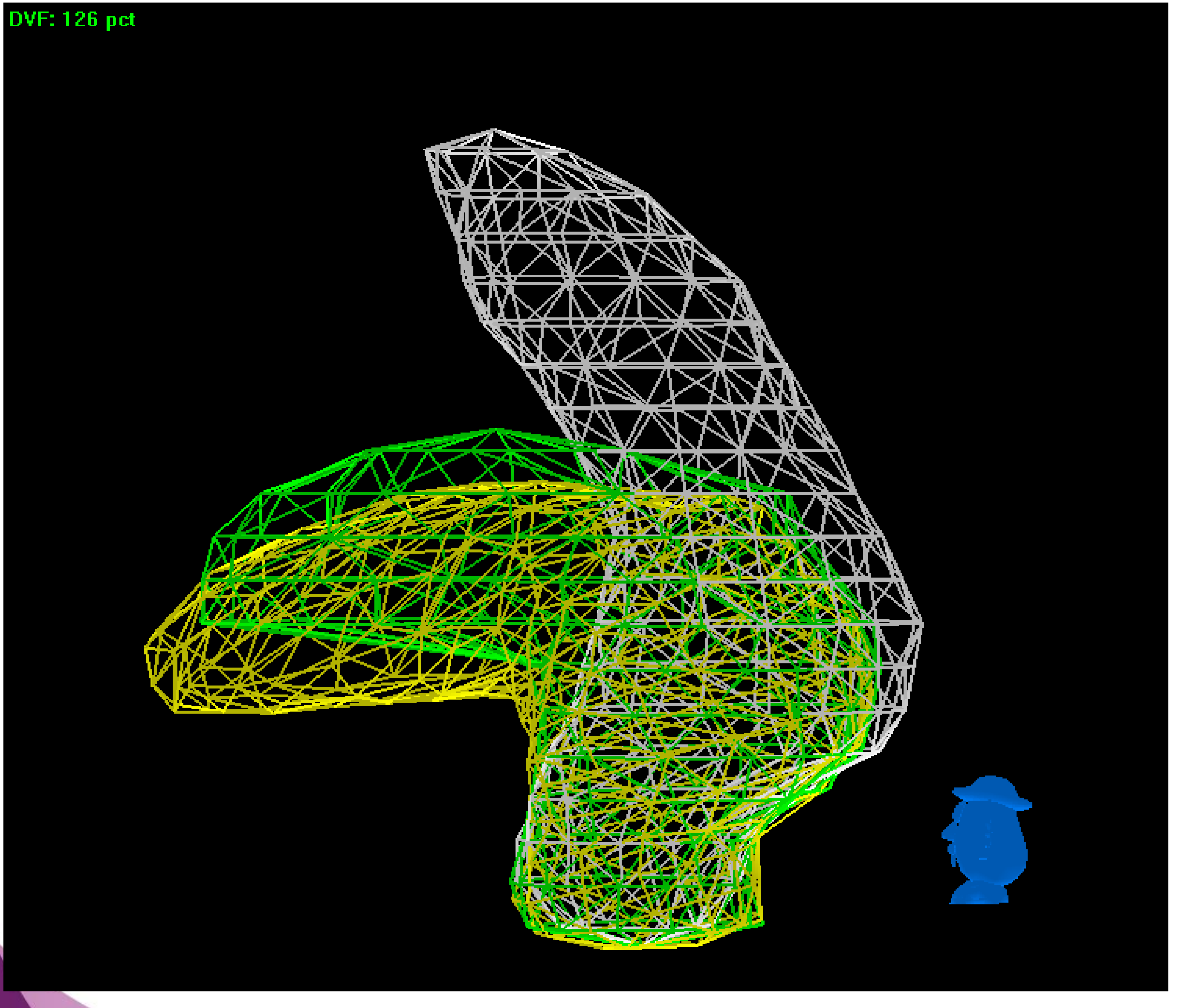
Deform full bladder contour

Generated warp field is model for organ motion



School

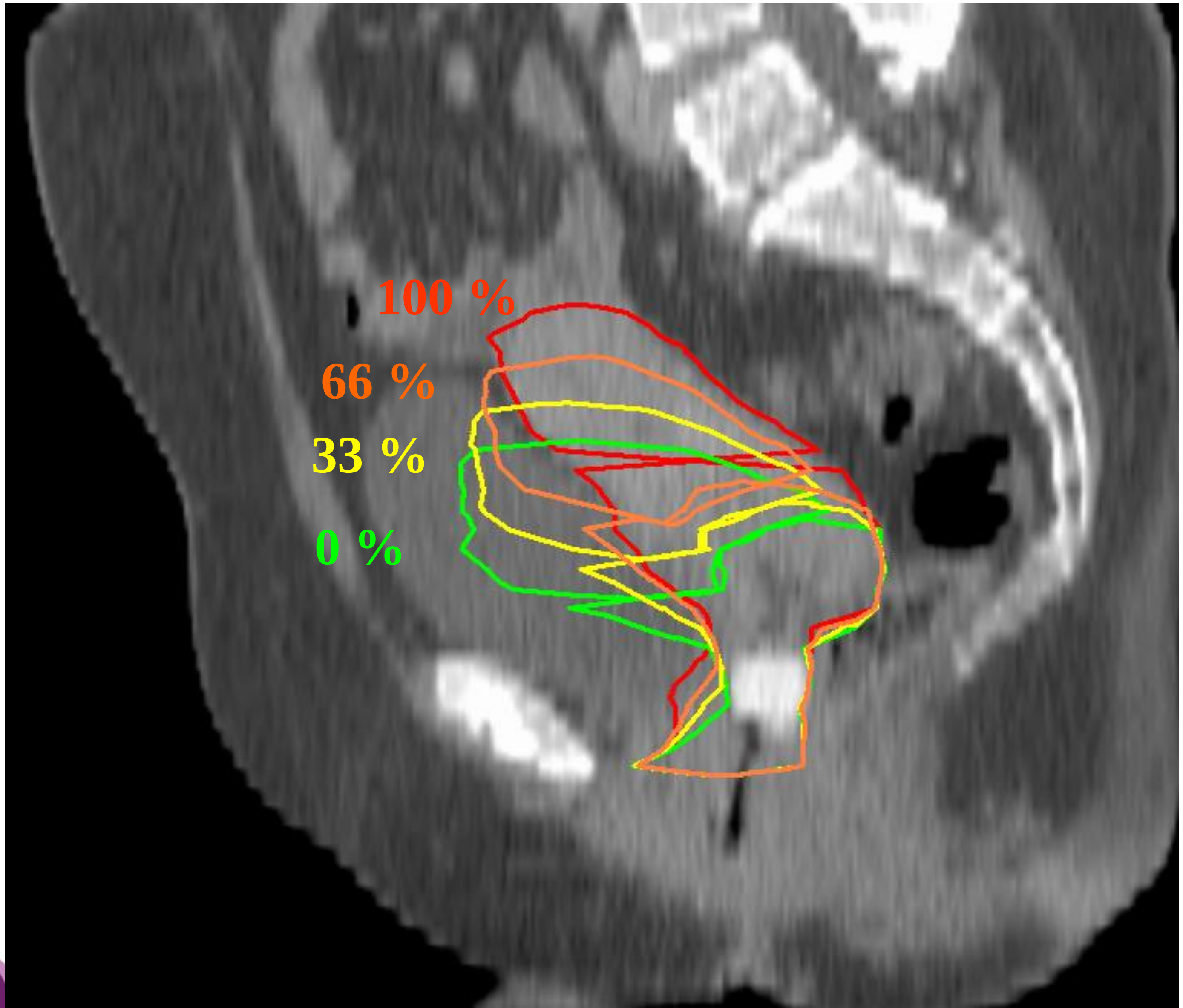
Uterus motion model



Select 4 bladder fillings based on this model:

- 0 %
- 33 %
- 66 %
- 100 %

Generated CTVs



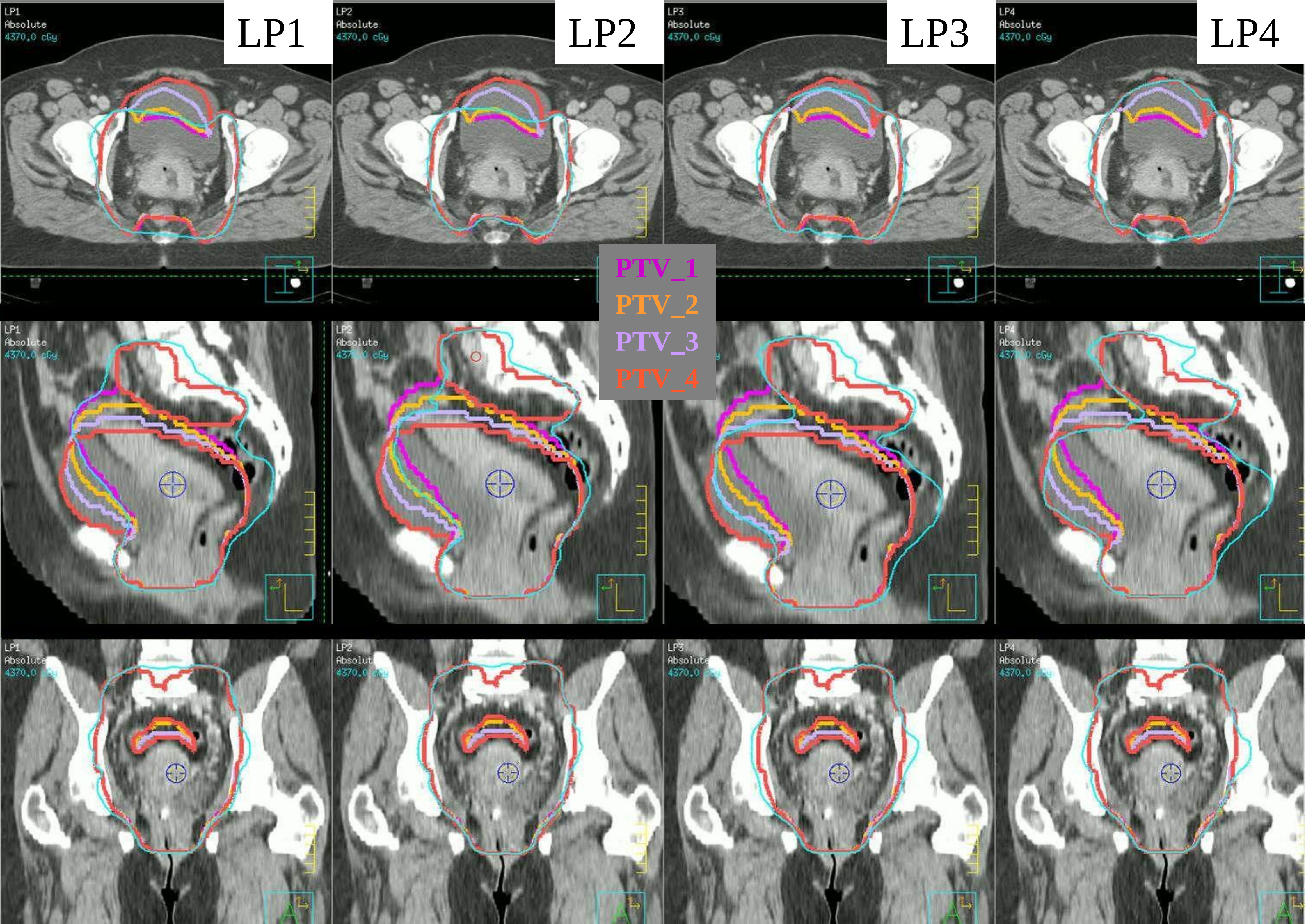
Select 4 bladder fillings based on this model:

- 0 %
- 33 %
- 66 %
- 100 %

Planning

Planning

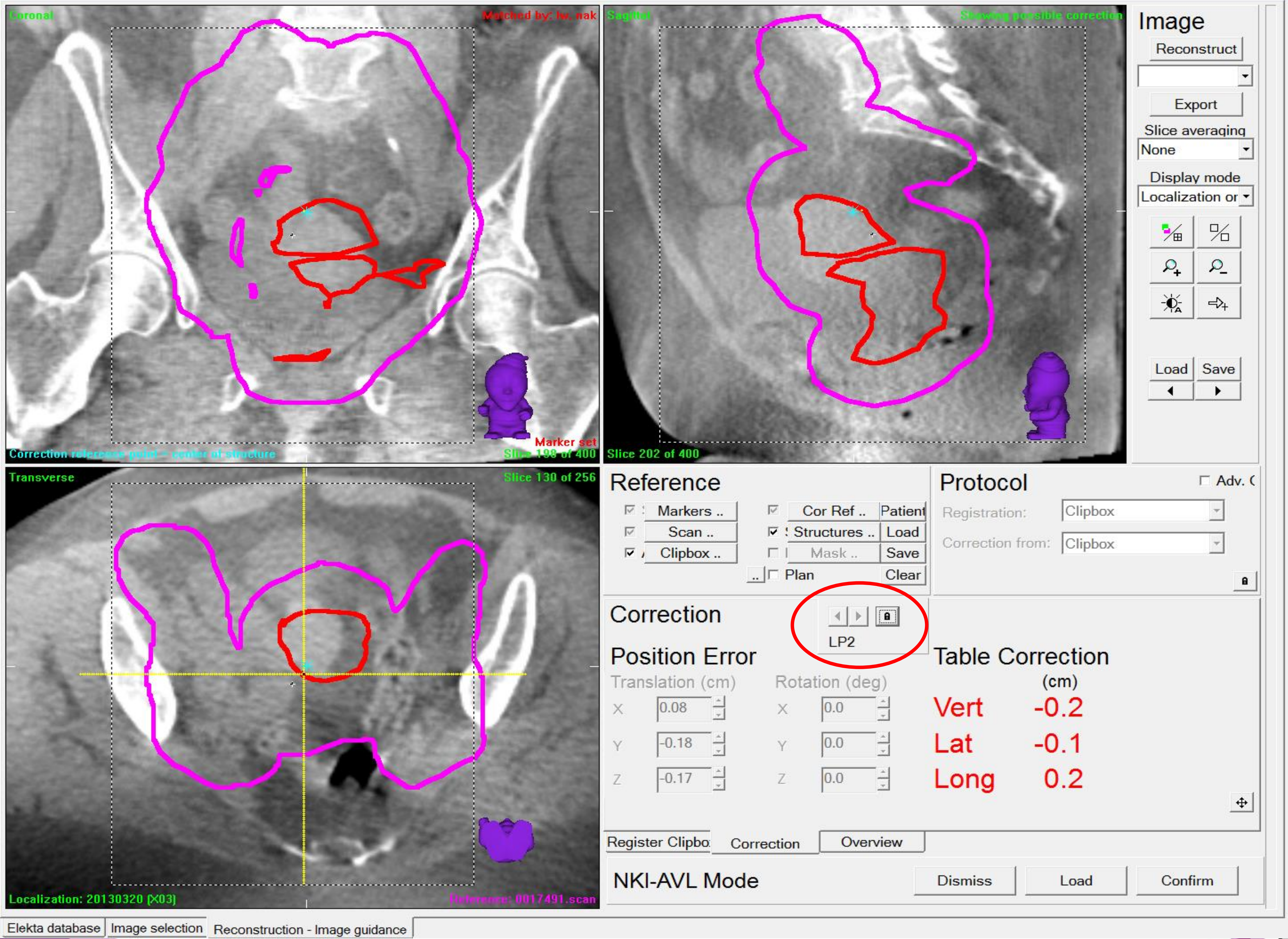
- 1 VMAT plan created manually (66%, LP2)
- Used as starting point to create three plans automatically (Pinnacle scripting)
- All plans based on full bladder CT scan
  - ➢ Dosimetrically not correct
  - ➢ Small deviations (1-2 %)



LP1
LP2
LP3
LP4
PTV_1
PTV_2
PTV_3
PTV_4
Absolute
4370.0 cGy

Treatment

- CBCT scan prior to treatment
- Select the ‘best fitting structure’
- Select corresponding plan on the linac
- Treat
- All steps are checked/interlocked using in-house software



LP1 = full bladder LP4 = empty bladder

Alternatives?

- Only use full/empty scan
  - Margin about half the motion
  - Other errors small compared to motion
- Use CBCT data from the first week
  - Import CBCT data in planning/delineation system
  - Delineate on scans, using planning scan as template
  - Create plan library
- Protocolize everything. It is easy to make mistakes when doing planselection on the linac!

Take home messages

- Drinking protocols are usually not very effective
- Multiple scans to estimate the range of motion are
- Large improvements in geometrical accuracy can be achieved with simple methods
- Protocolize the plan selection process (error prone!)
- Planning and dosimetry is the least of your problems!

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Cervix

ART Library of Plans

Rianne de Jong *RTT*,
Academic Medical Centre, Amsterdam

Prague 2017

m.a.j.dejong@amc.uva.nl

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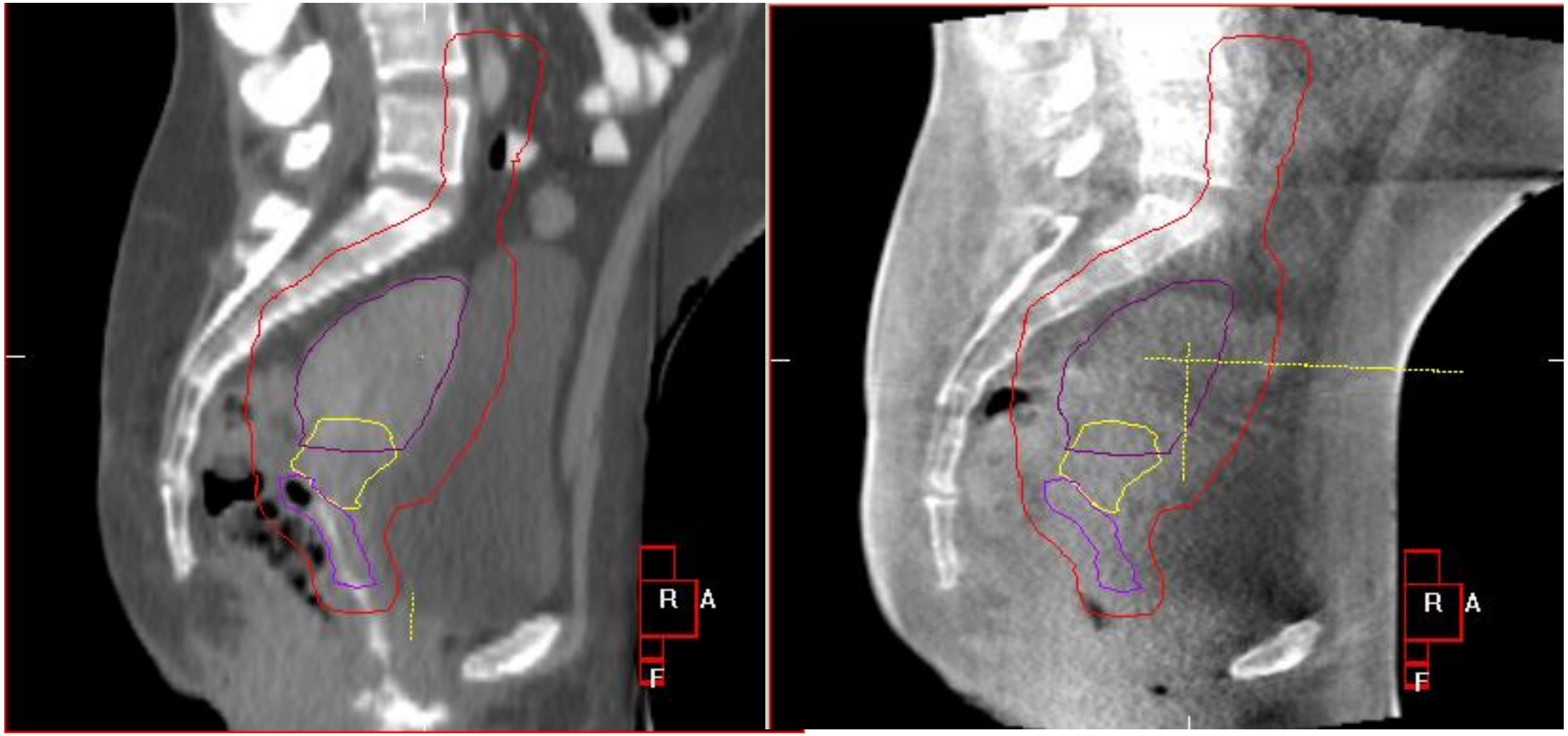
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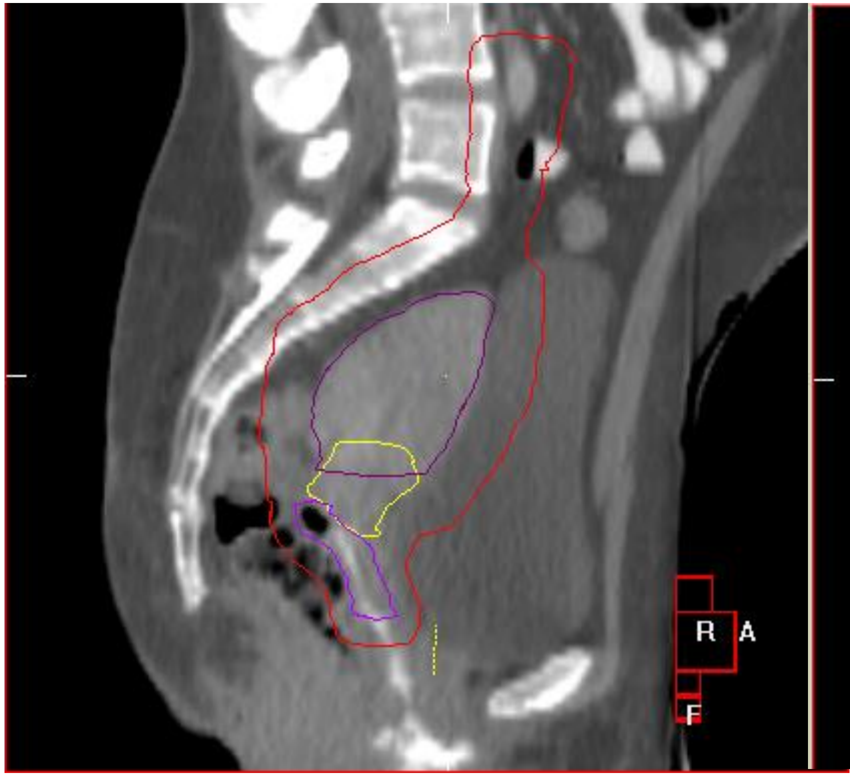
R A
F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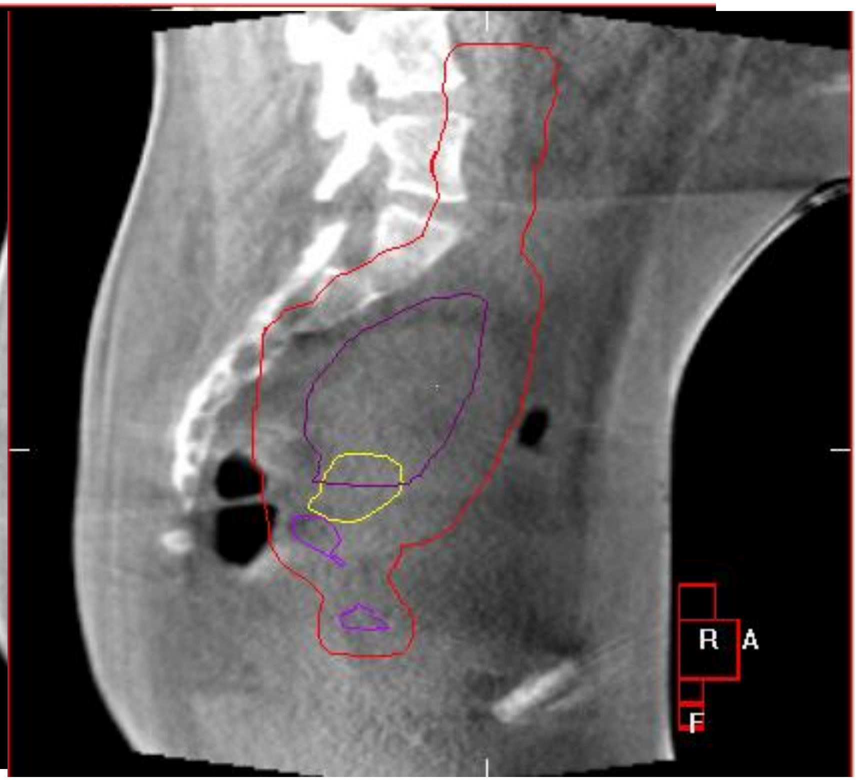
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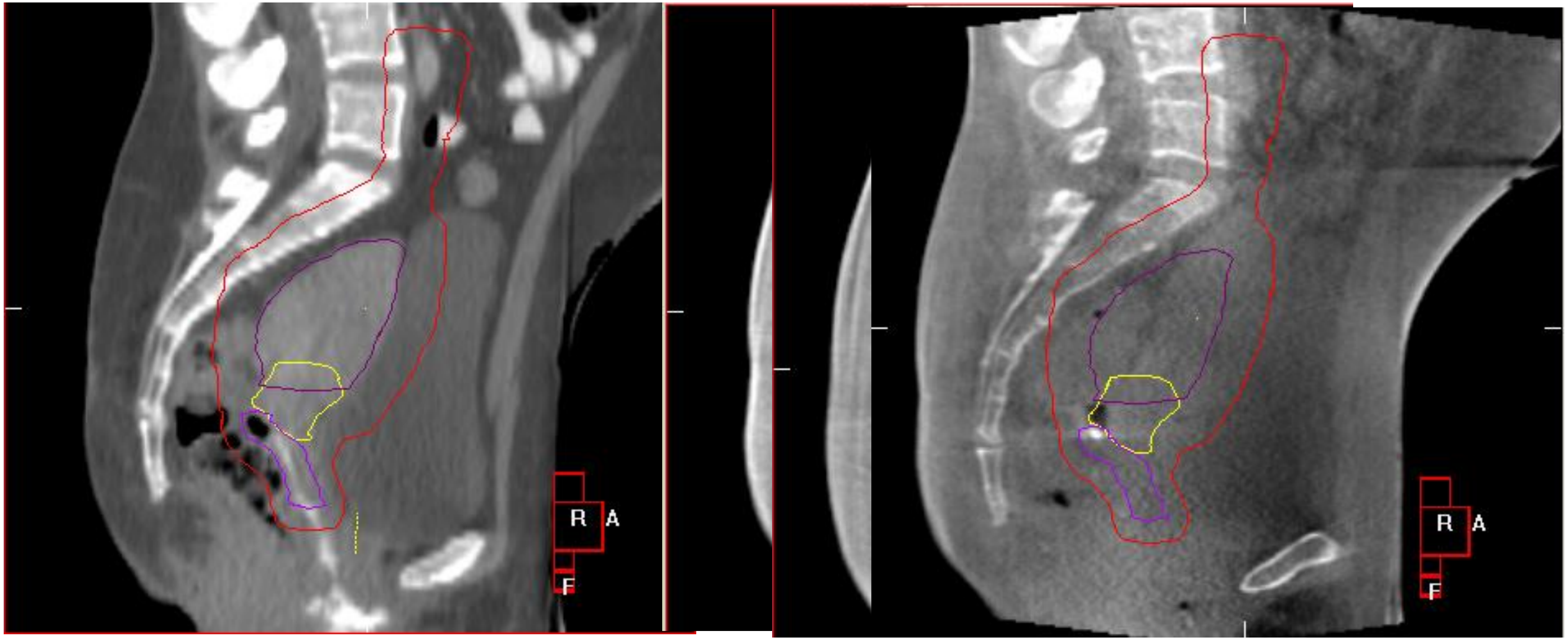
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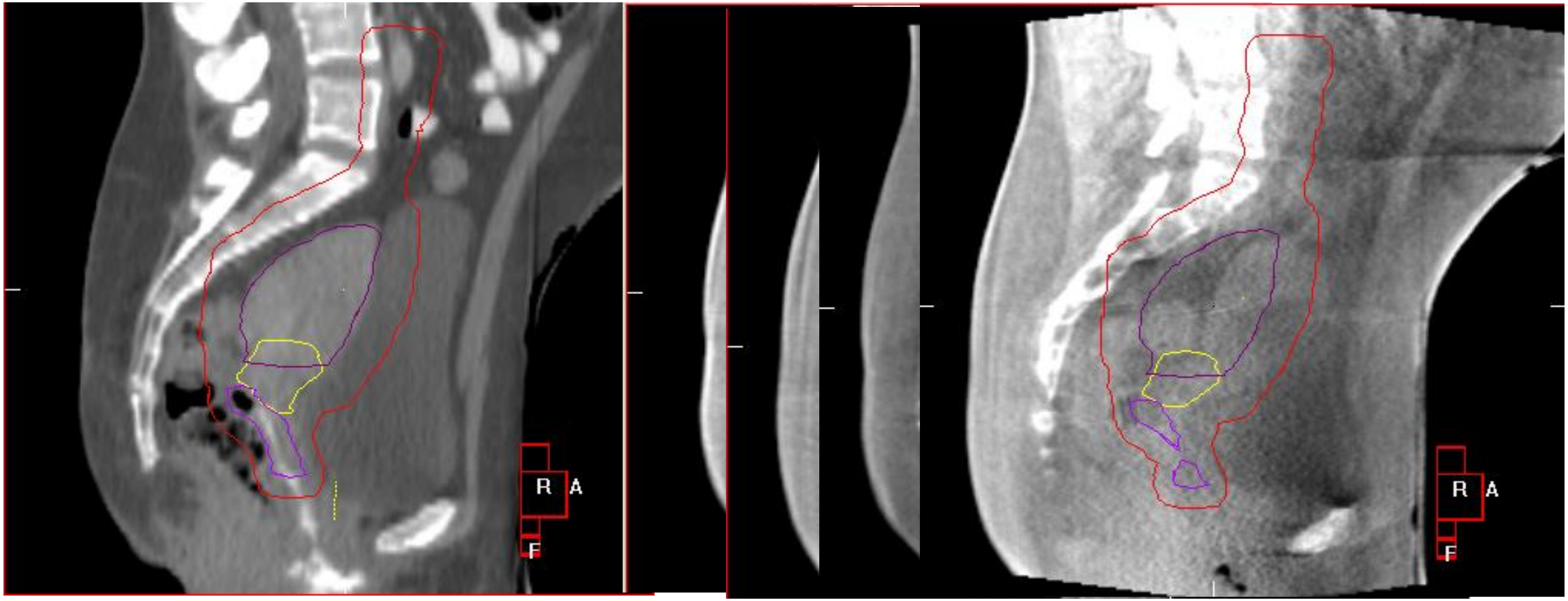
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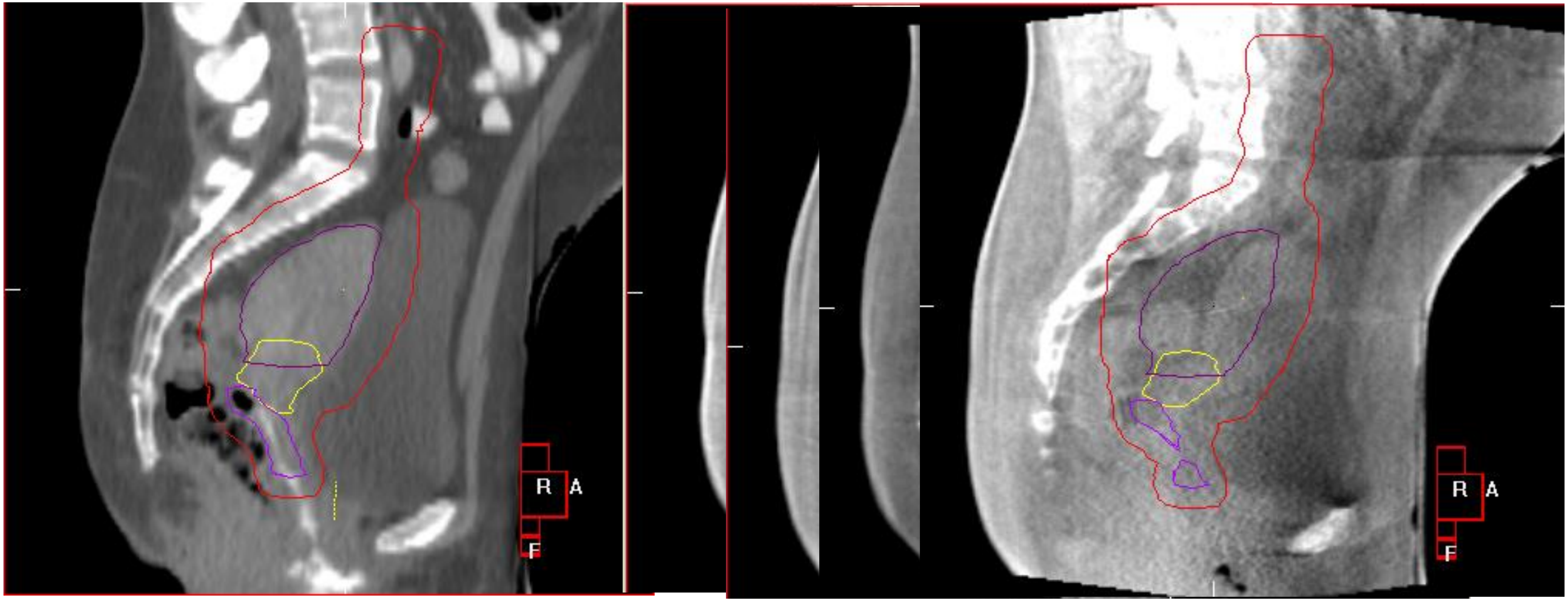
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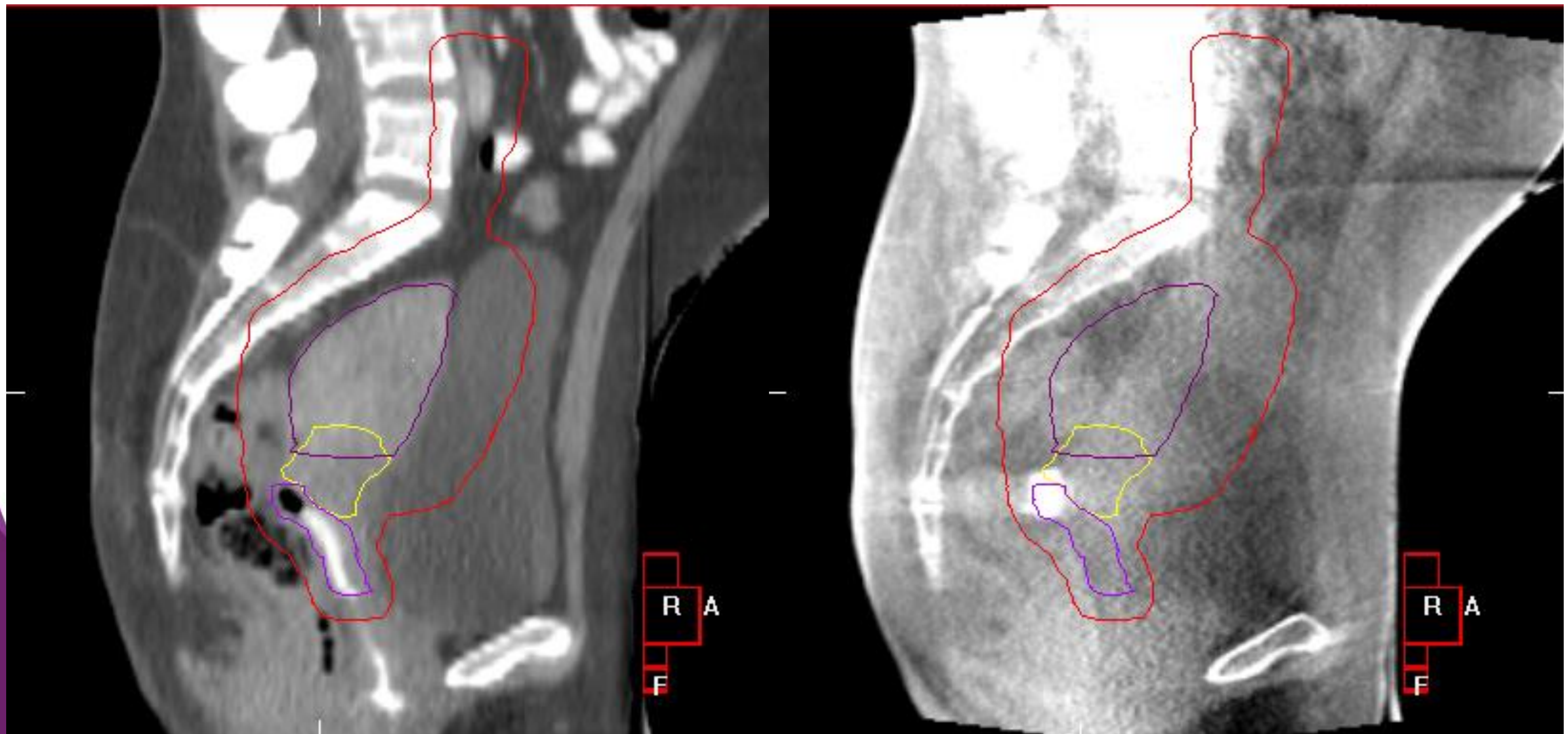
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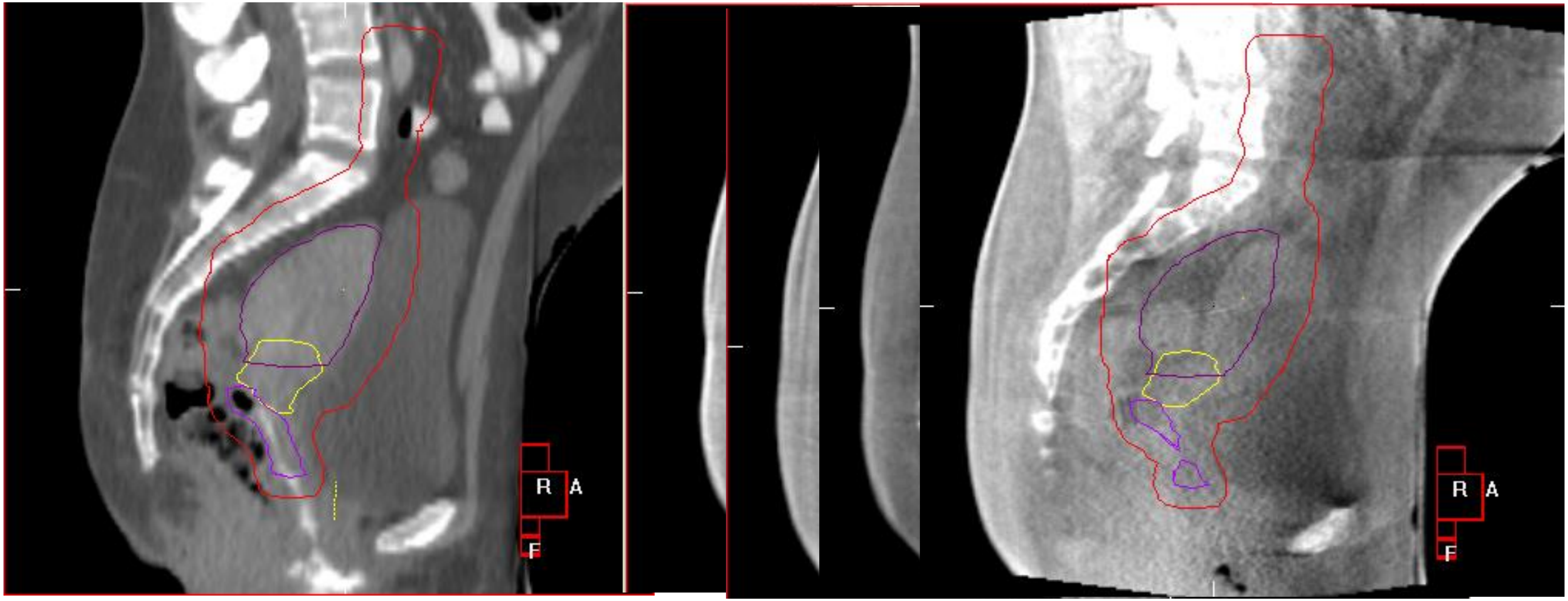
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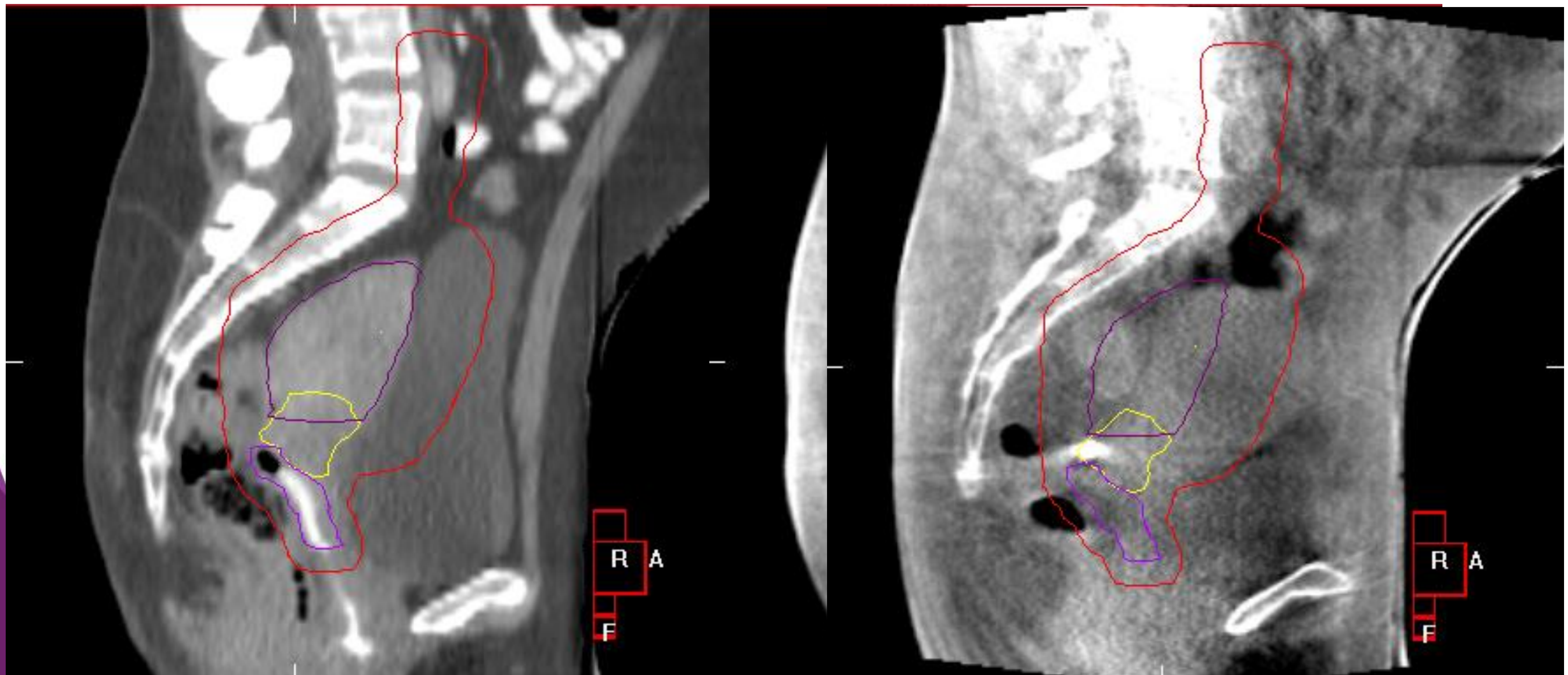
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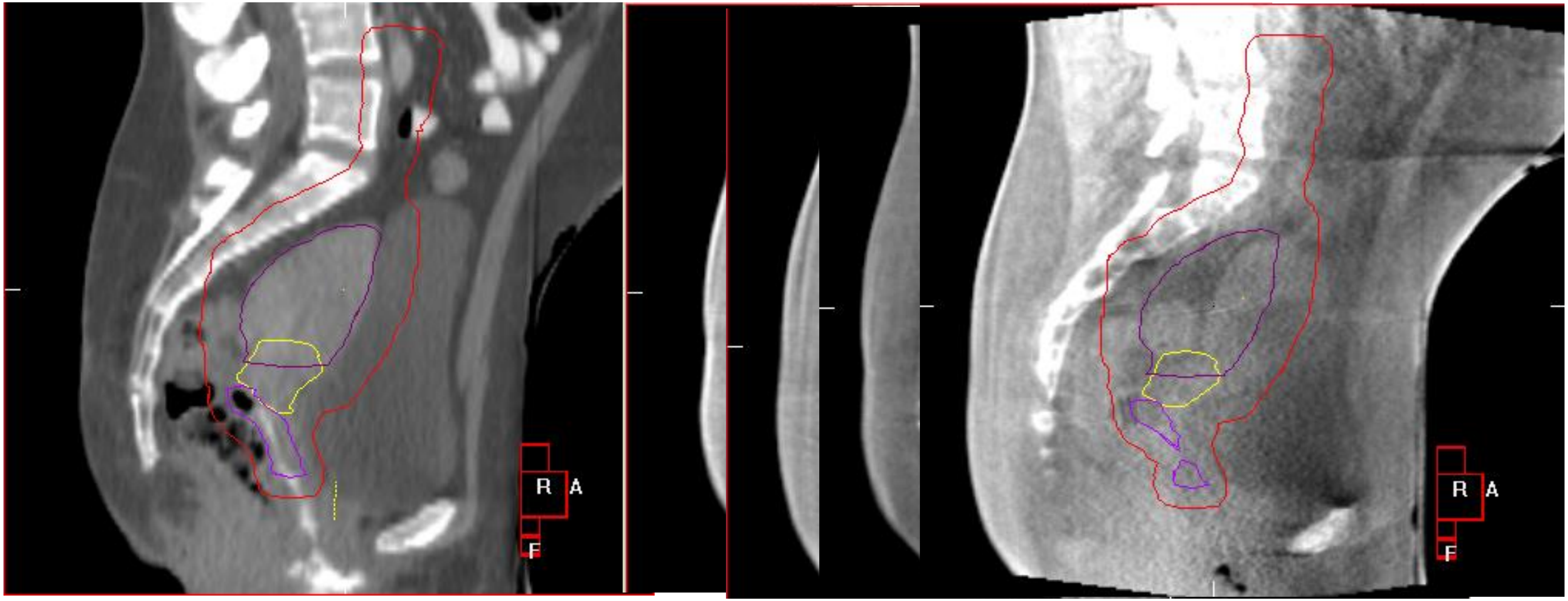

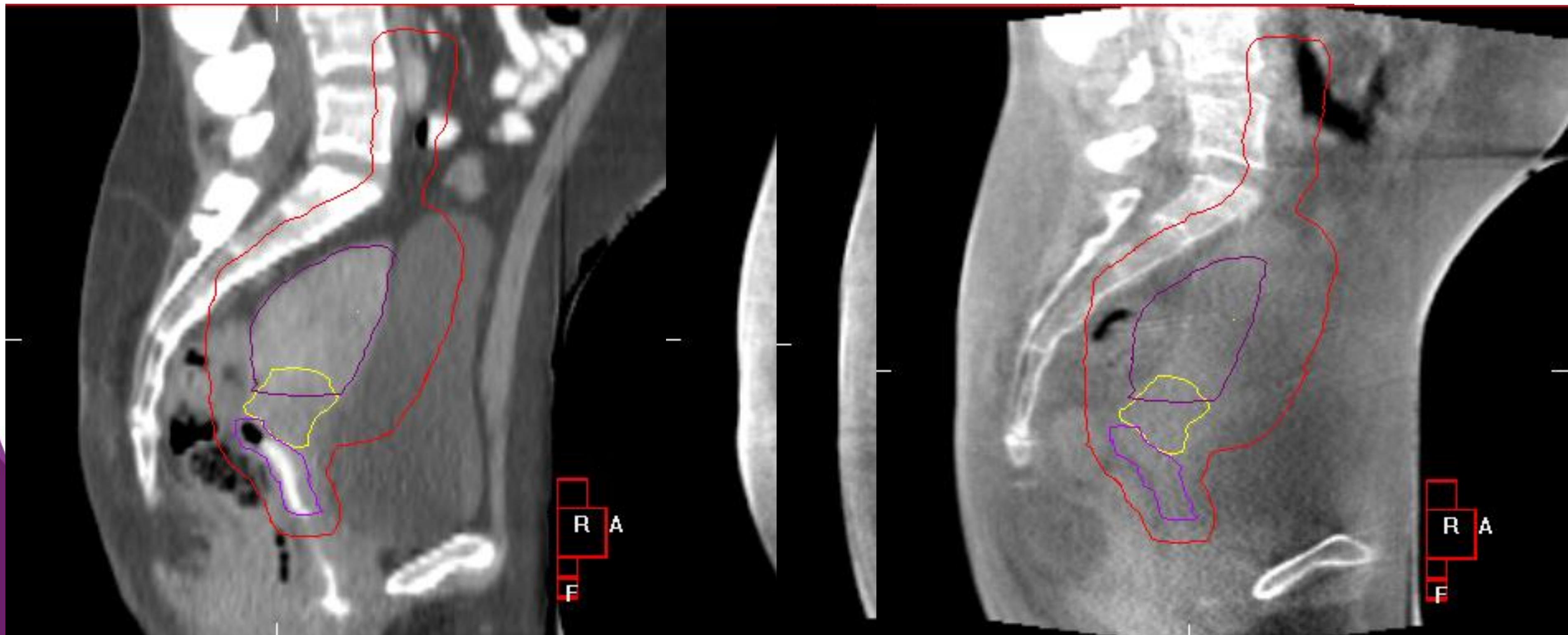

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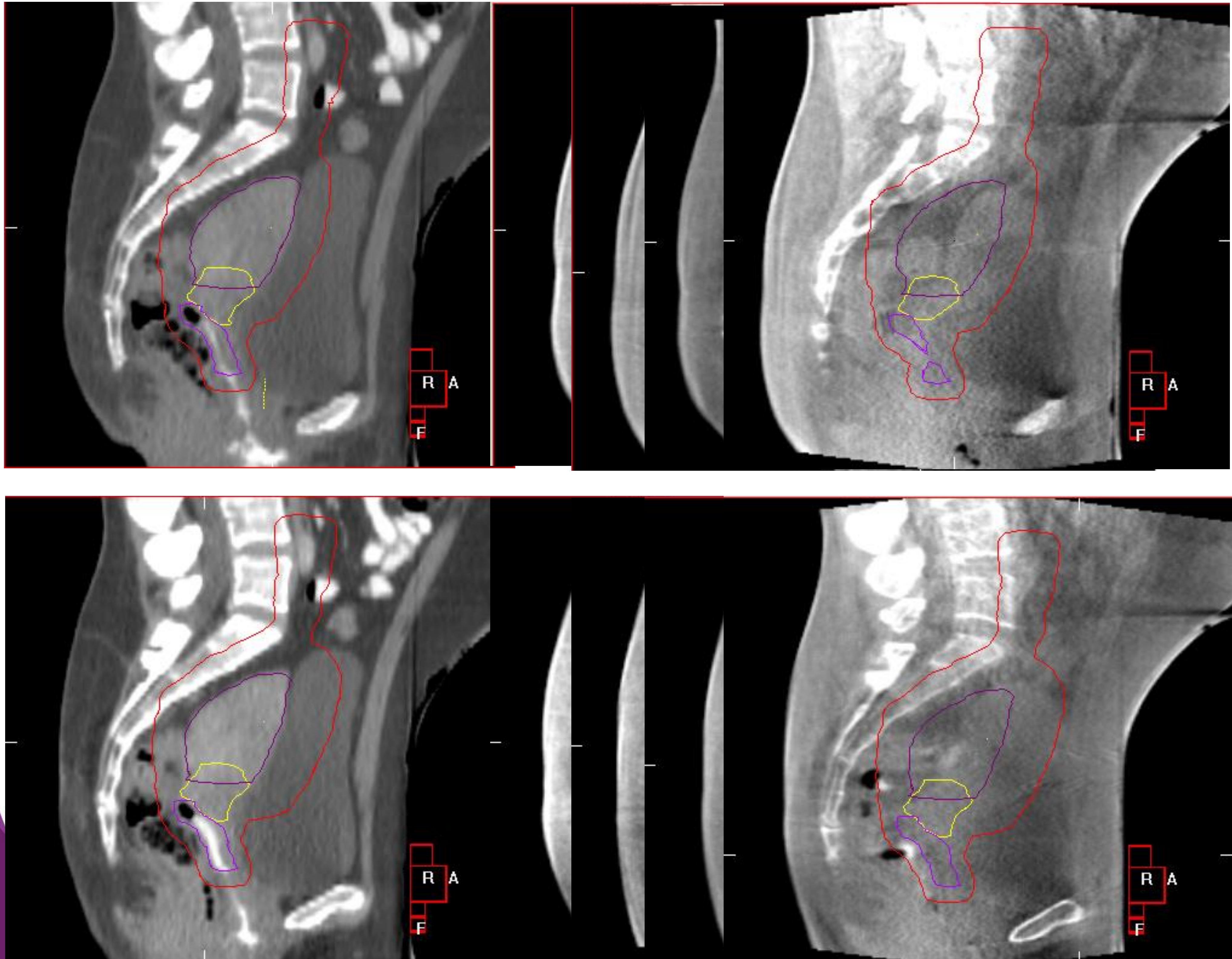
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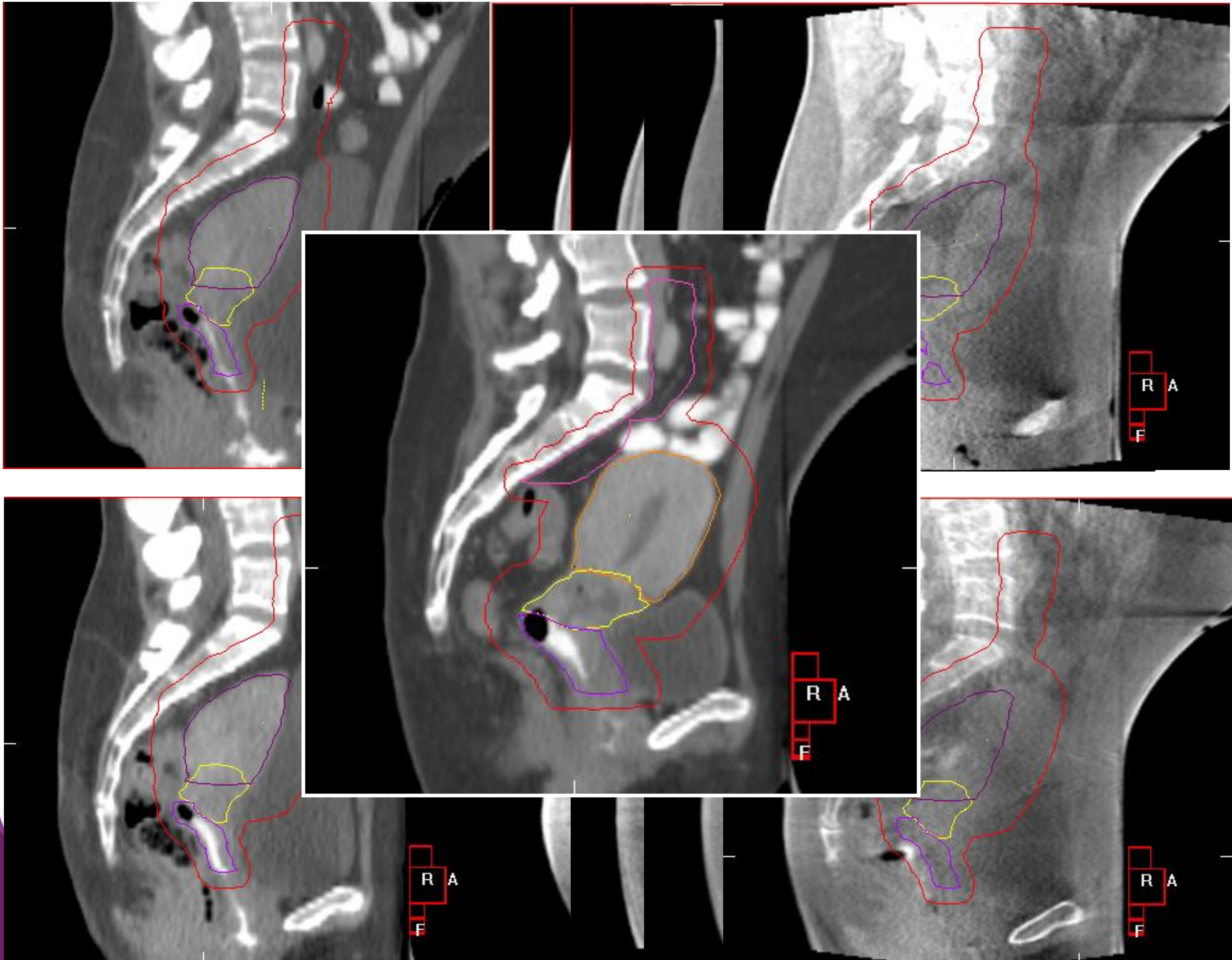
R A
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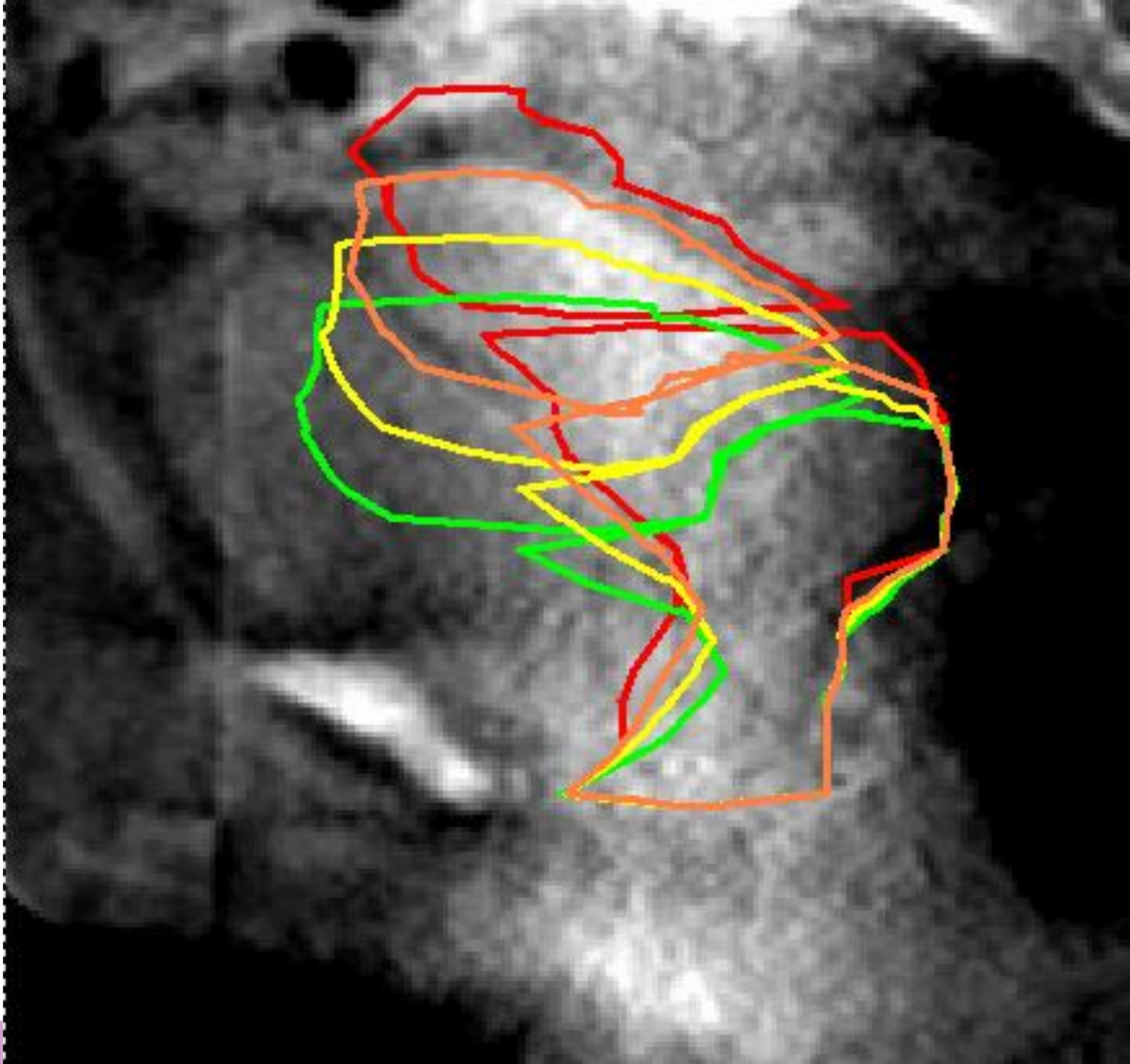
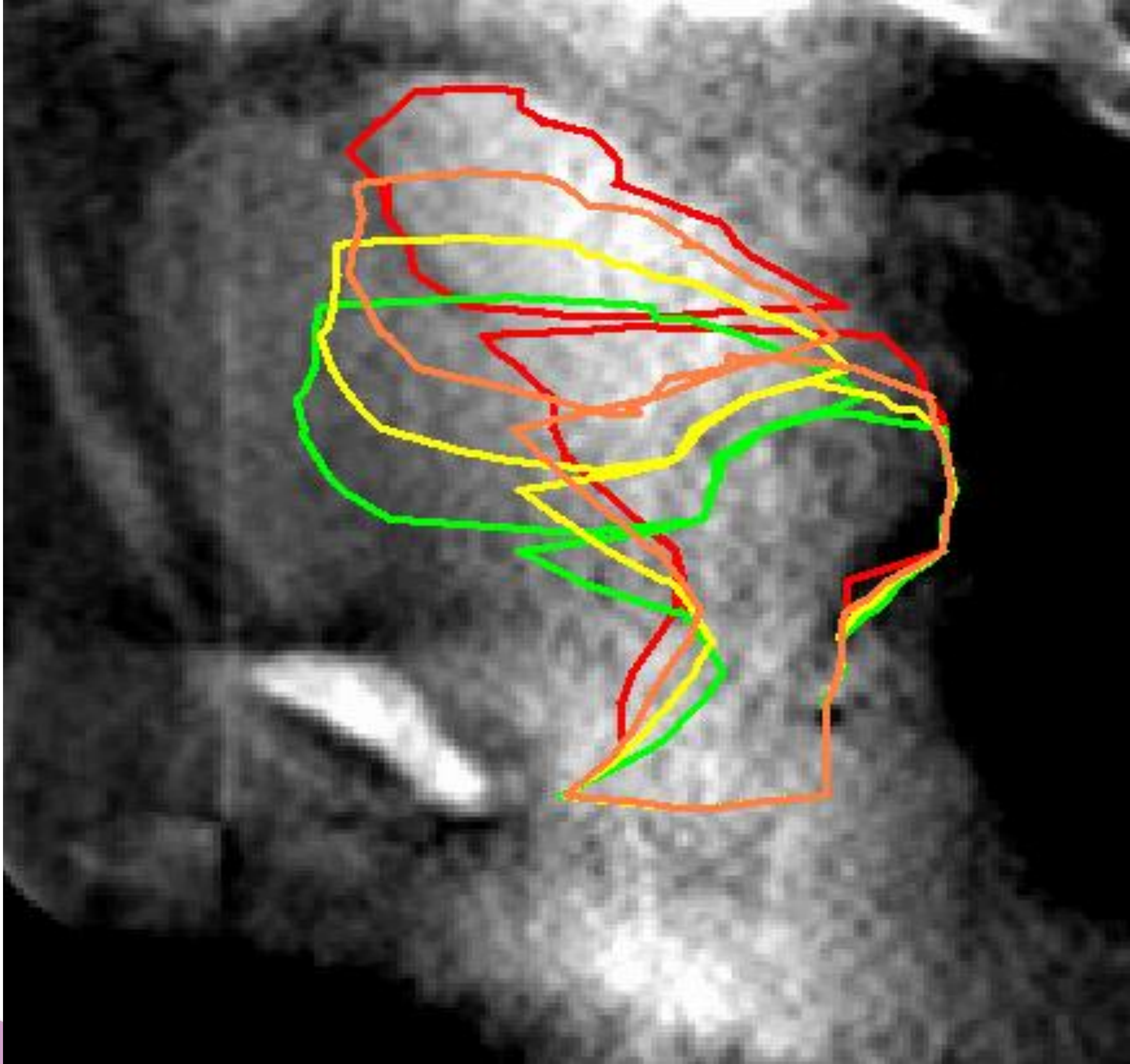
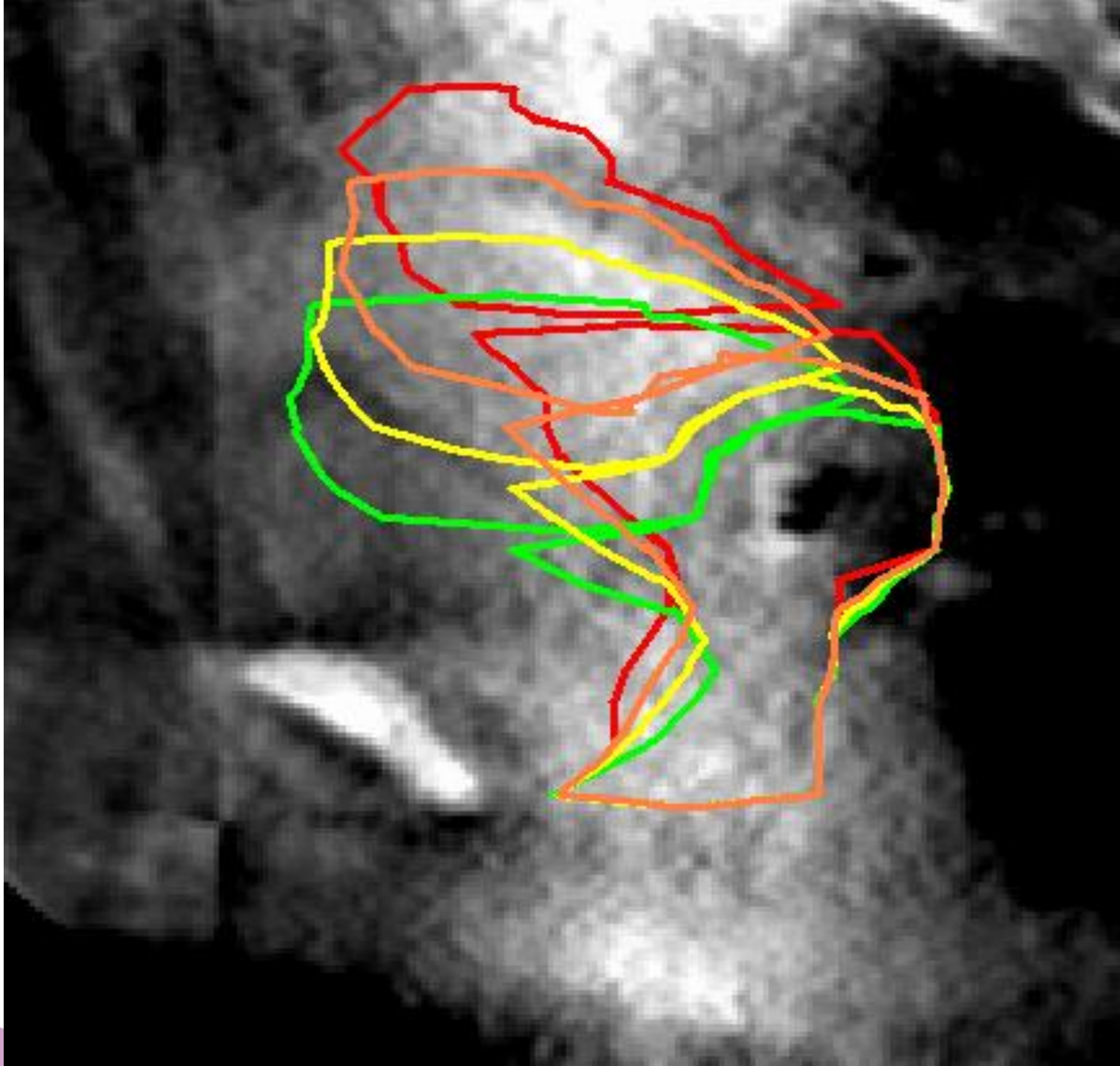






Question

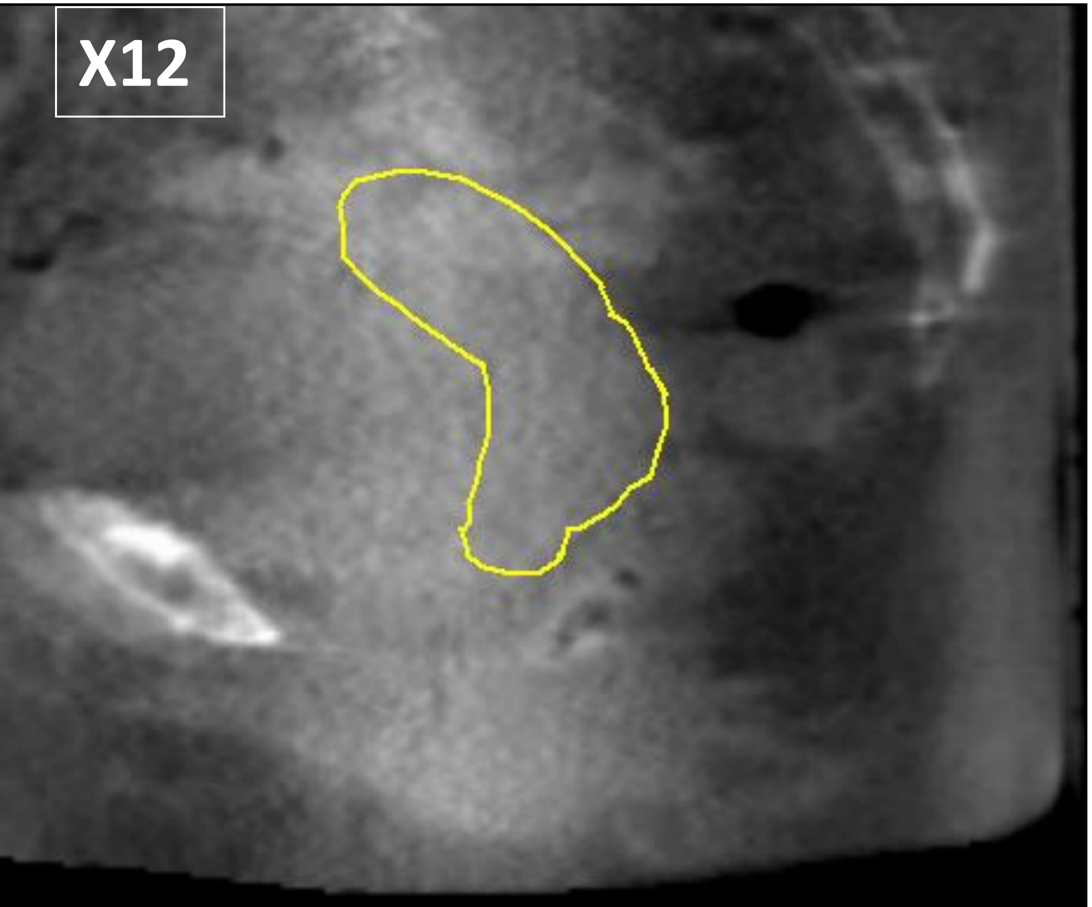
Is it possible to consistently select a best fitting CTV based on CBCT scans?

Observer study setup

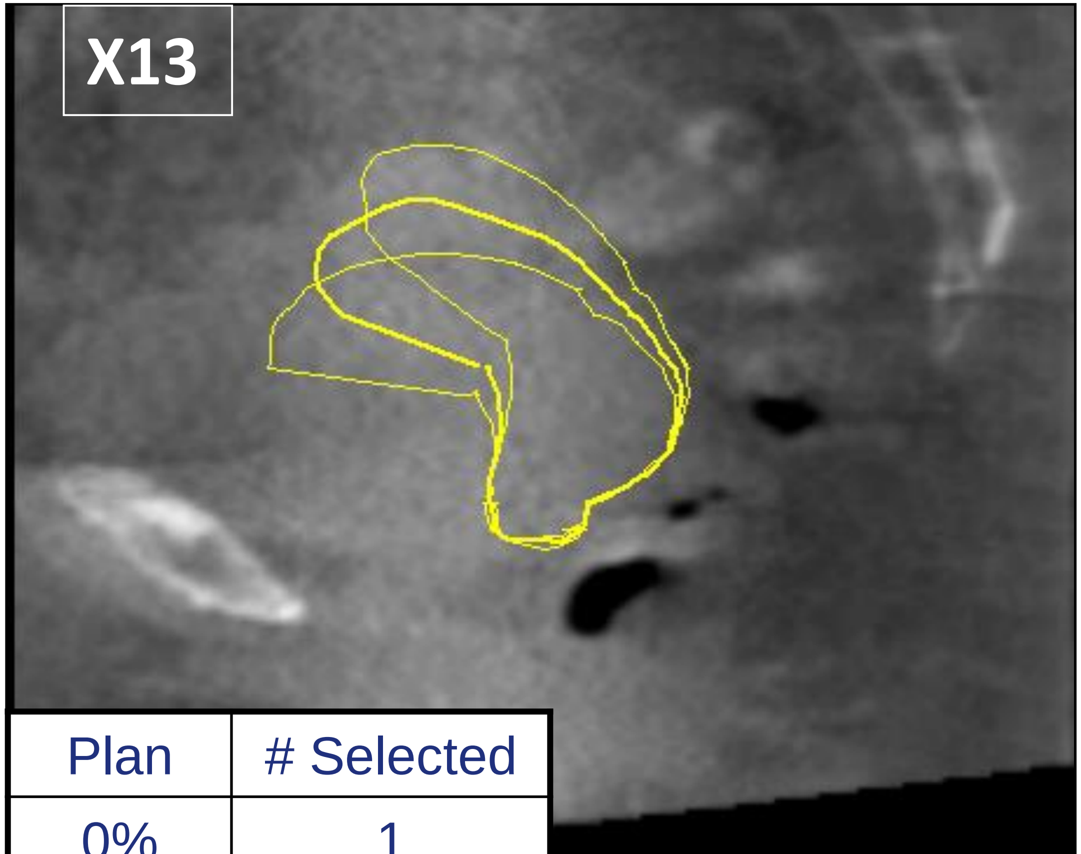
- 5 patients, 23 scans per patient (1 scan missing)
- Per patient 6 structures

  -20, 0, 33, 66, 100, 120%
- 9 observers (experienced RTTs)
- 2 sessions
- Workshop in between sessions to determine Gold Standard with observers: RTT, physicians and physicists

Patient 1



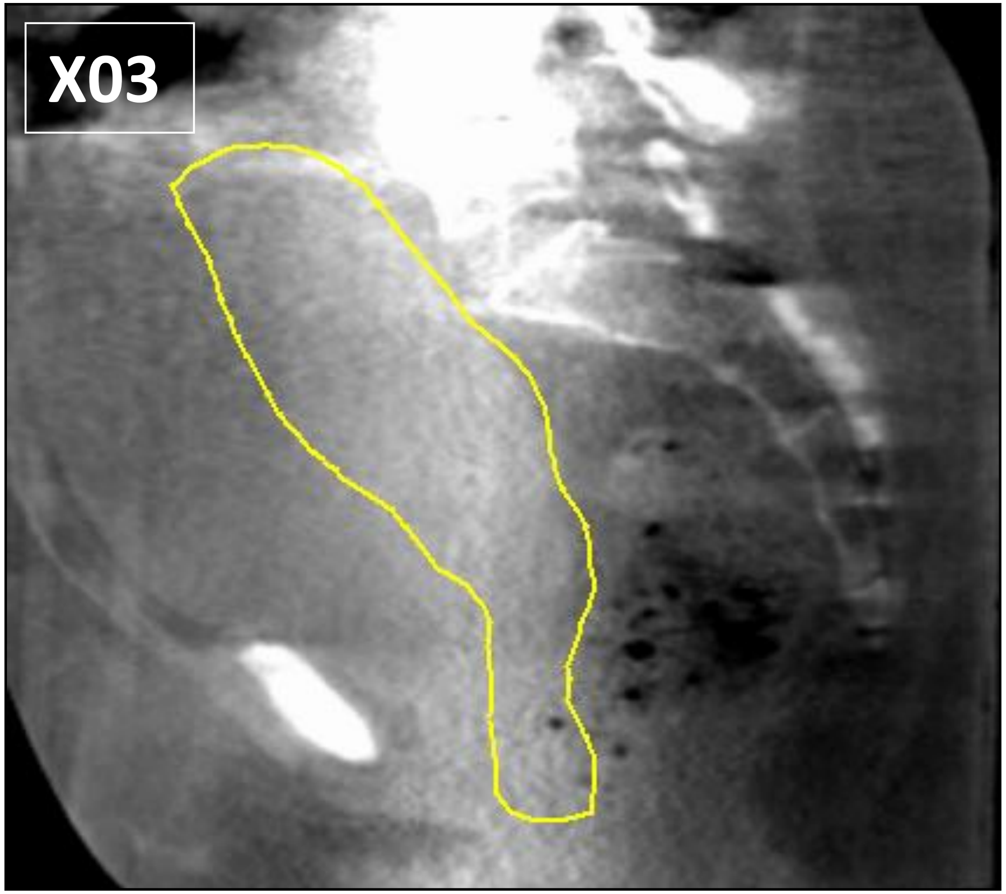
100% agreement



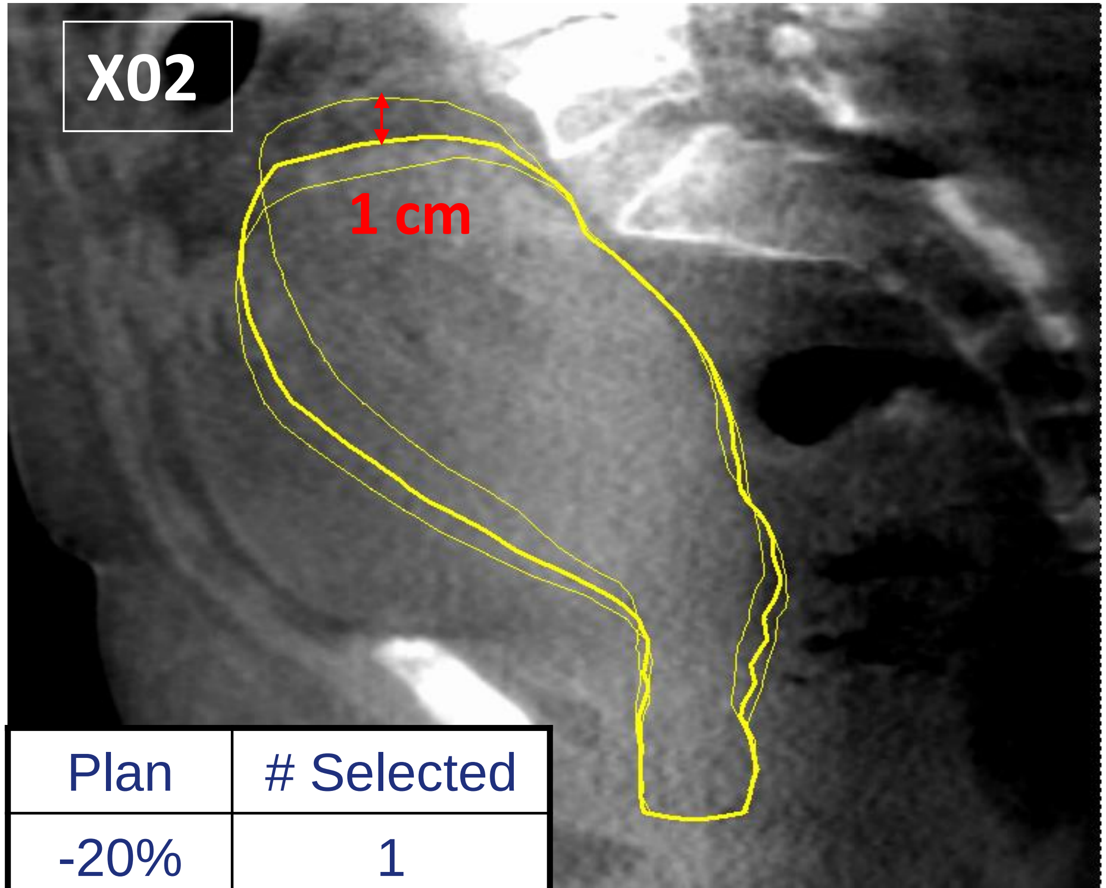
Plan	# Selected
0%	1
33%	4
66%	4

Golden star 3 %

Patient 2



100% agreement

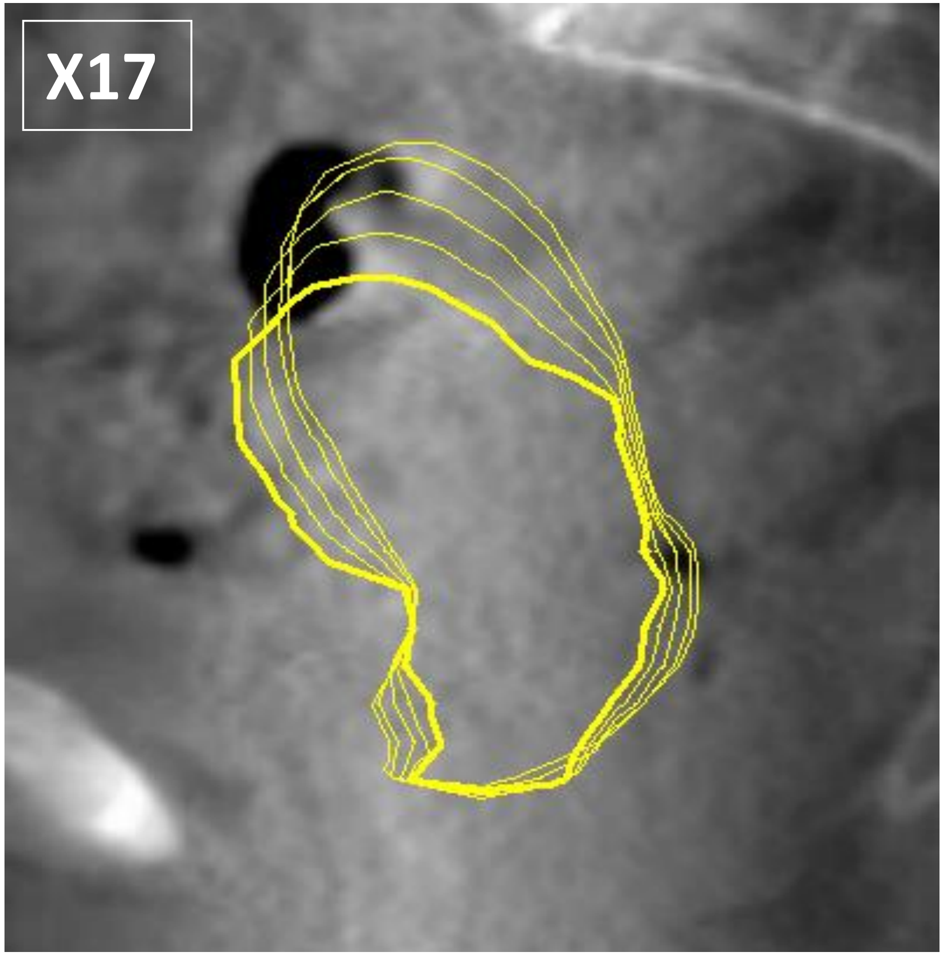


Plan	# Selected
-20%	1
0%	6
33%	2

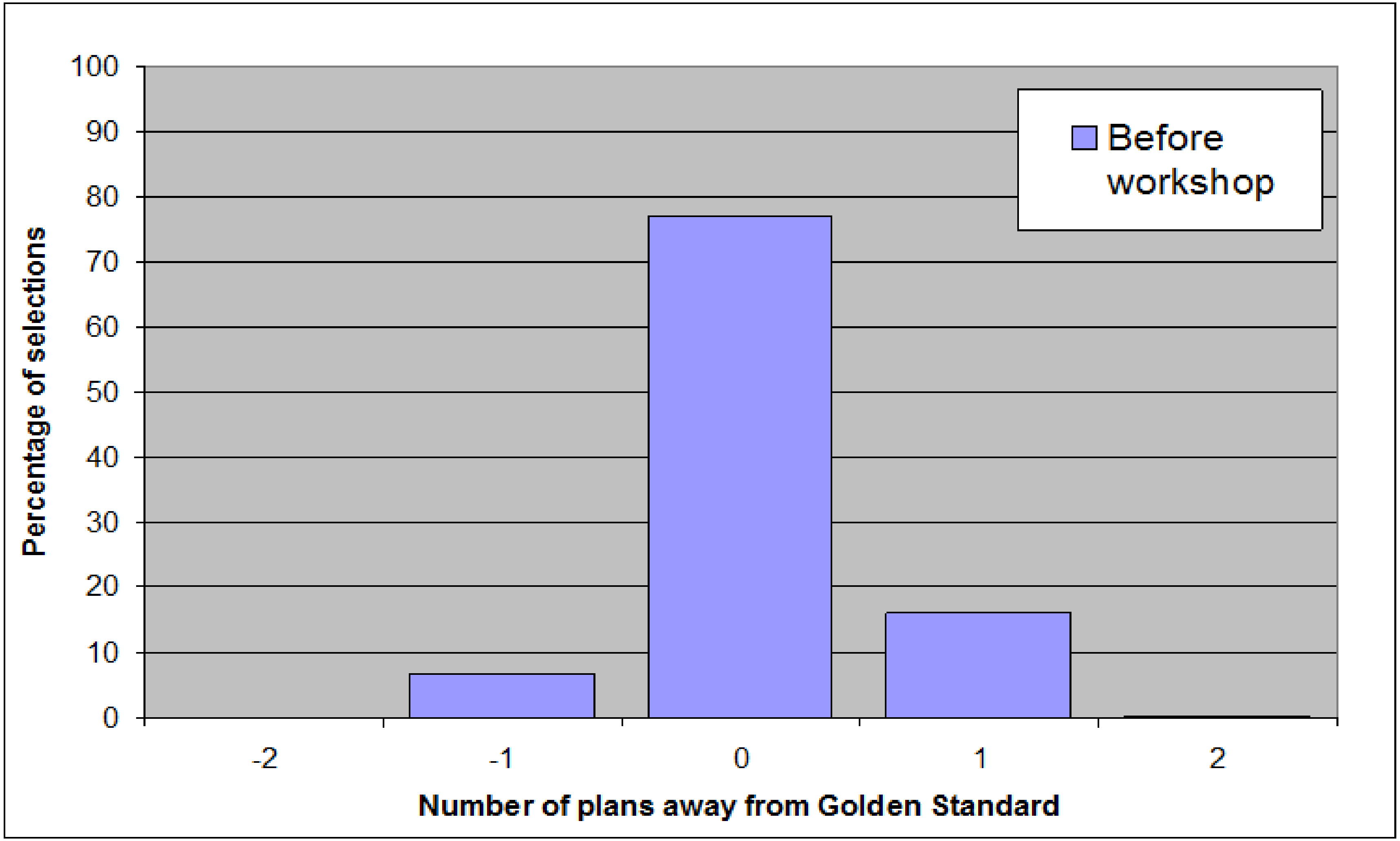
Golden star %

Patient 5

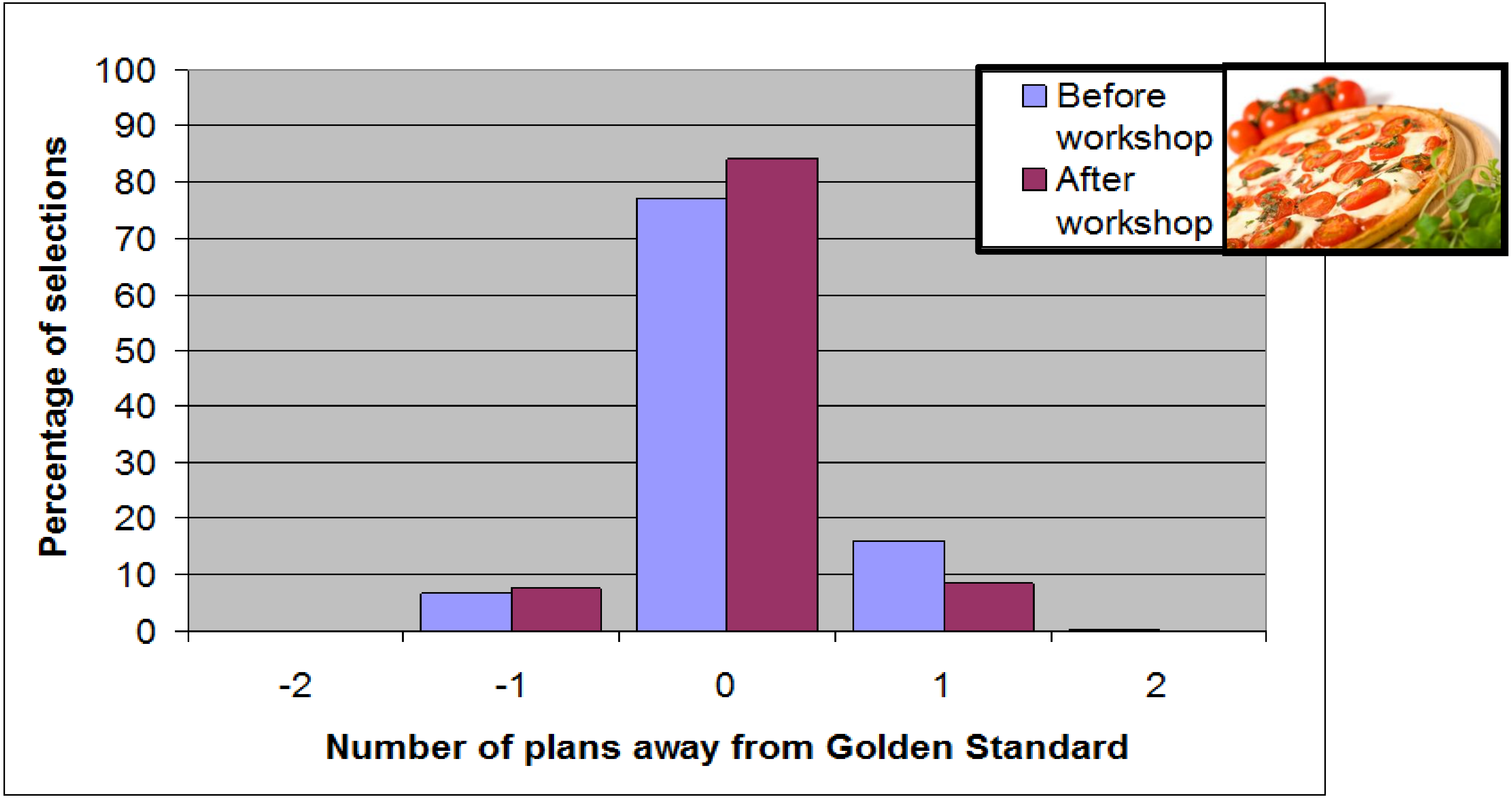
100% agreement



No agreement. Large anatomical change wrt planning CT



100
90
80
70
60
50
40
30
20
10
0
Percentage of selections
Before workshop
-2
-1
0
1
2
Number of plans away from Golden Standard


100
90
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70
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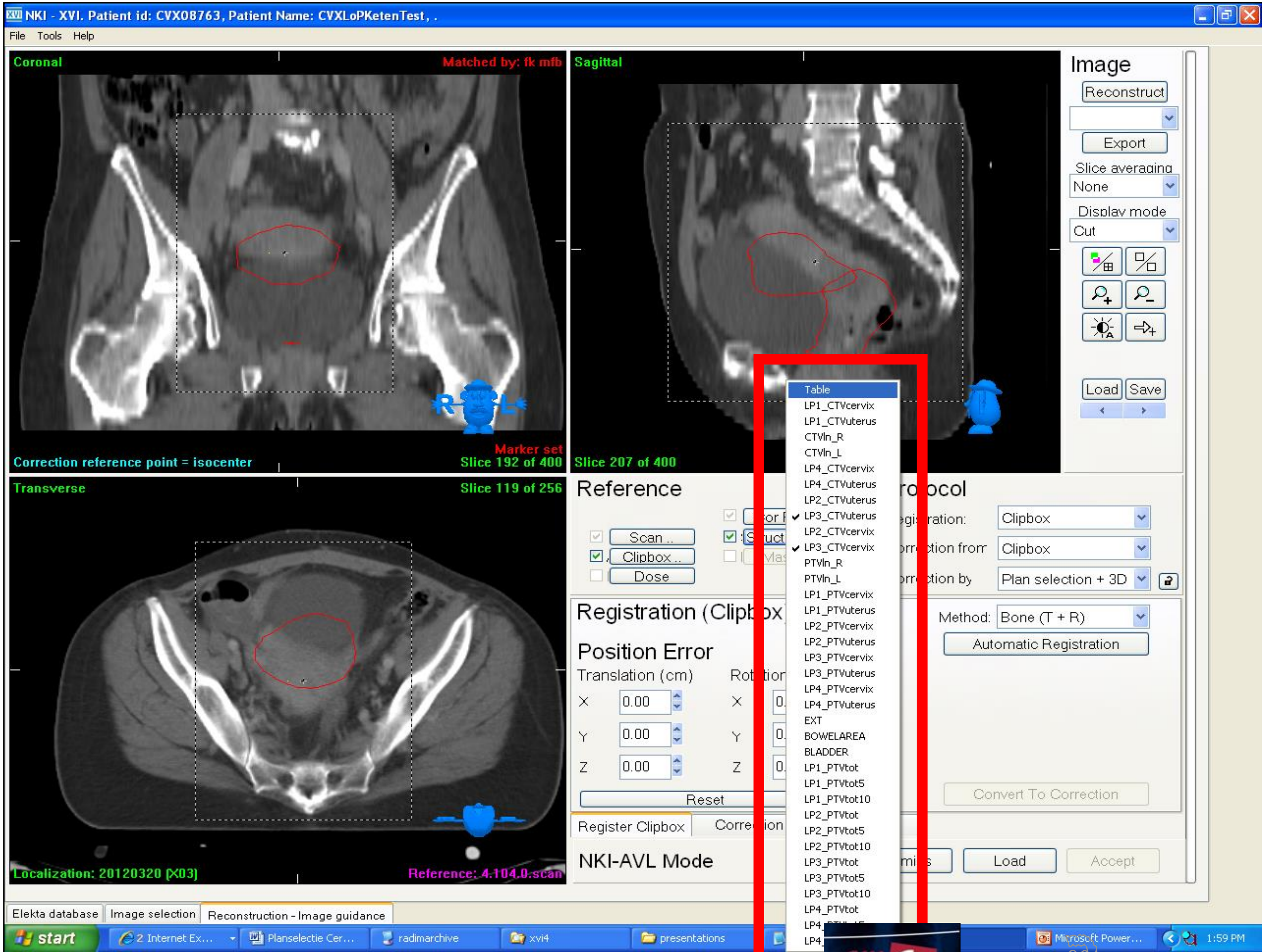
Percentage of selections
-2
-1
0
1
2
Number of plans away from Golden Standard
Before workshop
After workshop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Coronal
Matched by: fk mfb
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Correction reference point = isocenter
Slice 192 of 400
Sagittal
Slice 207 of 400
Transverse
Slice 119 of 256
Localization: 20120320 (X03)
Reference: 4.104.0.scan
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Slice averaging
None
Display mode
Cut
Load
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Reference
Scan ..
Clipbox ..
Dose
Table
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LP1_CTVuterus
CTVln_R
CTVln_L
LP4_CTVcervix
LP4_CTVuterus
LP2_CTVuterus
LP3_CTVuterus
LP2_CTVcervix
LP3_CTVcervix
PTVln_R
PTVln_L
LP1_PTVcervix
LP1_PTVuterus
LP2_PTVcervix
LP2_PTVuterus
LP3_PTVcervix
LP3_PTVuterus
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LP4_PTVuterus
EXT
BOWELAREA
BLADDER
LP1_PTVtot
LP1_PTVtot5
LP1_PTVtot10
LP2_PTVtot
LP2_PTVtot5
LP2_PTVtot10
LP3_PTVtot
LP3_PTVtot5
LP3_PTVtot10
LP4_PTVtot
Clipbox
Clipbox
Plan selection + 3D
Registration (Clipbox)
Method: Bone (T + R)
Automatic Registration
Position Error
Translation (cm)
X 0.00
Y 0.00
Z 0.00
Reset
Convert To Correction
Register Clipbox
NKI-AVL Mode
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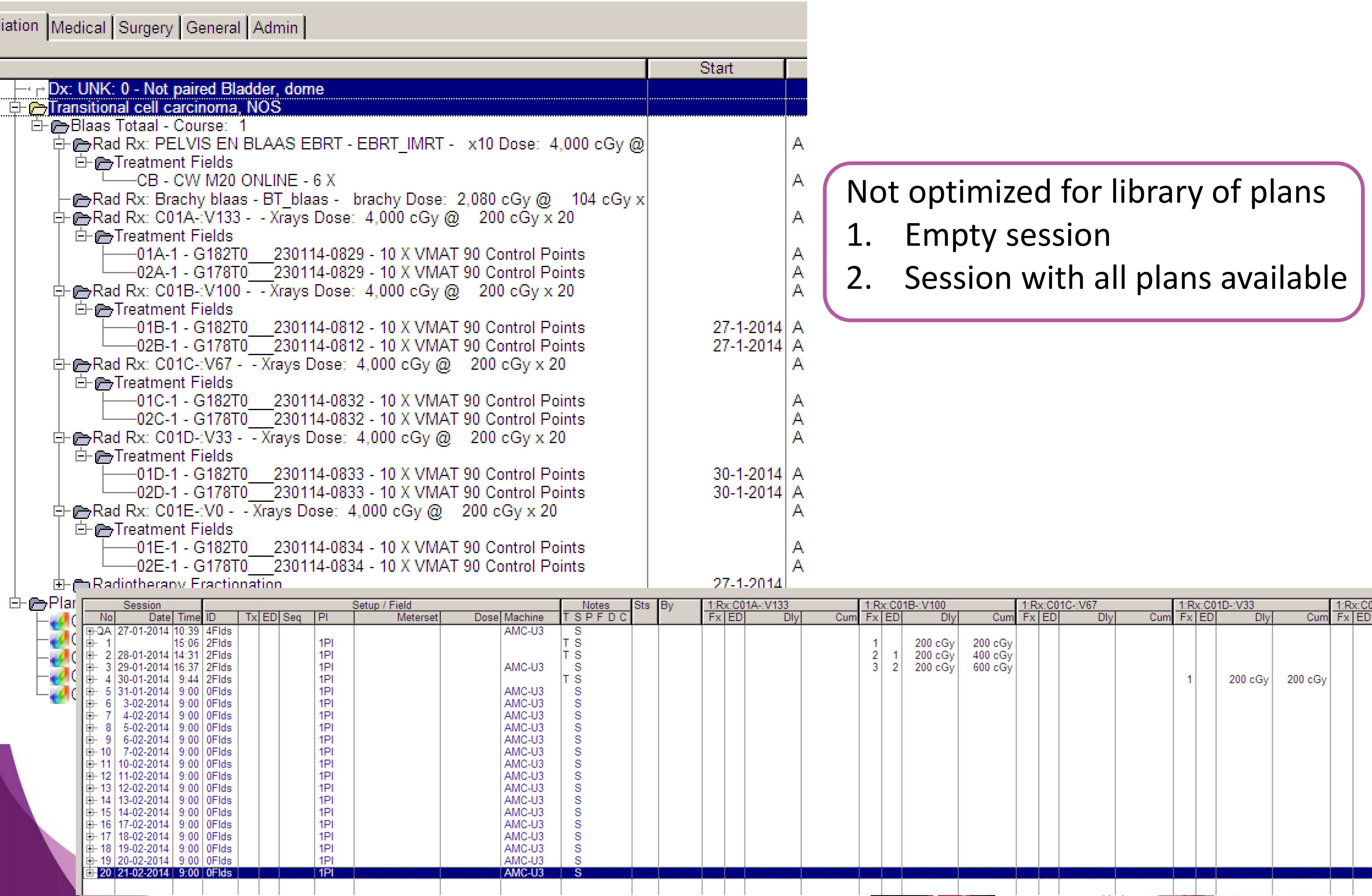
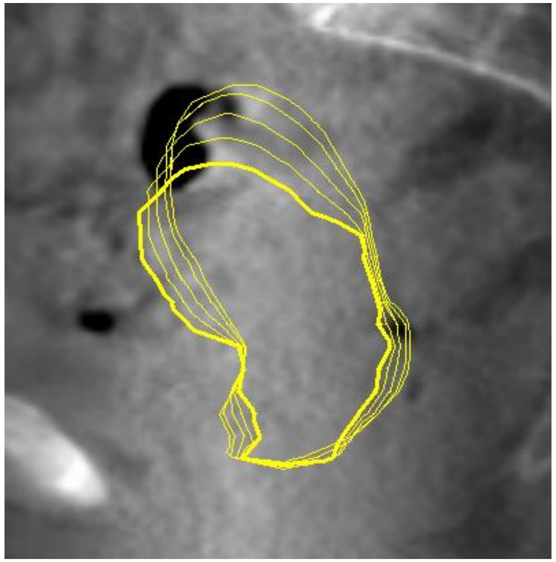


Not optimized for library of plans

1. Empty session
2. Session with all plans available



Not all anatomy change is due to bladder filling
~30% rectum filling

Anatomy change over course of treatment due to regression

ART - Cervix

Patiënt naam:	
Patiënt nummer:	8890230
Course:	1
Aantal plannen	3

Gegevens opslaan

Fractie	IGRT-laborant(en)	Datum	Plan	Opmerkingen
1		10 juni 2015	66-100%	
2		11 juni 2015	66-100%	
3		12 juni 2015	66-100%	
4		15 juni 2015	33-66%	krap
5		16 juni 2015	66-100%	
6		17 juni 2015	33-66%	buiten PTV
7		18 juni 2015	33-66%	op PTV
8		19 juni 2015	66-100%	krap
9		22 juni 2015	66-100%	op PTV
10	mka/jvr	23 juni 2015	33-66%	op PTV, bekkenkanteling, klieren gecovered
11	rjg/kgl/jvr	24 juni 2015	66-100%	krap binnen PTV craniaal
12	dwl mos ahk	25 juni 2015	66-100%	craniaal buiten PTV
13				
14				
15				
16				
17				
18				
19				
20				

Week	Eval.	Door	Opmerkingen
1	☑	rjg	
2	☑	rjg	iom LSS en EPQ volume vergroting akkoord
3	☐		
4	☐		

Per 13 april 2015 zijn we begonnen met planselectie voor cervixpatiënten: ART cervix. Zie voor complete werkinstructie Kwadraet 'Cervix ART'. Iedere dag moet er iemand van de IGART-groep aanwezig zijn bij planselectie.

Om inzichtelijk te maken voor het toestel welke plannen er worden gekozen graag bovenstaande tabel invullen. Als er vroeg in de behandeling 3 keer achter elkaar voor plan 0% - 33% wordt gekozen, graag in gesprek gaan met de patiënt of hierin verbetering kan worden aangebracht door meer te drinken of eerder uit te plassen. Dit graag noteren bij 'opmerkingen'.

NB: In tegenstelling tot ART-Blaas mag er bij ART-Cervix NOOIT geweakt worden!

Vragen en/of opmerkingen horen wij graag. Alvast dank.

Jorrit (62594)
Rianne (66857)

Sessies | Bestralingsoverzicht

CT scans full and empty bladder

1 full bladder CT

1 empty bladder CT

Judgement call of the RTT at CT simulation whether bladder is “full”

If not, patient needs to wait extra time and rescan.

			CBCT	
			>1.0 cm	<1.0 cm
		15 pts	12	3
pre-RT	>1.0 cm	7	**6**	**1**
	<1.0 cm	8	**6**	**2**

library possible

library beneficial

tip uterus CC motion

CT scans full and empty bladder

- RTT registers CT scans and determines movement:
  - <1 cm no planselection
  - Between 1 en 2 cm: 2 plans
  - 2 cm < 4 plans
- Physician delineates target volumes on full and empty bladder CT scan
- Physicist generates intermediate structures and PTV margins
- RTT delineates OAR and generate treatment plan with VMAT on full bladder CT scan, scripting generates the intermediate plans

Planselection workflow at Linac

1. Registration bones
2. Selection of plan
3. Marker check
   - Trained RTTs

Demo database for training of RTTs

Workshop

Extra, not commercial @AvL/NKI

Big Brother software checks consistency of selected plan in XVI and Mosaiq plan!

Big Brother software prohibits delivery of more than 1 plan!

Evaluation / safety procedures

1 x week by IGRT-group (expert RTT)

- Selection as discussed in workshop?
- Is uterus moving as predicted on full/empty bladder CT scan (mover/non-mover)?
  - Including those patients that had no planselection due to no movement at full/empty bladder CT scans
- Are the anatomy changes still valid? Think regression

Documents…

- *Patient letters for bladder instructions*
- RTT instructions for full bladders
- MRI of Pet CT in full bladder? CT scan full bladder obsolete?
- Delineation instructions and interpolations
- *Mosaiq*
- *Treatment Planning scripting*
- *IGRT*

Discussion

Cervix planselection: a RTTs job?

(Almost) every step of the way

Summary

- Development and implementation of ART (library of plans) is
  - Departement specific
  - Protocol specific
- Development and implementation of ART is a multi-diciplinairy effort
- Because of the multi-disciplinairy character one needs to be creative, like pizza meetings

- Training is key. Invest in training as it will improve quality, but also raises awareness as to the importance of IGRT/ART!

Special thanks to

AvL/NKI

Folkert Koetsveld

Simon van Kranen

Peter Remeijer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L
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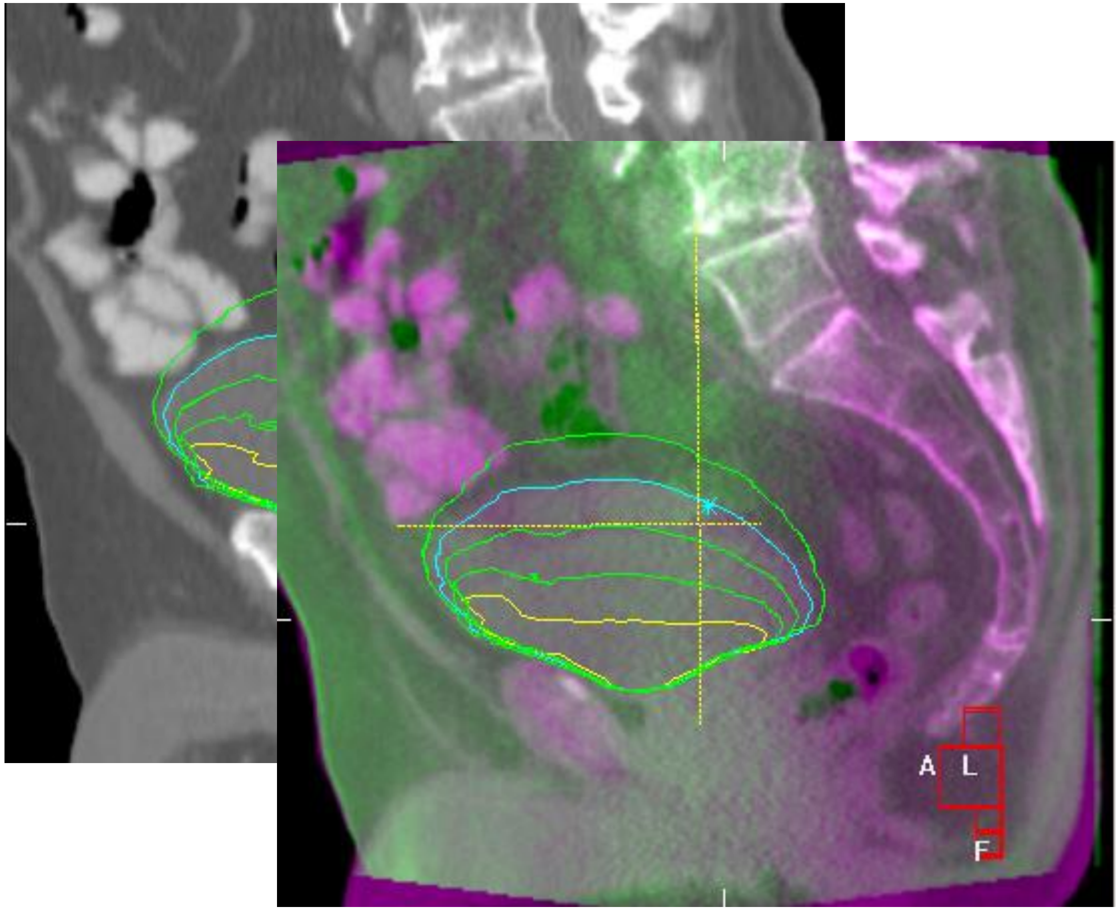

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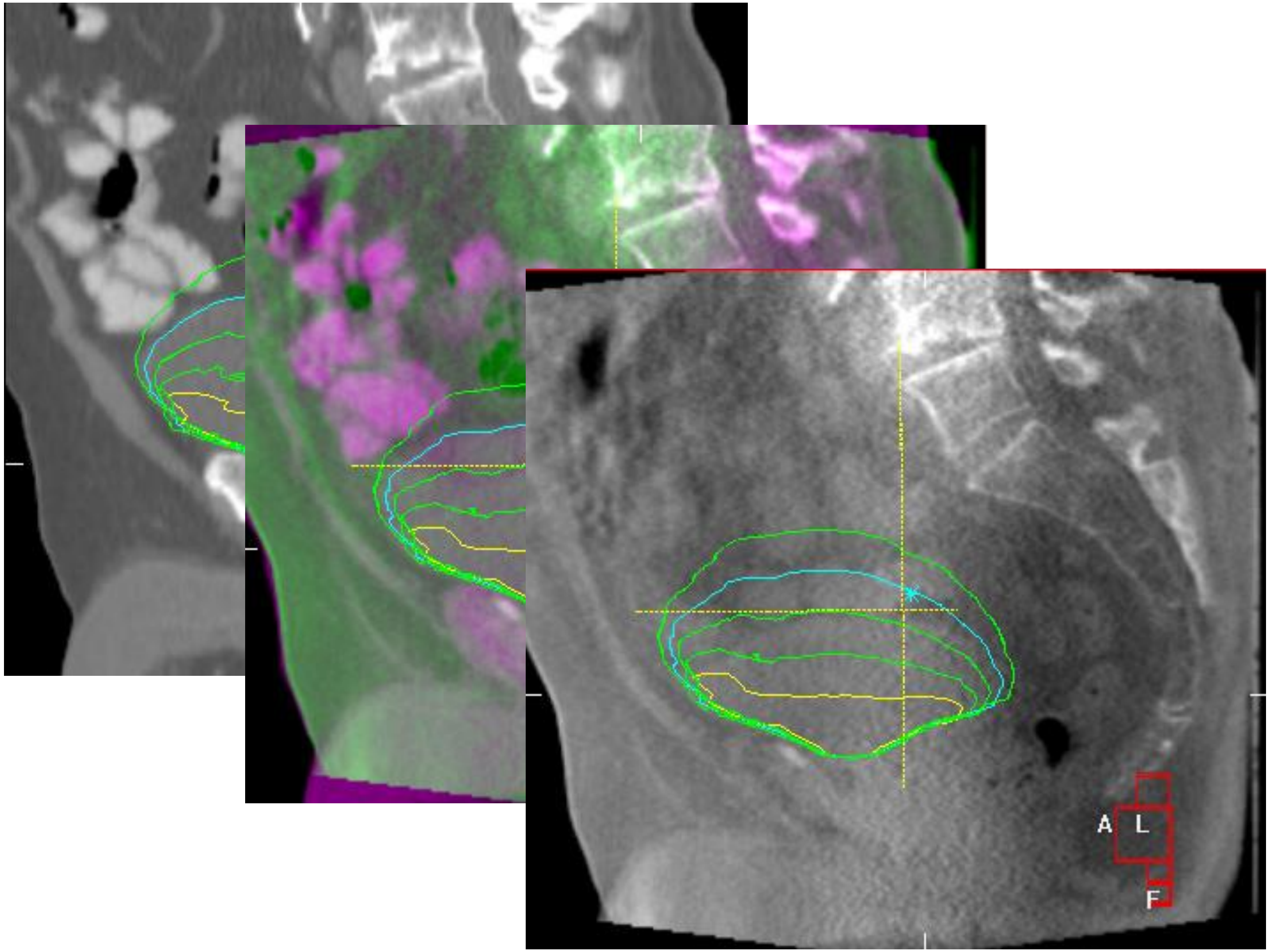
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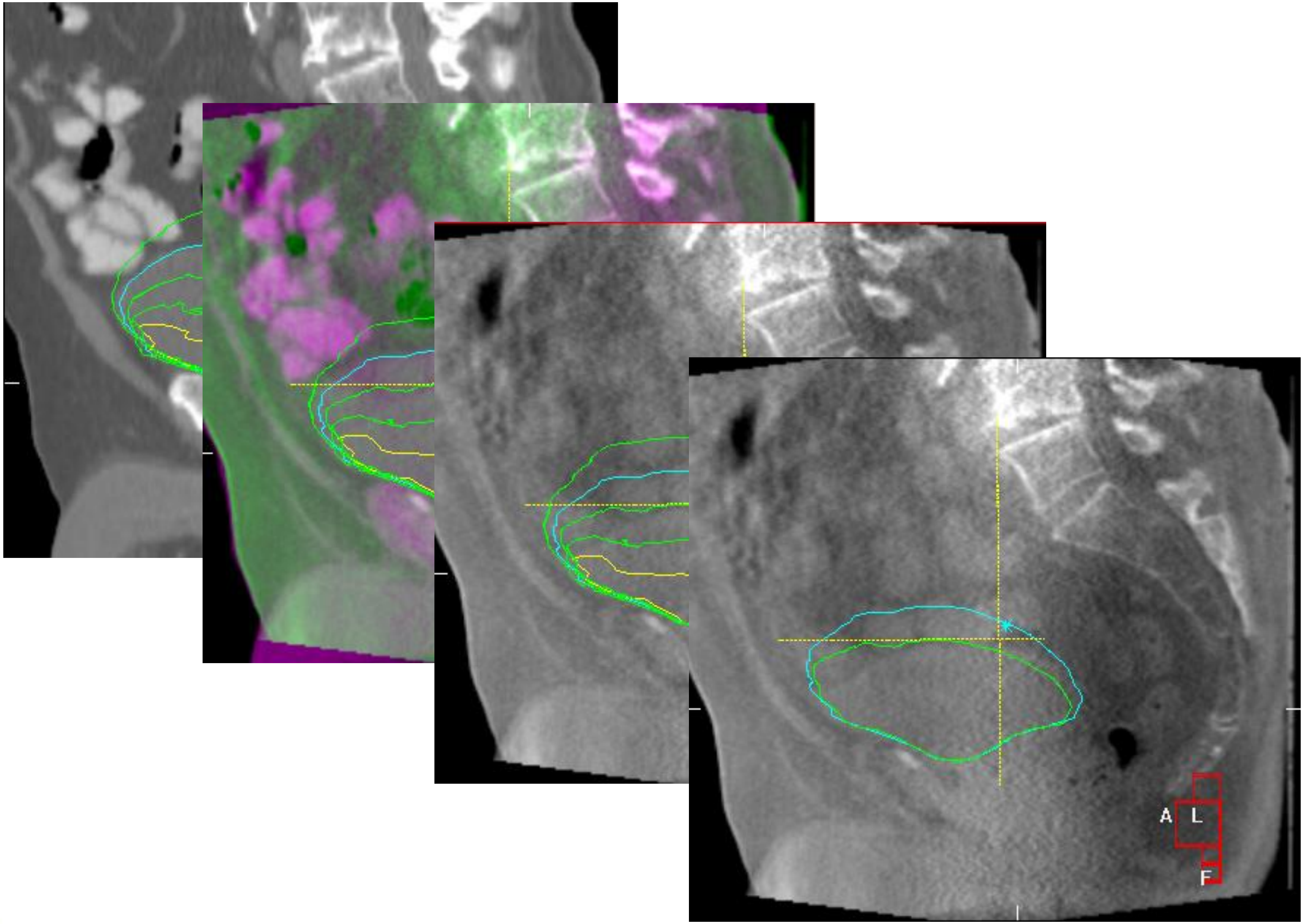
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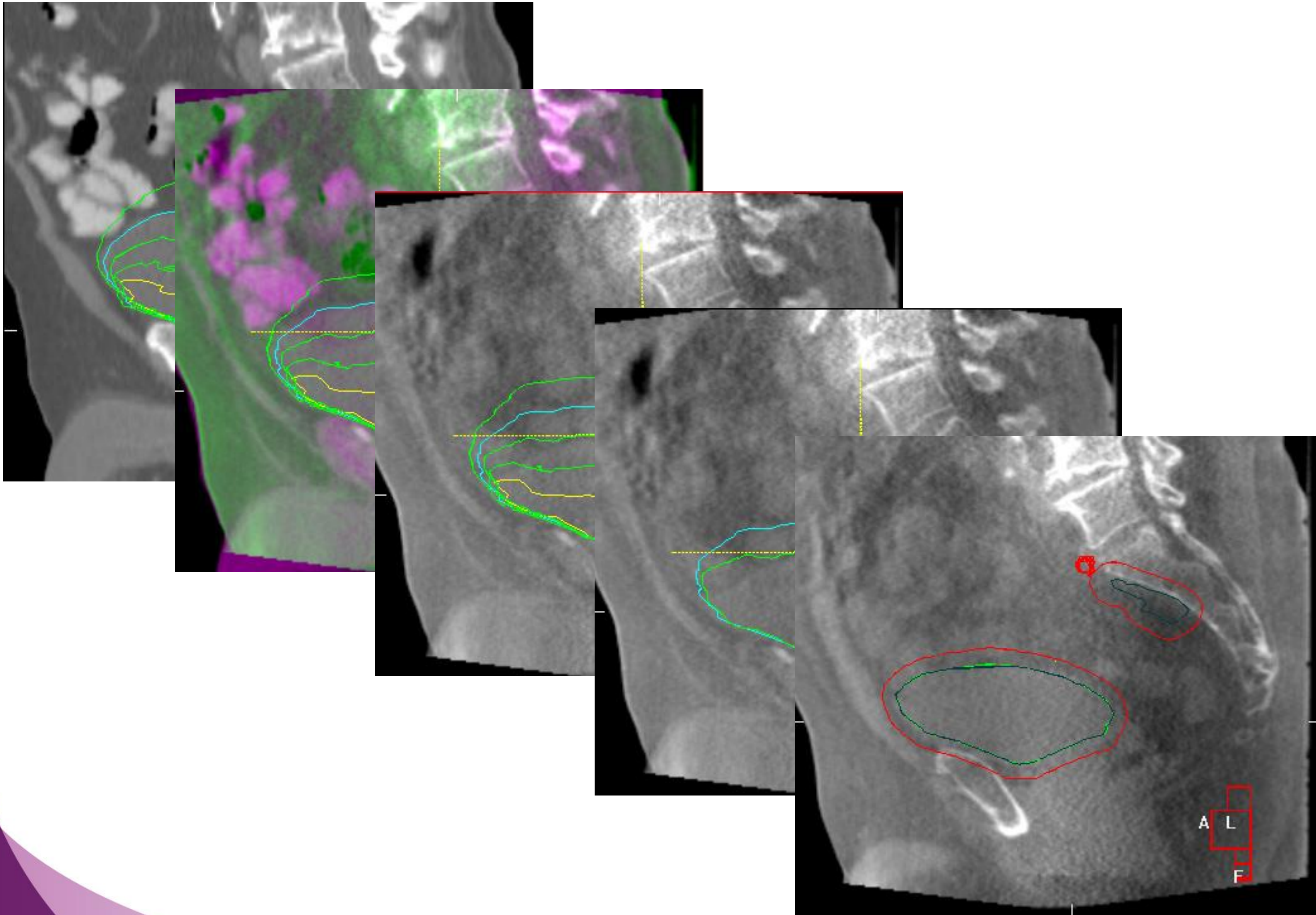
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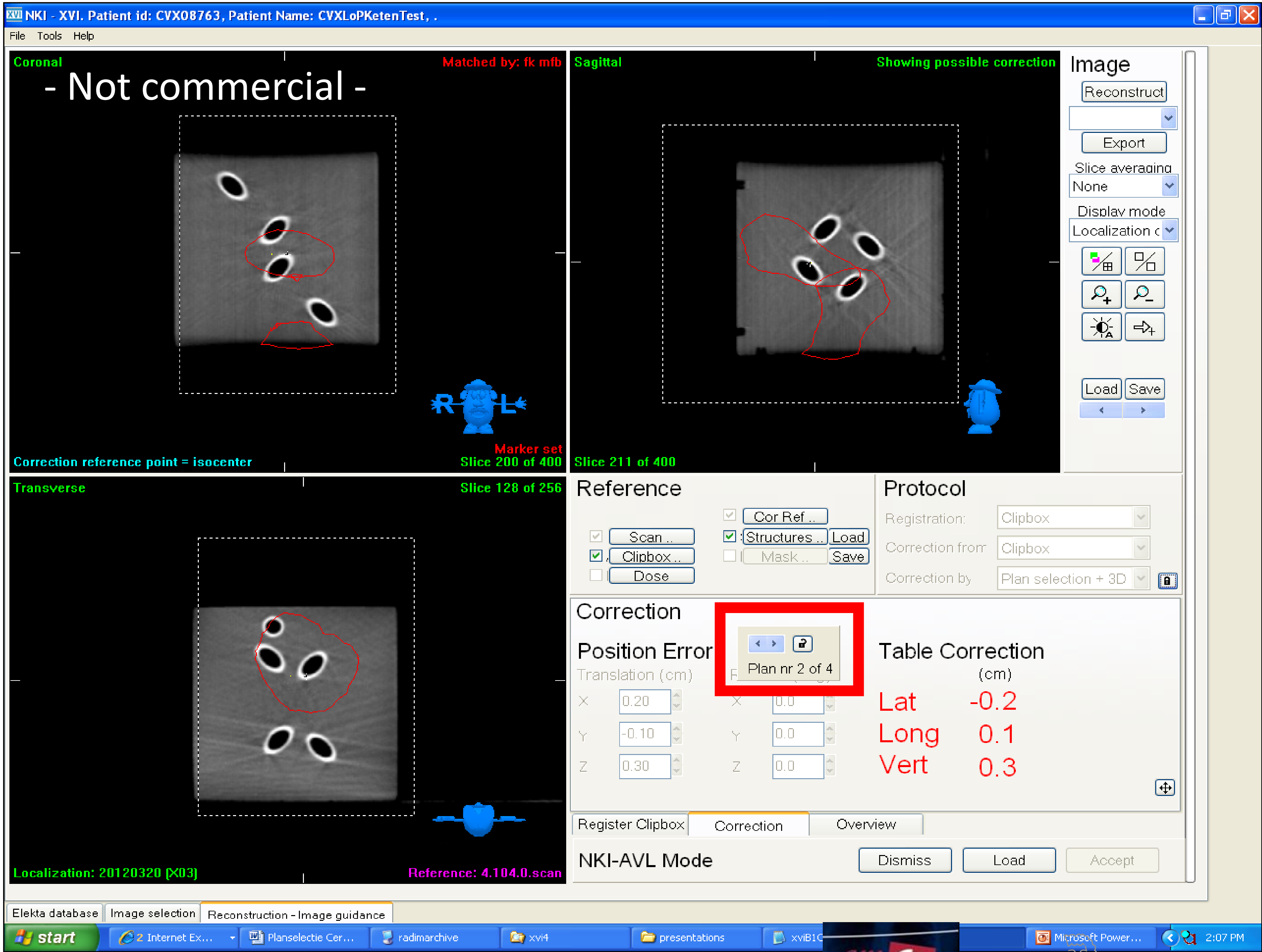
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Sagittal
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Slice 211 of 400
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Registration: Clipbox
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Correction
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Translation (cm)
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Y -0.10
Z 0.30
X 0.0
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Plan nr 2 of 4
Table Correction
(cm)
Lat -0.2
Long 0.1
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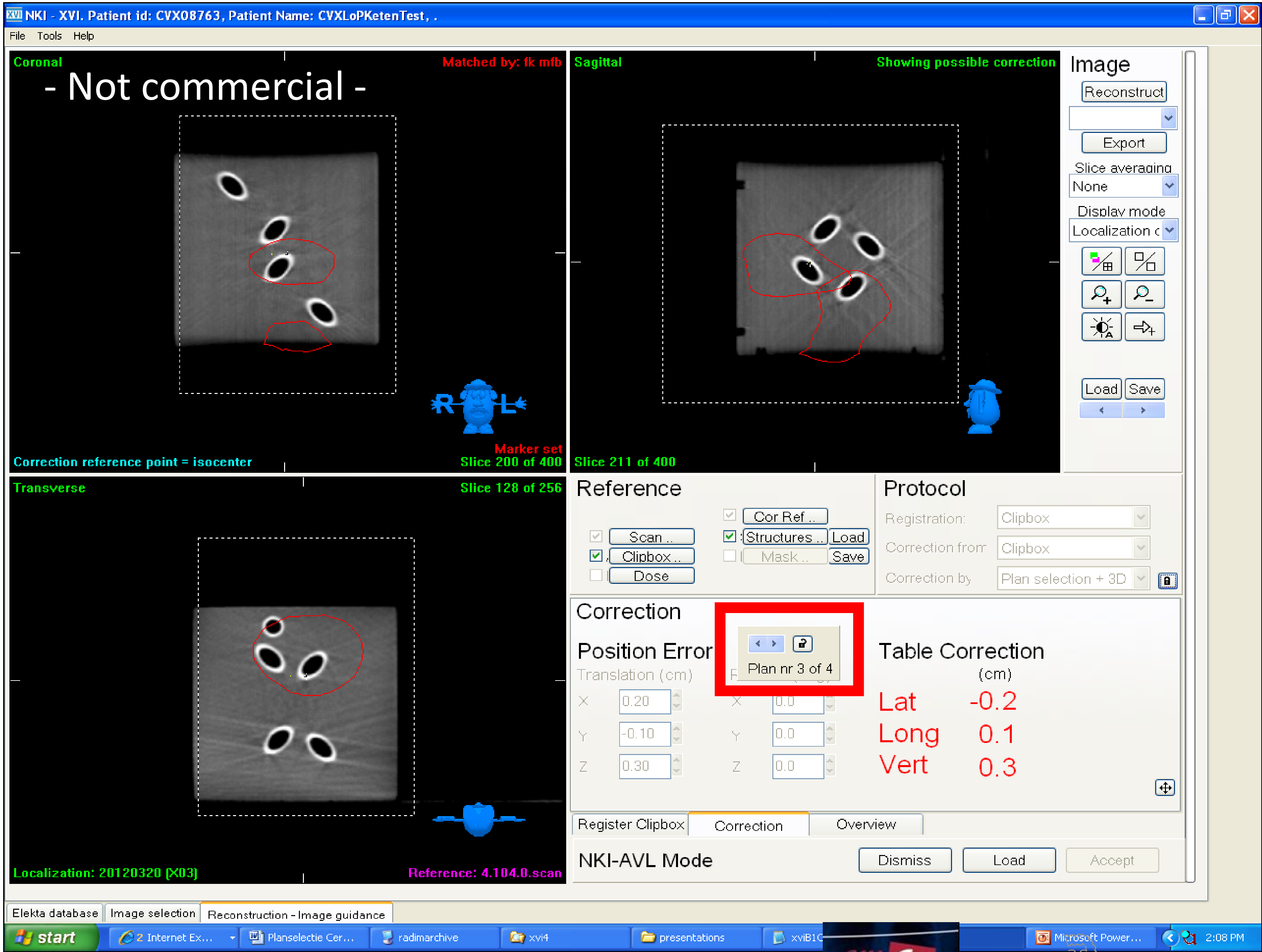
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Showing possible correction
Slice 211 of 400
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Reconstruct
Export
Slice averaging
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Localization c
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Localization: 20120320 (X03)
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Protocol
Registration: Clipbox
Correction from Clipbox
Correction by Plan selection + 3D
Correction
Position Error
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Y -0.10
Z 0.30
X 0.0
Y 0.0
Z 0.0
Plan nr 3 of 4
Table Correction
(cm)
Lat -0.2
Long 0.1
Vert 0.3
Register Clipbox
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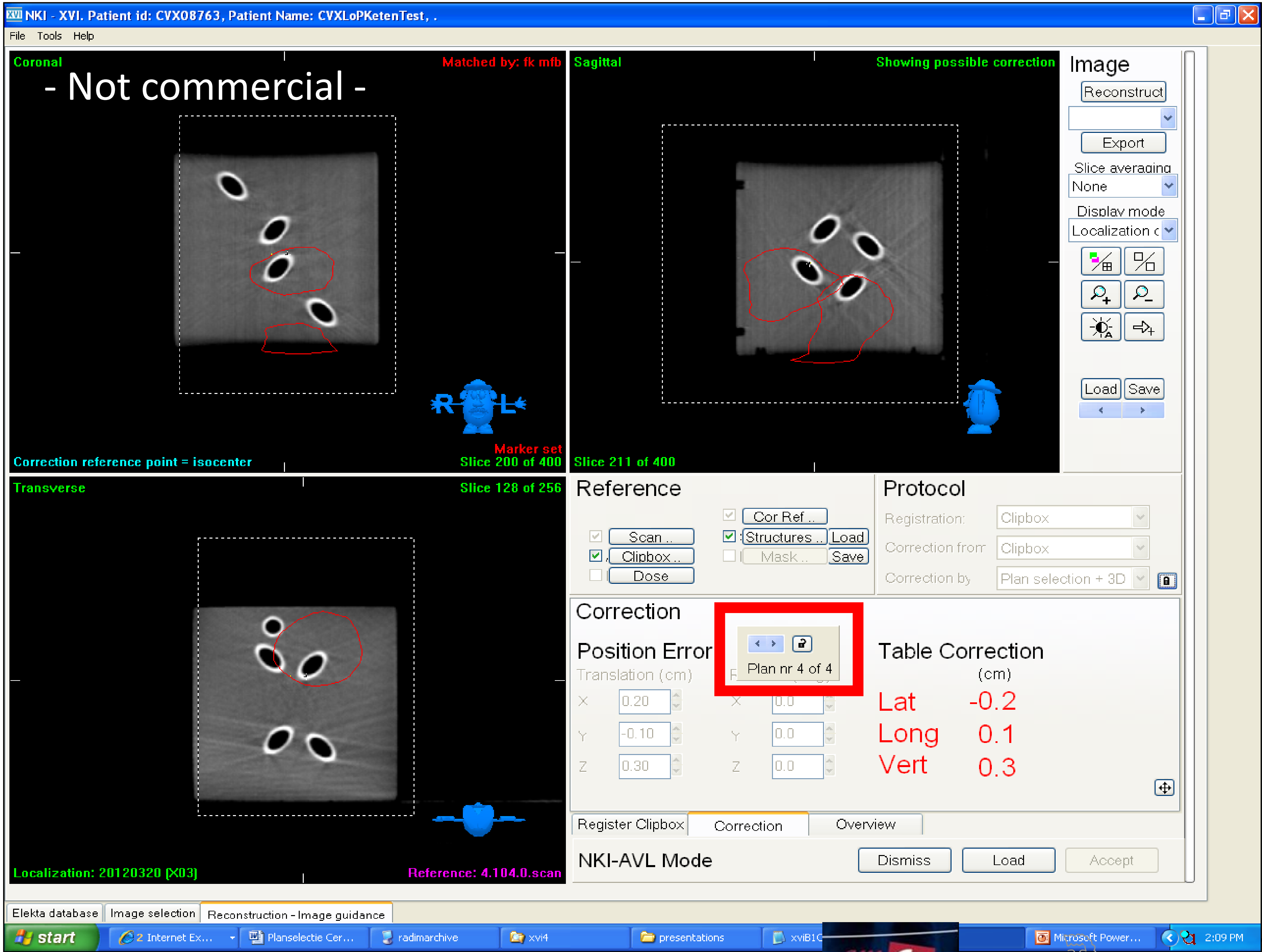

NKI-AVL

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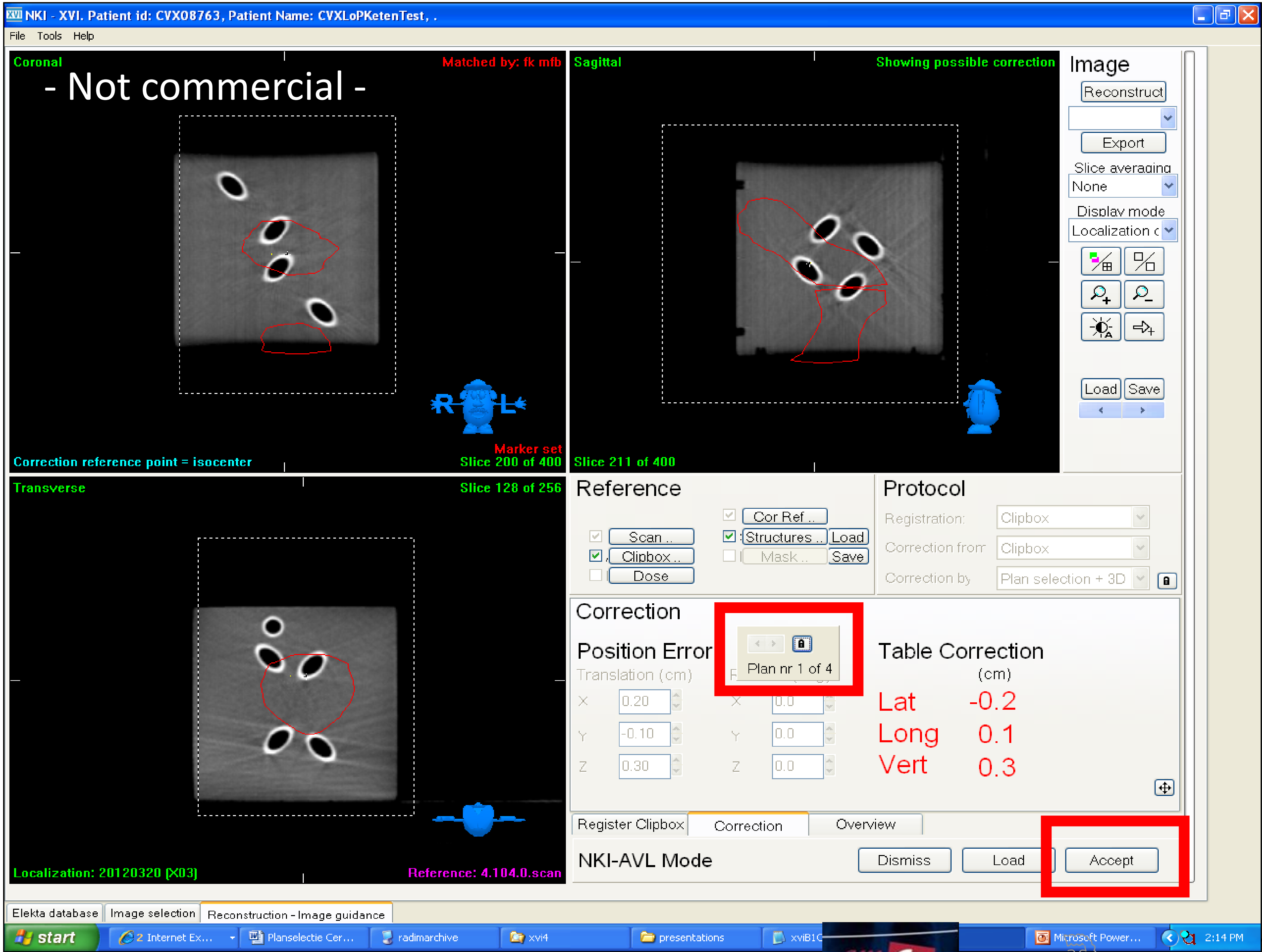
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Reference
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Clipbox
Correction from
Clipbox
Correction by
Plan selection + 3D
Correction
Position Error
Translation (cm)
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Y
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Z
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X
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Y
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Z
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Plan nr 1 of 4
Table Correction
(cm)
Lat -0.2
Long 0.1
Vert 0.3
Register Clipbox
Correction
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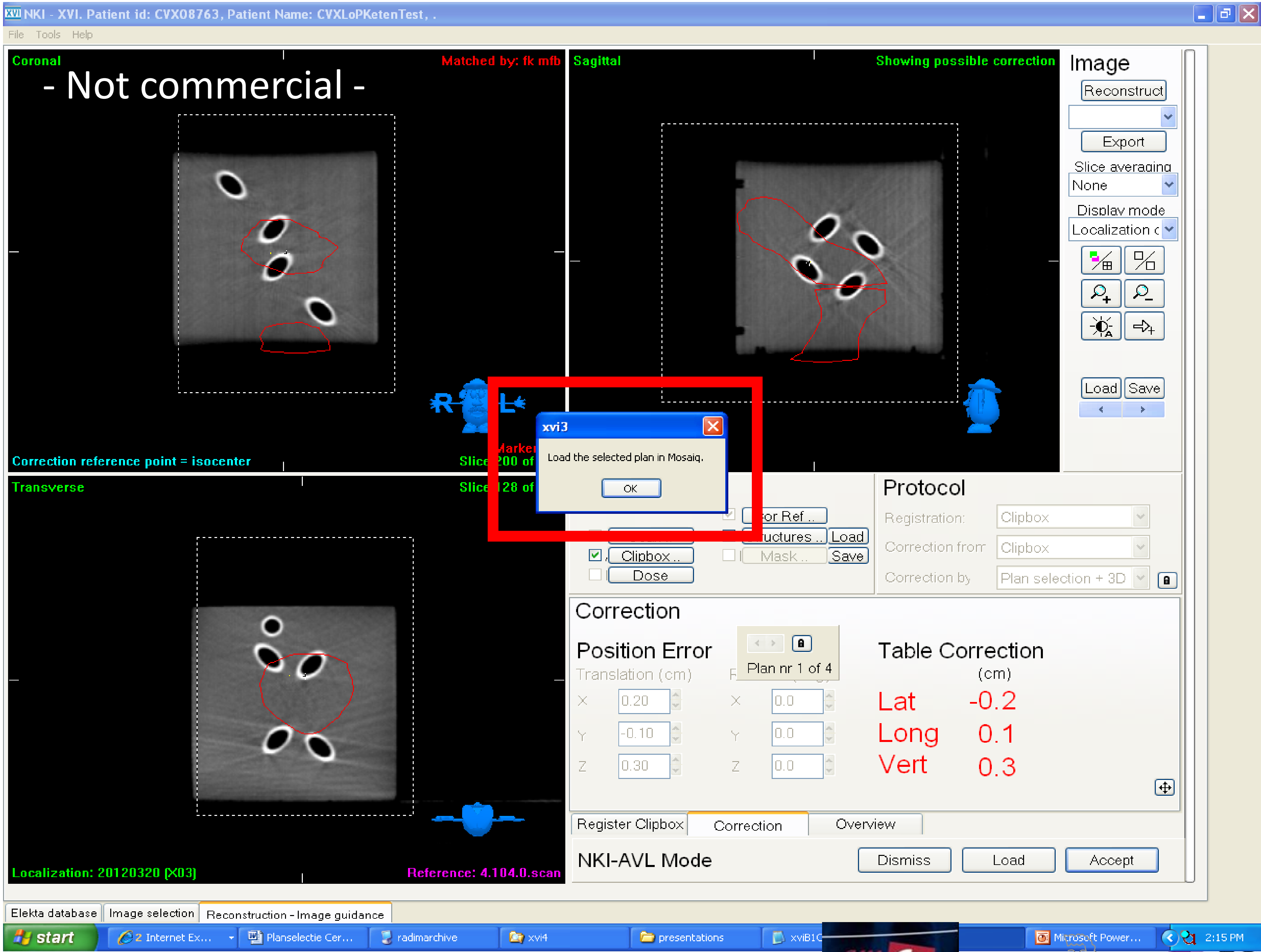
NKI - XVI. Patient id: CVX08763, Patient Name: CVXLoPKetenTest, .
File Tools Help
Coronal
Matched by: fk mfb
- Not commercial -
Sagittal
Showing possible correction
Image
Reconstruct
Export
Slice averaging
None
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Load Save
xvi3
Load the selected plan in Mosaiq.
OK
Correction reference point = isocenter
Transverse
Protocol
Registration: Clipbox
Correction from Clipbox
Correction by Plan selection + 3D
Clipbox ..
Dose
Mask ..
Load
Save
Correction
Position Error
Translation (cm)
Plan nr 1 of 4
Table Correction
(cm)
Lat -0.2
Long 0.1
Vert 0.3
X 0.20
Y -0.10
Z 0.30
Localization: 20120320 (X03)
Reference: 4.104.0.scan
Register Clipbox
Correction
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NKI-AVL Mode
Dismiss
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Accept
Elekta database
Image selection
Reconstruction - Image guidance
start
2:15 PM

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Case reports: **Prostate**
a physicist's perspective

Mirjana Josipovic

Dept. of Oncology, Rigshospitalet
& Niels Bohr Institute, University of Copenhagen
Denmark

Advanced skills in modern radiotherapy
June 2017

Imaging for prostate RT planning

Imaging immobilised patient in the treatment position

- CT scan
- MR scan

- Marker implantation into prostate gland

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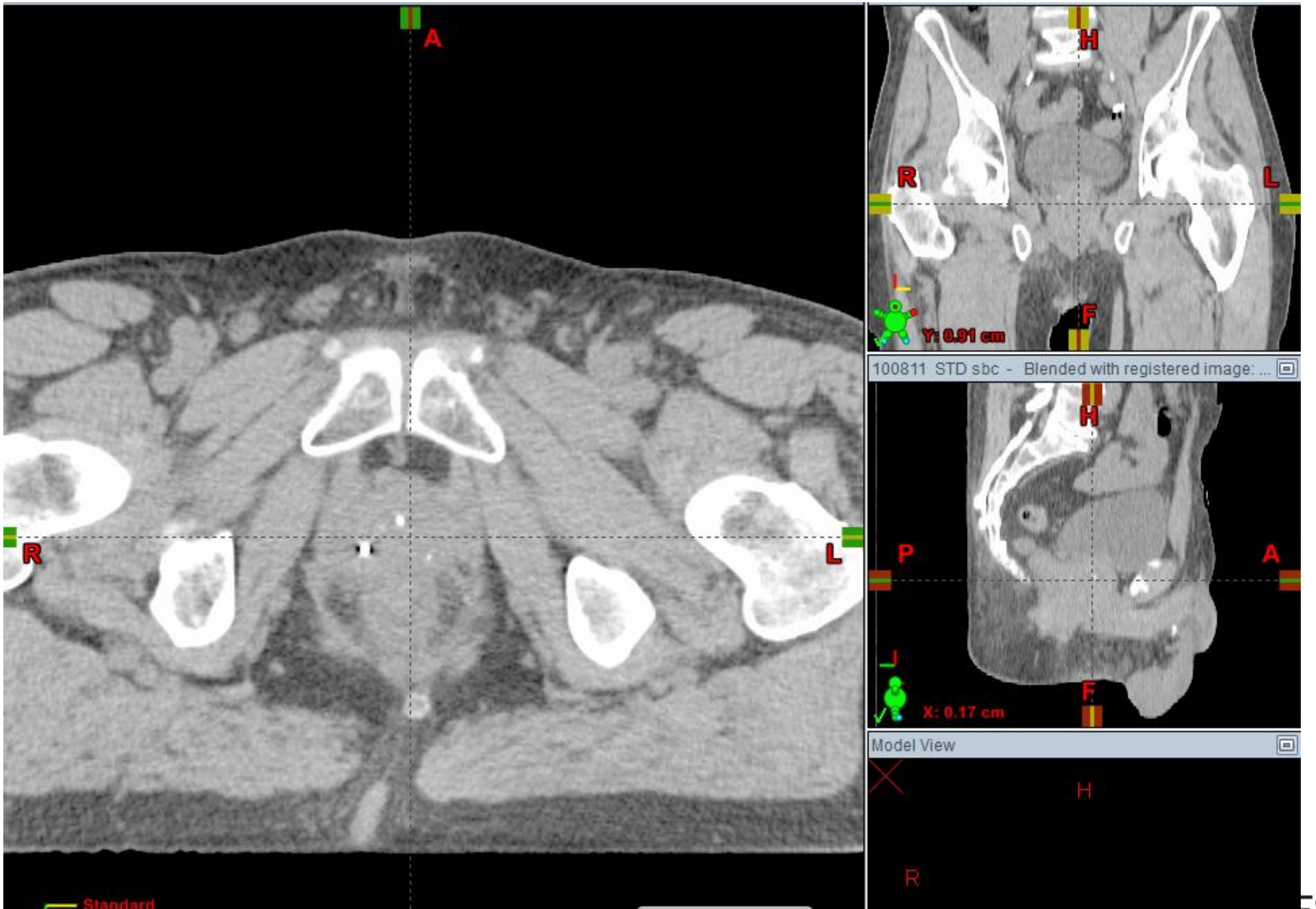
CT MR fusion



A
R
L
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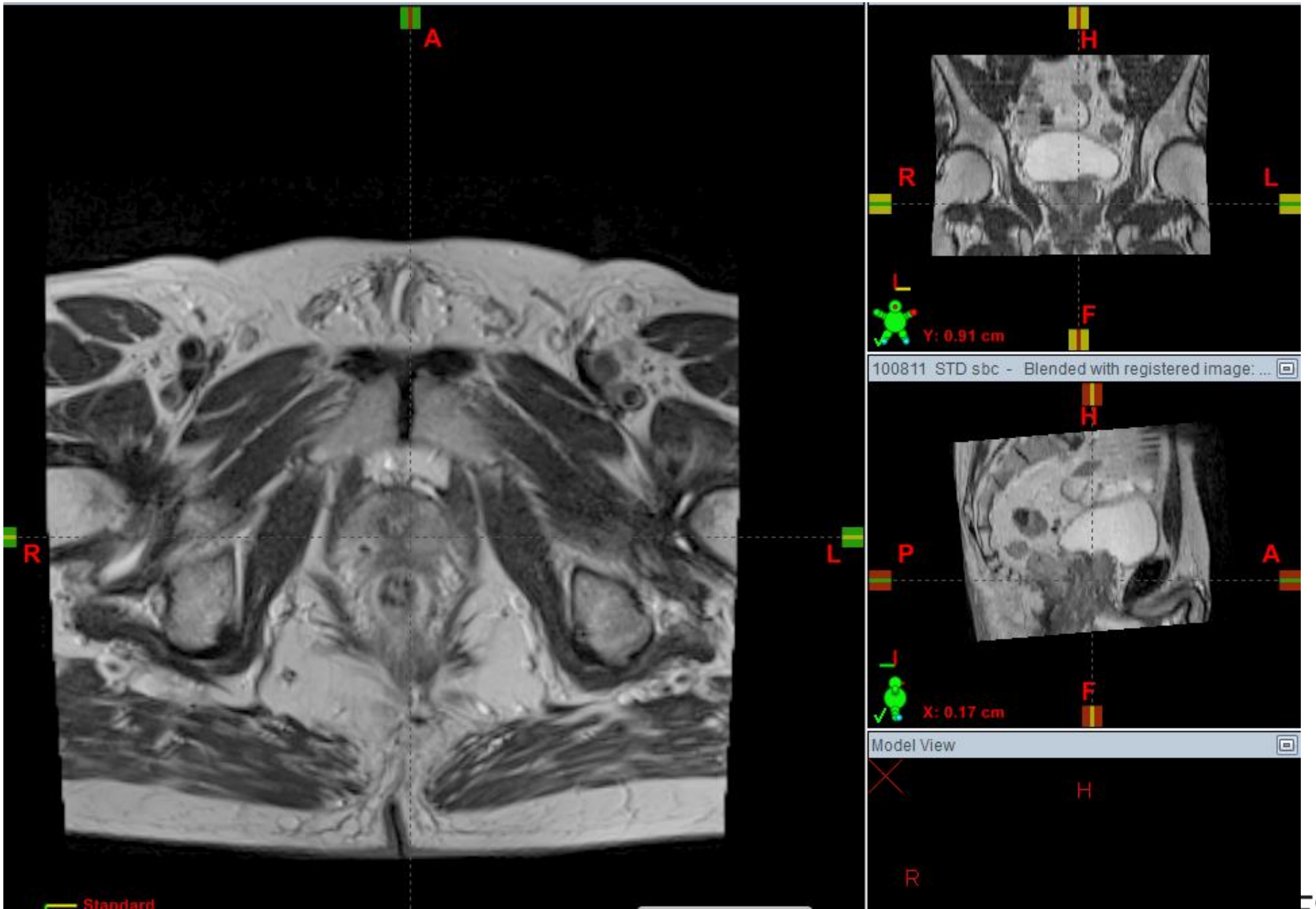
F
Y: 0.91 cm
100811 STD sbc - Blended with registered image: ...
P
X: 0.17 cm
Model View

CT MR fusion



A
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Y: 0.91 cm
100811 STD sbc - Blended with registered image: ...
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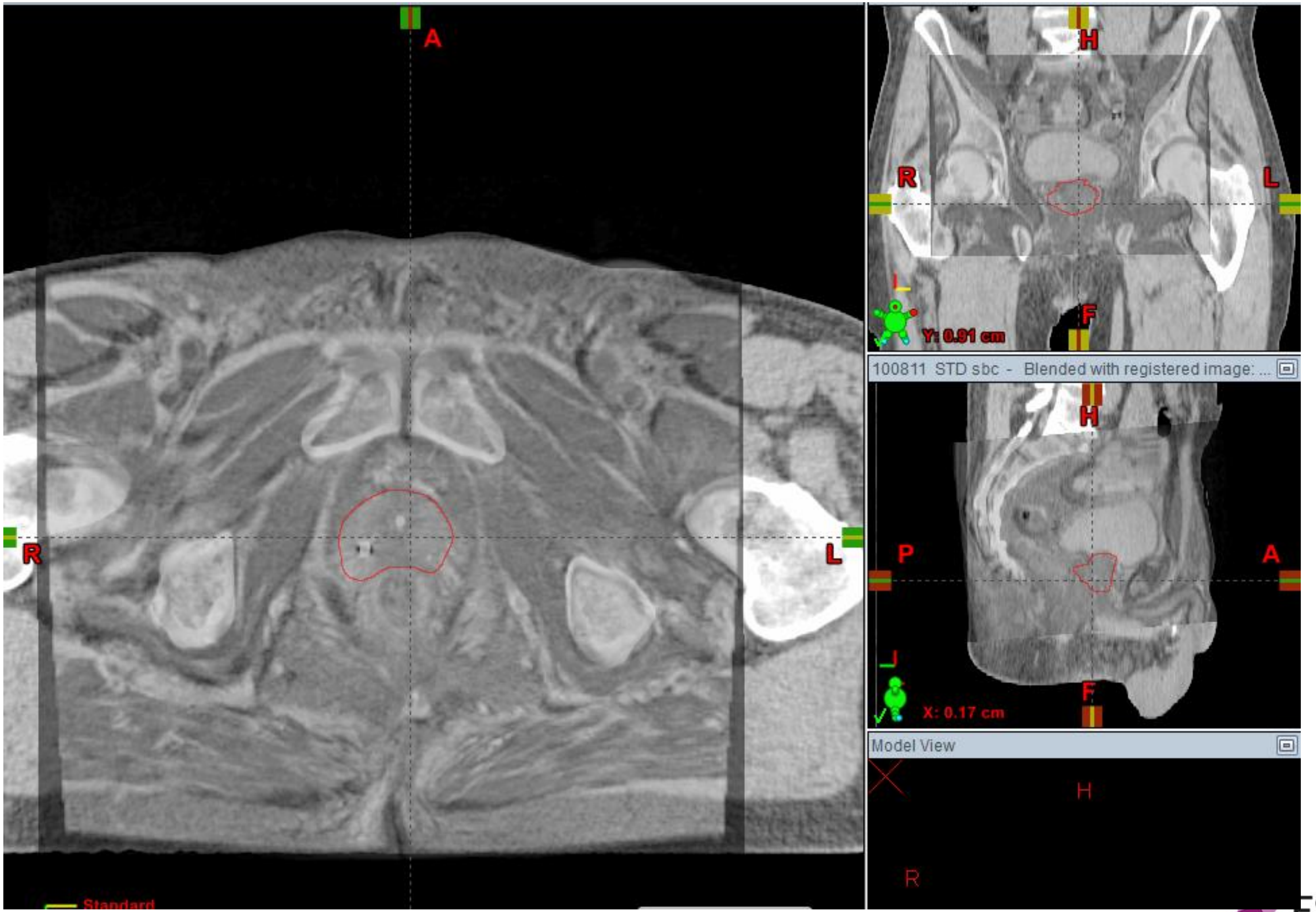
X: 0.17 cm
Model View
Standard

CT MR fusion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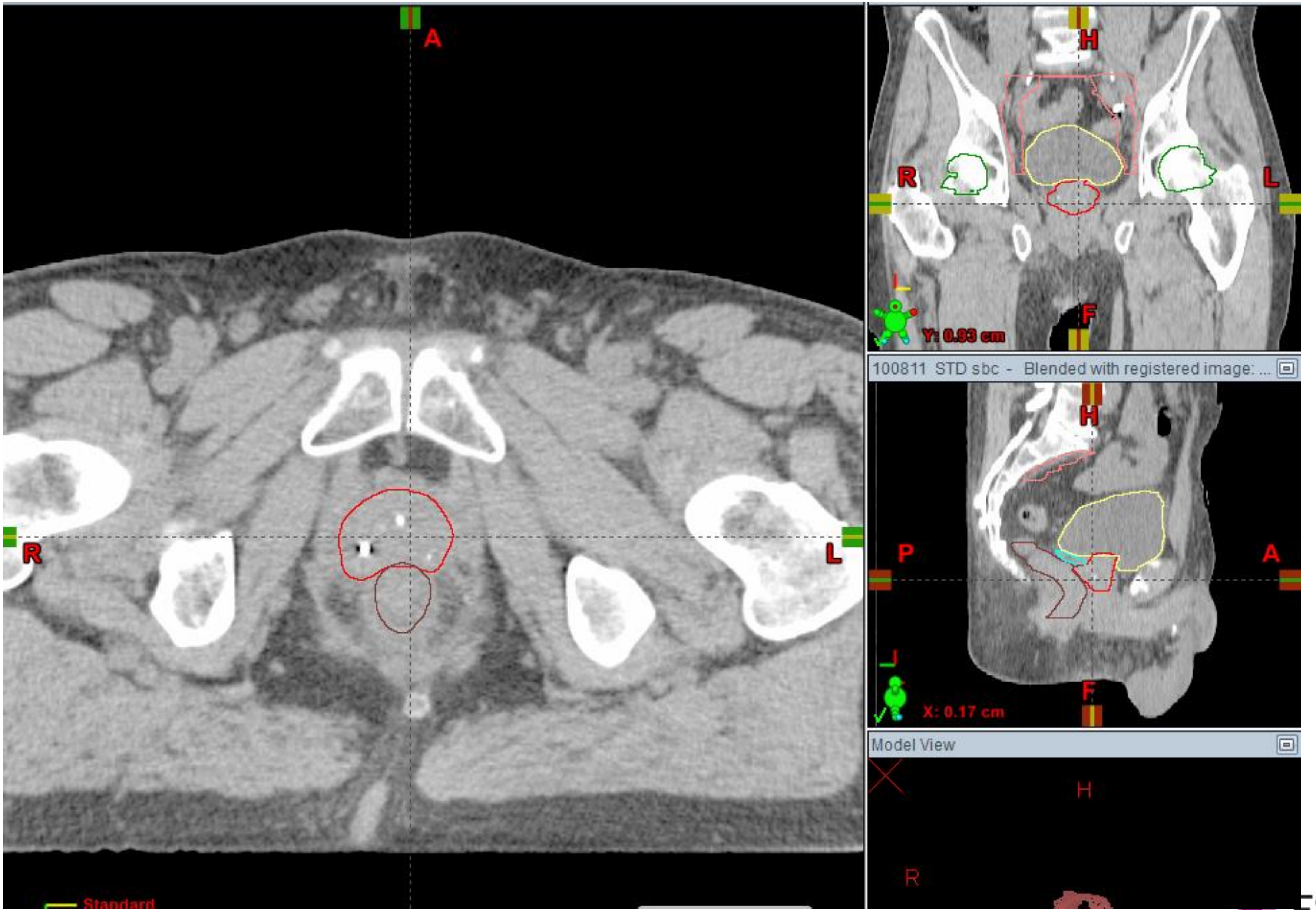
X: 0.17 cm
Model View
Standard

Target & OAR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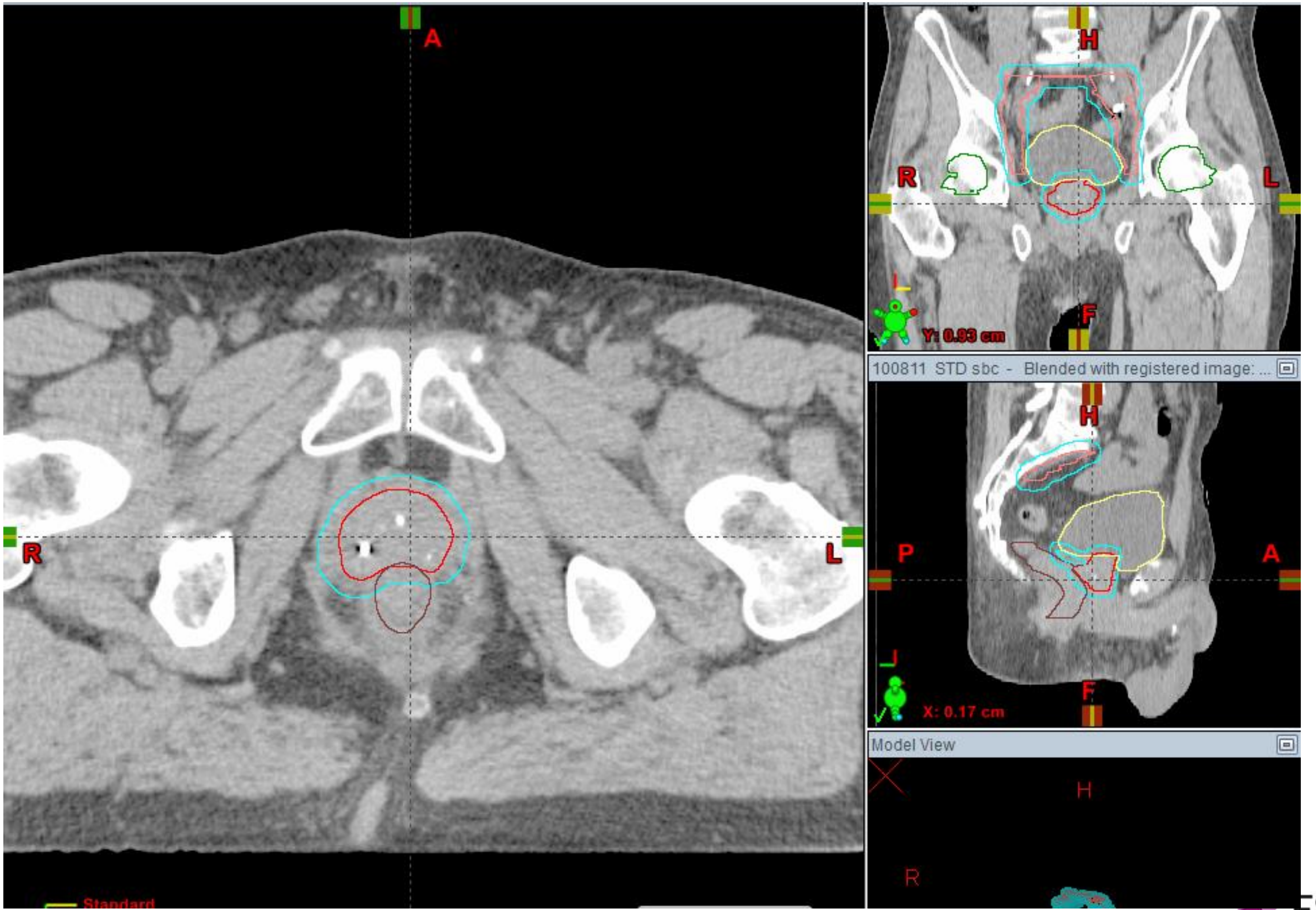
X: 0.17 cm
Model View
Standard

Target & OAR



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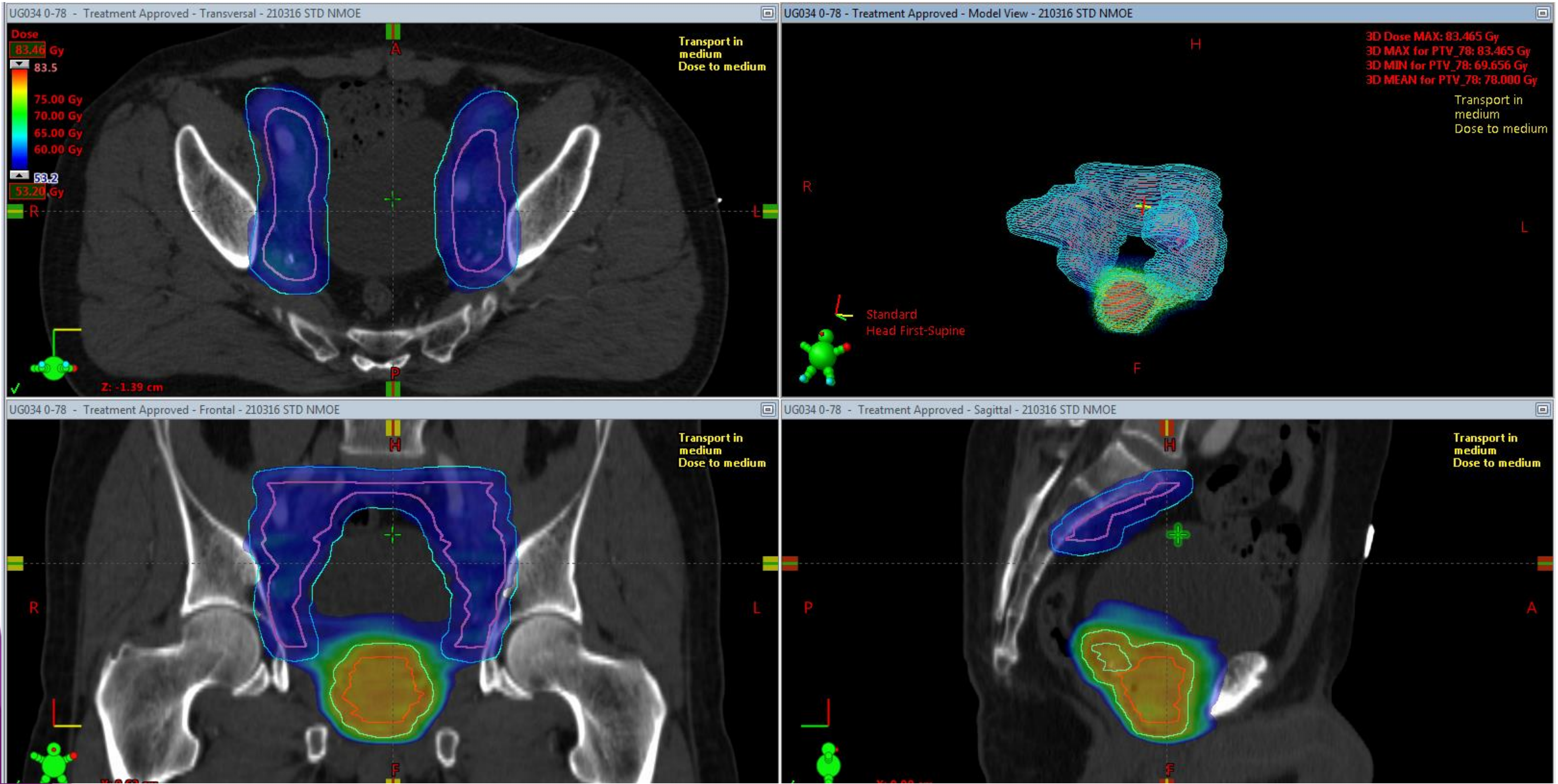
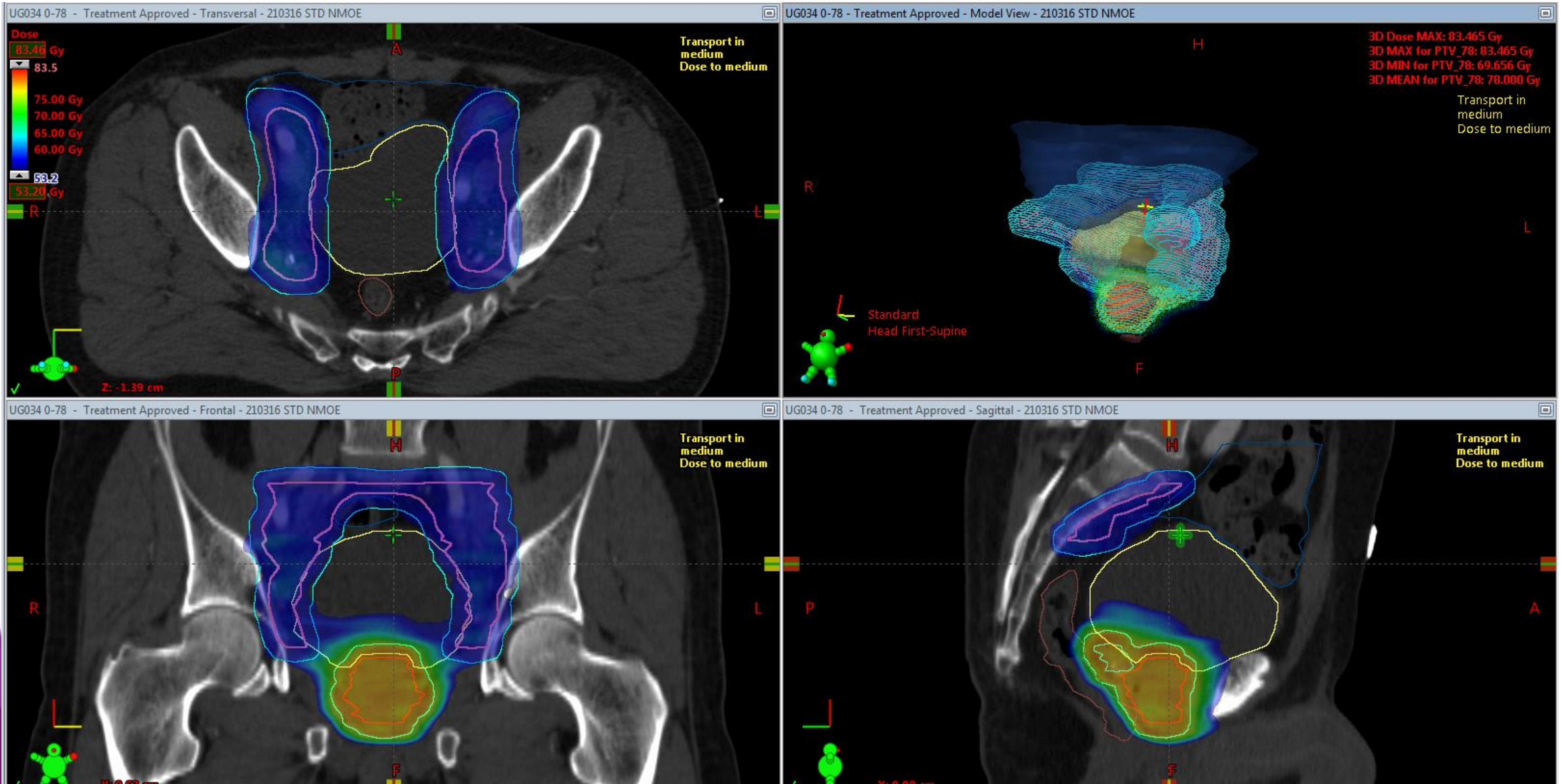
100811 STD sbc - Blended with registered image: ...
P
X: 0.17 cm
Model View
Standard

Treatment plan – VMAT with two arcs



Treatment plan – VMAT with two arcs



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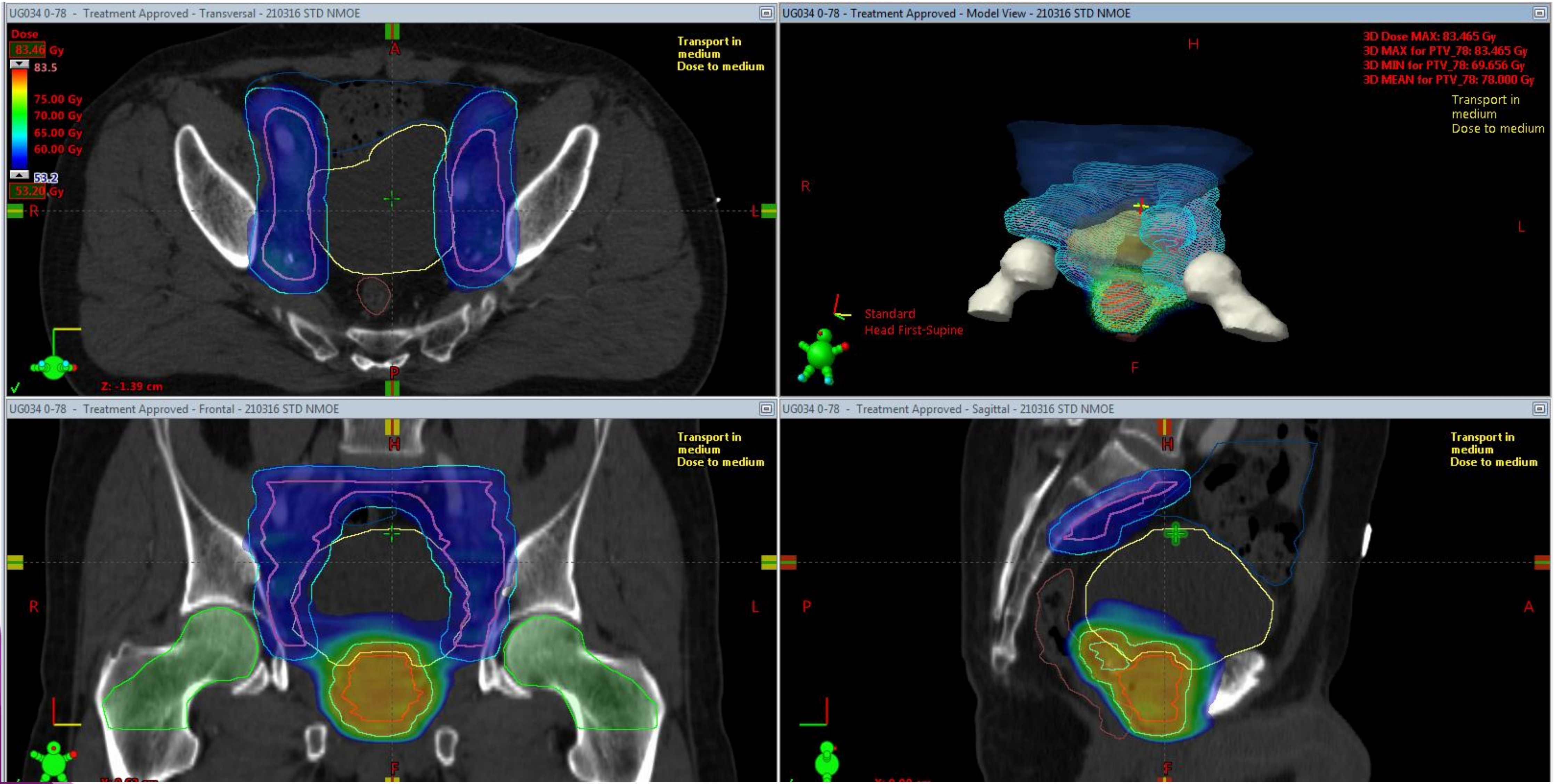
Treatment plan – VMAT with two arcs



Treatment planning

Copenhagen: 39 fractions of

- 2 Gy (total 78 Gy) to the prostate
- 1.49 Gy (total 58 Gy; $EQD2_{1.5}$= ~50 Gy) to the sem.vessicles & nodes

Seville: 28 fractions of

- 2.32 Gy (total 65 Gy; $EQD2_{1.5}$= ~71 Gy) to the prostate
- 2.14 Gy (total 60 Gy; $EQD2_{1.5}$= ~62 Gy) to the sem.vessicles & inv.nodes
- 1.75 Gy (total 50 Gy; $EQD2_{1.5}$= ~37 Gy) profilactic to the noninv.nodes

Challenge of overlap of PTV & OAR

Table 1 – Phase 3 randomized trials of moderate hypofractionation for intact prostate cancer

Study	Median FU, mo	Risk, GS, or NCCN	Technique	Regimen	BED, Gy	*n*	Outcome	Toxicity
Lukka et al. [15]	68	60% GS ≤6 31% GS 7 9% GS 8–10	3DCRT No IGRT	52.5 Gy/20 fx	62	466	5 yr FFBF 40% (NS)	Gr ≥3 2% (NS)
				66 Gy/33 fx	66	470	5 yr FFBF 43%	Gr ≥3 1%
Yeoh et al. [17]	90	n.s.	2D/3DCRT No IGRT	55 Gy/20 fx	66.8	108	7.5 yr FFBF 53% ($p < 0.05$)	Late GU; HR: 1.58 (95% CI, 1.01–2.47) favoring hypofractionation
				64 Gy/32 fx	64	109	7.5 yr FFBF 34%	
Dearnaley et al. [18]	51	n.s.	3D/IMRT No IGRT 3–6 mo ADT	57 Gy/19 fx	73.4	151	n.s.	Gr ≥2 GU 0% (NS) Gr ≥2 GI 1% (NS)
				60 Gy/20 fx	77	153		Gr ≥2 GU 2% Gr ≥2 GI 4%
				74 Gy/37 fx	74	153		Gr ≥2 GU 2% Gr ≥2 GI 4%
Kuban et al. [14]; Hoffman et al. [19]	60	28% low 71% intermediate 1% high	IMRT IGRT 21% ADT	72 Gy/30 fx	80.2	102	5 yr FFBF 96% (NS)	5 yr Gr ≥2 GU 16% (NS) 5 yr Gr ≥2 GI 10% (NS)
				75.6 Gy/42 fx	71.4	101	5 yr FFBF 92%	5 yr Gr ≥2 GU 17% 5 yr Gr ≥2 GI 5%
Arcangeli et al. [12,13]	70	26% GS ≤7 74% GS >7	3DCRT No IGRT 100% 9 mo ADT	62 Gy/20 fx	81.4	83	5 yr FFBF 85% ($p = 0.065$) *p ss for GS ≥4 + 3	3 yr Gr ≥2 GU 16% (NS) 3 yr Gr ≥2 GI 17% (NS)
				80 Gy/40 fx	80	85	5 yr FFBF 79%	3 yr Gr ≥2 GU 11% 3 yr Gr ≥2GI 14%
Pollack et al. [16]	68	34% GS ≤6 47% GS 7 19% GS 8–10	IMRT IGRT	70.2 Gy/26 fx	84	151	5 yr BCDF 23% (NS)	5 yr Gr ≥2 GU 13% ($p = 0.16$) 5 yr Gr ≥2 GI 9% (NS)
				78 Gy/36 fx	78	152	5 yr BCDF 21%	5 yr Gr ≥2 GU 13% 5 yr Gr ≥2 GI 9%

3DCRT = three-dimensional conformal radiotherapy; ADT = androgen-deprivation therapy; BCDF = biochemical or clinical disease failure; BED = biologically equivalent dose, calculated to be equivalent in 2 Gy fractions using an α/β of 1.5 Gy; CI = confidence interval; FFBF = freedom from biochemical failure; FU = follow-up; fx = fractions; GI = gastrointestinal; Gr = grade; GS = Gleason score; GU = genitourinary; HR = hazard ratio; IGRT = image-guided radiation therapy; IMRT = intensity-modulated radiation therapy; NCCN = National Comprehensive Cancer Network; NS = not significant; n.s. = not stated; ss = statistically significant.

Koontz et al. European Urology 2015

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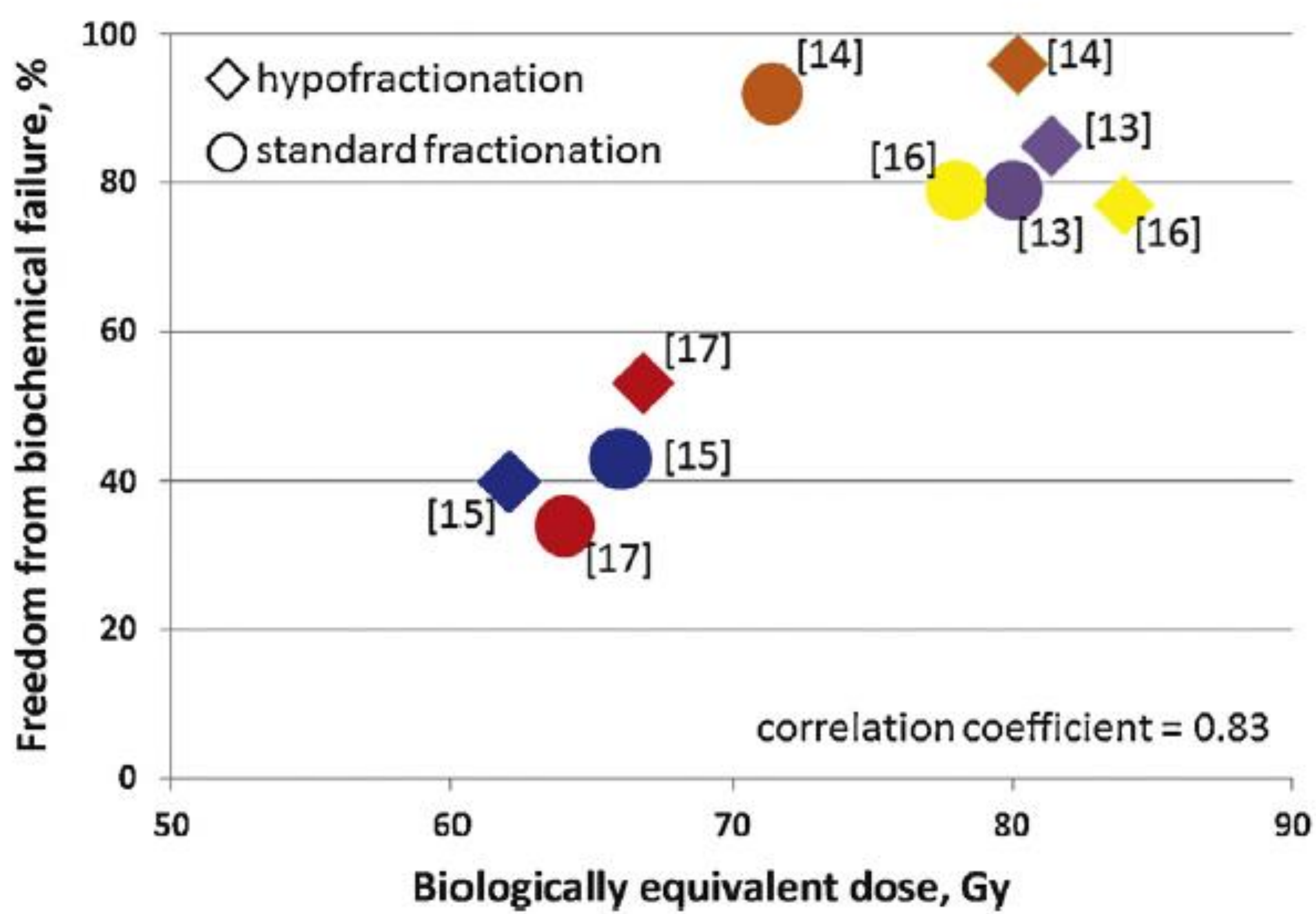
Table 1 – Phase 3 randomized trials of moderate hypofractionation for intact prostate cancer

Study
Lukka et al. [15]
Yeoh et al. [17]
Dearnaley et al. [18]
Kuban et al. [14]; Hoffman et al. [19]
Arcangeli et al. [12,13]
Pollack et al. [16]



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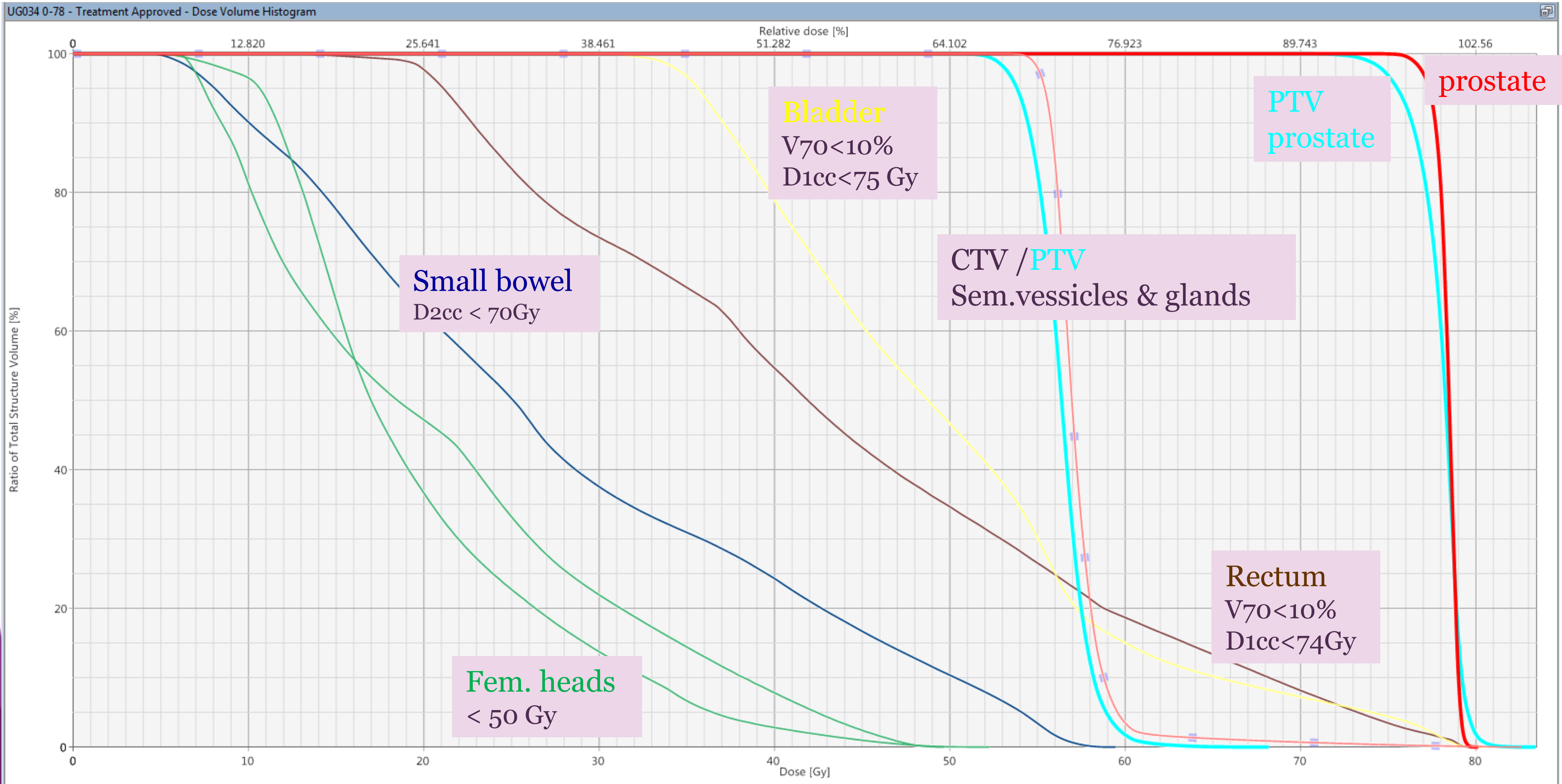
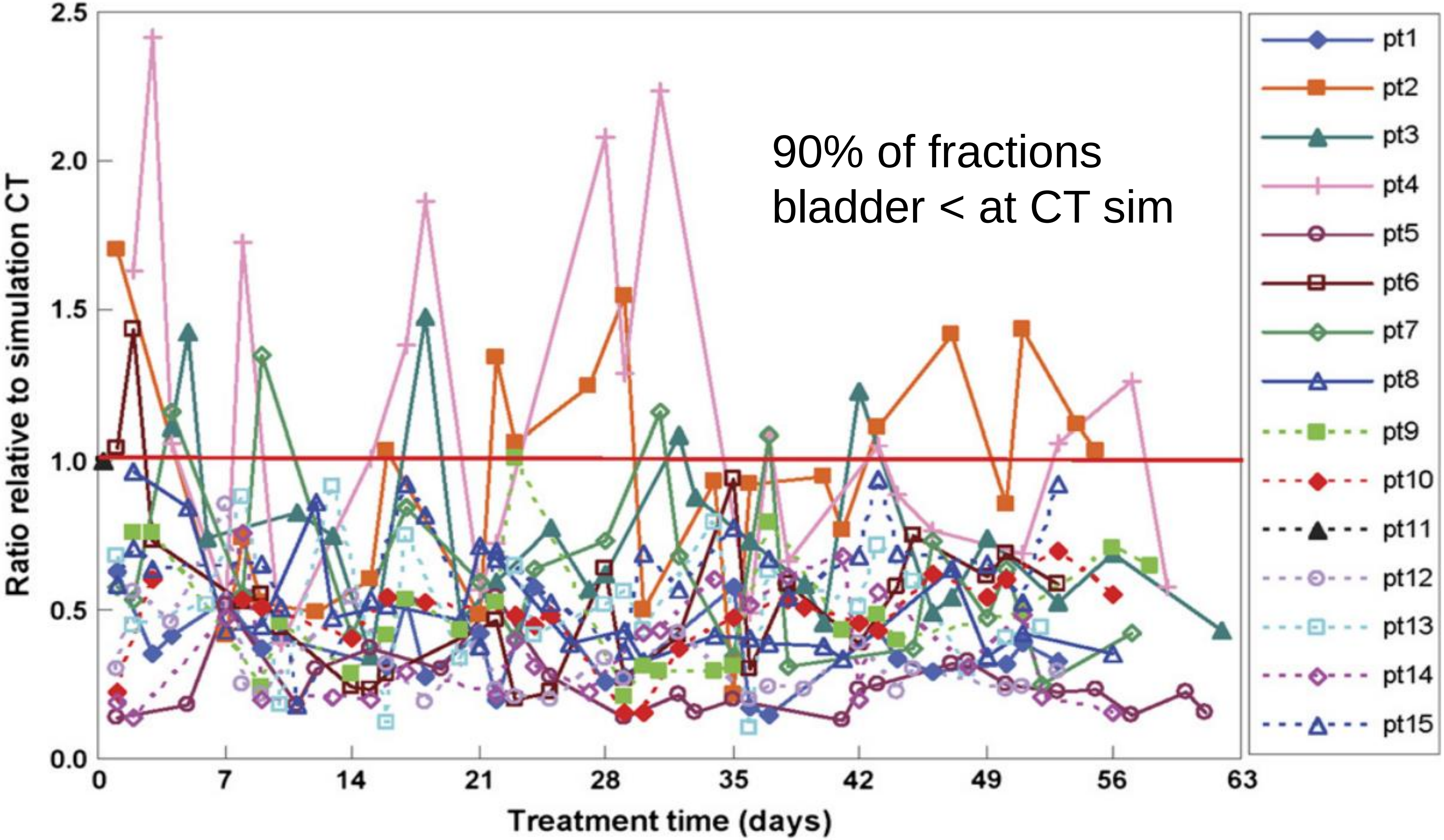
Koontz et al. European Urology 2015

Treatment plan – VMAT with two arcs



Changes in bladder volume during the RT



90% of fractions bladder < at CT sim

Frank et al. IJROBP 2007

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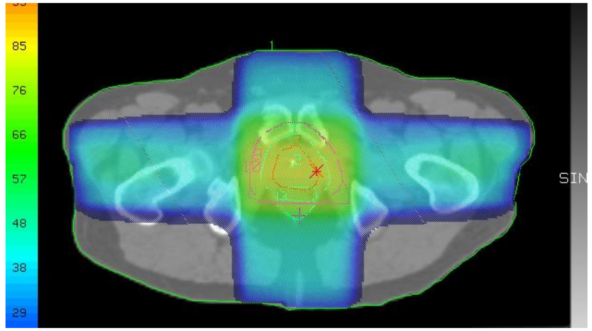
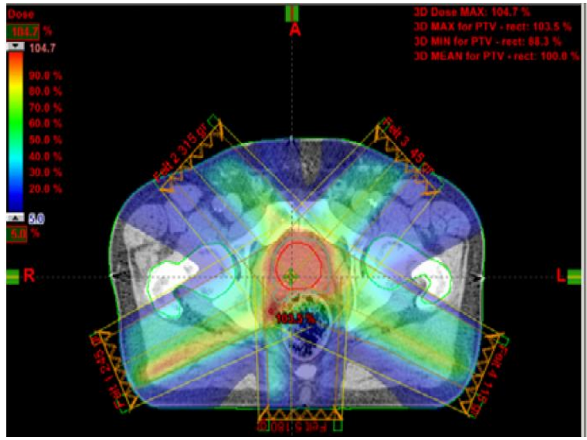
Treatment techniques

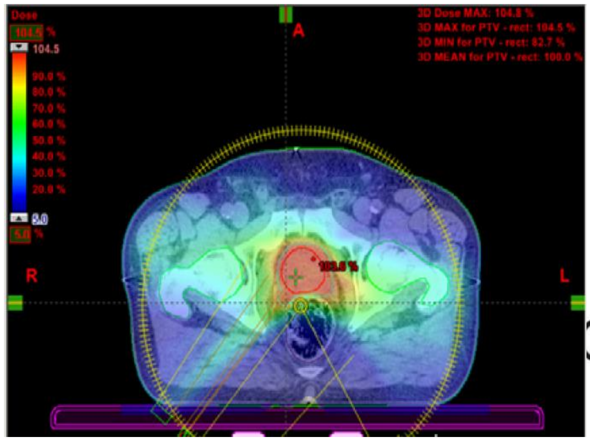
< 2005 — 3D conformal ”box” technique



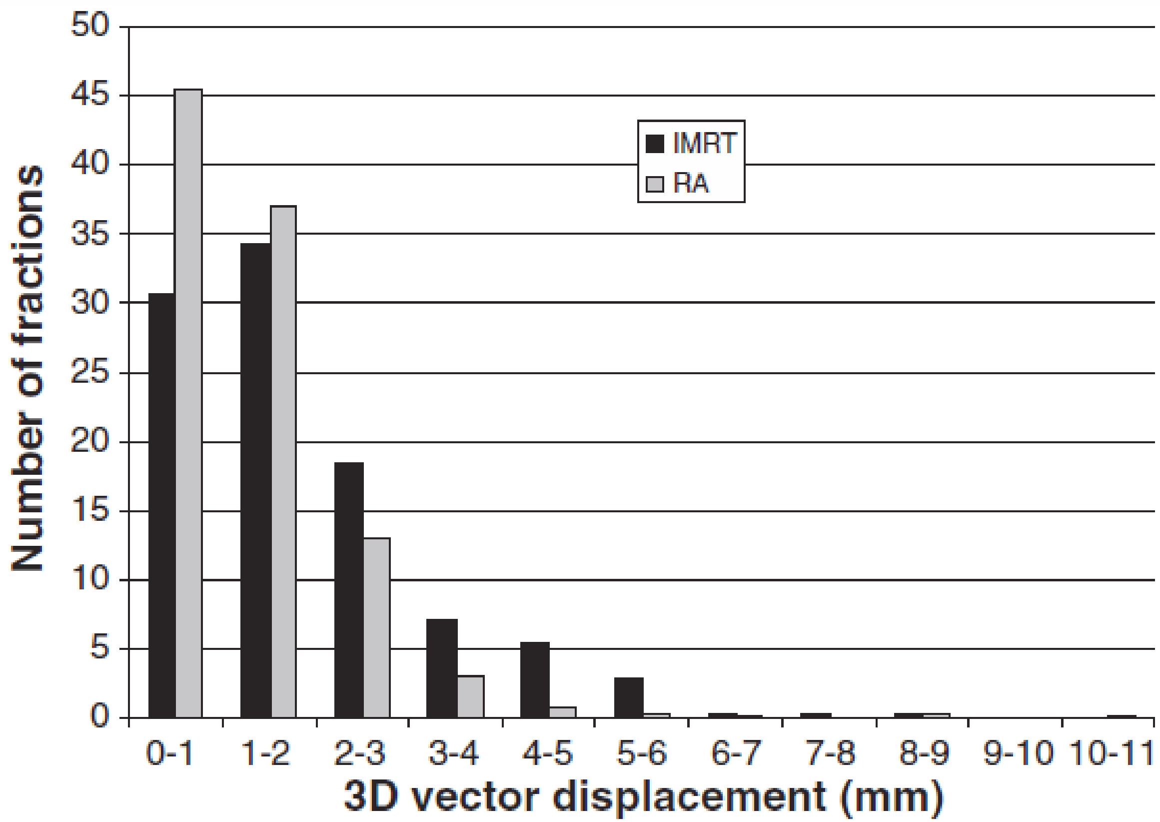
2005 — IMRT
- Gold seeds & daily IGRT
- Margins ↓



2008 — VMAT
- Faster treatment (1 arc = 1 min)
- Margins ↓



Treatment delivery time

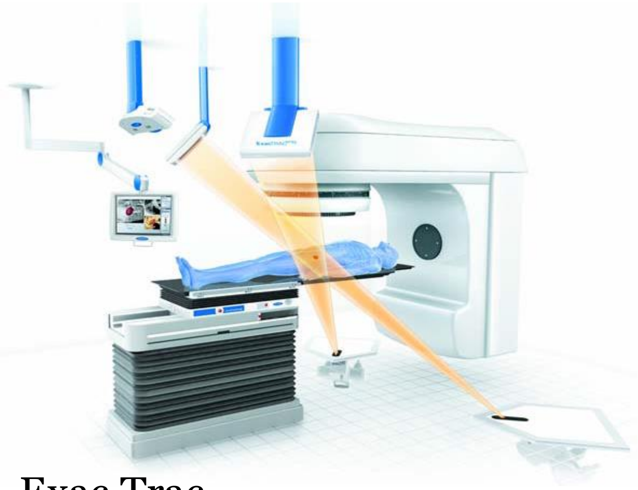


	IMRT	VMAT
Treatment delivery time	4.9 min	1.1 min
Intra-fractional prostate displacement > 3mm	16.7%	4.7%

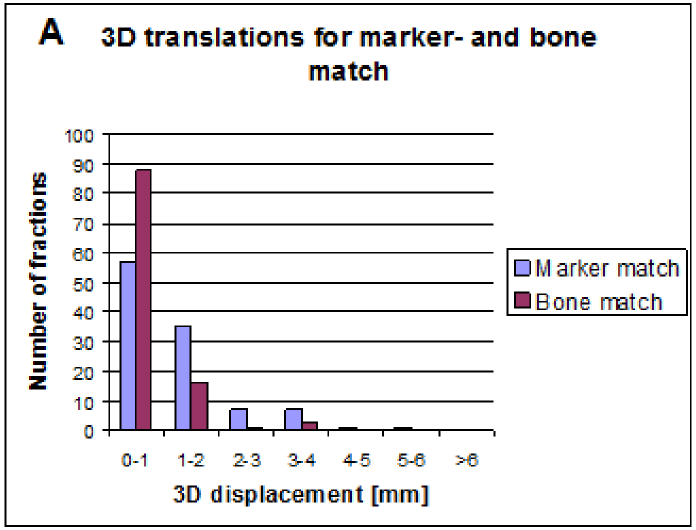
M Aznar et al, Radiother Oncol 2010

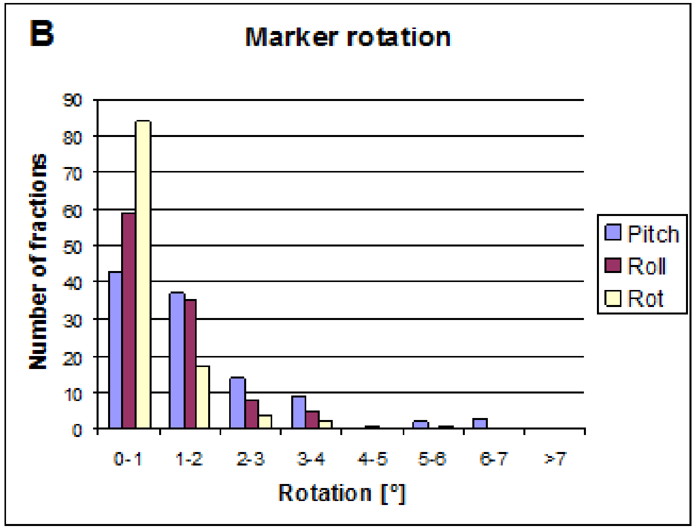
Prostate rotation

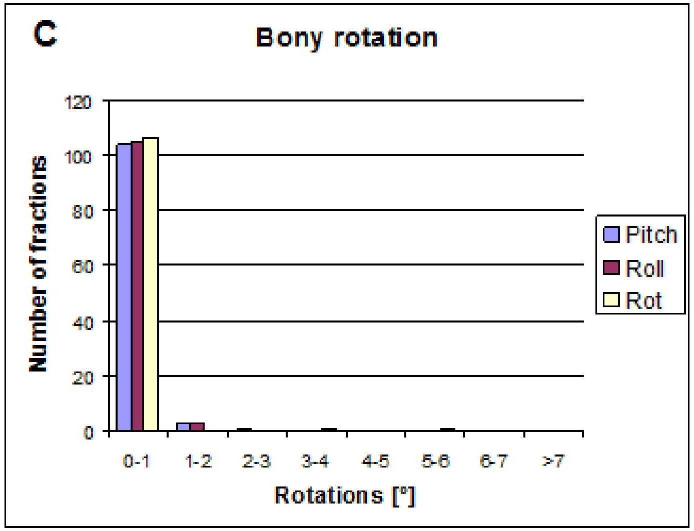
Courtesy of JS Rydhög



Exac Trac
with robotic couch







After the 6D correction, the deviation in prostate is larger than deviation in patient position, for both translation and rotation

IGRT for prostate cancer: RTT perspective

Martijn Kamphuis MSc MBA
Research Radiation Therapist IGRT

Department of Radiotherapy @ AMC
Amsterdam, the Netherlands

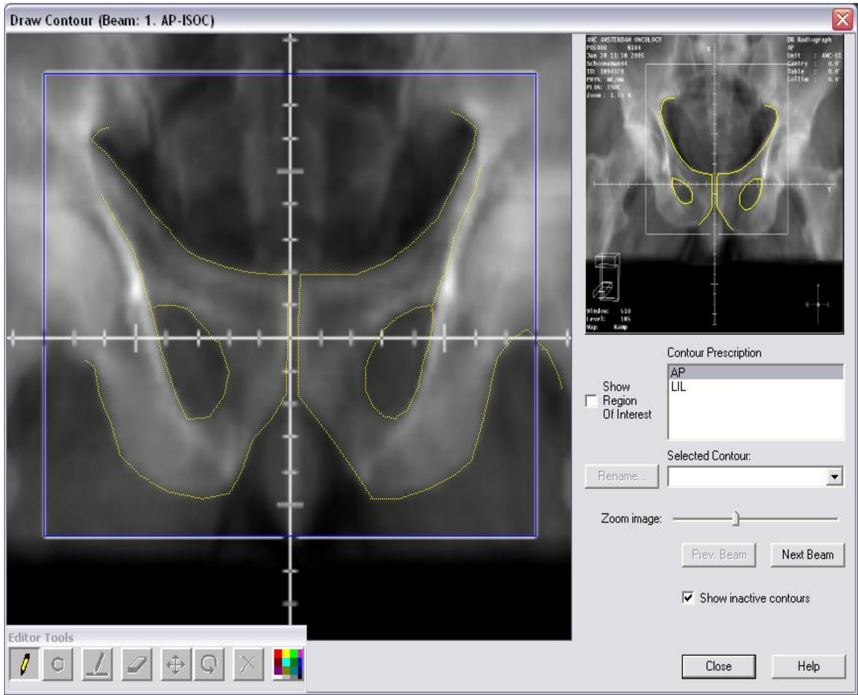
Content

- Prostate IGRT in general
  - ➢ Offline bony anatomy matching
  - ➢ Offline marker registration using fiducial markers and PI
  - ➢ Online marker registration using fiducial markers Portal or static kV imaging
  - ➢ Online marker registration using Conebeam-CT

- IGRT for this challenging case ☺

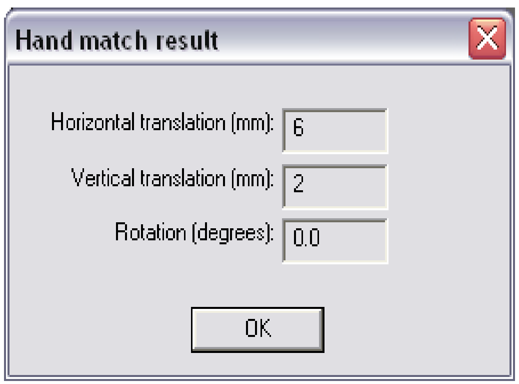
Offline/Online bony anatomy matching

- Create an image with sufficient data
- Draw contours (templates) in reference images
- Contours should have a proper correlation with target
  - E.g. no trochantor or femur
- Produce guidelines!



Offline/Online bony anatomy matching

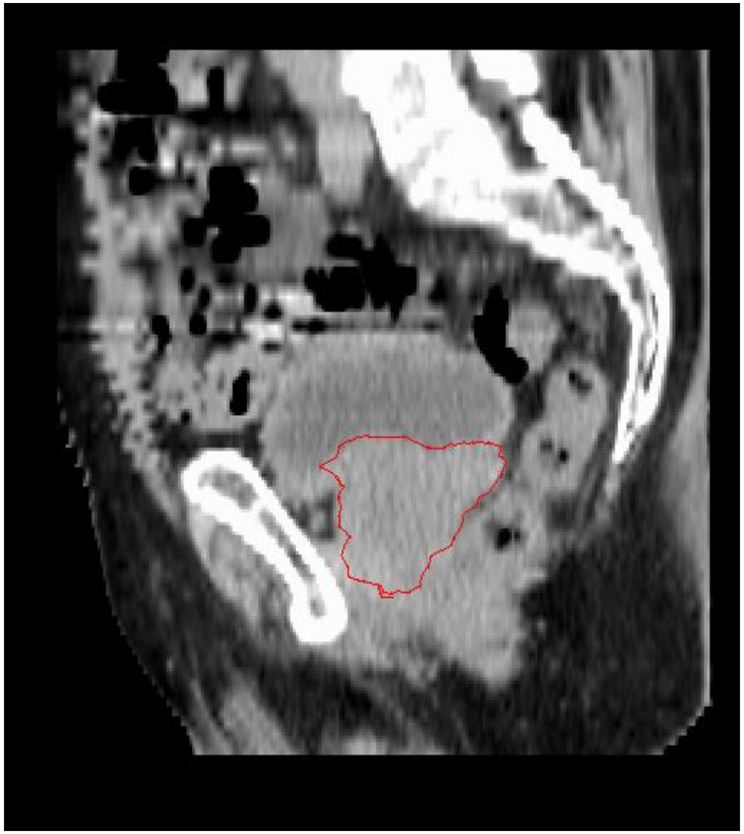
- Field edge match
- Match PIs



Offline marker registration using fiducial markers

Problem/challenge

- Displacement of bony anatomy does not (always) represent displacement of target



Van Herk et al.

Fiducial markers

- Displacement of bony anatomy does not (always) represent displacement of target
  - ➢ Neederveen et al. 2003: prostate cancer

	LR (mm)			AP (mm)			CC (mm)		
	marker	bone	mk. rel. bone	marker	bone	mk. rel. bone	marker	bone	mk. rel. bone
Mean	0.0	0.0	0.0	− 1.0	− 1.0	0.0	1.1	0.1	1.0
Σ	2.4	2.1	1.0	**4.4**	**4.4**	2.3	**3.7**	2.1	**4.1**
σ	2.1	1.8	0.8	**3.4**	**2.2**	2.4	**2.7**	1.7	**2.4**

Standard deviations for the systematic and random case that do differ significantly are printed in bold.

- ➢ For 6 out of 23 patients → increase of systematic error after correction based on bony anatomy !!

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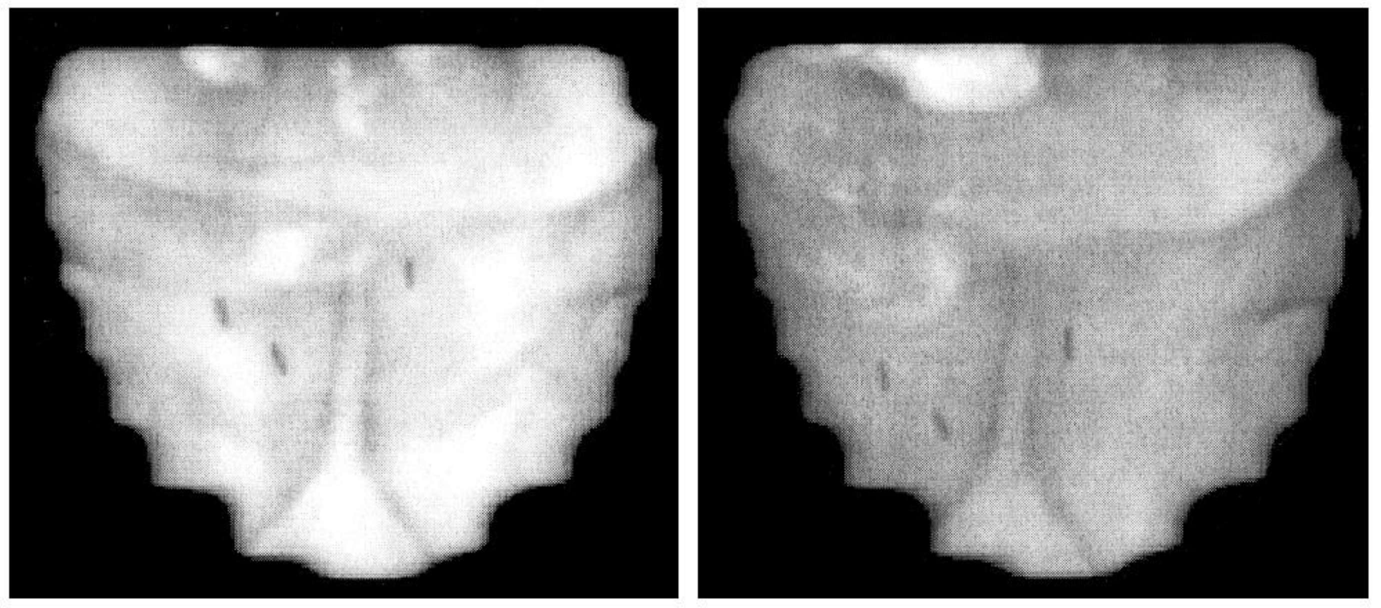
Fiducial markers: offline

Based on Van der Heide *et al.* 2007:

- ➢ 5 field IMRT treatment
- ➢ Daily offline imaging:
  - Treatment field: 40, 180 and 320 degrees
  - SAL (α=8, N=4)
  - Threshold SAL= $\alpha/\sqrt{N}$
- ➢ Limited (radiation) fields adequate
  - No additional dose!



Fiducial markers: offline

- Succesfull reduction of systematic error!
  - Without applying a correction protocol, the systematic errors (*Σ)* are:
    - 4.8, 2.2 and 2.9 mm in the vertical, lateral and longitudinal directions
  - The SAL protocol
    - 0.7, 0.8 and 0.8 mm, respectively.
  - Random position variations are not reduced in an off-line correction protocol

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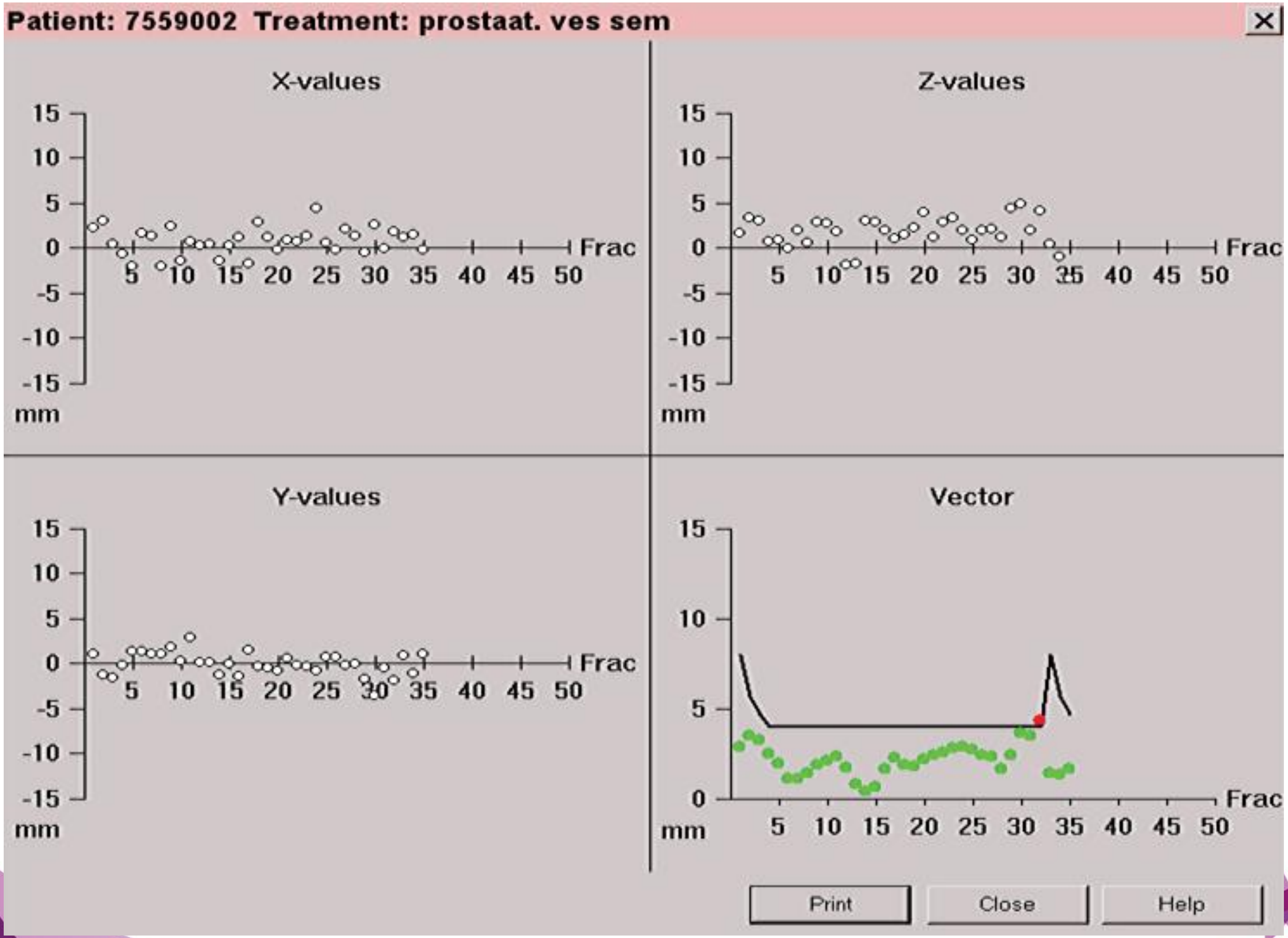
Online fiducial marker registration

Food for thought!

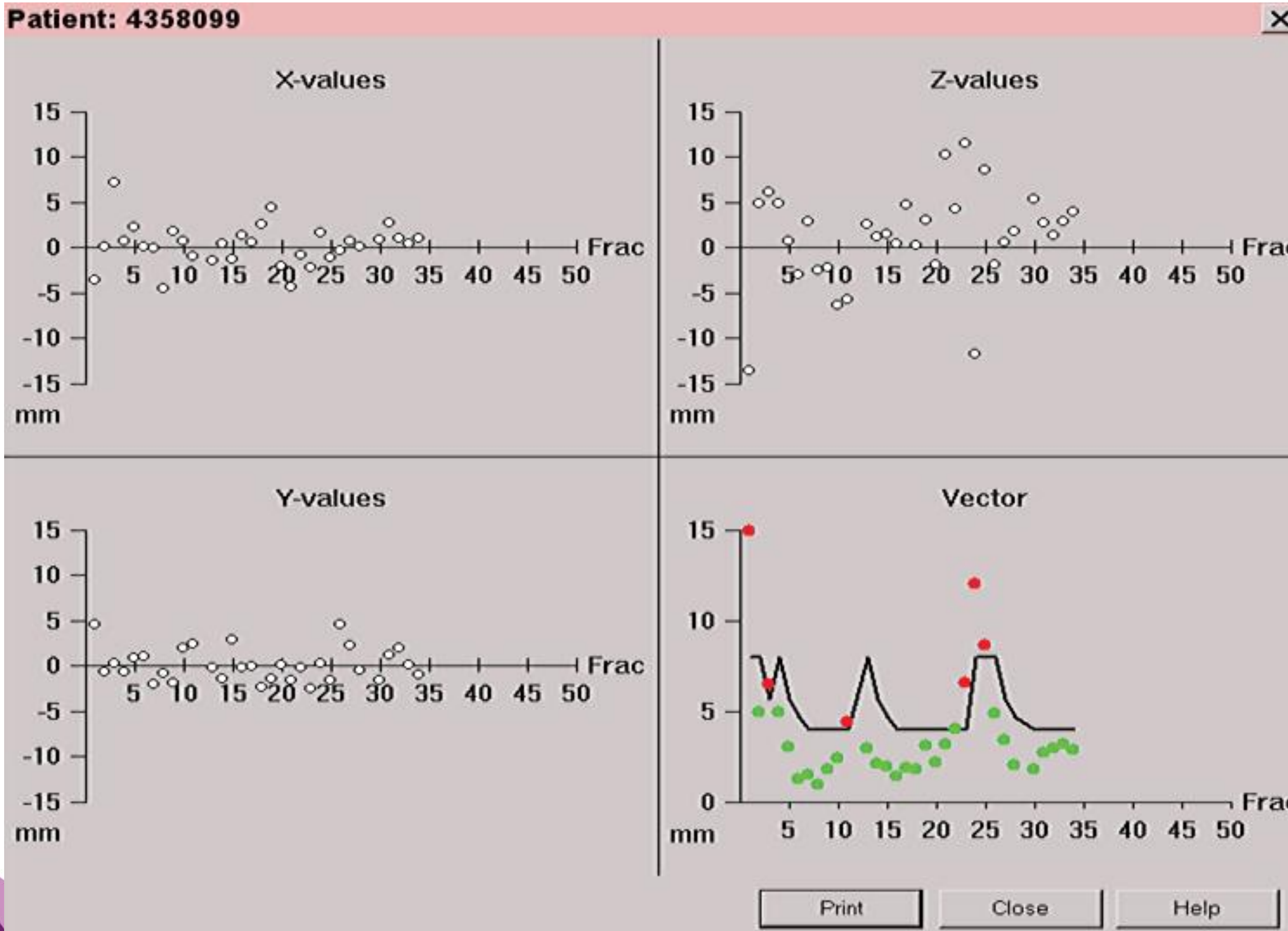


Would you like to treat a patient like this offline?

A. Yes

B. No

Food for thought!



Would you like to treat a patient like this offline?

A. Yes

B. No

Online Position Verification

- To reduce random error:
  - ➢ Online position verification is needed

- Different methods available
  - ➢ Two dedicated EPI field, e.g. 40 and 320 degrees
    - ▪ Correction for imaging dose necessary
  - ➢ Stereo Graphic Targeting
    - ▪ MV and kV together
    - ▪ Correction for imaging dose necessary
  - ➢ Two kV images
    - ▪ With CBCT or OBI
    - ▪ With ExacTrack system

Offline vs Online

		Results (mm)		
		X	Y	Z
Offline	Sys. error	0.8	0.8	0.7
	Random error	2.3	2.5	4.0
Online	Sys. error	0.8	0.6	0.9
	Random error	1.0	1.0	1.2

Online Position Verification

Online procedure

- Random error minimalized

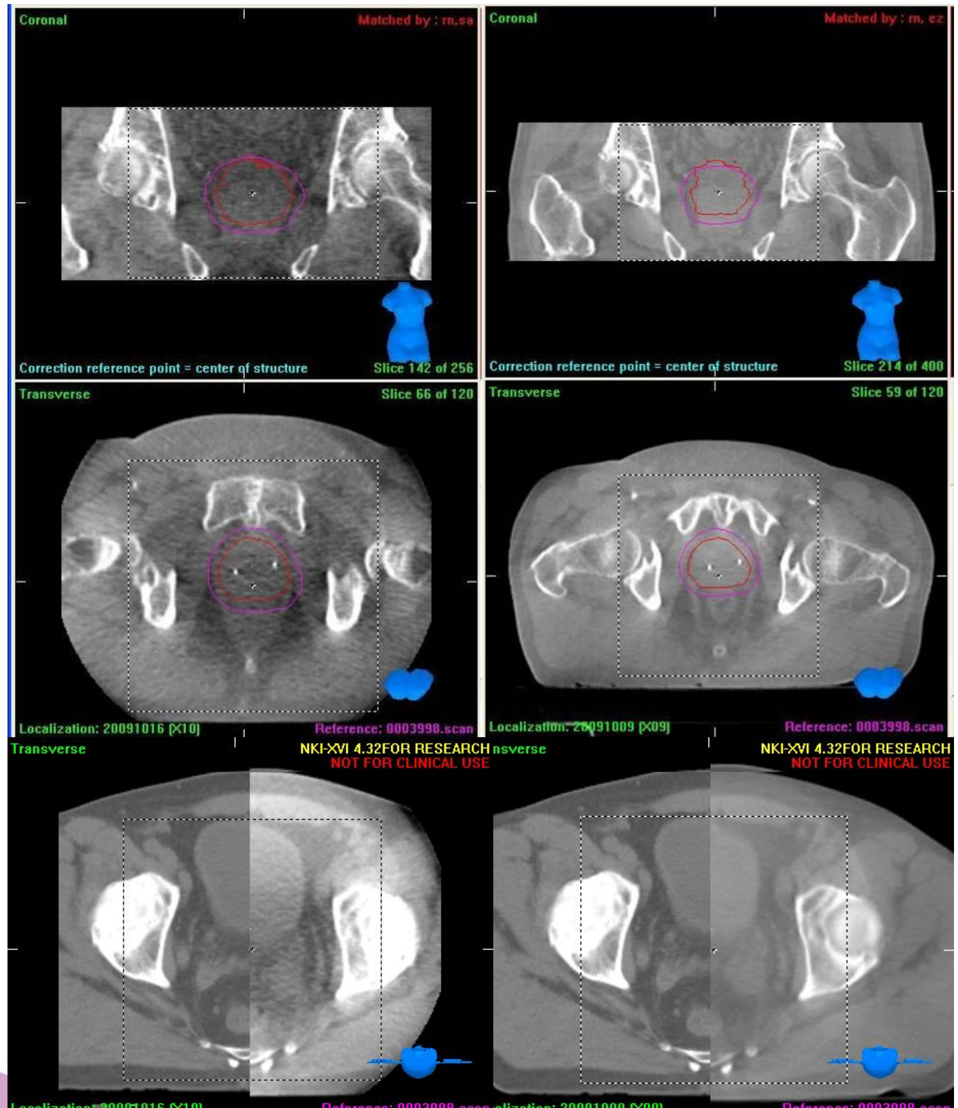
Enables **limited** margin reduction!

treatment execution β * σ	3.3	7.7	3.6
breathing b	0.0	0.0	0.0
scalar a - β * σ_p	-2.7	-6.6	-2.7
CTV-PTV marge (mm)	6.6	7.2	7.1
Eenvoudige formule van Herk: 2.5*SIGMA+0.7*sigma	8.0	7.8	8.7
Formule Stroom: 2.0*SIGMA+0.7*sigma	6.8	6.6	7.5

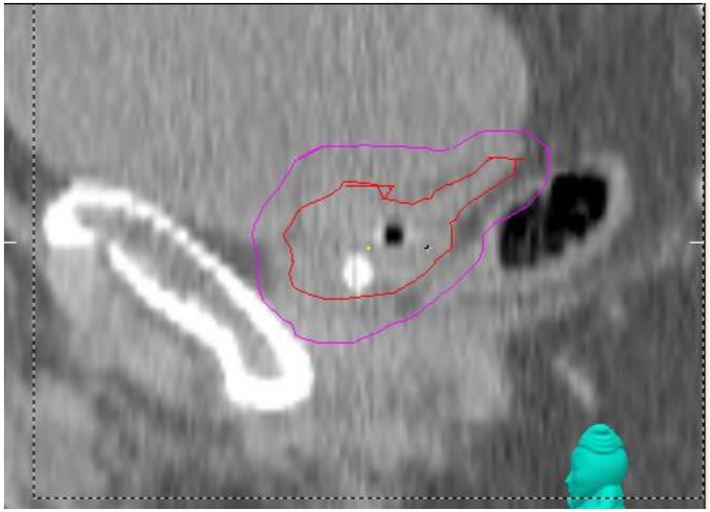
[illegible]	[illegible]	[illegible]	[illegible]
breathing b	0.0	0.0	0.0
scalar a - β * σ_p	-2.7	-6.6	-2.7
CTV-PTV marge (mm)	6.2	6.2	6.1
Eenvoudige formule van Herk: 2.5*SIGMA+0.7*sigma	7.1	6.8	7.0
Formule Stroom: 2.0*SIGMA+0.7*sigma	5.9	5.6	5.8

Online marker registration using CBCT

0.4 cGy 3 cGy

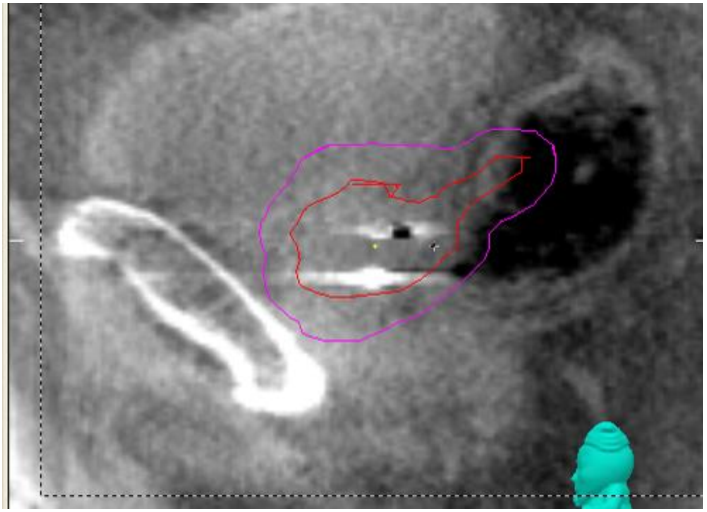


ConeBeam CT: soft tissue information



Red = Prostate + sem.ves.

Purple = PTV



CBCT : sem.ves outside PTV

Acknowledgements NKI/AvL

Many ways to Rome!

Method	Margin (AMC)	Extra treatment time	Imaging dose	Corretable?	Relevant anatomical information
Bone match	10 mm	2-3 minutes	(3cGY*2) High	Possible	-
Offline fiducial PI	8 mm	0 minutes	No	-	+
Online fiducial PI	7 mm	1-3 minutes	Very low (kV) to high (MV)	Correctable in case of PI	+
Online CBCT	7 mm	1-3 minutes	0.4-3.5 cGy/scan	Partly	+++

If there is a balance with the used margin:

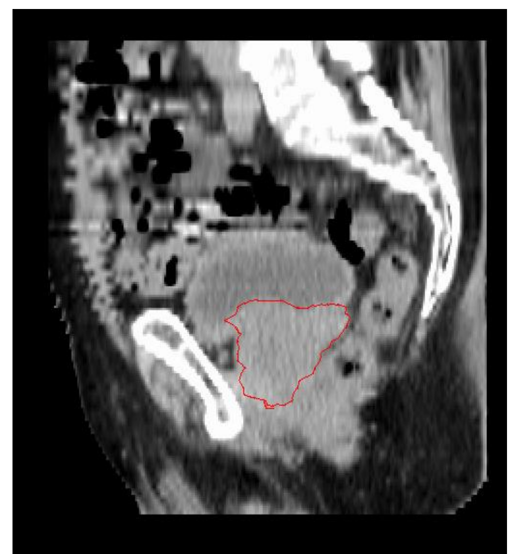
1. LC is about the same for the all different procedures
2. Toxicity probably lowest with online IGRT

The N1 case: SIB approach

Challenge: Independent moving targets

- Lymph nodes
  - Correlate nicely with bony anatomy
- Prostate
  - Doesn’t correlate with bony anatomy

Van Herk *et al*.



Option 1: solved by margins (AMC)

- Use guidelines for delineation: e.g.Tayl[illegible]
- Depending on correction protoco[illegible]te optimal margins
  - E.g. AMC offline eNA[illegible]on protocol 8 mm, 7 mm and 10mm for X[illegible]direction respectively

- If ,for th[illegible]te, no fiducials are used
  - [illegible]ould use 1 cm isotropic margin

- [illegible]vailable for everybody
- Not optimal concerning toxicity

Be aware of highly moving positive lymph nodes!

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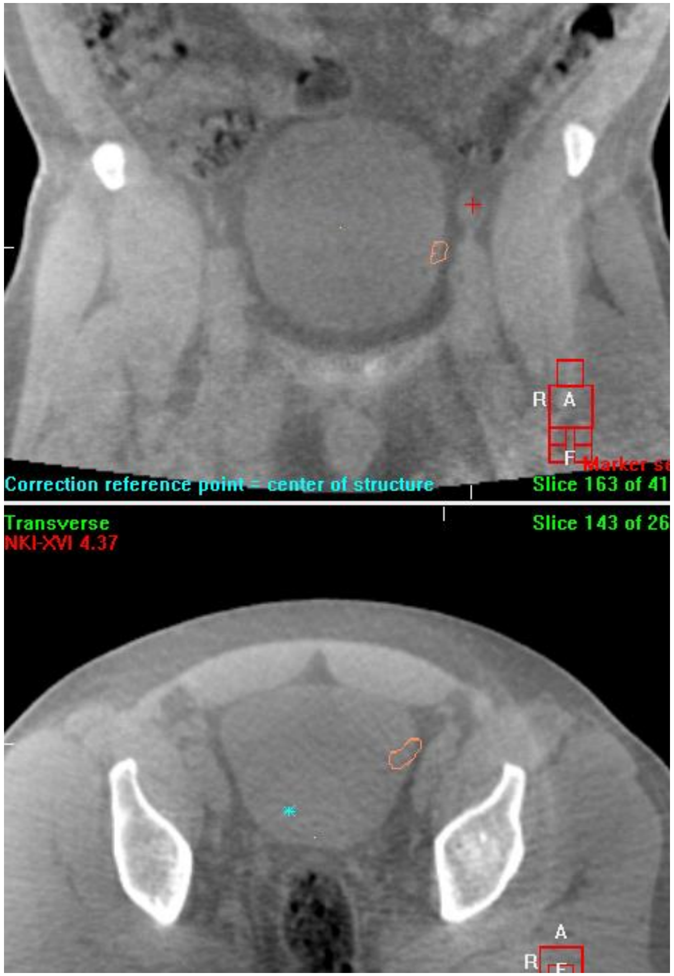
In practice large displacements were found in different cases

Correction for displacement of individual lymph nodes not always possible:

- multiple targets involved

Margins can be a solution

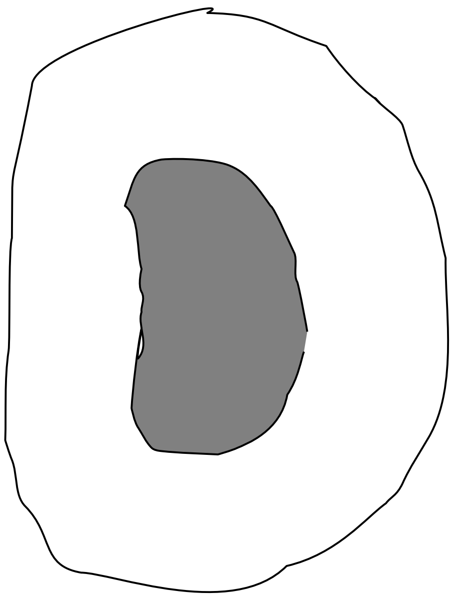
- But first quantify the problem



Option 2: Adaptive procedure

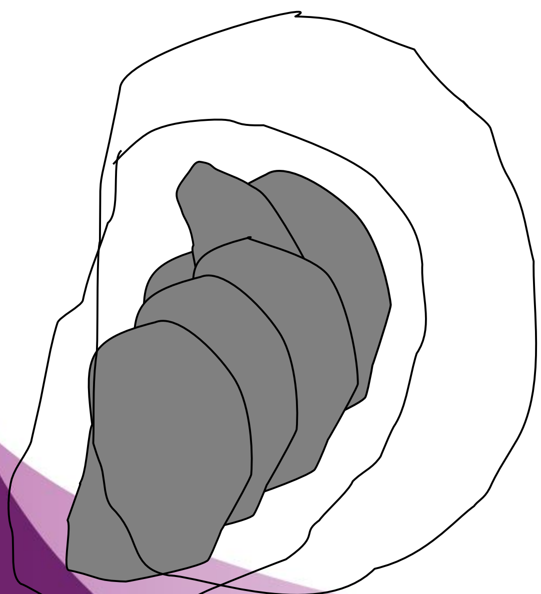
- Major problem:
  - “uncorrectable” systematic error between lymph nodes and prostate match
  - Peter’s rules: deformations can not be corrected with table corrections

Bladder: Focal adaptive margin strategy



Conventional focal boost technique:

one initial tumor position plus 2 cm margin



<u>Adaptive margin strategy</u>:

5 CT scans during first week of RT

Delineate 6 tumor positions plus 1 cm margin

- 40% boostvolume reduction *(pos et al 06)*
- less geografical missers

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Thank you for your attention!

Case report: **Breast**

ESTRO School

Sofia Rivera, M.D.
Radiation Oncology Department
Gustave Roussy
Villejuif, France

GUSTAVE ROUSSY
CANCER CAMPUS GRAND PARIS

Advanced skills in modern radiotherapy
June 2017

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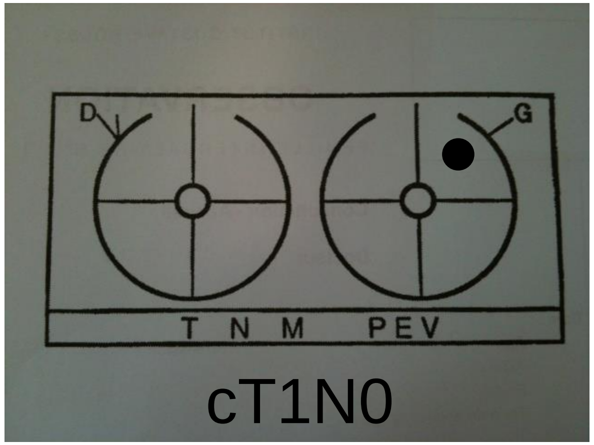
Clinical case

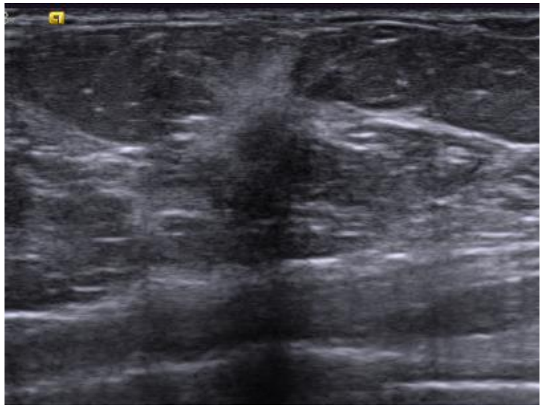


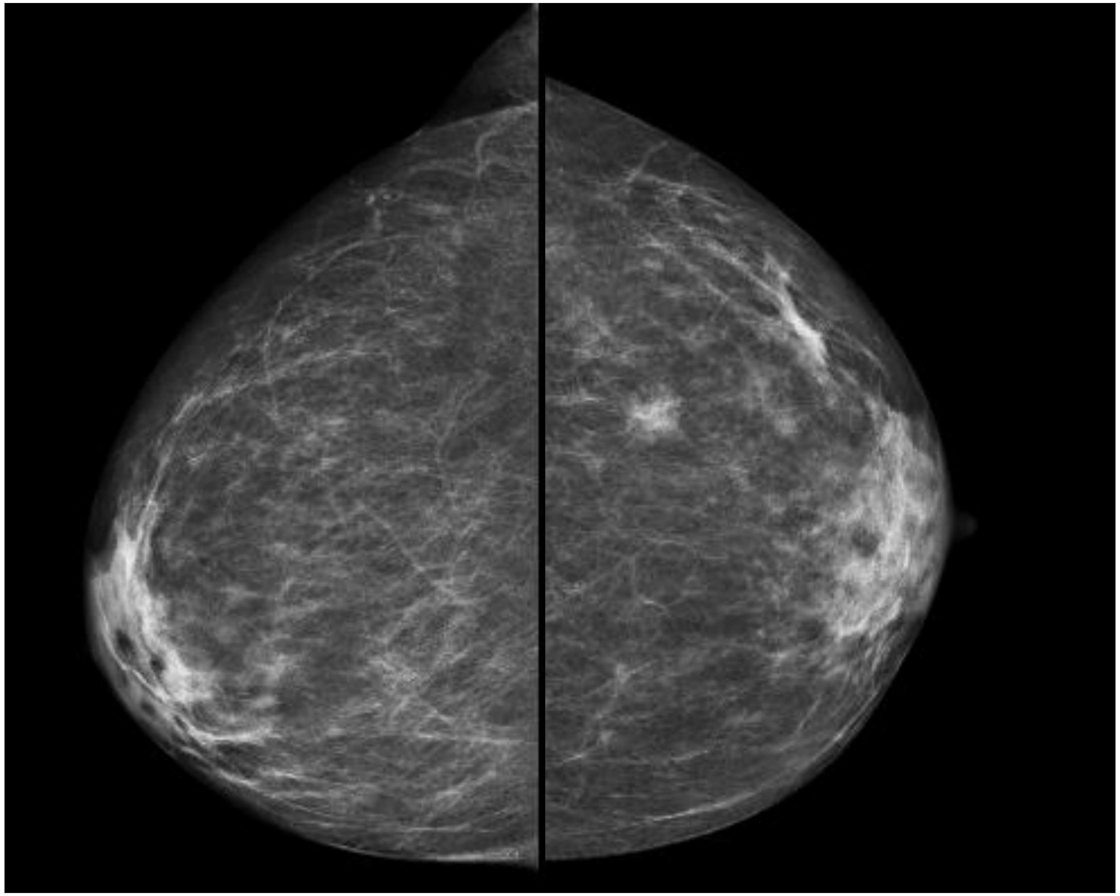
•72 years old female patient referred by her GP after palpation of a supra areolar hard mass of the left breast external upper quadrant measuring 1cm with no axillary or supraclavicular palpable node (breast cup: 95 D)

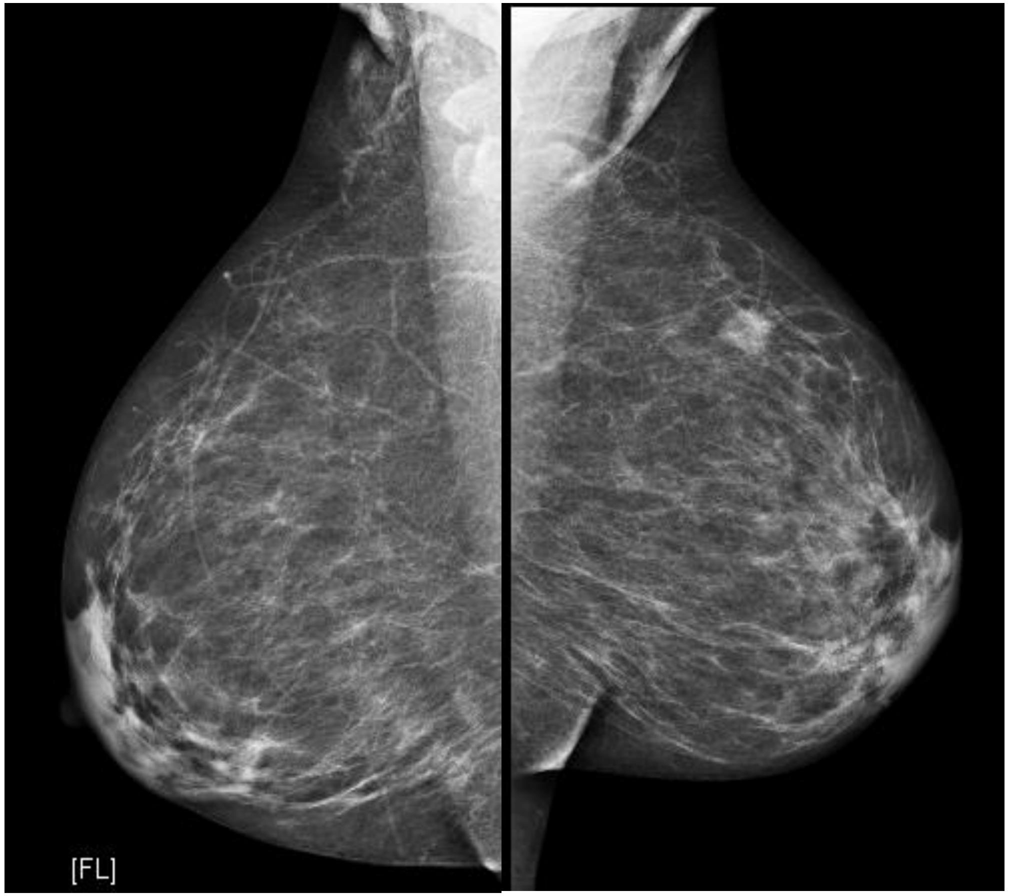
•Retired, yoga teacher, autonomous, living in an individual house with 5 cats

•Medical history of hypertension, diabetes and ischemic cardiopathy

Mammograms + US

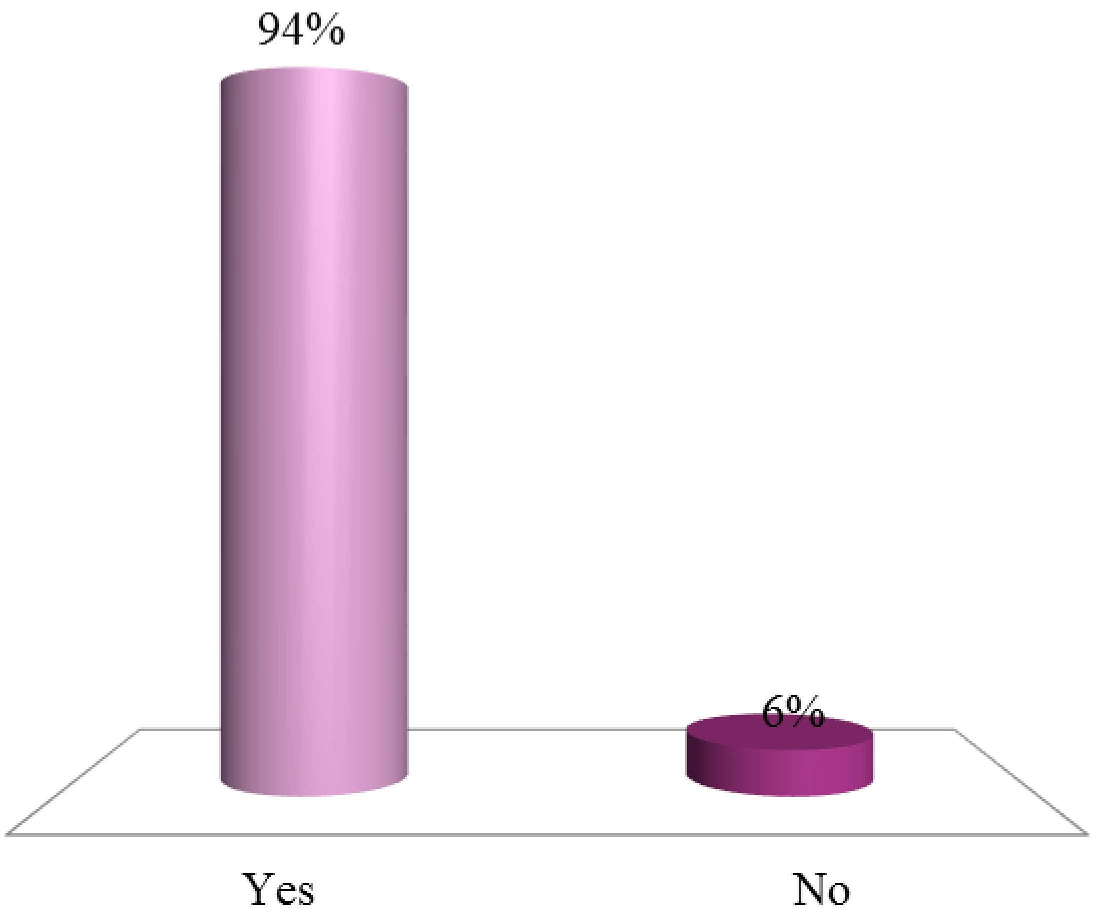




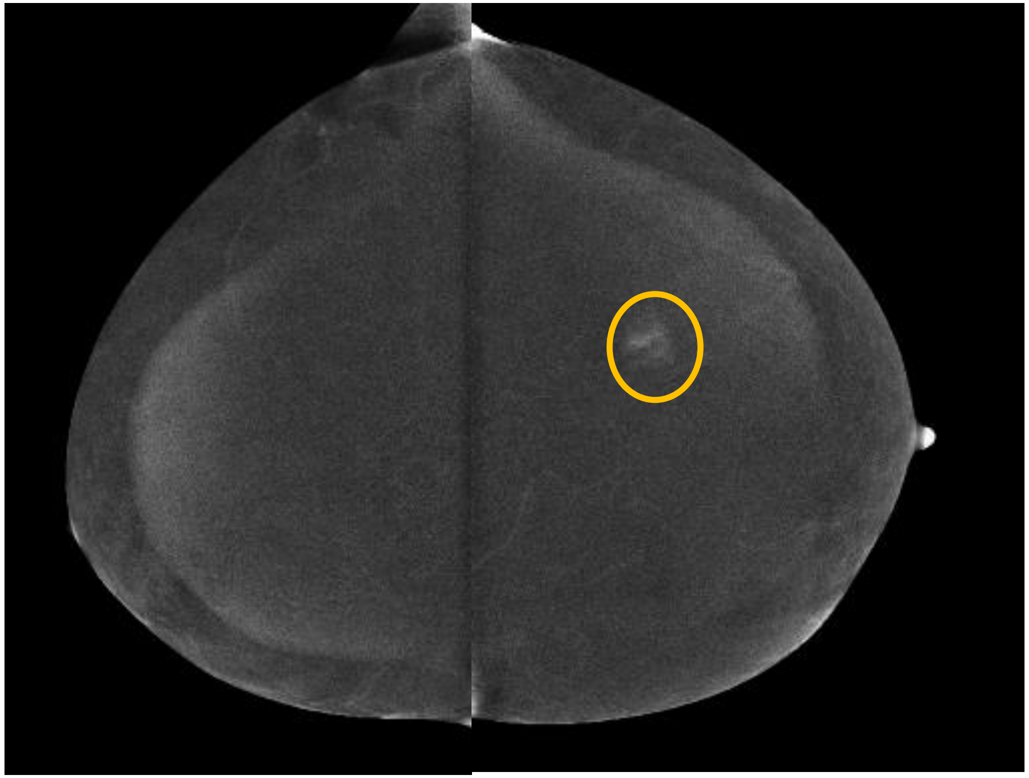


Do you see where the lesion is?

A. Yes
B. No



Angio mammography



Clinical case

•Imaging: confirmation of a single lesion without any suspicious lymph node

•Biopsy: Infiltrating ductal carcinoma, ER: 90%, PR: 80%, HER2- Ki67: 2%, grade I

•Lumpectomy + sentinel lymph node procedure: pT1cN0 in complete resection

•Adjuvant radiotherapy followed by hormonotherapy for 5 years

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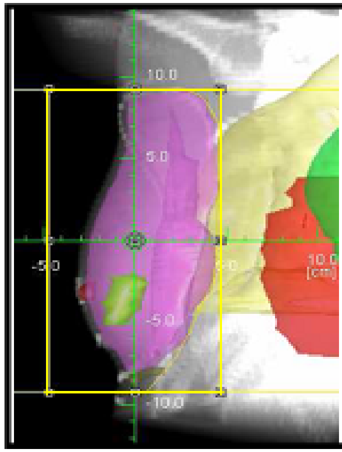
Therapeutic strategy: Which radiotherapy?

Two changing practice concepts have modified the standard whole breast irradiation 50Gy +/- boost



Hypo fractionated whole breast irradiation

Whelan NEJM 2010; START A and B Lancet Oncol 2008

Accelerated partial breast irradiation

Vaidya Lancet 2010; Bourgier IJROBP 2010 ; Lemanski IJROBP 2010; Taghian IJROBP 2005; Polgar IJROBP 2004 ; Vicini IJROBP 2003; Formenti IJROBP 2003;

Whole breast irradiation

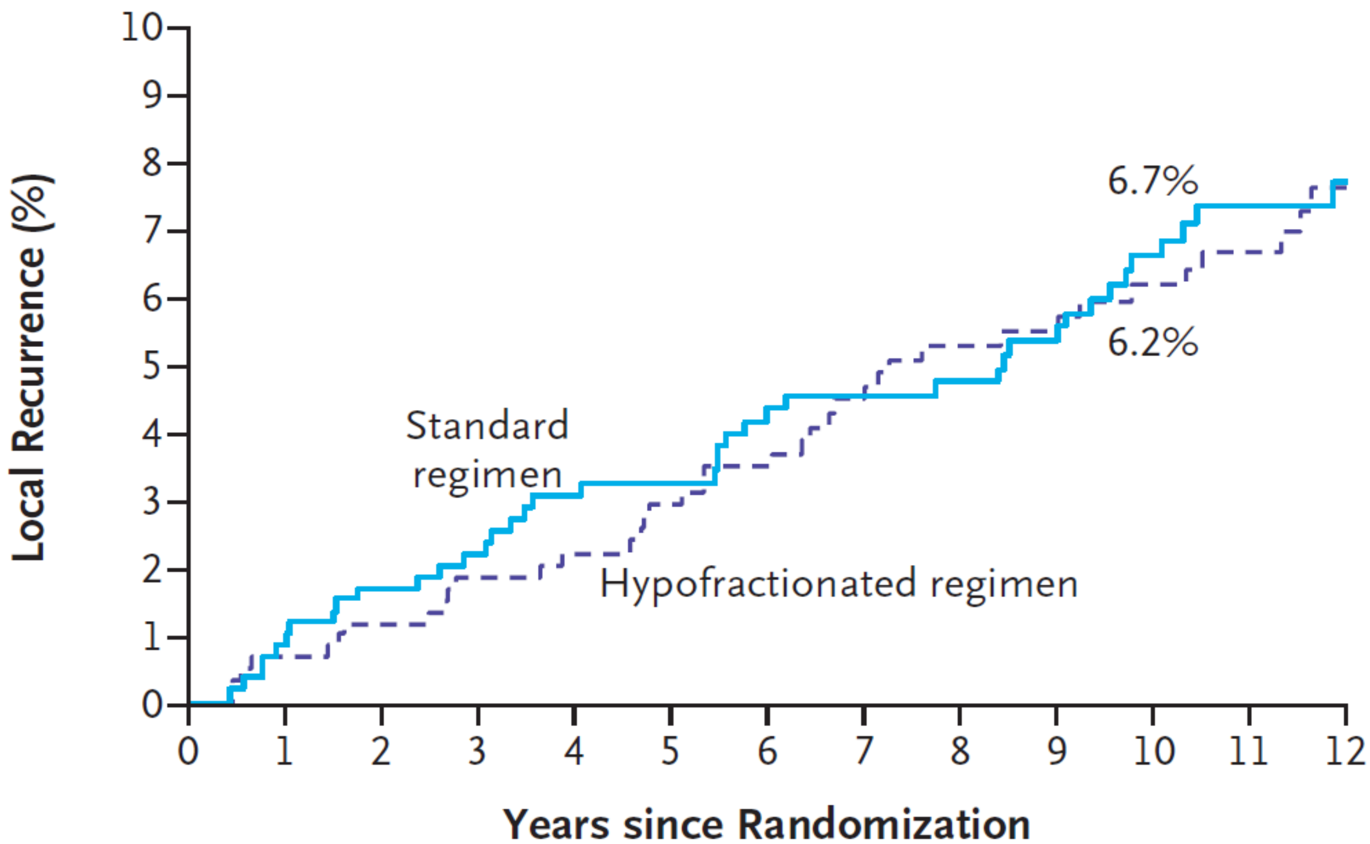
ORIGINAL ARTICLE

Long-Term Results of Hypofractionated Radiation Therapy for Breast Cancer

Timothy J. Whelan, B.M., B.Ch., Jean-Philippe Pignol, M.D., Mark N. Levine, M.D.,

N=1234

Short fractionated schedule	Long fractionated schedule
N=622	N=612
42.5Gy /16f	50Gy /25f



Whelan NEJM 2010

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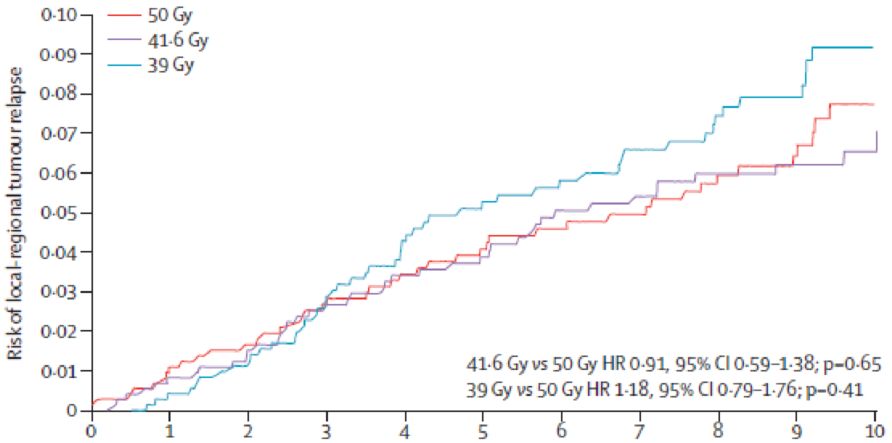
Whole breast irradiation

START A
2236 patients

50 Gy/25 fractions/ 5 weeks

41.6 Gy/13 fractions/ 5 weeks

39 Gy/13 fractions/ 5 weeks



Number at risk

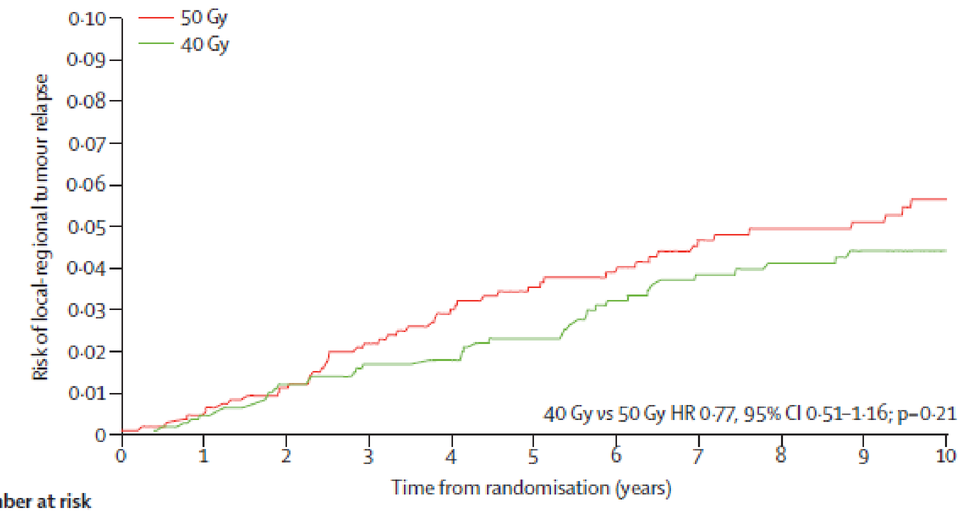
	0	1	2	3	4	5	6	7	8	9	10
50 Gy	749	725	702	674	645	607	563	534	470	368	196
41·6 Gy	750	732	710	689	662	623	574	547	501	408	206
39 Gy	737	724	702	668	631	583	540	500	452	362	184

Median follow up = 9,3 yrs
LRR-10y (50Gy) : 7,4% [5,5-10]

START B
2215 patients

50 Gy/25 fractions/ 5 weeks

40 Gy/15 fractions/ 3 weeks



Number at risk

	0	1	2	3	4	5	6	7	8	9	10
50 Gy	1105	1077	1047	1002	952	893	816	749	688	620	388
40 Gy	1110	1085	1055	1016	982	927	843	772	710	639	412

Median follow up = 9,9 yrs
LRR-10y (50Gy) : 5,5% [4.2-7,2]

JS Haviland; Lancet Oncol 2013

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Partial breast irradiation indication guidelines

ESTRO	ASTRO
• >50 years	• ≥60 years
• IDC, mucinous, tubular, medullary, and colloid cc.	• Invasive ductal or other favorable subtypes
• Associated LCIS allowed but not DCIS	• Pure DCIS not allowed
• Any grade, ER, PR	• ER status positive
• pT1–2 (⩽30 mm)	• pT1 : ≤2 cm
• Negative surgical margins (⩾2 mm)	• Negative surgical margins by at least 2 mm
• Unicentric, Unifocal	• Unicentric only, Clinically unifocal with total size ≤2.0 cm
• pN0 (by SLNB or ALND)	• pN0 (i^-, i^+) (by SLNB or ALND)

Polgar, Radiother Oncol 2010

Smith IJROBP 2009

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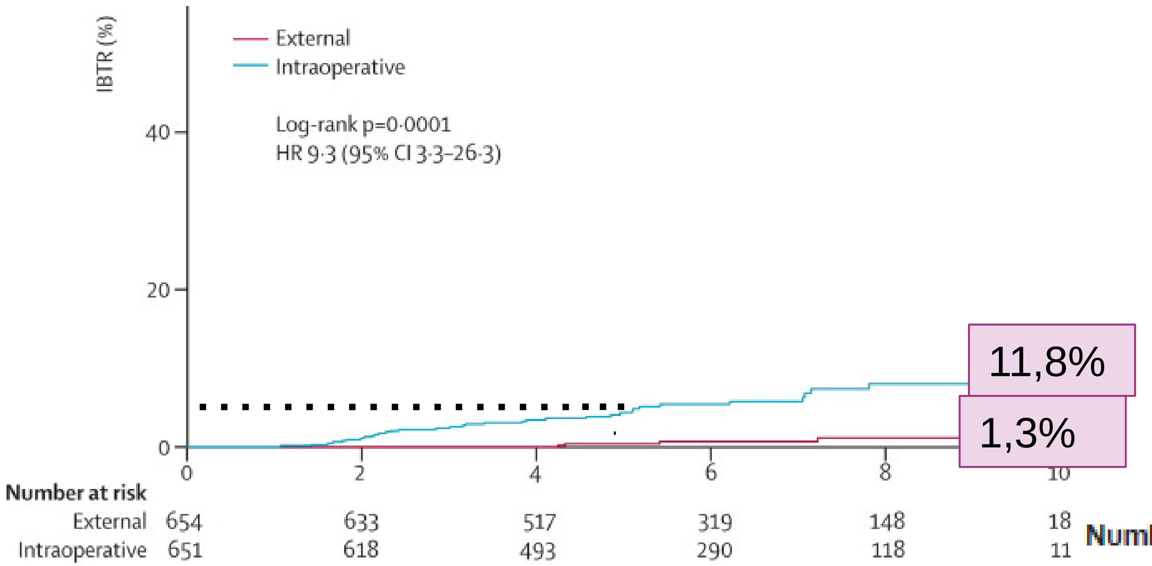
Intraoperative Partial breast versus whole breast irradiation

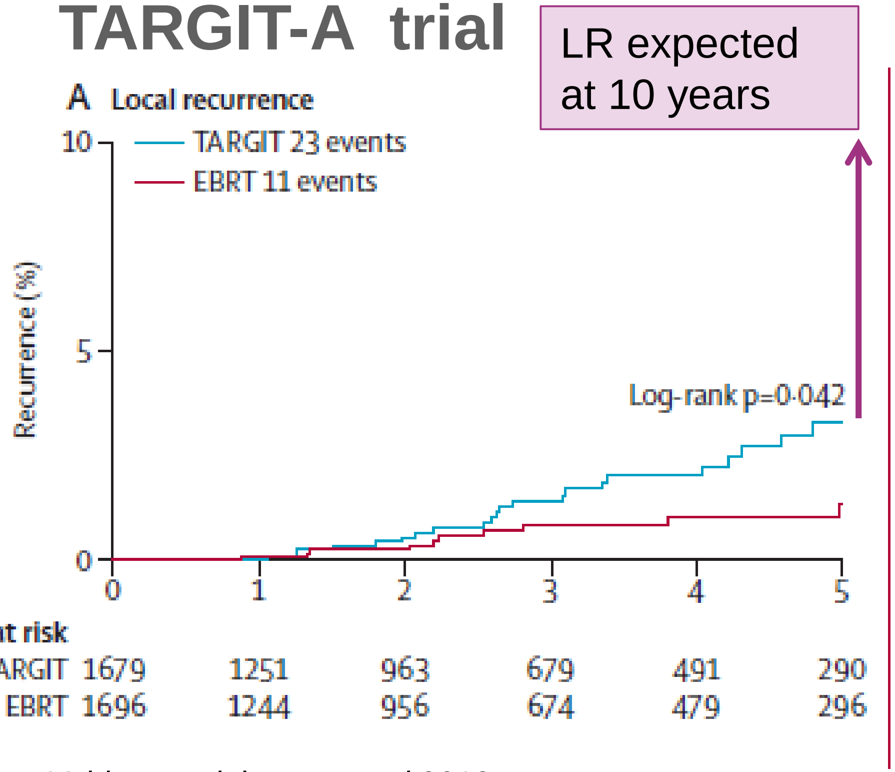
- Ipsilateral breast recurrence

ELIOT trial



Veronesi et al; lancet oncol 2013

TARGIT-A trial



Vaidya et al; lancet oncol 2013

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Radiotherapy and Oncology xxx (2012) xxx–xxx

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journal homepage: www.thegreenjournal.com

Special commentary

Has partial breast irradiation by IORT or brachytherapy been prematurely introduced into the clinic?

Harry Bartelink [a,*], Celine Bourgier [b], Paula Elkhuizen [a]

[a] *Netherlands Cancer Institute, The Netherlands;* [b] *Institut Gustave Roussy, France*

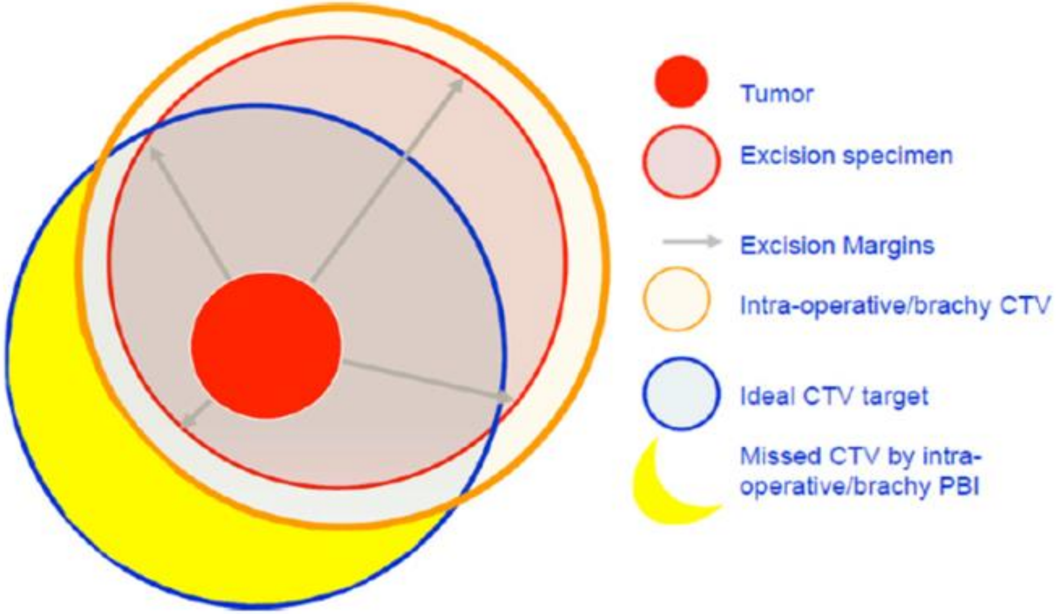
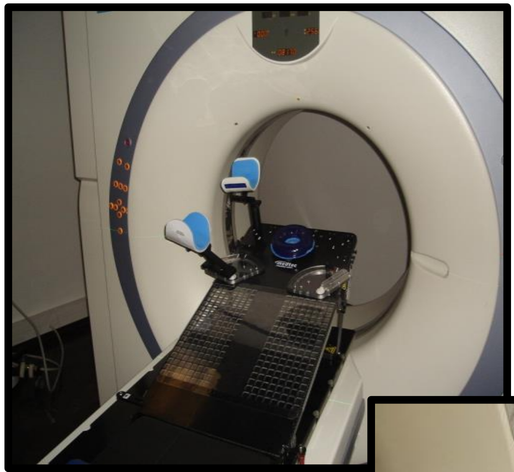
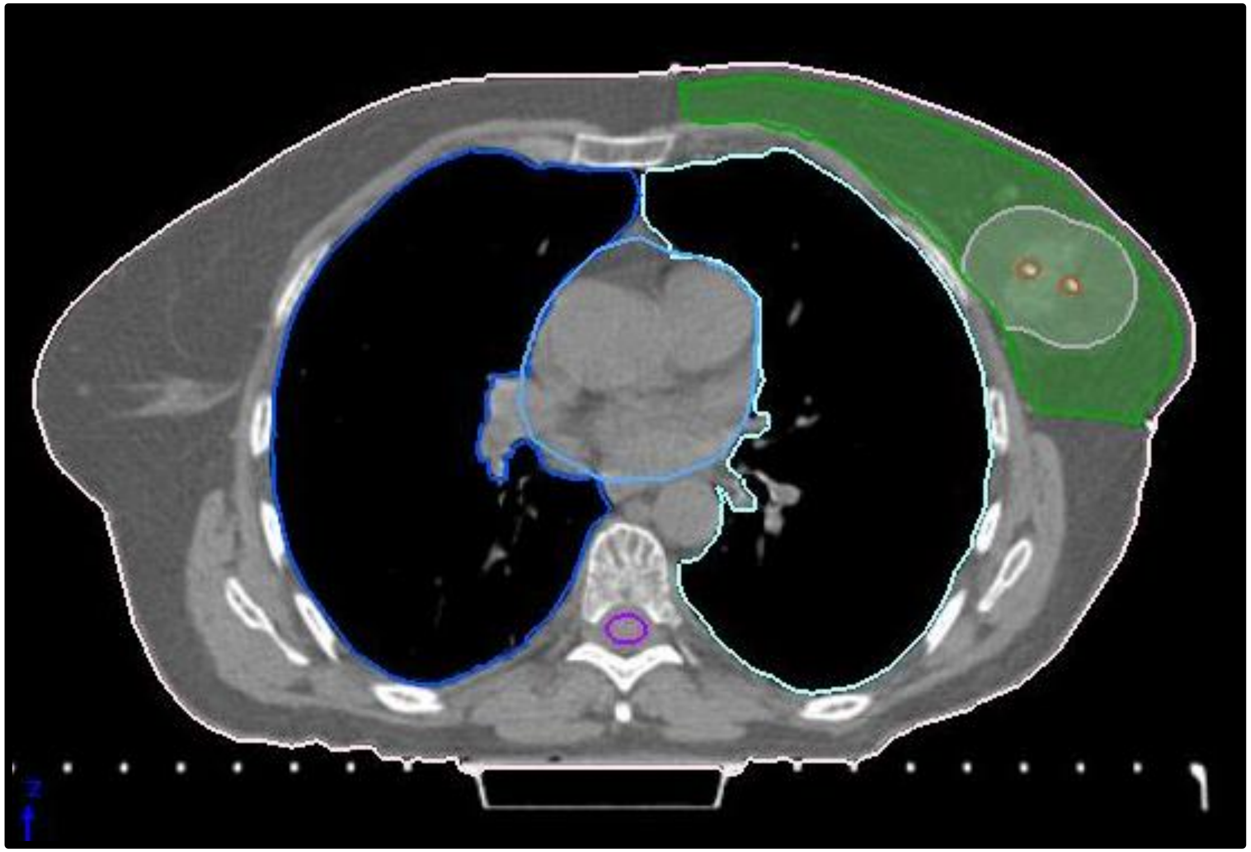


Fig. 1. Breast tumors are often eccentric located with highest risk of residual tumor in the region of the narrowest resection margin, therefore CTV by brachy or IORT is not covered.

EBRT allows for conformal treatment

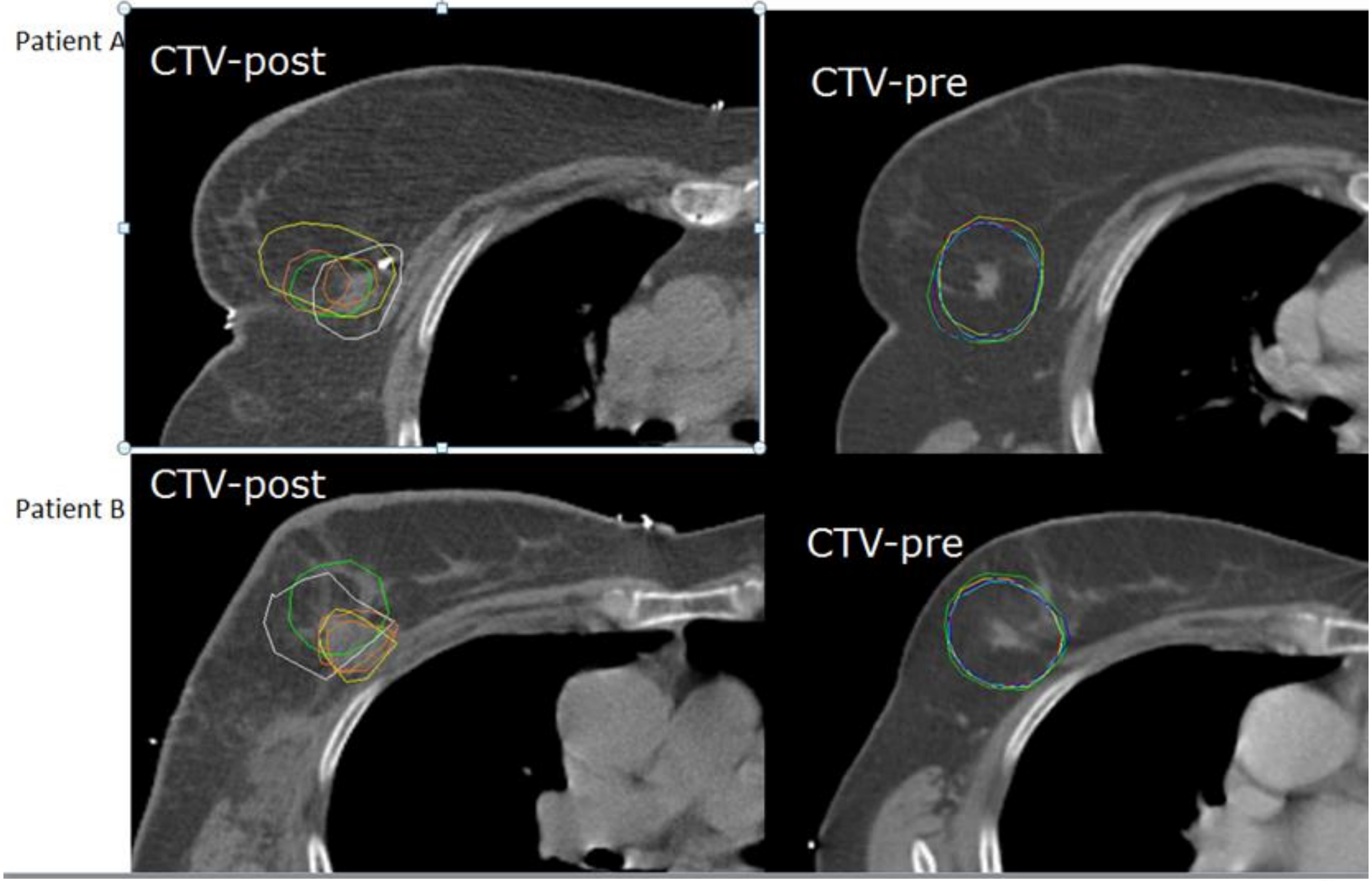
- In pre operative or post operative (several ongoing trials)
- Positioning and contouring are essential : more risks to miss the target!



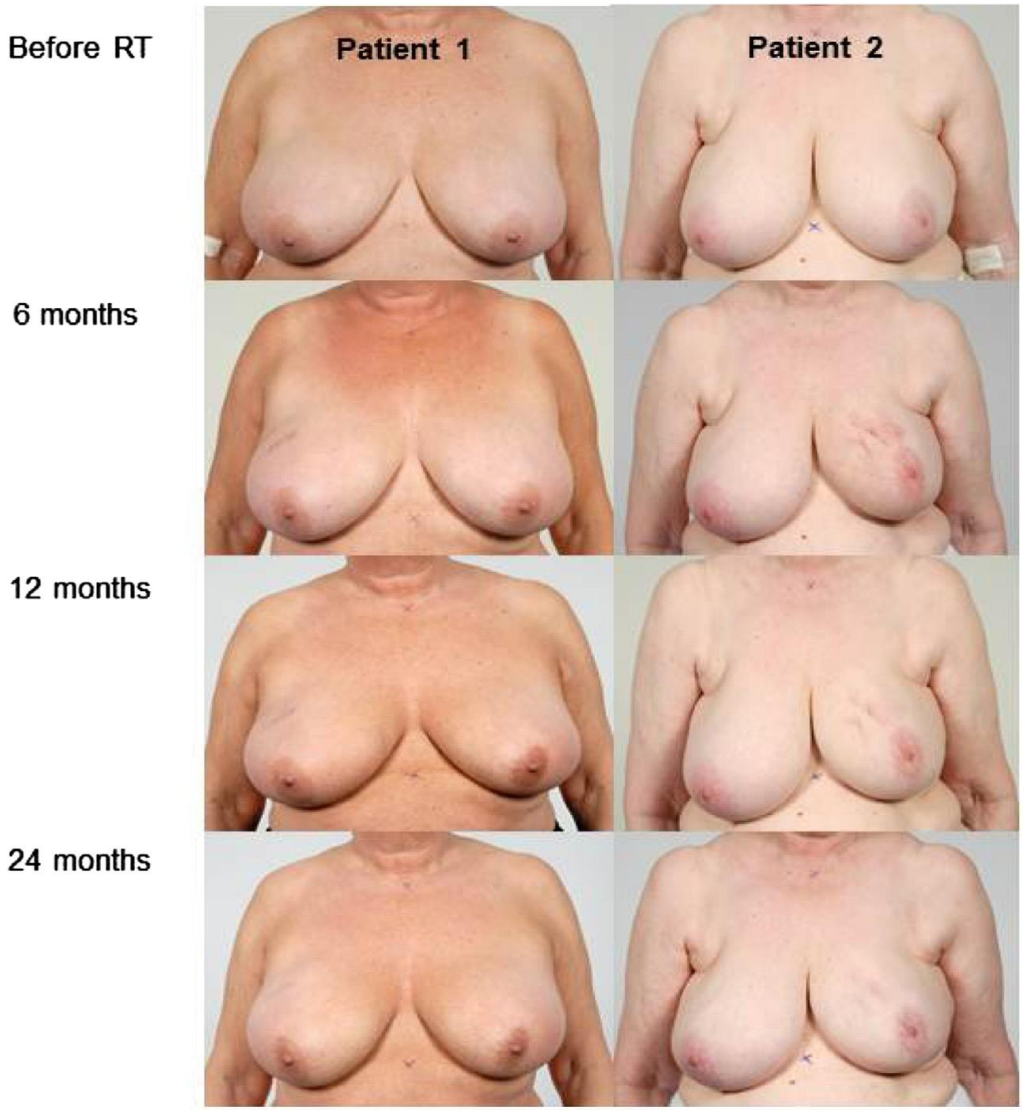


Preop. vs postop. delineation

van der Leij et al *Radiother Oncol* 2014



PAPBI: first résults

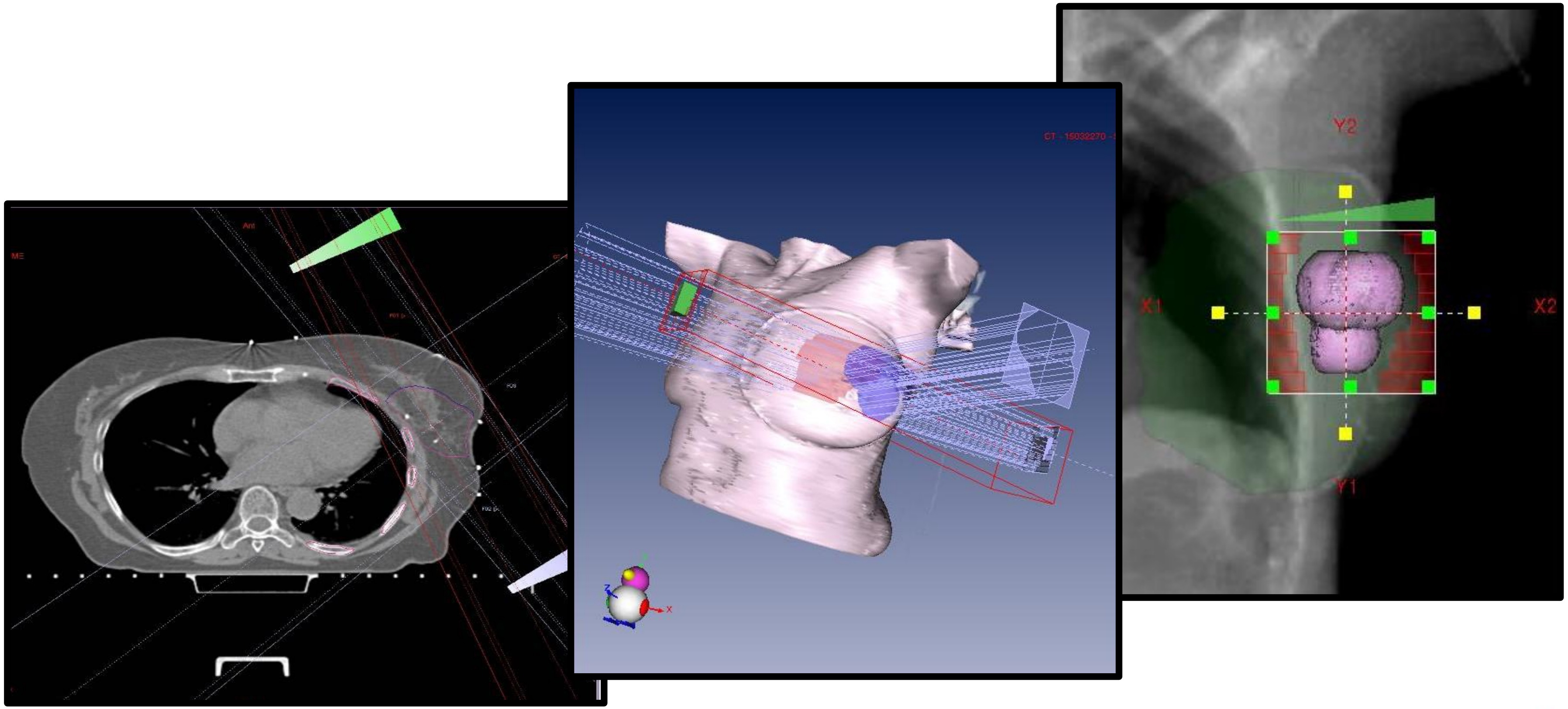


F. Van Der Leij, Radiot Oncol 2015

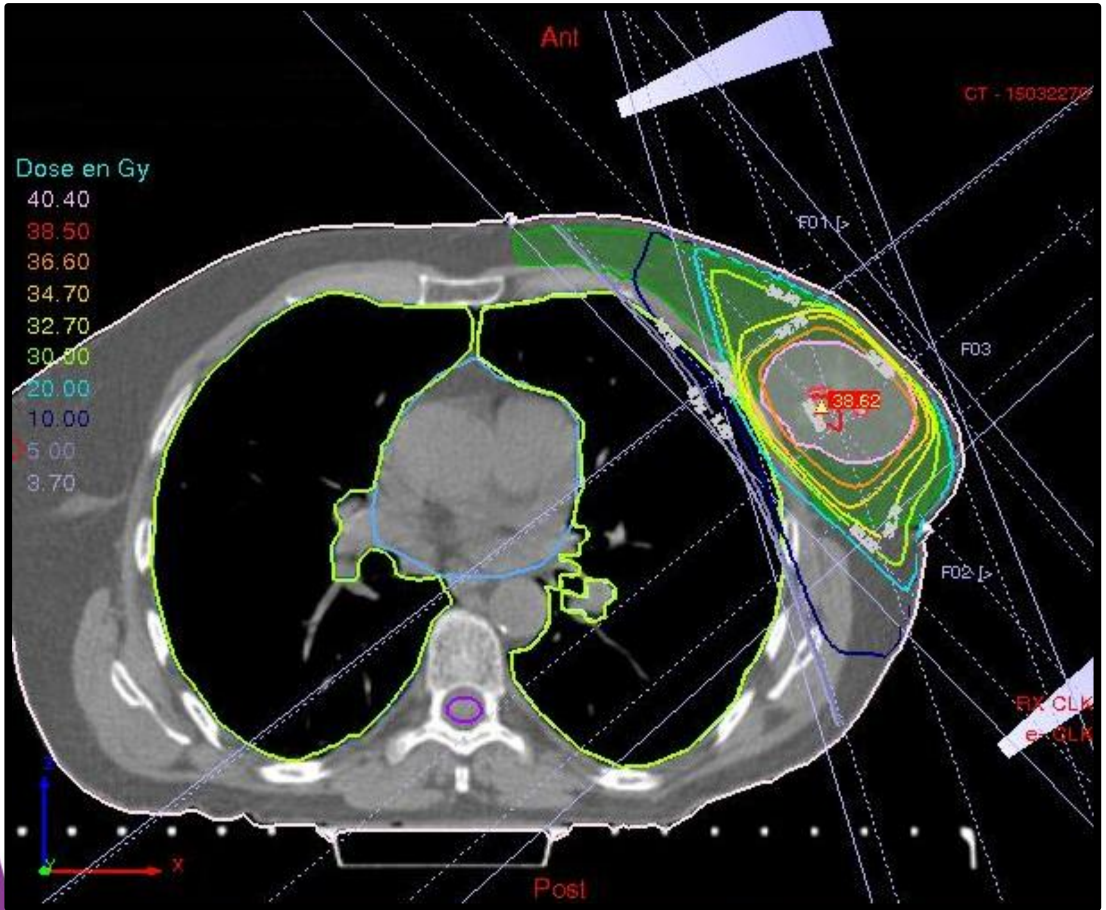
Dosimetry

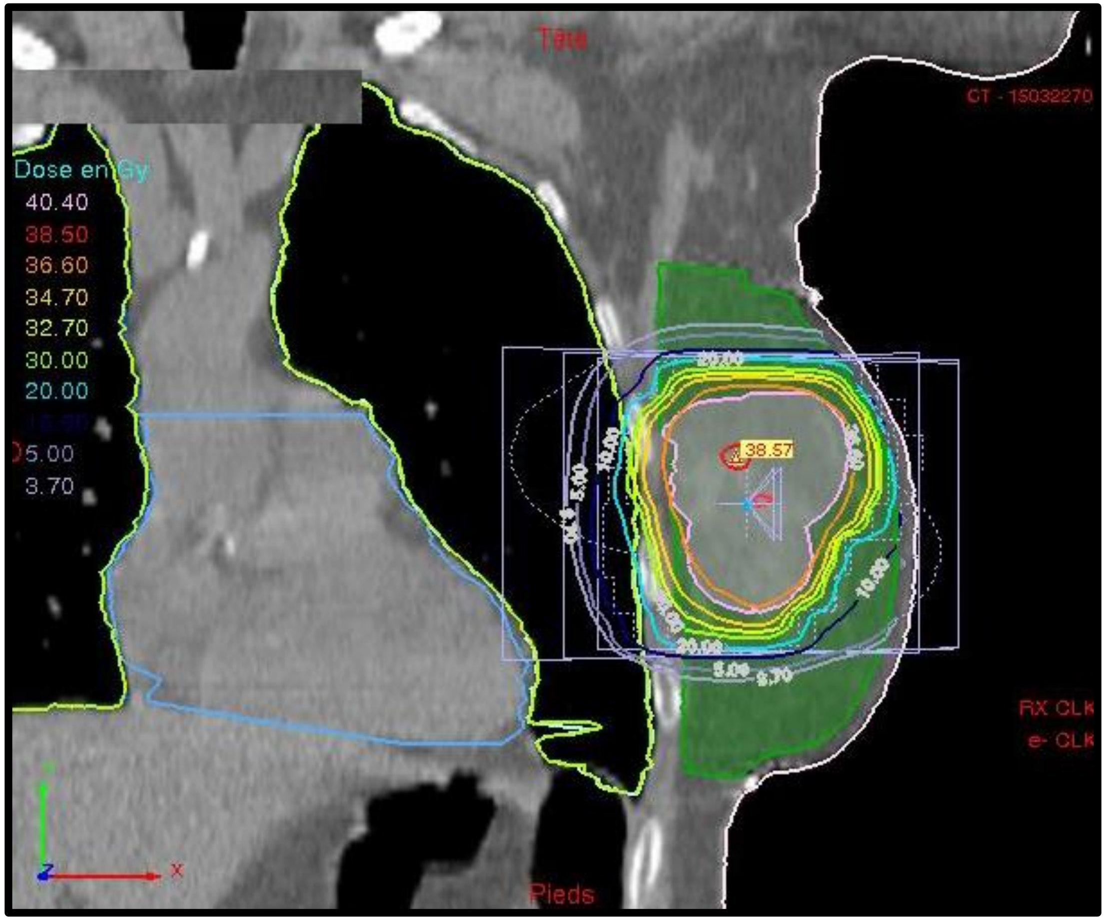
Technique used in routine at Gustave Roussy:

- 2 tangential 6MV photon beam
- 1 direct electron beam



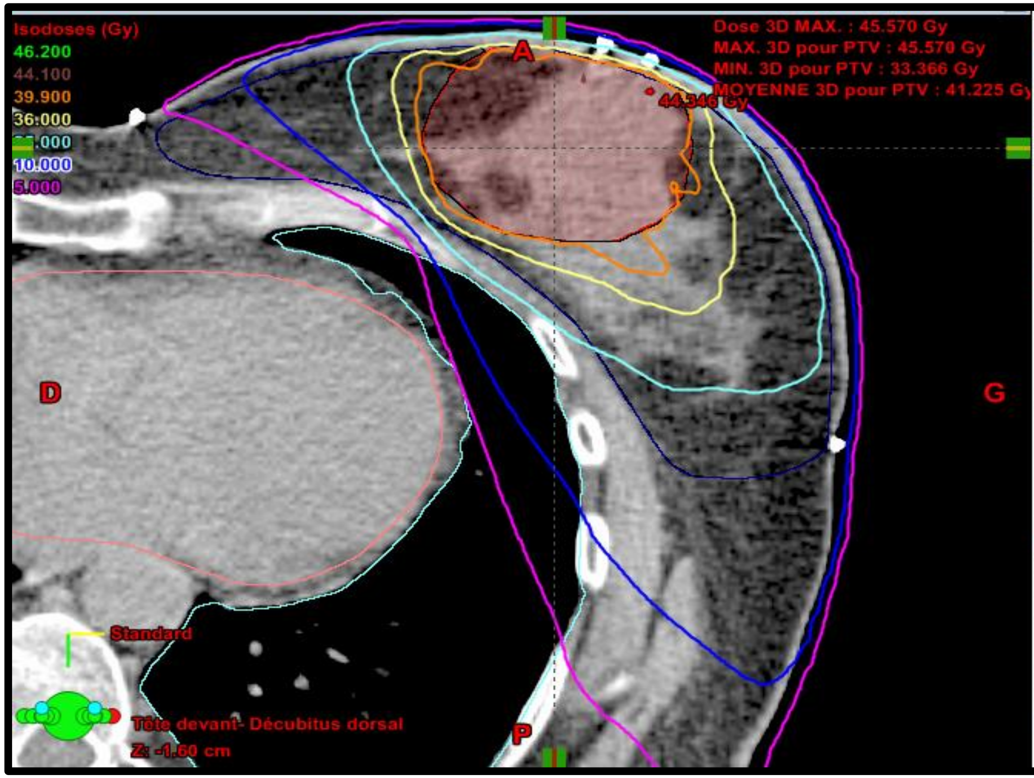
Dosimetry

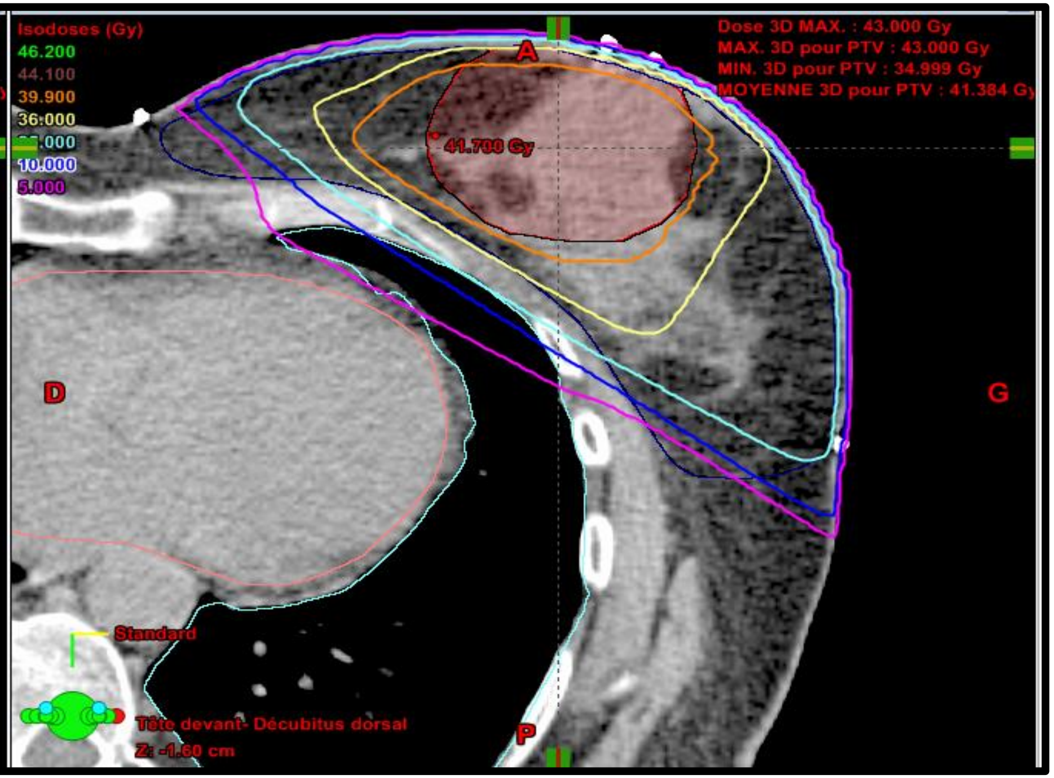

Ant
CT - 15032270
Dose en Gy
40.40
38.50
36.60
34.70
32.70
30.00
20.00
10.00
5.00
3.70
F01
F03
F02
38.62
RX CLK
e- CLK
x
Post


Tête
CT - 15032270
Dose en Gy
40.40
38.50
36.60
34.70
32.70
30.00
20.00
5.00
3.70
38.57
RX CLK
e- CLK
x
Pieds

Dosimetric comparision between APBI

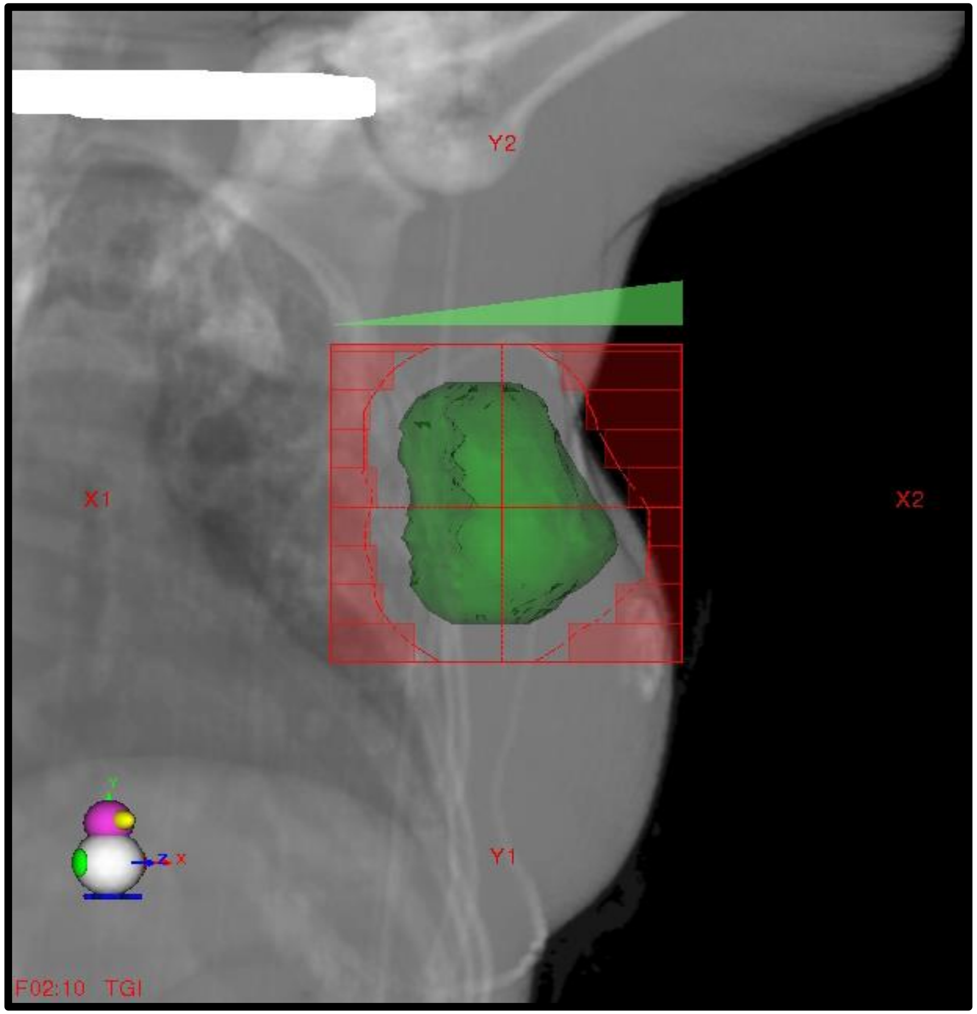
Rapidarc technique	3D conformal with photons and electrons

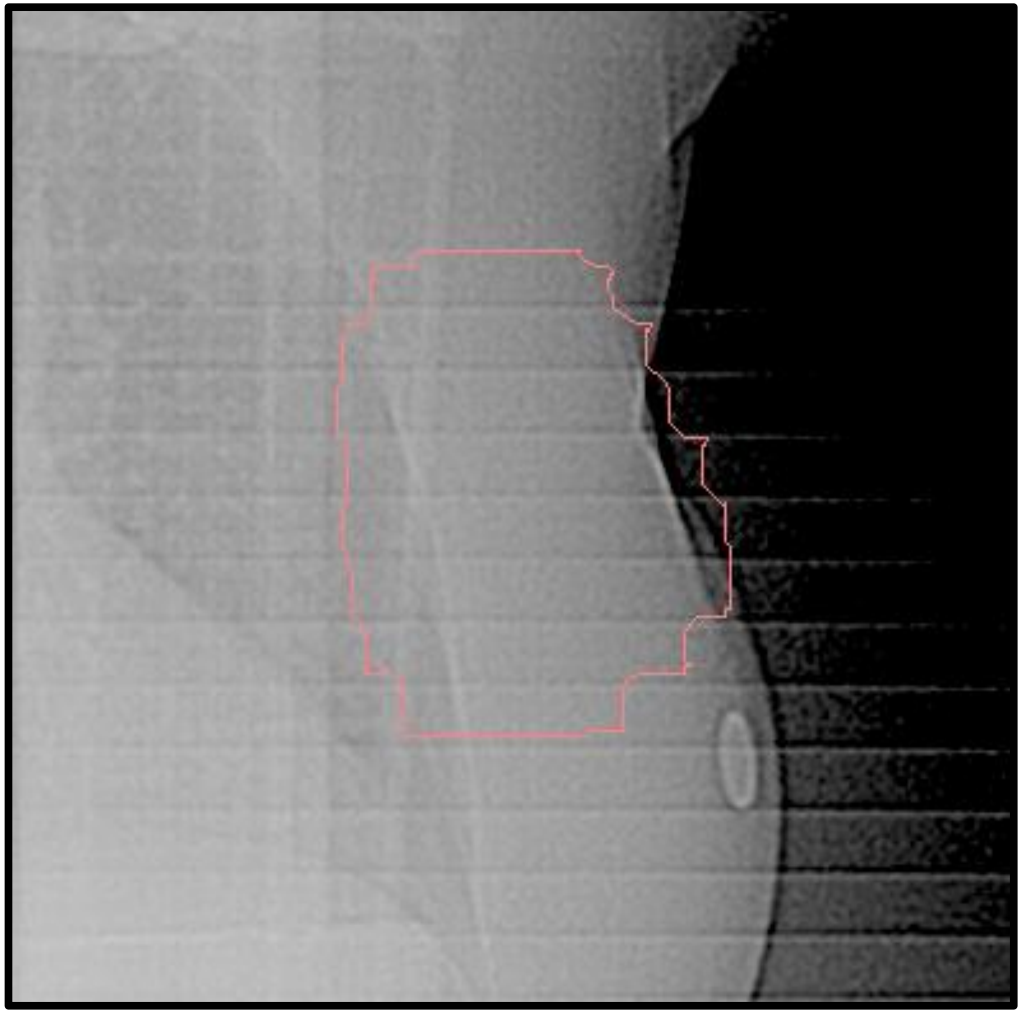




Advantages	Drawbacks
Lower heart dose	Higher hot spot
Lower whole breast dose	Increased low doses to lung

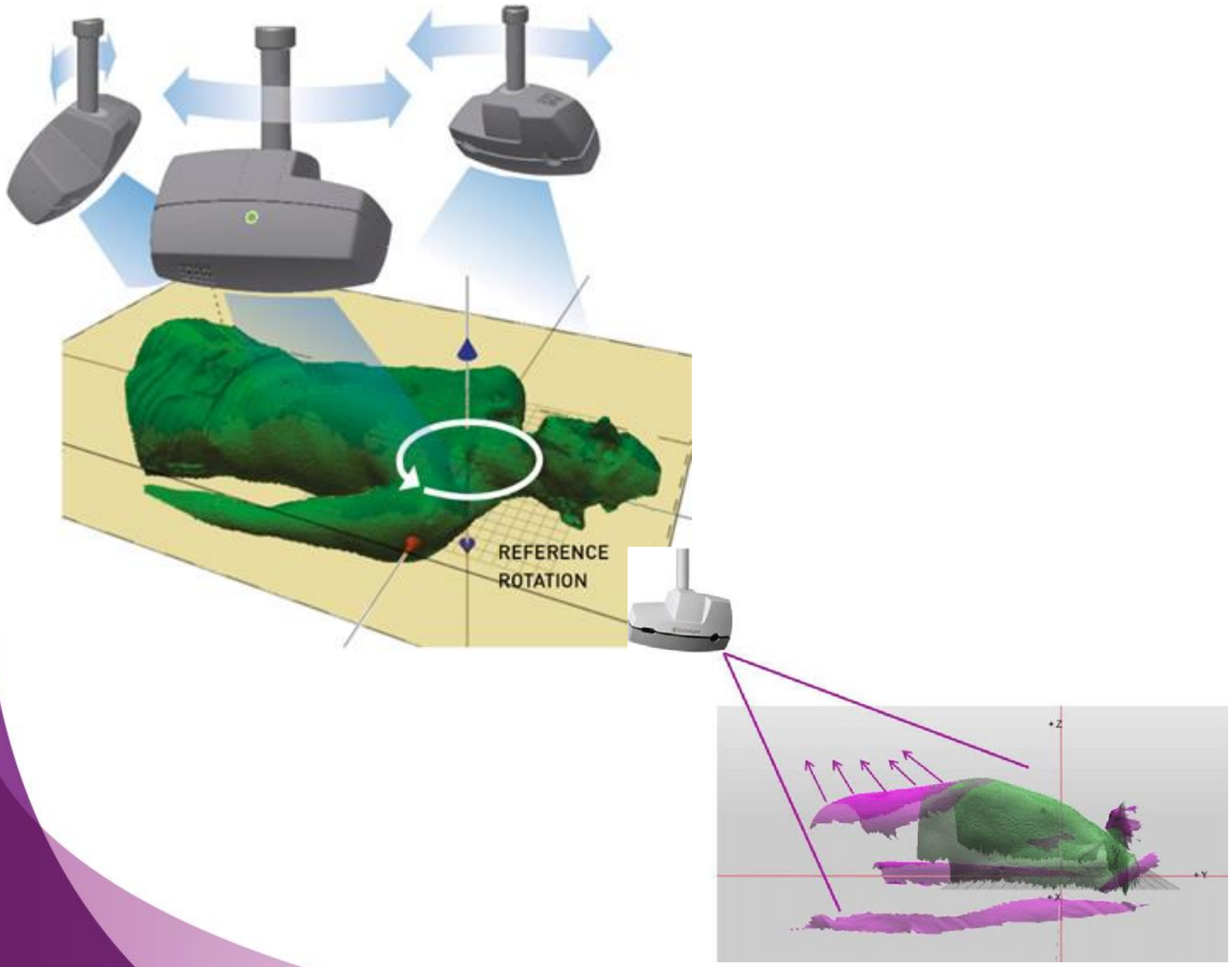
Re-positioning control

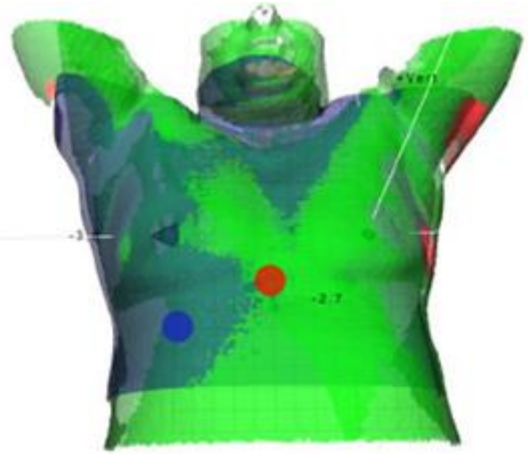


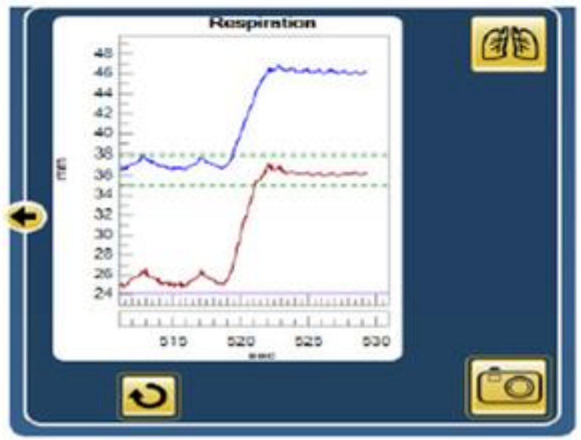


Positioning control

- Ex: C-RAD Catalyst system

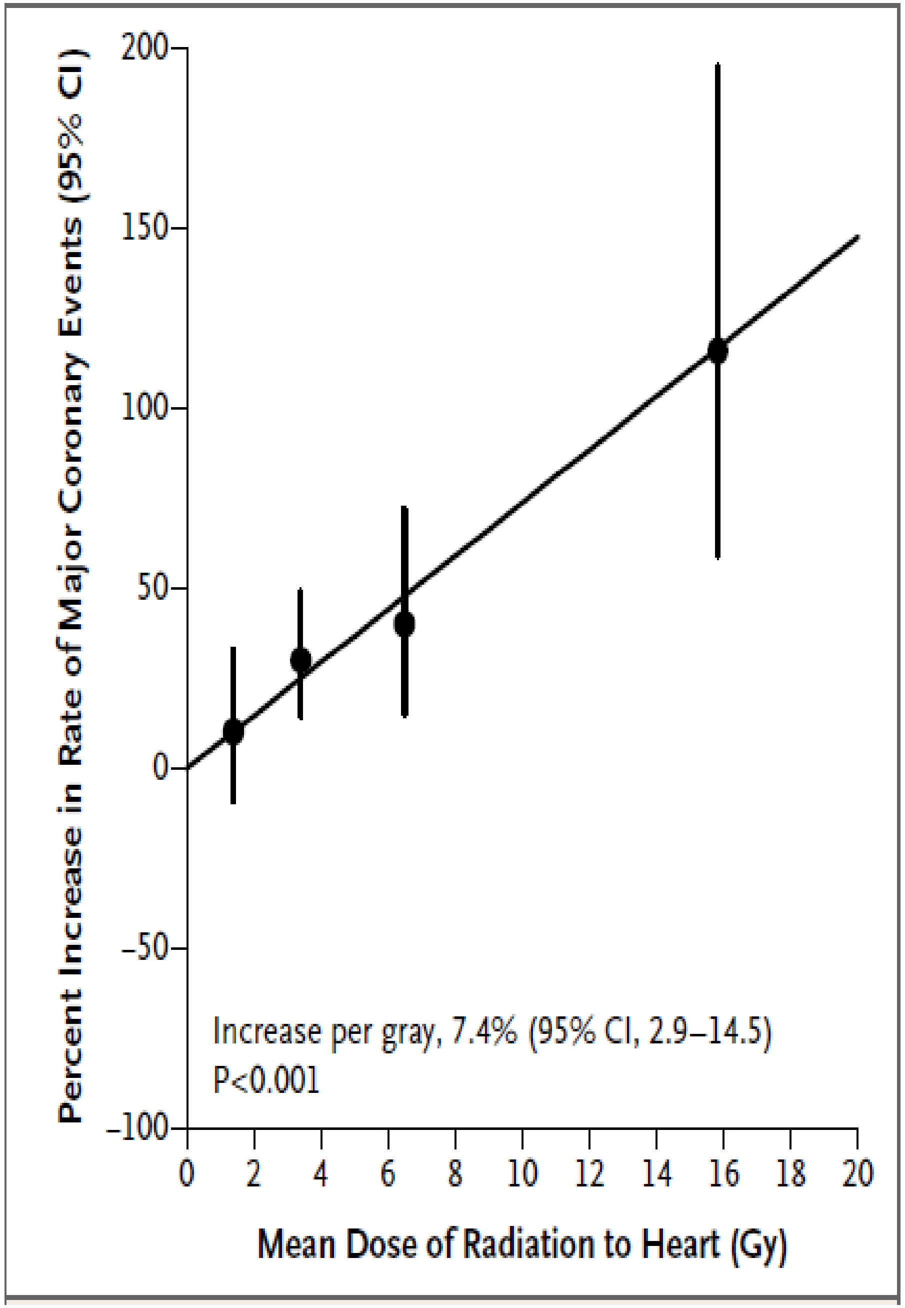






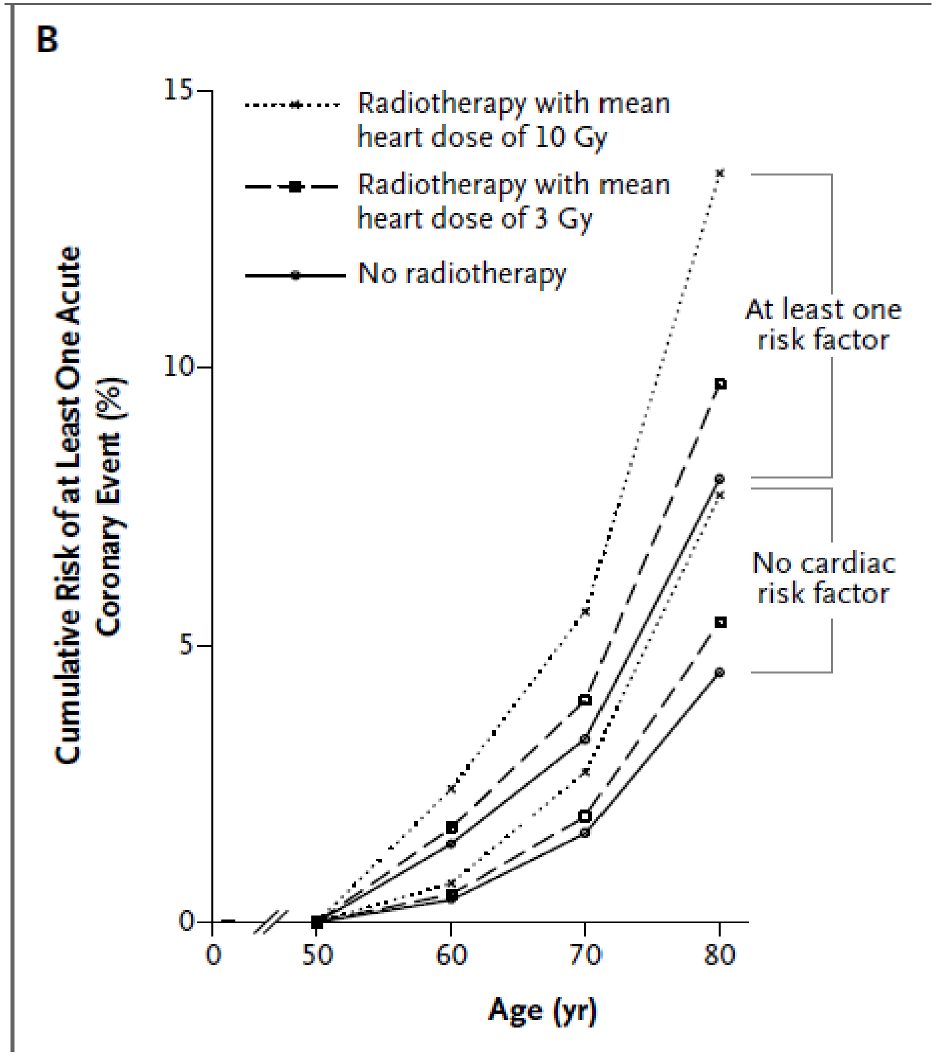
Heart Toxicity

- “The overall average of the mean doses to the whole heart was 4.9 Gy (range, 0.03 to 27.72). Rates of major coronary events increased linearly with the mean dose to the heart by 7.4% per gray (95% confidence interval, 2.9 to 14.5; P<0.001), with no apparent threshold. The increase started within the first 5 years after radiotherapy and continued into the third decade after radiotherapy. The proportional increase in the rate of major coronary events per gray was similar in women with and women without cardiac risk factors at the time of radiotherapy”



Darby NEJM 2013

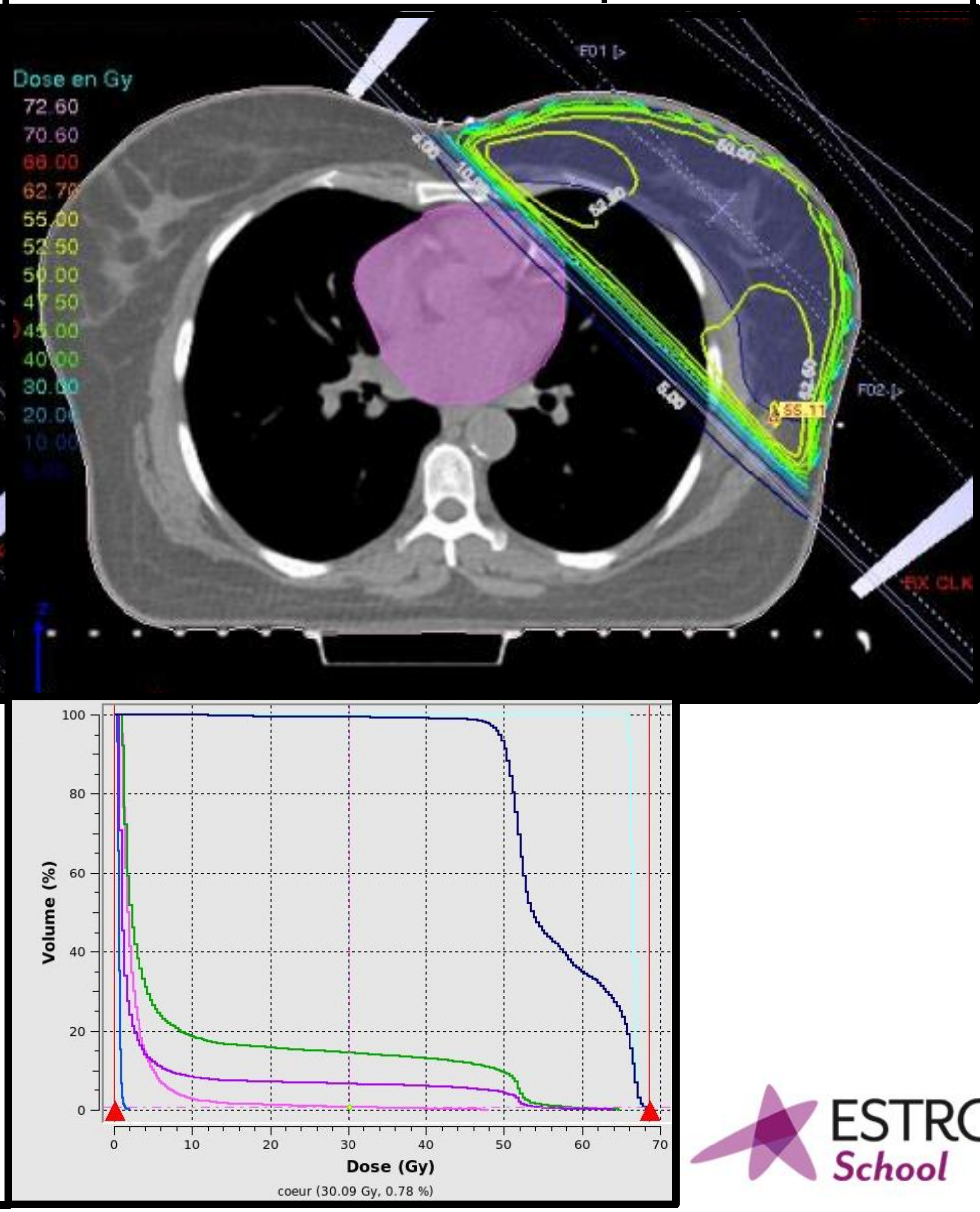
Cardiac risk is increased by cardiovascular risk factors



Darby NEJM 2013

Improved heart sparing by breath hold

Free breathing	Breath hold inspiration



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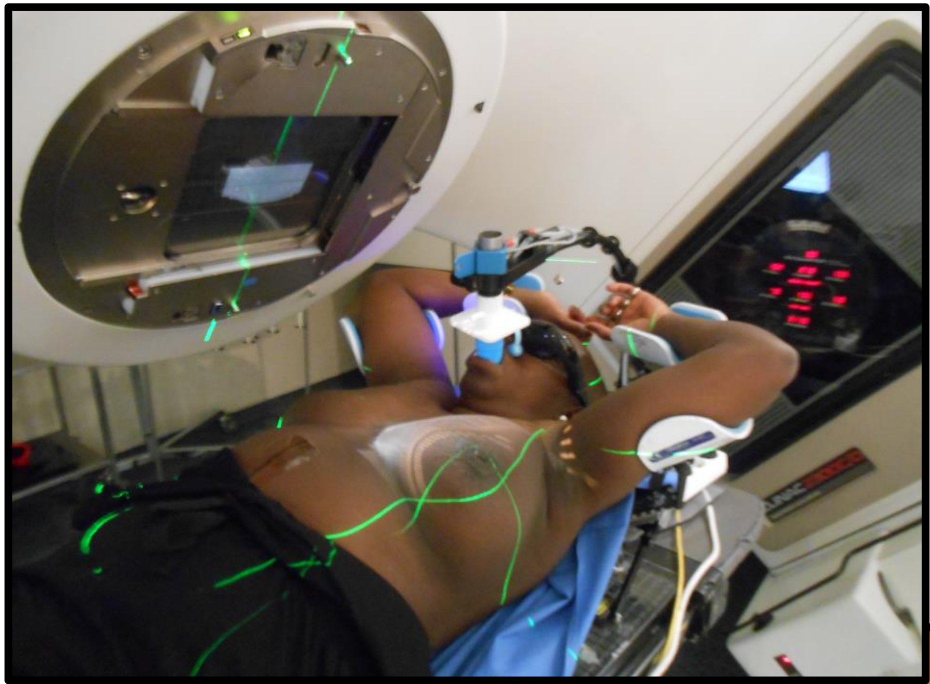
How to improve heart sparing?



- Inspiration breath hold technique

Take home messages:

- Accelerated hypofractionated whole breast and partial breast irradiation are changing our practices for early breast cancers with good prognosis factors

- Contouring and positioning remain key points for these treatment strategies

- Moving toward better sparing OAR means we need to assess low dose consequences as well

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WWW.ESTRO.ORG/SCHOOL

Breast case – Physics or metaphysics?

Peter Remeijer
Department of Radiation Oncology
The Netherlands Cancer Institute

NETHERLANDS CANCER INSTITUTE
ANTONI VAN LEEUWENHOEK

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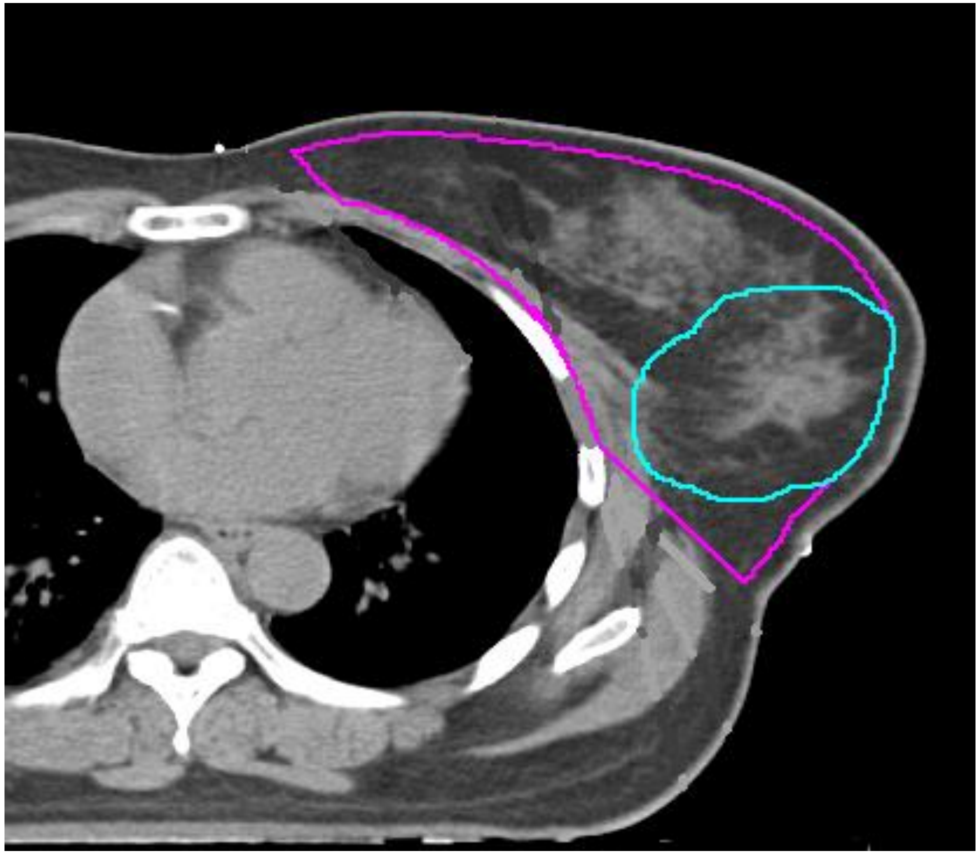
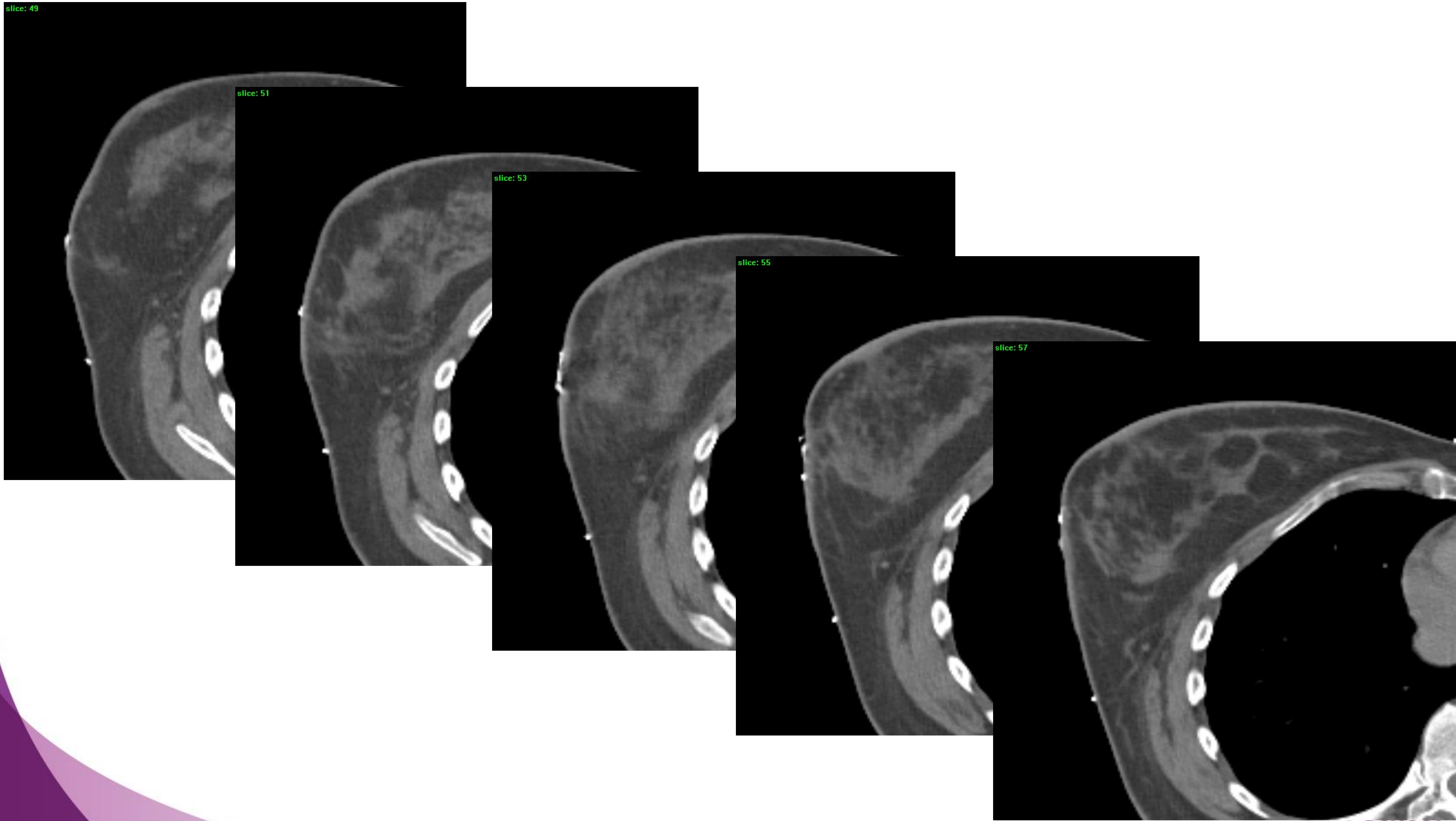
Common target volumes



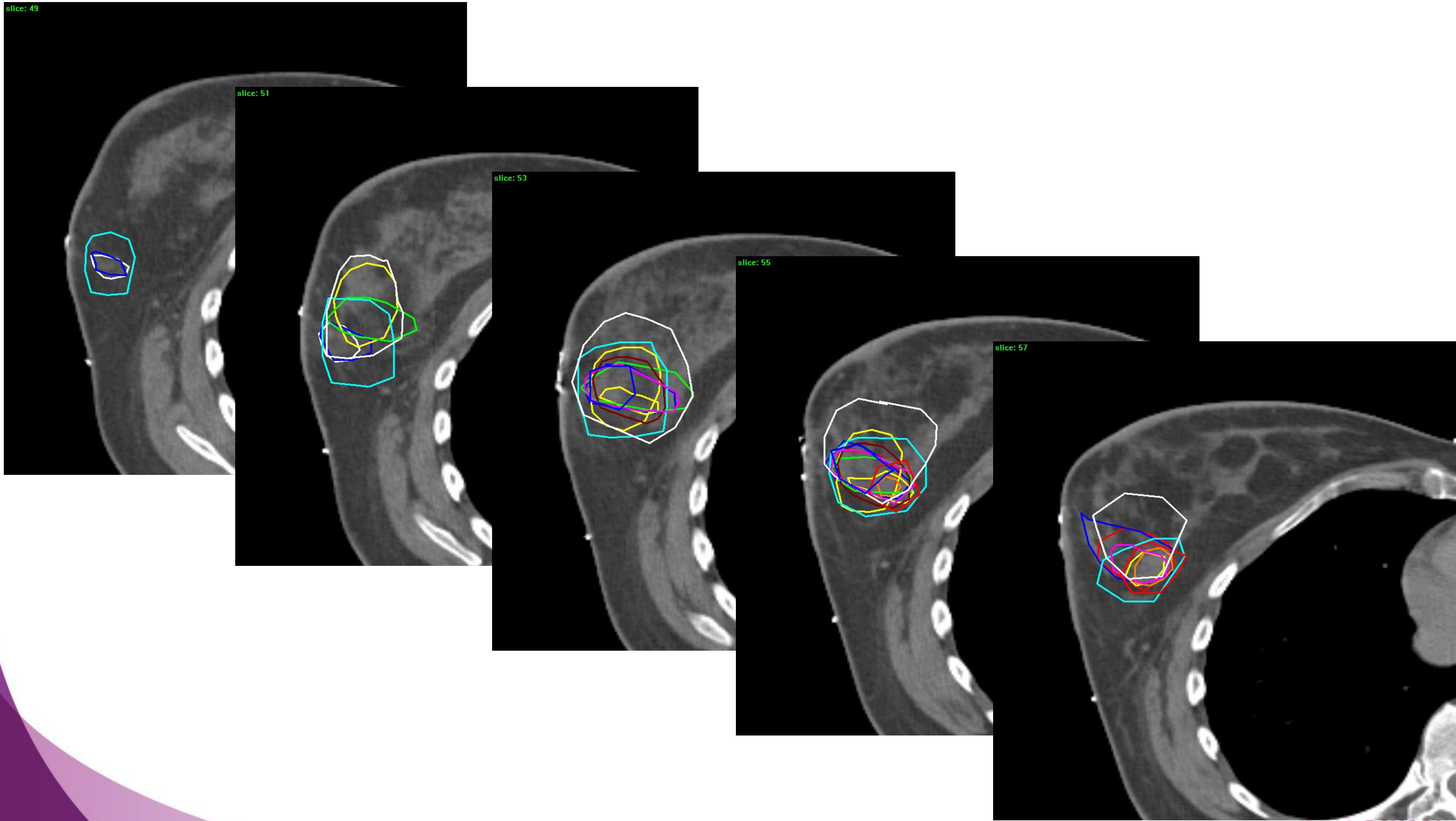
Whole breast (50 Gy)

Excision cavity (16 Gy)

Target volume delineation - variability



Target volume delineation - variability

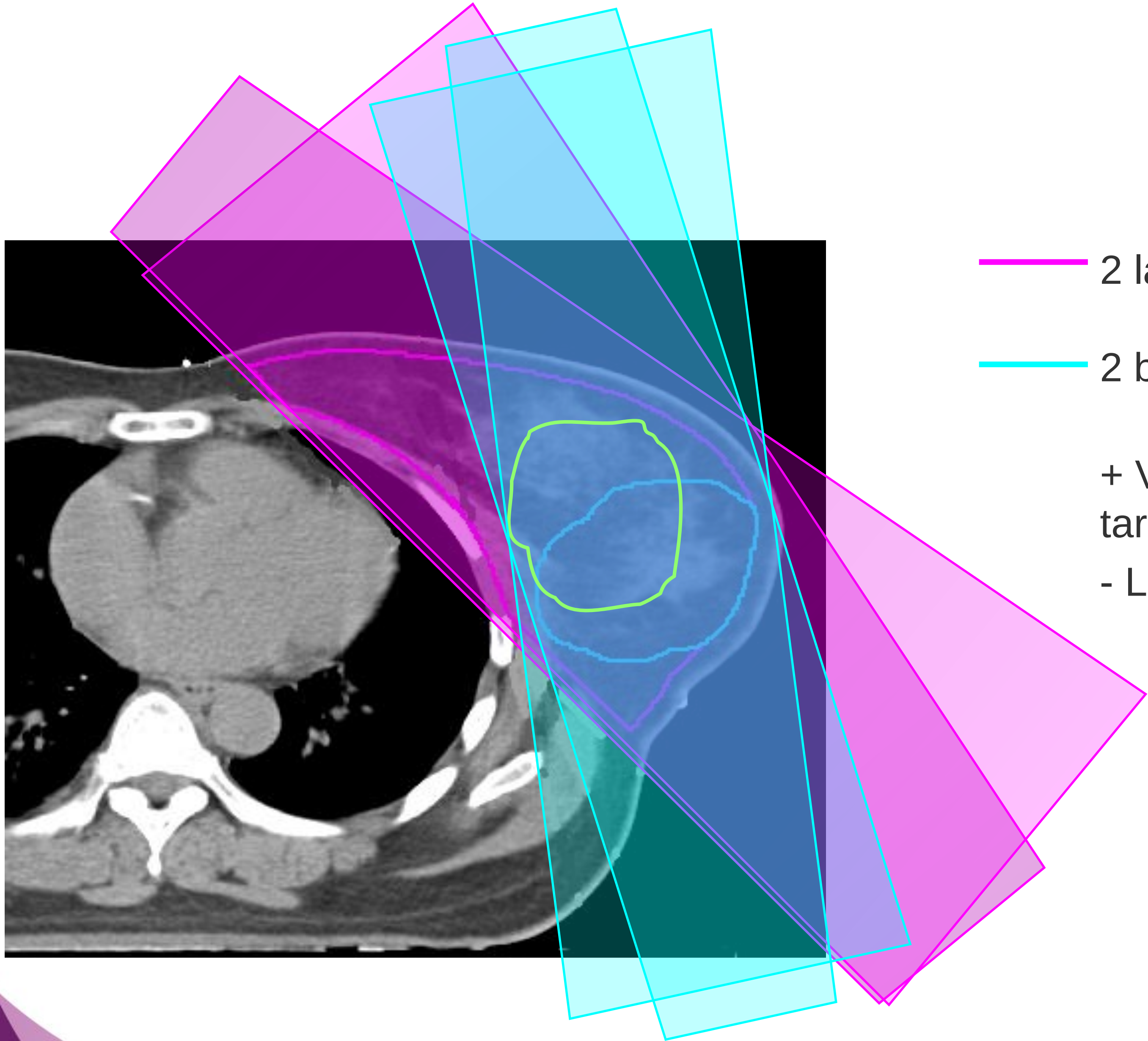


Target volume delineation - variability

- Possible causes
  - Different opinion of the clinicians
  - Image quality

- Possible solutions
  - Clear protocols, good collaboration between OR, Pathology, RT
  - Markers
  - Registration of pre-and post-op imaging (difficult!)
  - Multiple modalities

Treatment planning – Typical beam set-up



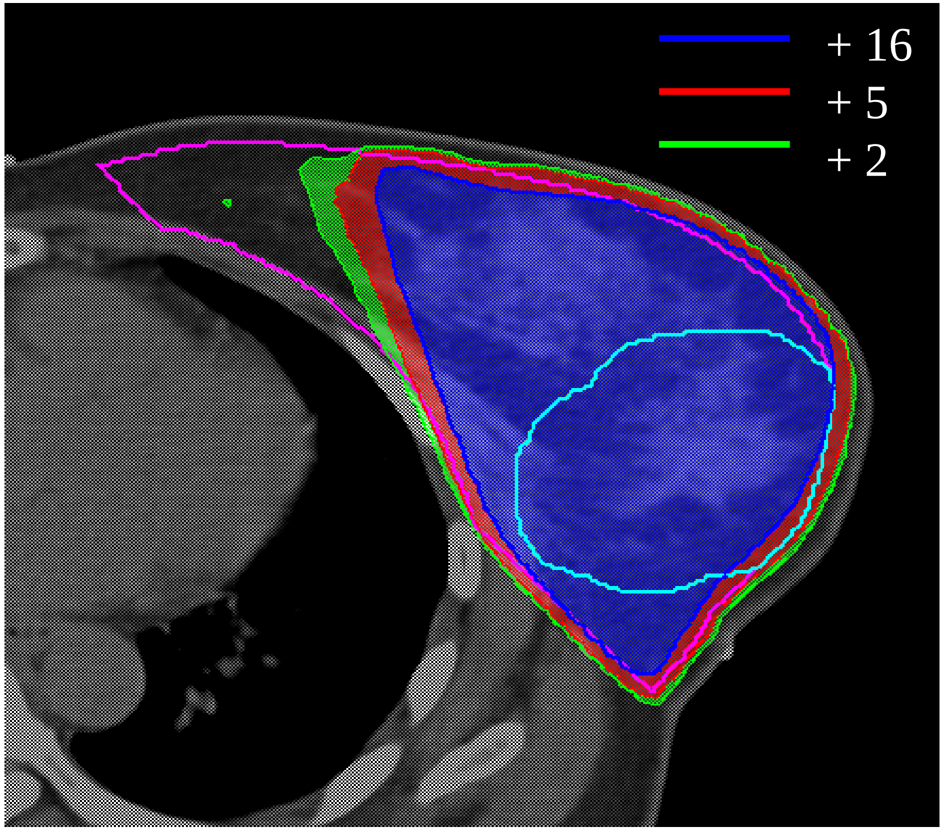
2 large fields for whole breast (50Gy)

2 boost fields for additional dose (16Gy)

+ Very insensitive to exact position of target volume

- Large volume irradiated to boost dose

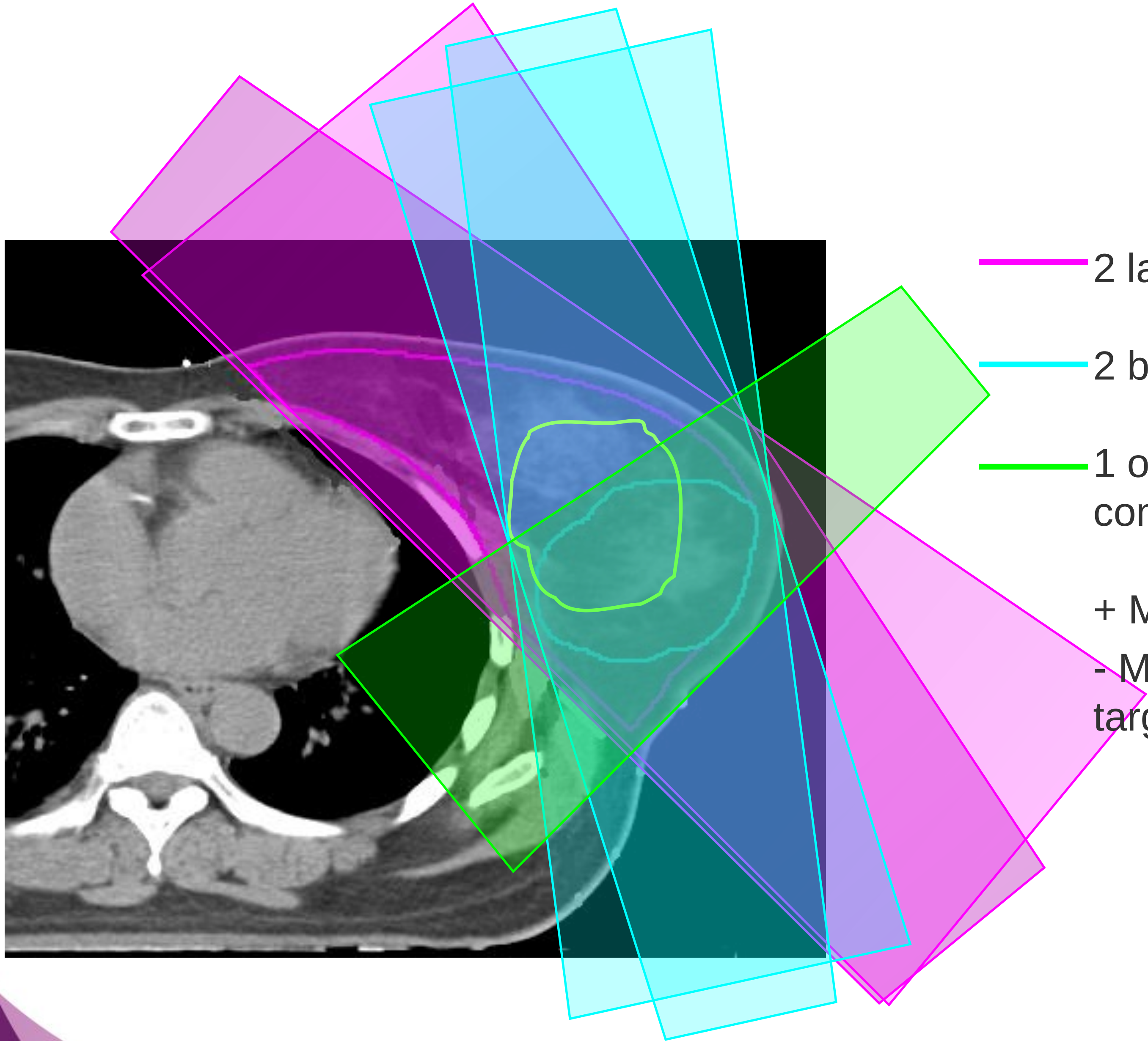
Treatment planning – Typical beam set-up



+ Very insensitive to exact position of target volume

- Large volume irradiated to boost dose

Treatment planning – Typical beam set-up



2 large fields for whole breast (50Gy)

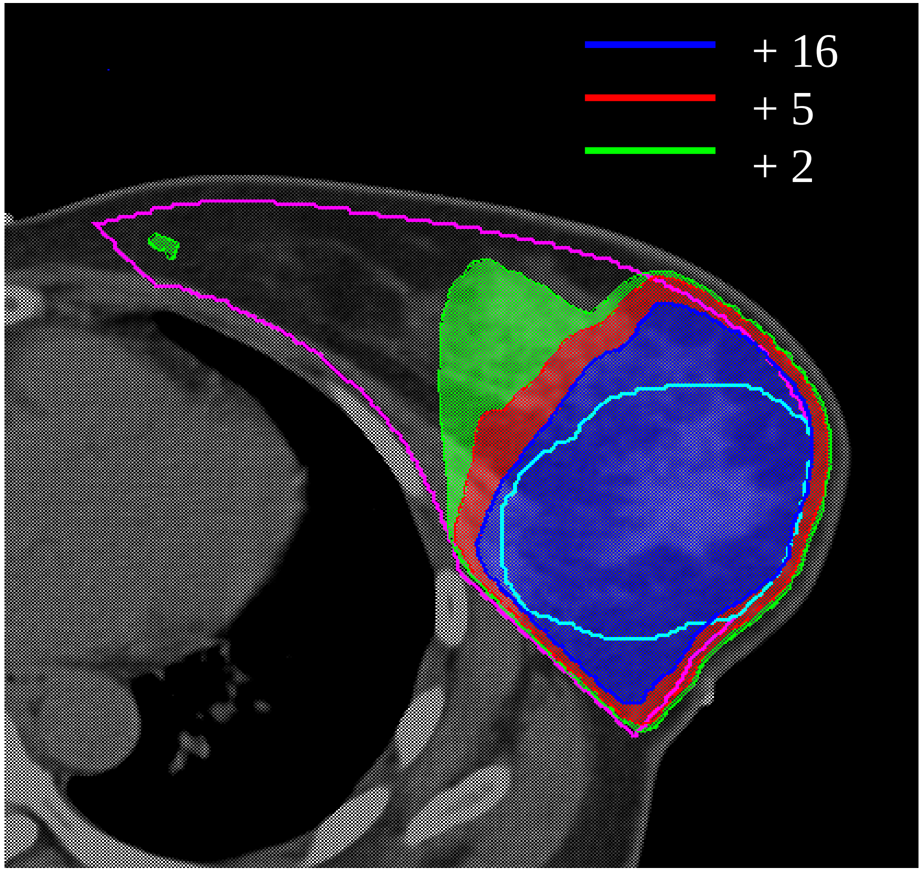
2 boost fields for additional dose (16Gy)

1 orthogonal beam to improve conformance

+ Much smaller high dose volume

- More sensitive to exact position of target volume

Treatment planning – Typical beam set-up



+ Much smaller high dose volume

- Sensitive to exact position of target volume

→ Image guidance / position verification

Changes during treatment

Setup errors

	No-correction$_{meas}$				Offline$_{meas}$			
	CBCT				CBCT			
		CC	LR	AP		CC	LR	AP
Σ (mm)		3.8	3.1	2.5		1.7	1.4	1.2
σ (mm)		2.8	2.2	2.6		3.1	2.3	3.0
$2.5\Sigma + 0.7\sigma$ (mm)		11.5	9.2	8.0		6.4	5.2	5.1

Seroma changes

- Possibly occurs after breast sparing surgery
- Fluid in excision cavity

- Boost is generally based on this seroma volume

T. Alderliesten, S. den Hollander[1], J. Yang[2], P. Elkhuizen[1], A. van Mourik[1], C. Hurkmans, C v. Vliet

Seroma changes

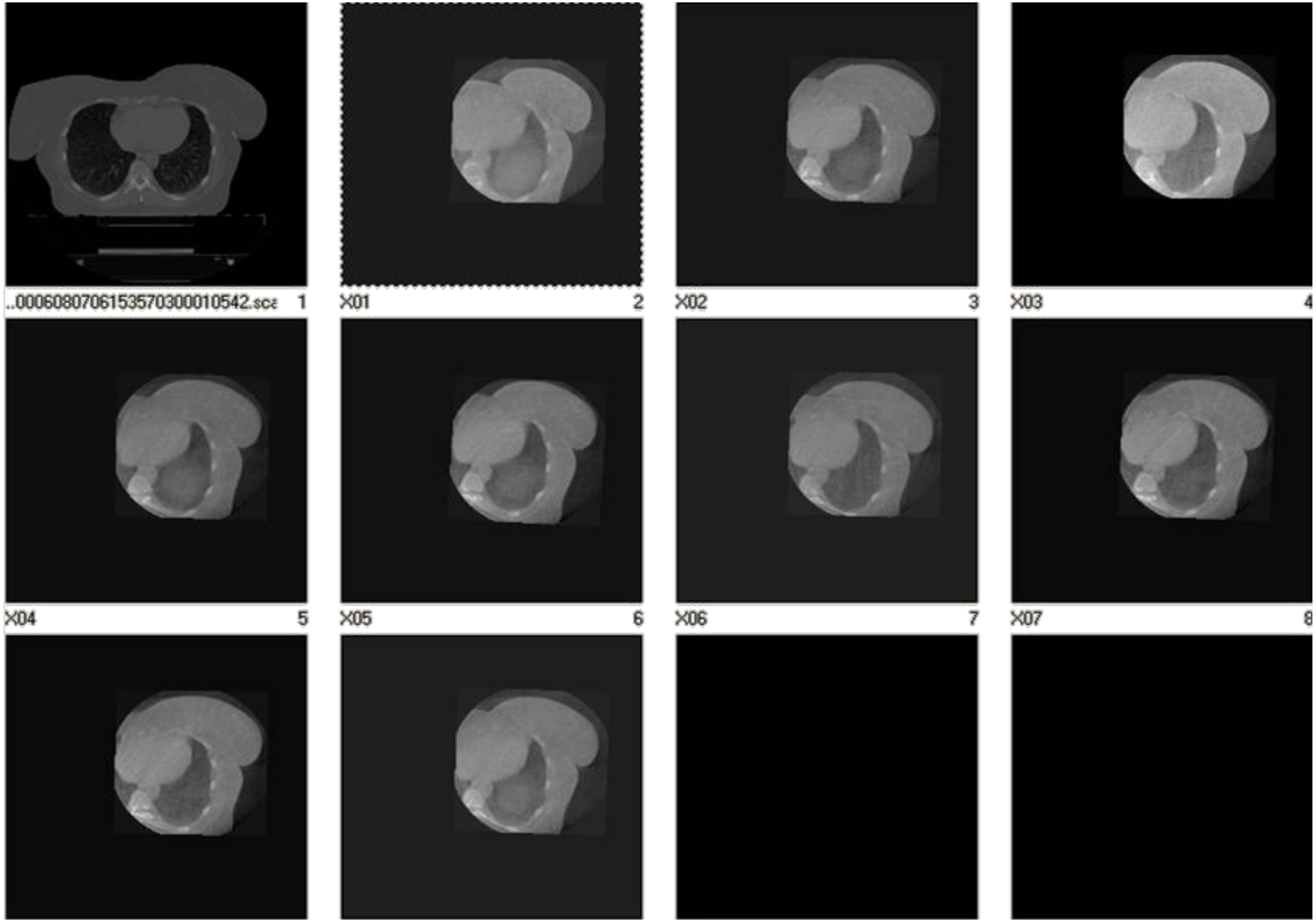
- Seroma shrinkage

Planning CT

Repeat CT (during treatment)

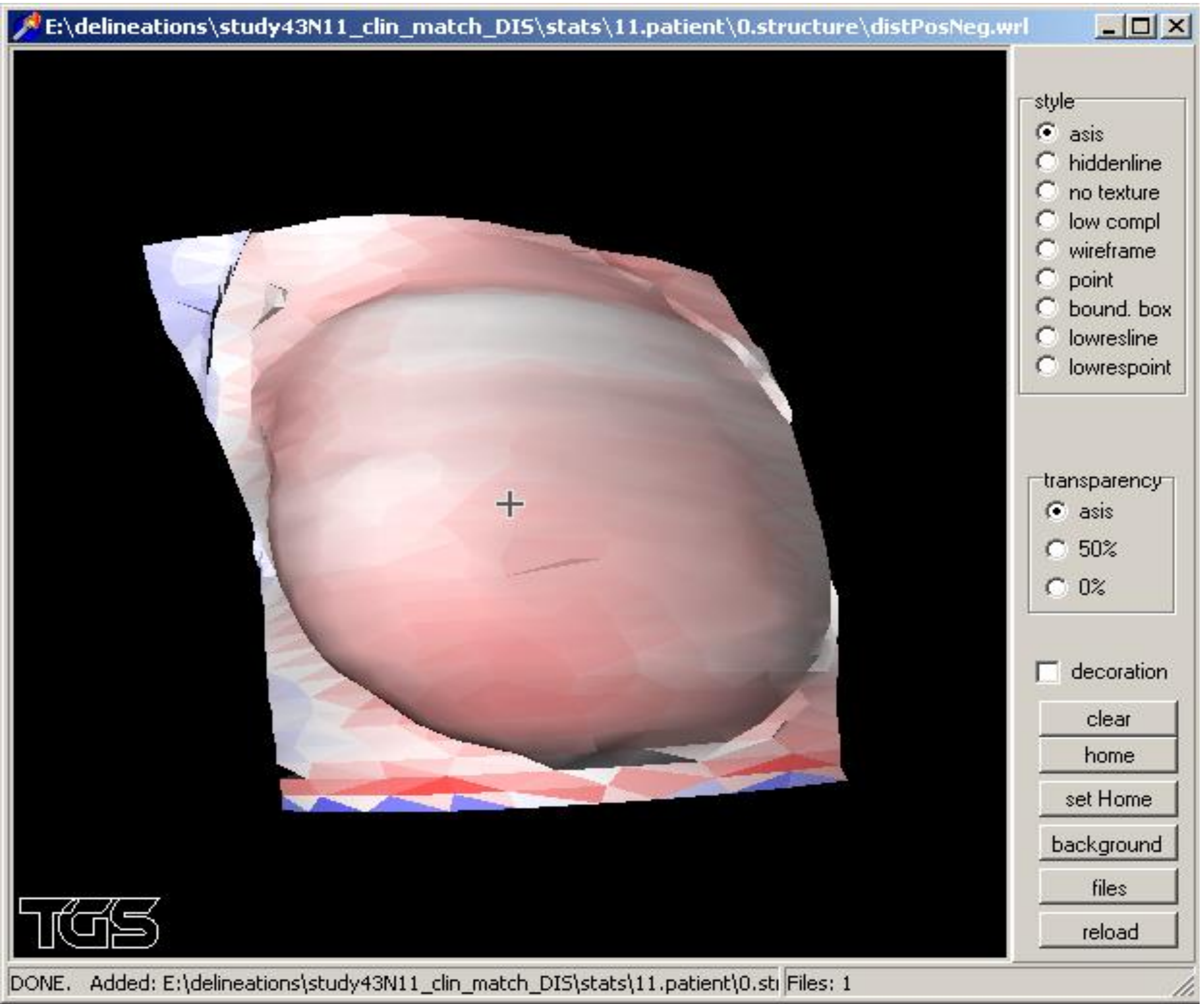
- Can be partially solved by adaptive RT

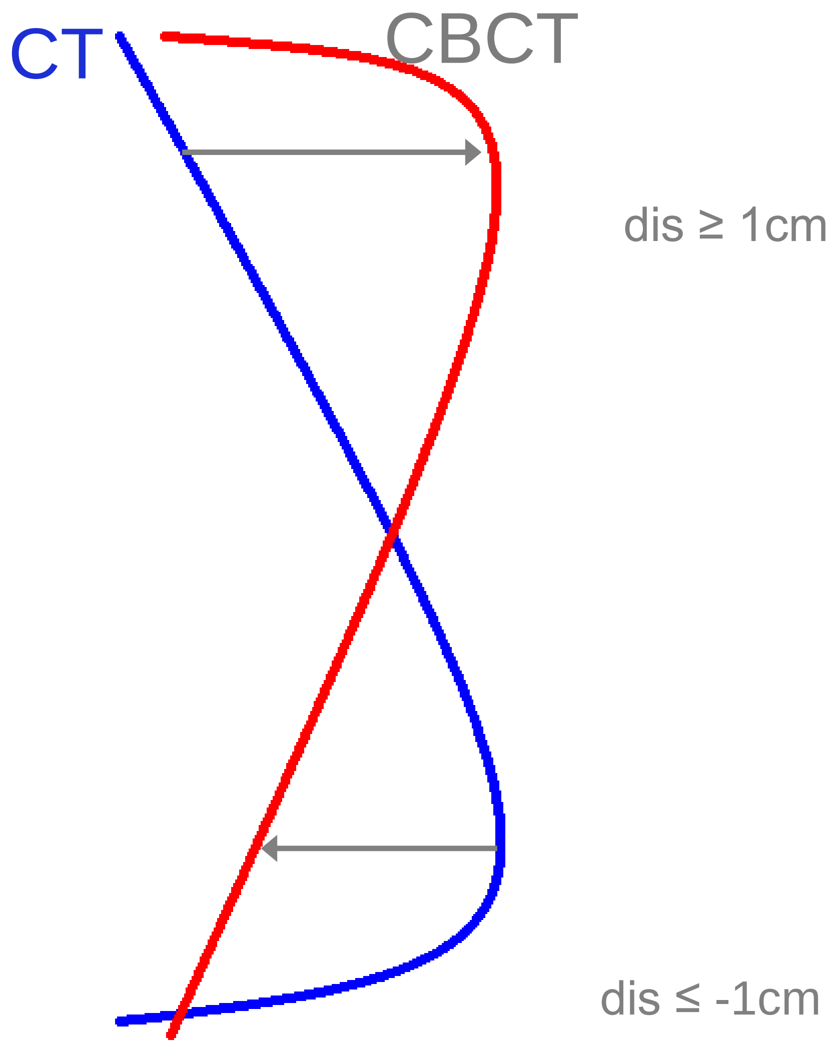
Changes in breast shape

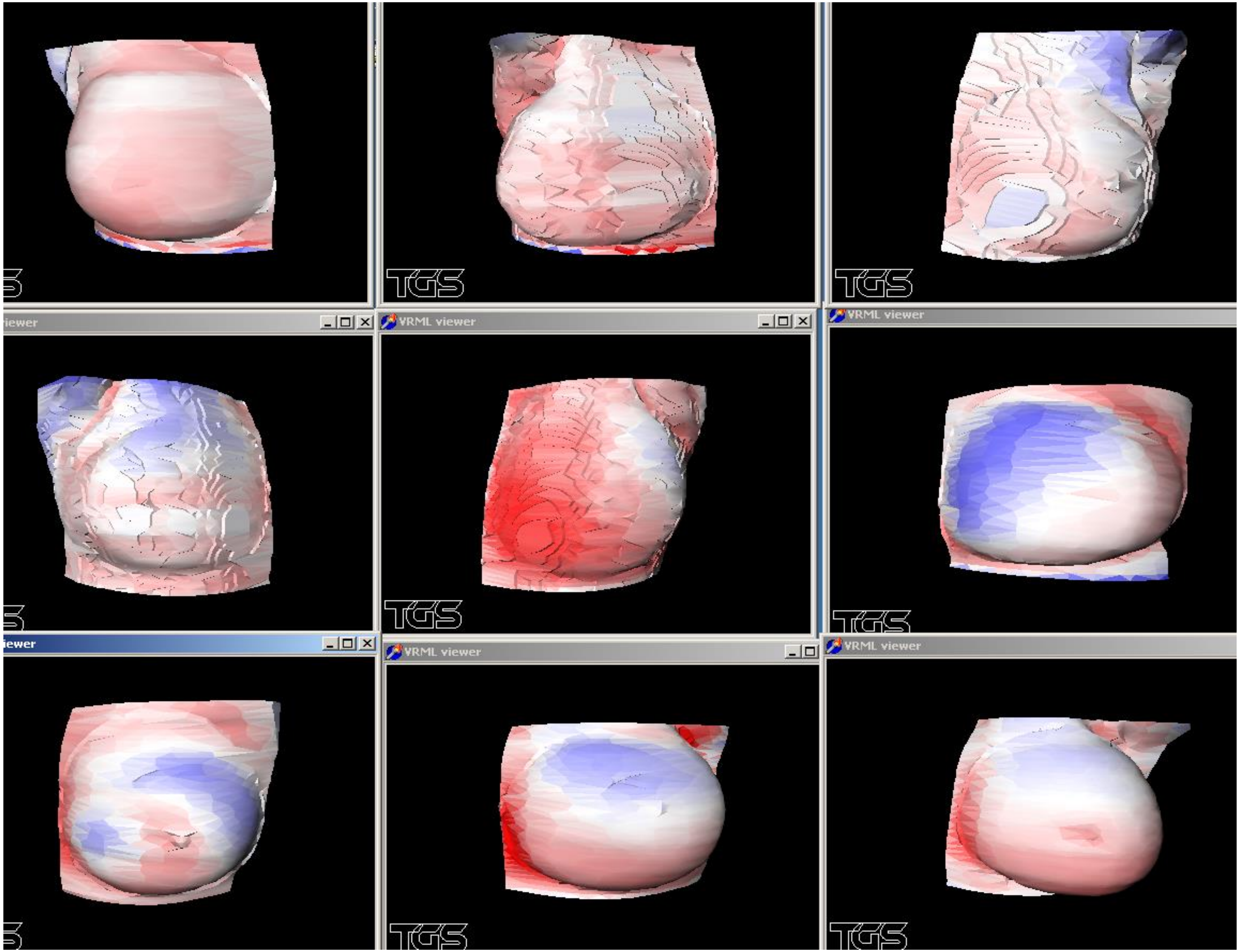


R.Topolnjak et al

Average difference (treatment → planning)



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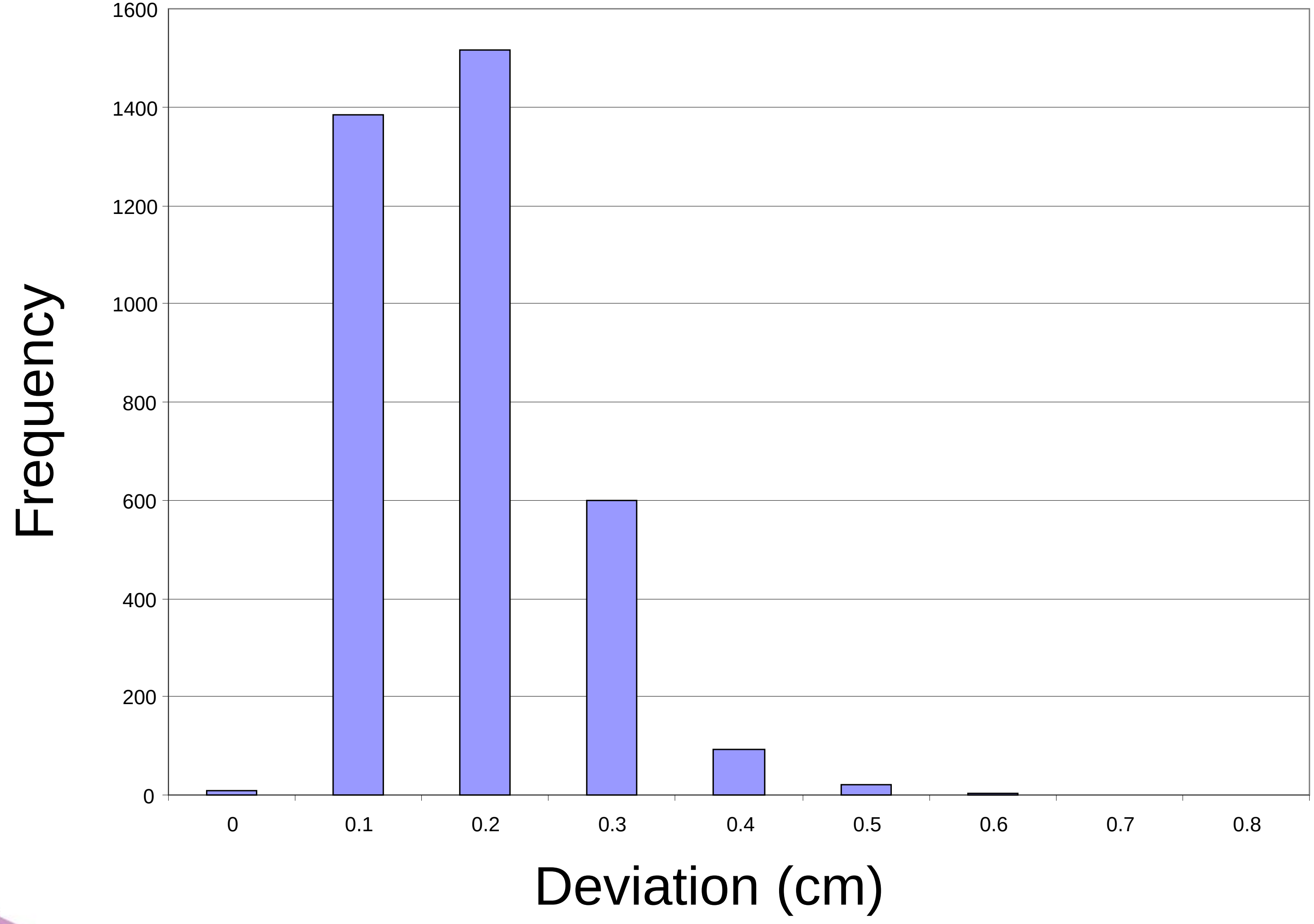
TGS

Average difference (treatment → planning)



Margins

Metaphysics margins?

- Clinically used margin for breast: **0 mm!**
  – Adapted from sim-technique - it's just beam setup
  – Clearly not enough according to conventional margin ideas

- Clinically used margin for boost: 5 mm
  – Let's see if that's enough

	Systematic	Random
Delineation	2.0 mm	-
Setup	1.5 mm	2.5 mm
Shape changes	2.0 mm	2.0 mm
Total	3.2 mm	3.2 mm

  – Margin: 2.5 * 3.2 + 0.3 * 3.2 = **9 mm**

Because of background dose

Metaphysics margins?

- So why is this not leading to lots of local recurrences?

Metaphysics margins?

- For the whole breast
  - It’s a CTV. Small underdosage does not necessarily underdose actual tumor cells

    → Risk of tumor cell underdosage small
  - Ongoing debate whether it’s even necessary to treat the whole breast

Metaphysics margins?

- For the boost
  - It's a boost with a 50 Gy background dose, so severe underdosage will not occur
  - CTV margin for the excision cavity is usually large → compensates for small PTV margin
  - Conformity is not very good with current planning techniques → effectively the margin is bigger
  - This is however **not** the case for partial breast treatments

Take home messages

- Conventional treatment techniques are not very critical with respect to geometrical uncertainties

- Partial breast treatments will be more critical because of lack of background dose and more advanced and conformal treatment techniques (e.g. VMAT)

Breast IGRT:
An RTT Perspective

Liz Forde, RTT
Assistant Professor
The Discipline of Radiation Therapy
School of Medicine
Trinity College Dublin

Fundamental IGRT Questions

- ***When** should I image?*
  - *Frequency*
- ***How** should I image?*
  - *Technology*
  - *Projection*
- ***What** can I see?*
  - *What is my target*
- ***What** should I match to?*
  - *Surrogate for target position*

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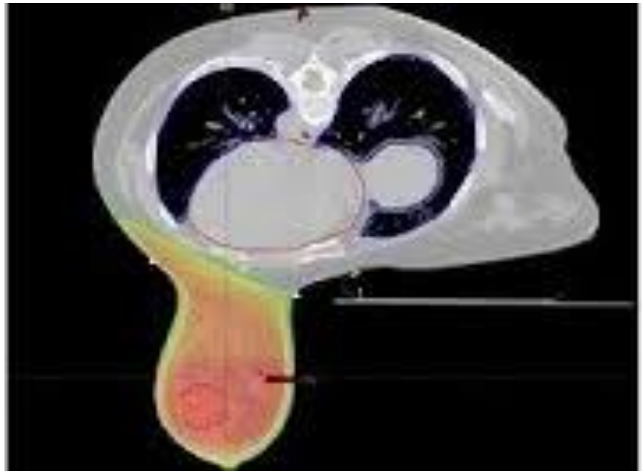
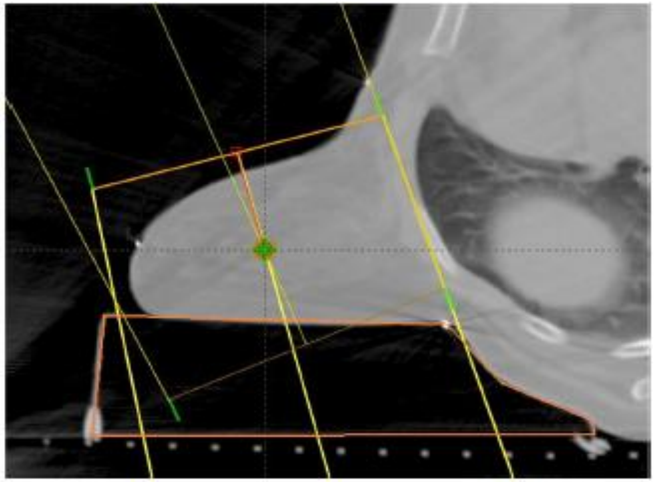
Site Specific Points to Consider

- Laterality
  - ➢ Right/Left
    - ▪ Cardiac dose
- Patient positioning
  - ➢ Supine, Prone or lateral decubitus
- Target volume
  - ➢ Whole or Partial Breast
  - ➢ Boost
- Simulation
  - ➢ 3D or 4D
- Breathing motion
  - ➢ DIBH
  - ➢ Free breathing

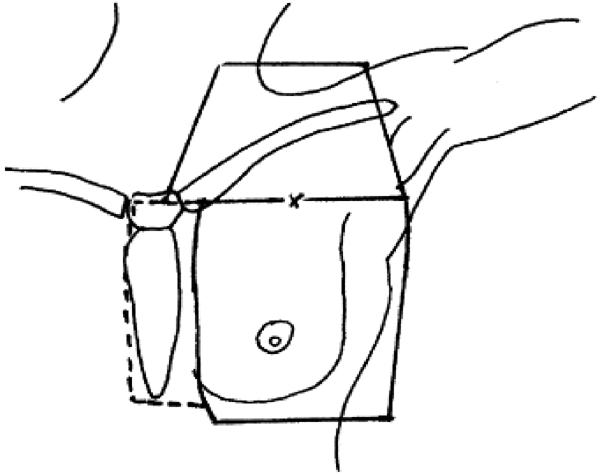
All of these factors will influence how we image this patient group



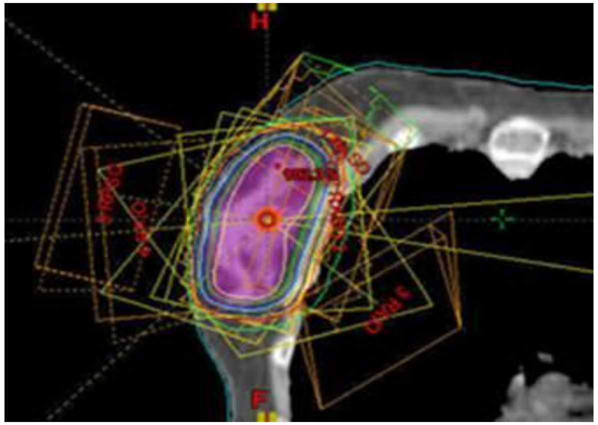
Prone



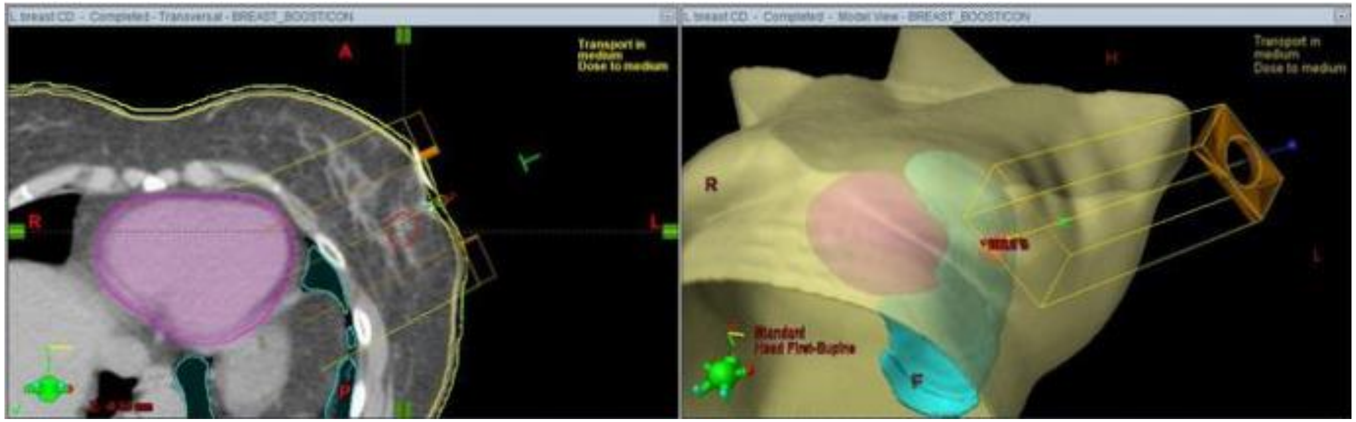
Lateral decubitus



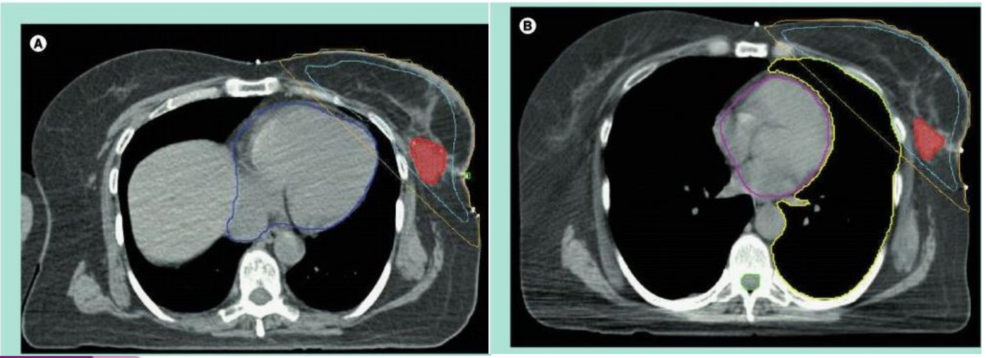
Supine: IMC (ph/e junx)



APBI



Electron boost to surgical bed



DIBH

IMRT and VMAT

On Treatment Verification

- ***Look! There is it! I can see the target!***
  - Whole breast RT
- Confirm gross external positioning information
  - Light field
  - FSDs
- What else do we want to see?
  - Contour changes
  - Tumour bed
  - Seroma
  - Surgical clips

Match Anatomy

- Breast contour
- Lung volume
- Ribs
- Seroma
- Surgical Clips

Surgical Clips

- Act as a surrogate for the tumour bed
- Improve accuracy in delineation and used for positional verification
- Clip insertion after breast conservation surgery
- Caution artefact on planning CT
    - ➢ Impact on electron beam dosimetry?

- Either use directly in match or export isodose lines from planning to ensure they fall within required dose
    - ➢ Donovan *et al*., 2012
    - ➢ Similar to Post Prostatectomy clips

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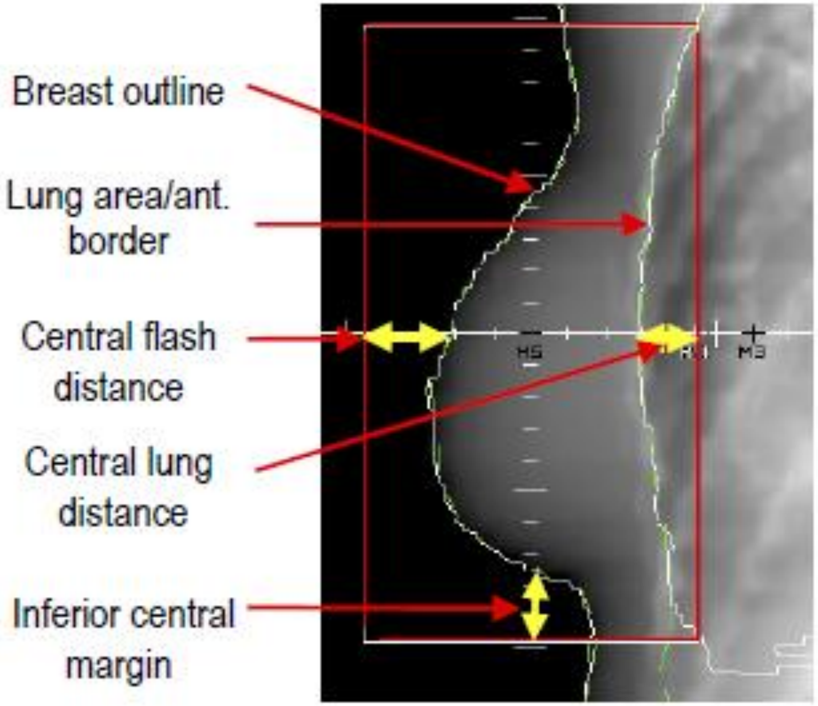
On Treatment IGRT

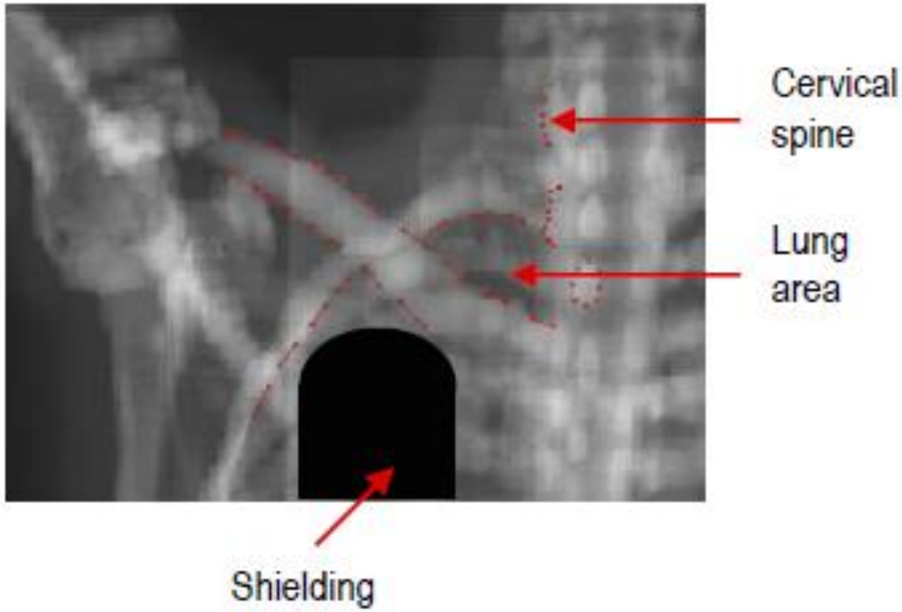
- Largely driven by what is available to you
- Make the most of it
- Consider the clinical impact
    - ➢ Tighter margins?
    - ➢ Reduced Toxicity?

MV 2D

- Widely available
- Ability to acquire continuous “snapshot” during the fraction
- Will provide field border information
- Will provide assessment of lung volume, breast contour
- Adequate for whole breast RT with standard fractionation
- Typically 5mm tolerance is acceptable
- Difficult to visualise surgical clips
- Depending on lung in field, generally sufficient information from a “single” acquisition

MV 2D





On Target: Ensuring geometric accuracy in radiotherapy. 2008

2D/2D (Paired orthogonal 2D)

Used for isocentre position check

Field border information is not displayed

A minimum requirement for all advanced techniques

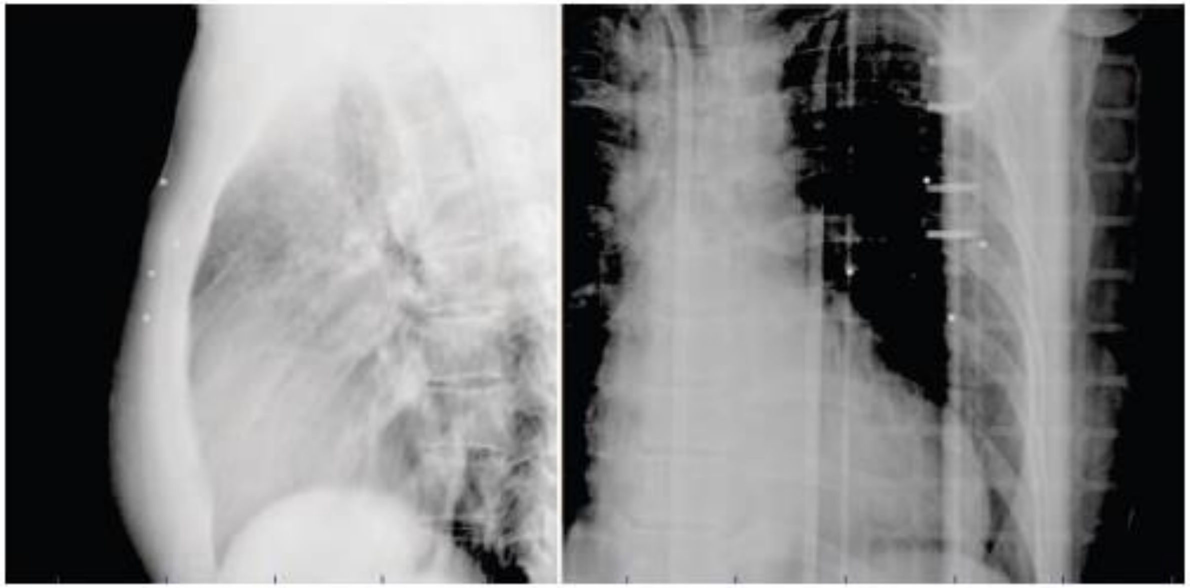


FIG. 2. Anterior–posterior and lateral paired kV images of a patient on treatment day 1. *Yue at al., 2013*

kV decreases dose burden and increases image quality

3D (CBCT)

- Provides:
  - Isocentre position verification
  - Internal soft tissue anatomy
  - Clearer image of clips
  - Information on changes in target during treatment
    - Seroma changes

- Consider:
  - Dose
  - Collision risk
  - Ease of accurate registration and match

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3D (CBCT)

- Limitations
  - Collision
  - Field of view
  - Increased dose to contra lateral breast
- CBCT not acquired at the isocentre to avoid collision
- Then once matched the shift includes the offset from isocentre position
- Adds time and potential errors
- Donovan et al. (2012) stipulate limitations on iso position to account for this

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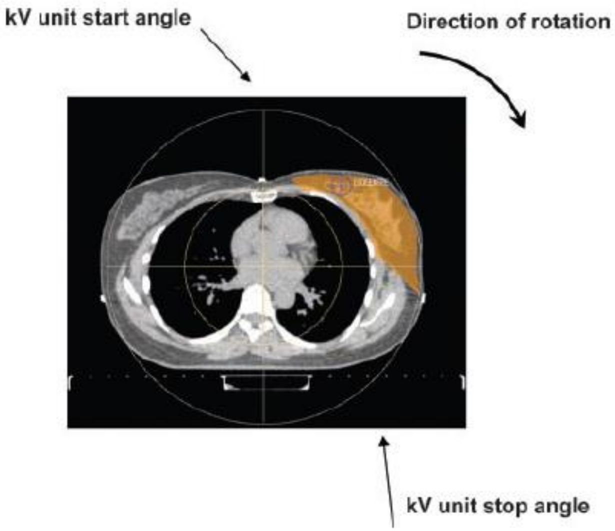
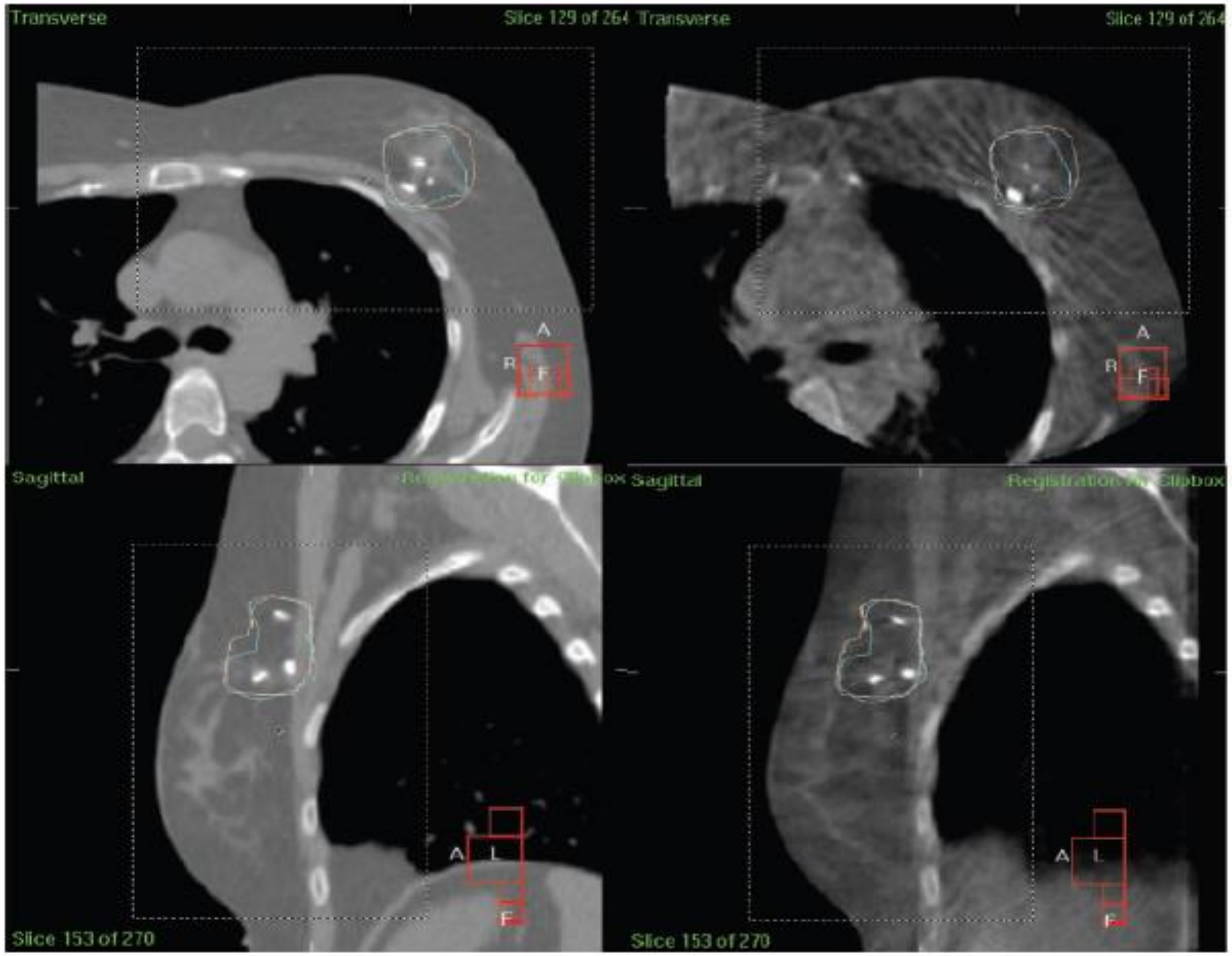
3D (CBCT): Clarity of Surgical Clips





Isodose lines have been exported to confirm coverage

Donovan et al., 2012

3D (CBCT): Clarity of Surgical Bed

Setup error for EPID and cone-beam CT ● R. Topolnjak *et al.*

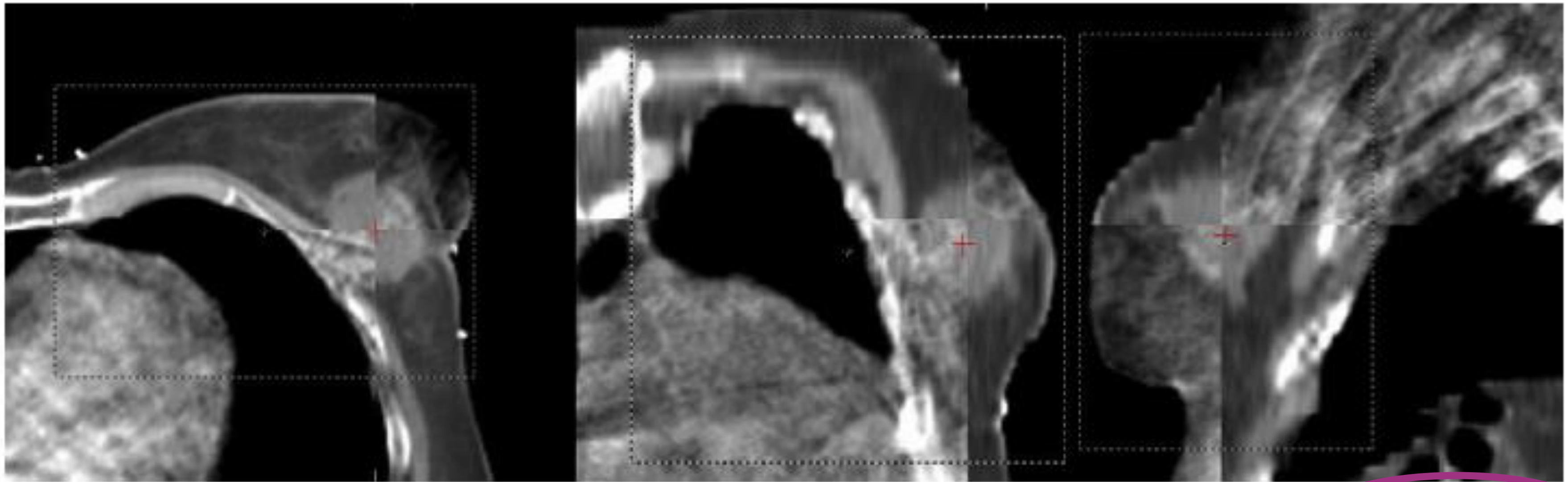


Fig. 2. Match of planning computed tomography (CT) and cone-beam CT (CBCT) images after bony (sternum and rib) anatomy registration. A bony anatomy rigid registration was performed based on image data in a user-defined, three-dimensional, box-shaped region of interest (white dashed line) using a chamfer matching algorithm.

Topolnjak et al., 2009

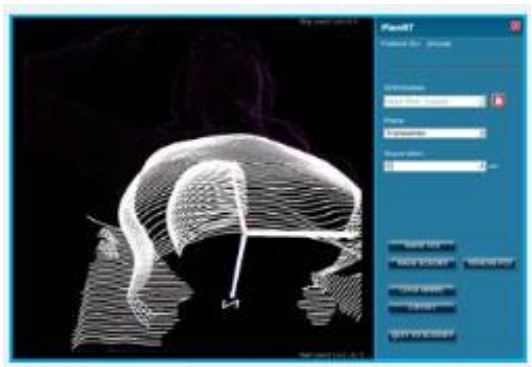
Video-Based Surface Mapping

- Whole surface shape matching

- Provides surface anatomy information and can demonstrate the impact of breathing

- Can this be correlated to provide shift/positional information?
  - ➢ Often used in conjunction with other imaging devices

- No additional radiation



A Look at the Literature

Table 4.5 Articles that discuss doses, anatomy matching methods and seroma visualisation

KV imaging Method	Author	Matched Method	Sample Size>20	Seroma Visible	Surgical clips	Auto co-registration	Reported imaging dose to patient.	Safe to acquire at iso centre
CBCT	Jain et al.(2009)	Bones	No	No	No	Yes	Yes	No
	White et al. (2007)	Lung/external contour	Yes	Yes	No	Potential	Yes	Yes
	Kim et al. (2007)	Clips	No	Yes	Yes	Yes	Yes	No
	Topolnjak et al. (2010)	Sternum/ribs	Yes	Unknown	No	Yes	No	Unknown
	Yang et al.(2010)	Unknown	No	Yes	No	Yes	Yes	Unknown
	Donovan et al.(2012)	Clips	Yes	Yes	Yes	Yes	Yes	Yes
kV*	Yue et al. (2011)	Bony to gold fiducials	Yes	Yes	Yes	Unknown	No	Unknown
	Lawson et al. (2008)	Bony	Yes	Unknown	Yes	No	Yes	Unknown
kV* vs. CBCT	Fatunase et al. (2008)	Bones, then soft tissue	No	Yes	Yes	No	Yes	No for both.

*orthogonal kV imaging

L. Lewis Improving Radiotherapy for Breast Cancer: Identification of the tumour bed and characterisation of target volume changes. 2013 MSc Thesis, available online

What is Happening in Europe?

- **2010** Survey of EORTC affiliated institutions
- "Electronic portal imaging for patient set-up is used by **92%** of the institutions." *(van der Laan et al., 2010)*
- So what does Europe look like in 2017?
- What is happening in Europe today?

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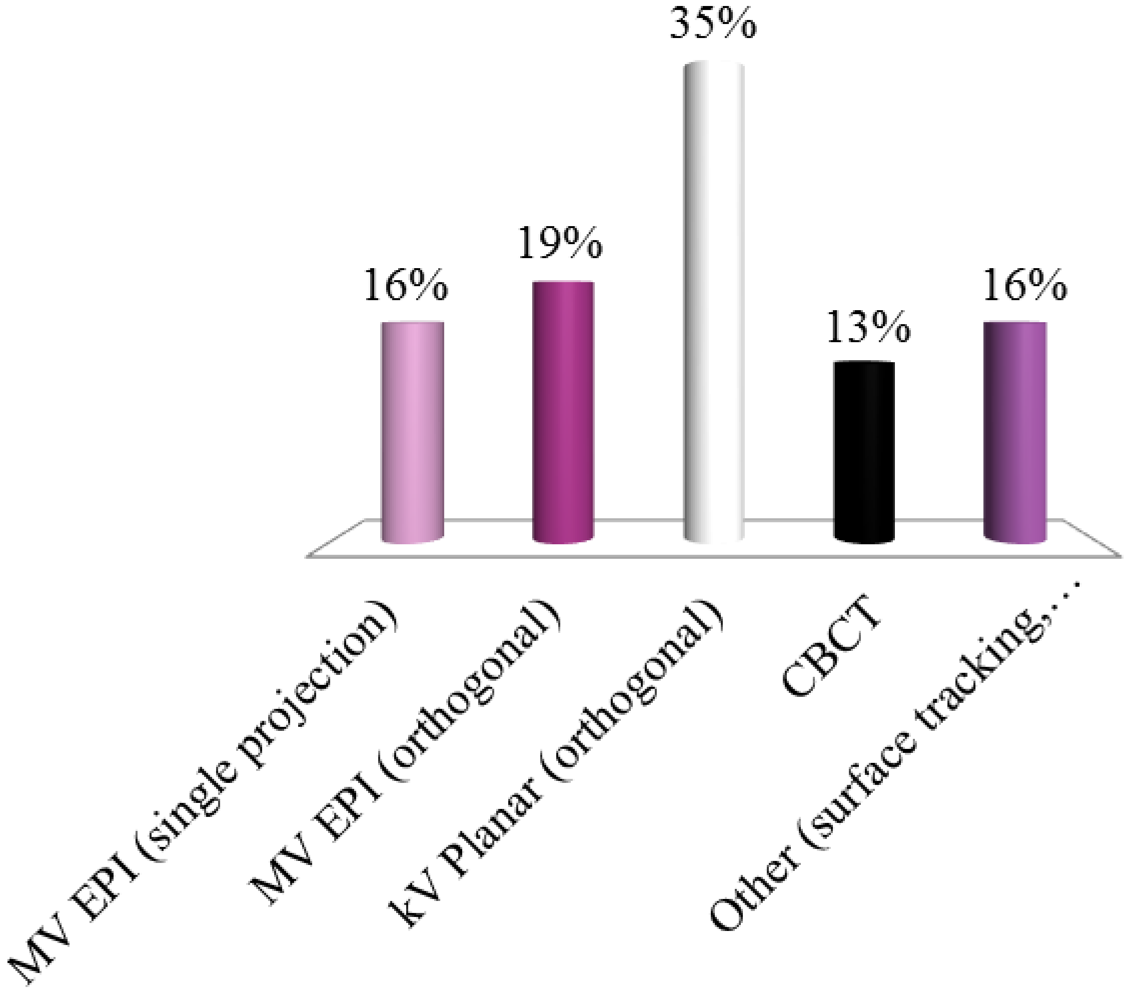
In my clinical department, for standard WBRT, we image using:

A. MV EPI (single projection)
B. MV EPI (orthogonal)
C. kV Planar (orthogonal)
D. CBCT
E. Other (surface tracking, Tomotherpy)



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How did you compare with The US?
2016 Survey of ASTRO Members *(Nabavizadeh et al., 2016)*

Technology Used

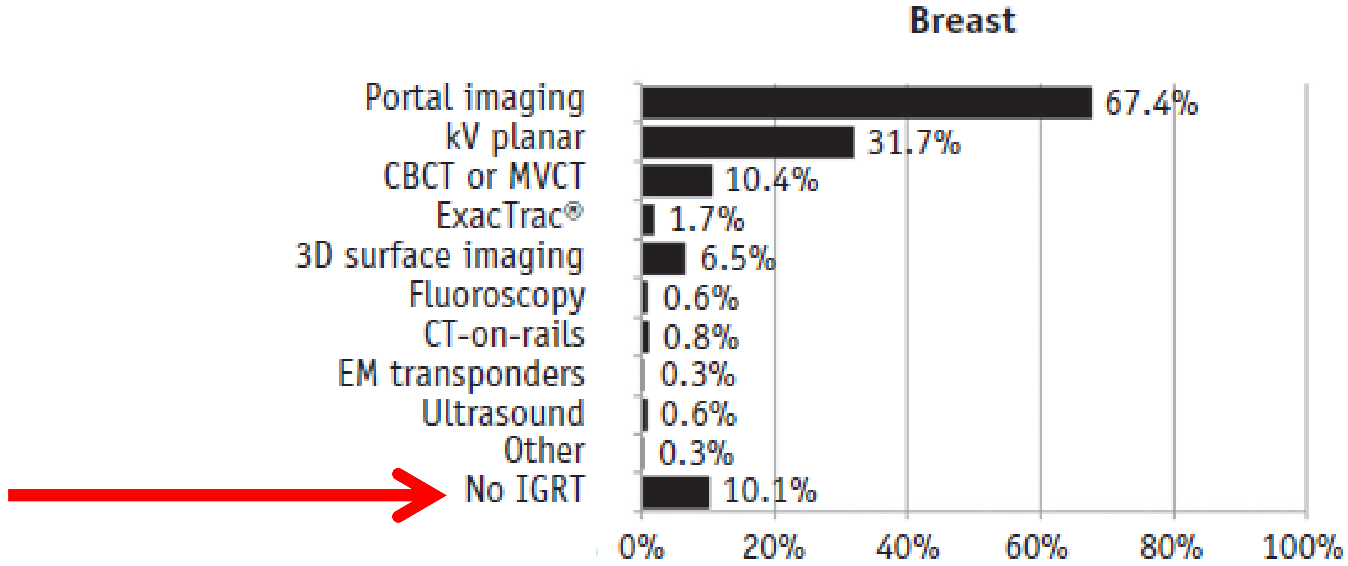


Fig. 2. Physician-reported image guided radiation therapy frequency (black) and on-line image verification frequency (gray) for standard fractionation treatments, by disease site. *Abbreviations:* 3D-CRT = 3-dimensional conformal radiation therapy; fx = fractions; IMRT = intensity modulated RT.

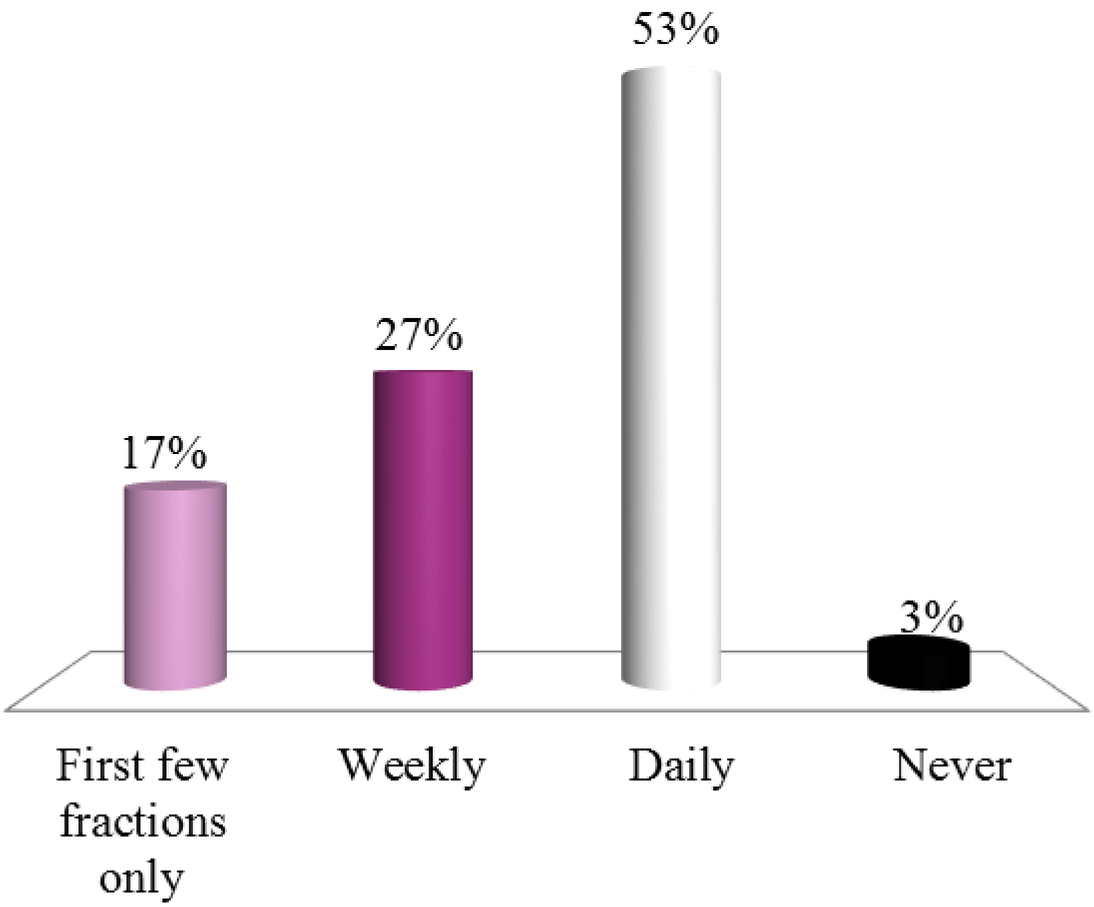
In my clinical department, for standard WBRT, we image :

A. First few fractions only

B. Weekly

C. Daily

D. Never



ESTRO School

How did you compare with The US?
2016 Survey of ASTRO Members *(Nabavizadeh et al., 2016)*

Frequency of Imaging

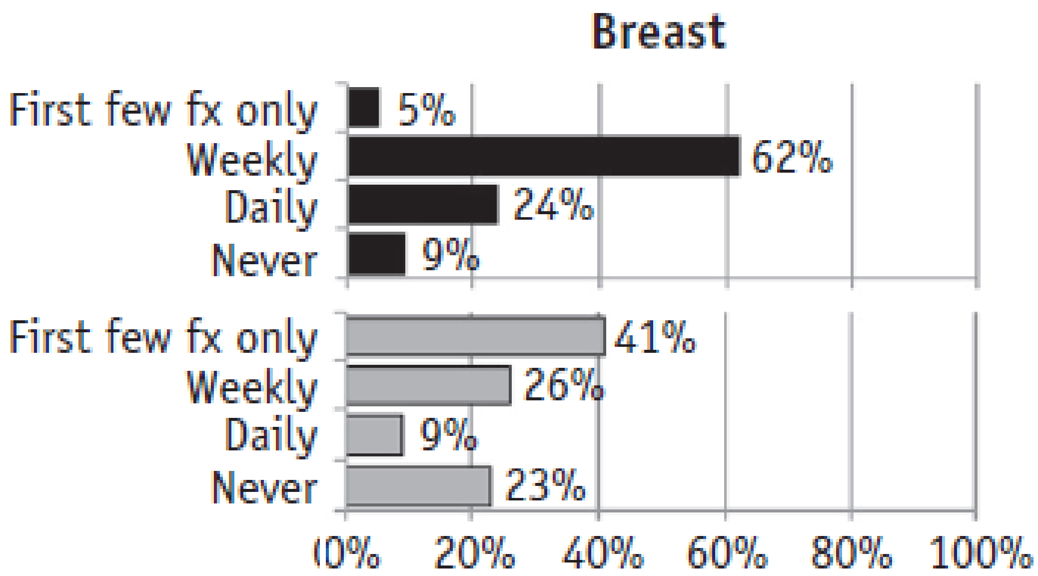
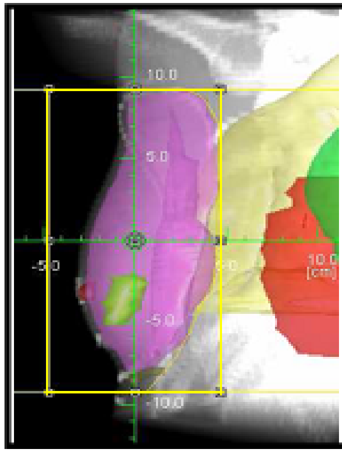


Fig. 2. Physician-reported image guided radiation therapy frequency (black) and on-line image verification frequency (gray) for standard fractionation treatments, by disease site. *Abbreviations:* 3D-CRT = 3-dimensional conformal radiation therapy; fx = fractions; IMRT = intensity modulated RT.

Therapeutic strategy: Which radiotherapy?

Two changing practice concepts have modified the standard whole breast irradiation 50Gy +/- boost has been replaced



Hypo fractionated whole breast irradiation

Whelan NEJM 2010; START A and B Lancet Oncol 2008

Accelerated partial breast irradiation

Vaidya Lancet 2010; Bourgier IJROBP 2010 ; Lemanski IJROBP 2010; Taghian IJROBP 2005; Polgar IJROBP 2004 ; Vicini IJROBP 2003; Formenti IJROBP 2003;

IGRT for *(Supine)* APBI: What are people doing?

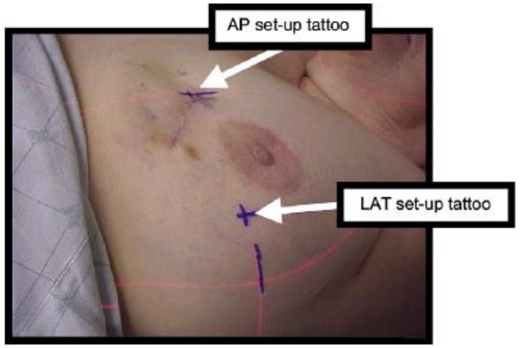


Fig. 1. Patient with skin marker crosshairs representing isocentric setup at surgical cavity.

Int. J. Radiation Oncology Biol. Phys., Vol. 76, No. 2, pp. 528–534, 2010

0360-3016/10/$–see front matter

doi:10.1016/j.ijrobp.2009.02.001

CLINICAL INVESTIGATION **Breast**

CLINICAL EXPERIENCE WITH IMAGE-GUIDED RADIOTHERAPY IN AN ACCELERATED PARTIAL BREAST INTENSITY-MODULATED RADIOTHERAPY PROTOCOL

Charles E. Leonard, M.D.,* Michael Tallhamer, M.S.,* Tim Johnson, Ph.D.,* Kari Hunter, C.M.D.,* Kathryn Howell, M.D.,* Jane Kercher, M.D.,† Jodi Widener, M.D.,† Terese Kaske, M.D.,‡ Devchand Paul, M.D.,§ Scot Sedlacek, M.D.,§ and Dennis L. Carter, M.D.*

*Rocky Mountain Cancer Centers, Littleton, CO; †Arapahoe Surgical Associates, Littleton, CO; ‡Sally Jobe Diagnostic Breast Center, Greenwood Village, CO; and §Rocky Mountain Cancer Centers, Rose Hospital, Denver, CO

2010
One of the first reports on IGRT APBI

Orthogonal **MV** images taken **daily**

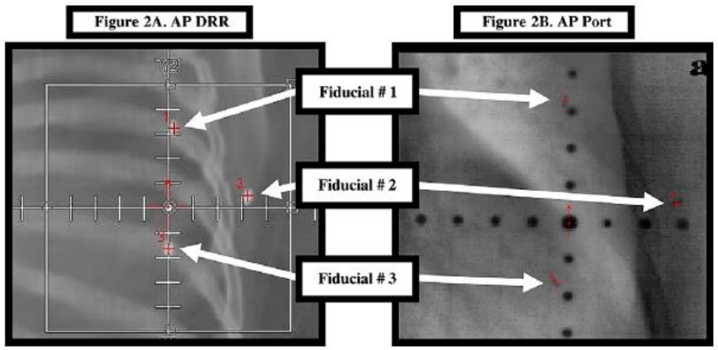


Fig. 2. Anterior/posterior digital reconstruction radiograph and corresponding port film (arrows indicate respective fiducial location).

Imaging dose included in plan

Table 5. Individual and total dose contribution of AP and lateral port films for 5 patients over the course of accelerated partial breast radiotherapy to the isocenter and 100% of PTV using image-guided radiotherapy

	ISO dose (cGy)			
Patient	AP	Lateral	Total	100% PTV
1	30.7	25.3	56	45
2	28.1	30.7	58.8	48
3	26.4	30.1	56.5	50
4	29.7	28	57.6	49
5	30.3	29.9	60.2	54
As a percentage of prescription dose of 3,850 cGy				
1	0.8	0.7	1.5	1.2
2	0.7	0.8	1.5	1.3
3	0.7	0.8	1.6	1.3
4	0.8	0.7	1.5	1.3
5	0.8	0.8	1.6	1.4

IGRT for *(Supine)* APBI: What are people doing?

Int. J. Radiation Oncology Biol. Phys., Vol. 76, No. 2, pp. 528–534, 2010

0360-3016/10/$–see front matter

ELSEVIER

doi:10.1016/j.ijrobp.2009.02.001

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Because of the reliability of these fiducial markers, we have reduced the size of port films for IGRT. Before the use of fiducials, reviewing physicians required visualization of the surrounding anatomy, specifically the ribs, clavicle, and sternum. This required the more traditional double-exposure port with the second larger field exposure. When it is not necessary to view surrounding anatomical landmarks because of fiducial placement in proximity to the target cavity, it is possible to reduce port field sizes.

cerning their use in partial breast treatment. This could suggest that margins might be reduced for a smaller PTV volume than is used currently. Up to this time, an additional margin of 1 cm from the CTV had been used. However, owing to the use of these fiducial markers, this additional margin may be reduced by 5 mm. This would be well within two standard deviations of the average mean error of our IGRT experience.

IGRT for *(Supine)* APBI: What are people doing?

Distinction b/w surgical clips and fiducials

Textured gold fiducials for stability and visualisation

Daily orthogonal MV EPI

Published 2012

Clinical Investigation: Breast Cancer

Validating Fiducial Markers for Image-Guided Radiation Therapy for Accelerated Partial Breast Irradiation in Early-Stage Breast Cancer

Catherine K. Park, M.D., M.P.H.,* Jakub Pritz, M.S.,† Geoffrey G. Zhang, Ph.D.,* Kenneth M. Forster, Ph.D.,* and Eleanor E.R. Harris, M.D.*

*From the *Department of Radiation Oncology, H. Lee Moffitt Cancer Center & Research Institute, Tampa, FL; and †Department of Physics, University of South Florida, Tampa, FL*

Received Jan 12, 2011, and in revised form Jun 22, 2011. Accepted for publication Jul 18, 2011

Visualisation of fiducials on 100% MV images
Centre of fiducials correlated to centre of seroma

When matching to fiducials margins can be reduced to 6mm compared to bone (10mm)

IGRT for *(Supine)* APBI: What are people doing?

Aim: to assess the residual and intrafraction errors

PTV = CTV+10mm
5 fld non coplanar
95%/95%

Cai *et al. Radiation Oncology* 2010, 5:96
http://www.ro-journal.com/content/5/1/96

RADIATION ONCOLOGY

RESEARCH Open Access

Impact of residual and intrafractional errors on strategy of correction for image-guided accelerated partial breast irradiation

Gang Cai[1†], Wei-Gang Hu[1*†], Jia-Yi Chen[1*], Xiao-Li Yu[1], Zi-Qiang Pan[1], Zhao-Zhi Yang[1], Xiao-Mao Guo[1], Zhi-Min Shao[2], Guo-Liang Jiang[1]

Pre and post fx XVI
Grey value match
Manual adjustment with:
skin, chest wall and clips
2-3 mins
Matched by RO

CBCT does not guarantee absolute accuracy
13mm margin required to account for initial setup and intrafraction errors

MRI Based IGRT – The Future?

Clinical Investigation

Magnetic Resonance Image Guided Radiation Therapy for External Beam Accelerated Partial-Breast Irradiation: Evaluation of Delivered Dose and Intrafractional Cavity Motion

Sahaja Acharya, MD, Benjamin W. Fischer-Valuck, MD, Thomas R. Mazur, PhD, Austen Curcuru, BS, Karl Sona, MS, Rojano Kashani, PhD, Olga Green, PhD, Laura Ochoa, ANP, PhD, Sasa Mutic, PhD, Imran Zoberi, MD, H. Harold Li, PhD, and Maria A. Thomas, MD, PhD

Department of Radiation Oncology, Washington University School of Medicine, St. Louis, Missour

Received Jan 9, 2016, and in revised form Jul 8, 2016. Accepted for publication Aug 10, 2016.

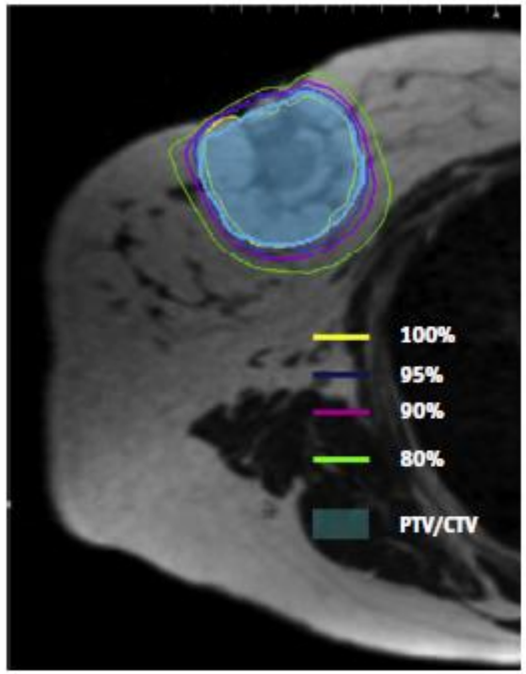

Fig. 1. Plan visualized on magnetic resonance simulation. Planning target volume (PTV) (= clinical target volume [CTV]) is shown in light blue color wash. Isodose lines: 100% (yellow), 95% (dark blue), 90% (magenta), 80% (green). (A color version of this figure is available at www.redjournal.org.)

Take Home Message

- There is an abundance of imaging technologies and strategies available for this site

- IGRT for breast is largely dependant not only what is available to you, but the planning technique that is used

- Advanced treatment techniques require more sophisticated imaging techniques
  - APBI, IMRT, VMAT

Lung

ESTRO School

Jose Lopez, M.D., Ph.D
Radiation Oncology
University Hospital Virgen del Rocio
Seville, Spain

Advanced skills in modern radiotherapy
Prague, Czech Republic –11-15 June 2016

igure 2: Estimated most frequent cancer type in 184 countries for both sexes, 2012
ata are from GLOBOCAN 2012. Data in parentheses are the number of countries in which that cancer is the most common. The map was produc
nternational Agency for Research on Cancer (Lyon, France), and reproduced with permission.

The Lancet Oncology 2015; vol 16: Issue 10

Outline of Talk

- Preclinical rationale behind **oligometastatic** state
- **Clinical data supporting** benefit to local treatment in oligometastatic NSCLC
- Case report
- Discussion of current multidisciplinary (physician, phisyc and RTTs) management

Introduction

- Definitive radiotherapy has historically been reserved for patients with stage I-III disease.
- The most common indication for RT in patients with metastatic lung cancer has been palliation for pain or other symptoms
- However, stage IV lung cancer is a very broad category , and prior studies have suggested that some patients with stage IV lung cancer and only a few distant metastases (‘**oligometastasis**’) may benefit from local therapy to both the primary tumor and the distant sites of disease .

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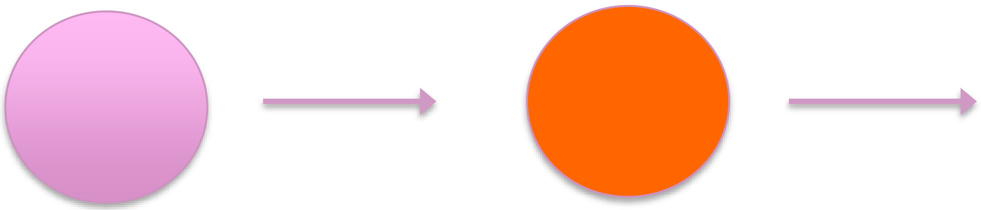
Introduction

- Spectrum of metastatic patients exists
  - ➢ Indolent vs. aggressive course
- In-between locoregionally confined and true metastatic state, there appears to exist intermediate state of low disease burden systemically=oligometastasis
  - ➢ Can these patients be “cured”?

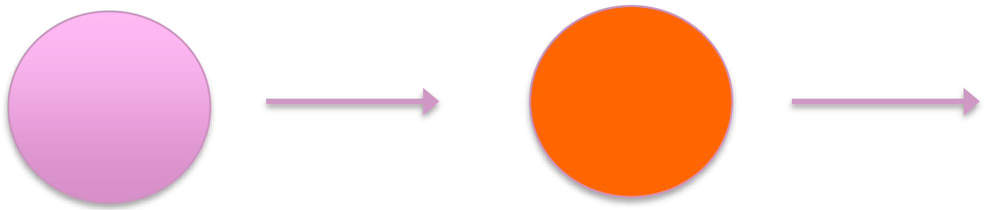
“Oligo” means “having few, having little.”

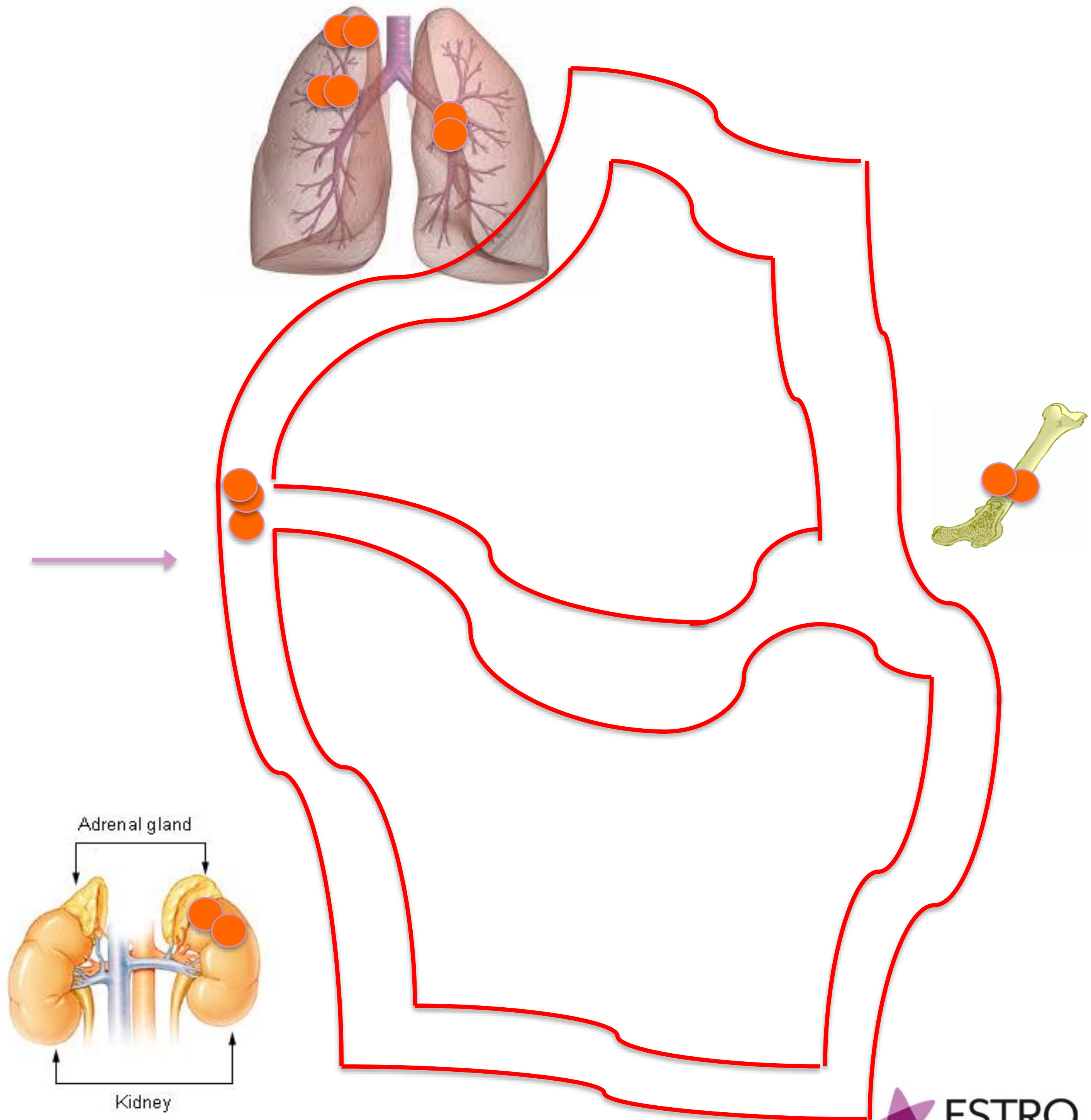
Studies with lung cancer have defined oligometastatic disease as up to 5 metastatic lesions.



“Oligo” means “having few, having little.”

Studies with lung cancer have defined oligometastatic disease as up to 5 metastatic lesions.





Dr Daniel Gomez. MD Anderson Cancer Center

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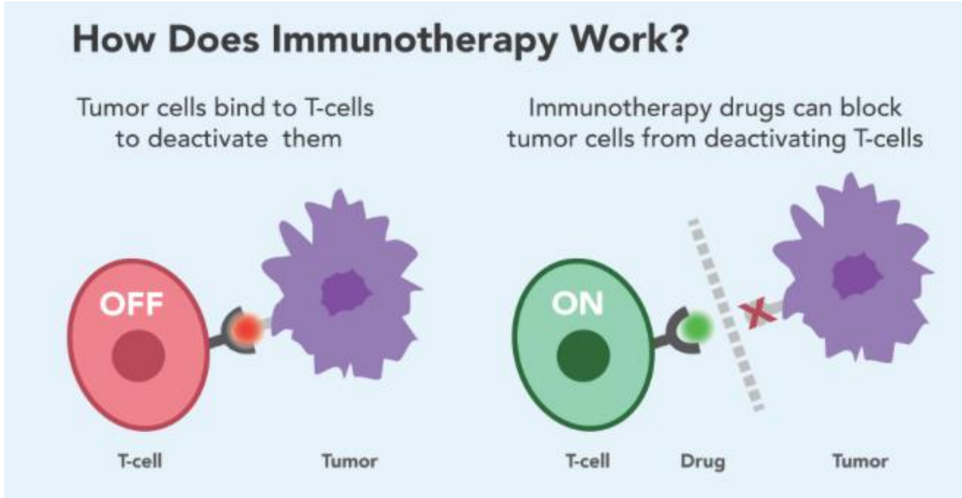
Recent Trials Addressing Management of Oligometastatic NSCLC

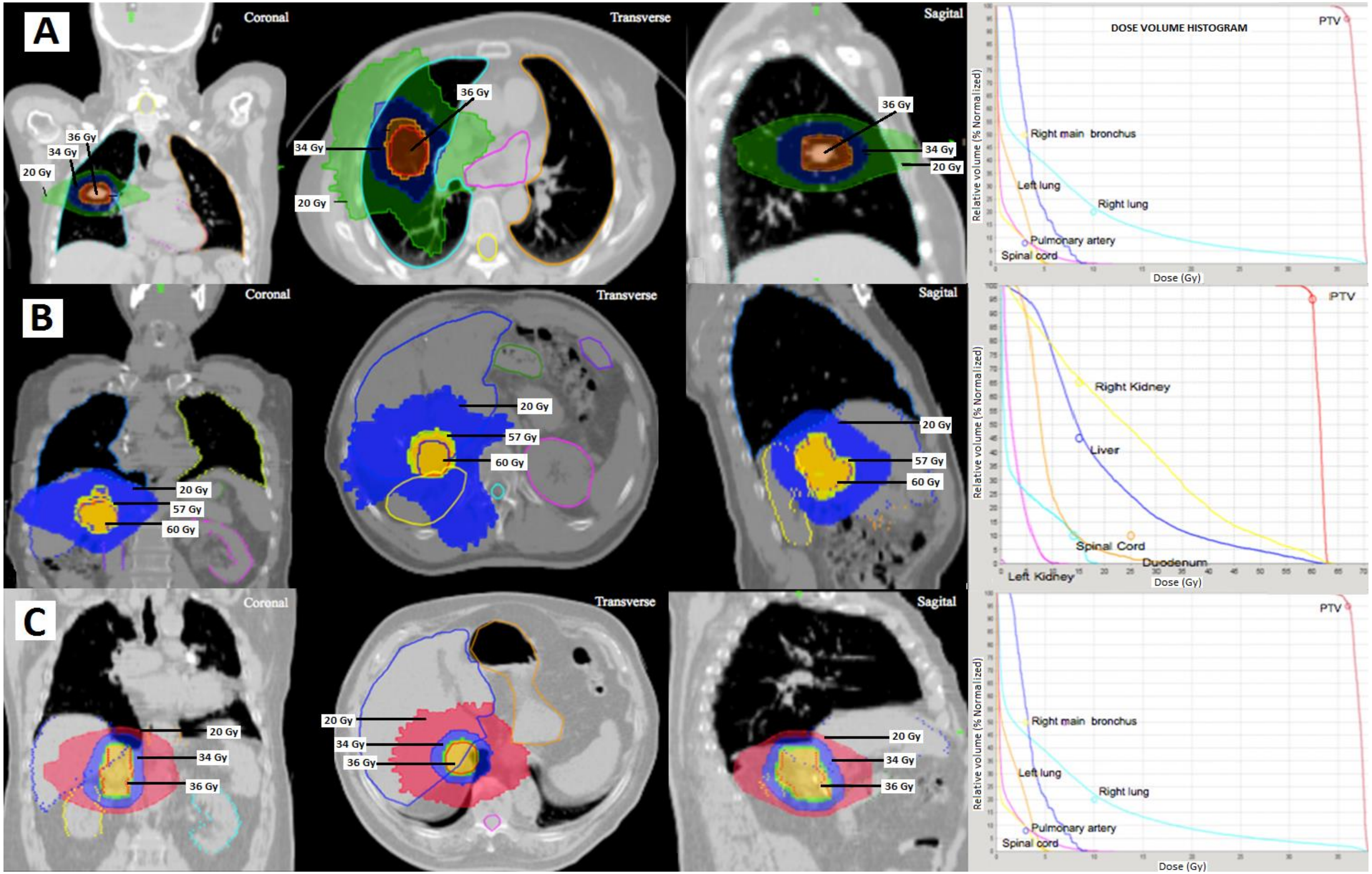


- Recent developments
  - Targeted agents
  - Maintenance chemotherapy
  - Technologic advances permitting ablative doses of radiation therapy

Clinical Data Supporting Local Treatment in Oligometastatic Setting

Author	Year	n	Timespan (years)	Single institution
Twomey	1982	2	14	Yes
Reyes	1990	5	4	Yes
Raviv	1990	3	nr	Yes
Kirsch	1993	1	6	Yes
Higashiyama	1994	5	12	Yes
Ayabe	1995	3	9	Yes
Urschel	1997	1	9	Yes
Bendinelli	1998	4	4	Yes
Tsuji	1998	1	2	Yes
Linos	1998	1	1	Yes
Porte	1998	11	8	Yes
Wade	1998	14	7	No (159 centers)
de Perrot	1999	1	5	Yes
Bretcha-Boix	2000	5	nr	Yes
Ambrogi	2000	5	7	Yes
Porte	2001	43	12	No (8 centers)
Mercier	2004	23	14	Yes
Lucchi	2005	11	10	Yes
Pfannschmidt	2005	11	7	Yes
Sebag	2006	9	9	Yes
Munoz	2006	1	5	Yes
Strong	2007	29	11	Yes

STEREOTACTIC ABLATIVE RADIOTHERAPY DELIVERED BY HELICAL TOMOTHERAPY FOR EXTRACRANEAL OLIGOMETASTASIS



Sole CV, Lopez Guerra JL, et al. Clin Transl Oncol. 2013

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STEREOTACTIC ABLATIVE RADIOTHERAPY DELIVERED BY HELICAL TOMOTHERAPY FOR EXTRACRANEAL OLIGOMETASTASIS

CONTOURS

- GTV: defined only as the solid abnormality on CT + PET
- ITV: using a multiple CT scan (free breathing, maximal inspiration, and maximal expiration)
- PTV: 0.5 cm in the axial plane and 1.0 cm in the craneocaudal plane

DOSE PRESCRIPTION

- Lung (not chest wall): 3 fractions of 20 Gy
- Lung (chest wall): 3-5 fractions of 12 Gy for lesions
- Lung (central): 8 fractions of 7.5 Gy

CHEMOTHERAPY (90%)

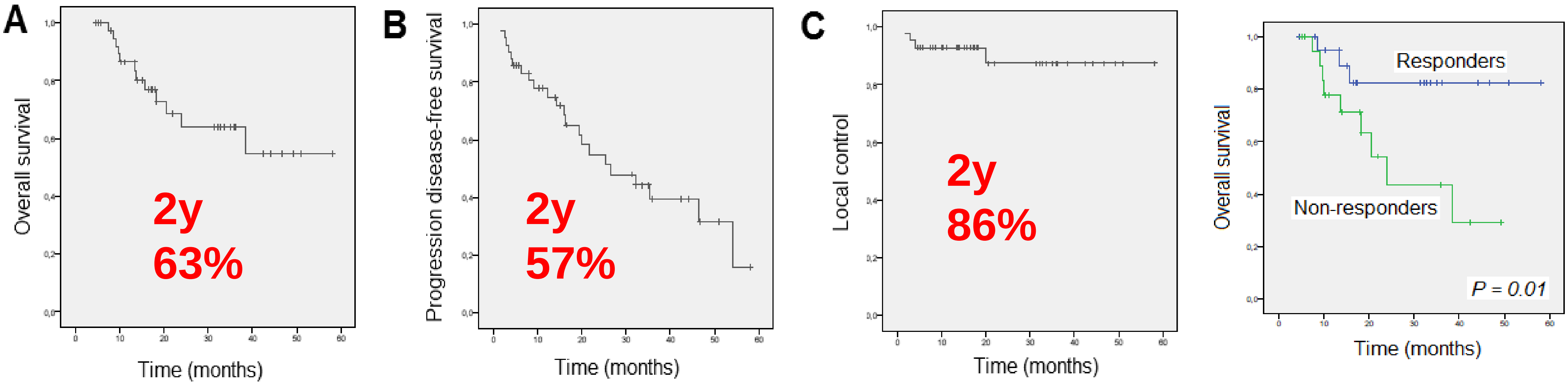
- FOLFOX/FOLFIRI

Sole CV, Lopez Guerra JL, et al. Clin Transl Oncol. 2013

DOSE CONSTRAINTS

THORAX

- Chronic lung disease: 70% of the lungs <17 Gy.
- Healthy lungs: 60 % of the lungs <20 Gy.
- Esophagus: Dmax < was 4.0 Gy per fraction.
- Chest wall: <30 Gy to 30 cc and <60 Gy to 3 cc.
- Spinal cord: <2 Gy per fraction and <45 Gy total.

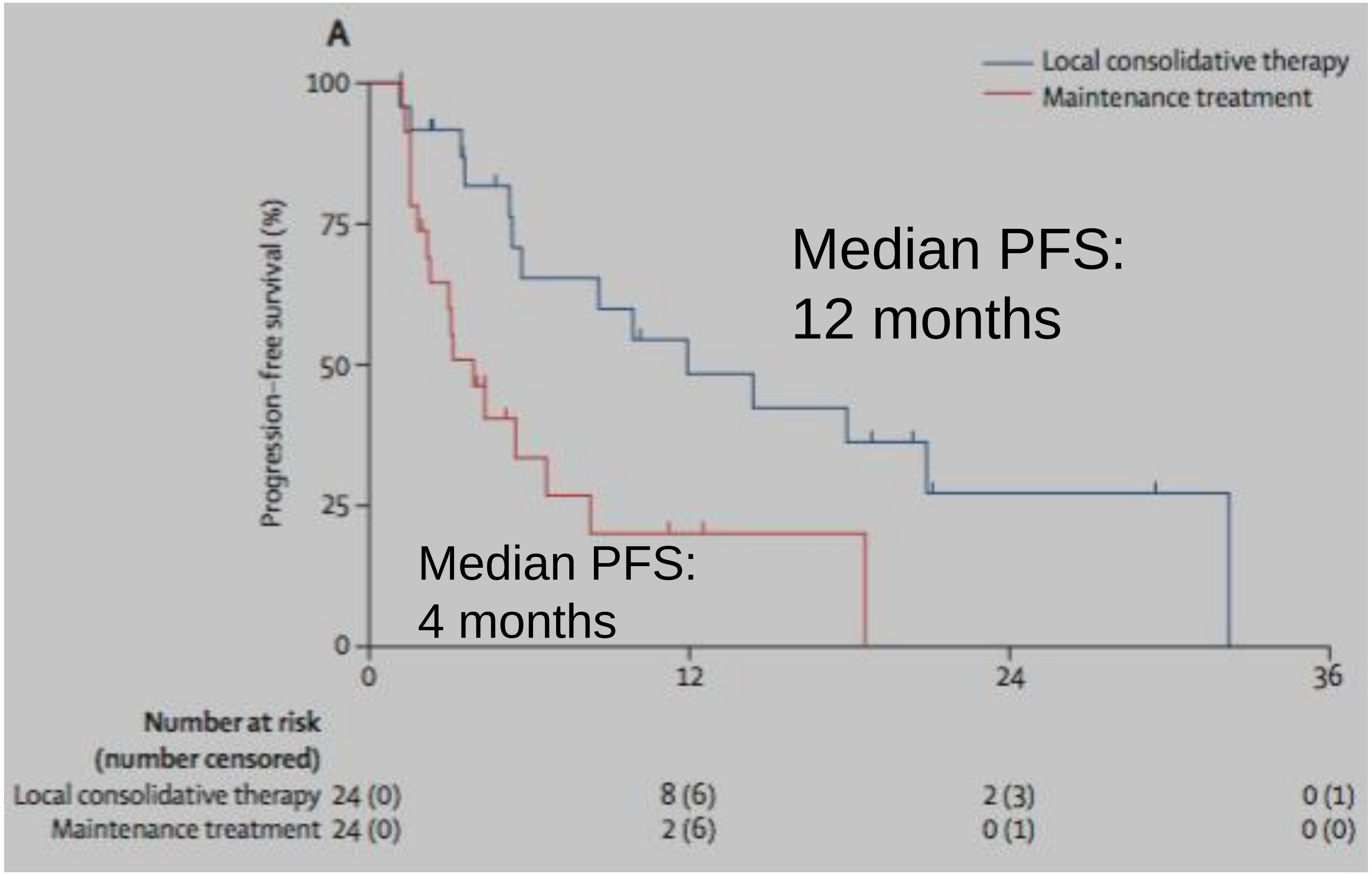


Toxicity (N=28)	Grade I	Grade II	Grade III
Pneumonitis	11	3	1
Chest wall pain	6		
Skin	6		
Esophagitis	3		

Select group of patients that benefit from aggressive local treatment for oligometastatic disease

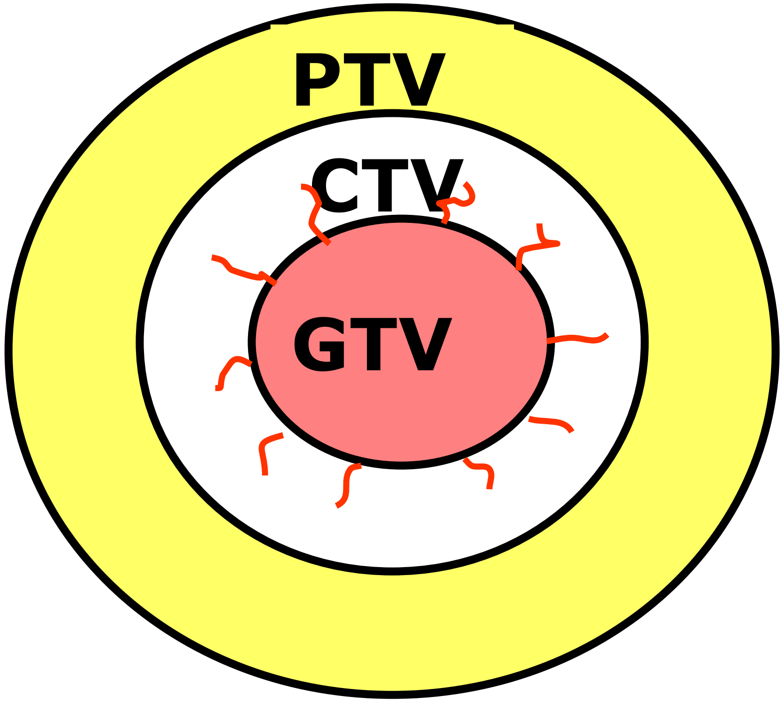
Sole CV, Lopez Guerra JL, et al. Clin Transl Oncol. 2013

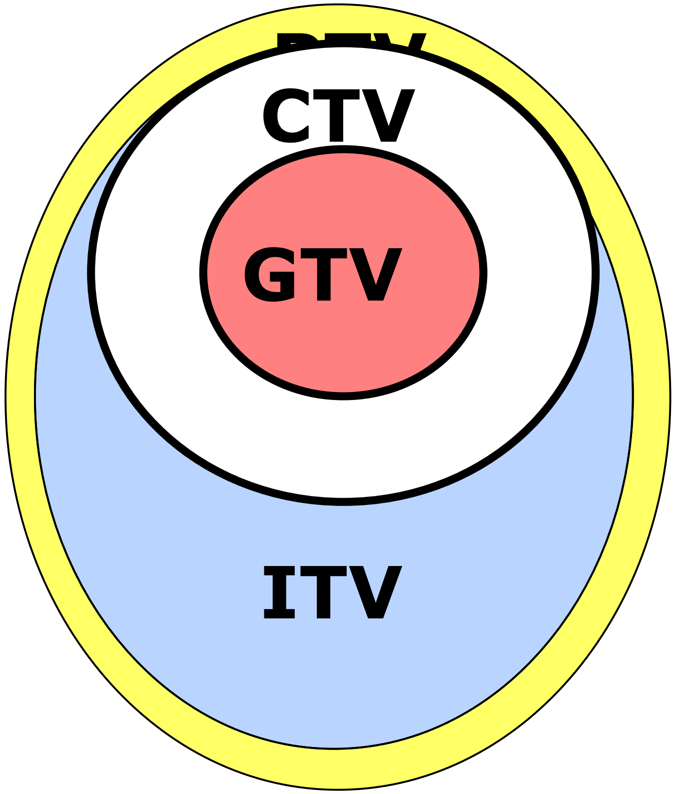
Local consolidative therapy versus maintenance therapy or observation for patients with oligometastatic NSCLC



Gomez D et al. Lancet 2016

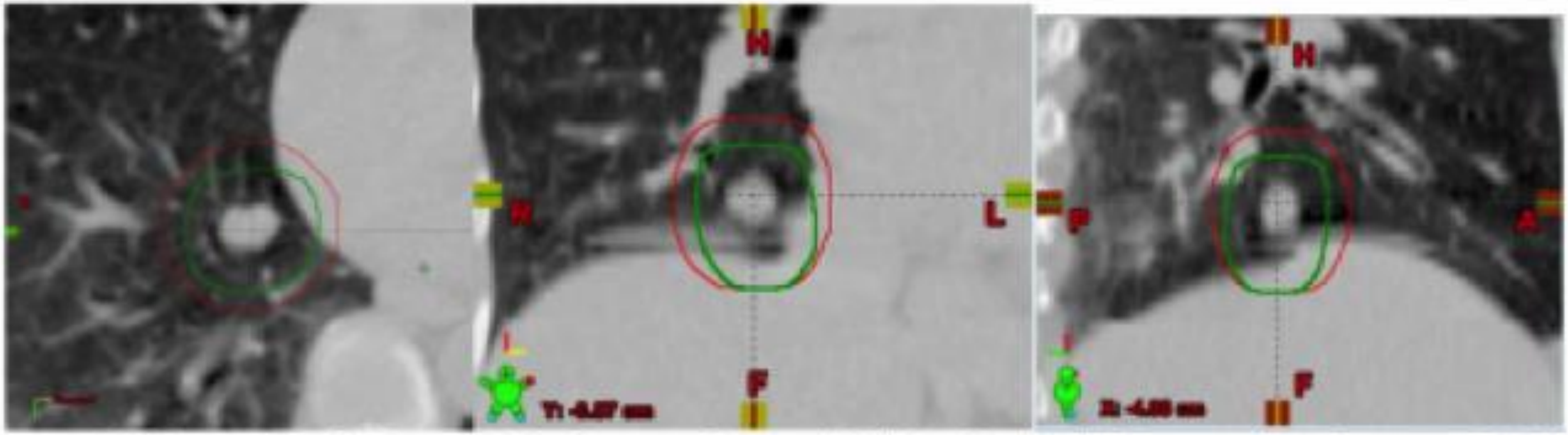
ICRU 50 ICRU 62



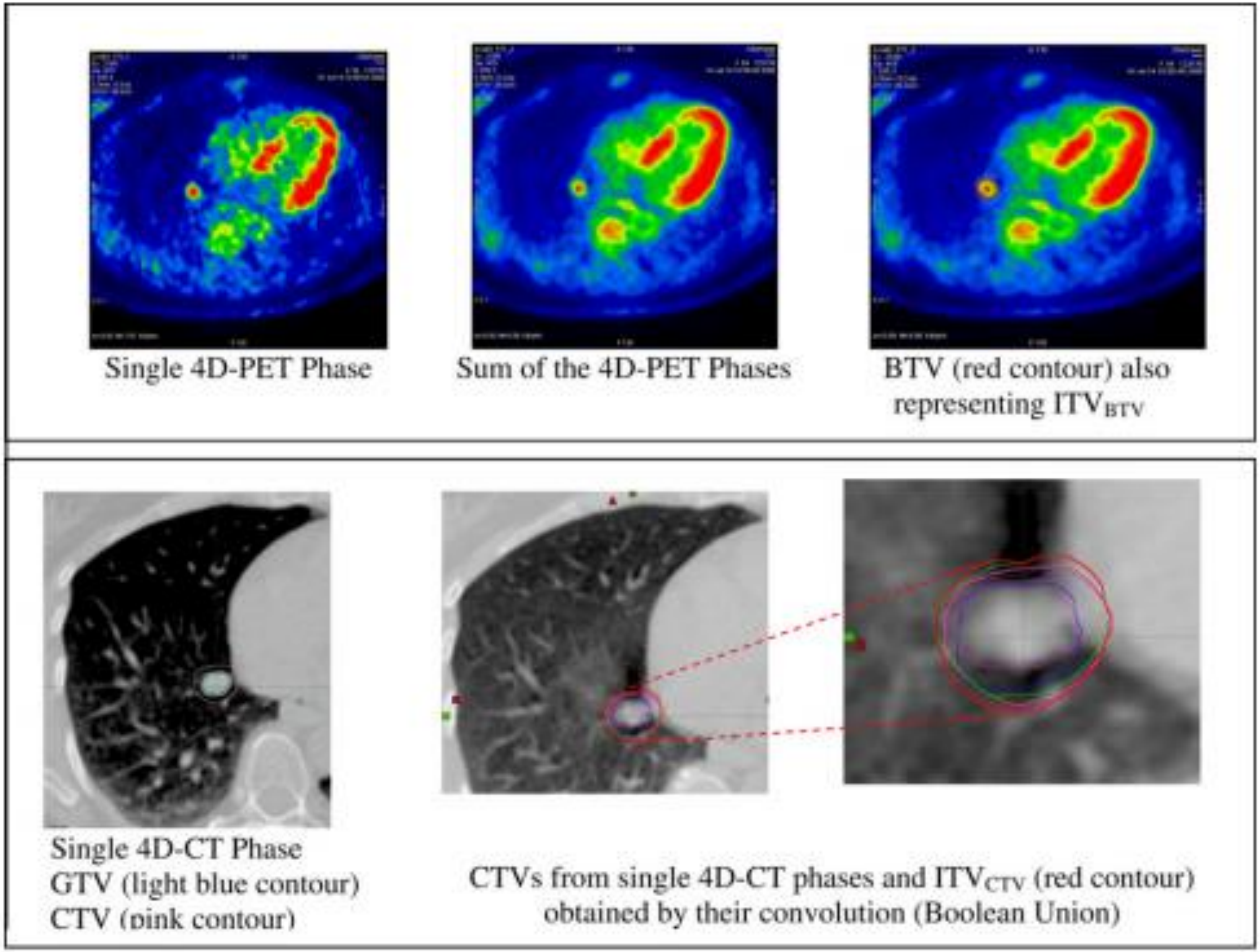


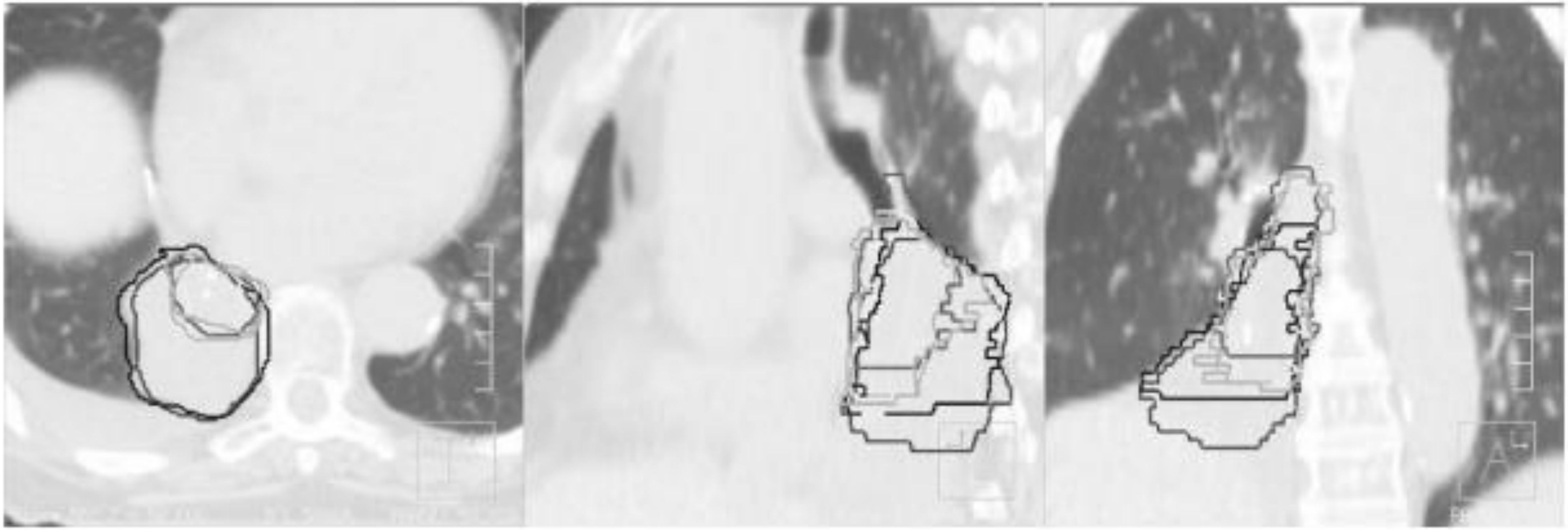
GTV= Gross Tumor Volume, CTV=Clinical Target Volume, PTV=Planning Target Volume, ITV=Internal Target Volume

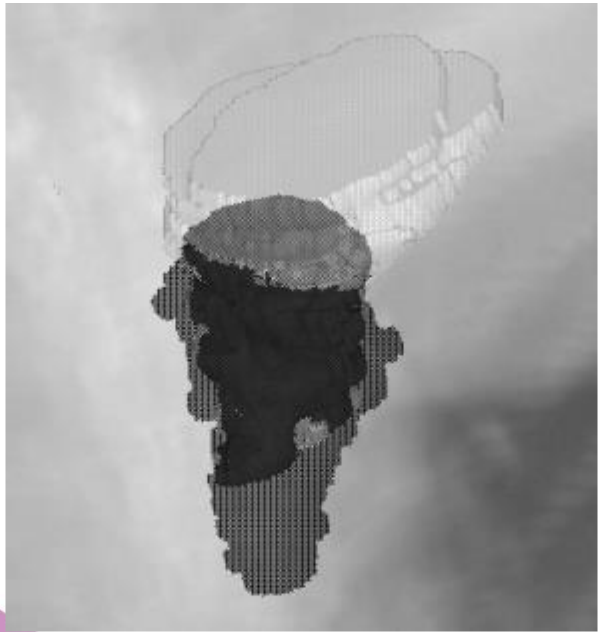
V. Bettinardi et al. / Radiotherapy and Oncology 96 (2010) 311–316



CT Image (Left Transaxial, Center: Coronal, Right: Sagittal).Comparison between PTV_{4D} (green contour) and PTV obtained by standard expansions (red contour)


Single 4D-PET Phase
Sum of the 4D-PET Phases
BTV (red contour) also representing ITV_{BTV}
Single 4D-CT Phase
GTV (light blue contour)
CTV (pink contour)
CTVs from single 4D-CT phases and ITV_{CTV} (red contour) obtained by their convolution (Boolean Union)





Inter-observer and intra-observer reliability for lung cancer target volume delineation in the 4D-CT era

Radiotherapy and Oncology 95 (2010) 166–171

Radiotherapy and Oncology 101 (2011) 322–328

Contents lists available at SciVerse ScienceDirect

Radiotherapy and Oncology

journal homepage: www.thegreenjournal.com

Lung cancer radiotherapy

An evaluation of an automated 4D-CT contour propagation tool to define an internal gross tumour volume for lung cancer radiotherapy

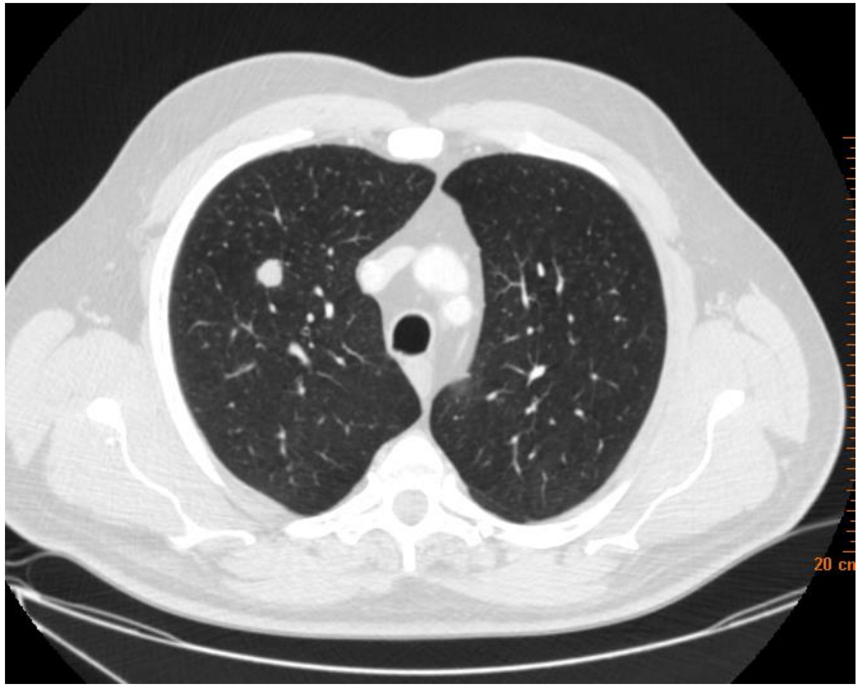
Stewart Gaede [a,b,c,d,*], Jason Olsthoorn [e], Alexander V. Louie [b], David Palma [b,c], Edward Yu [b,c], Brian Yaremko [b,c], Belal Ahmad [b,c], Jeff Chen [a,b,c,d], Karl Bzdusek [g], George Rodrigues [b,c,f]

[a] *Physics and Engineering Department; and* [b] *Department of Radiation Oncology, London Regional Cancer Program, Canada;* [c] *Department of Oncology; and* [d] *Department of Medical Biophysics, University of Western Ontario, Canada;* [e] *Department of Mathematics, University of Waterloo, Canada;* [f] *Department of Epidemiology and Biostatistics, University of Western Ontario, Canada;* [g] *Philips Radiation Oncology Systems, Flitchburg, WI, USA*

Conclusions: Automated 4D-CT propagation tools can significantly decrease the IGTV delineation time without significantly decreasing the inter- and intra-physician variability.

Case 1: Oligorecurrence of lung cancer

- A 65-year-old male presented to the emergency department with a two-week history of upper back pain
- Pertinent social history includes a 34-pack year history of tobacco smoking, as well as history of heavy alcohol consumption in the past.
- Chest X-ray and CT scan showed a RUL nodule (14 mm)



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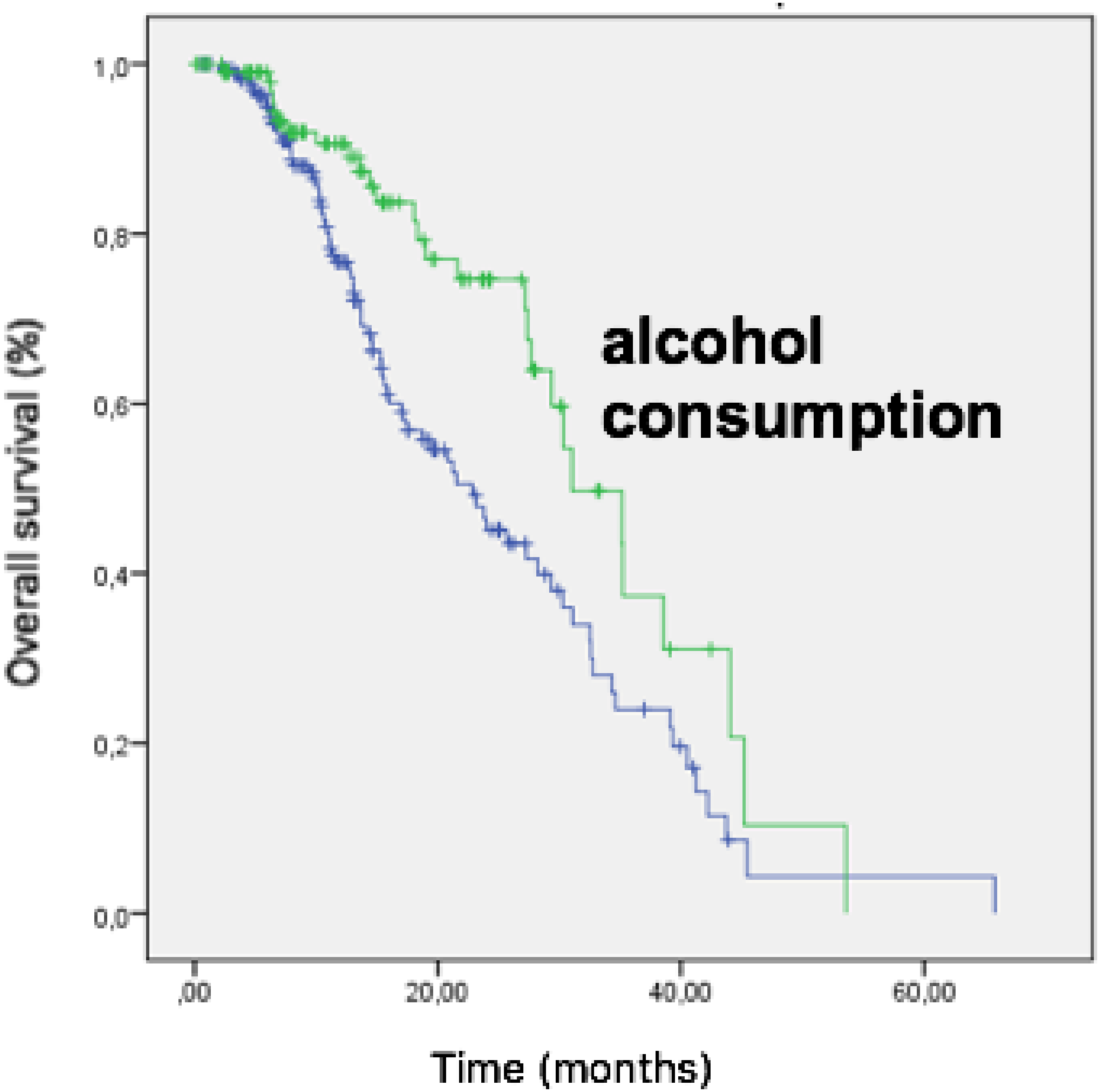
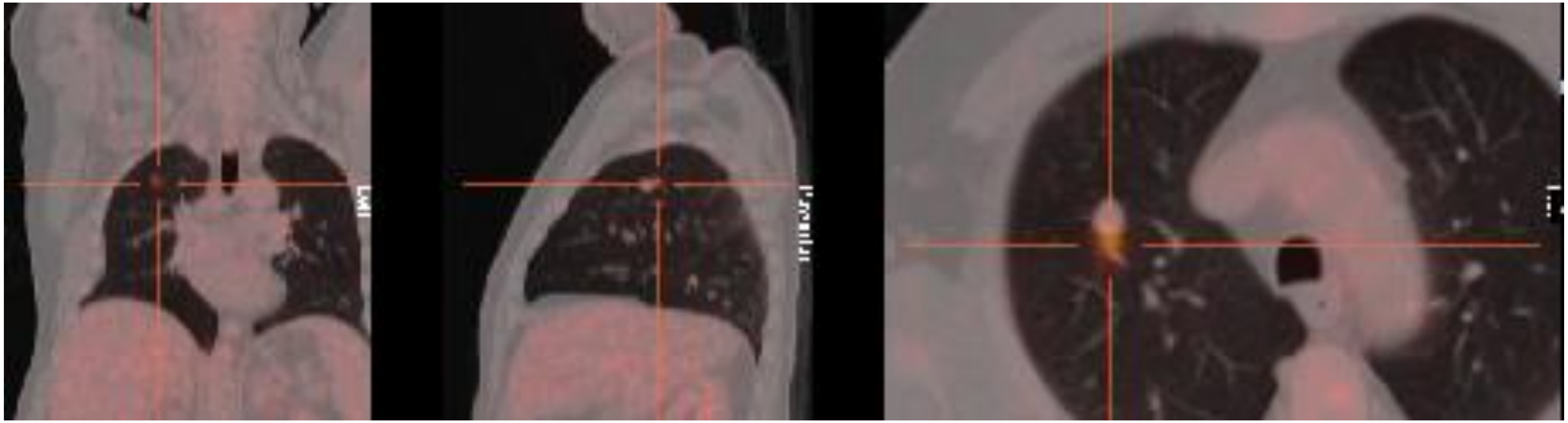
NSCLC in Seville (Spain) 2013-2016

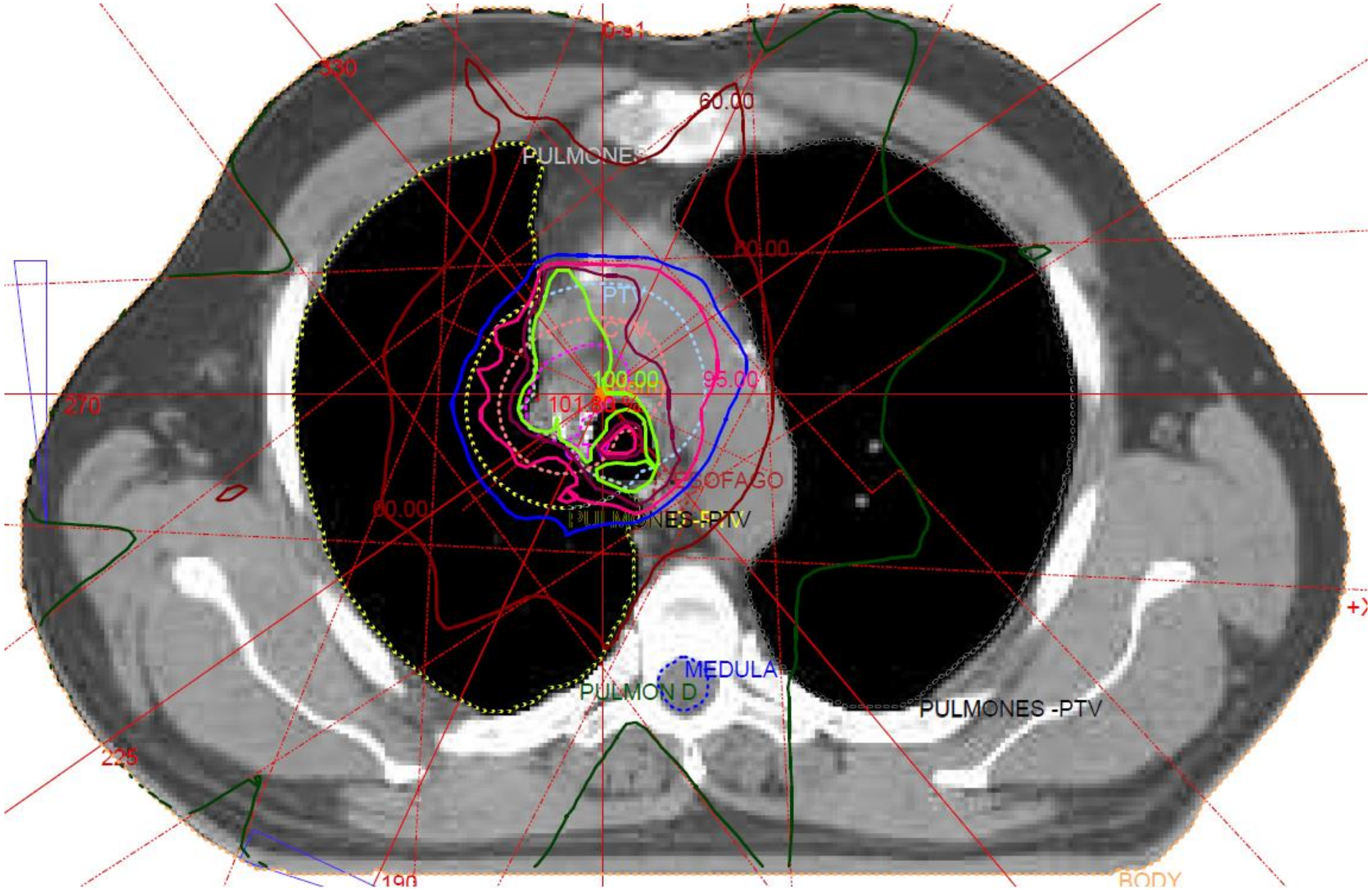


- PET/CT: SUVmax 5,1



- The patient underwent RUL lobectomy and mediastinal lymph node dissection.
- Final pathology report was consistent with high-grade large cell neuroendocrine carcinoma.

- At 2 years follow up , the CT scan showed mediastinal recurrence that was treated with concomitant radiochemotherapy (total radiation dose 66 Gy at 2 Gy/fraction).



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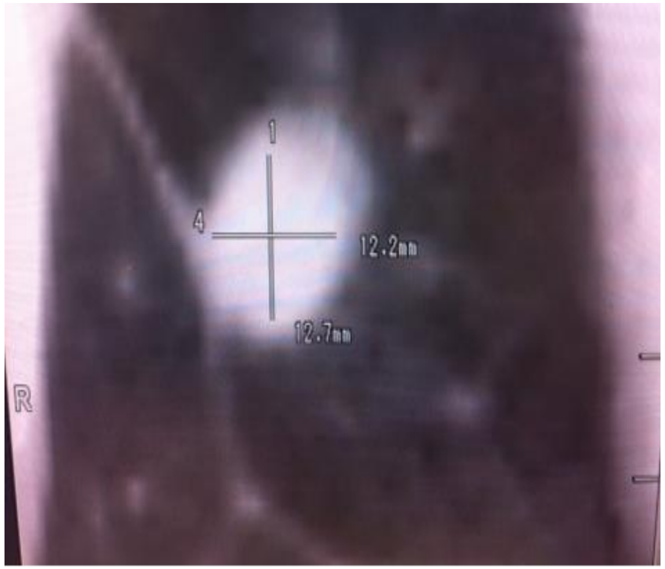
- At 3 years follow up , the CT scan showed a RML recurrence (15 mm nodule).

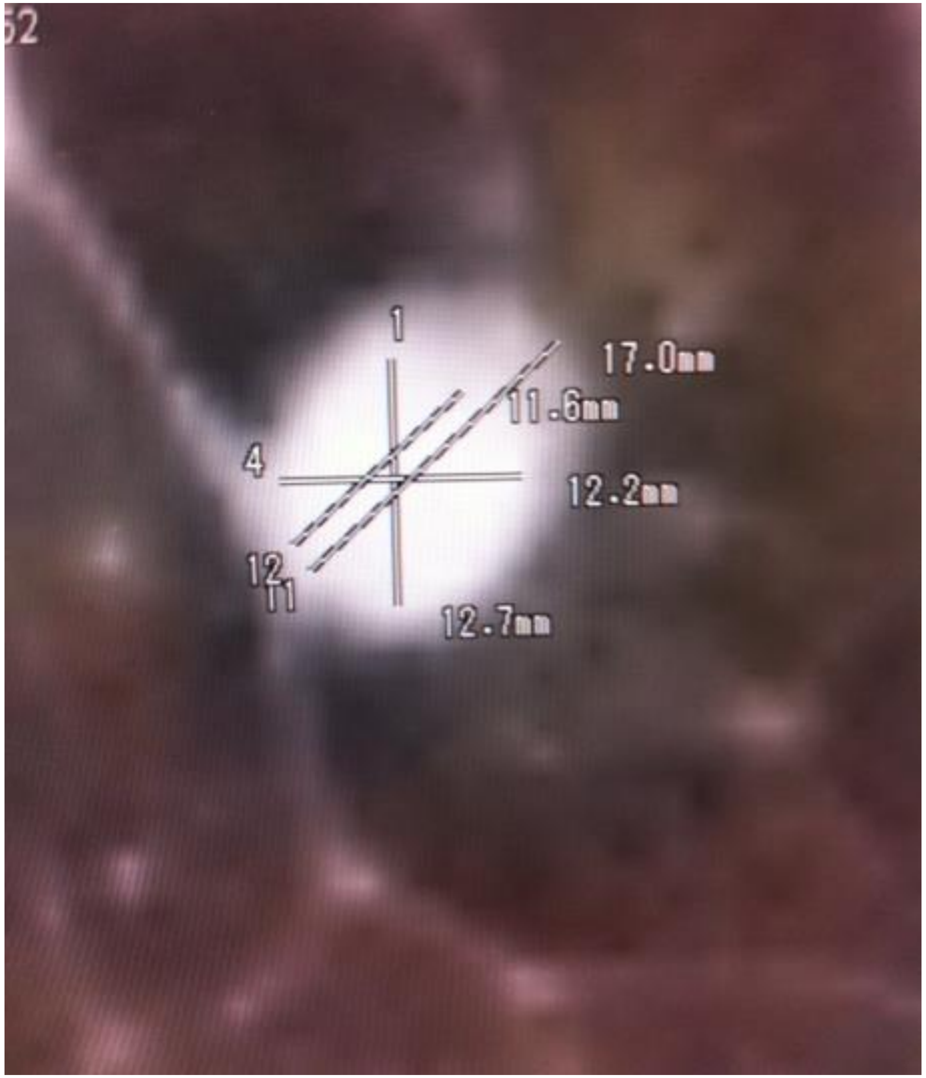
IMG_4190 (1).MOV

Motion artifacts are commonly seen with thoracic CT images

Motion artifacts



Tumor movement



- Diagnosis

- Oligorecurrence of lung cancer

- Treatment

- Radiation Therapy (SBRT)

- Radiation Therapy Dose Prescription:

- PTV (RML nodule): 50 Gy at 12,5 Gy/fraction

Take home message

- Further research is necessary to assess the survival outcome and late toxicity with a longer follow-up for oligometastatic lung cancer
- Different strategies such as 4D repiratory gated acquisition techniques are needed for tumor motion control
- The consecuences of lower doses (“bath dose”) in the OAR is still unknown

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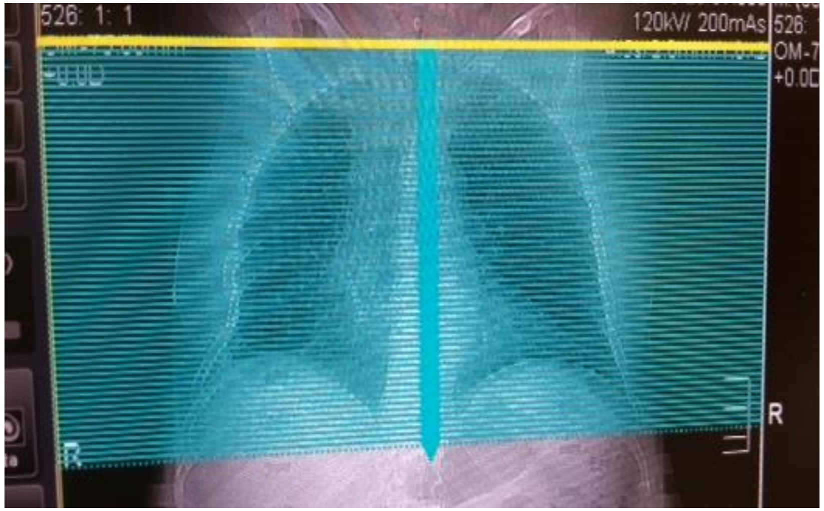

Questions:

- Immobilization
- Positioning
- Organ at risk contouring
- Set-Up
- Verification
- Radiation technique

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WWW.ESTRO.ORG/SCHOOL

Case reports: **Lung**

Mirjana Josipovic

Dept. of Oncology, Rigshospitalet
& Niels Bohr Institute, University of Copenhagen
Denmark

Advanced skills in modern radiotherapy
June 2017

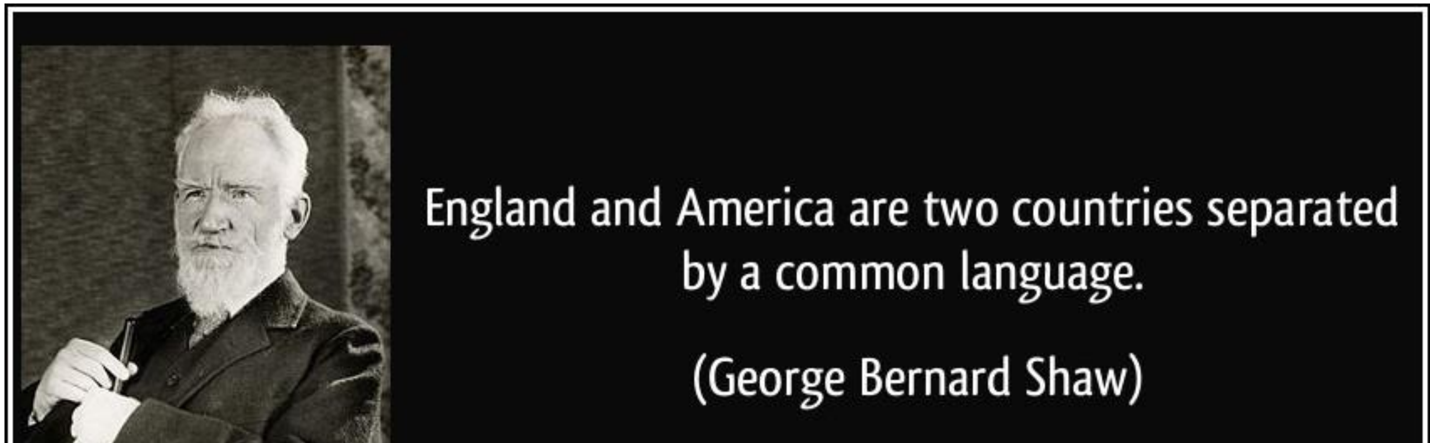
Dose prescription in lung SBRT

Danish national guidelines for lung SBRT

- Prescribed dose: 22 Gy x 3
  - ➢ To the isocenter
  - ➢ PTV encompassed by 15 Gy isodose

Nordic SBRT study group (& Rigs)

- Prescribed dose : 15 Gy x 3
  - ➢ To the PTV encompassing isodose
  - ➢ Isocenter dose should be 22 Gy / fraction



Dose prescription in lung SBRT

Table 1
Patient and treatment details: conformity index (CI) is defined as the volume enclosed by the prescription isodose divided by the PTV volume. Delta[4] phantom was used to measure gamma agreement index (GAI, 2 mm/3%).

Patients	Tumor site	PTV (ccm)	Treatment schedule	Energy	# arcs	# MU	Mean DR (MU/min)	Max DR (MU/min)	Mean treatment time (min)	Mean overall time (min)	GAI (%)	CI
P1	Lung	15.6	8 × 4.5 Gy @70%	X6FFF	2	1074	851	1200	1.26	18.2 (±4.4)	99.3	1.06
P2	Lung	37.7	10 × 5 Gy @80%	X6FFF	1	1563	1351	1400	1.16	26.8 (±7.1)	97.3	1.21
P3	Lung	14.7	5 × 8.5 Gy @85%	X6FFF	2	2530	1225	1400	2.06	18.1 (±4.8)	98.8	1.19
P4, V1	Lung	37.5	3 × 10 Gy @84%	X6FFF	2	3018	1372	1400	2.20	15.5 (±3.9)	98.7	1.07
P4, V2	Lung	37.7	3 × 10 Gy @84%	X6FFF	2	2309	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	1.07
P5	Lung	9.8	4 × 10 Gy @89%	X6FFF	2	3074	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P6	Lung	64.0	10 × 6 Gy @85%	X6FFF	3	1129	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P7	Lung	18.7	15 × 3.3 Gy @85%	X6FFF	2	902	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P8, V1	Lung	14.1	12 × 4 Gy @79%	X6FFF	2	1079	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P8, V2	Lung	5.9	11 × 4 Gy @87%	X6FFF	2	1116	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P9	Liver	36.3	10 × 5 Gy @85%	X6FFF	2	956	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P10	Liver	283.5	10 × 4 Gy @80%	X6FFF	2	1114	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P11	Pancreas	131.8	2 × 6 Gy @78%	X6FFF	1	1258	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P12	Pancreas	24.0	10 × 5 Gy @87%	X6FFF	1	1079	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P13	Lung	27.4	8 × 7.5 Gy @73%	X6FFF	2	1704	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P14	Lung	32.7	12 × 4 Gy @72%	X6FFF	2	1082	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P15	Lung	24.4	4 × 12 Gy @71%	X6FFF	3	4017	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]	[illegible]
P16	Liver	42.9	4 × 10 Gy @75%	X6FFF	2	2139	1374	1400	1.55	18.7 (±5.7)	98.4	0.97
P17	Lung	53.8	4 × 10 Gy @85%	X6FFF	2	2263	1355	1400	1.66	17.6 (±3.6)	100.0	1.04
P18	Pancreas	40.9	2 × 6 Gy @76%	X6FFF	2	1760	1056	1400	2.04	18.3 (±4.0)	98.9	1.00
P19	Pancreas	30.2	2 × 6 Gy @75%	X10FFF	2	1851	1842	2400	1.05	17.9 (±1.2)	97.8	0.99
P20	Liver	131.8	4 × 12 Gy @80%	X6FFF	2	3860	1396	1400	2.78	15.3 (±3.3)	99.5	0.98
P21	Lung	19.6	4 × 12 Gy @79%	X6FFF	4	3974	1302	1400	3.01	14.0 (±2.1)	99.4	1.02
P22	Adrenal	53.5	3 × 10 Gy @78%	X10FFF	2	3813	1860	2400	2.03	22.5 (±5.1)	98.9	1.01
P23	Lung	22.6	4 × 12 Gy @84%	X6 FFF	2	5668	1396	1400	3.36	13.5 (±2.7)	97.9	1.20
P24	Adrenal	77.9	4 × 10 Gy @88%	X6 FFF	2	3172	1198	1200	2.65	19.7 (±4.1)	99.6	1.02
P25	Lung	40.7	10 × 5 Gy @79%	X6FFF	2	1364	993	1400	1.38	16.2 (±3.9)	99.2	1.06
P26	Lung	61.7	5 × 7.5 Gy @78%	X10FFF	2	2170	1076	2400	2.02	18.0 (±2.4)	98.3	1.02

No international consensus on dose prescription in SBRT

…not yet…

Caution when interpreting literature!

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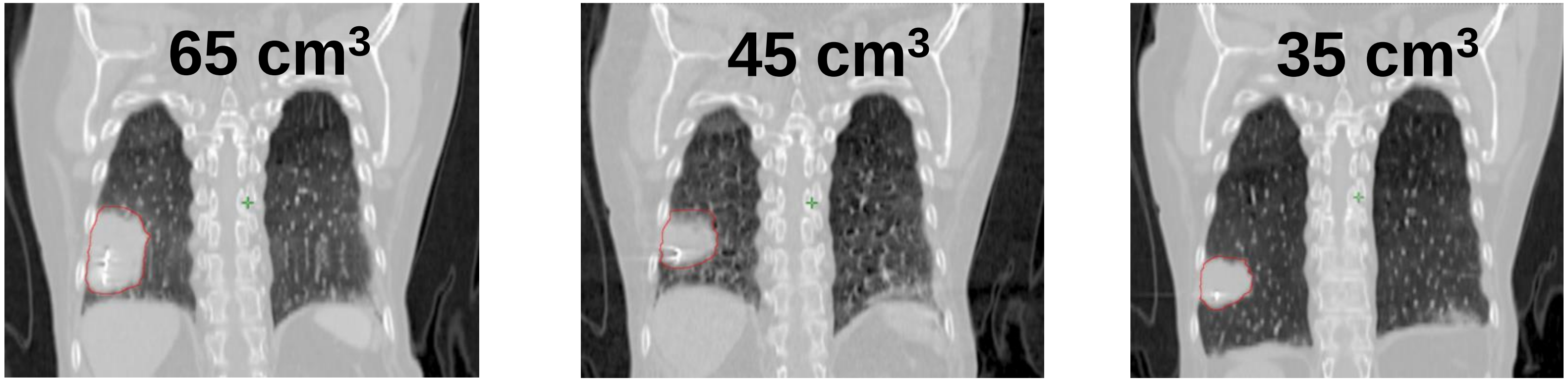
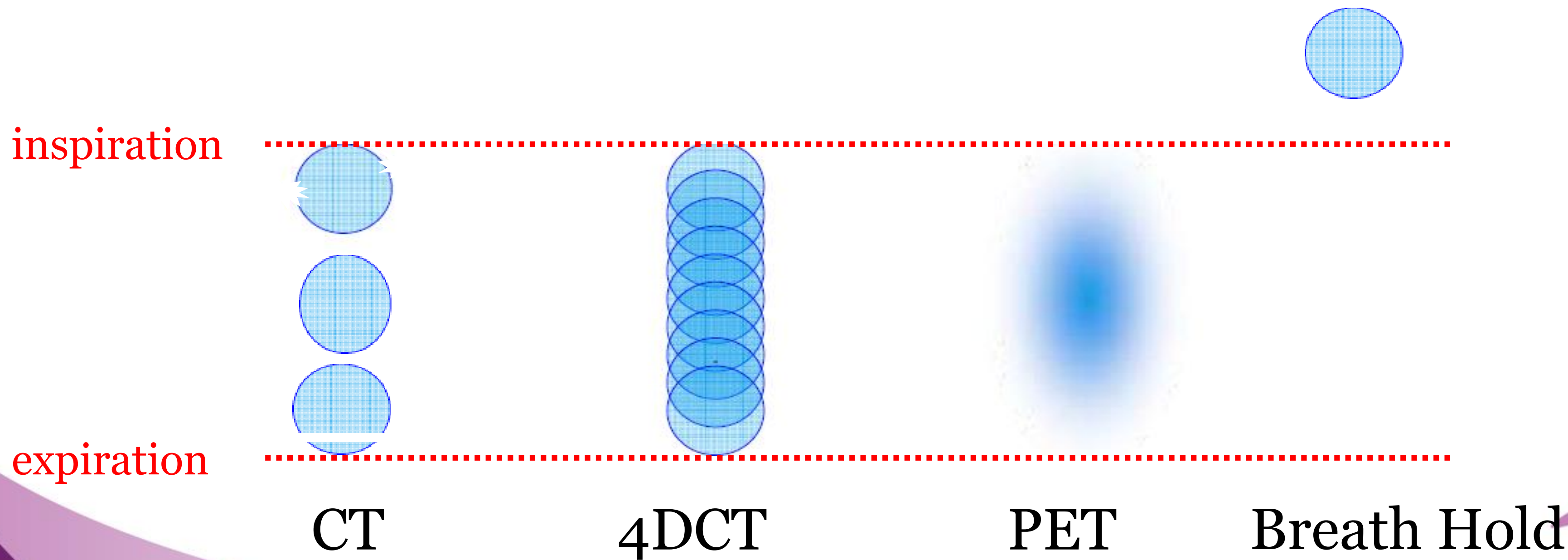
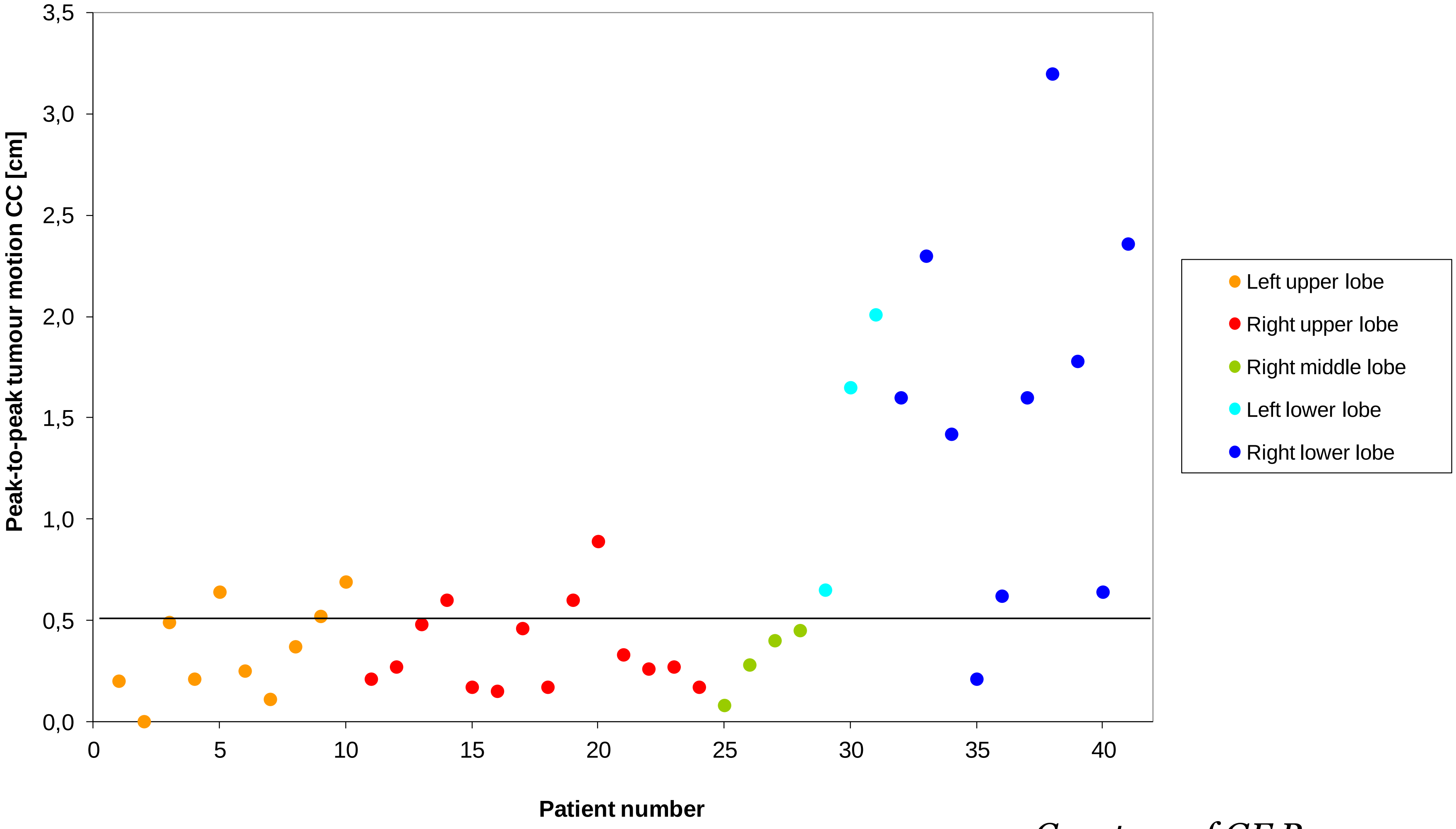
Pre-treatment imaging in lung cancer

- What is the true tumour size?



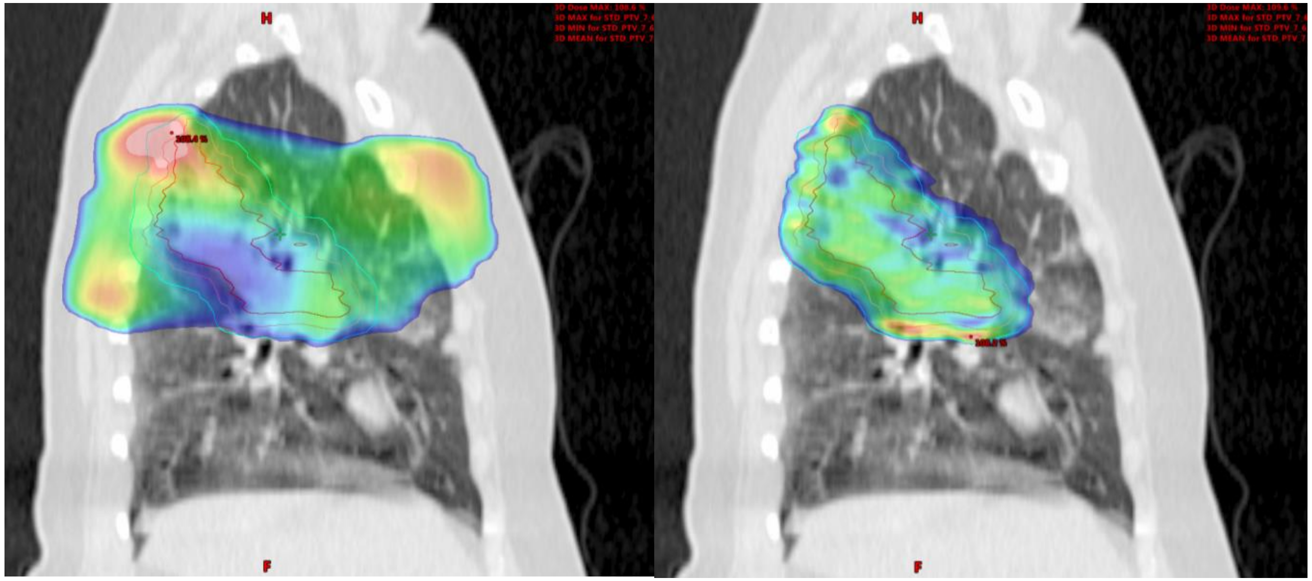


How much do lung tumours move?



Courtesy of GF Persson

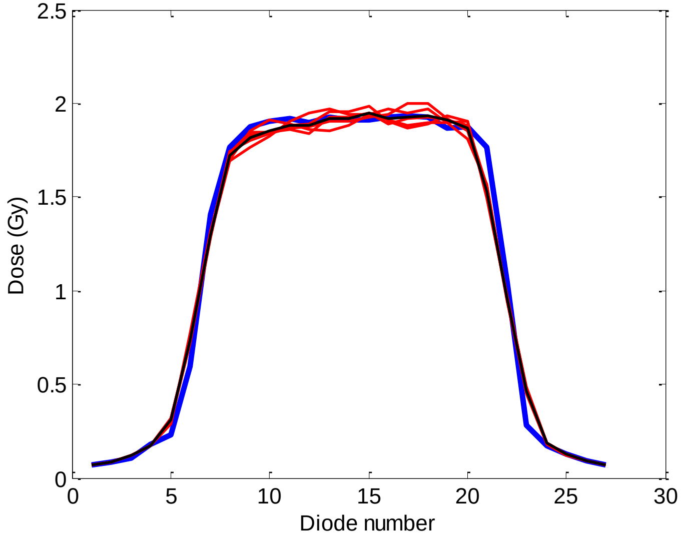
3D conformal vs. VMAT technique

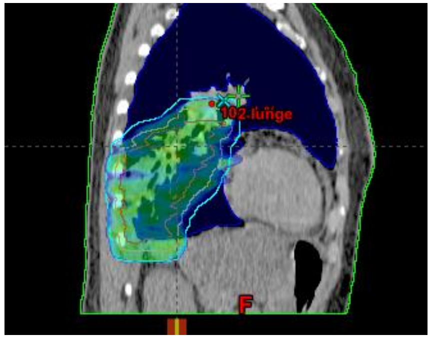


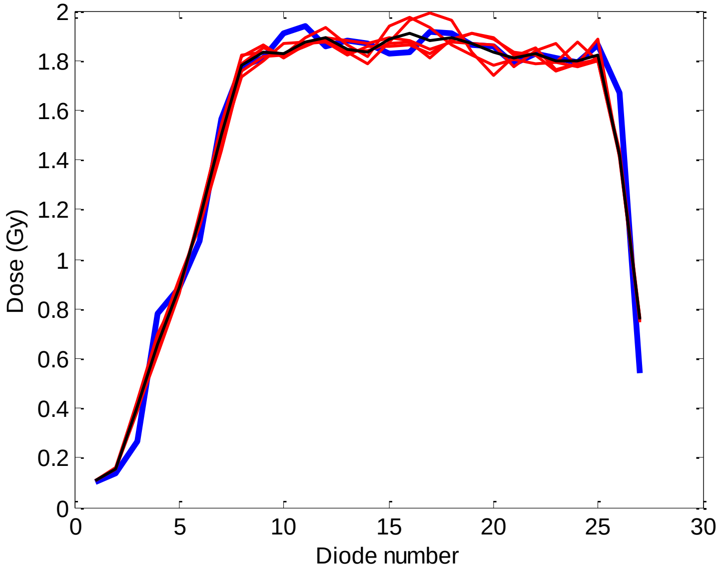
3DC

VMAT

Interplay effect?



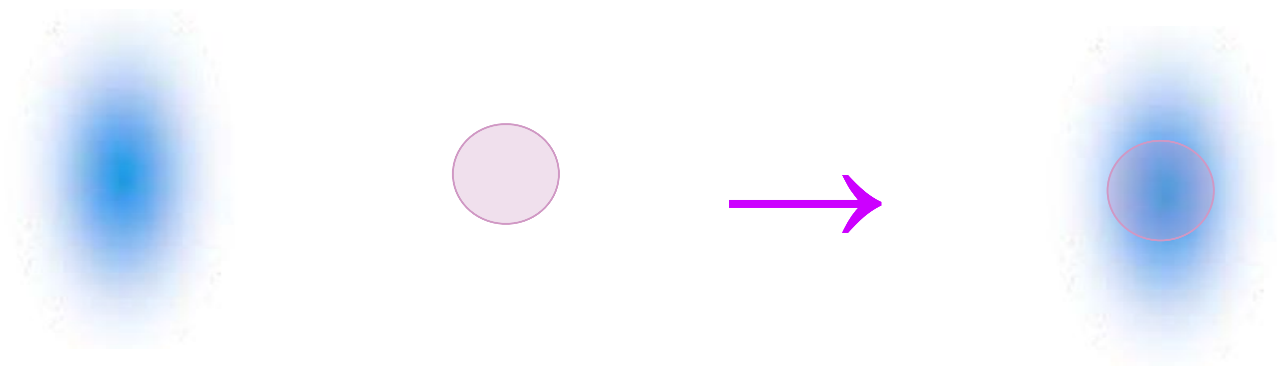




2 cm respiration amplitude

Daily treatment verification

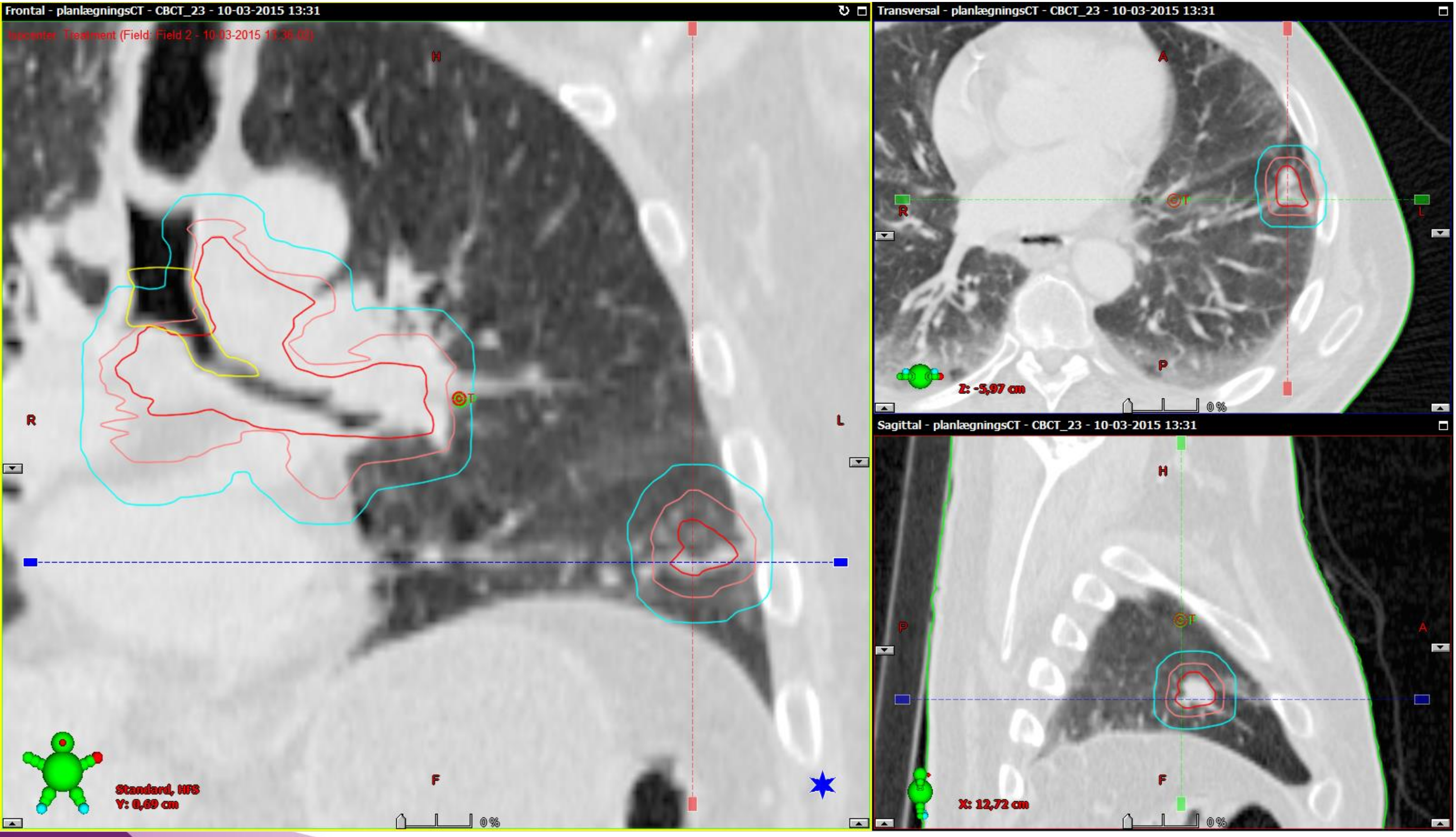
- CBCT acquisition takes ~1 min
  - ➢ Tumour visualisation on CBCT is blurred



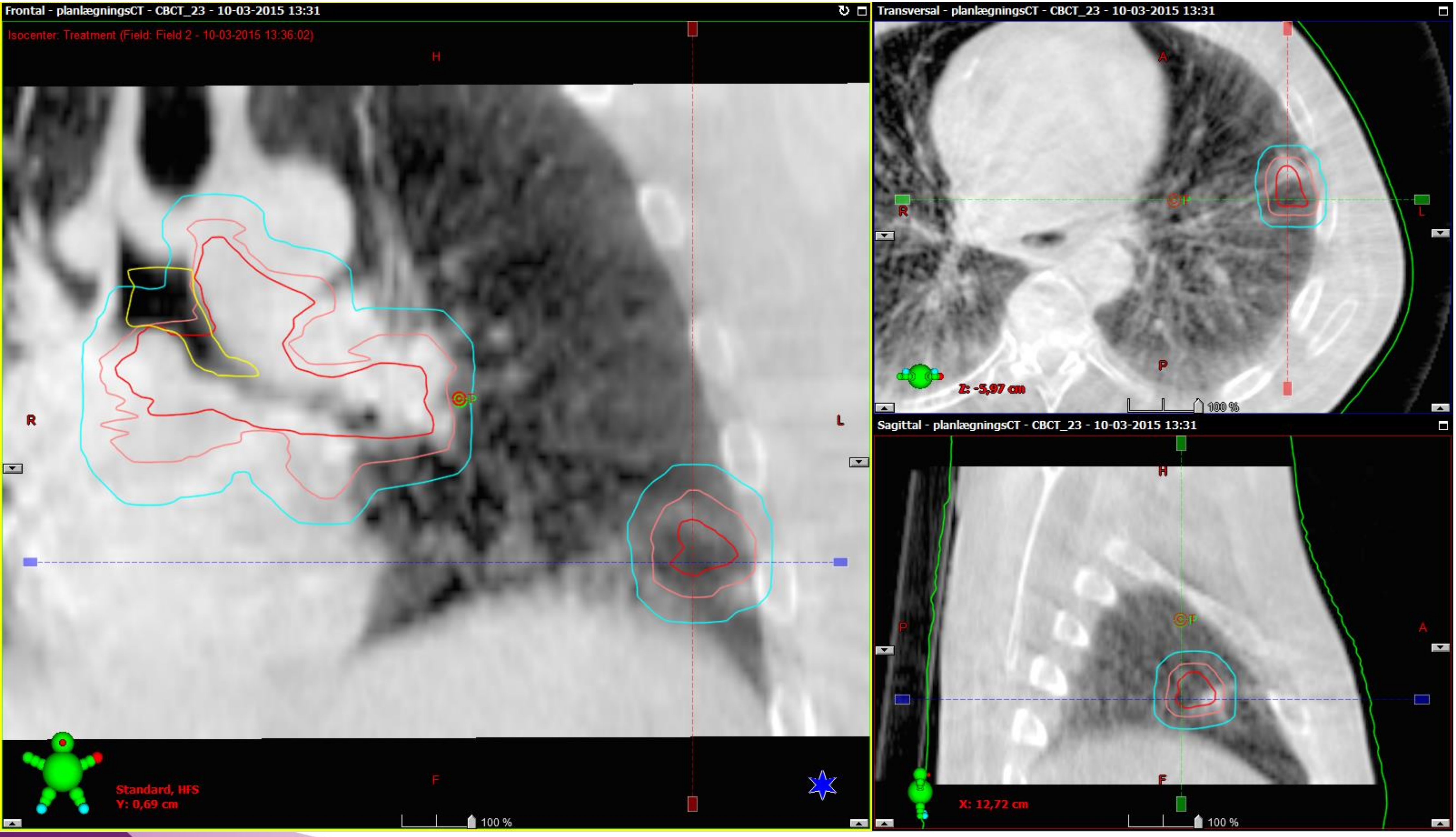
CBCT CT (MidV) match

- ➢ ...but the image signal (of the tumour) on CBCT is strongest where the tumour is most of the time

Case – locally advanced lung cancer



Case – locally advanced lung cancer



Case – differential motion

The correct answer is…

- What is your IGRT strategy?
- How are your margins designed?

- Is it the first time, (too) large differential motion was observed?

Margins – complex target & daily IGRT

Peripheral tumour registration

10.4 mm

6.3 mm

10.4 mm

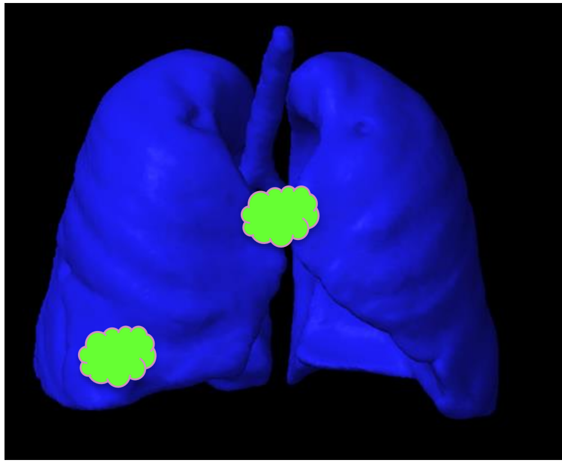
margin for mediastinum

Carina registration

5.4 mm*

6.1 mm*

5.1 mm*



4.4 mm

5.0 mm

3.2 mm

margin for peripheral tumor

9.9 mm

6.7 mm

9.9 mm

CC

AP

LR

Josipovic et al, Radiotherapy & Oncology 2016

Individual margins

Based on van Herk's margin formula

$$PTV\ margin \quad = \quad \alpha\,\Sigma + \beta\sqrt{\sigma^2 + \sigma_p^2} - \beta\sigma_p$$

- Respiration amplitude / breath hold reproducibility
- Uncertainties evaluated base on your own data
  - Tumour baseline shift
  - 3D instead of 6D match
  - Delineation uncertainty
  - Differential motion
- No. of fractions
- Penumbra width
  - Lung/bone/softtissue

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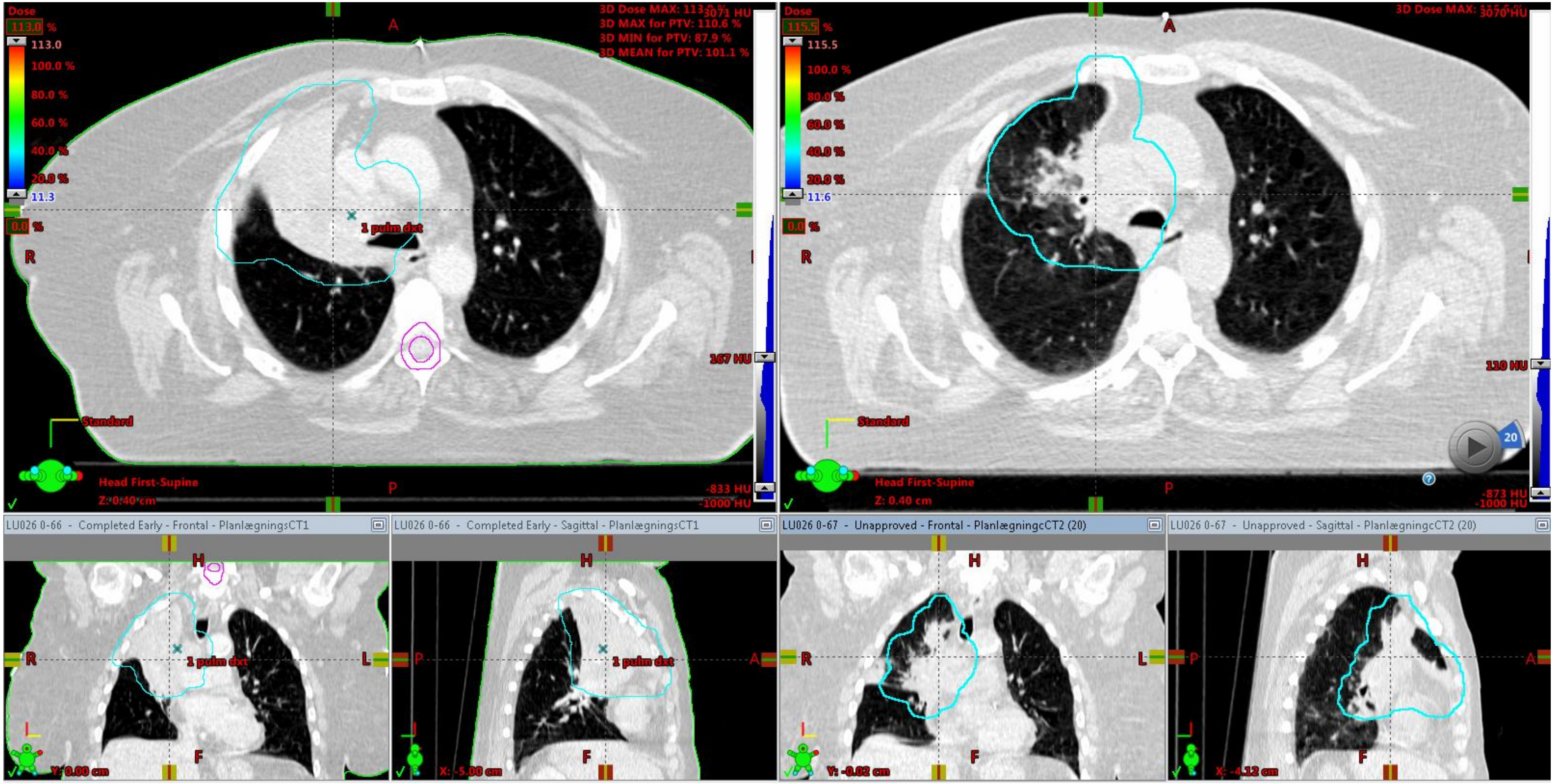
IGRT – uncertainties

- Differential motion
  - Displacement of primary tumour to/from the glands
- Tumour shrinkage during a course of 33 fractions
- Anatomical changes (atelectasis, weight loss, pleural fluid, …)

Day 1 Day 11



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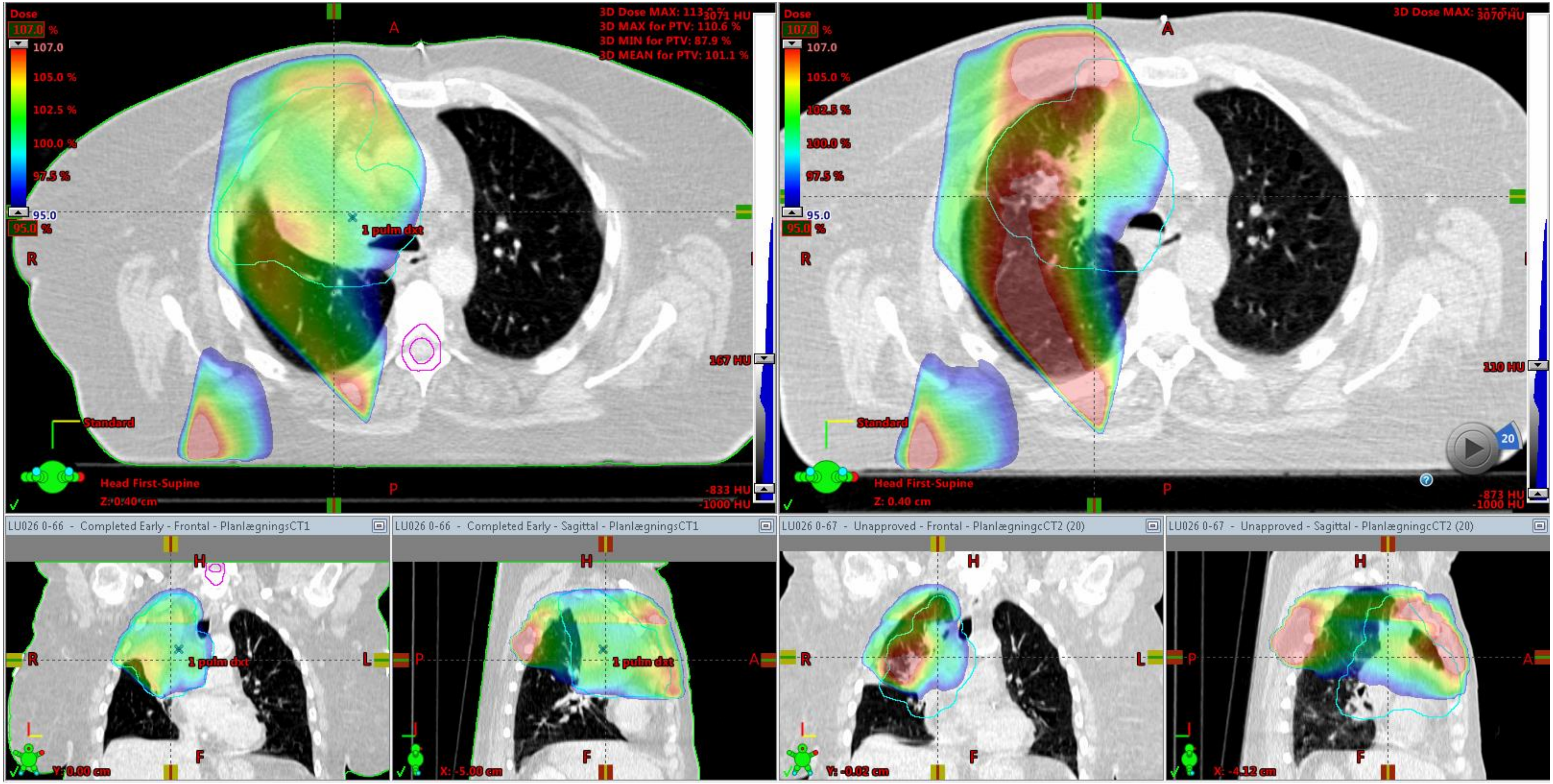
Day 1 Day 11

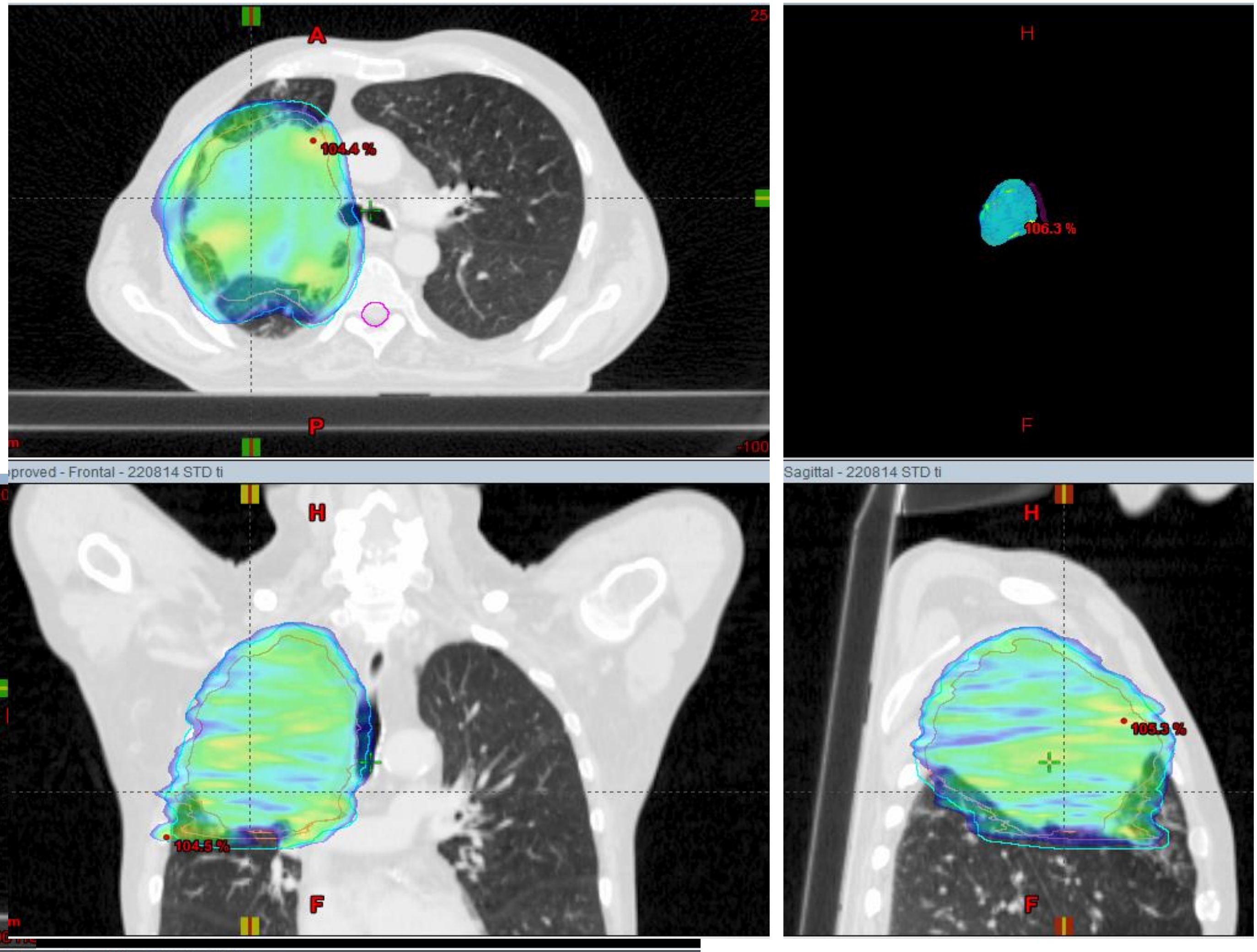


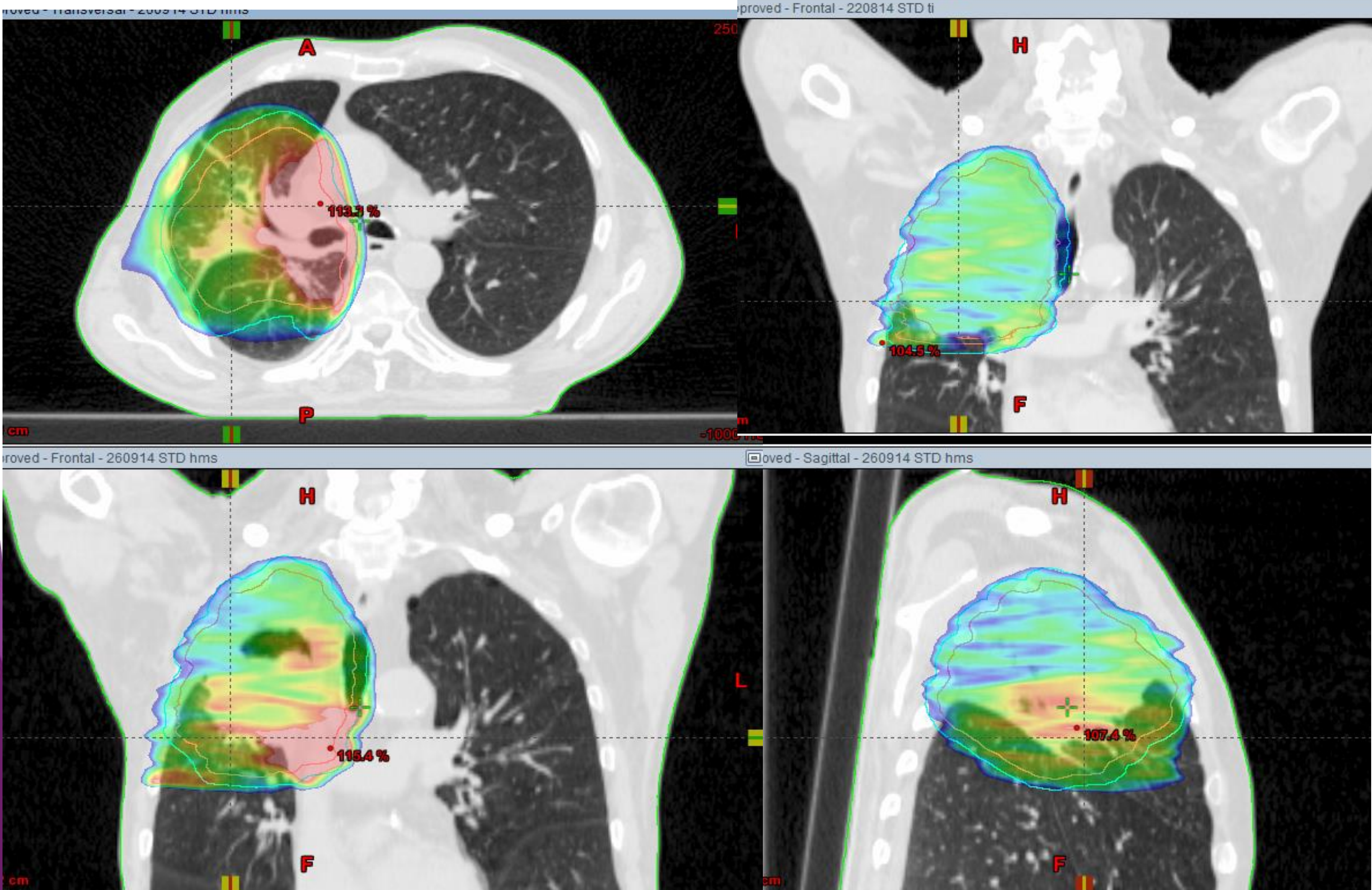
3DC RT

Dmax 107 →115%
Dmean 100 → 91 %

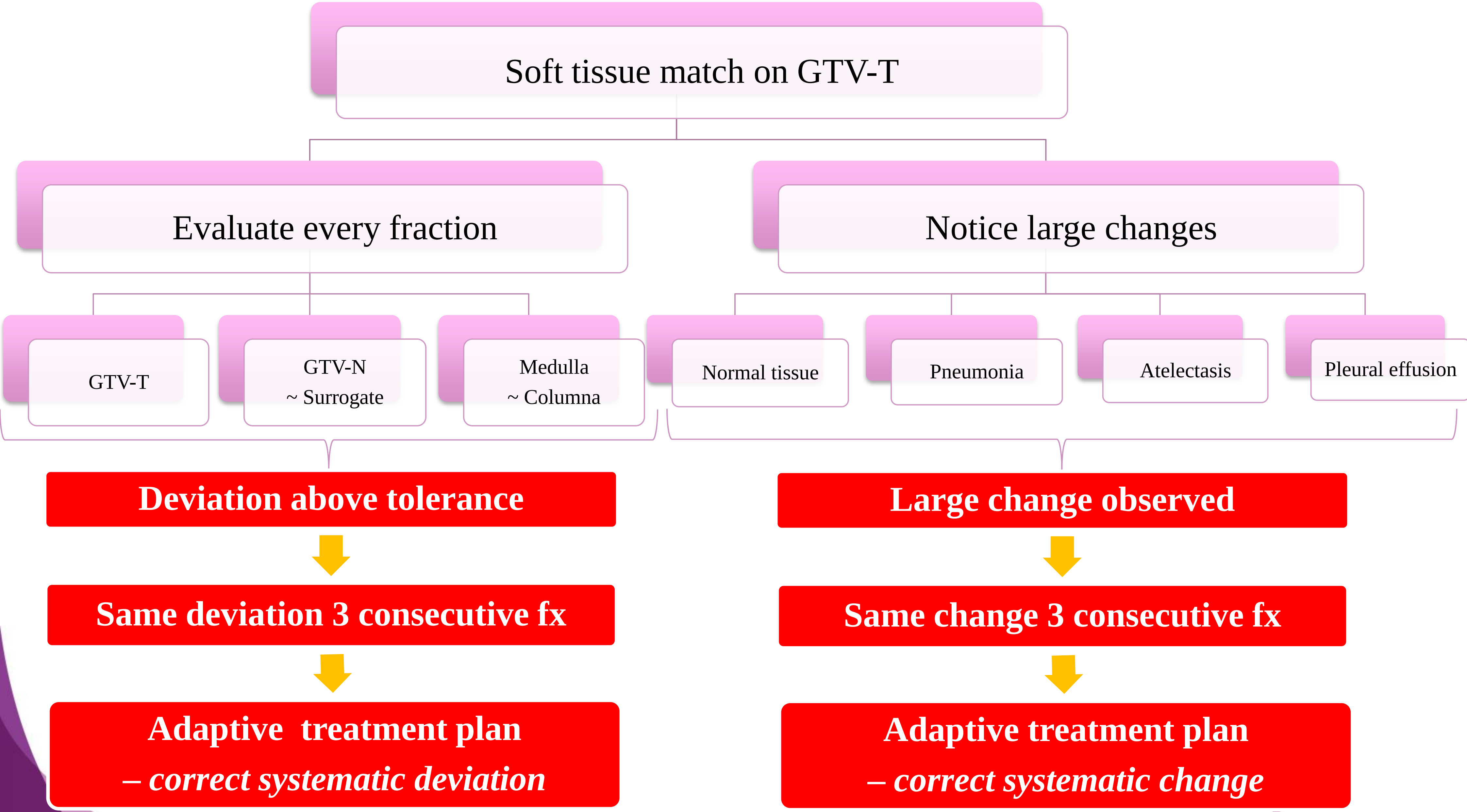
VMAT

Dmax 106 →117%
Dmean 100 → 102.4 %





Example of adaptive strategy in lung cancer RT



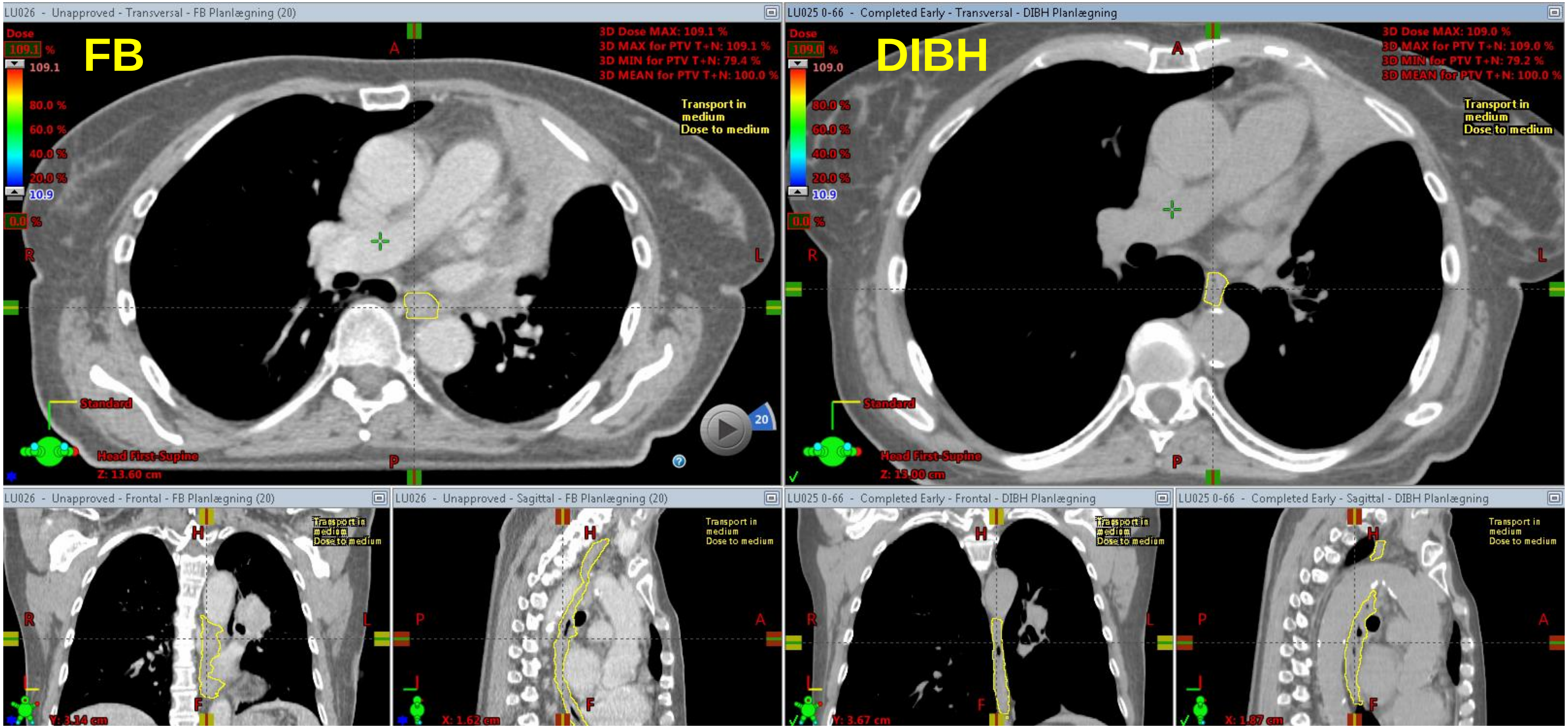
Courtesy of D Møller & L Hoffman, Aarhus, DK

IGRT does not solve all challenges

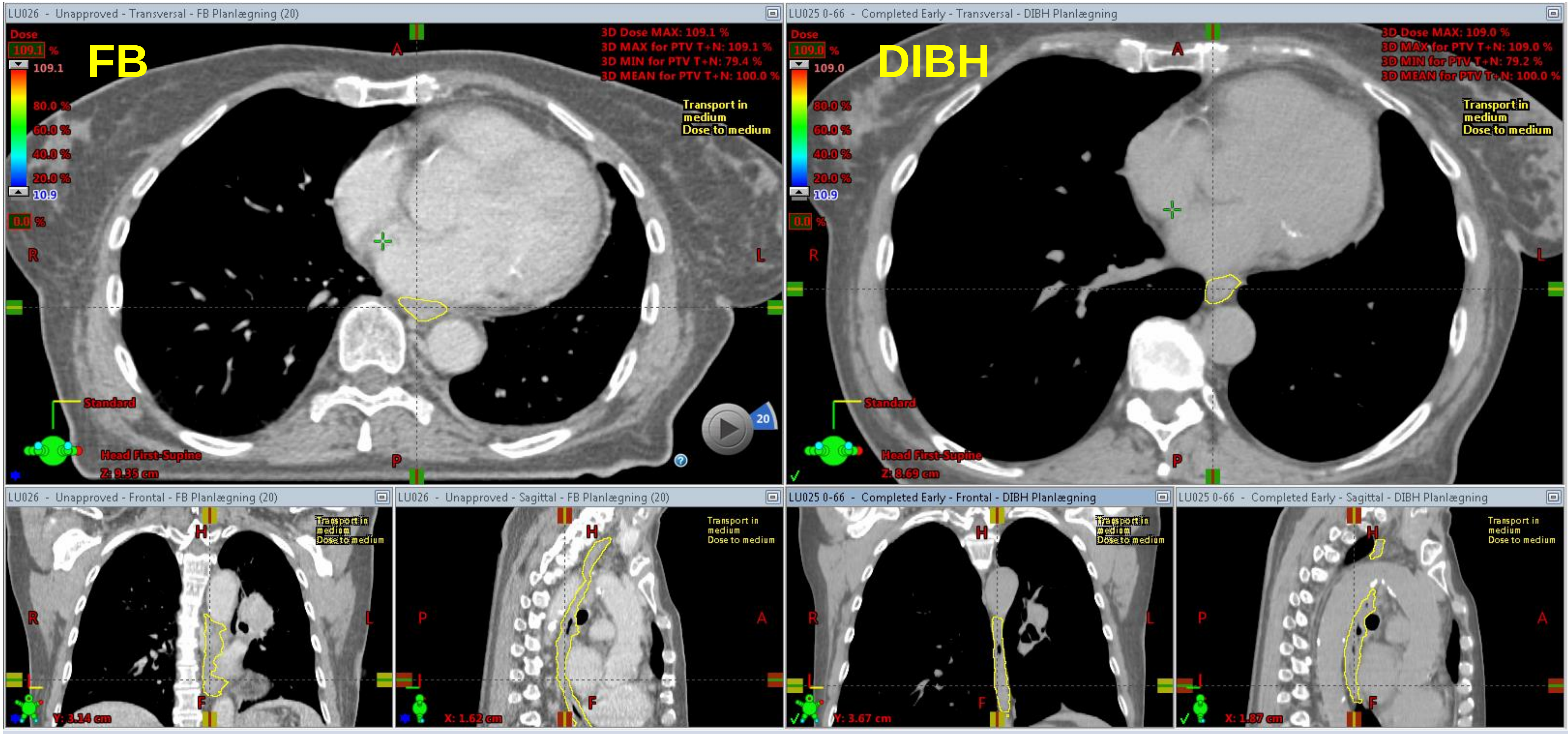
- When has the anatomical change a significant impact on the treatment
  - i.e. when is it necessary to re-plan the patient?

- How to do the plan adaptation?
  - No published guidelines as yet.
  - Usually, conservative approach with the unchanged CTV delineation is applied

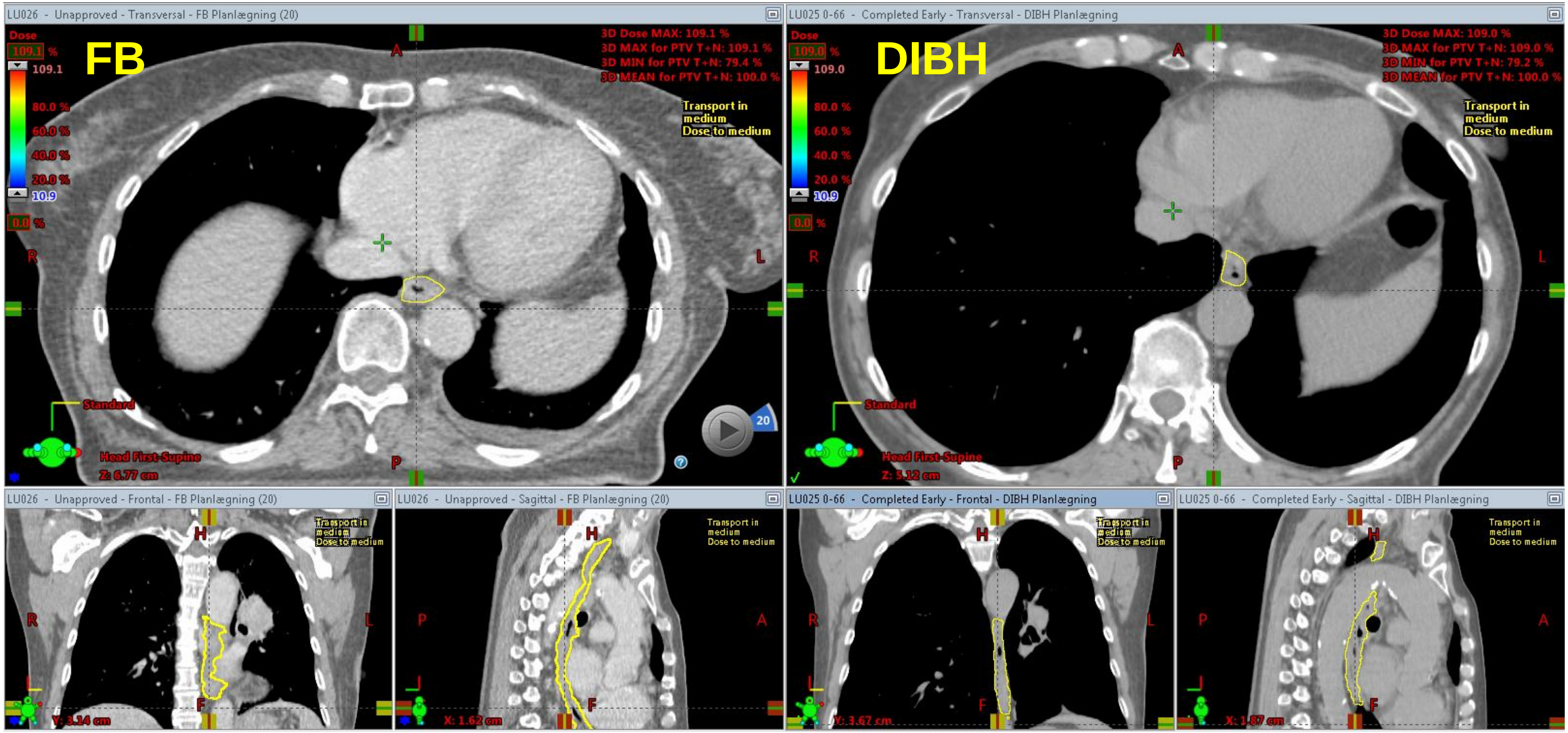
Oesophagus delineation – FB vs DIBH

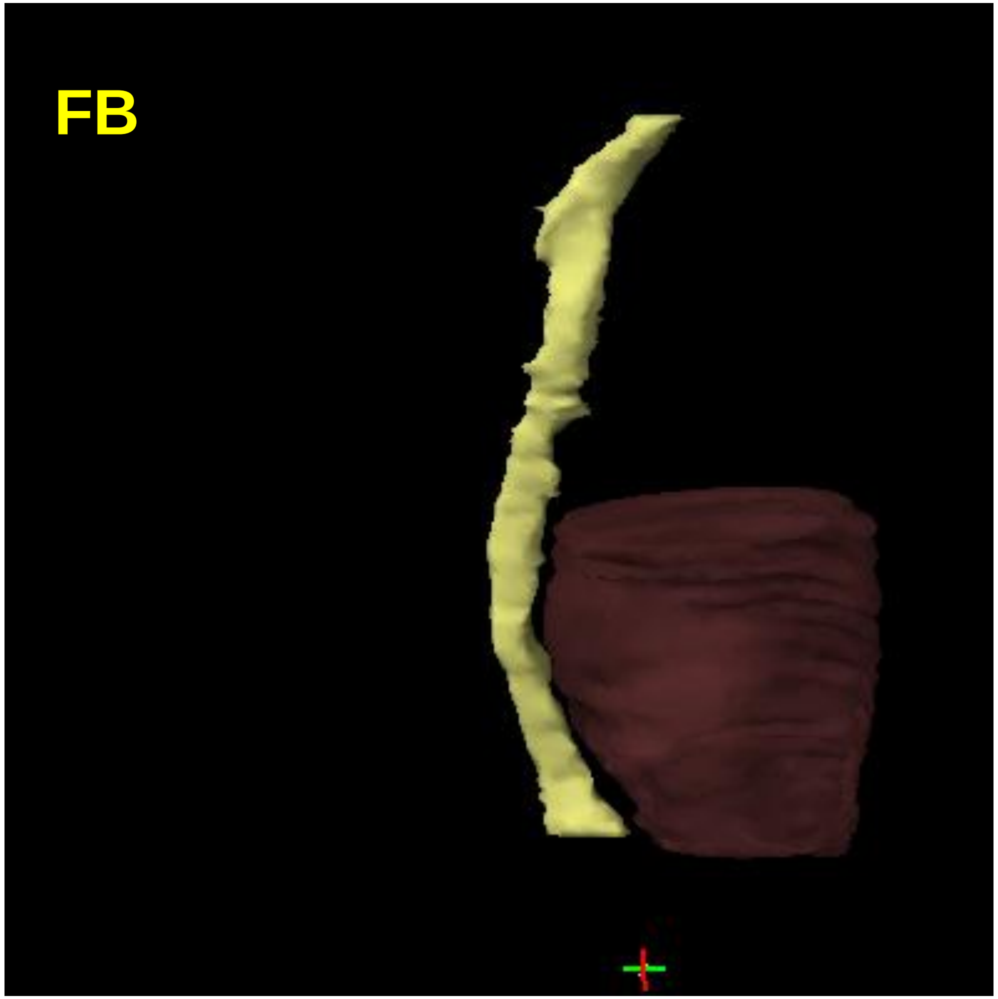


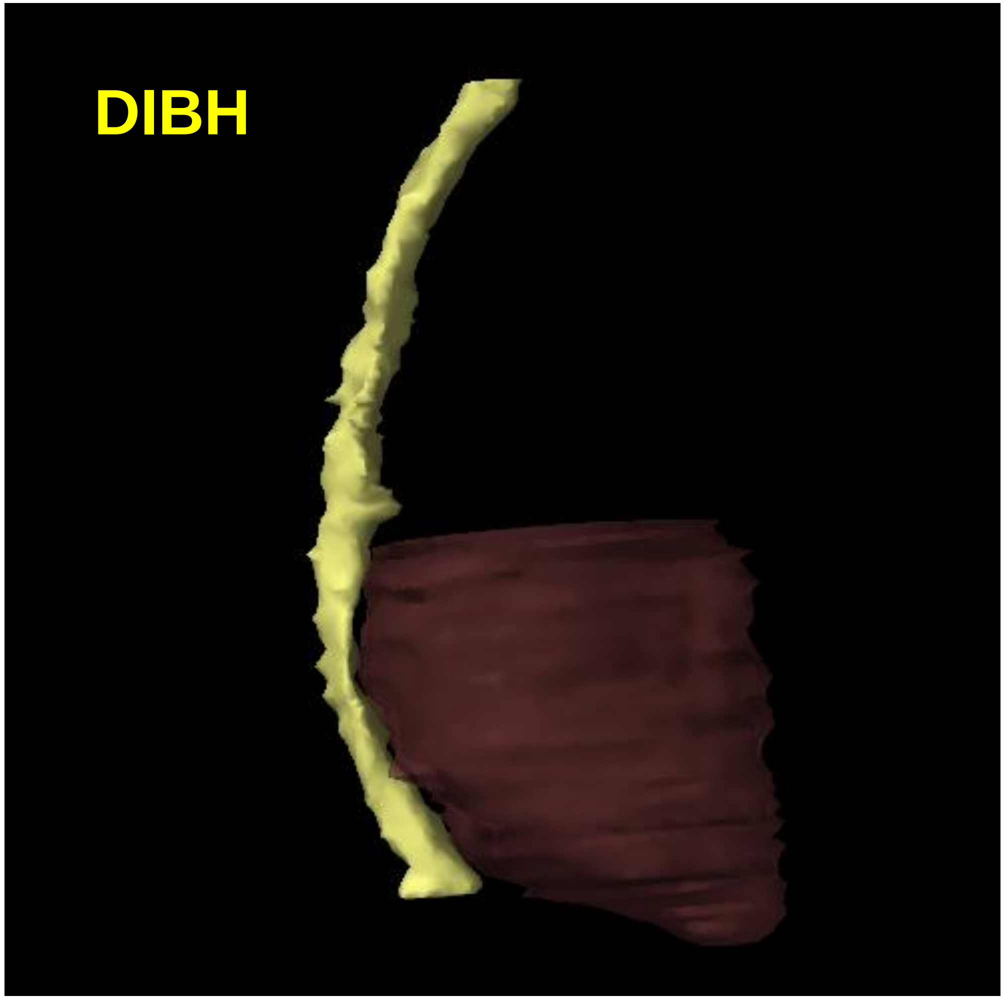
Oesophagus delineation – FB vs DIBH

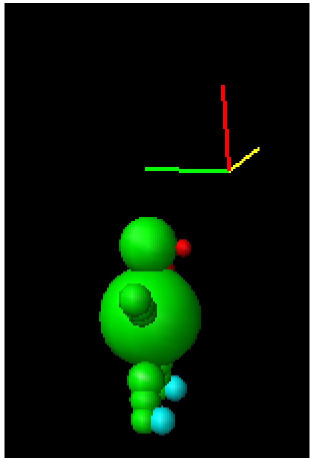


Oesophagus delineation – FB vs DIBH









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Lung SBRT on the linac

Martijn Kamphuis MSc
Research Radiation Therapist IGRT

Department of Radiotherapy @ AMC
Amsterdam, the Netherlands

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Key features SBRT

- Reproducable rigid patient fixation
- Managing tumor motion:
  - ➢ During imaging
  - ➢ During planning
  - ➢ During RT
- Very steep dose gradients
- Extreme high BED (100-180 Gy)
  - ➢ 66Gy/2,75Gy→BED 85 Gy
  - ➢ 3*20Gy →BED 180 Gy (Δ 95 Gy)

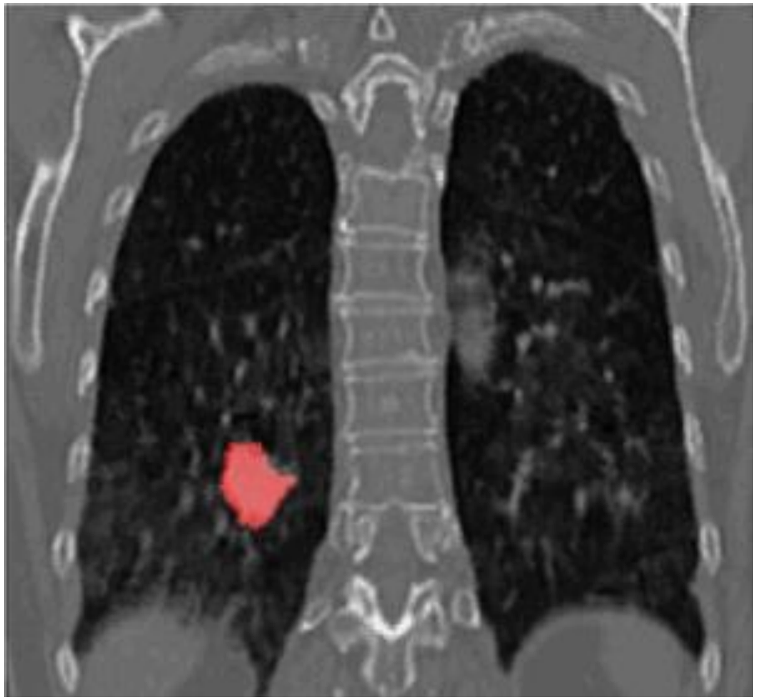
What do we have to manage?

Intra fraction motion

- Breathing pattern

Inter fraction motion

- Baseline shift

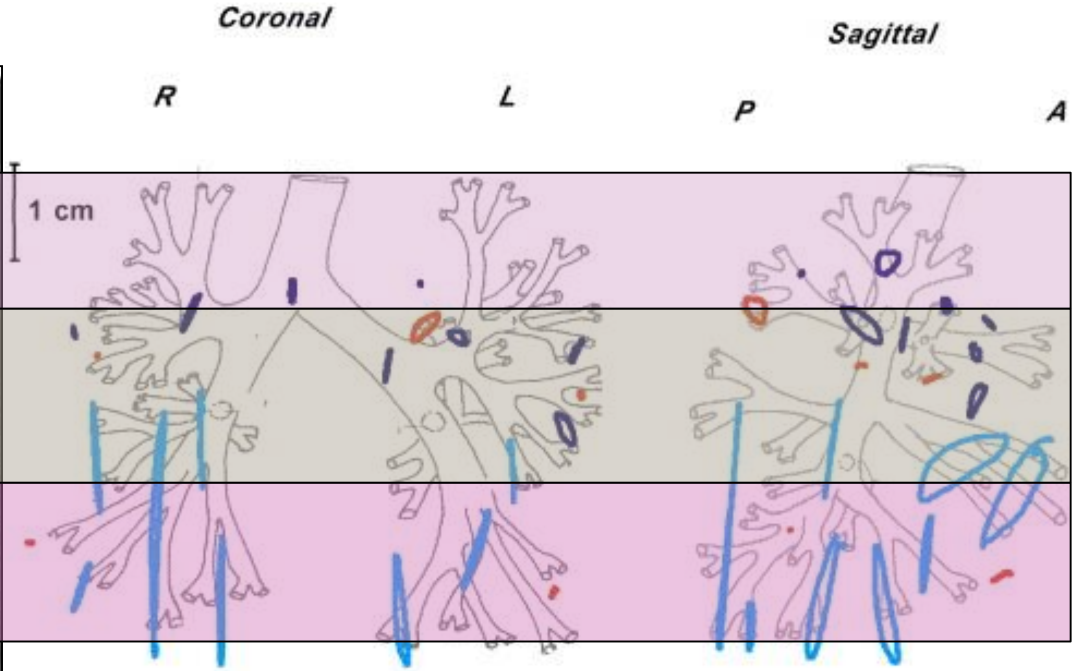


https://www.imi.uni-luebeck.de

Intra fraction motion: amplitude

CC	ML	AP
4.3 ± 2.4 (2.6 to 7.1)	3.4 ± 1.6 (1.3 to 5.3)	2.8 ± 1.3 (1.2 to 5.1)
7.2 ± 1.8 (4.3 to 10.2)	4.3 ± 2.4 (1.5 to 7.1)	4.3 ± 2.2 (1.9 to 7.5)
9.5 ± 4.9 (4.5 to 16.4)	6.0 ± 2.8 (2.9 to 9.8)	6.1 ± 3.3 (2.5 to 9.8)

Tumor mobility in quiet respiration [mm]



Seppenwolde et.al.

Managing intra fraction motion

Passive approaches

Slow scanning

Multi CT scanning

Inhale&exhale scanning

Abdominal compr…

ITV concept

Mid-v…

Acti… …oaches

…acking

…oach tracking

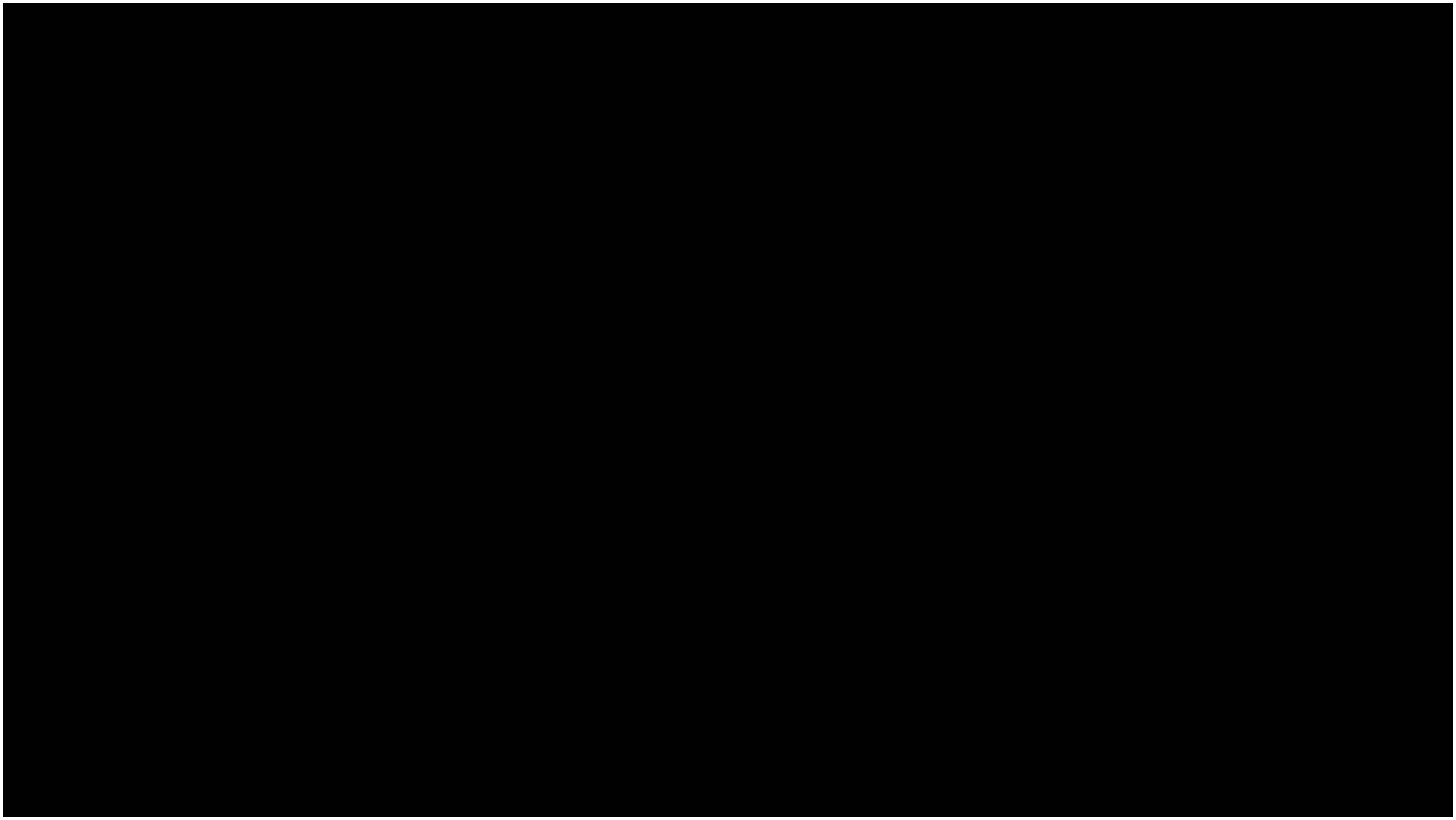
Breathhold

Gating

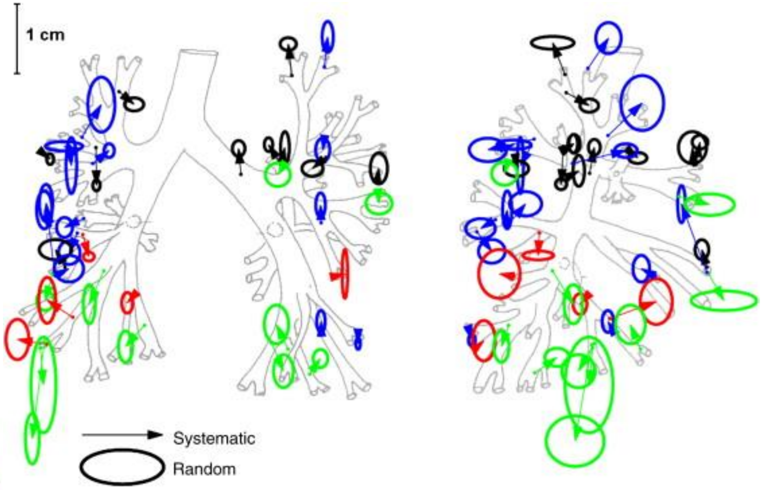
Chasing/tracking

Mirjana took care off this part ☺

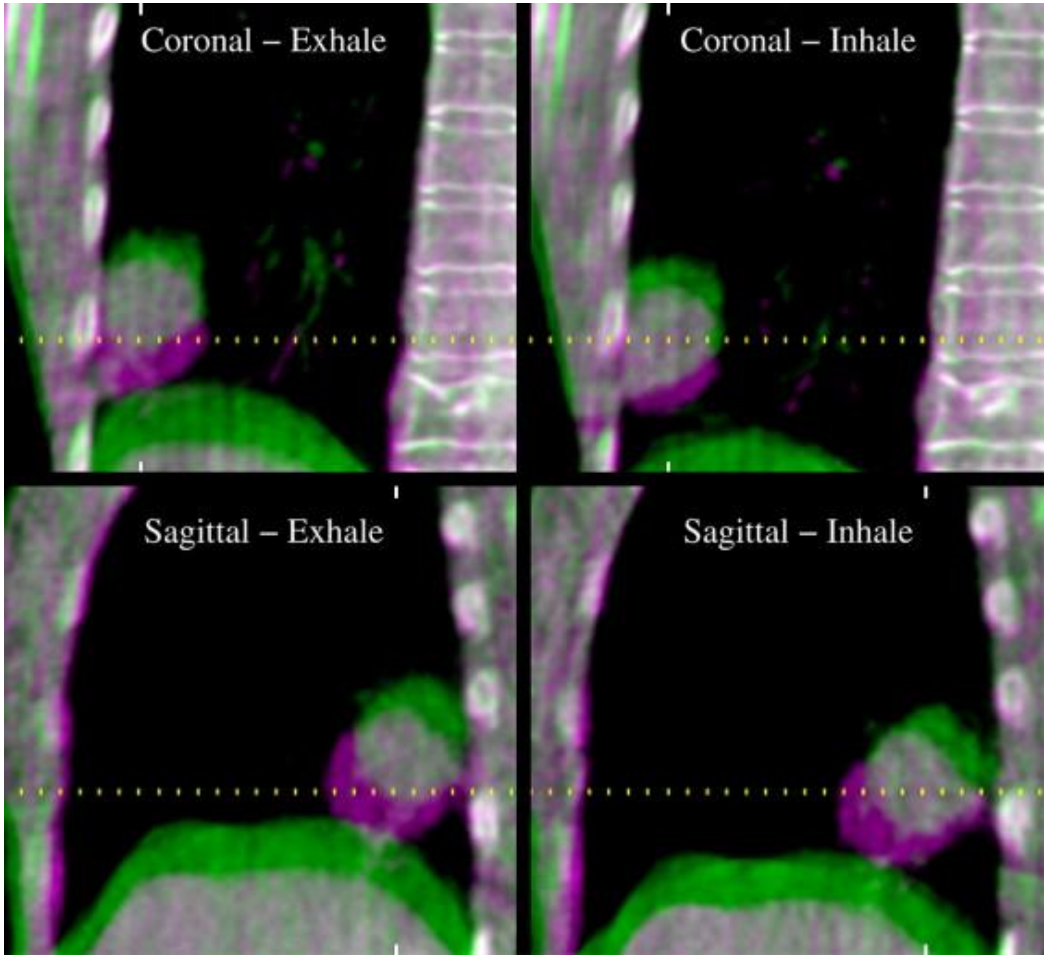
Inter fraction motion: baseline shift



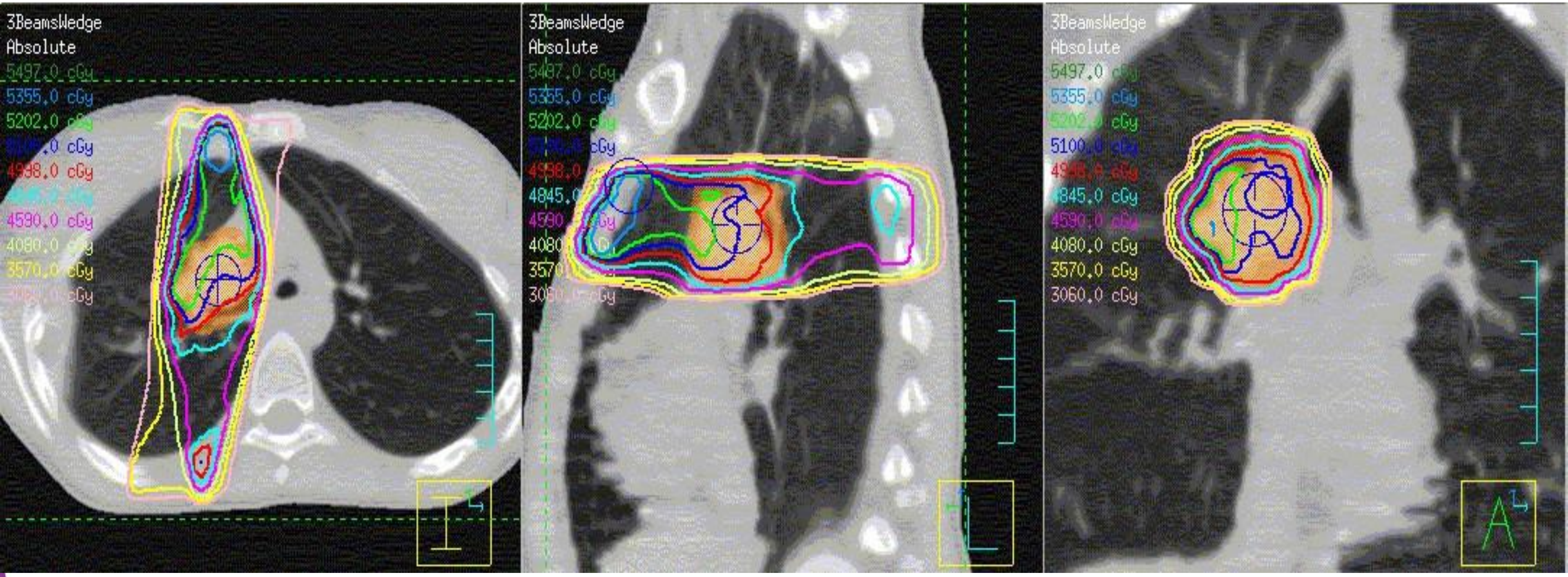
Baseline shift



J.J. Sonke *et al*, 2007



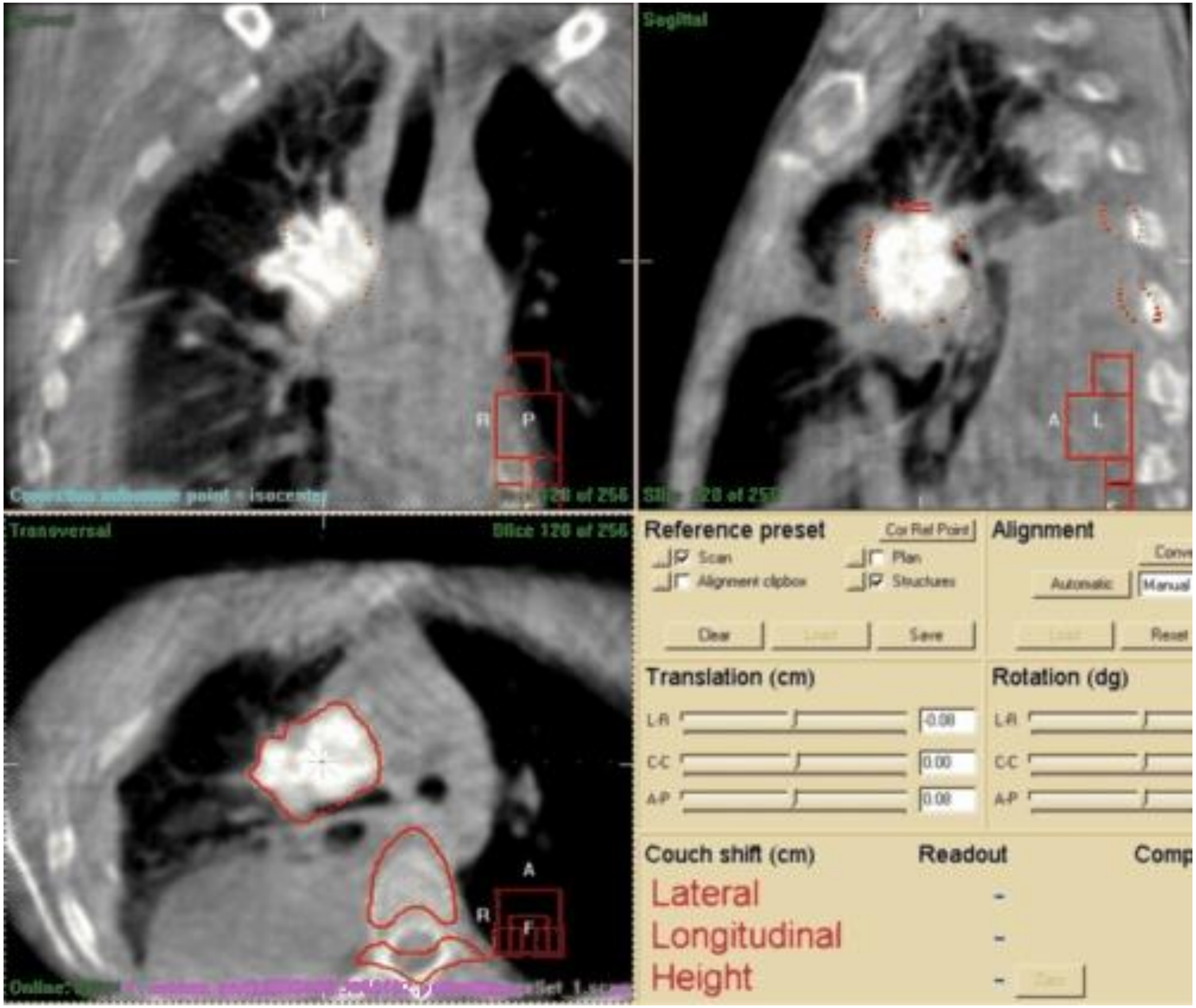
Plan: 3 wedged fields, 300 cGy/fx, 5100 cGy total



Courtesy to Alvaro Martinez

Beaumont
William Beaumont Hospital

ESTRO School



If corrected online on CBCT

Courtesy to Alvaro Martinez

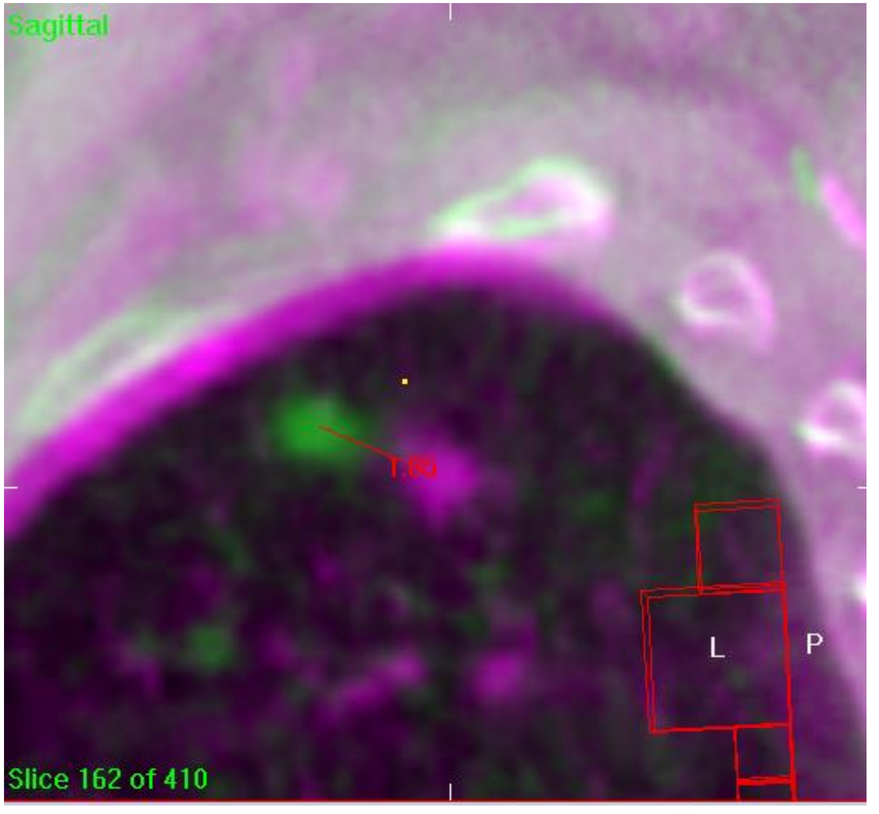
Management of baseline shifts

Introduction of the Planning Risk Volume (PRV)

•Margin around OAR

Combined with:

1. Commercial software
2. Critical isodose line



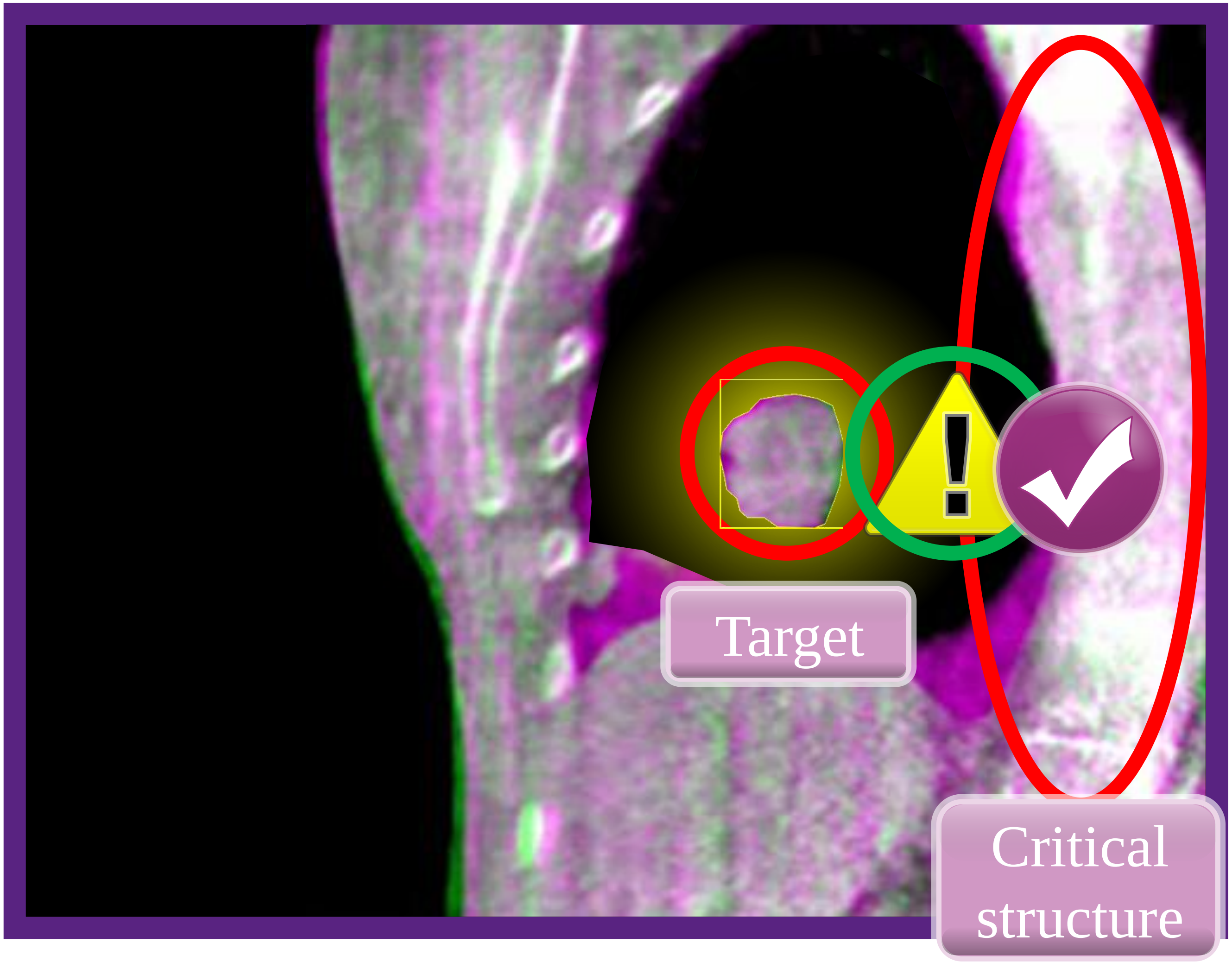
Option 1: NKI/ELEKTA solution

- Image registration on tumor & OAR (dual registration)

- Allowed deviations in distances between tumor and OAR deteremined on Treatment planning
  - Based on dose distributions

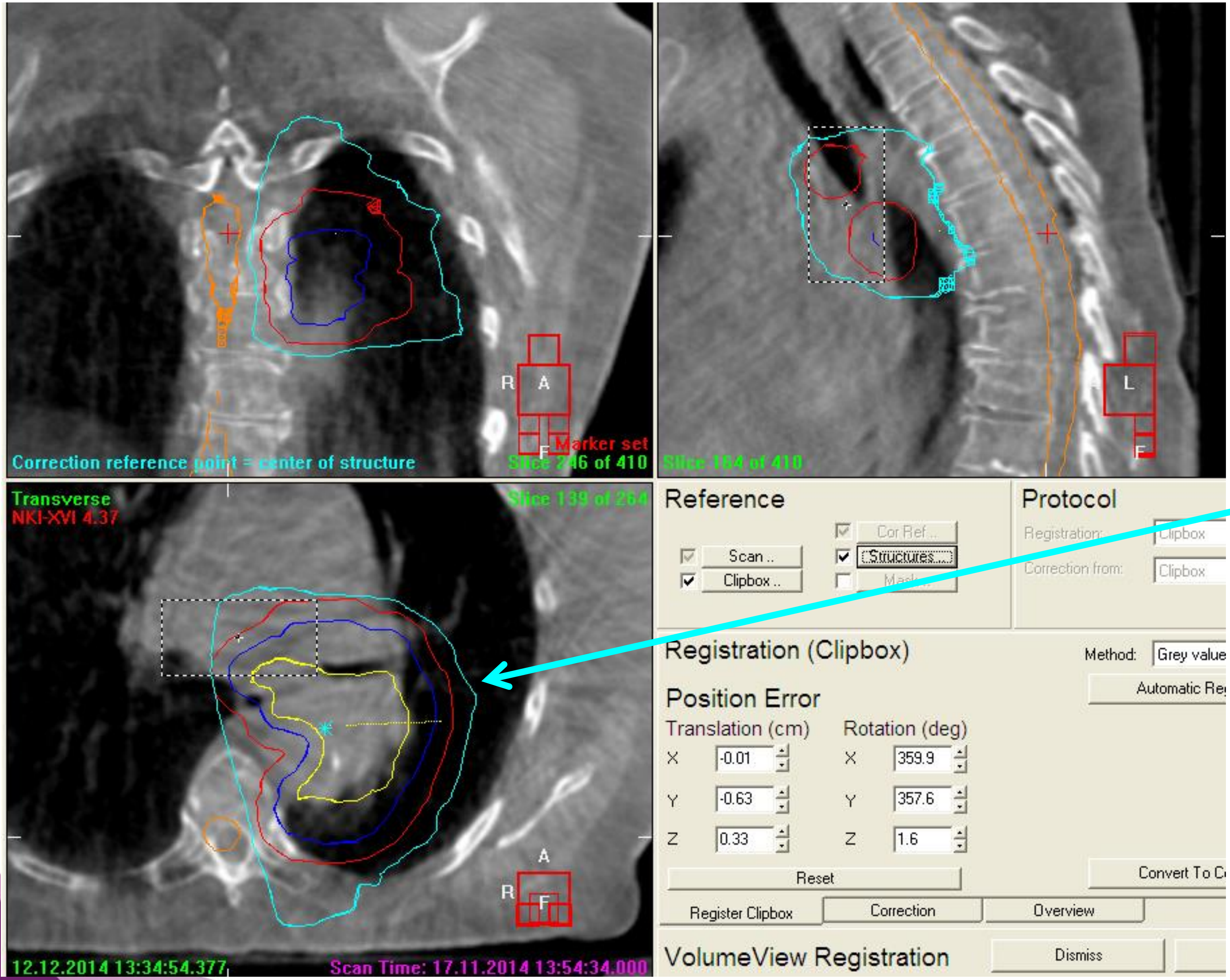
- Personal margins are put into the CB-system
  - E.g. 5mm to the Left, 15 mm to the Right

Option 1: NKI/ELEKTA solution



Critical Structure Avoidance (Dual Registration)

Option 2: critical isodose



51 Gy isodose

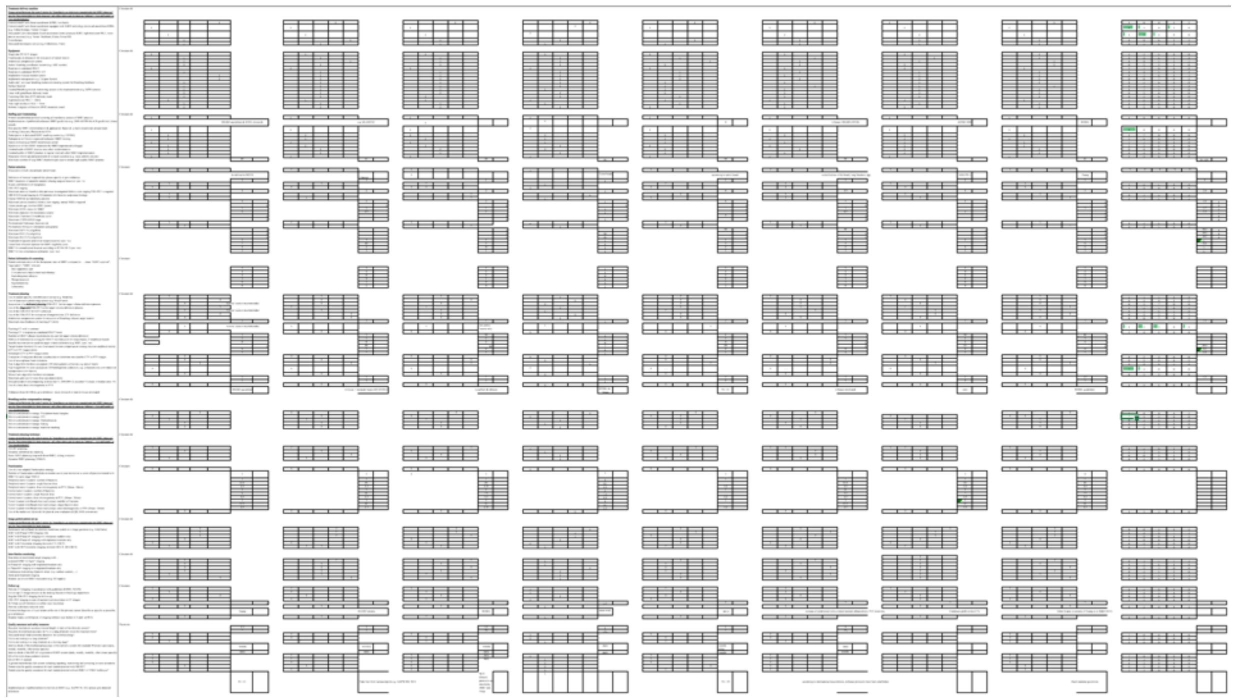
Department of Radiation Oncology
Chairman: Prof. Dr. Matthias Guckenberger

Focus on lung cancer: What a radiotherapy department should offer their patients

UniversityHospital Zurich

ESTRO

ESTRO ACROP guideline development



- Questionnaire of 140 items
- **Consensus** of 11 experts from the ESTRO SBRT teaching course and their **8 institutions**

ESTRO ACROP guideline development

Category	Definition:
Mandatory	**Minimum** equipment and methodology required to achieve clinical **outcome in agreement to published prospective clinical trials**.
Recommended	Equipment and methodology achieving **potentially best clinical outcome and best accuracy** currently achievable.
Optional	Equipment and methodology that **might improve clinical outcome and accuracy of SBRT without clinical evidence** available, yet.
Insufficient	Equipment and methodology resulting in **potentially worse clinical outcome** compared to published prospective clinical trials.
Discouraged	Equipment and methodology resulting in no improvement in accuracy or clinical outcome and in **no other obvious advantage**.

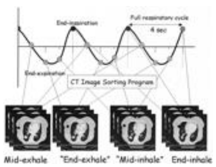
Radiotherapy delivery device

	Device	Mandatory	Recommended	Optional	Insufficient	Discouraged
	**Conventional C-arm linac**	1	0	0	5	2
	**Conventional C-arm linac with IGRT technology**	6	1	0	1	0
	**Dedicated C-arm stereotactic linac**	1	5	1	0	0
	**Tomotherapy**	0	0	6	1	1
	**Dedicated stereotactic device**	0	2	6	0	0

- Mandatory: C-arm linac with CBCT
- Recommended: "Stereotactic" C-arm linac

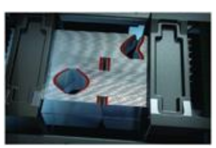
Additional technologies

Mandatory



	Mandatory	Recommended	Optional
Respiration correlated 4D-CT	**5**	3	0

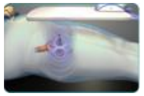
Recommended



	Mandatory	Recommended	Optional
High-resolution MLC < 10mm	2	**6**	0

- Mandatory: 4D-CT
- Recommended: HR-MLC (5-9mm)

Additional technologies



	Mandatory	Recommended	Optional
Fluoroscopy at simulation for evaluation of tumor motion	0	0	**6**
Abdominal compression system	0	0	**5**
Active breathing coordinator system (e.g. ABC system)	0	2	**5**
Respiration correlated 4D-PET-CT	0	0	**8**
Implantable fiducial marker system	0	1	**6**
Implantable transponders e.g. Calypso System	0	0	**7**
Audio and / or visual breathing motion monitoring system for breathing feedback	0	2	**6**
Surface Scanner	0	1	**5**
External breathing motion monitoring system in the treatment room (e.g. RPM system)	0	3	**5**
Linac with gated beam delivery mode	0	2	**6**
Flattening filter free (FFF) delivery mode	0	2	**6**
Very high resolution MLC < 5mm	0	2	**6**
Robotic 6 degrees of freedom (DOF) treatment couch	1	2	**5**

- Most additional technologies optional

Staffing and Credentialing

	Mandatory
Written departmental protocol covering all mandatory aspects of SBRT practice	8
Site-specific SBRT implementation & application based on **a multi-disciplinary project team** involving Clinicians, Physicists & RTTs	8
Structured follow-up and assessment of clinical outcomes (e.g. local control, toxicity)	8

- Mandatory: Protocols, multi-professional team & structured follow-up

Staffing and Credentialing

	Mandatory	Recommended	Optional
Participation in dedicated SBRT teaching course (e.g. **ESTRO SBRT course**)	1	7	0
Particpation in **Vendor**-organized dedicated SBRT training	2	6	0
Supervision of first SBRT treatments by SBRT-experienced colleague	2	5	1
Hands-on training at SBRT-experienced center	3	5	0
External audit of SBRT practice **once** after implementation	0	4	4
External audits of SBRT practice in **regular** intervalls after SBRT implementation	0	4	4

- Recommended: investment in training and teaching instead of technology

Treatment planning: Planning technique

	Mandatory	Recommended	Optional
3D CRT planning	**6**	2	0
Dynamic conformal arc planning	2	1	4
Static IMRT planning	0	0	5
Dynamic IMRT planning	0	**5**	3

- Mandatory: 3D-CRT
- Recommended: VMAT

Breathing motion compensation

	Mandatory	Recommended	Optional	Insufficient
Population-based margins	1	0	0	**4**
ITV	**7**	1	2	0
Midventilation	0	**4**	4	0
Gating	0	2	**6**	0
Real-time tracking	0	1	**7**	0

- Mandatory: ITV
- Recommended: Mid-ventilation

Image guidance

	Mandatory	Recommended	Optional	Insufficient / discouraged
Stereotactic set-up based on external coordinate system	0	0	2	6
IGRT with Planar EPID imaging only	0	0	0	8
IGRT with Planar kV imaging w/o implanted markers only	1	0	0	7
IGRT with Planar kV imaging with implanted markers only	1	0	**6**	0
IGRT with Volumetric imaging	**6**	1	1	0
IGRT with 4D Volumetric imaging	0	**7**	2	0

- Mandatory: in-room 3D IGRT
- Recommended: in-room 4D IGRT

Thank you for your attention!

‘steps’of registration @AMC

Reference settings – 1x

1. Visualize your patient in full
2. Ask yourself what you are going to treat
3. Ask yourself what is the best surrogate for your target volume (within the department protocol)
4. Define structures to be displayed, clipbox, corr ref point and algorithm
5. Are there patientspecific variables?

Image registration and evaluation

1. Visualize your patient in full in green/purple overview
2. Automatisch registration (match)
3. Evaluation of your registration (match)
4. Evaluation of CTV coverage – target within PTV?
5. Are the rotations within tolerance
6. Are there any changes in patient anatomy that might influence the dose distribution
7. Evaluation the correction without rotations – target within PTV?

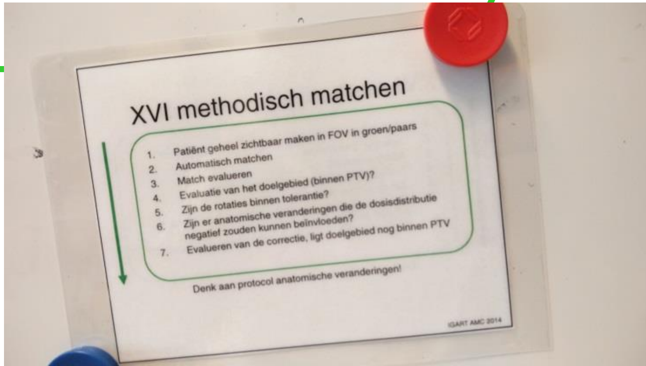


Image registration and evaluation

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Image registration and evaluation

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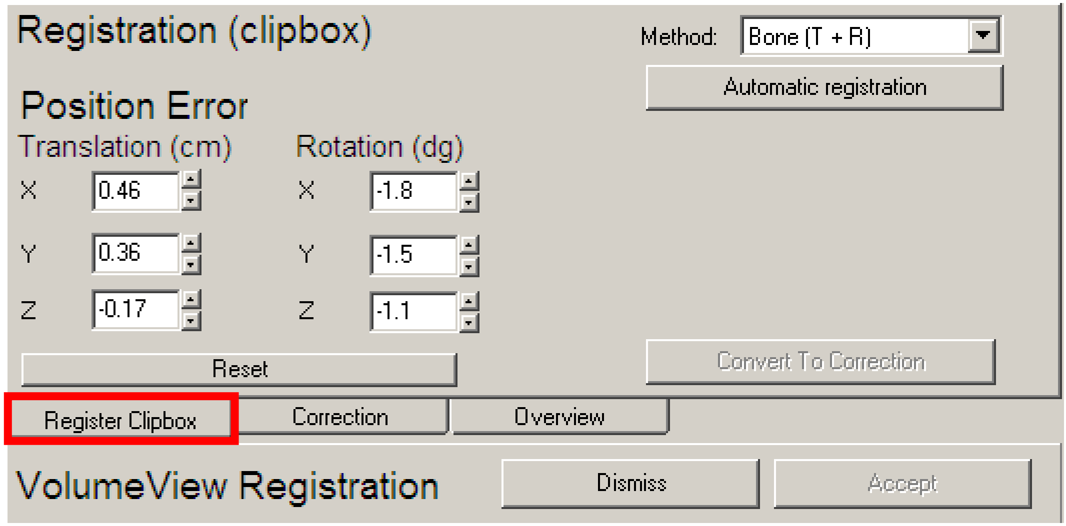
5. Are the rotations within tolerance
6. Are there any changes in patient ana
   the dose distribution
7. Evaluation the correction without rota

Fr.	Datum	PTV?		Rotatie		(cm)	(cm)
		JA	NEE	<4°	≥4°		
1		☐	☐	☐	☐		
2		☐	☐	☐	☐		
3		☐	☐	☐	☐		
4		☐	☐	☐	☐		
5		☐	☐	☐	☐		

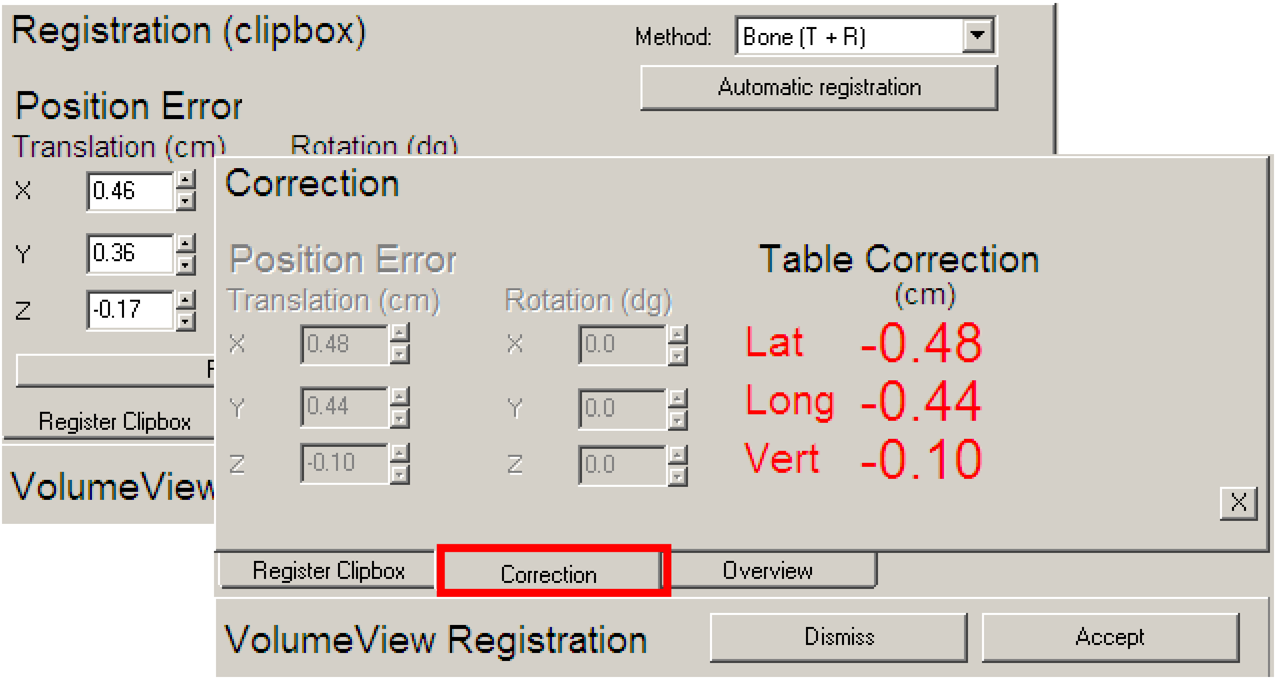
Symantics @Elekta



Tab Register Clipbox:

Full registration in translations and rotations.

On this tab you check the registration and evaluate patient anatomy

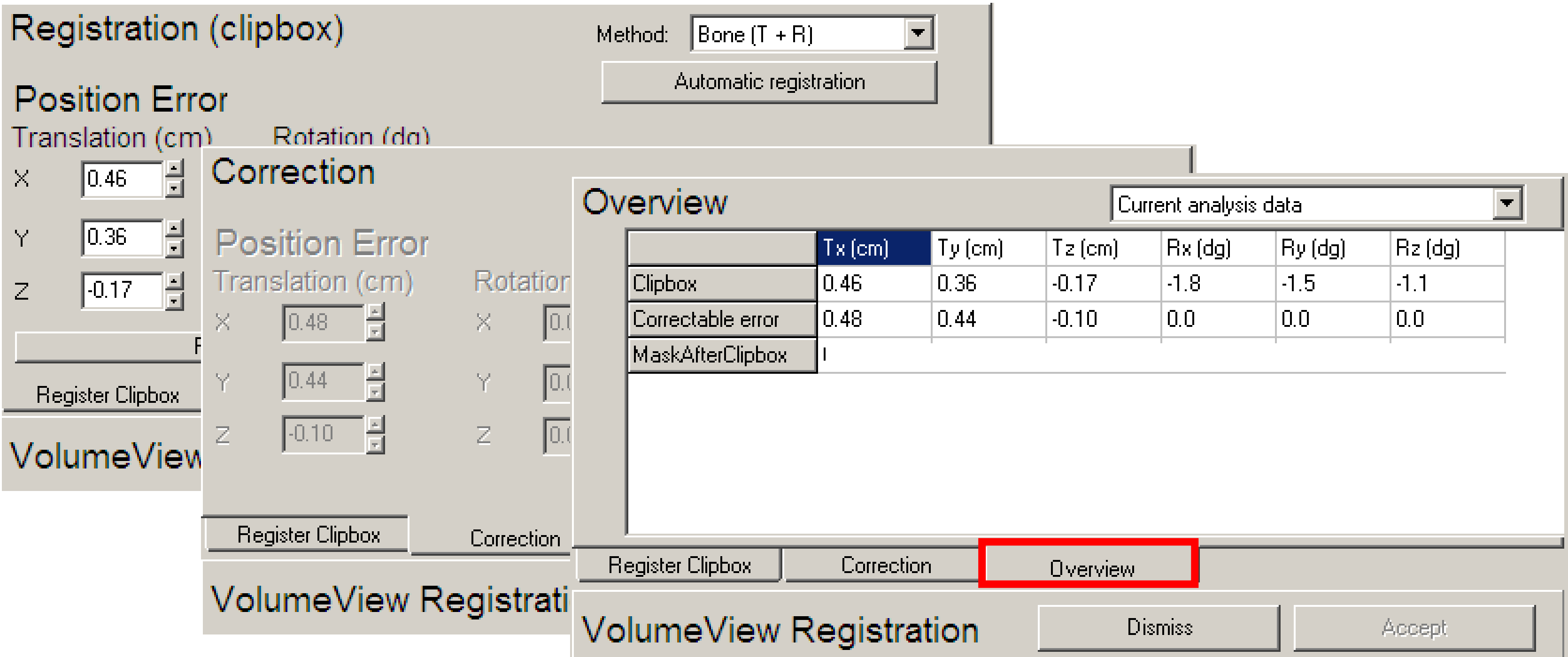


Tab Correction:

Displays the correctable error. It is the registration where the rotations have been recalulated. The registration ourcome is grey because you cannot change the registration in this tab.

In red it displays the table shift to get to the correctable error. In the viewer the position you are going to treat the patient.

Notice the opposite direction of the numbers between correctable error and table shift in x and y.



Tab Overview:

Display an overview:

Full match in translations en rotations: Clipbox

Correctable error: Correctable error

This tab does not display the table shift!!

You can only find that in the tab Correction.

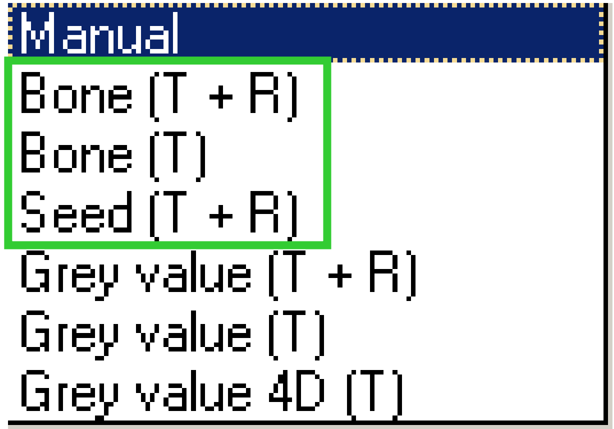
Algorithms @Elekta

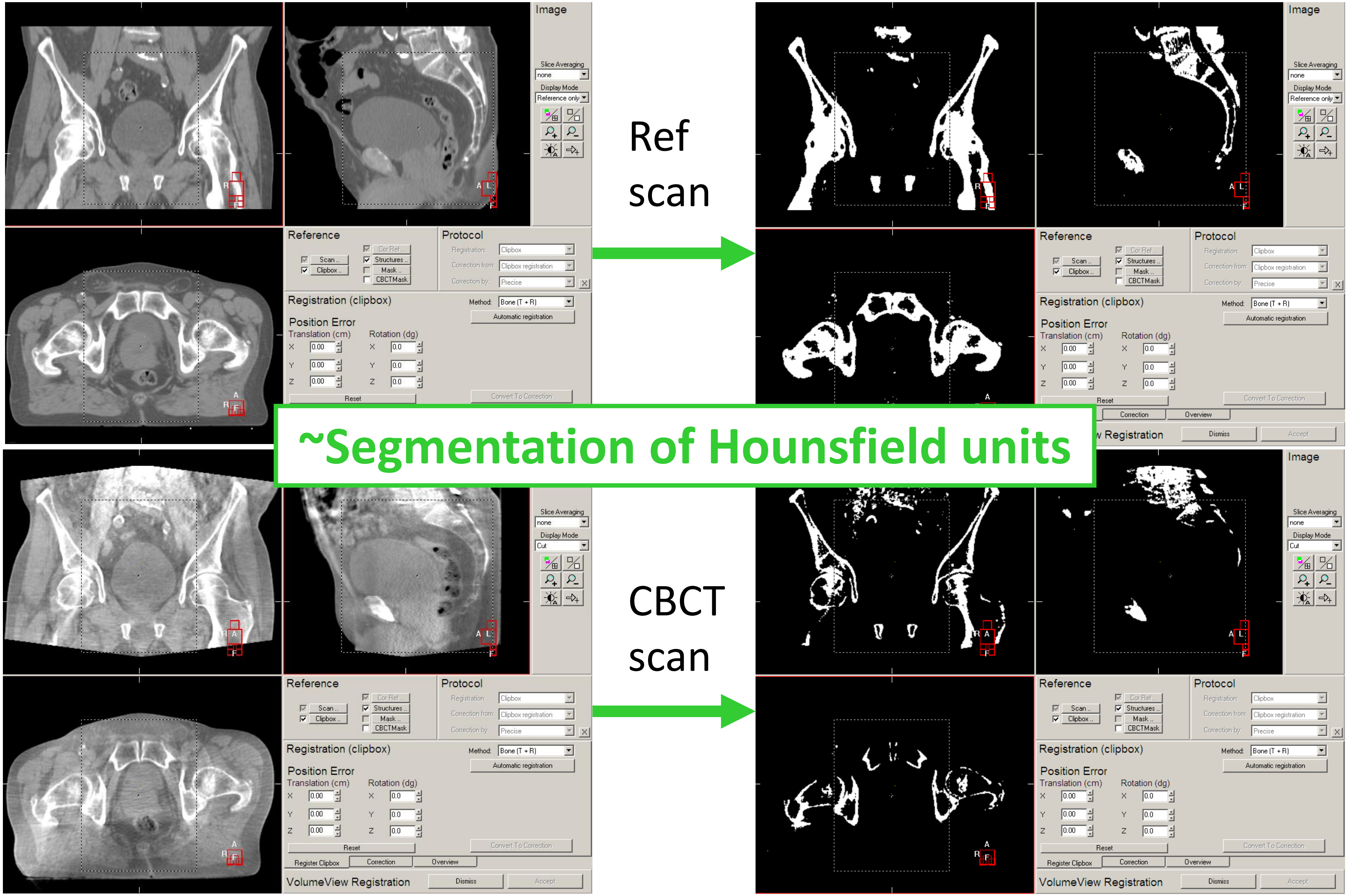
Algorithms

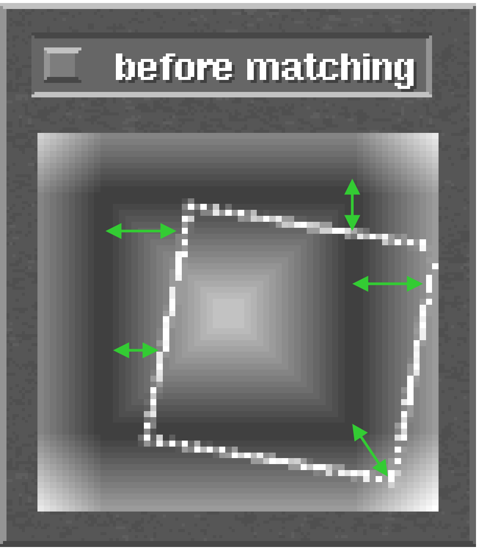
<u>Bone & Seed</u>: <u>chamfer match</u>

T+R = Translations and rotations

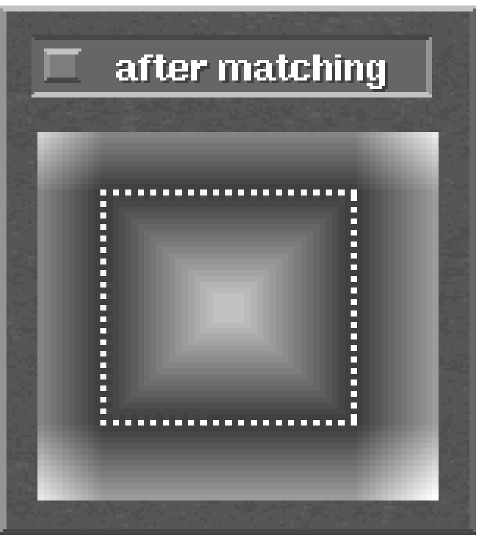
T = Translations only




Ref
scan
~Segmentation of Hounsfield units
CBCT
scan
Image
Slice Averaging
Display Mode
Reference
Protocol
Registration (clipbox)
Position Error
Translation (cm)
Rotation (dg)
Automatic registration
Reset
Convert To Correction
Register Clipbox
Correction
Overview
VolumeView Registration
Dismiss
Accept

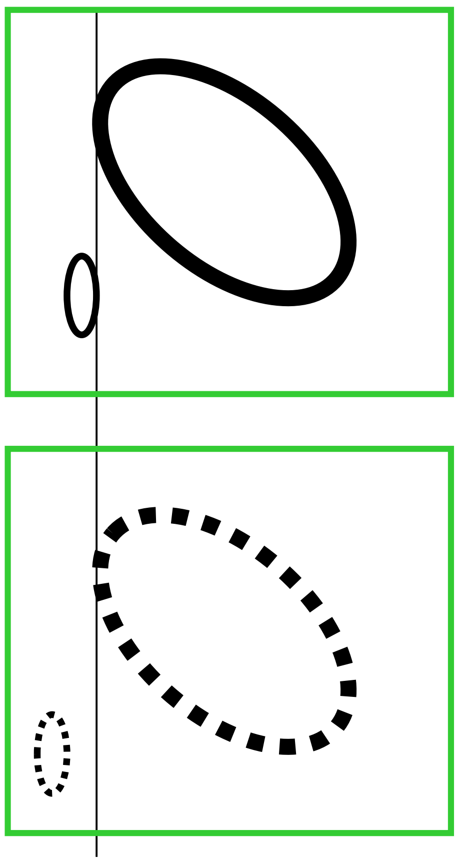


Bone and seed match:
Registration quality is measured by the average distance between the two segmented objects.



Is quick and reliable. The algorithm indicated whether the outcome was perfect or not *'match may be inaccurate'*

Bone and seed algoritme

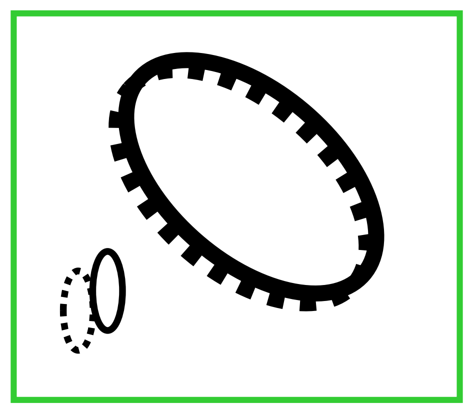


Ref CT

CBCT

Pitfall:

If the object is not rigid and not equally balanced in size, the biggest part has more importance.

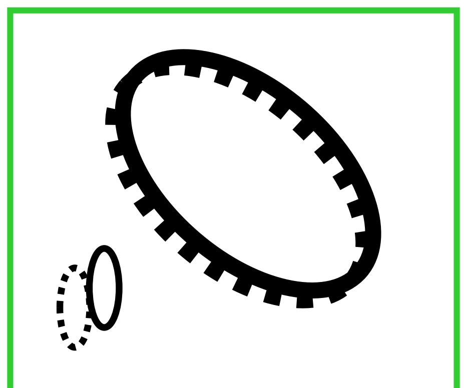


Chamfer match

Bone and seed algoritme

Pitfall:

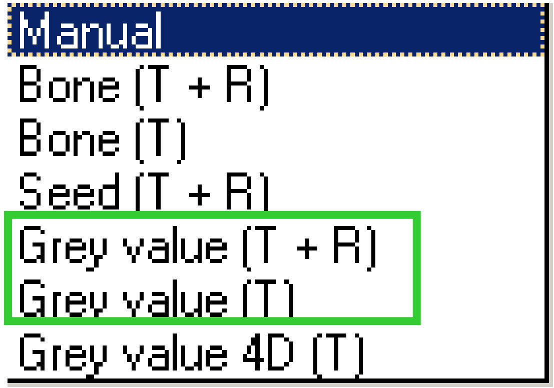
If the object is not rigid and not equally balanced in size, the biggest part has more importance.



Chamfer match

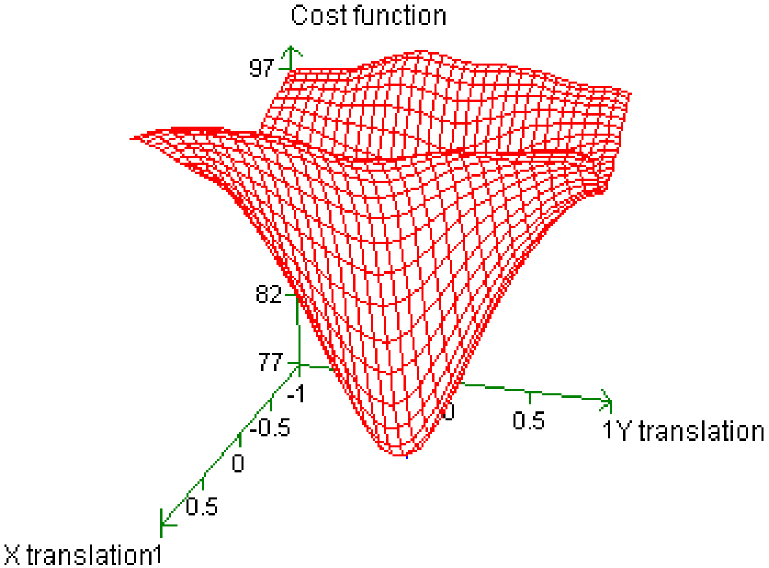
Always visually check whether you got your desired answer

Algoritmes



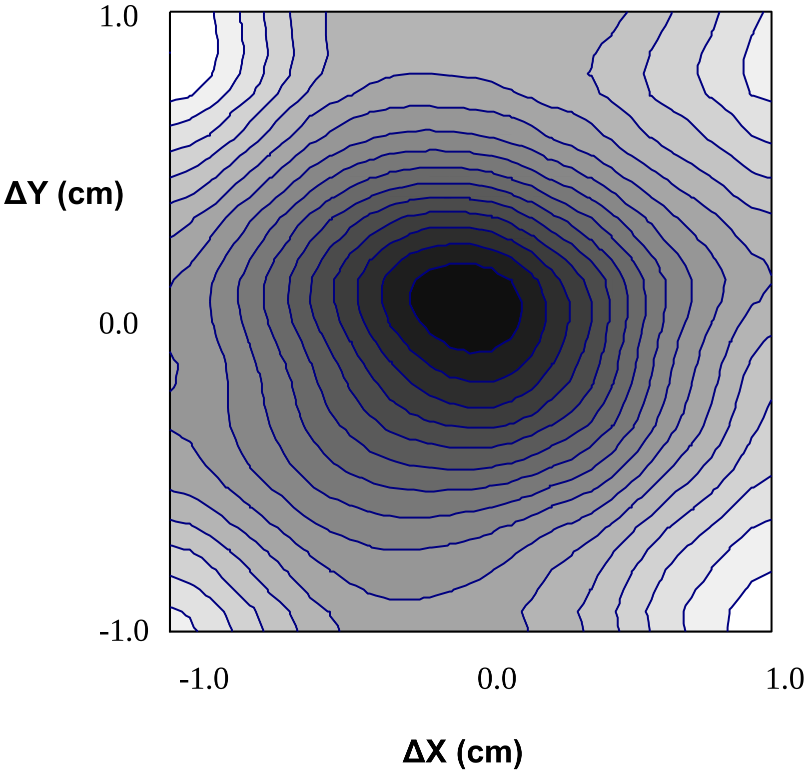
Grey value:

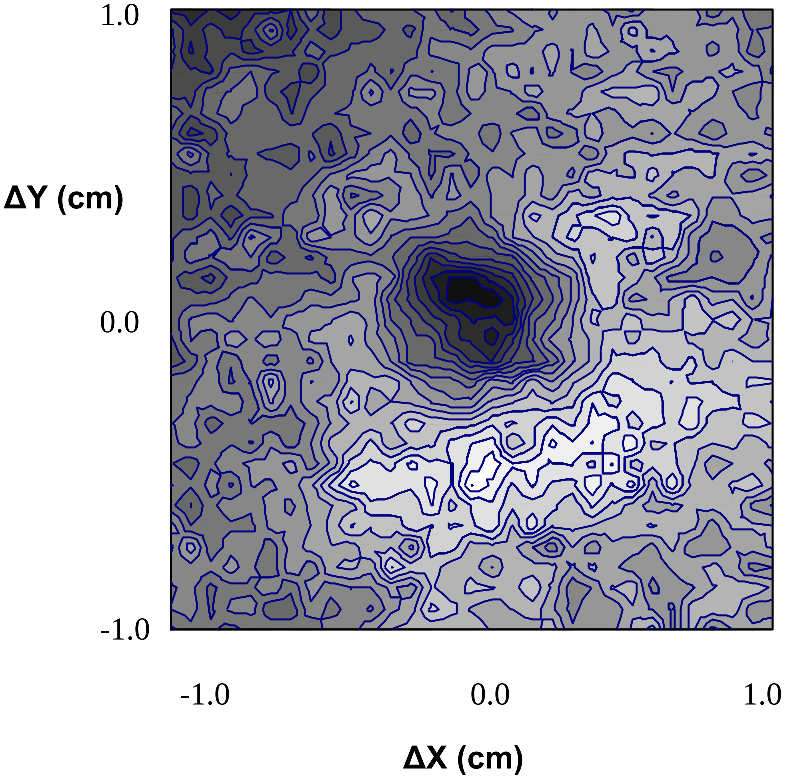
Takes all the pixel values into account:



Cons:

Local minima: specifically a problem for small regions of interest depending on cost function





Pitfalls:

If the object is not rigid and not equally balanced in size, the biggest part has more importance.

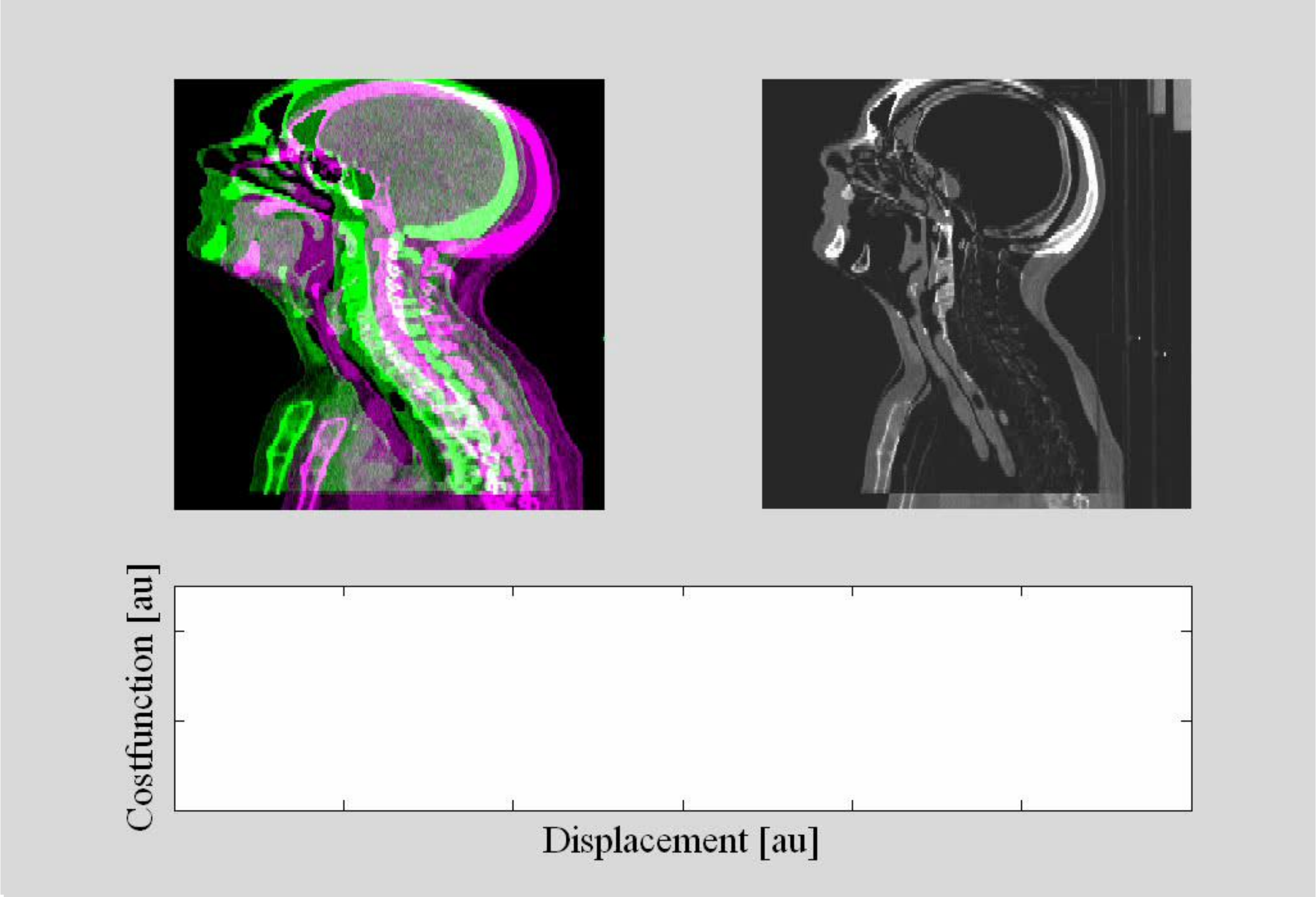
High densities have more influence

Big densities drops have big influence

Artefacts!!

Always visually check the outcome!

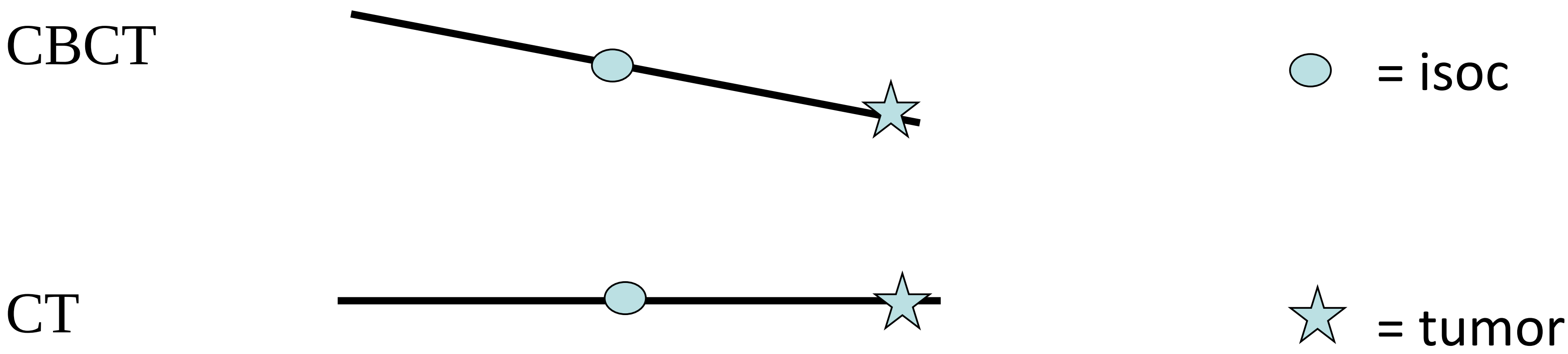
Uses all pixel values in ROI: e.g., sum of squared differences



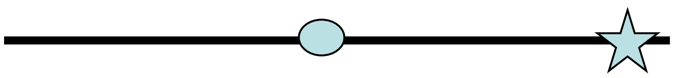
Somewhat slower to process all voxels: depends on the size of the ROI

CRP @Elekta

Correction Reference Point

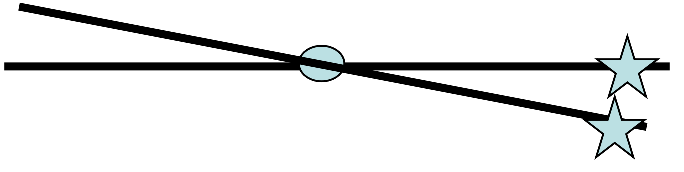


Correction Reference Point



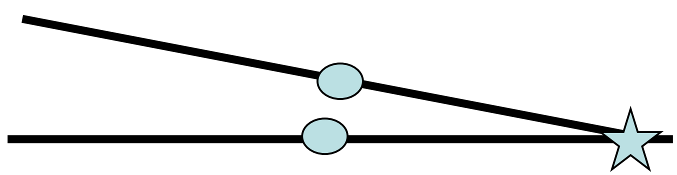
CBCT registered (matched) to reference CT:
Perfect! With 6 degrees of freedom (dof):
3 translations and 3 rotations

Correction Reference Point



After ‘convert to correction’ with correction reference point at isocentre: isoc is perfecty registerd, tumor is not.

Correction Reference Point

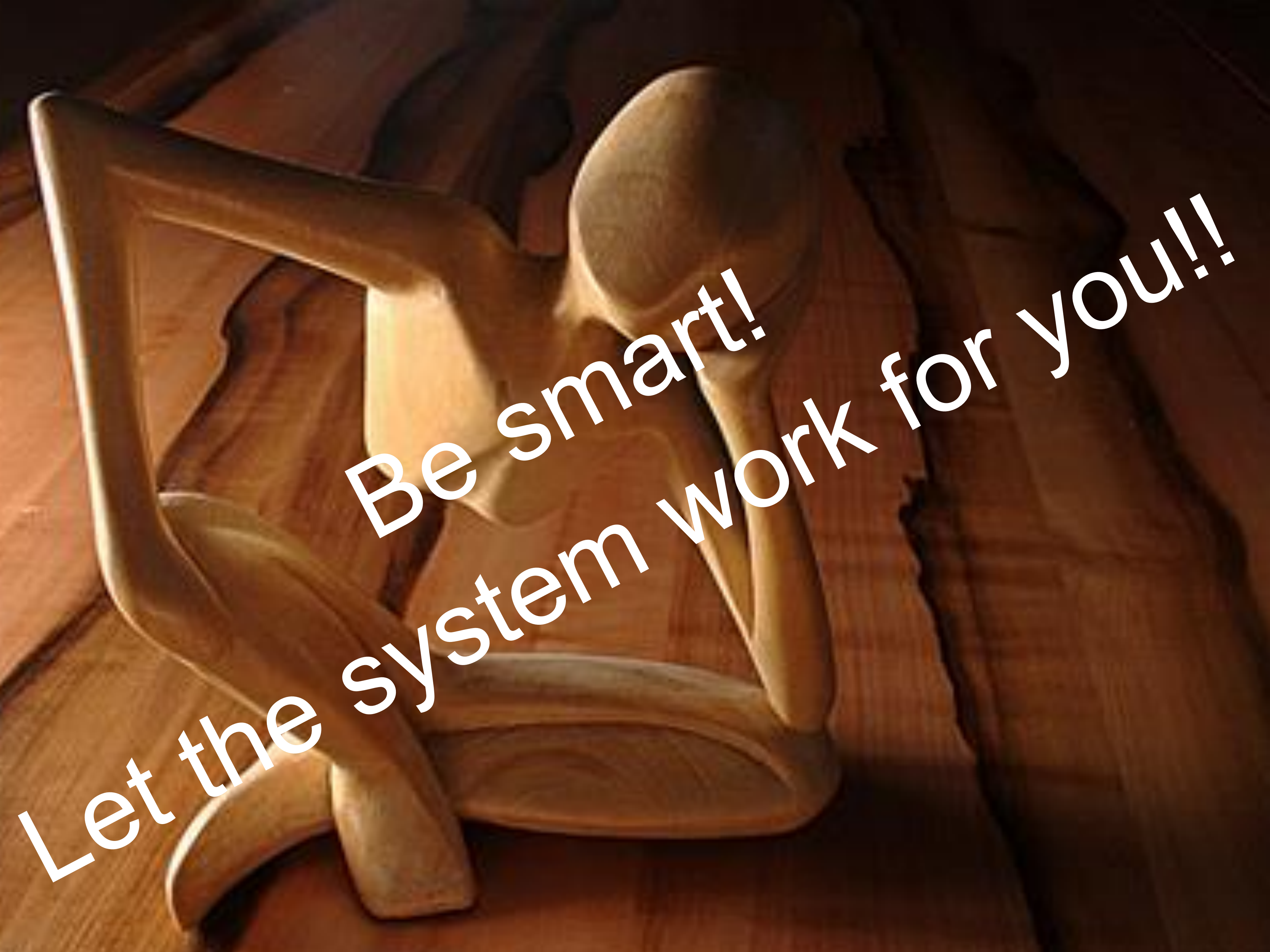


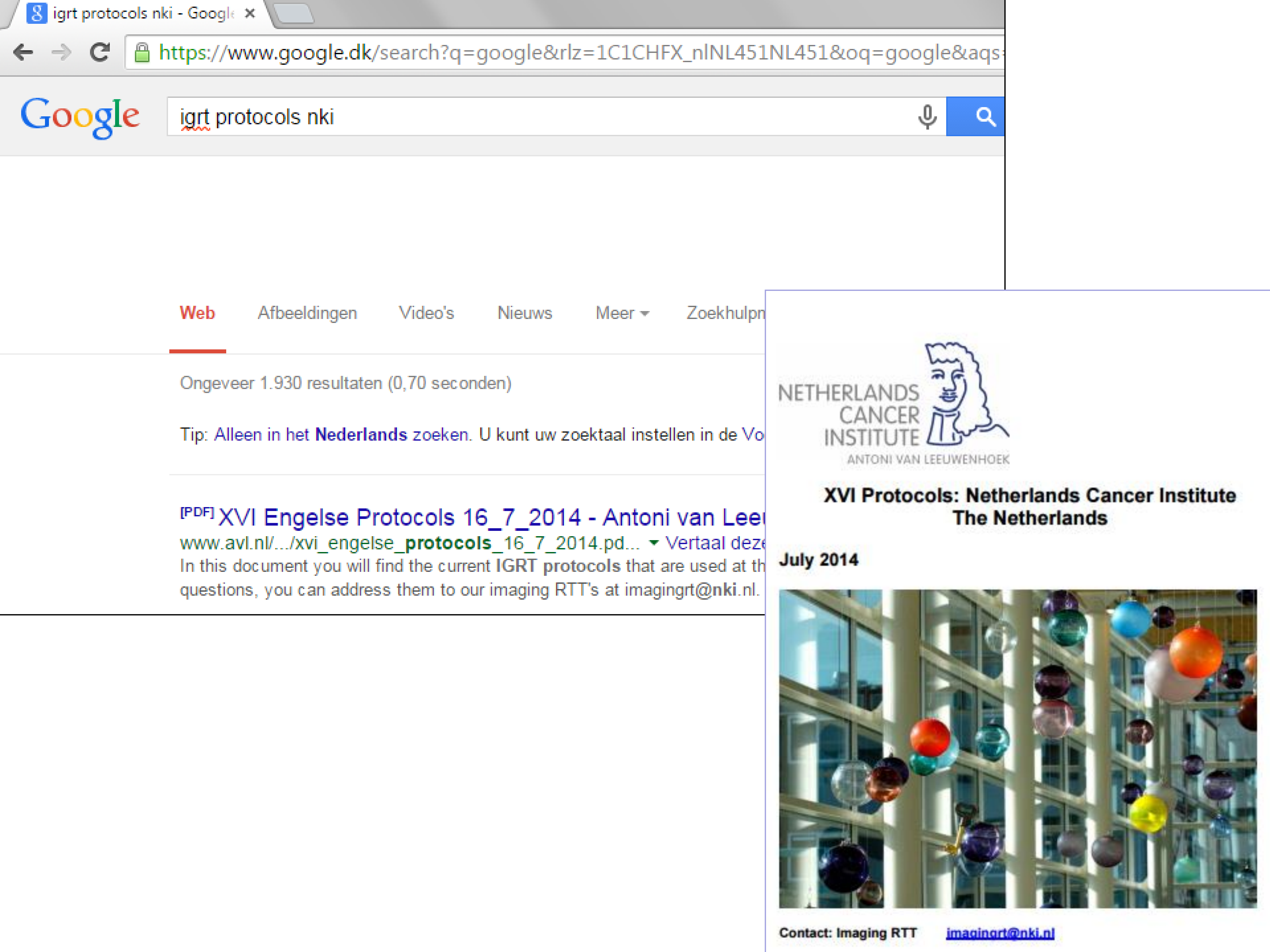
After ‘convert to correction’ with correction reference point in the tumor: tumor is perfectly registered, isoc is not.

Correction Reference Point

For lazy people only

You can already think IGRT at Treatment Planning!
Choose your isocentre at your rotation point of preference
(= centre of gravity of target volume (PTV))


Be smart!
Let the system work for you!!



igrt protocols nki - Googl
https://www.google.dk/search?q=google&rlz=1C1CHFX_nlNL451NL451&oq=google&aqs
Google
igrt protocols nki
Web
Afbeeldingen
Video's
Nieuws
Meer
Zoekhulpn
Ongeveer 1.930 resultaten (0,70 seconden)
Tip: Alleen in het Nederlands zoeken. U kunt uw zoektaal instellen in de Vo
[PDF] XVI Engelse Protocols 16_7_2014 - Antoni van Leeu
www.avl.nl/.../xvi_engelse_protocols_16_7_2014.pd... Vertaal deze
In this document you will find the current IGRT protocols that are used at th
questions, you can address them to our imaging RTT's at imagingrt@nki.nl.
NETHERLANDS CANCER INSTITUTE
ANTONI VAN LEEUWENHOEK
XVI Protocols: Netherlands Cancer Institute
The Netherlands
July 2014
Contact: Imaging RTT imagingrt@nki.nl

Break-up sessions

Image Registration and Evaluation

Demo Database
XVI - Elekta

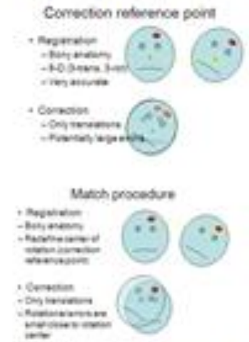
ESTRO course
Advanced Skills for Treatment Delivery
Amsterdam 2014

Images
Peter Remeijer NKI / AvL
Rianne de Jong AMC

MATCH PARAMETERS		SCAN PARAMETERS	
Structures	[illegible]	Preset collimator	[illegible]
Correction reference point	[illegible]	Gantry rotation	The arc of the CBCT scan
Registration	[illegible]	Gantry speed	[illegible]
Method	[illegible]	Detector position	[illegible]
Resolution rotations	[illegible]	Filter	[illegible]
		Collimator	[illegible]

MATCH PARAMETERS

[illegible]



[illegible]

Paul Pelvis

Cleo Cervix

Emma Endometrium

Inguinal Glands

ESTRO
School

WWW.ESTRO.ORG/SCHOOL

Image Registration and Evaluation: Part 2 CBCT (Varian)

Liz Forde, RTT
Assistant Professor
The Discipline of Radiation Therapy
School of Medicine
Trinity College Dublin

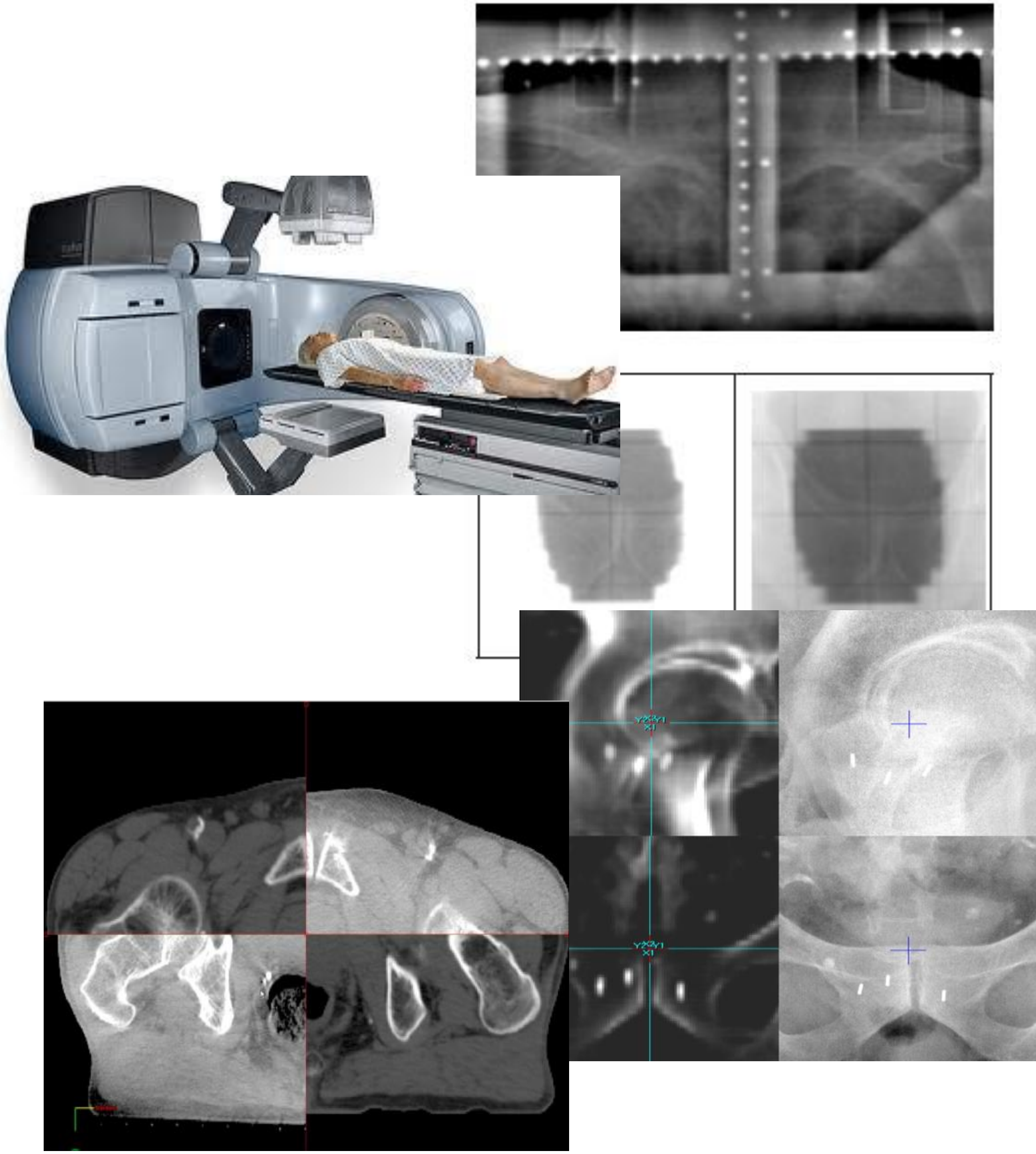
Learning Outcomes

- Identify the key features of the Varian OBI system
  - 2D and 3D image acquisition, registration and verification
- Outline the CBCT acquisition, registration and evaluation process
- Discuss what influences CBCT image quality
- Identify appropriate match structures for the main tumour sites
  - kV 2D/2D and CBCT
- Discuss possible clinical scenarios that require troubleshooting

Key Features of Varian OBI

- 2D
  - ➢ MV and kV
- 2D/2D
  - ➢ MV and kV
- 3D
  - ➢ kV
- Fluoroscopy (2D + time)

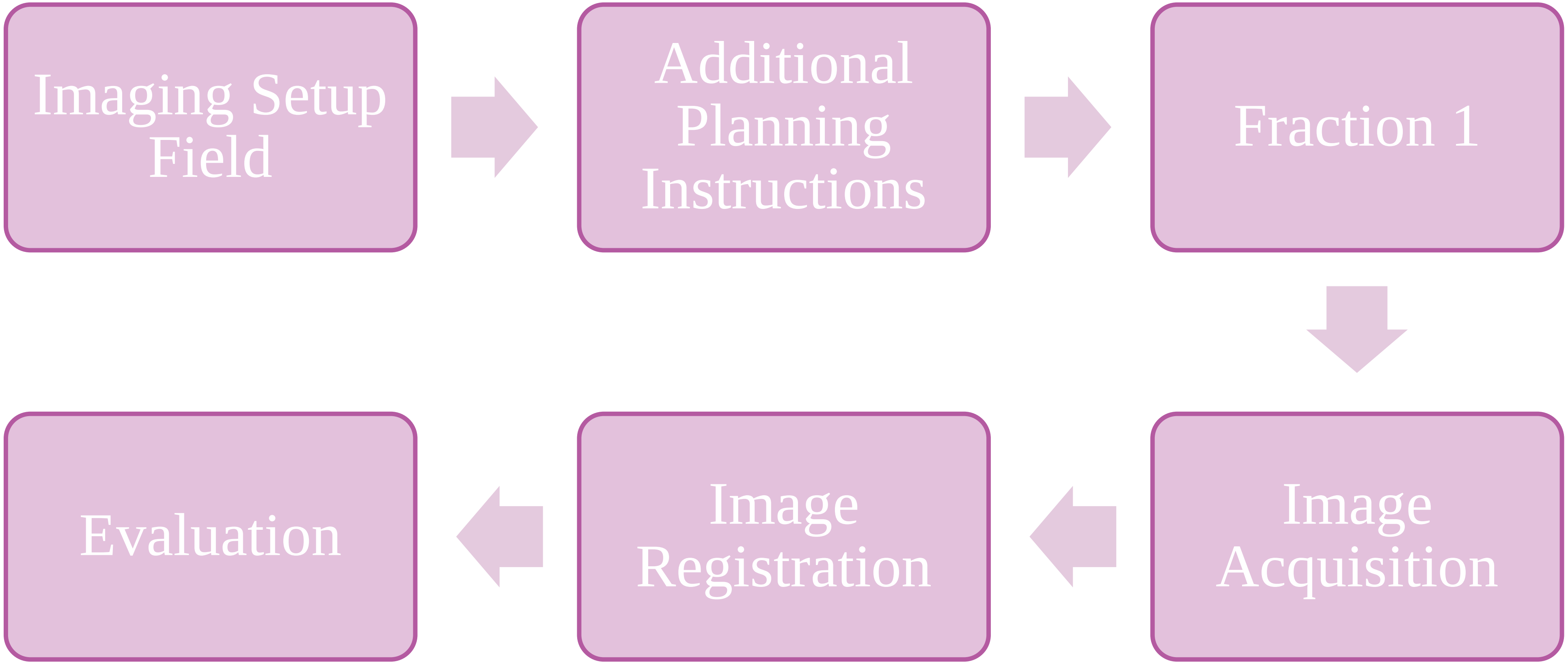
- Remote couch shift

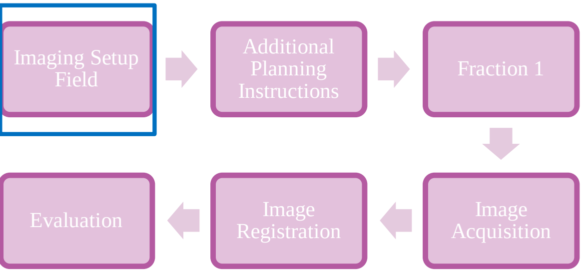


Key Features of Varian OBI

	Standard-Dose Head	Low-Dose Head	High-Quality Head	Pelvis	Pelvis Spotlight	Low-dose Thorax
X-Ray Voltage [kVp]	100	100	100	125	125	110
X-Ray Current [mA]	20	10	80	80	80	20
X-Ray Millisecond [ms]	20	20	25	13	25	20
Gantry Rotation Range [degrees]	200	200	200	360	200	360
Number of Projections	360	360	360	655	360	655
Exposure (mAs)	145	72	720	680	720	262
CTDIw (mGy / 100 mAs)	2.7	2.7	2.7	2.6	2.0	1.8
Dose (cGy)	0.39	0.2	1.94	1.77	1.44	0.47
Fan Type	Full Fan	Full Fan	Full Fan	Half Fan	Full Fan	Half Fan
Bow Tie Filter	**FULL**	**FULL**	**FULL**	**HALF**	**HALF**	**HALF**
Default Pixel Matrix	384 x 384	384 x 384	384 x 384	384 x 384	384 x 384	384 x 384
Slice Thickness [mm]	2.5	2.5	2.5	2.5	2.5	2.5
Reconstruction Filter	Sharp	Standard	Sharp	Standard	Smooth	Standard

The IGRT Process

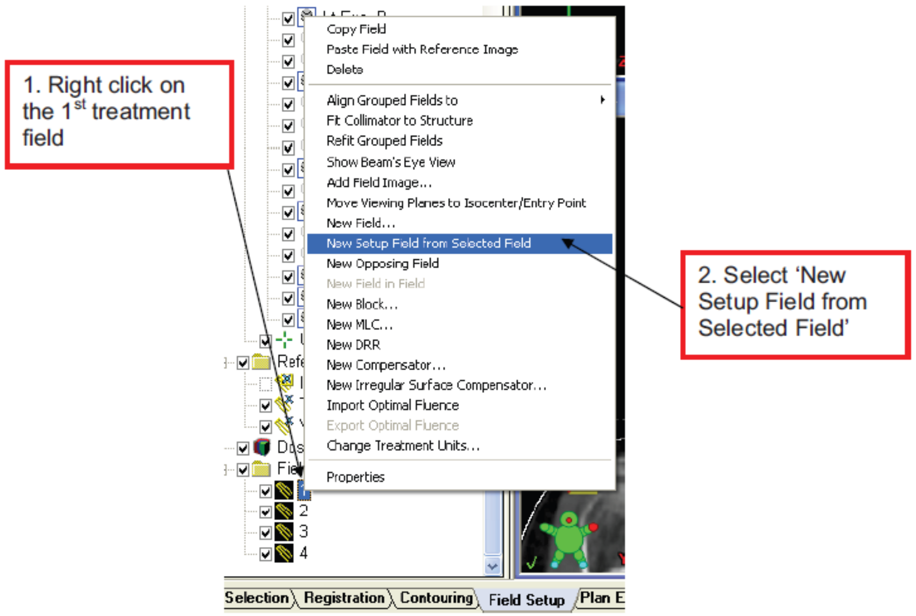


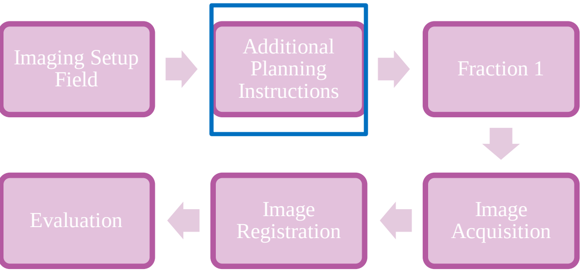


IGRT Setup in Planning

- Create setup fields in planning

- Consider the position of the isocentre
  - Varian does not have a “Correction reference point”
  - IMRT and VMAT are forgiving with isocentre placement
  - CBCT may need to shift laterally for clearance
  - You will be prompted on the linac

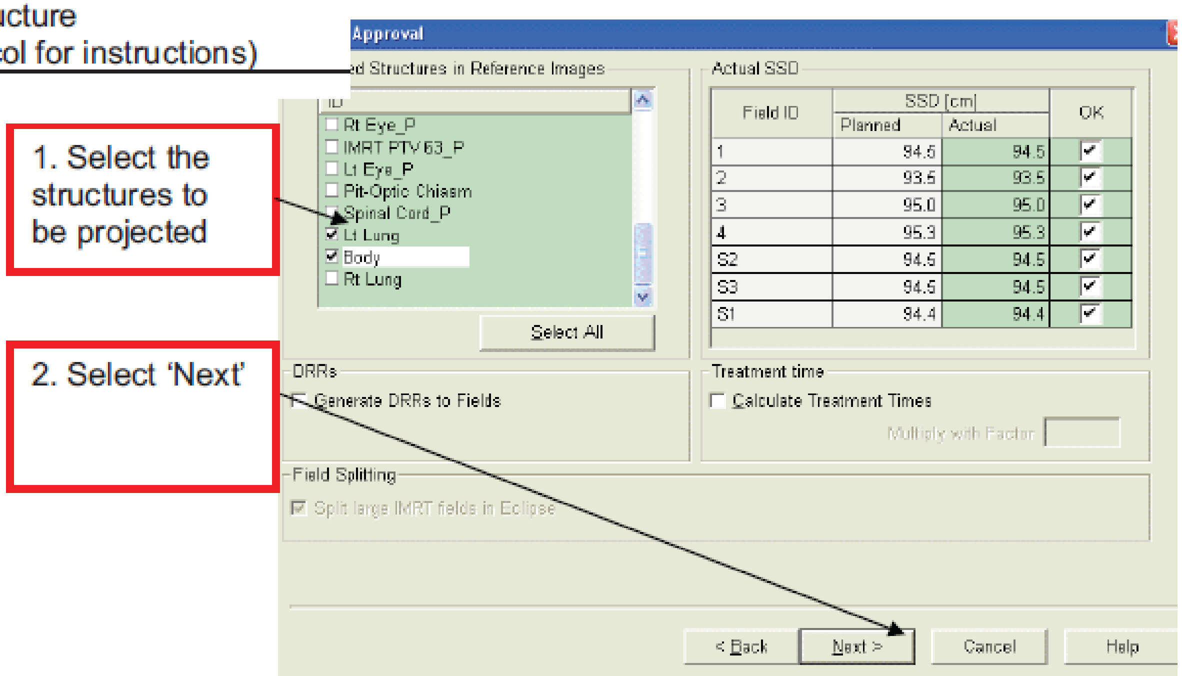




IGRT Setup in Planning

- Additional contours to be outlined and/or "sent across" for image verification

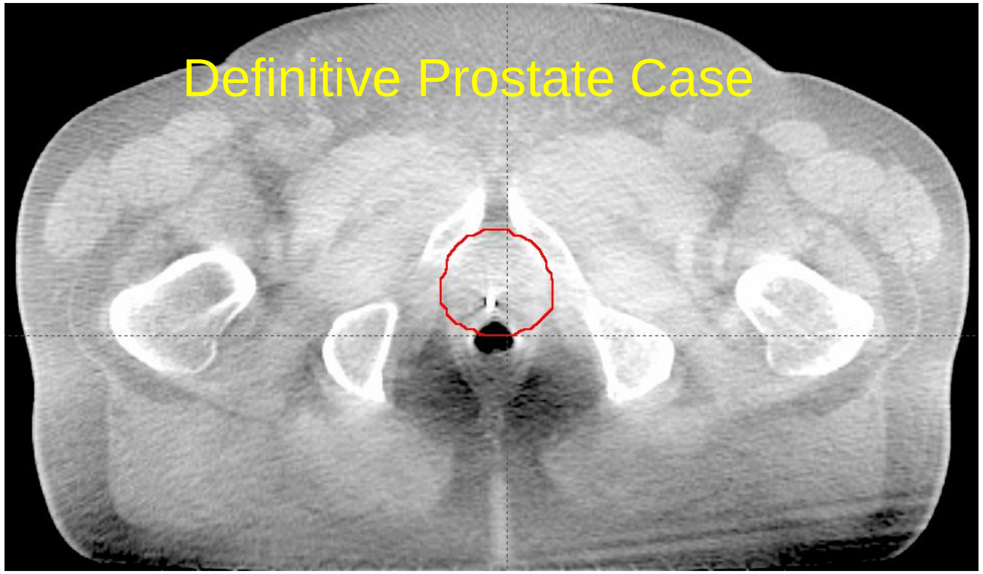
Treatment Area	Imaging Type	Extra Contouring
All treatment areas	CBCT, kV or MV	PTV
All treatment areas	CBCT	FSD tolerance rings (see site specific planning protocols for instructions and size of the rings)
Chest	kV or MV or CBCT	Carina
Abdomen	kV or MV or CBCT	Carina
Breast/Chest Wall	MV	Lung (treatment side) and Body
Prostate	CBCT	Convert dose to structure (see prostate protocol for instructions)
Post-Prostatectomy	CBCT	Convert dose to structure (see prostate protocol for instructions)



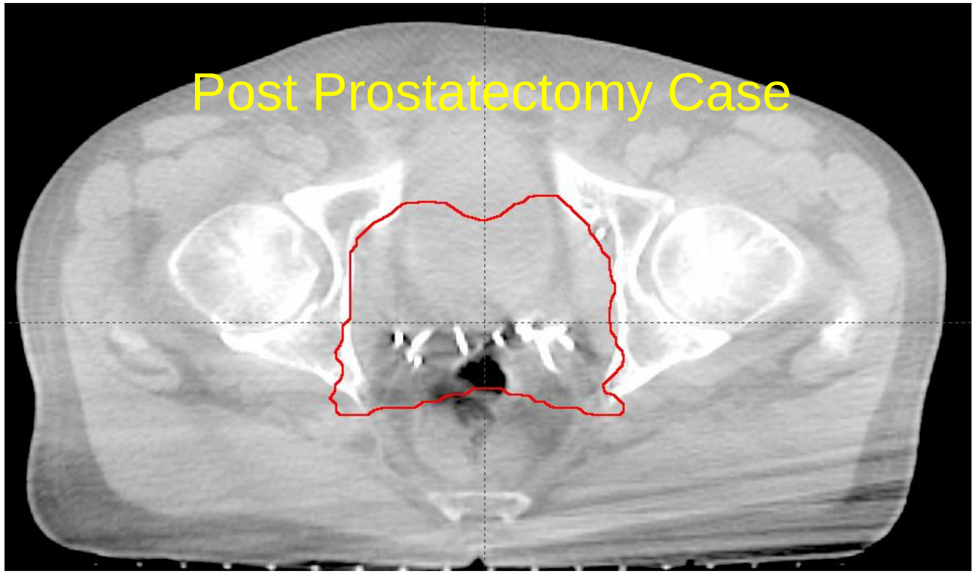
IGRT Setup in Planning

- Additional contours to be outlined and/or "sent across" for image verification
  - ➢ In Field Setup (Eclipse TPS) "Convert isodose line to structure"

80Gy isodose line

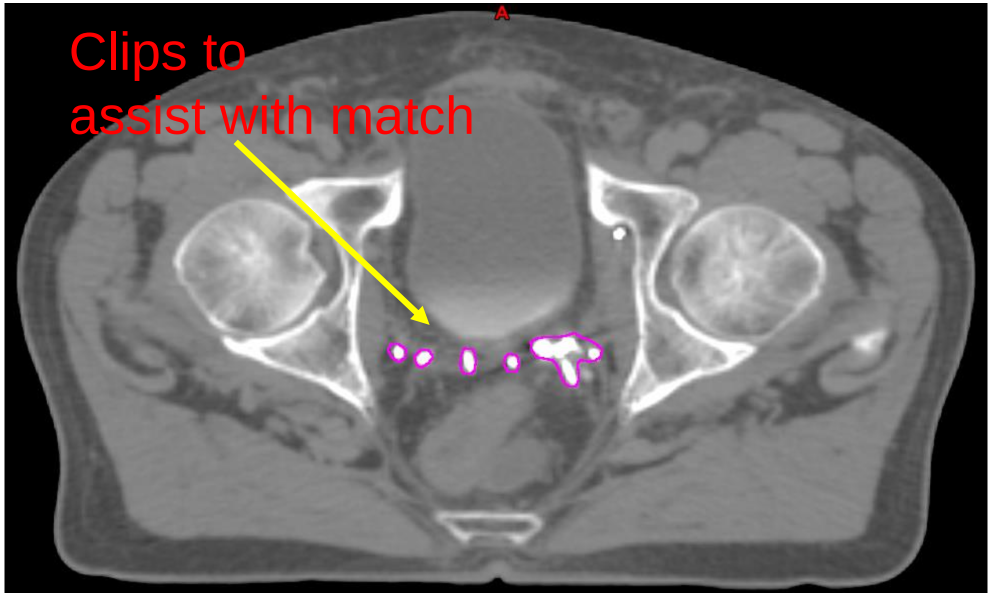


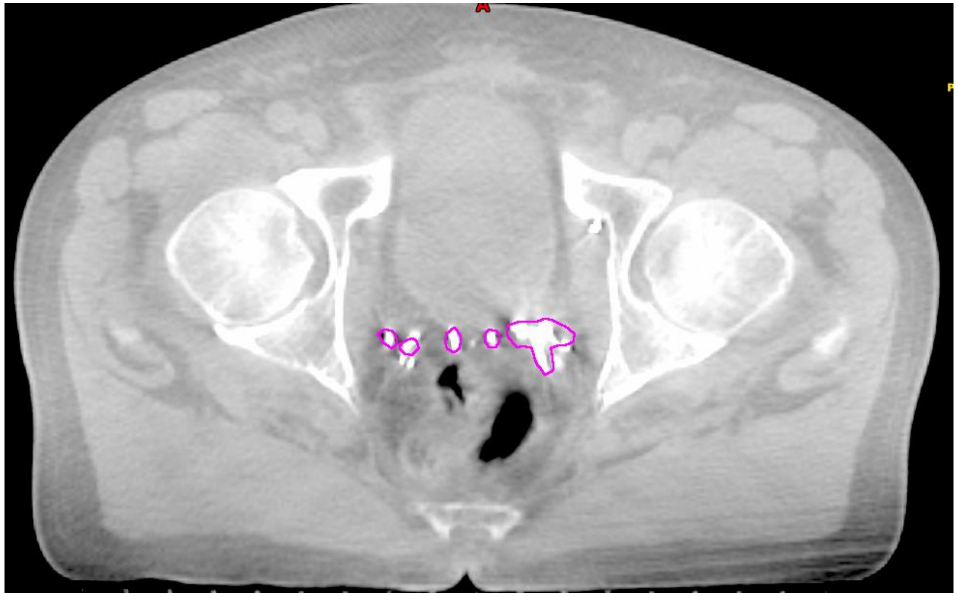
68Gy isodose line



IGRT Setup in Planning

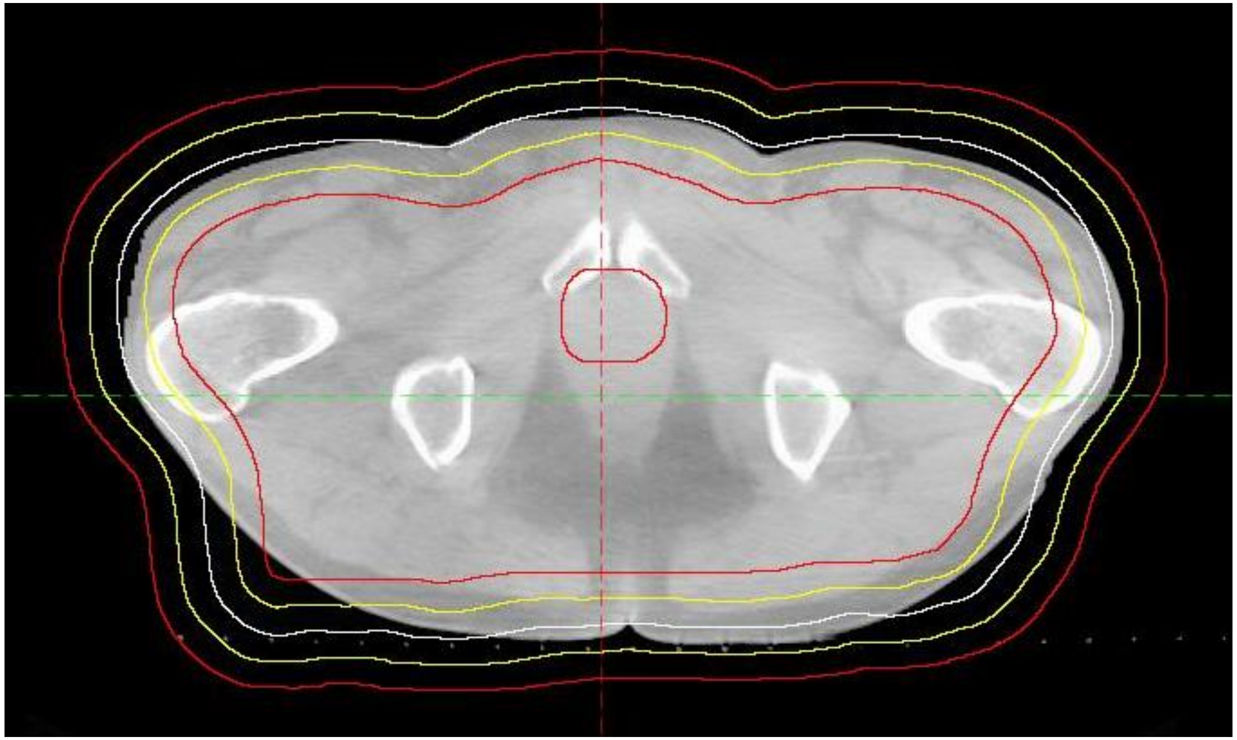
- Additional contours to be outlined and/or "sent across" for image verification
  - ➢ In Contouring Workspace in Eclipse TPS

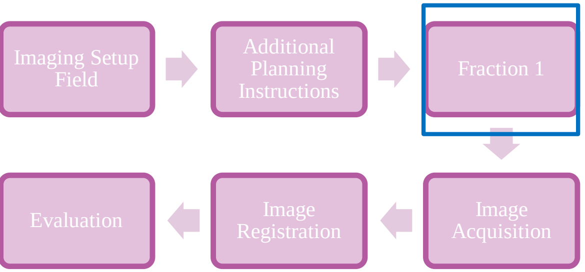




IGRT Setup in Planning

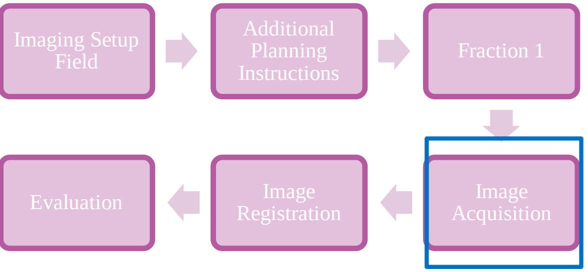
- Additional contours to be outlined and/or “sent across” for image verification
  - In Contouring Workspace in Eclipse TPS “Wall Extraction” tool from Body contour





Fraction 1 Considerations

- Clearance
- Education
  - ➢ Who should be present for first day scan?
  - ➢ RO, MP, RTT responsible for plan, Senior RTT
- Documentation!
  - ➢ Anything weird and wonderful
  - ➢ Structures to include/avoid
- Set VOI box and decide on additional registration variables
  - ➢ This will ensure consistency throughout the course



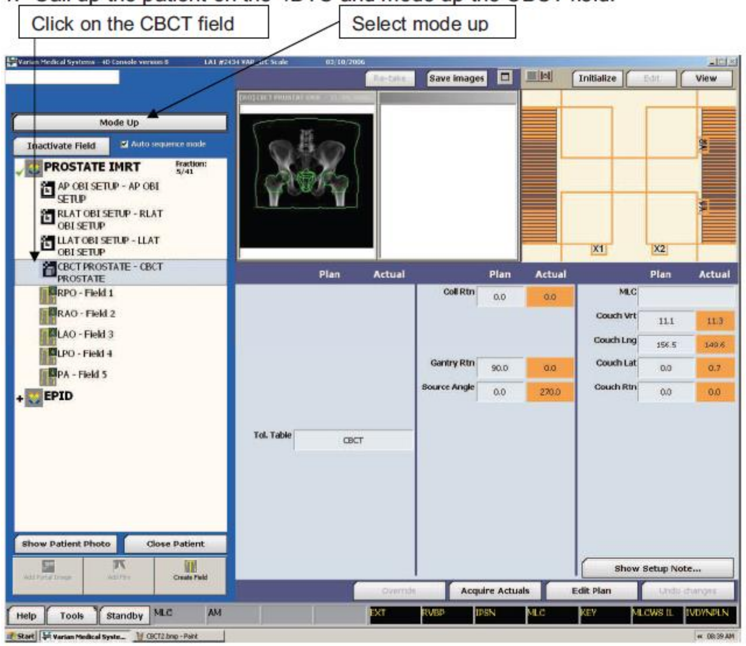
The Image Acquisition Process - CBCT

1. Select correct bow tie filter for treatment site
2. On fraction 1 consider checking rotation/clearance whilst in room
3. Mode up CBCT setup imaging field
    1. Note this is incorporated in the individual patient's plan

Scan Name	Gantry Rotation Required	Bow-tie Filter Required	Treatment sites to be used on	Field of View
Standard-dose head	200	Full	-	24cm
Low-dose head	200	Full	-	24cm
High-quality head	200	Full	Head & Neck Brain	24cm
Pelvis	360	Half	Pelvis (includes: Prostate Rectum Bladder Gynecological)	45cm
Pelvis spotlight	200	Full	-	24cm
Low-dose thorax	360	Half	Chest Abdomen	45cm

NB: See pictures below to distinguish between the bow-tie filters

1. Call up the patient on the 4DTC and mode up the CBCT field.



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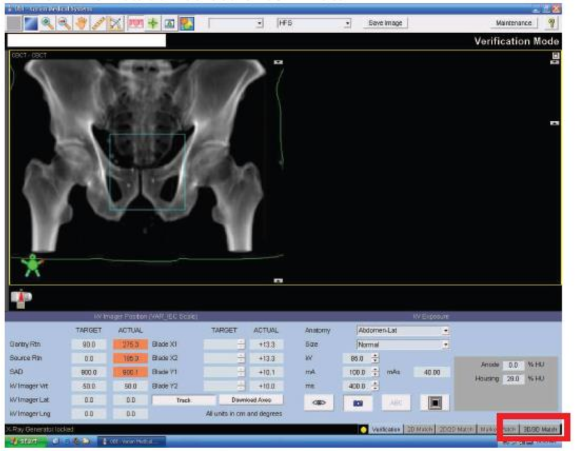
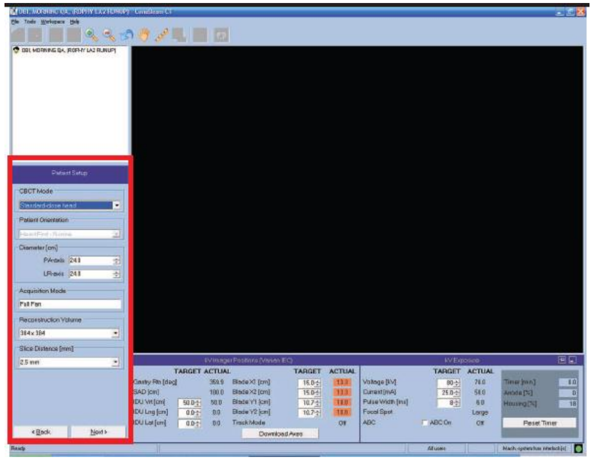
The Image Acquisition Process - CBCT

4. Select 3D/3D match



5. Acquire new scan

6. Complete details
    1. Slice thickness
    2. Orientation
    3. Full fan or half fan



7. Start scan

8. Accept and export

CBCT Image Quality

- What impacts on image quality?
  - CBCTs use a large flat panel detector – increases scatter
  - Permanent anti scatter filter built into detector panel

Scatter decreases image contrast, increases noise, possible registration errors and also patient dose

↓

CT Numbers (HU) affected

CBCT Image Quality

- **Machine characteristics**
  - MV or kV
  - Acquisition time
  - Scan length
  - Filters used
    - Bow Tie filter added to source panel

Bow Tie Filters

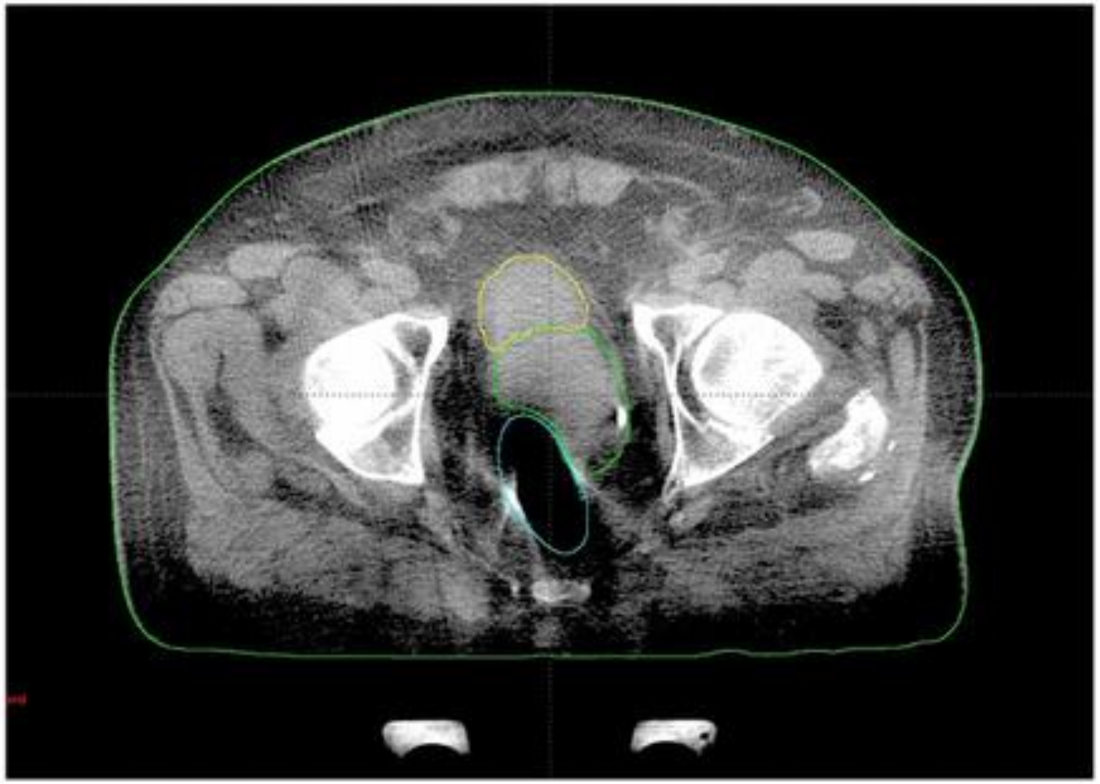
- Decrease patient dose
- Two types used in different modes: Full fan or half fan mode
- Full fan mode: image is acquired at the central axis on the detector panel and images acquired from 200^{o} rotation
- Half fan mode: the detector is offset laterally acquiring only half of the projection of the patient
  - ➢ Detector panel is offset laterally, rotates a full 360^{o} captures only half a projection and reconstructs the image from that
  - ➢ Recommended for larger FOV (pelvis)
  - ➢ Half fan filters result in the greatest HU discrepancy b/w CT and CBCT (Ding *et al.*, Yoo and Fang-Fang, Seet *et al.*)

CBCT Image Quality

- **Patient characteristics**

  - Size
    - Poor image quality as the patient contour approached the limits of the FOV
  - Tissue heterogeneity
  - High dense structures
    - Hip prosthesis
  - Motion
    - Increased risk of motion with slow scan time
    - E.g. peristalsis, breathing and gas

CBCT Image Quality

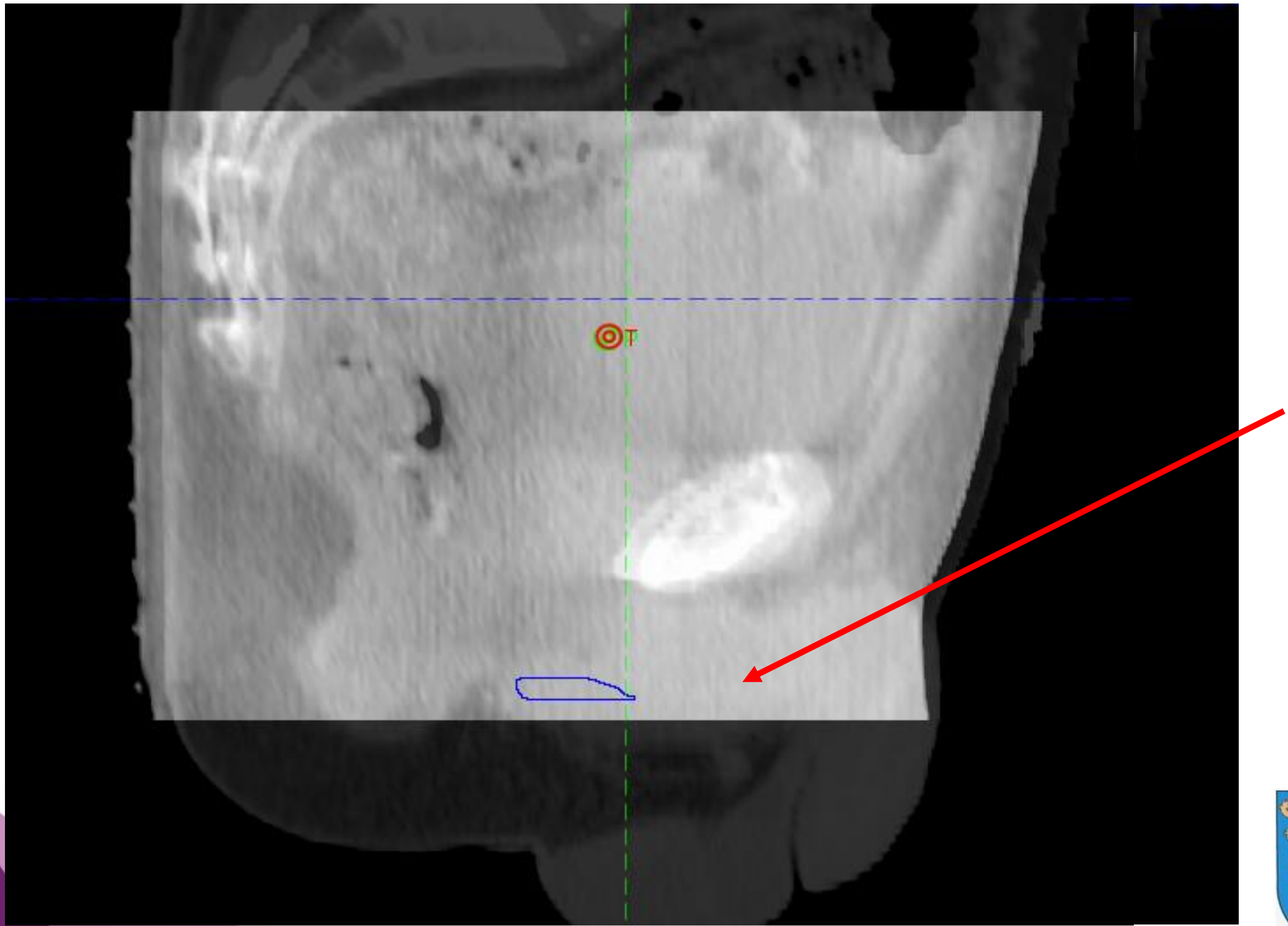


Reggiori et al., 2010

Degradation of image quality due to patient size and gas passing through rectum at time of scan

The Image Acquisition Process

- Make sure you image what you need to match and review to
- Option to offset the couch to ensure appropriate anatomy is visualized



Definitive Prostate Case

Couch now offset to include Penile Bulb in image

The Image Acquisition Process

- Option to offset the couch to ensure appropriate anatomy is visualized

Missing Superior PTV

Excessive inferior

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journal homepage: www.thegreenjournal.com

Review

The European Society of Therapeutic Radiology and Oncology–European Institute of Radiotherapy (ESTRO–EIR) report on 3D CT-based in-room image guidance systems: A practical and technical review and guide

Stine Korreman[a], Coen Rasch[b], Helen McNair[c], Dirk Verellen[d], Uwe Oelfke[e], Philippe Maingon[f], Ben Mijnheer[b], Vincent Khoo[c,g,*]

[a]Department of Radiation Oncology, The Finsen Centre, Rigshospitalet, Copenhagen, Denmark; [b]Department of Radiation Oncology, The Netherlands Cancer Institute/Antoni van Leeuwenhoek Hospital, Amsterdam, The Netherlands; [c]Department of Clinical Oncology, Royal Marsden NHS Foundation Trust, Chelsea and Sutton, London, UK; [d]UZ Brussel, Oncologisch Centrum, Radiotherapie, Brussels, Belgium; [e]Department of Medical Physics in Radiation Oncology, Deutsches Krebsforschungzentrum, Heidelberg, Germany; [f]Département de Radiothérapie, Centre Georges-François-Leclerc, Dijon, France; [g]Institute of Cancer Research, Chelsea, London, UK

Table 1
Factors for consideration in image acquisition and their relevance.

What field of view (FOV) length is available in the cranio-caudal direction?
Determines the length of scan available and possible solutions if longer scan lengths are required
What size is the reconstruction circle?
Determines the lateral FOV
Are filters required? – Which filters are available?
Involves time to select and insert, and affects image quality
Are filters interlocked?
If not, then risk of poor quality or unusable scans from incorrect filters selection
Can panel be positioned remotely? If so, does this the system come with an anti-collision system?
Will involve time to position if not remotely accessed
What are the available rotation speeds?
Determines the acquisition time
What are the possible angles of rotation?
Affects the flexibility of scanning; e.g. the possibility of performing half-scans for small regions, rotations through 180 degrees (underneath the patient) and using preset or flexible start and stop angles
How ergonomic is the operation?
One- or two-button operation, foot- or hand-control, several screens affects the ease of operation and the risk of aborted scans
Can the scan be stopped and restarted?
Will result in extra dose if the scan is interrupted inadvertently, and has to be started from the beginning
Also allows the scan to be acquired with the patient in several breath holds.

ARTT Applied Radiation Therapy Trinity Research Group

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The Image Registration Process

Automatic Match

- Uses matching algorithm based on “Mutual Information” within the defined field of view

Manual Match

- Allows adjustments to be made using either mouse or keyboard

- User dependant
  - Respect the learning curve

The Image Registration Process

- The Region of Interest Box
- Used for the automatic registration algorithm
- Defines the greyscale range (HU) that the algorithm will use for the solution
- The interface has additional options
  - Consider the “Stucture VOI” option
  - Margin added to this Structure VOI will help drive the MI algorithm
  - Intensity Range
  - **Be willing to adjust settings to ensure you are getting the most out of your system!**

  - Similar to Elekta, the anatomy included is very important

The Image Registration Process

- Correctional shifts are displayed to the nearest 1mm
- Any automatic match ***must*** be reviewed by both the RTTs prior to treatment
- No machine can replace clinical judgement
- Know your volumes
  - Be aware of possibility of additional "planning volumes"

The Image Registration Process

- How can we decrease inter observer variability?

  - Education of staff (encourage CPD, training packages, competency based assessment)

  - Protocolised imaging methods

  - Protocolised matching methods
    - Sequence of matching process
      - Automatic Match ***must be followed by manual review*** and adjustment

    - VOI and intensity levels set for each site and “locked” on Fx 1
      - Anatomy to include in VOI box

Imaging Setup Field → Additional Planning Instructions → Fraction 1 → Image Acquisition → Image Registration → Evaluation

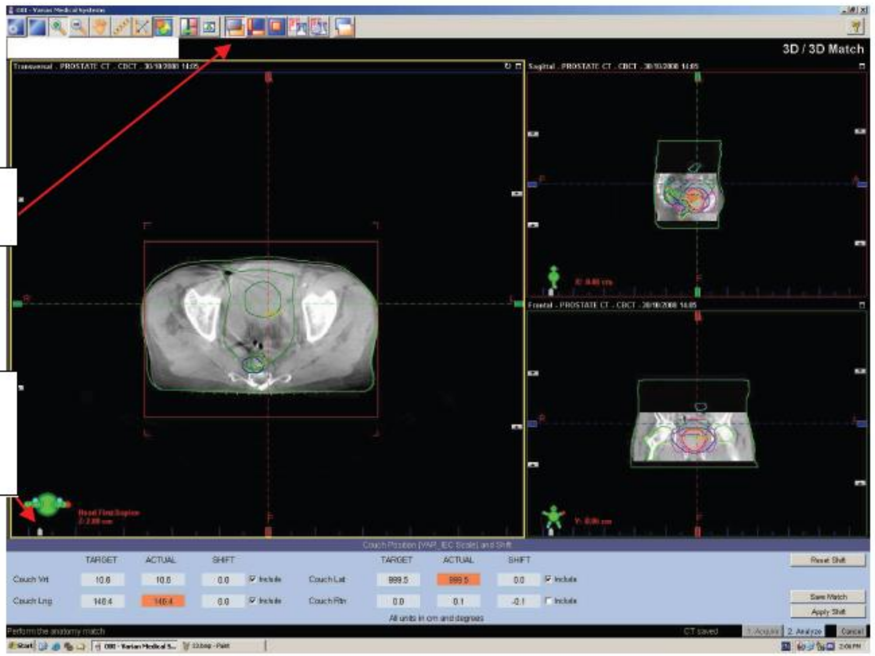
The Image Evaluation Process

- Processes available to assist in image evaluation

- Blending
  - ➢ Blending of the planned and acquired image
  - ➢ Colour or greyscale

Select the blend tool.

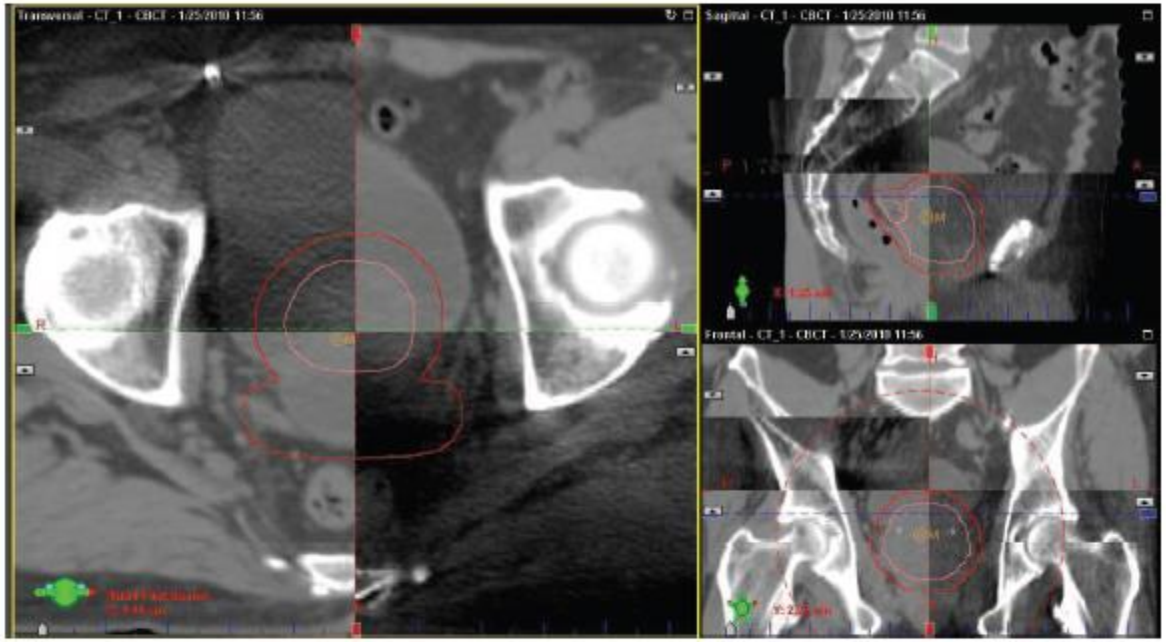
Drag the blend arrow to the LEFT to see the CBCT



The Image Evaluation Process

- Processes available to assist in image evaluation

- Split screen

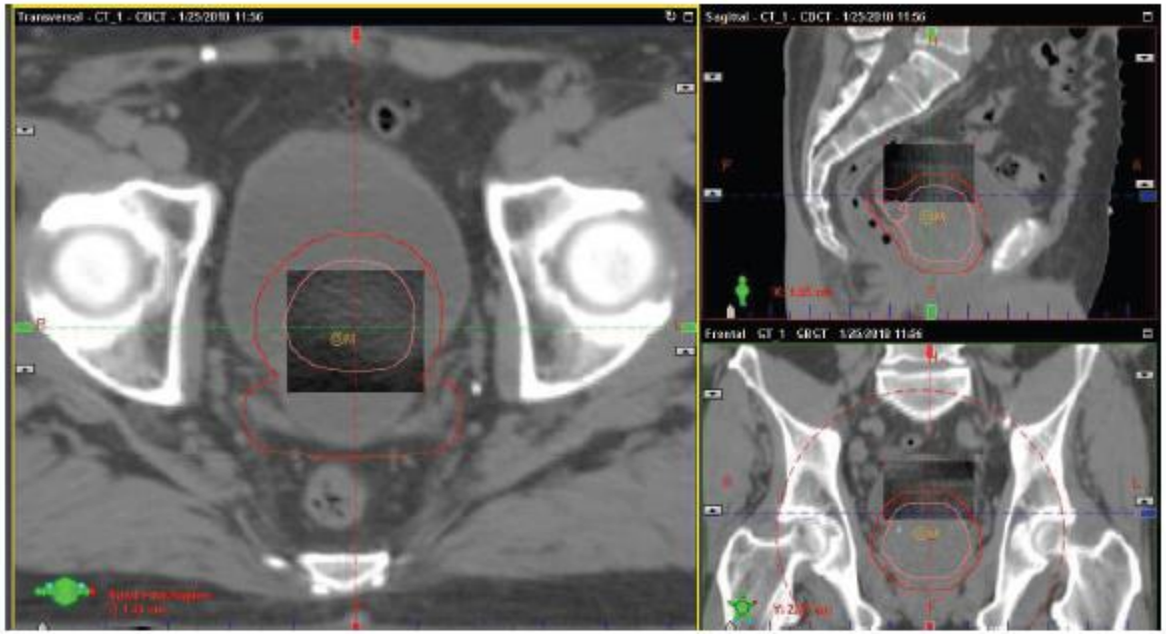


Don't forget to adjust the window level and move your views around

The Image Evaluation Process

- Processes available to assist in image evaluation

- Moving window tool

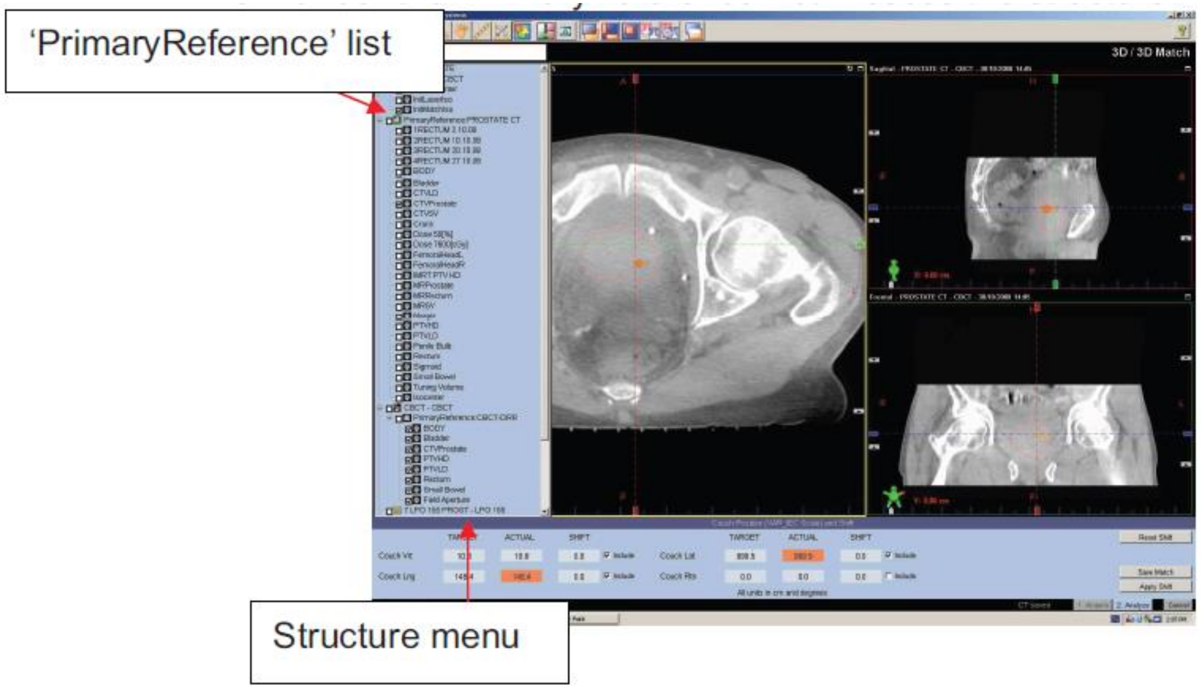


Don’t forget to adjust the window level and move your views around

The Image Evaluation Process

- Processes available to assist in image evaluation

- Overlay Structure
  - ➢ Volumes that were contoured at the planning stage

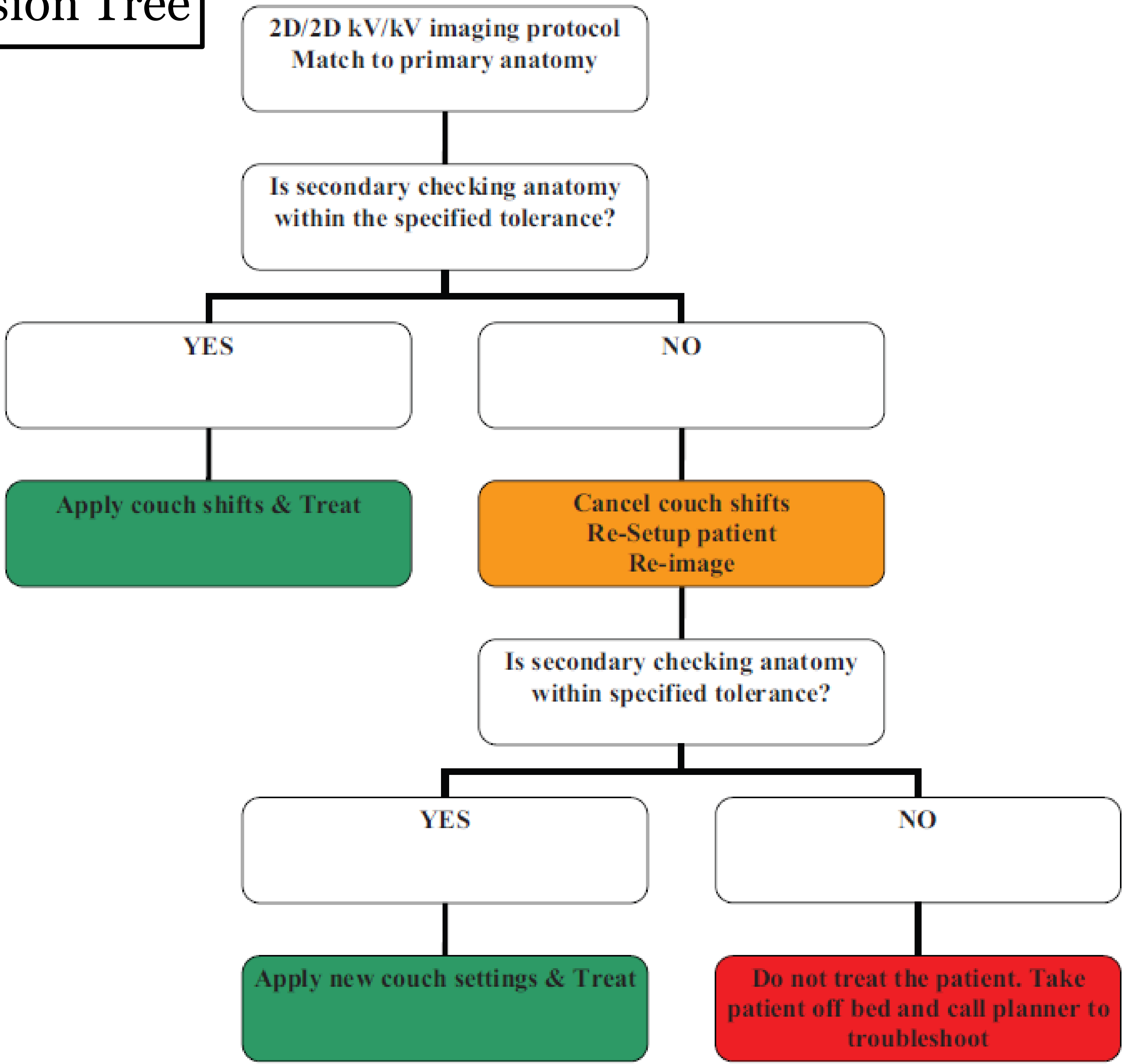


The Image Evaluation Process

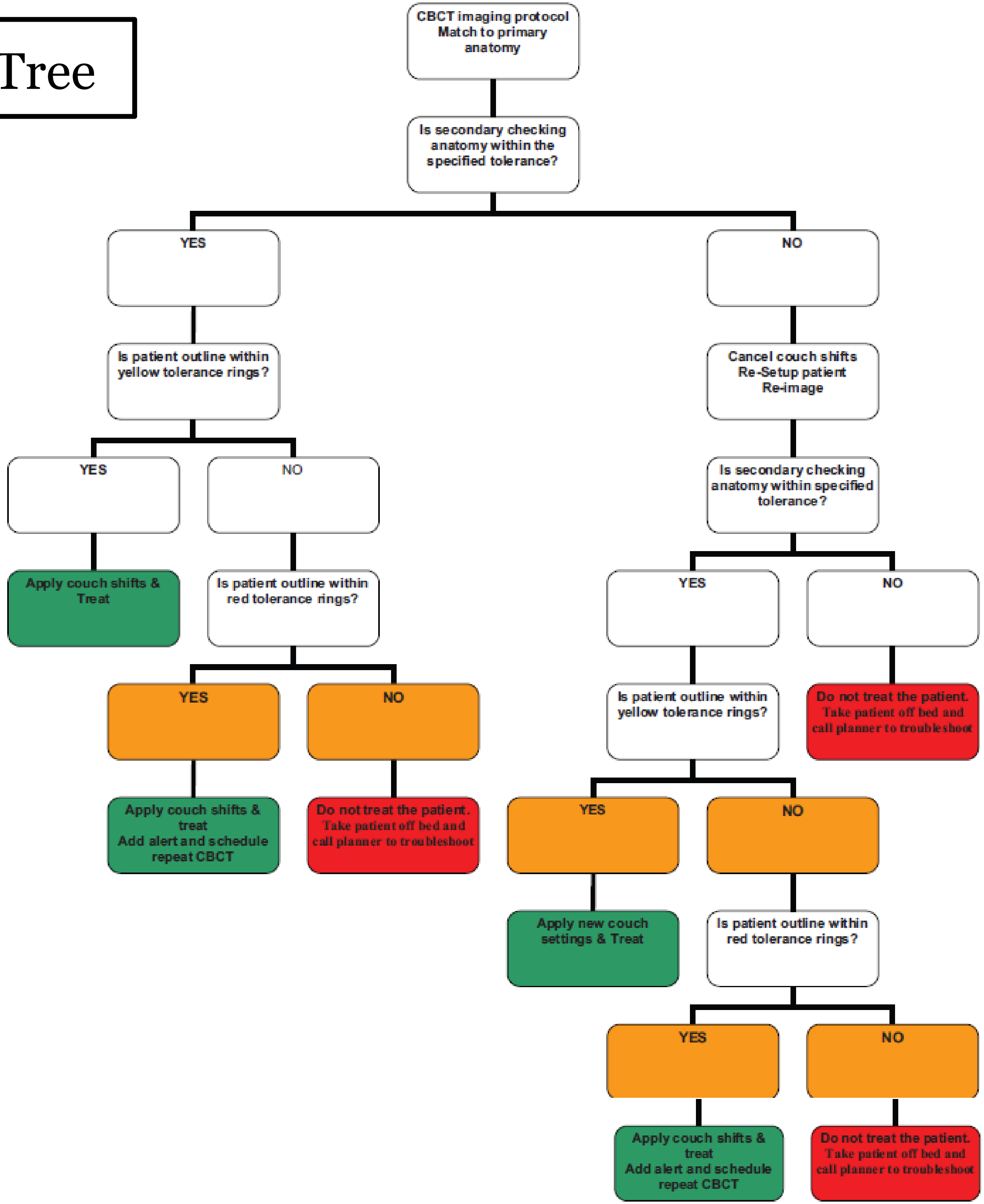
- The evaluation process must not be rushed
  - ➢ Check that the shifts are *sensible*
- Both RTTs must confirm the match
- *"If that were my mum…"*
- It is better be check than treat the patient incorrectly
- IGRT is a team approach and if unsure there are always people to help
- Communicate!
  - ➢ Journal, Alerts, annotation on the image

"the importance of this visual inspection cannot be over-emphasized and the user is encouraged to assess the accuracy of these automated registration tools" *(Korreman et al., 2010)*

2D/2D Decision Tree



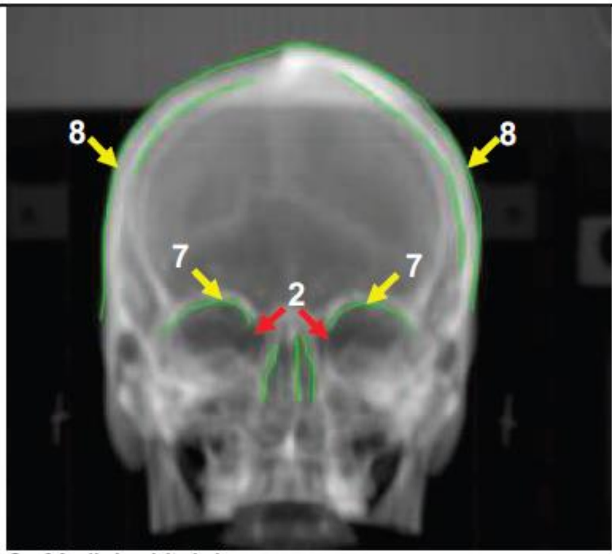
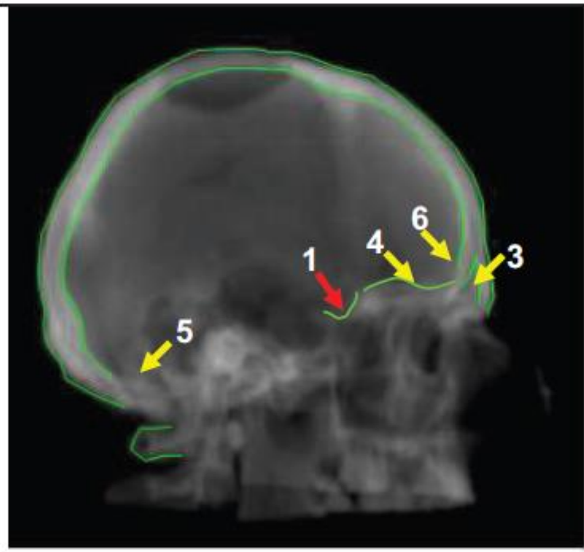
CBCT Decision Tree



Site Specific Application

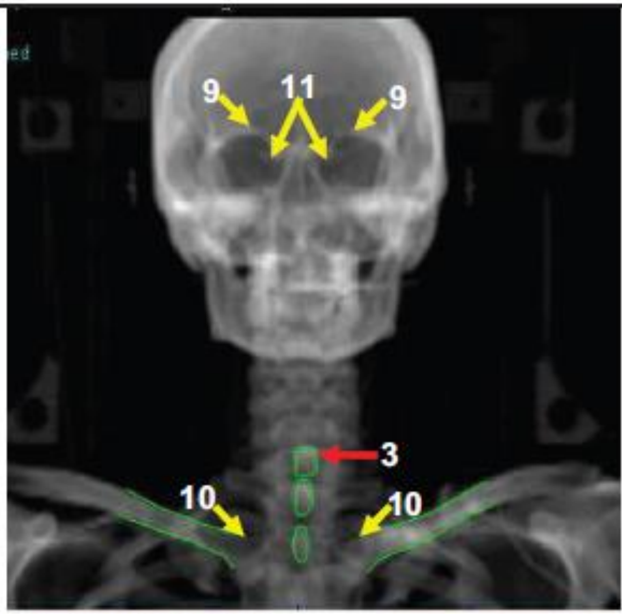
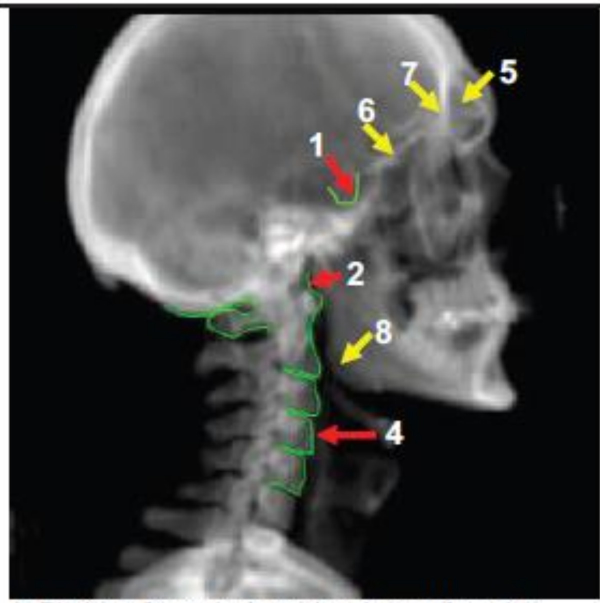
Radical CNS

- Examples of structures to outline on DRR for 2D/2D match

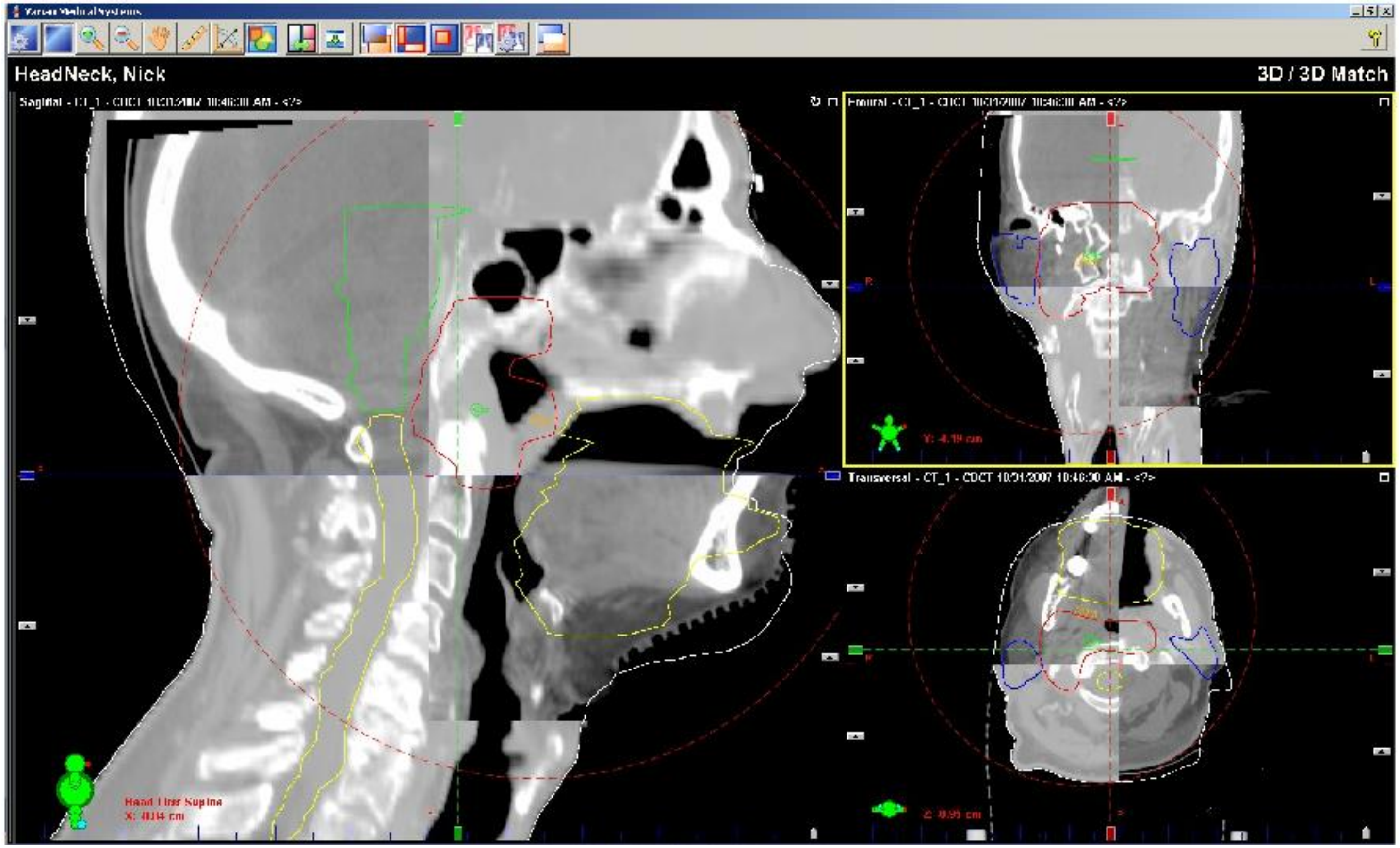
Site	Image type	Primary (red) and Confirming (yellow) matching anatomy
Brain	KV & CBCT	 2. Medial orbital rims 7. Superior orbital rims 8. Lateral skull wall (parietal region)  1. Pituitary fossa (volumend and transferred to reference image) 3. Frontal sinus 4. Base of skull in pituitary fossa region 5. Base of skull in Occipital bone region 6. Anterior cranial fossa

Head and Neck

- Examples of structures to outline on DRR for 2D/2D match

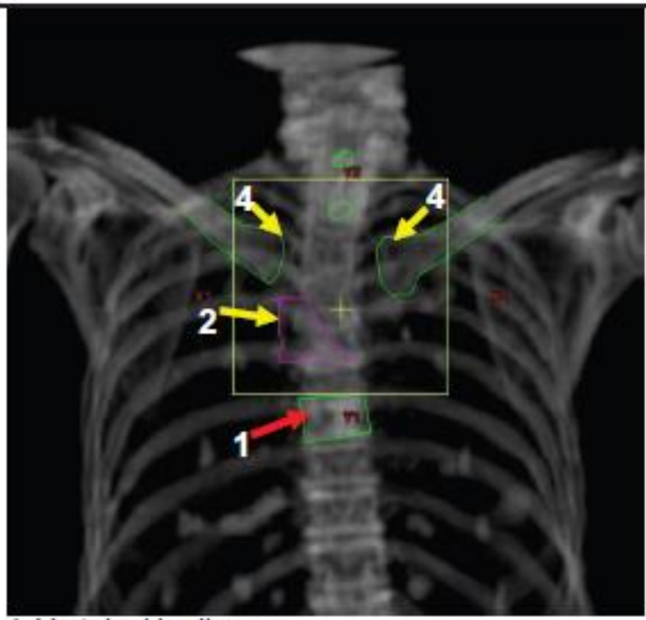
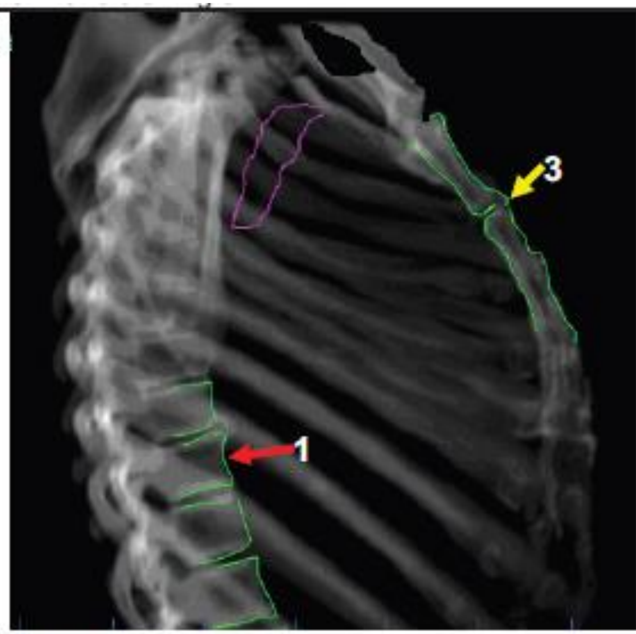
Naso-Pharynx	kV & CBCT	 3. Spinuous processes 9. Superior orbital rim 10. Head of Clavicles 11. Medial orbital rims	 1. Pituitary fossa (volumed and transferred to reference image) 2. Intersection of anterior vertebral column and base of skull 4. Vertebral bodies 5. Frontal sinus 6. Base of skull in pituitary fossa region 7. Anterior cranial fossa 8. Mandible angle

Head and Neck



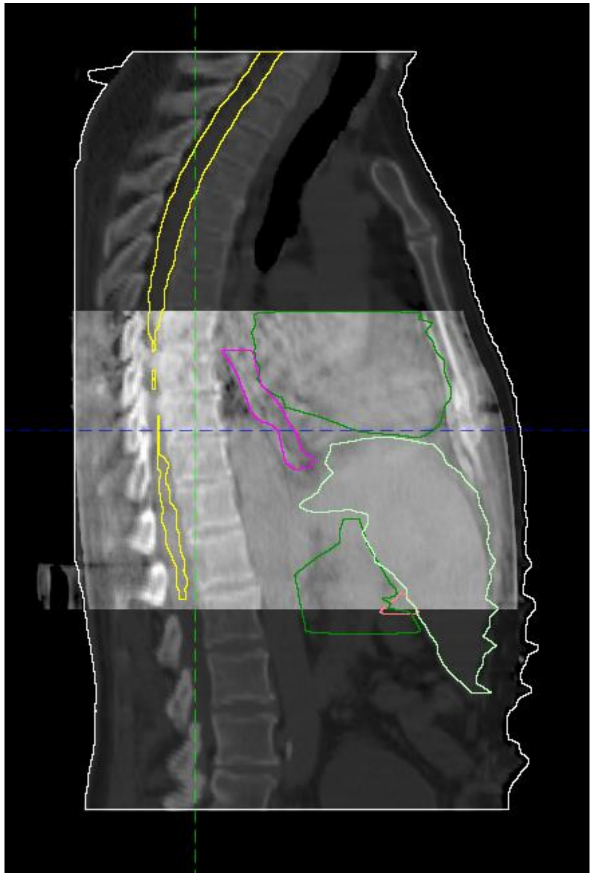
Thorax and Upper Abdomen

- Examples of structures to outline on DRR for 2D/2D match

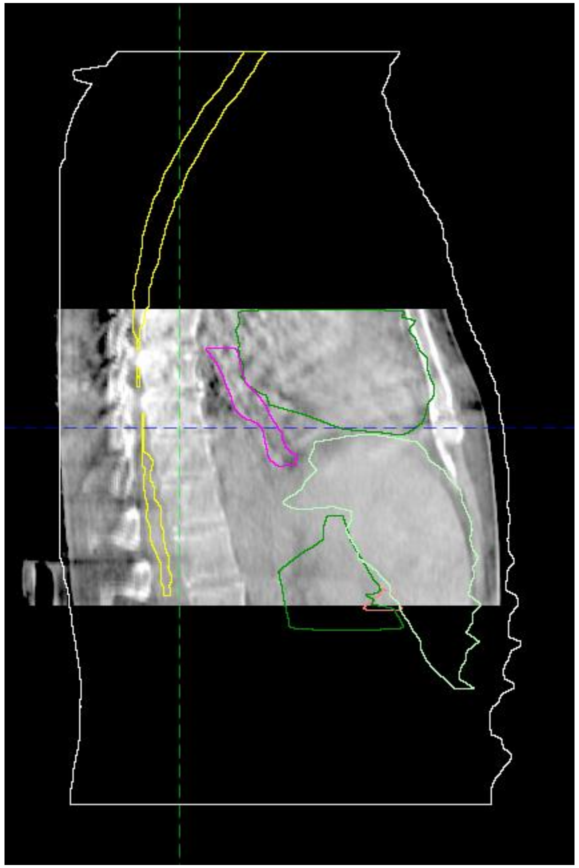
Chest	kV & CBCT	 1. Vertebral bodies 2. Contoured Carina 4. Head of Clavicles	 1. Vertebral bodies 3. Manubrial-sterno joint

Thorax and Upper Abdomen

Blended View

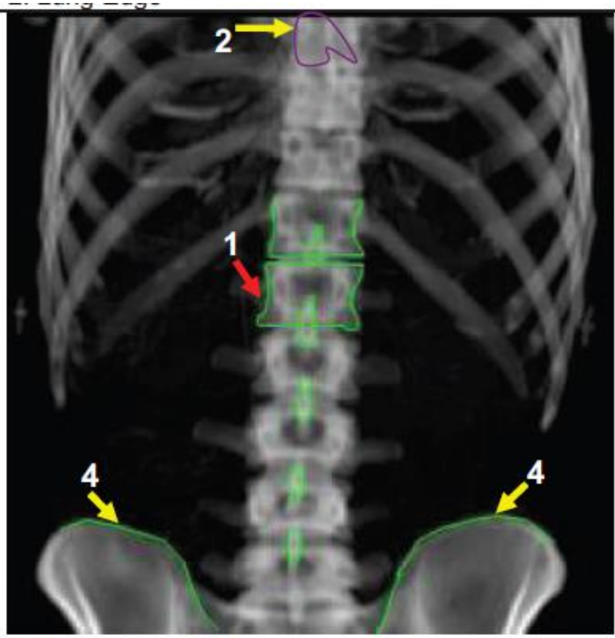
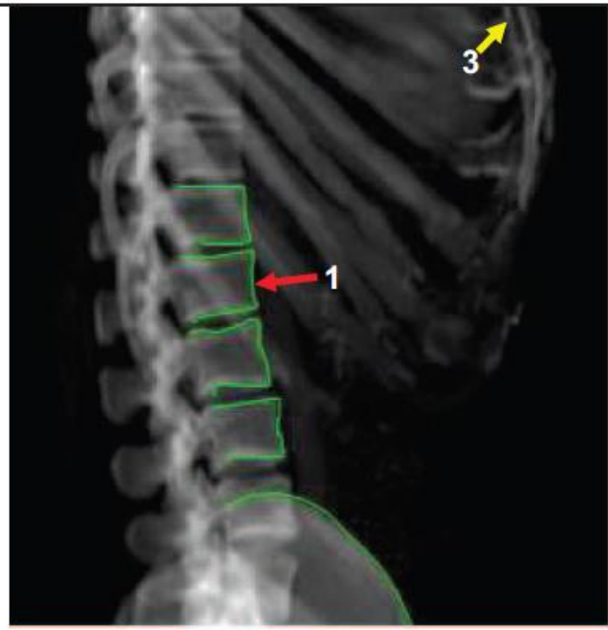


Contour Overlay



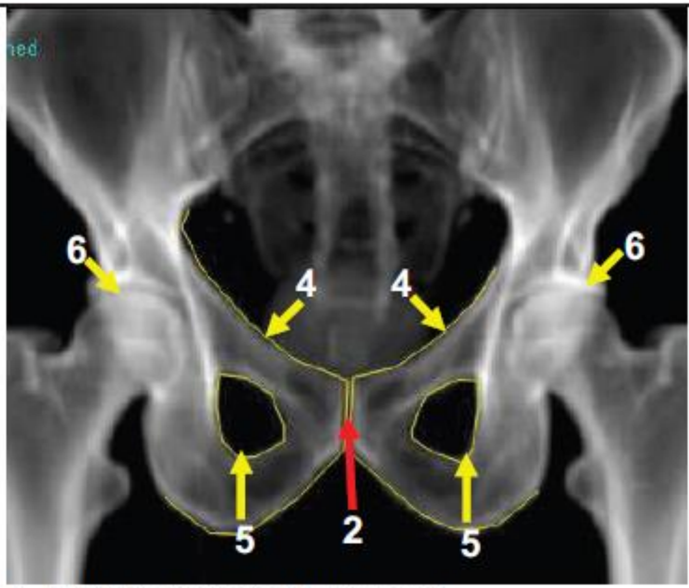
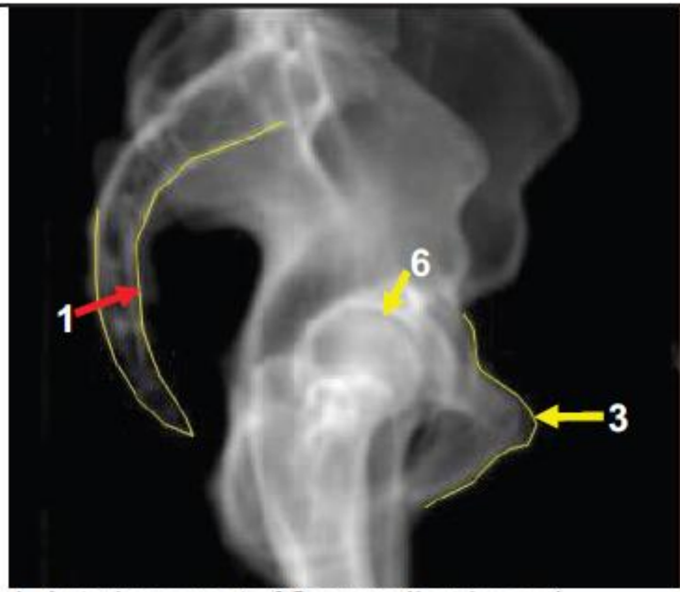
Abdomen

- Examples of structures to outline on DRR for 2D/2D match

Abdomen Pancreas Adrenal Gastric	kV & CBCT	 1. Vertebral bodies 2. Contoured Carina (if on image) 4. Iliac crest	 1. Vertebral bodies 2. Contoured Carina (if on image) 3. Manubrial-sterno joint

Rectum

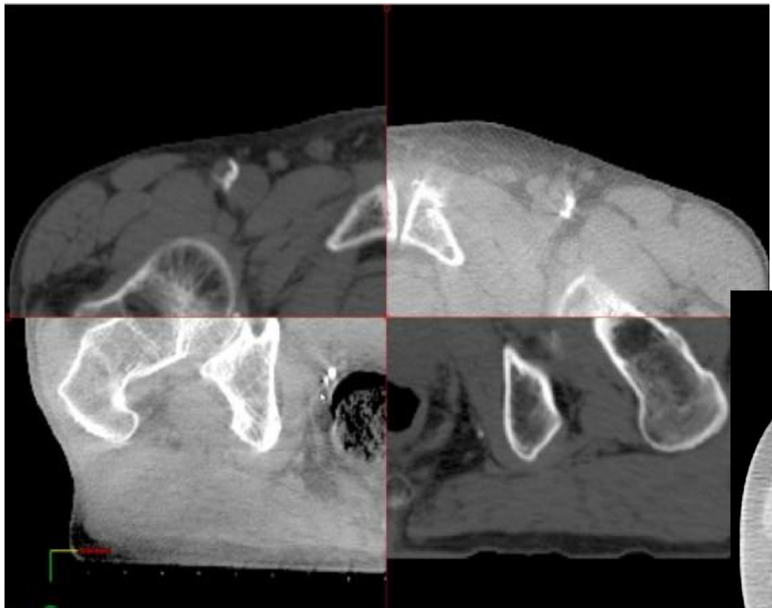
- Examples of structures to outline on DRR for 2D/2D match

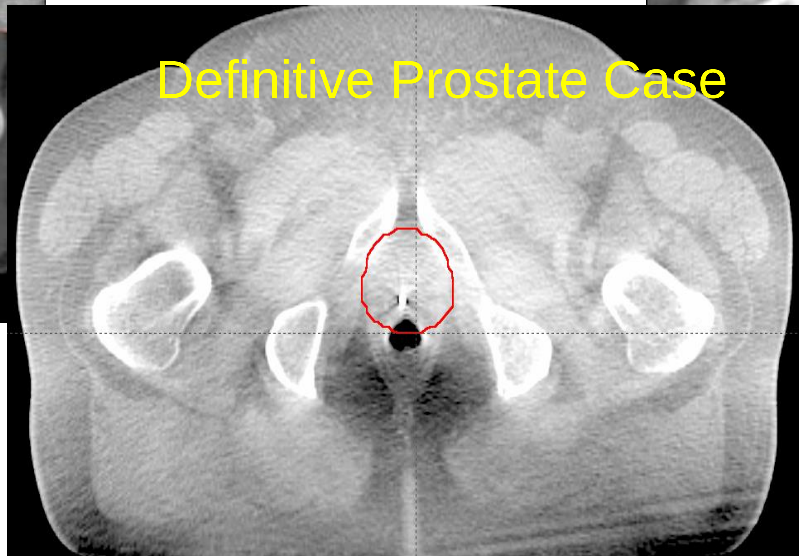
Rectum/ Anus	kV & CBCT	 2. Pubic Symphasis **(AP image)** 4. Pelvic Rim 5. Obturator Foramen 6. Head of Femur	 1. Anterior aspect of Sacrum **(Lat image)** 3. Pubic Symphasis 6. Head of Femur

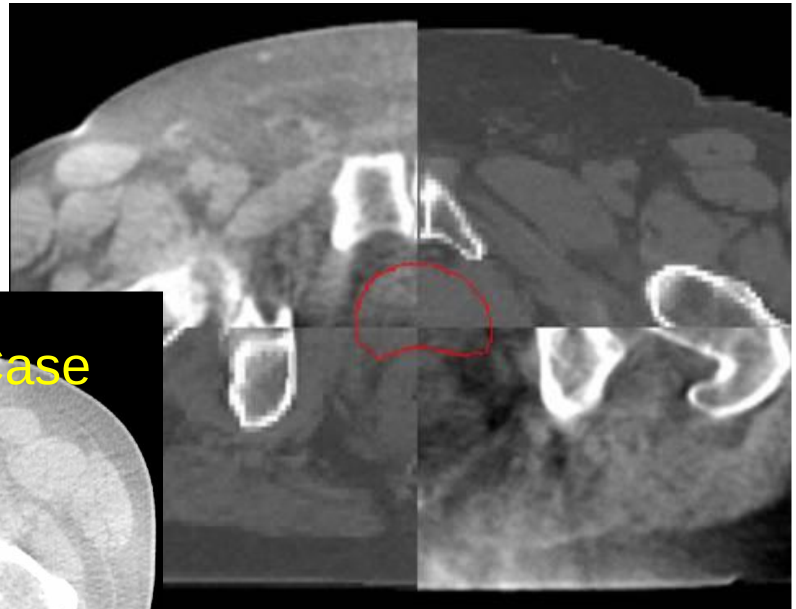
Prostate

- Do ***not*** match to bones for definitive cases

Definitive Prostate (seeds)	kV	All fractions except CBCT	Daily moves
	CBCT	1,2,3,5,10,15,20,25,30,35,40	
Definitive Prostate (soft tissue)	CBCT	All fractions	Daily moves

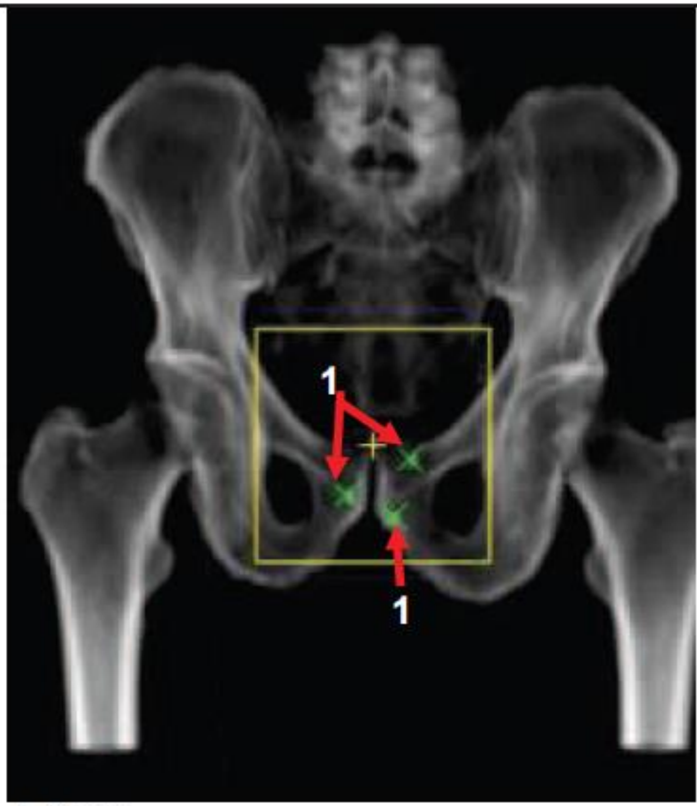
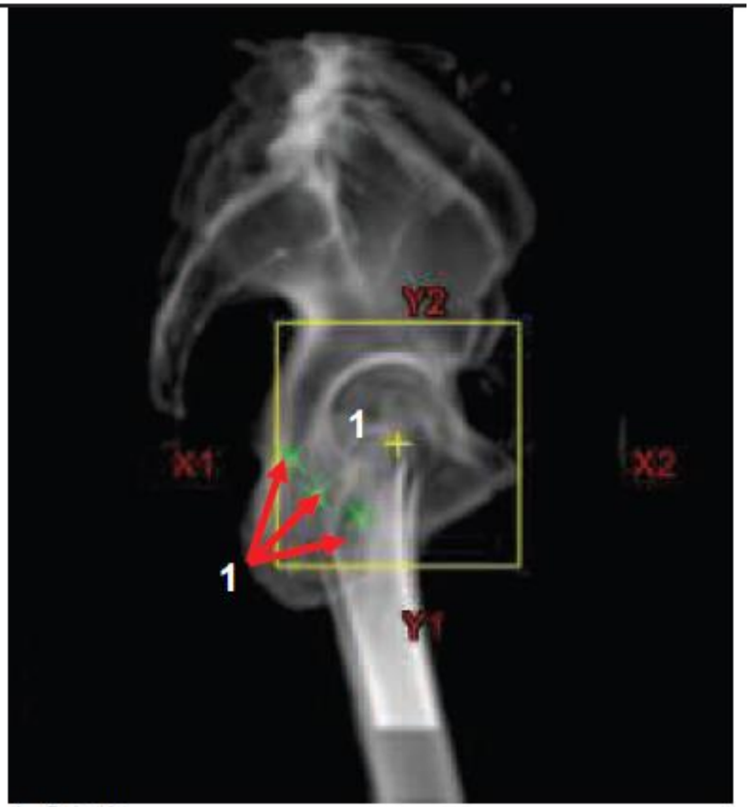




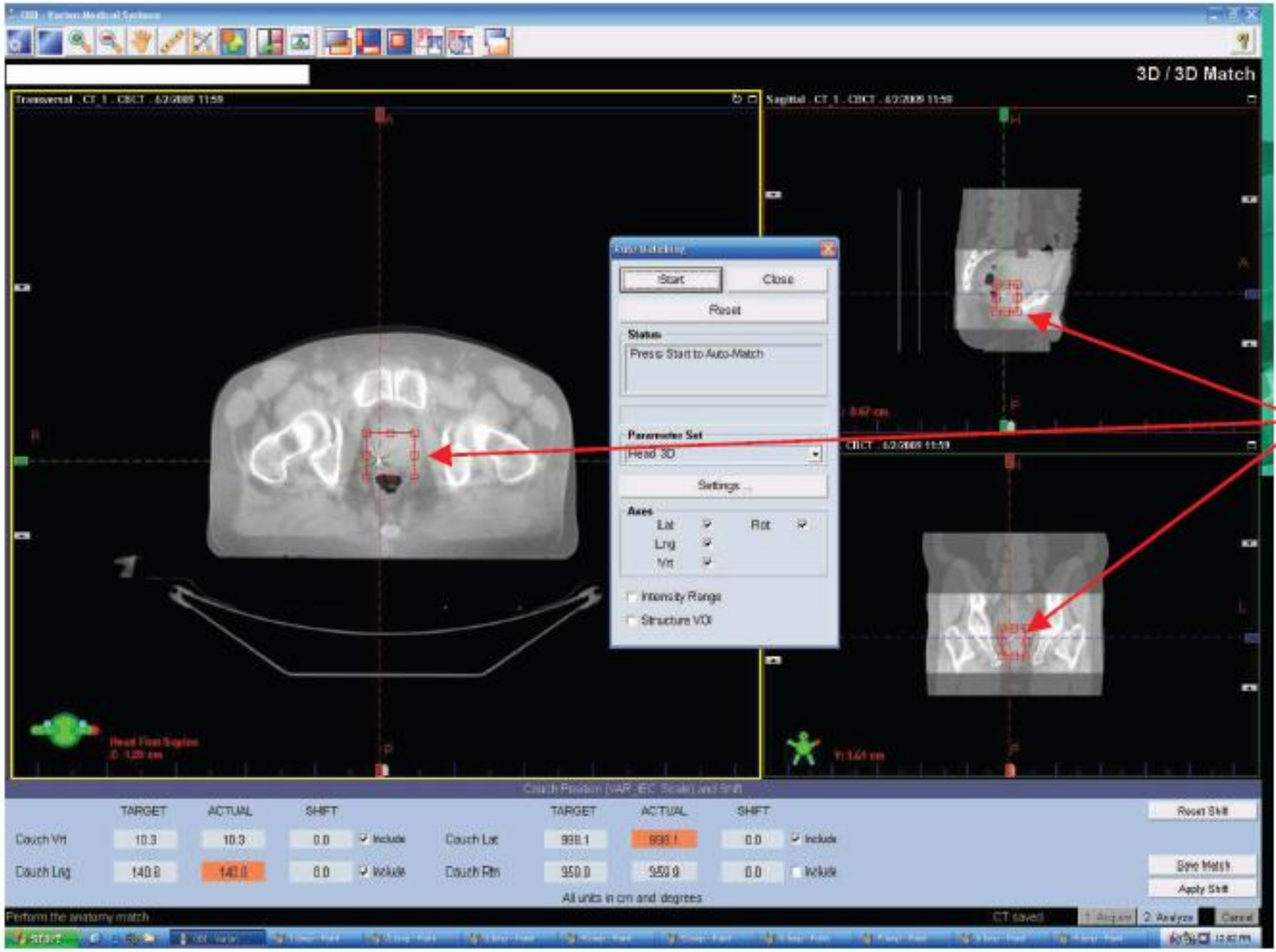


Prostate – 2D/2D fiducial match

- Match points used for 2D/2D fiducial match

Prostate (Seeds)	kV & CBCT	 1. Seeds	 1. Seeds

Prostate – CBCT fiducial match



Move the VOI box on all three views to cover the matching area.
Eg in this picture the fiducial markers

Always scroll through the entire length of the PTV and view in all 3 planes

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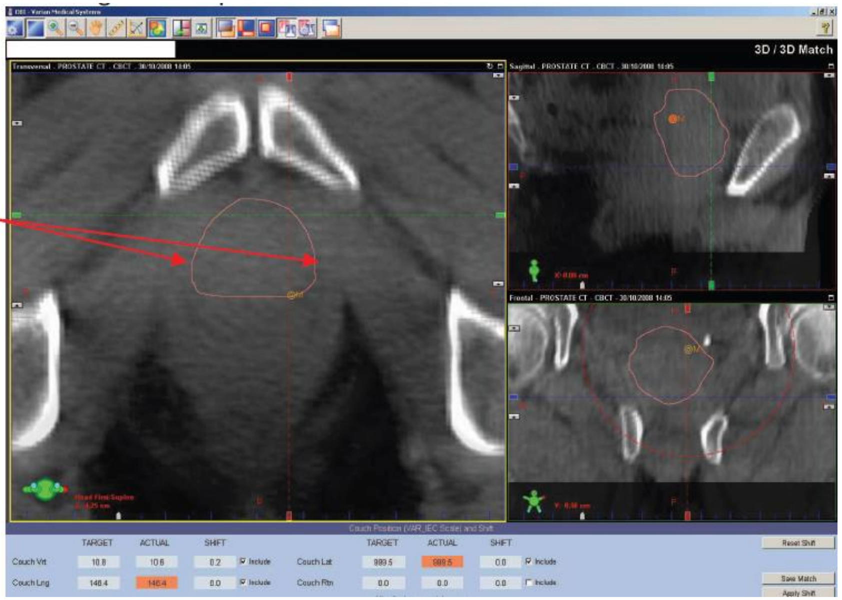
Prostate – Soft tissue

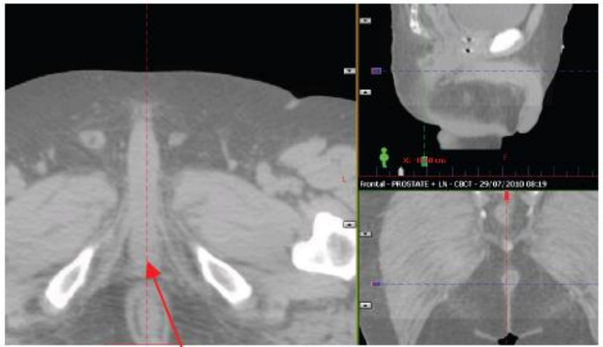
- Process for CBCT soft tissue match
  - *Manual confirmation* of match

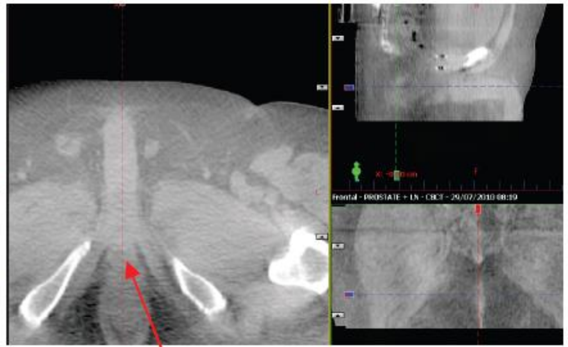
1. Change window level to visualise rectum & superior prostate
2. Position superior CTV prostate contour to superior aspect of prostate at junction with bladder
3. Position posterior edge of CTV prostate structure (at mid prostate) to the anterior rectal wall
4. Check inferior CTV prostate structure to inferior edge of prostate, using penile bulb to assist
5. Position lateral edges of CTV prostate to pelvis muscles

Prostate – Soft tissue

Check the Prostate CTV contour is positioned to the lateral edges of the prostate

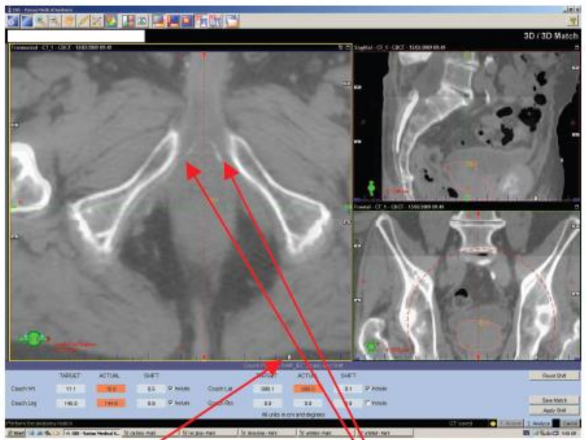


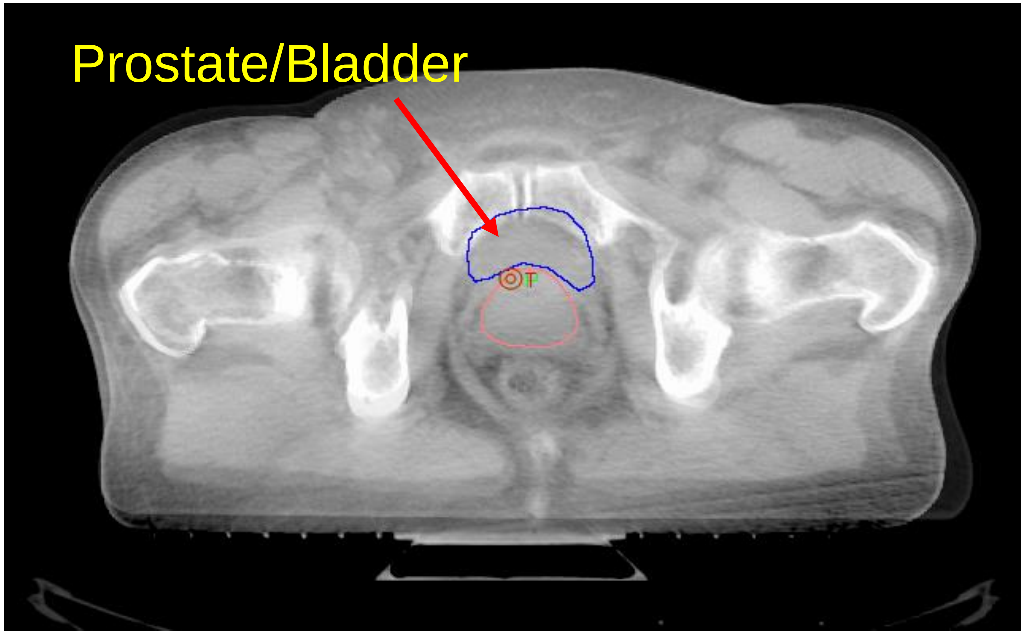




Penile Bulb seen on the GE scan

Penile Bulb seen on the CBCT scan





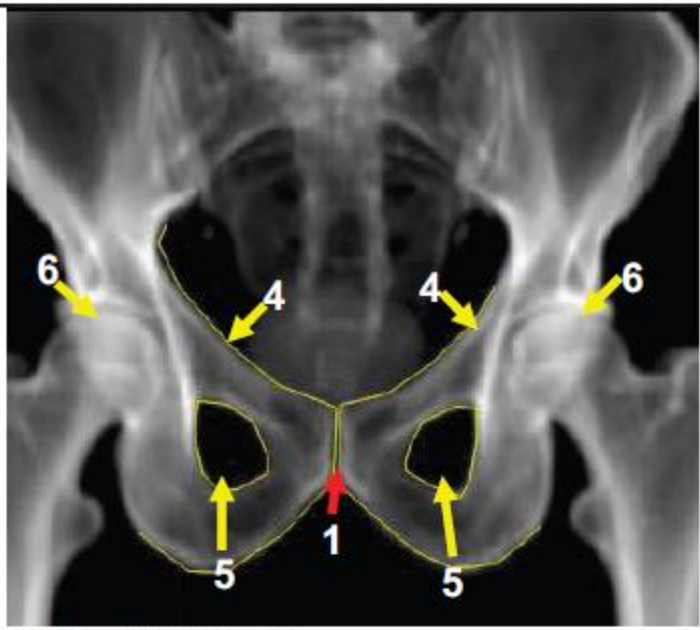
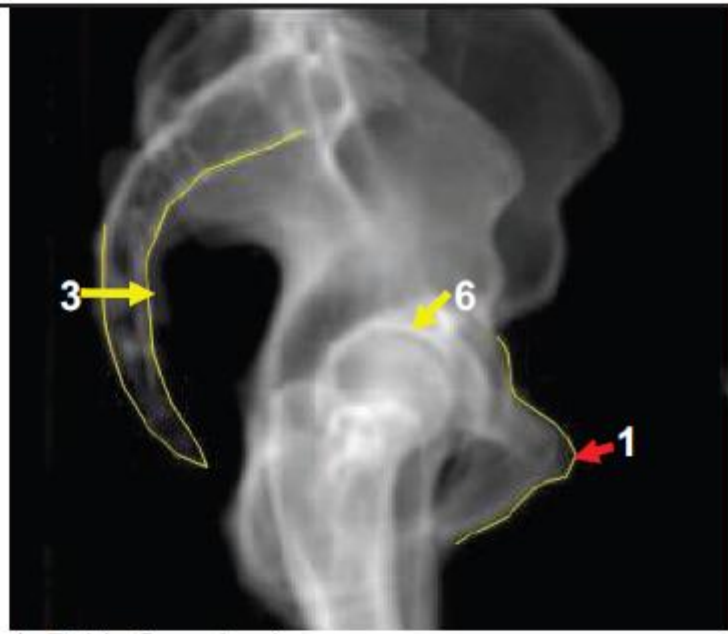
Calcifications seen on the CBCT scan

Slide the blend tool to see the GE scan

Calcifications seen on the GE scan

Prostate Bed

- Example of 2D anatomy to outline on the DRR

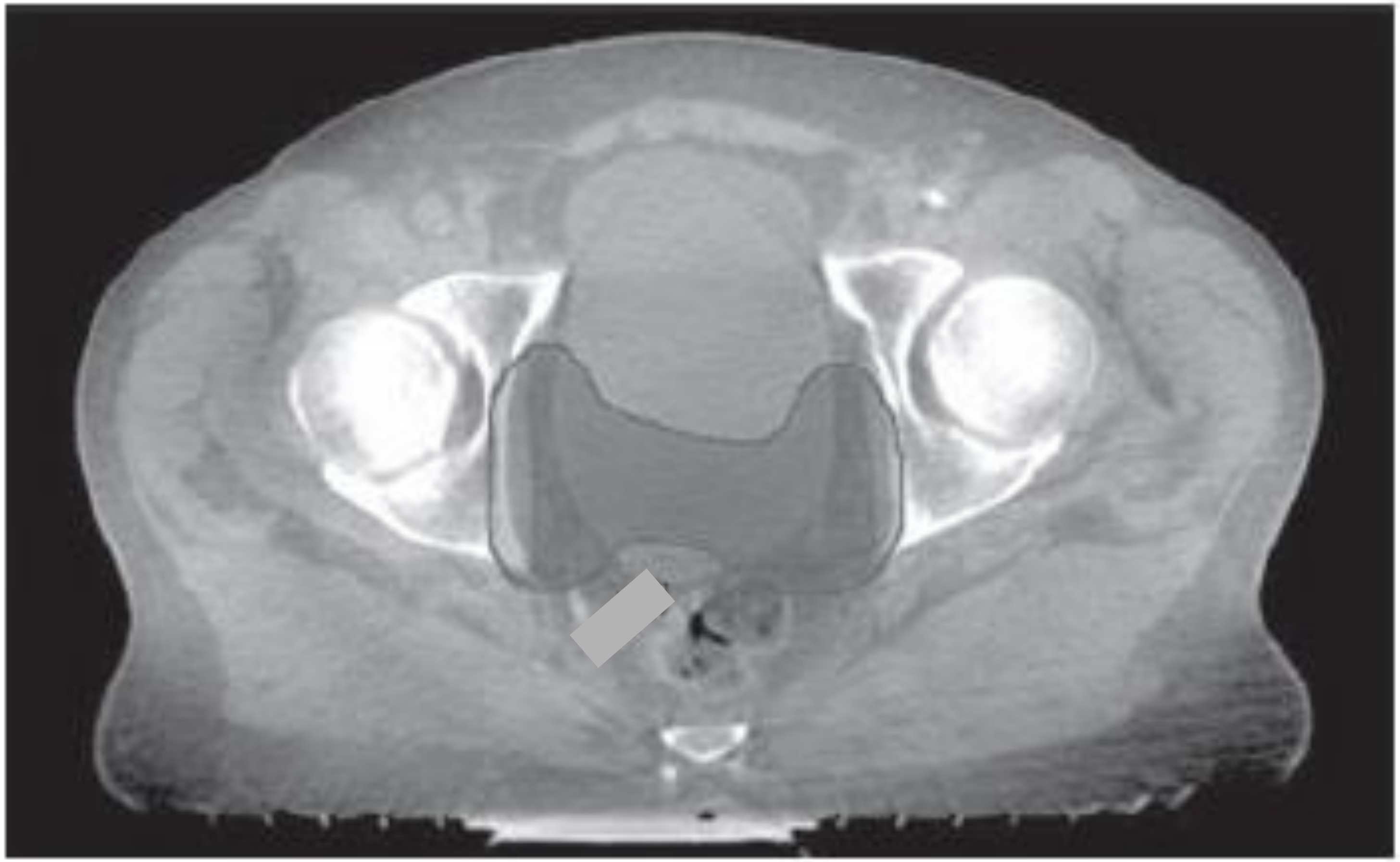
Prostate (Bone)	kV & CBCT	 1. Pubic Symphasis 2. Check any clips are covered with PTV for CBCT 4. Pelvic Rim 5. Obturator Foramen 6. Head of Femur	 1. Pubic Symphasis 2. Check any clips are covered with PTV for CBCT 3. Anterior Sacrum 6. Head of Femur

Troubleshooting

- These are all well suited and ideal cases
- What about when things aren't so clear?! *Troubleshoot*

Prostate Bed

- Instructions match to bones
- Perfect match
- Isodose lines hug the PTV very nicely



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Prostate Bed

- Have an anatomical understanding of exactly what the target is post surgery

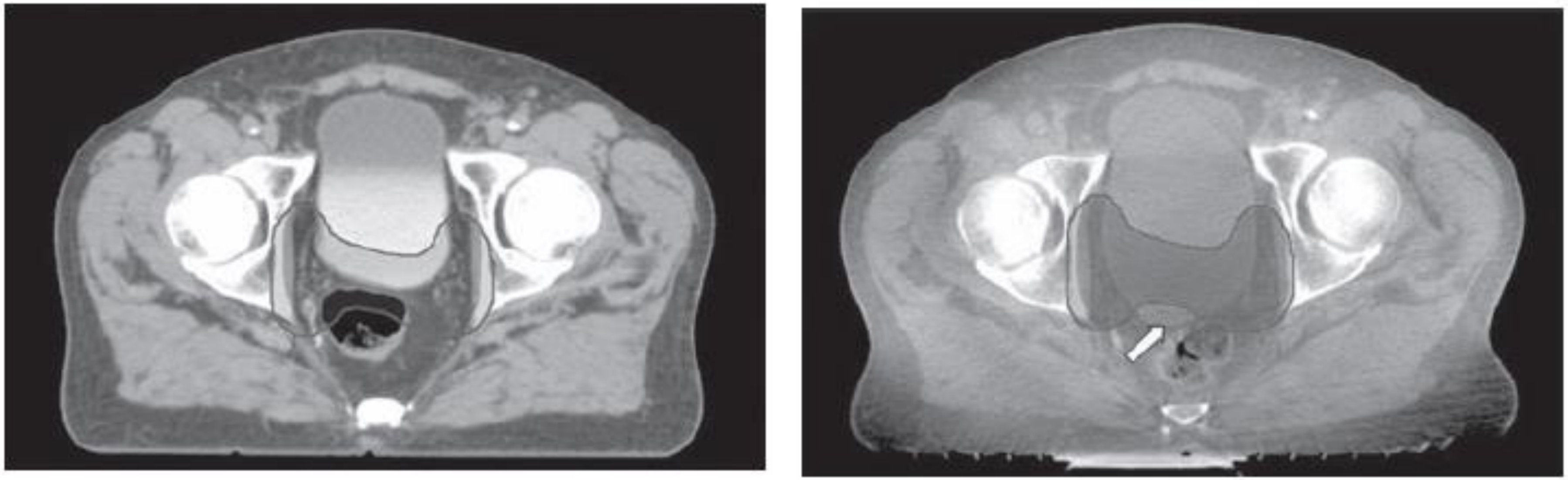

Fig. 4. CBCT of a patient undergoing radiotherapy following radical prostatectomy. Panel (a) shows the initial planning scan with the PTV displayed. Panel (b) shows a change in rectal volume resulting in the treated volume shifting outside the planning PTV (white arrow). CBCT, cone beam computed tomography; PVT, planning target volume.

ARTT Applied Radiation Therapy Trinity Research Group

ESTRO School

Prostate Bed

Radiation Oncology—Original Article

Prostate bed motion may cause geographic miss in post-prostatectomy image-guided intensity-modulated radiotherapy

Linda J Bell[1,2,*], Jennifer Cox[1,2], Thomas Eade[1], Marianne Rinks[1,†], Andrew Kneebone[1]

Article first published online: 9 JUL 2013

DOI: 10.1111/1754-9485.12089

Issue

Journal of Medical Imaging and Radiation Oncology

Volume 57, Issue 6, pages 725–732, December 2013

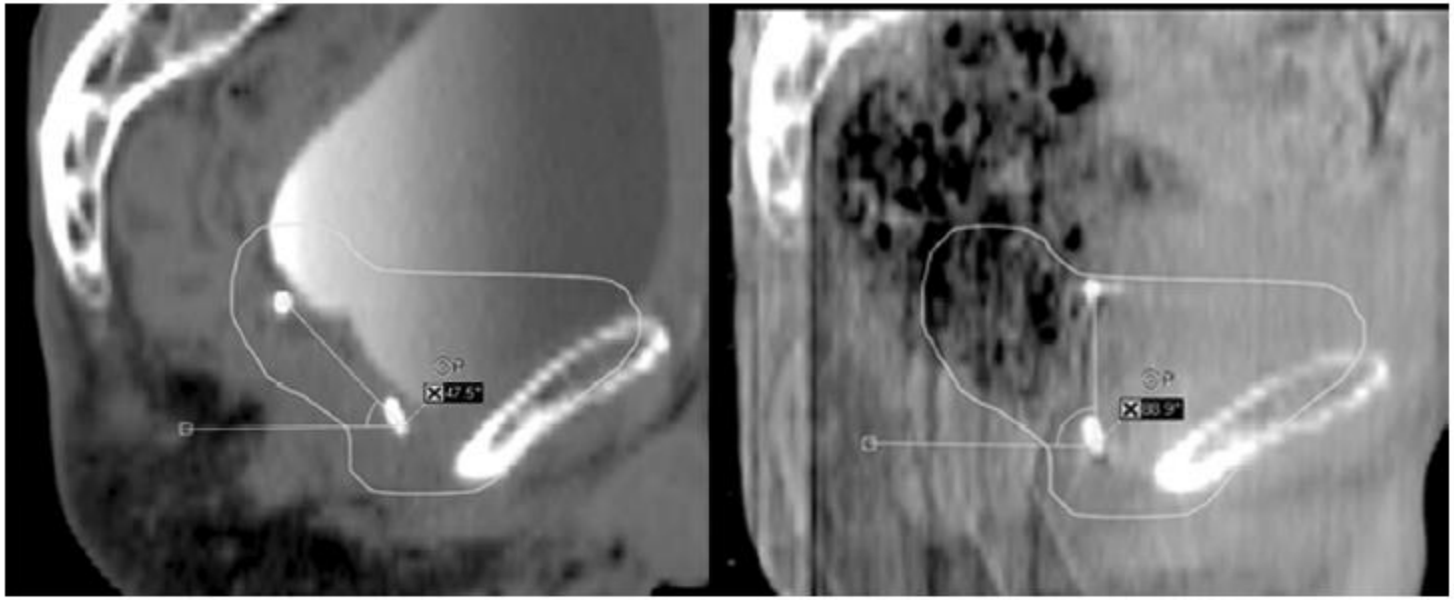

Fig. 1. Method used to measure prostate bed tilt. The angle between the superior and inferior clip relative to a horizontal line at the inferior clip was measured on the planning CT scan (left) and the cone beam CT scans (right). The angle-measuring tool in the Varian Offline Review® software was used to calculate this on the sagittal slice closest to midline of each scan where the clips could be visualised. The difference between the planning CT and cone beam CT angles was calculated. In this extreme case the angle on the planning CT (left) is 47.5° and that on the cone beam CT scan (right) is 88.9°. This is a difference of 41.4°. The FROGG-acceptable planning target volume expansion is delineated on these scans.

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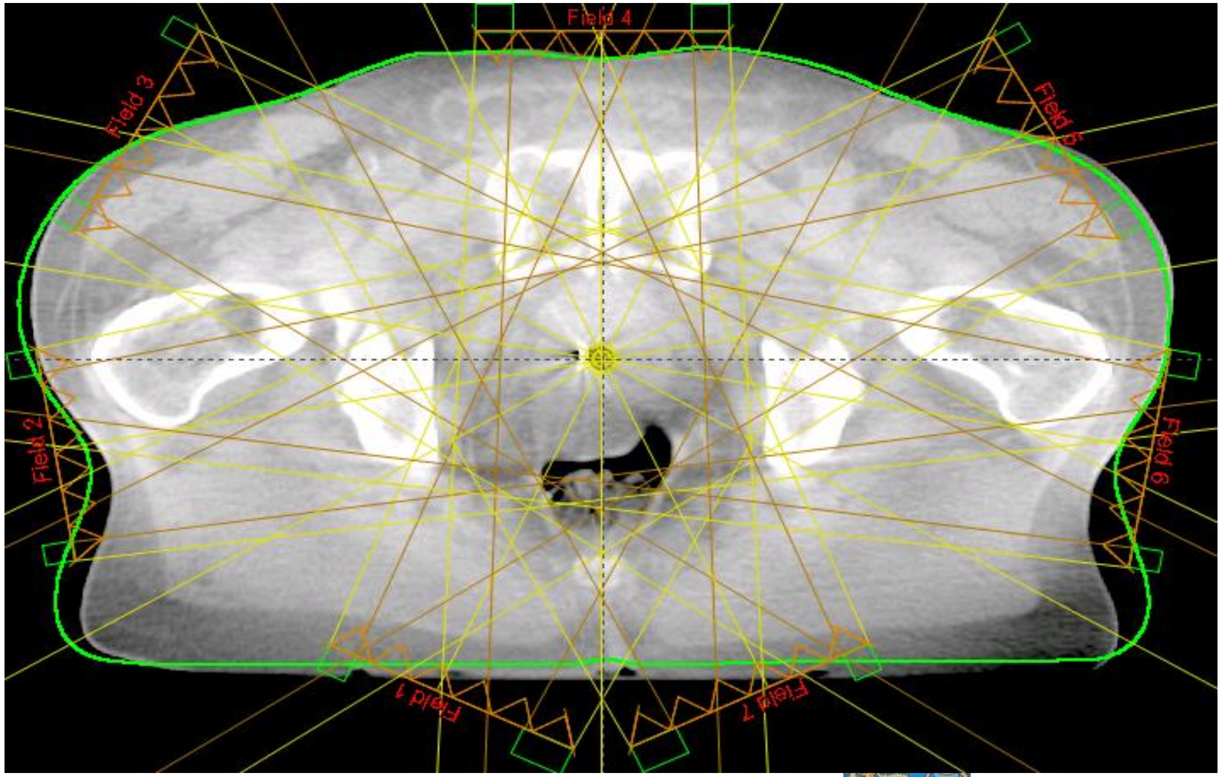
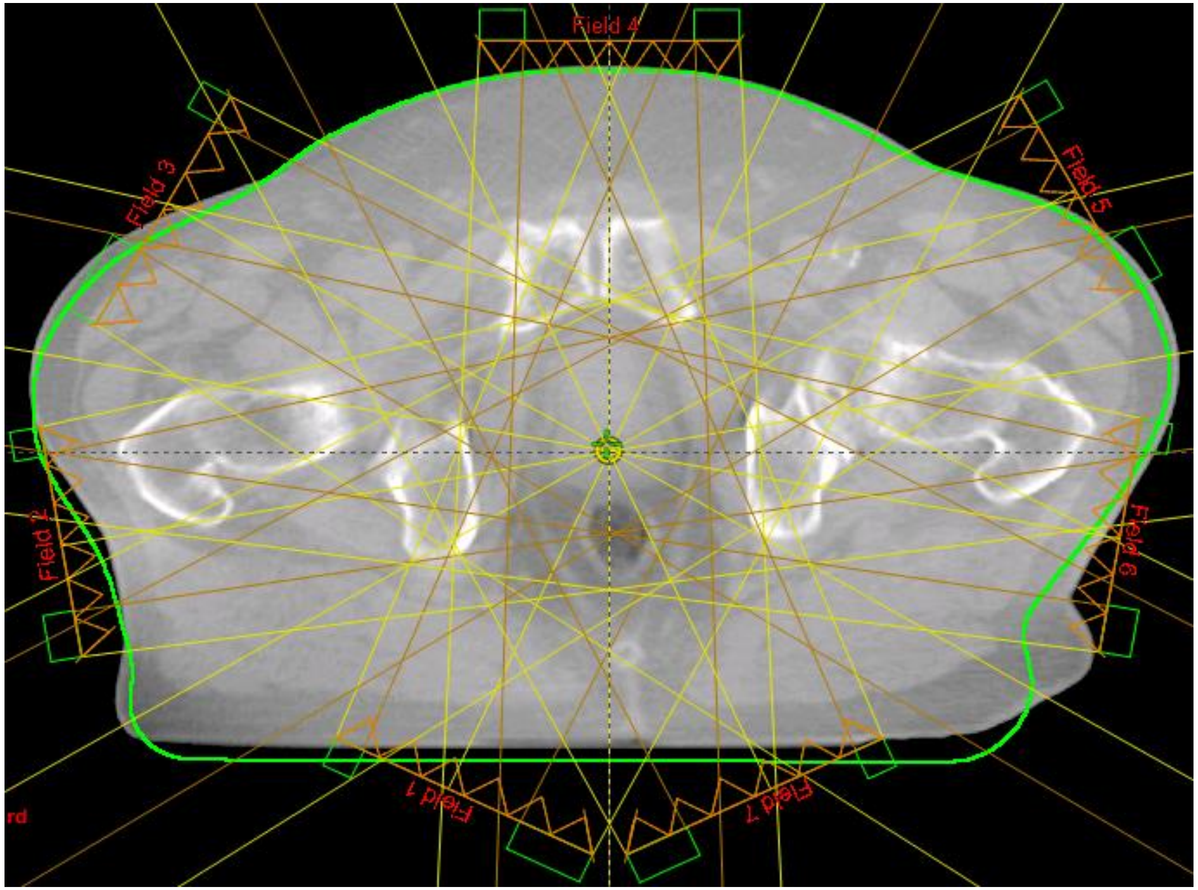
Definitive Prostate

- IMRT
- Daily online
- Match to implanted fiducials



Troubleshooting

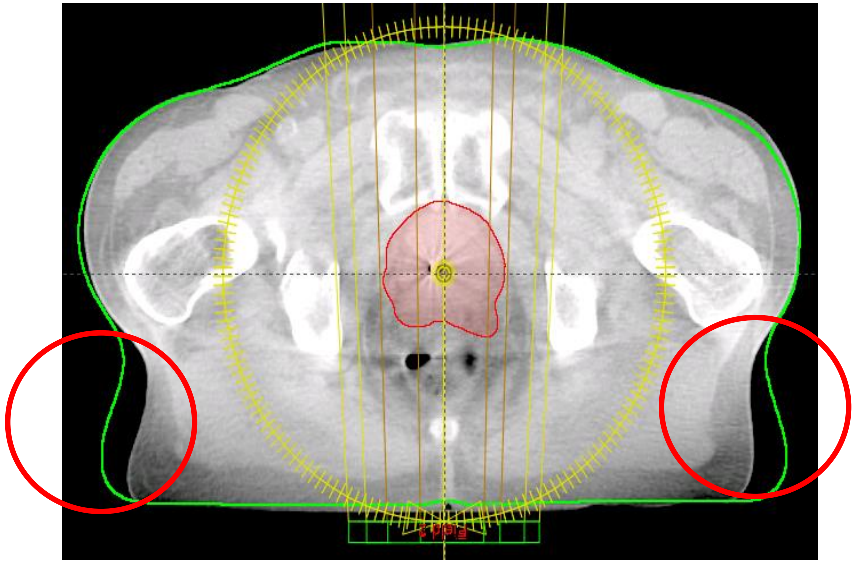
- Look beyond the target!
- Impact not on target ***position***, but on target ***dosimetry***

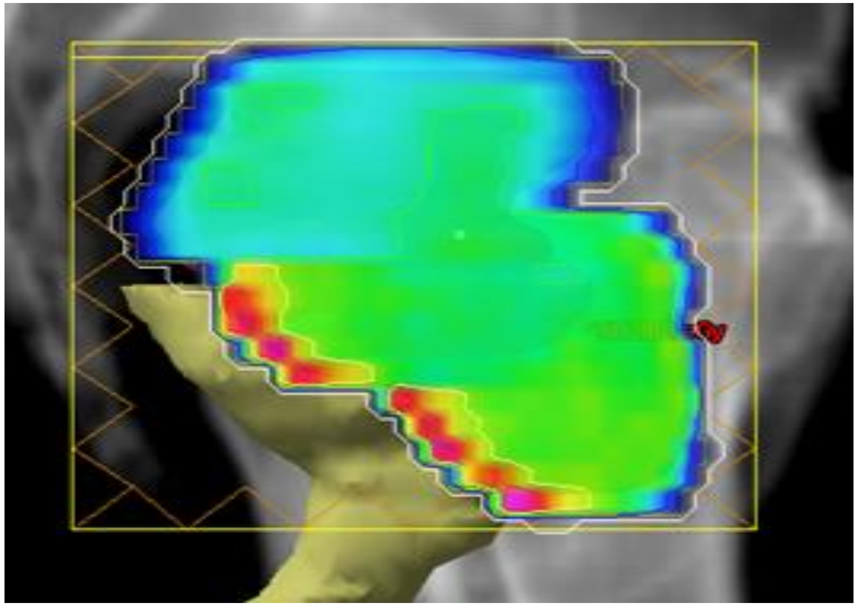


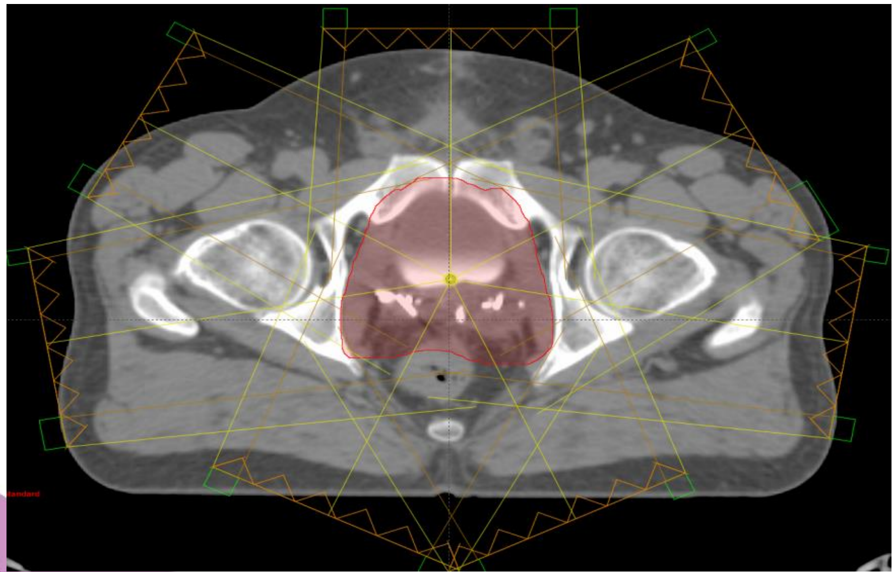
Troubleshooting

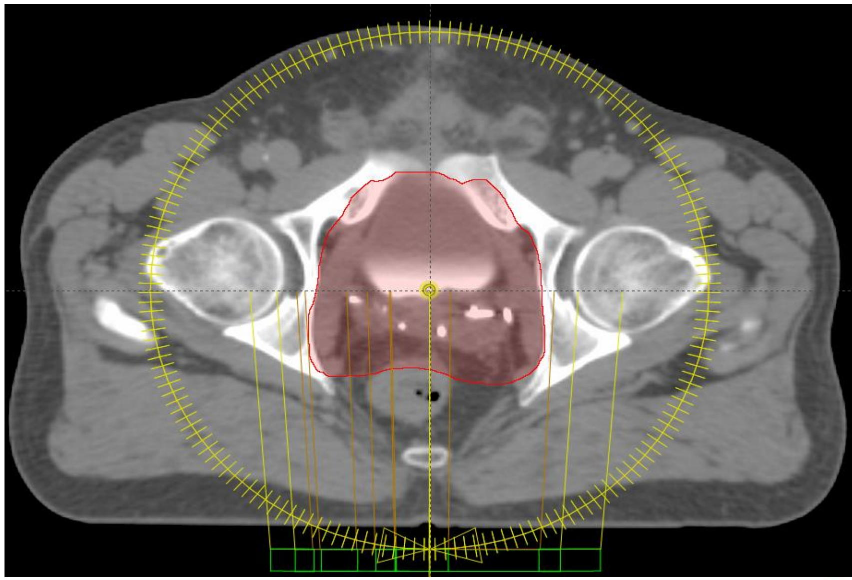
Integrate your planning knowledge –

Clinical Intelligence!





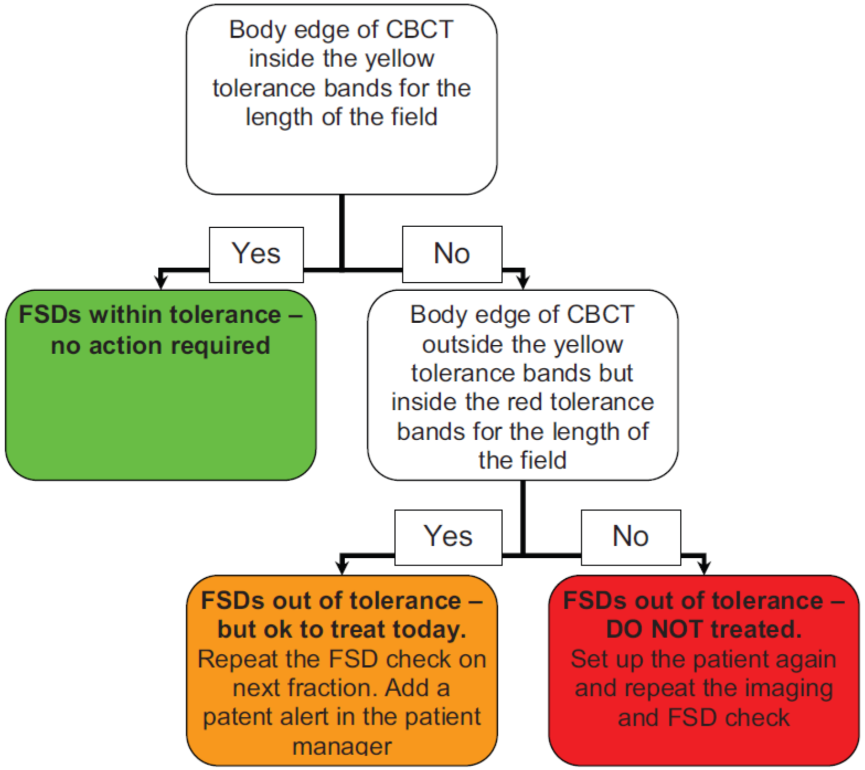




Troubleshooting

- What about when things aren't so clear?! *Troubleshoot*

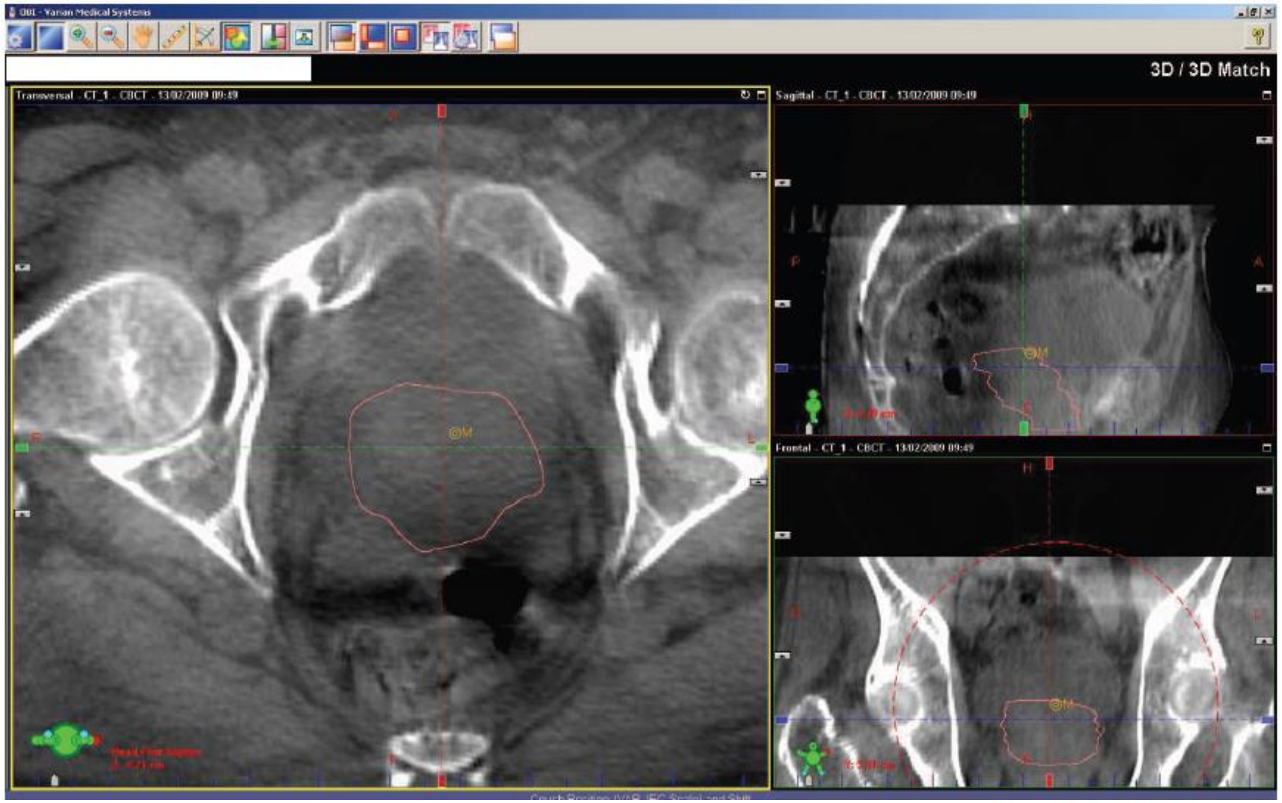
  - ➢ Contour Variation
    - Weight Loss/Gain
    - Shoulder position
      - Neubauer et al 2012



Troubleshooting

- What about when things aren't so clear?! *Troubleshoot*

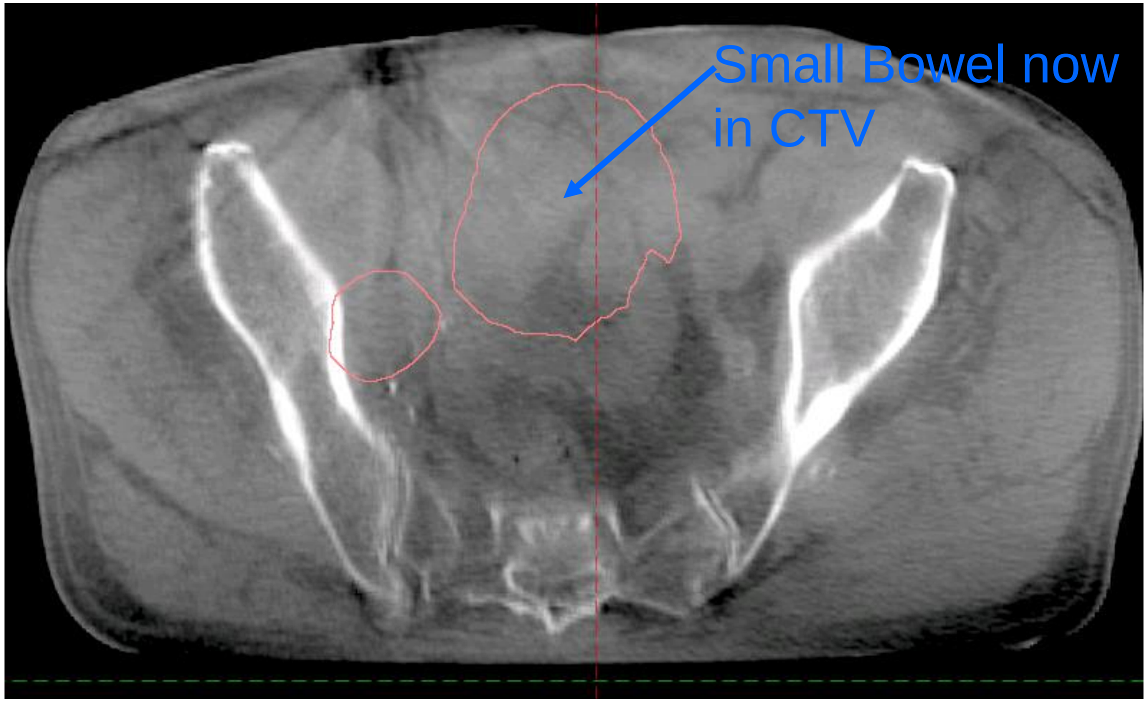
  - Internal organ motion
    - Inter and intrafraction
      - Gas



Troubleshooting

- What about when things aren't so clear?! *Troubleshoot*

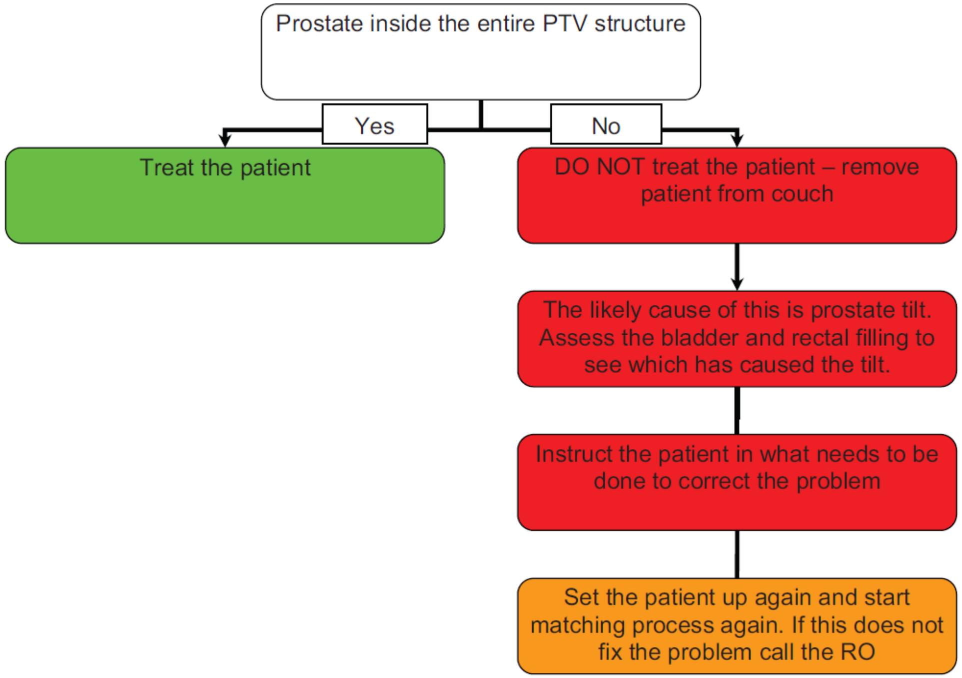
  - Changes in bowel and bladder filling
    - Impact on target position and possibly dose
    - Impact on OAR dose



This is a bladder case, but also applicable to other sites (prostate bed)

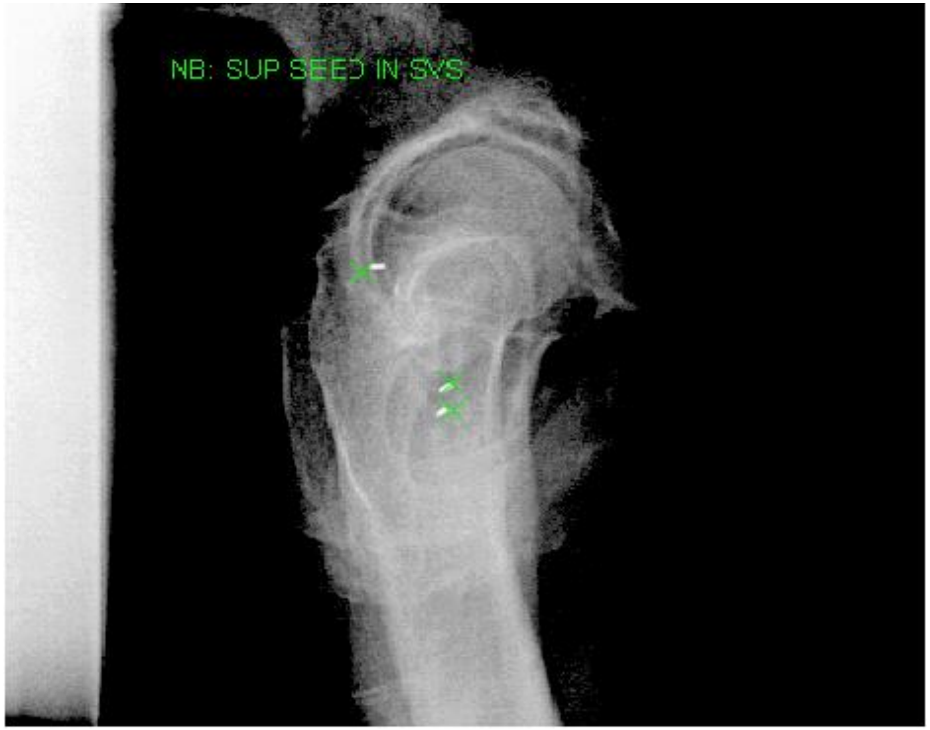
Troubleshooting

- What about when things aren't so clear?! *Troubleshoot*
  - ➢ Displacement of CTV/PTV
    - ▪ Likely cause rotation or tilt
    - ▪ Motion of adjacent structures
    - ▪ Anatomical changes of target



Troubleshooting

- What about when things aren't so clear?! *Troubleshoot*
  - Seed Migration
  - Poorly placed fiducials (SVs, Rectal wall etc)
  - Need to guide the ***system*** here to ensure most appropriate match

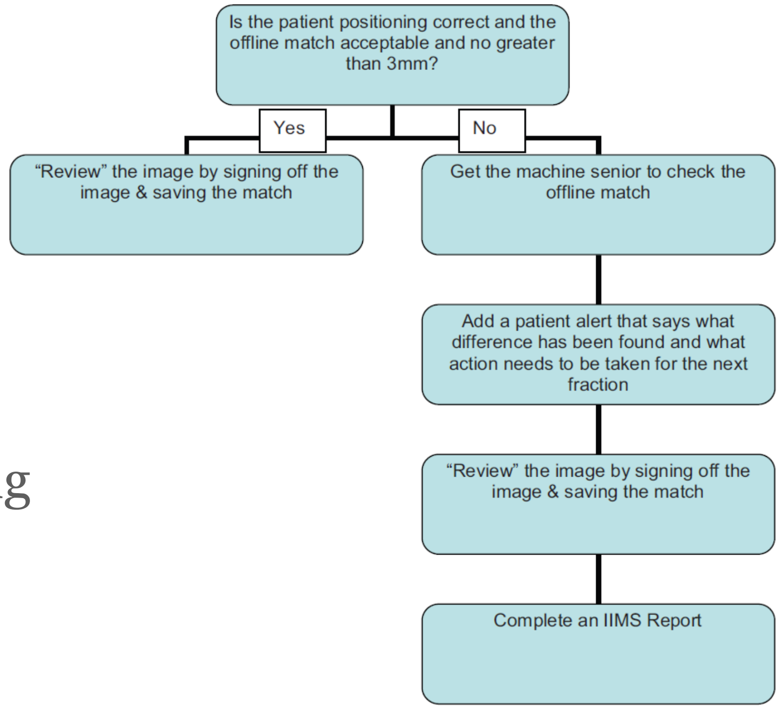


Troubleshooting

- Online IGRT protocols should still include an offline review by an independent party

- This eliminates the time pressures of the machine

  - ➢ RTT on machine
  - ➢ RTT in planning
  - ➢ RO
    - ▪ Can also then feedback to patient
    - ▪ Patient education
  - ➢ Discuss at weekly MDT Audit Meeting



"The therapists are the front-runners for execution of the developed IGRT programs, and the quality of their performance will have a substantial impact on the success of IGRT" *(AAPM Report 104)*

Take Home Message!

- Use your "clinical intelligence"
  - ➢ Don't just automatch and hit apply to whatever the result is.
  - ➢ ***Think!*** Does the match result make sense?

- Dosimetric Impact – Thinking beyond the treatment unit

- Good idea to overlay the planned D95 or D100 isodose line on the CTV position

- Consider what is your target and what is the best surrogate for that

- Include the whole MDT

Acknowledgements

- **Linda Bell**, RTT and IGRT Specialist at Northern Sydney Cancer Centre

Brain

ESTRO School

Jose Lopez, M.D., Ph.D
Radiation Oncology
University Hospital Virgen del Rocio
Seville, Spain

Advanced skills in modern radiotherapy
Prague, Czech Republic –11-15 June 2016

Outline of Talk

- General pearls for Pediatric (CNS) tumors
- Protons
- Case report
- Discussion of current multidisciplinary (physician, phisyc and RTTs) management

Pearls

- The number one cause of death in children is accidents (44%), followed by cancer (10%).

- Of childhood cancers, leukemias are the most common followed by CNS neoplasms (~20%)

- Of pediatric CNS neoplasms, gliomas are most common (lowgrade astrocytomas ~35–50%, brainstem gliomas ~15%, malignant astrocytomas ~10%, optic pathway gliomas ~5%)

Inmovilization

Planning images

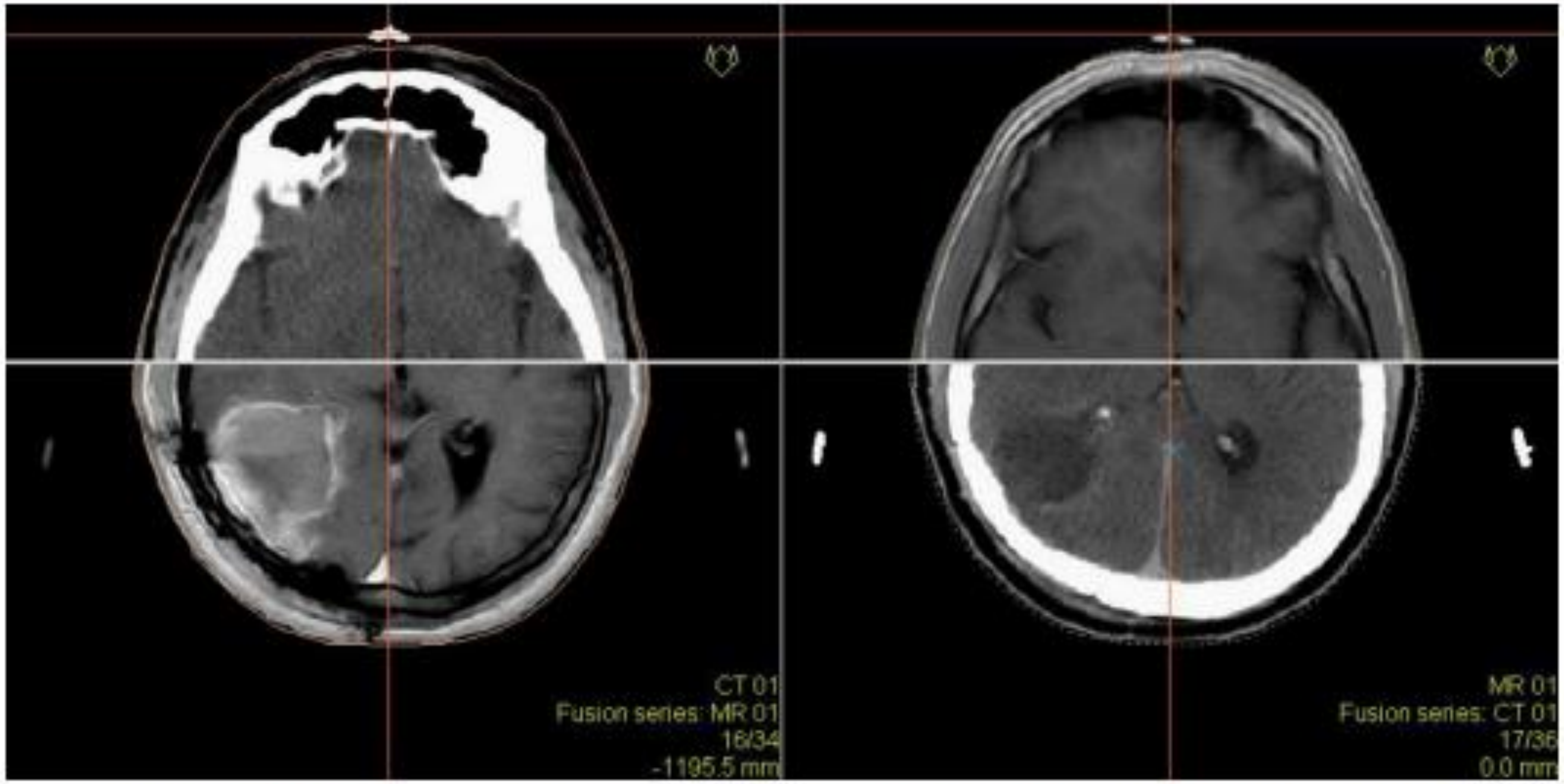
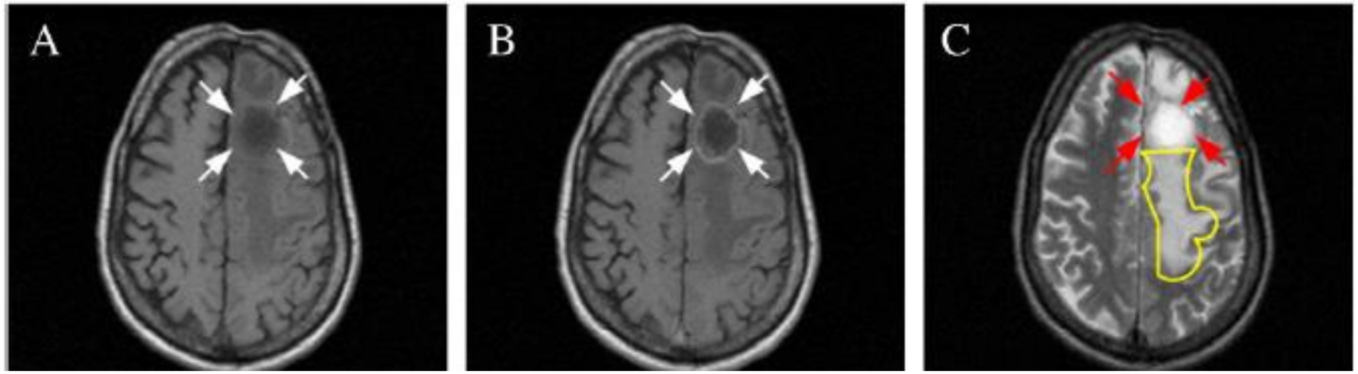


Fig. 2. Image registration of CT and MR image sets. Left image: top (CT), bottom (MR). Right image: top (MR), bottom (CT). The center of the middle fiducial marker pointed out on the left image is shown via registration on the right.

Radiotherapy and Oncology 87 (2008) 100–109



T1 without contrast T1 with contrast T2

Fig. 4. Appearance of astrocytoma tumor on three sequences. (A) Isointense tumor (diffused) on T1-weighted image. (B) Isointense, peripherally enhanced homogeneous tumor on postcontrast T1-weighted image. (C) The tumor is seen as a homogeneous, hyperintense mass on T2-weighted image (in red) as is the edema, which, however, is less bright (in yellow).

T1 hyperintense T1 isointense

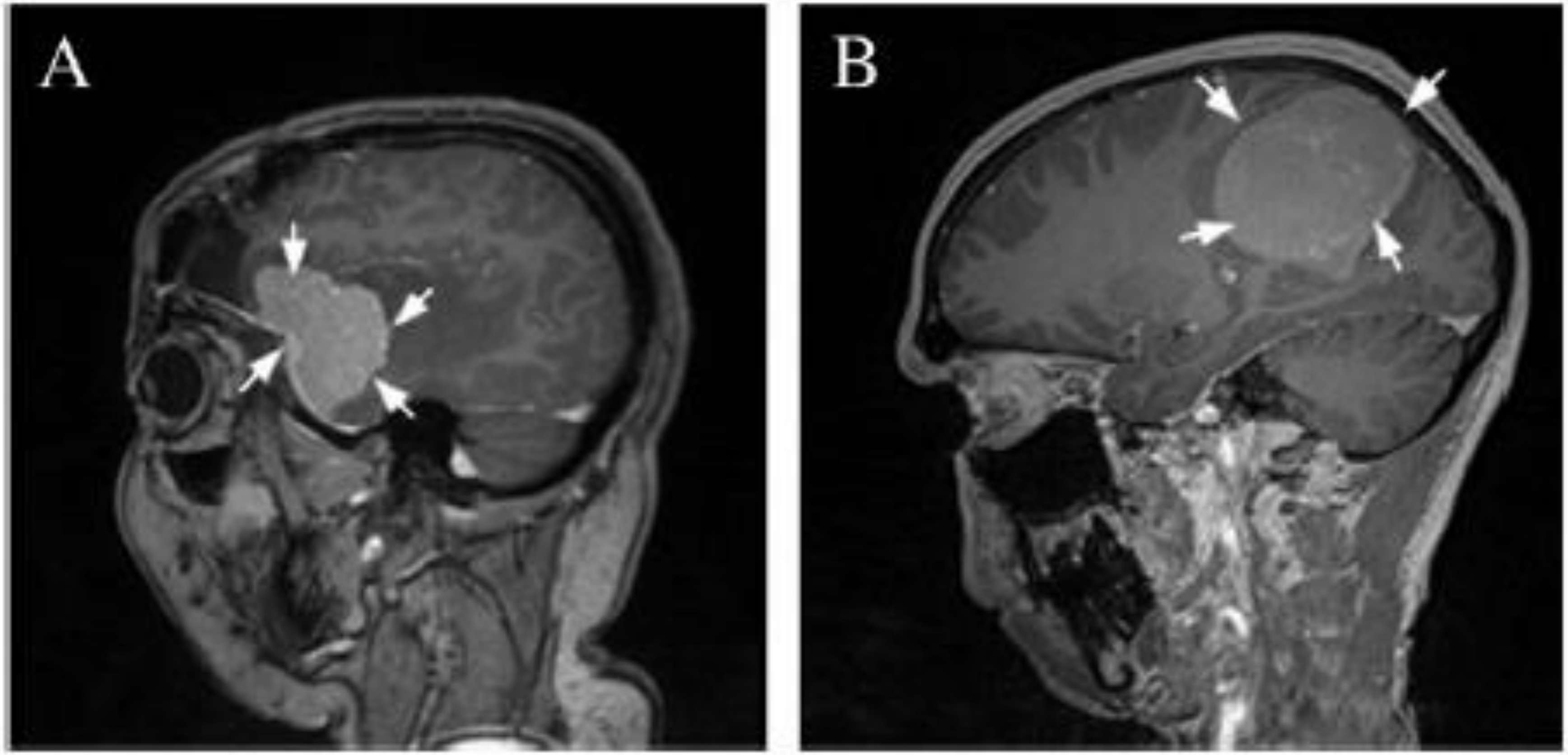


Fig. 2. Degree of enhancement of same tumor (meningioma) of different patients on postcontrast T1-weighted images. (A) Full enhancement of meningioma tumor (hyperintense signal). (B) No enhancement of meningioma tumor (isointense signal).

Homogeneous | Heterogeneous

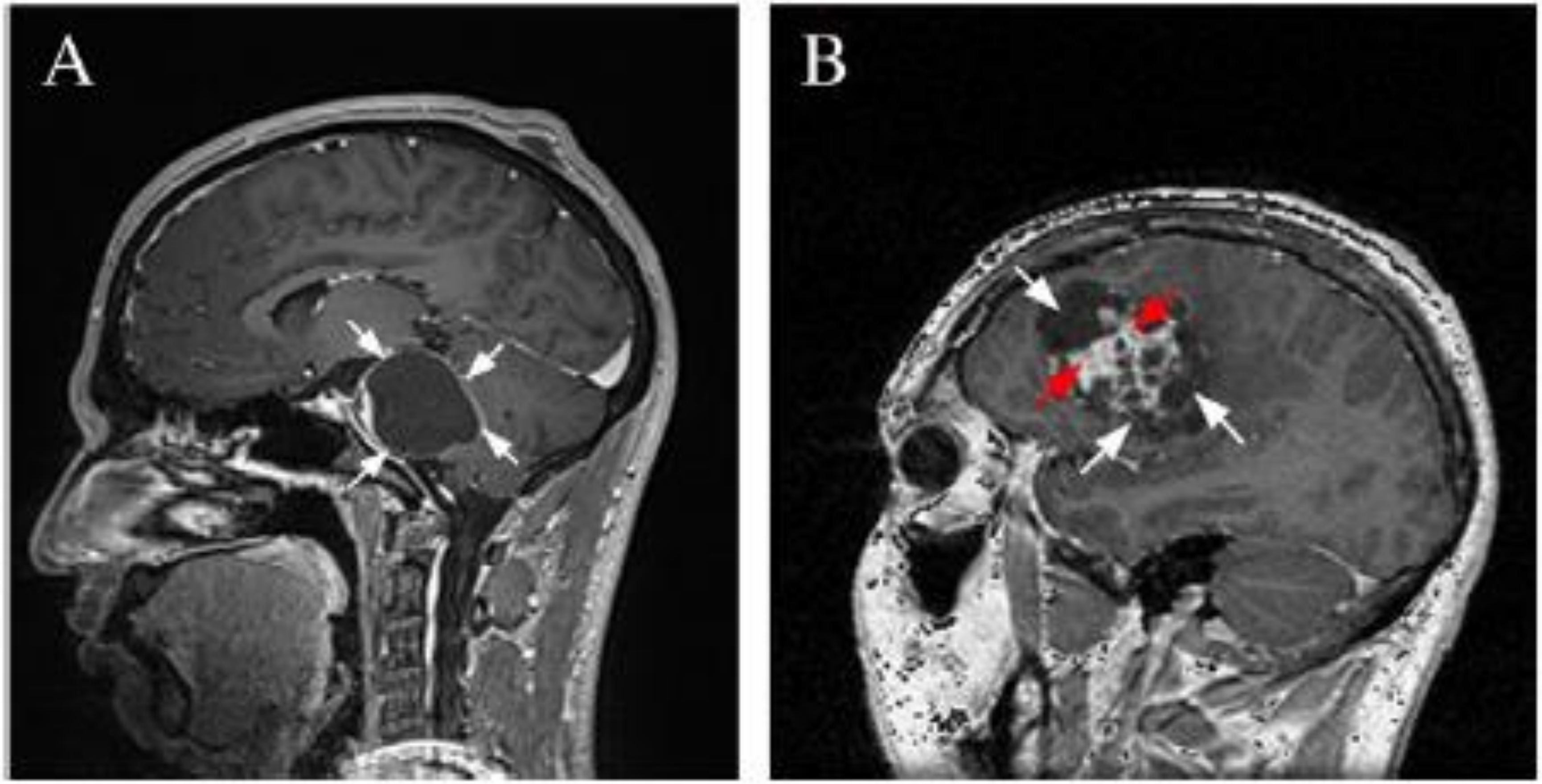


Fig. 3. Homogeneous and heterogeneous tumors. (A) Homogeneous astrocytoma tumor — hypointense signal, peripheral enhancement. (B) Heterogeneous glioma tumor with hypointense necrotic part (in red) and hyperintense-cystic components (in white).

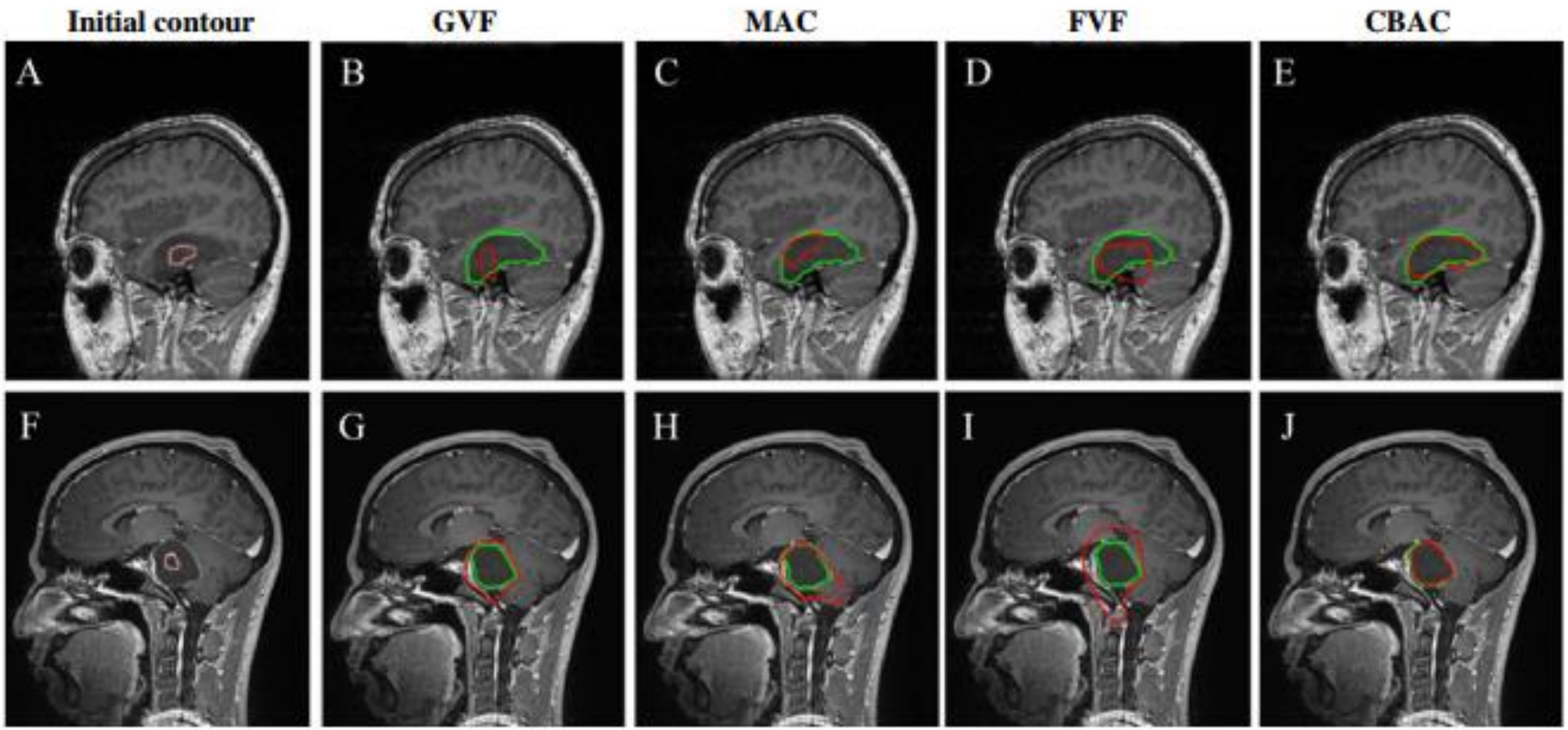
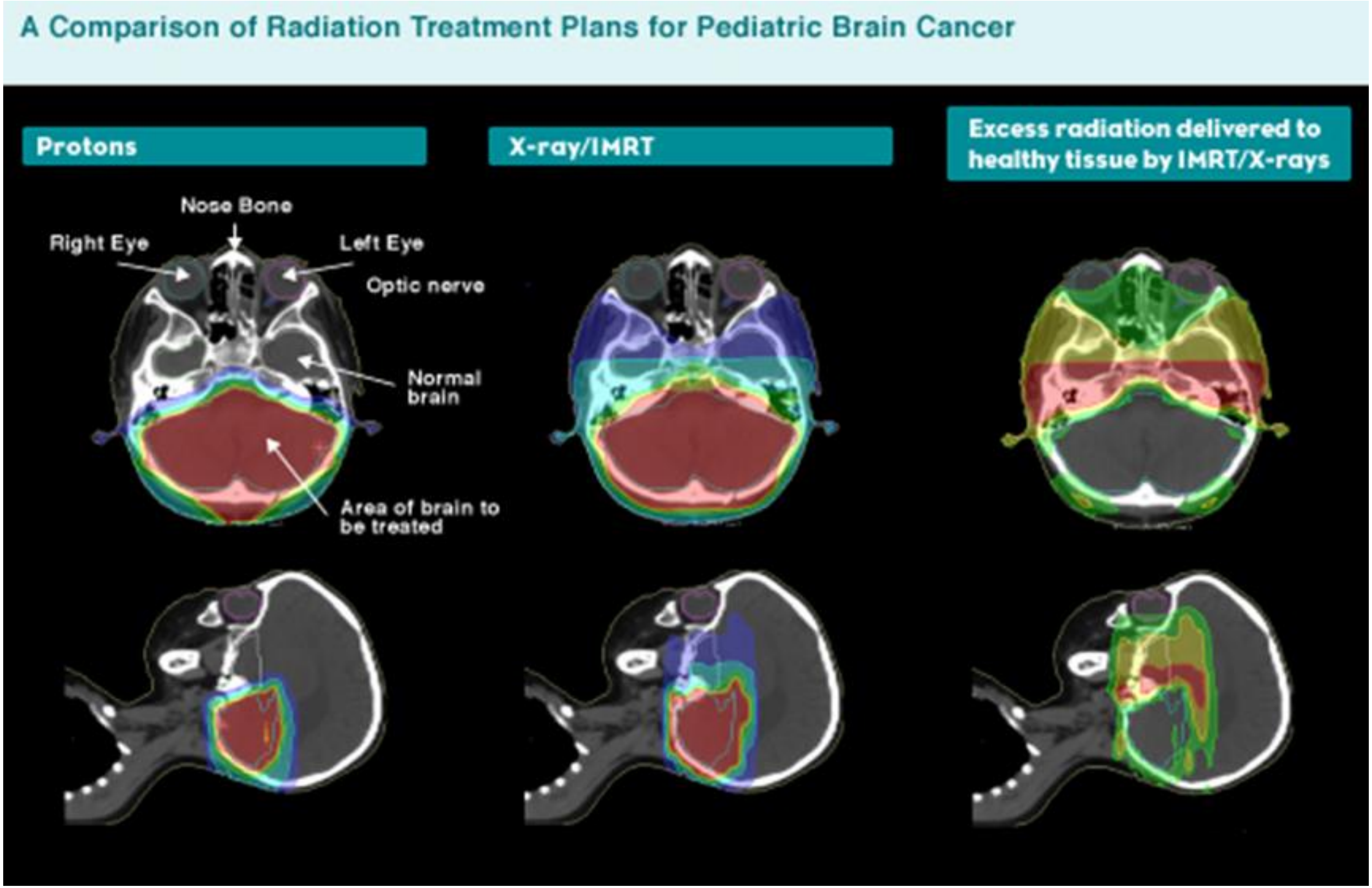


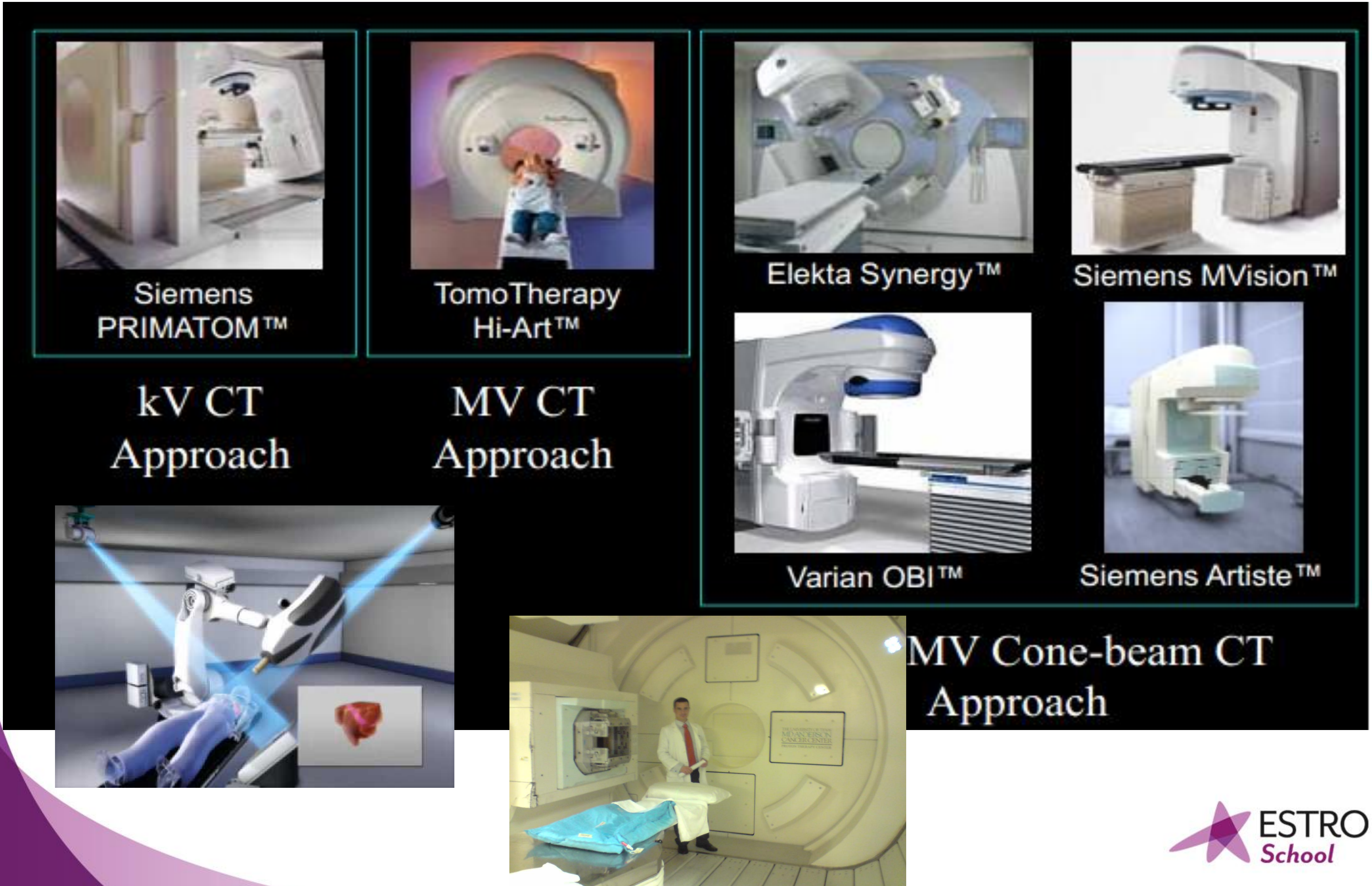
Fig. 10. Comparative segmentation results on postcontrast T1-weighted image. Green — ground truth marked by the radiologist; red — tumor boundary extracted by different methods. Row 1: tumor type, low-grade glioma; appearance, homogeneous tumor with isointense signal; the tumor shows no enhancement. Row 2: tumor type, astrocytoma; appearance, homogeneous tumor with hypointense signal; the tumor shows peripheral enhancement.

Magnetic Resonance Imaging 30 (2012) 694–715



http://www.procure.com/ForMedicalProfessionals/ClinicalIndications.aspx

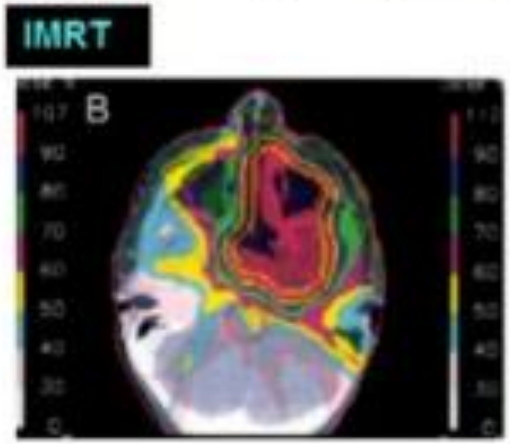
Technologies

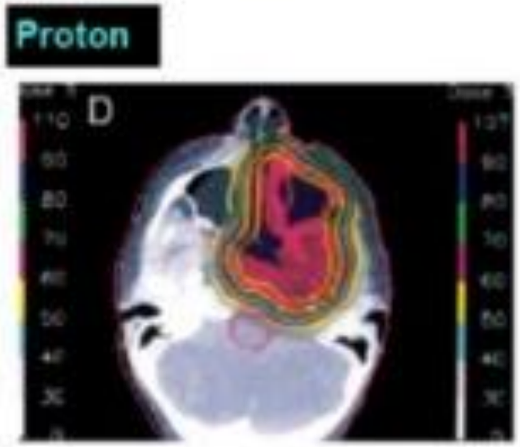


Proton Therapy

Claims:

- Opportunity to treat previously untreatable disease because of challenging geometry
  - ➢ Concave CTV/PTV partially surrounding a convex OAR





- Second cancer reduction

CLINICAL INVESTIGATION — Pediatric Tumors

POTENTIAL REDUCTION OF THE INCIDENCE OF RADIATION-INDUCED SECOND CANCERS BY USING PROTON BEAMS IN THE TREATMENT OF PEDIATRIC TUMORS

Raymond Miralbell, M.D.,* Antony Lomax, Ph.D.,† Laura Cella, M.Sc.,* and Uwe Schneider, Ph.D.†

Controversies of cost-effectiveness with new technologies, e.g. protons

American Cancer Society

Is proton beam therapy for prostate cancer worth the cost?

February 20, 2013

By Durado Brooks, MD, MPH

Proton therapy popular and profitable

The lack of evidence has not slowed the rapid increase in the use of proton treatment for prostate cancer. One recent study documented a 67% increase in the number of cases of proton treatment for prostate cancer billed to Medicare between 2006 and 2009. This rate of growth is particularly noteworthy given the limited access to proton therapy: there are at present only 10 proton beam centers operating in the United States, and each center treats only a few hundred cancer patients each year.

- Cost of proton therapy nearly double compared to IMRT
- Benefit of proton therapy in prostate cancer is unproven
  - Neither better tumor control nor lower toxicity
    - A few studies suggest that toxicity rates might even be higher

pace? Financial incentives may be playing a role. Proton beam therapy for prostate cancer is reimbursed at a much higher rate than traditional radiation treatment for the same condition. Medicare pays about $19,000 for a full dose of standard radiation therapy for prostate cancer, but it pays nearly double for proton therapy - more than $32,000.

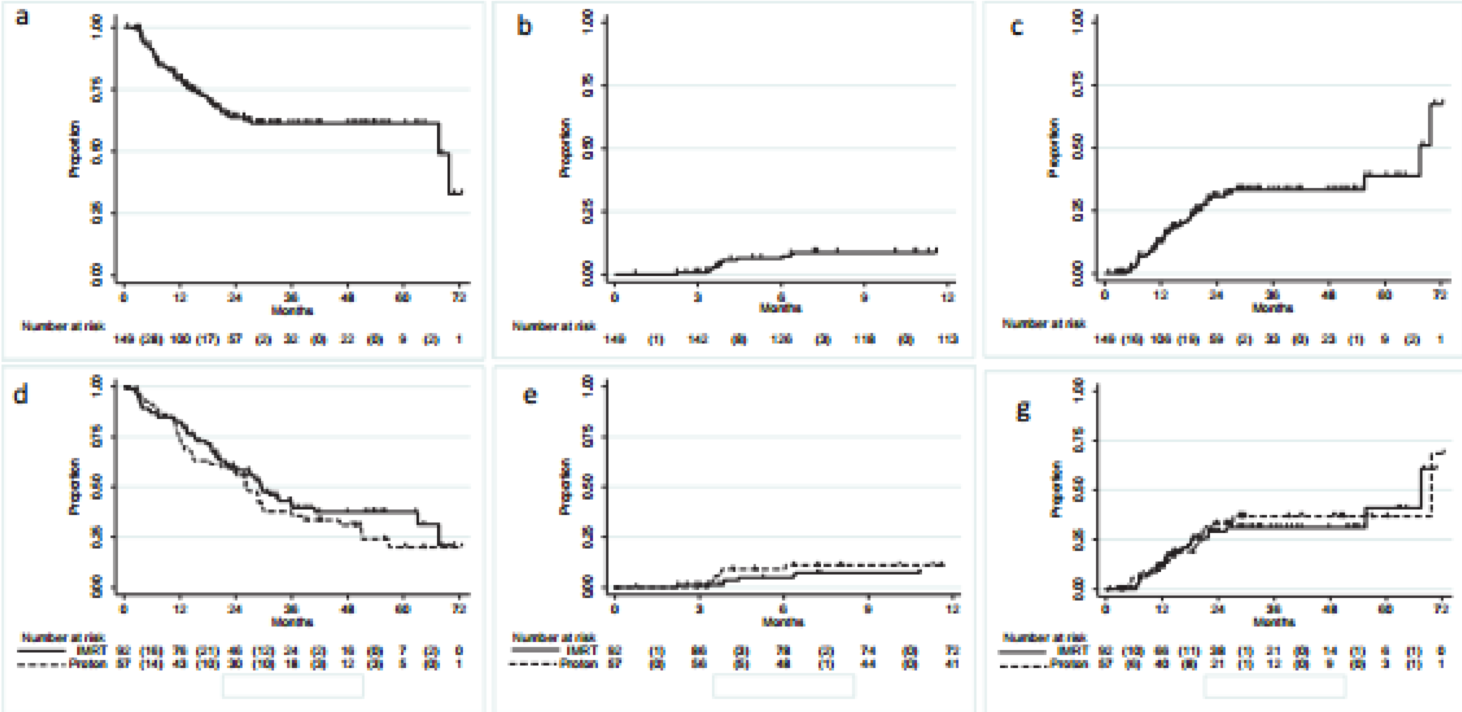


Figure 2. Time to treatment failure defined as 1) grade ≥ 3 RP, 2) Local recurrence as first occurence in randomised patients. Upper panels show the time to the development of (a) combined treatment failure, (b) grade ≥ 3 RP, and (c) local recurrence as a whole group. Lower panels shox the comparison between IMRT (solid) vs. 3D-PBT (dashed) in time to the development of (d) combined treatment failure, (e) grade ≥ 3 RP, and (g) local recurrence.

Lung cancer
Photons vs protons
Phase III
MDA

ESTRO 35

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International Journal of
Radiation Oncology
biology • physics

www.redjournal.org

Vol. 87, No. 1, pp. 46-52, 2013

Clinical Investigation: Late Effect

Incidence of Second Malignancies Among Patients Treated With Proton Versus Photon Radiation

Christine S. Chung, MD, MPH,* Torunn I. Yock, MD, MCh,† Kerrie Nelson, PhD,‡ Yang Xu, MS,‡ Nancy L. Keating, MD, MPH,§,* and Nancy J. Tarbell, MD†,||

- Conflicting hypotheses:
  - ➢ whether proton radiation has less risk than photon therapy
    - scattering with photons vs neutron contamination with protons
- 558 proton pts treated from 1973 to 2001 Harvard cyclotron vs 558 matched photon pts from SEER
- Second Ca: 29 protons (5.2%) and 42 Photons (7.5%)
- No evidence for or against (adjusted for age at treatment, sex, site, year diagnosed)

A systematic literature review of the clinical and cost-effectiveness of hadron therapy in cancer

Mark Lodge[a,*], Madelon Pijls-Johannesma[b], Lisa Stirk[c], Alastair J. Munro[d], Dirk De Ruysscher[b,e], Tom Jefferson[a]

[a]Cochrane Cancer Network, Oxford, UK, [b]MAASTRO Clinic, Maastricht, The Netherlands, [c]Centre for Reviews & Dissemination, University of York, UK, [d]University of Dundee, Scotland, UK, [e]University Hospital Maastricht, GROW, MAASTRO Clinic, Maastricht, The Netherlands

Table 1

Results literature review in comparison with conventional therapy classified by tumour site

Tumour site	Protons		Ions	
	n studies/*N*	Result	*n* studies/*N*	Result
Head and neck	2/62	No firm conclusions	2/65	Similar to protons
ACC (locally advanced)	—	—	1/29	Superior
Prostate cancer	3/1751	Similar	4/201	No firm conclusions
Ocular tumours	10/7708	Superior	2/1343	Similar to protons
Gastro-intestinal cancer	5/369	No firm conclusions	2/73	No firm conclusions
Lung cancer (non-small cell)	3/156	No firm conclusions	3/205	Similar to SRT
CNS[a]	10/839	Similar	3/405	Similar to protons
Chordomas of skull base	3/302	Superior	2/107	Similar to protons
Sarcoma's	1/47	No firm conclusions	1/57	No firm conclusions
Pelvic tumours	3/80	No firm conclusions	2/49	No firm conclusions

Abbreviations: *N*, number of patients; ACC, adenoid cystic carcinomas; SRT, stereotactic radiotherapy.

[a] CNS, central nerve system tumours; inclusive skull base, spinal cord chondroma and chondrosarcomas.

- Brada et al. (JCO 2008) concluded that there is insufficient evidence at the present to recommend the use of proton therapy in any disease sites
- Reviewers / Authors have different views as to what constitutes evidence

Radiotherapy and Oncology 103 (2012) 8–11

Contents lists available at SciVerse ScienceDirect

Radiotherapy and Oncology

journal homepage: www.thegreenjournal.com

Systematic review

An evidence based review of proton beam therapy: The report of ASTRO's emerging technology committee

Aaron M. Allen[a,*], Todd Pawlicki[b], Lei Dong[c], Eugene Fourkal[d], Mark Buyyounouski[d], Keith Cengel[e], John Plastaras[e], Mary K. Bucci[c], Torunn I. Yock[f], Luisa Bonilla[a], Robert Price[d], Eleanor E. Harris[g], Andre A. Konski[h]

- In pediatric CNS malignancies PBT appears superior to photon approaches but more data is needed.
- In large ocular melanomas and chordomas, we believe that there is evidence for a benefit of PBT over photon approaches.
- PBT is an important new technology in radiotherapy
  - Current evidence provides a limited indication for PBT
  - More robust prospective clinical trials are needed to determine the appropriate clinical setting for PBT

Essen, Germany
Berlin, Germany
Uppsala, Sweden
Munich, Germany
St. Petersburg, Russia
Vancouver, Canada
Dubna, Russia
Clatterbridge, England
Moscow, Russia
San Francisco, CA
Heidelberg, Germany
Austron, Austria
Seoul, South Korea
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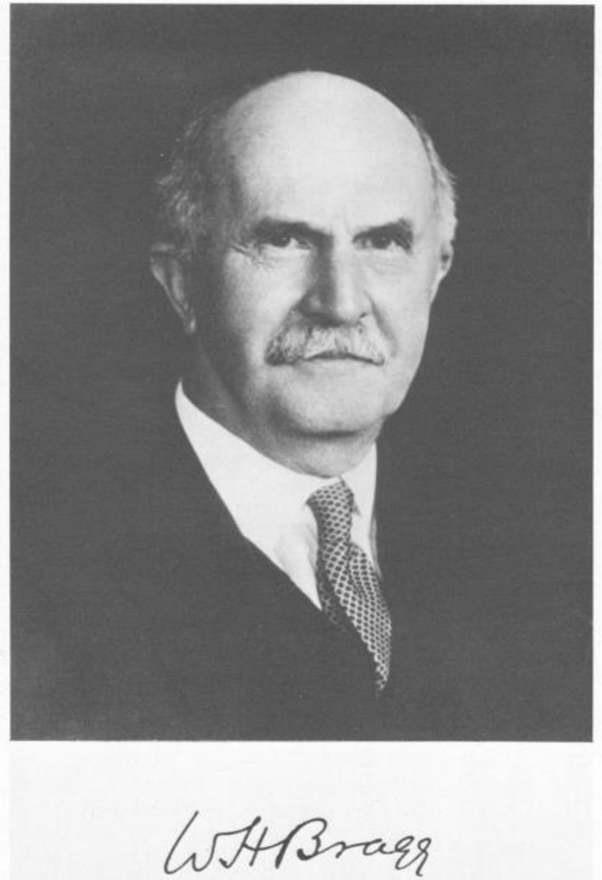
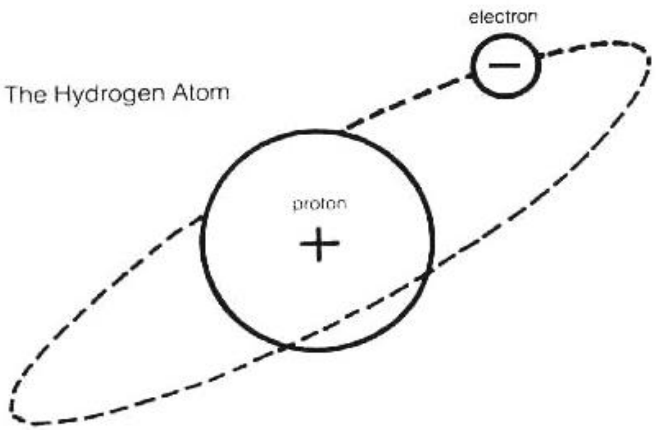
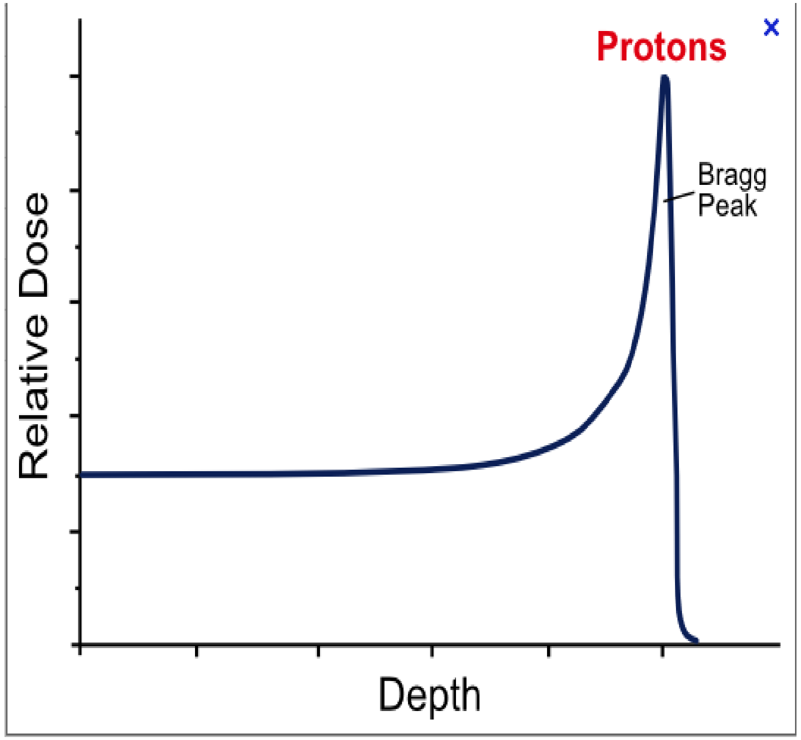
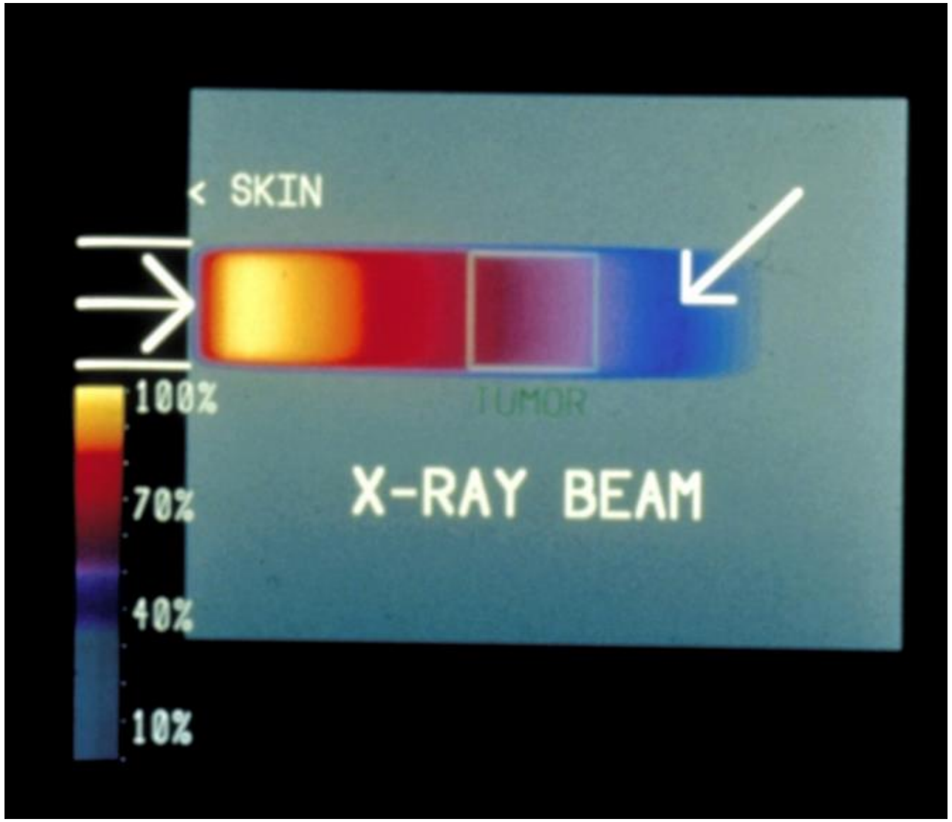
Tsukuba, Japan
Boston, MA
Chiba, Japan
Koeln, Germany
Trento, Italy
Zibo, China
Bloomington, IN
Kashiwa, Japan
Catania, Italy
Loma Linda, CA
Villigen, Switzerland
Milan, Italy
Shuzuoka, Japan
Orsay, France
Houston, TX
Jacksonville, FL
Nice, France
Hyogo, Japan
Gauteng, South Africa
Western Cape, South Africa
Physics research-based facility
Medical facility
Planned or under construction

BRAGG PEAK

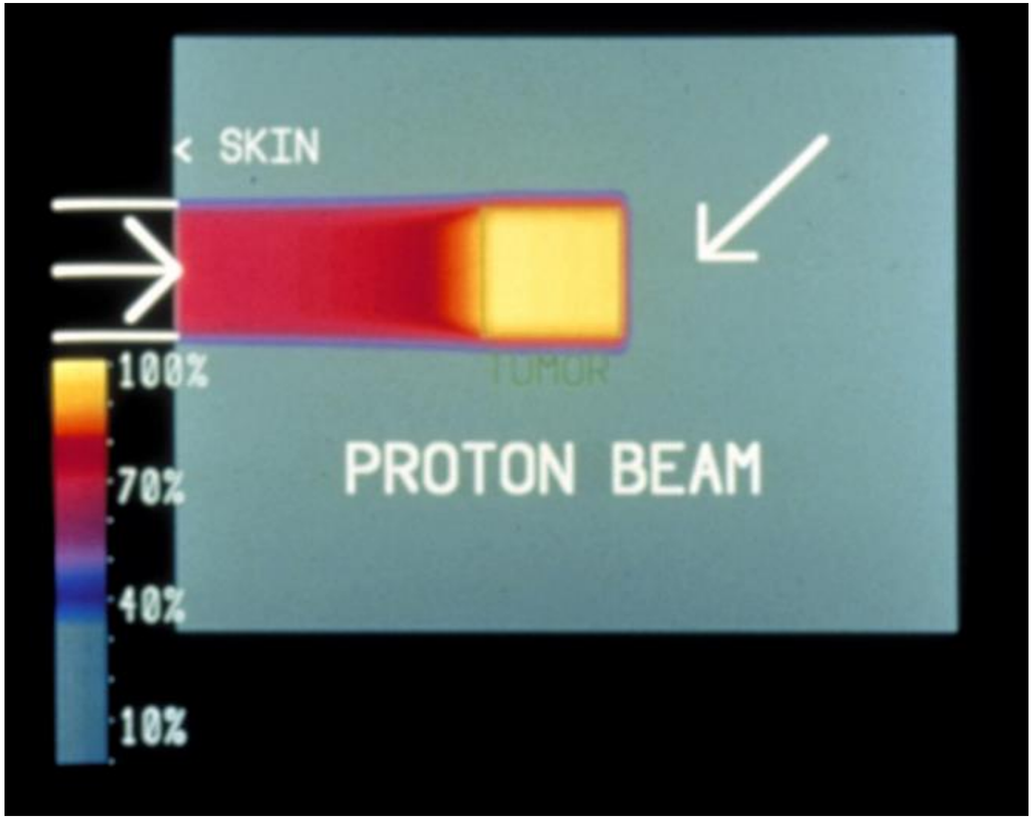



The Hydrogen Atom
electron
proton


Protons
Bragg Peak
Relative Dose
Depth



< SKIN
100%
TUMOR
70%
X-RAY BEAM
40%
10%



< SKIN
100%
TUMOR
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PROTON BEAM
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10%


2460
2575
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2460
2575
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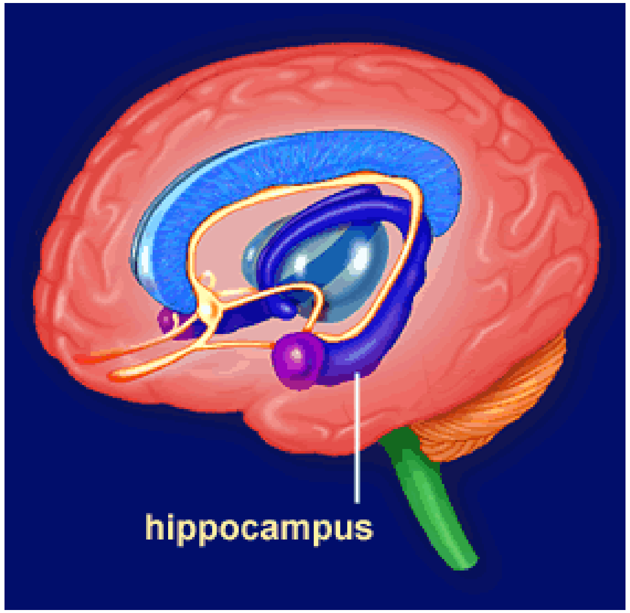
2225
2000


PH H-F

PTC

Association between hippocampal dosimetry and impairment in Wechsler Memory Scale-III Word Lists Delayed Recall at 18 months

Dosimetry	Dosimetric cut point	No impairment	Impairment*	*p* value
Bilateral hippocampi				
Maximum	≤24.7 Gy	66.7%	33.3%	0.500
	>24.7 Gy	55.6%	44.4%	
D30%	≤8.2 Gy	77.8%	22.2%	0.167
	>8.2 Gy	44.4%	55.6%	
D40%	≤7.3 Gy	88.9%	11.1%	0.025
	>7.3 Gy	33.3%	66.7%	
D50%	≤3.8 Gy	66.7%	33.3%	0.500
	>3.8 Gy	55.6%	44.4%	
D80%	≤0.5 Gy	55.6%	44.4%	0.500
	>0.5 Gy	66.7%	33.3%	
D100%	≤0.0 Gy	76.9%	23.1%	0.047
	>0.0 Gy	20.0%	80.0%	
Left hippocampus				
Maximum	≤15.0 Gy	55.6%	44.4%	0.500
	>15.0 Gy	66.7%	33.3%	



Int J Radiat Oncol Biol Phys. 2012 Jul 15;83(4):e487-93.

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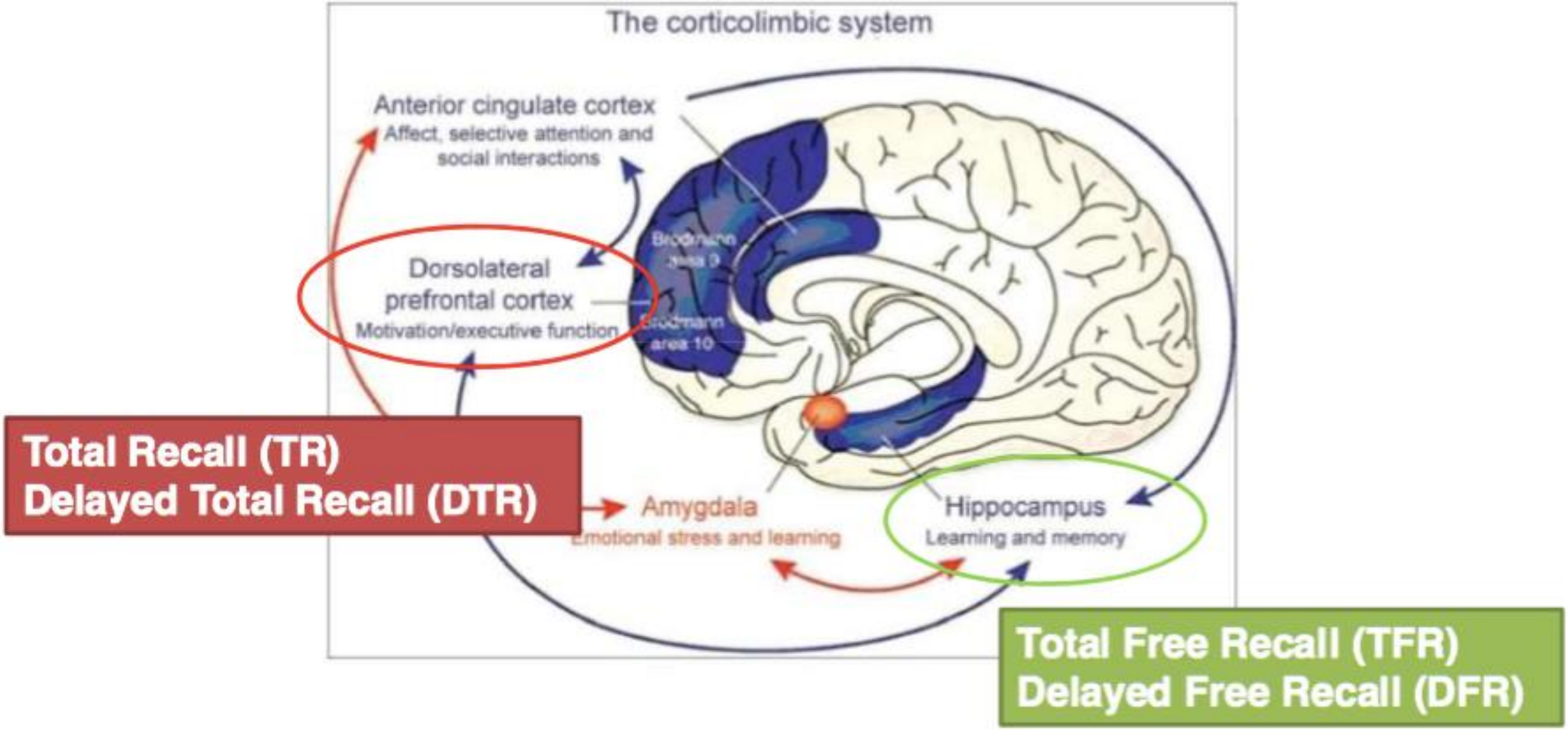
The corticolimbic system
Anterior cingulate cortex
Affect, selective attention and social interactions
Dorsolateral prefrontal cortex
Motivation/executive function
Amygdala
Emotional stress and learning
Hippocampus
Learning and memory
Total Recall (TR)
Delayed Total Recall (DTR)
Total Free Recall (TFR)
Delayed Free Recall (DFR)

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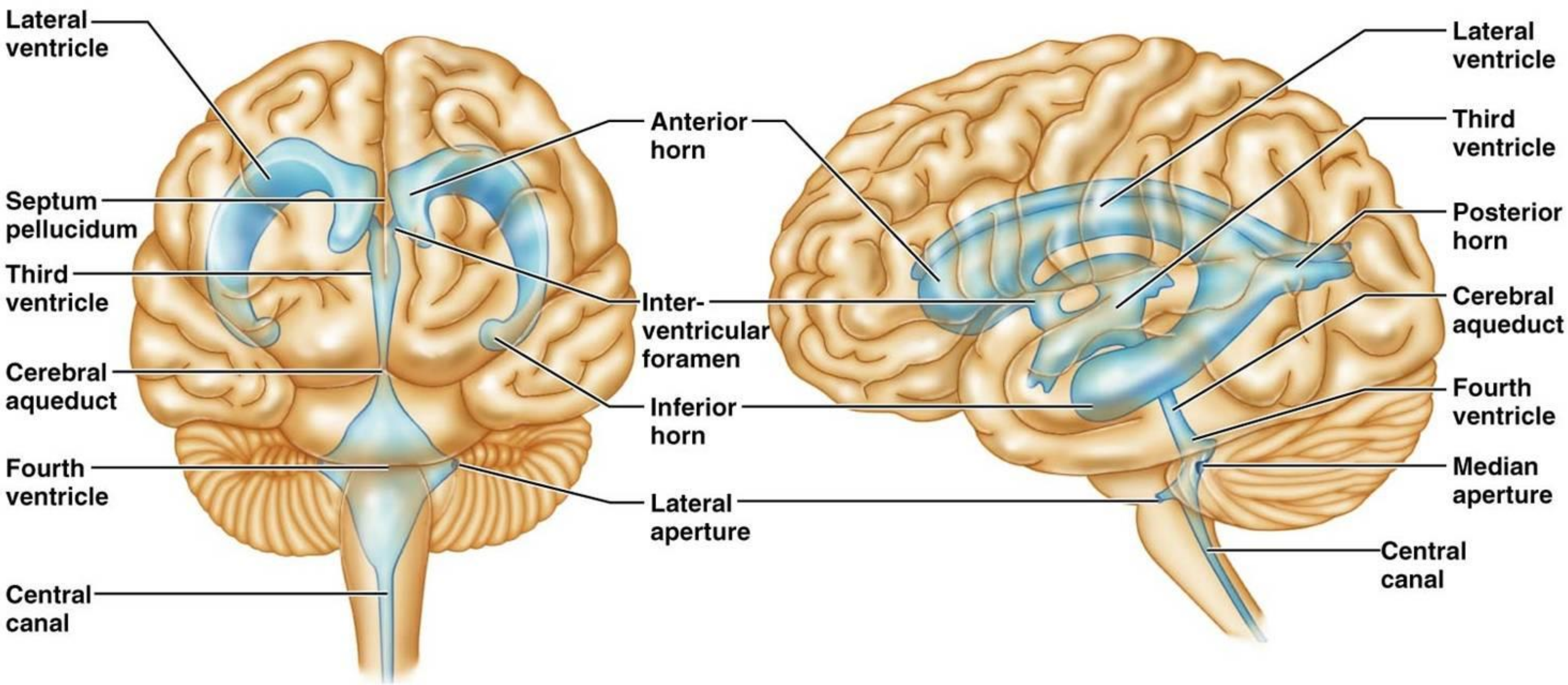
	FIRST TIME	TOTAL FREE RECALL (TFR)	FREE RECALL (TR)	DELAYED FREE RECALL (DFR)	DELAYED T. RECALL (DTR)
BASAL-3					
PCI	2 (6,7%)	4 (13,3%)	7 (23,3%)	8 (26,7%)	8 (26,7%)
Hippocampal sparing	4 (13,3%)	2 (6,7%)	3 (10%)	1 (3,3%)	5 (16,7%)
	NS	NS	NS	**0,01 RR 8 [1,06- 60,08]**	NS
BASAL-6					
PCI	11 (40,7%)	9 (33,3%)	14 (51,9%)	13 (48,1%)	14 (51,9%)
Hippocampal sparing	3 (14,3%)	1(4,8%)	3 (14,3%)	1 (4,8%)	5 (23,8%)
	0,06 RR 2,8 [0,9- 8,9]	**0,01 RR 7 [0,9- 50,9]**	**0,01 RR 3,6 [1,19- 11,0]**	**0,001 RR 10 [1,4- 71,23]**	0,07 RR 2,1 [0,9- 5,08]

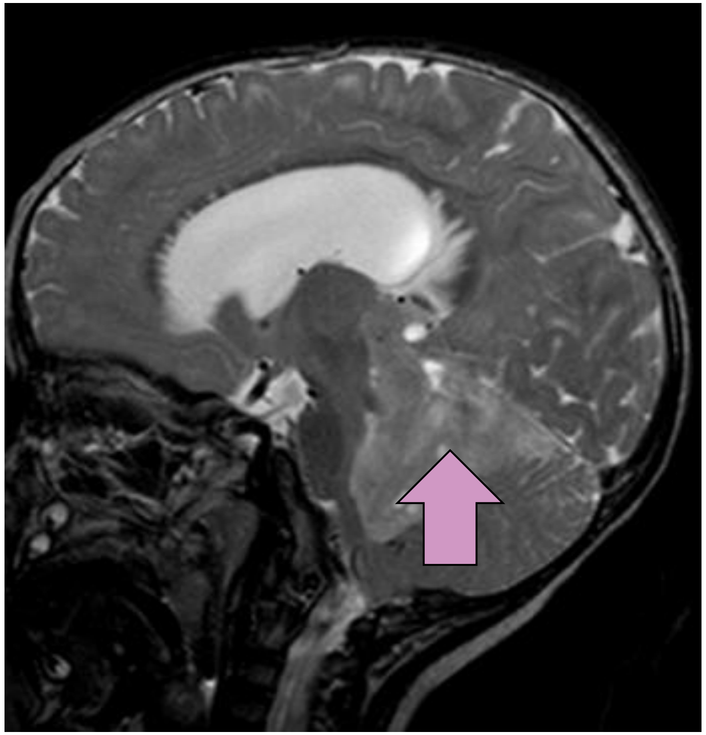
Case 1: patient with teratoid rhabdoid tumor

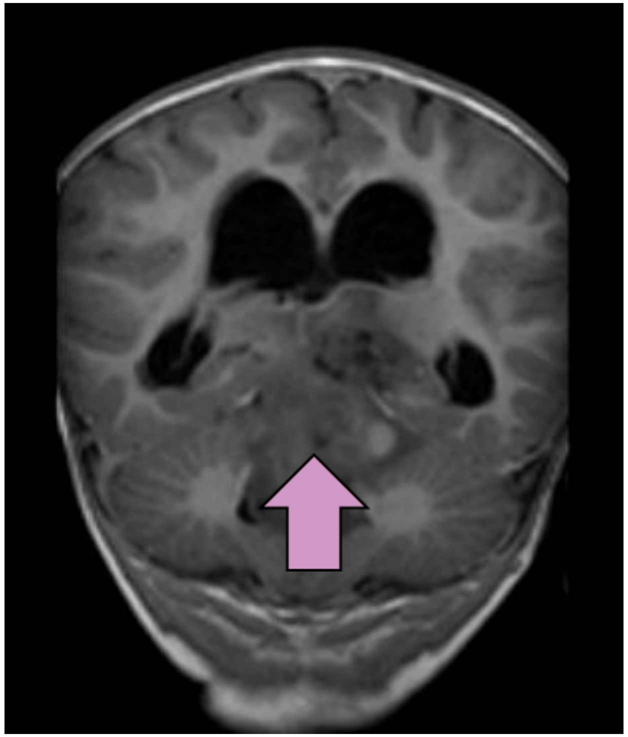
- A 19-month-old female infant was referred because of headache and weakness
- Magnetic resonance imaging revealed a mass that occupied the fourth ventricle

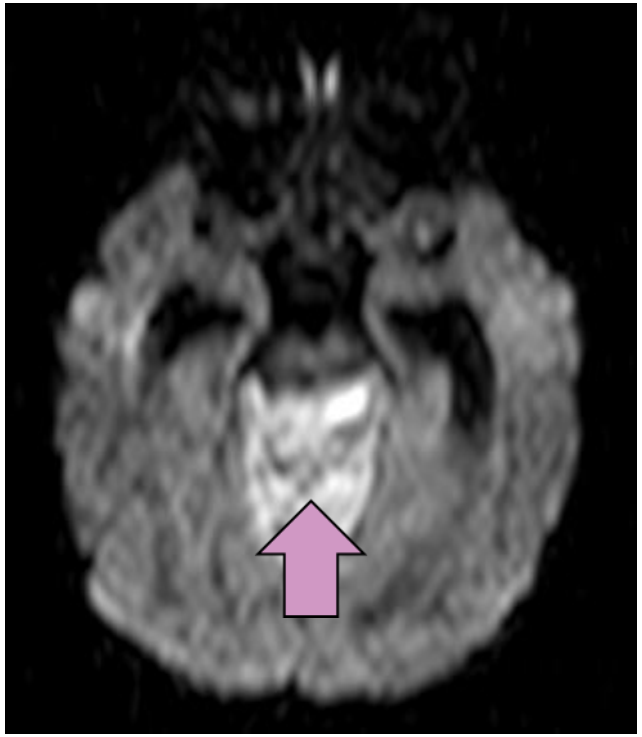


(a) Anterior view **(b) Left lateral view**

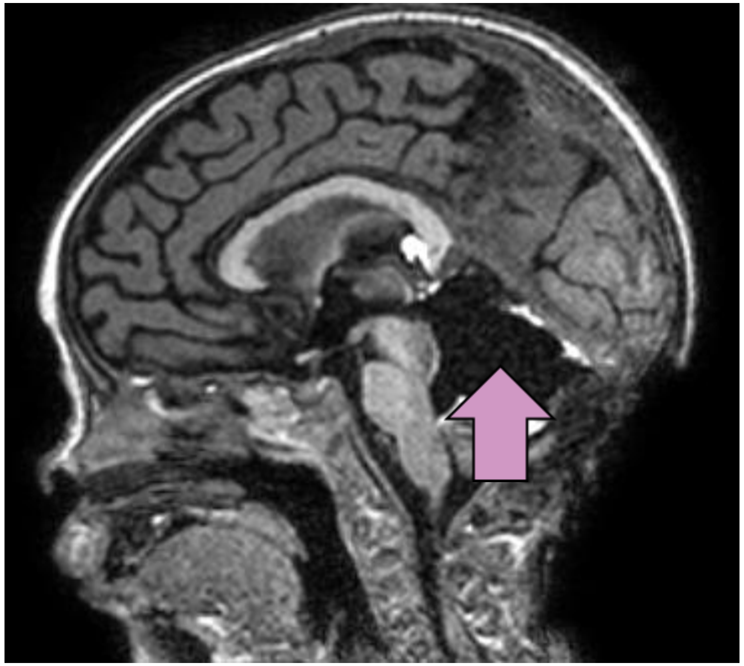
Mass at the fourth ventricle

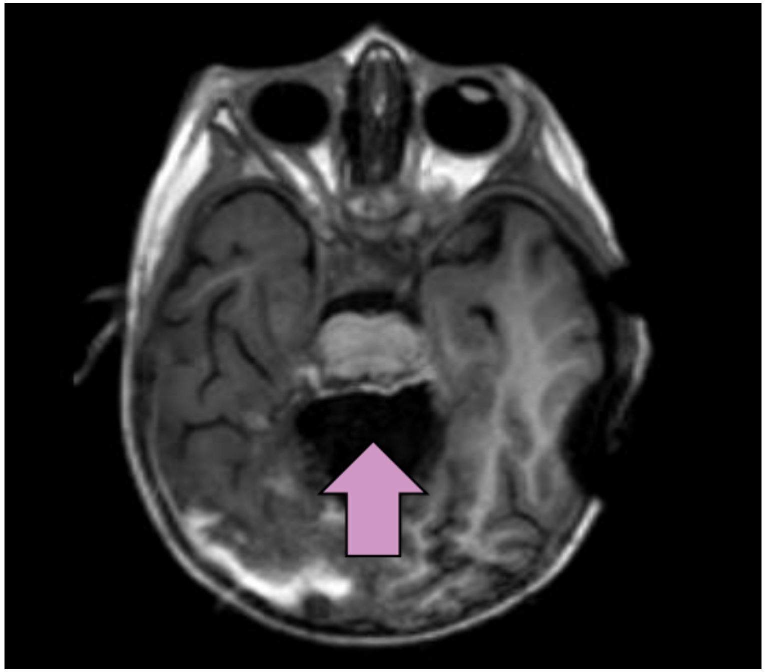






- The child underwent total removal of the tumor mass





- Pathological findings showed an **atypical teratoid/rhabdoid tumor**

- Diagnosis

- Atypical teratoid/rhabdoid tumor

- Treatment

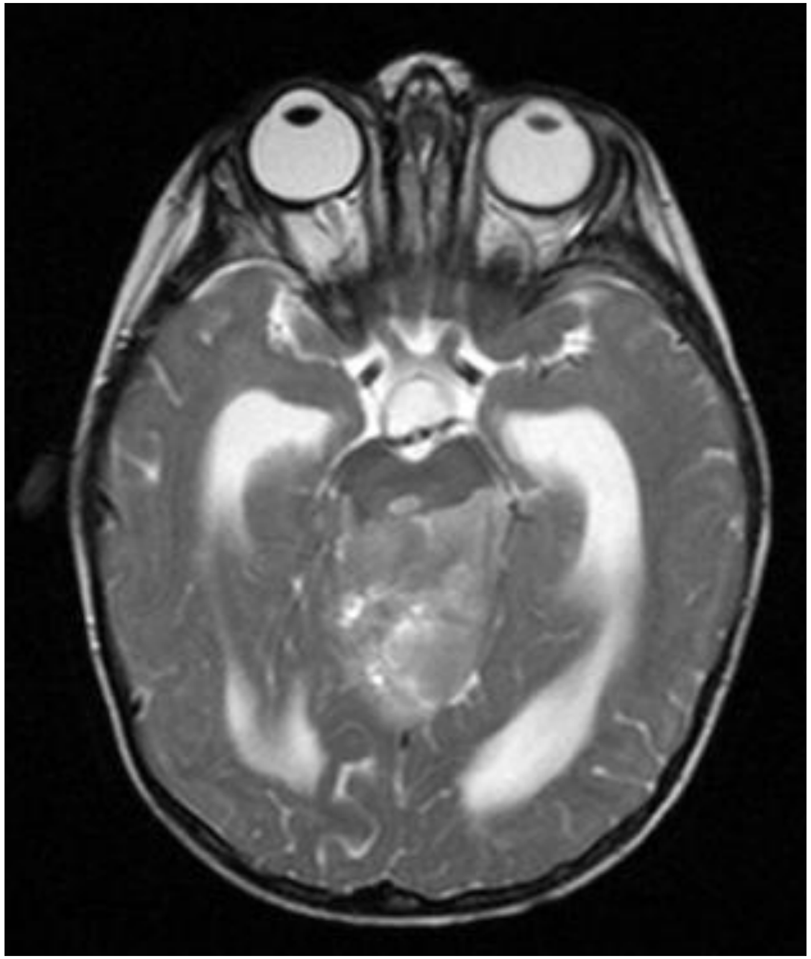
- Chemotherapy + Surgery + Radiation Therapy

- Radiation Therapy Dose Prescription:

- PTV (surgical bed + 5mm margin): 54 Gy at 2 Gy/fraction

- **Organ at risk**

  Whole brain
  Braim stem
  Chiasm
  Pituitary
  Eyes
  Crystalline lens
  Nerve optic



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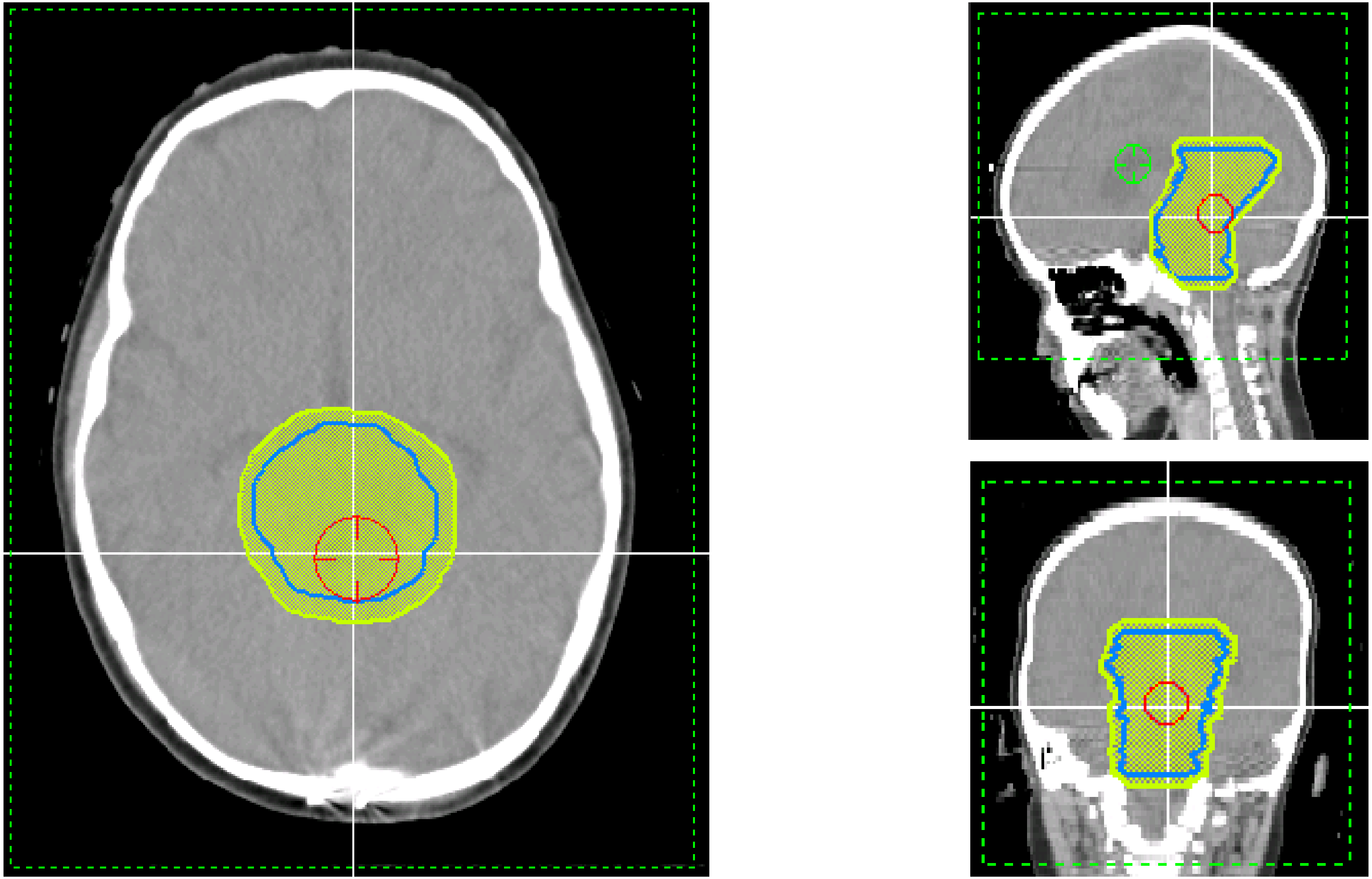
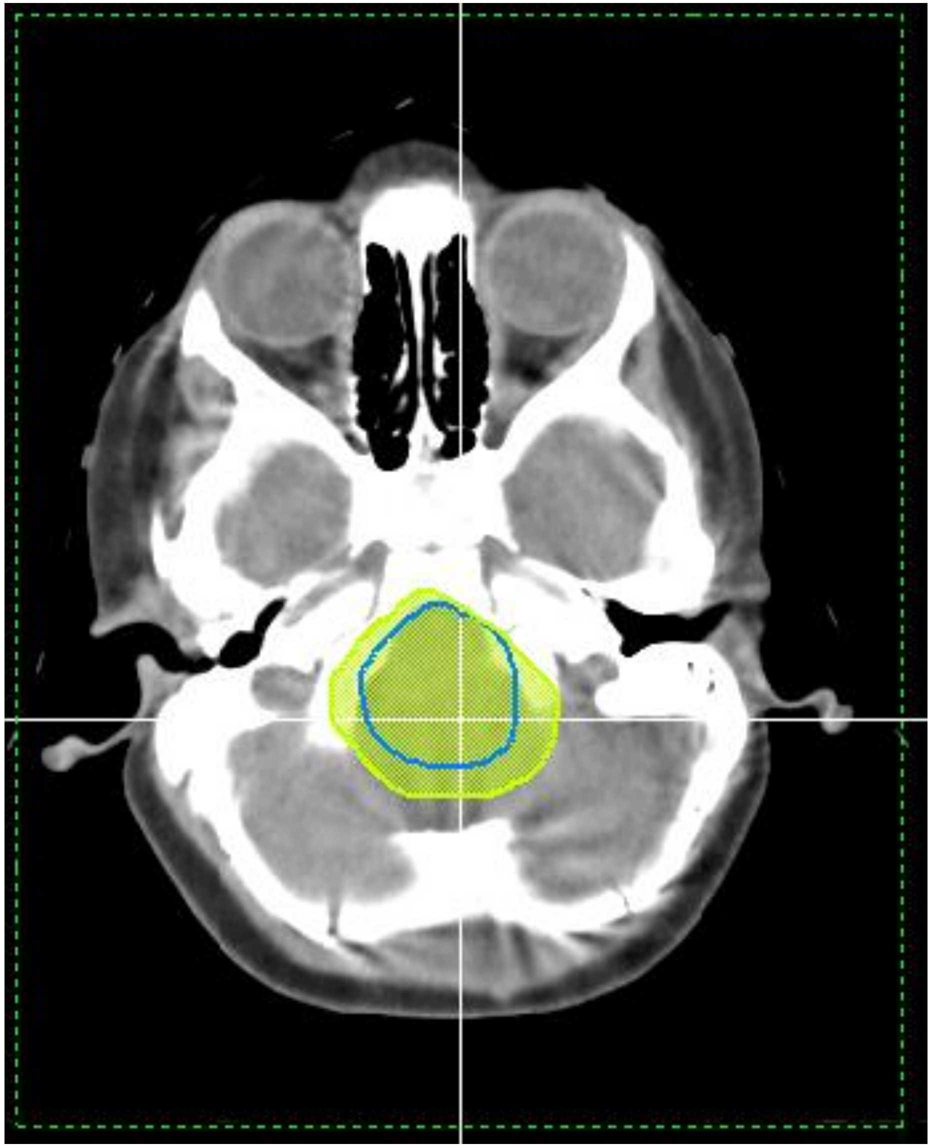
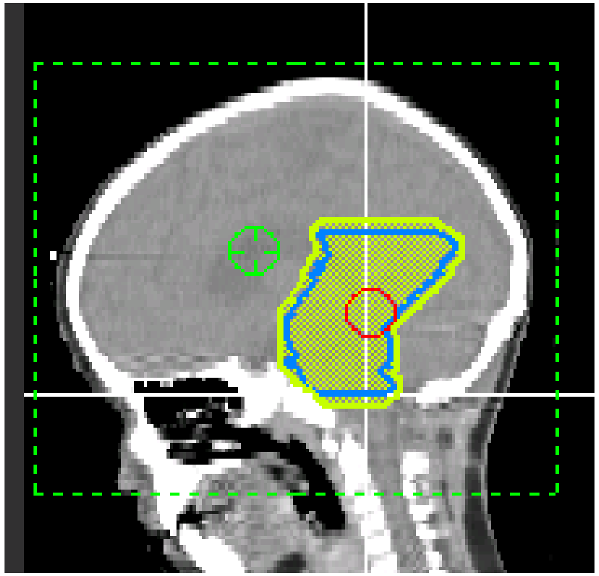
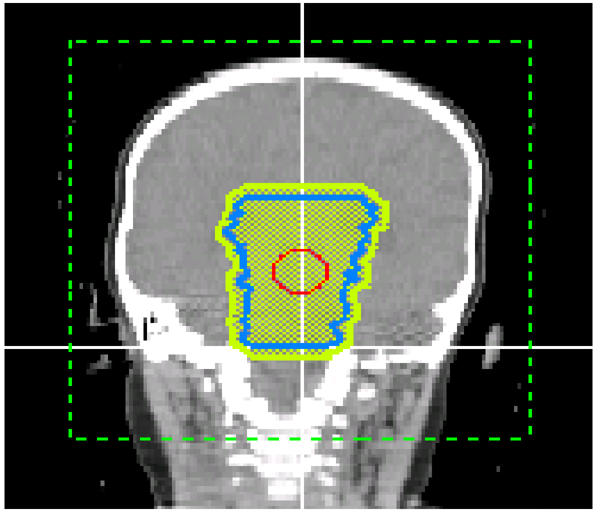
PTV (surgical bed + 5 mm margin)



PTV(yellow)

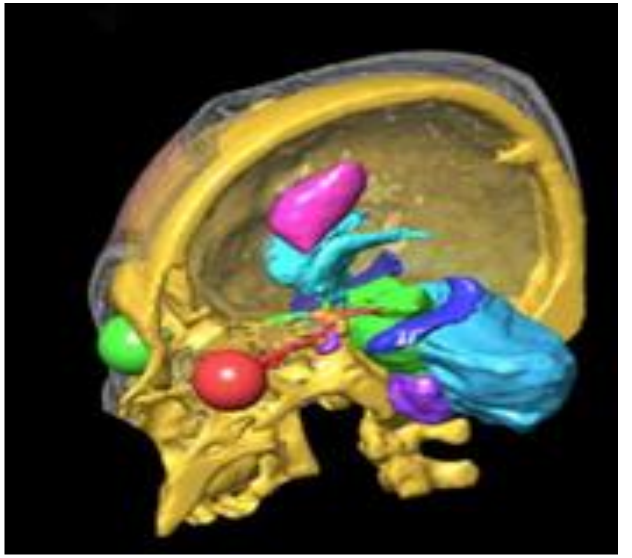






Take home message

- Inmovilization is crucial to reduce toxicity
- The addition of MRI gives vastly superior soft-tissue visualization
- The radiation technique (IMRT, Tomotherapy, Protons, Cyberknyfe) should be individualised for each patient



Questions:

- Preparation (thermoplastic mask)
- Positioning
- Organ at risk contouring
- Set-Up
- Verification
- Radiation technique

???

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Case reports: **Brain**

a physicist's perspective

Mirjana Josipovic

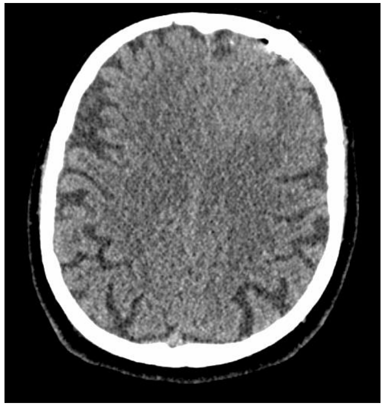
Dept. of Oncology, Rigshospitalet
& Niels Bohr Institute, University of Copenhagen
Denmark

Advanced skills in modern radiotherapy
June 2017

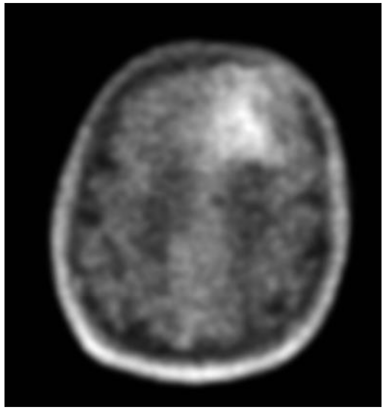
Imaging for brain RT planning

Imaging immobilised patient in the treatment position

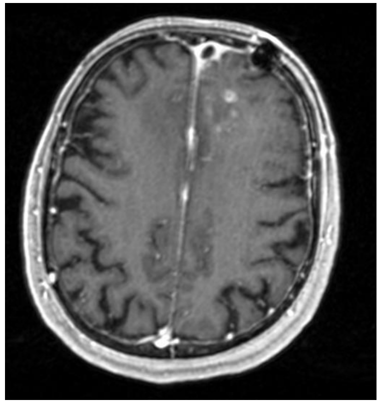
CT scan

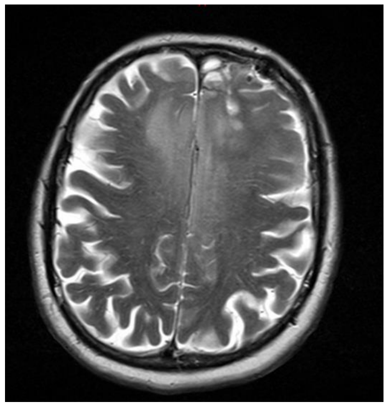


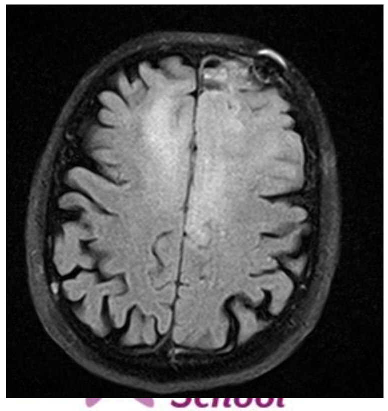
FET PET scan



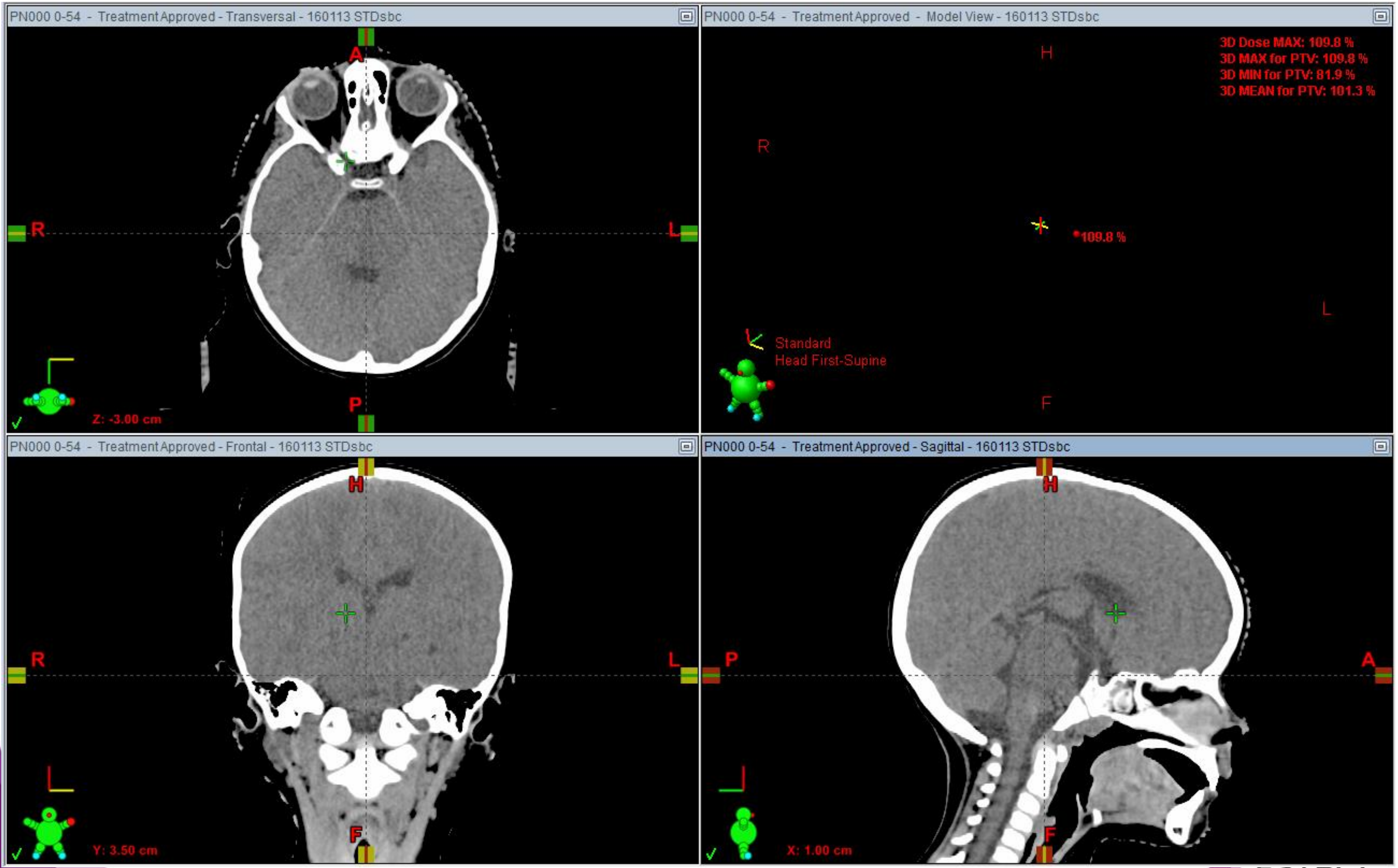
MR scan (T1,T2,FLAIR)







Thin scan slices ~1 mm



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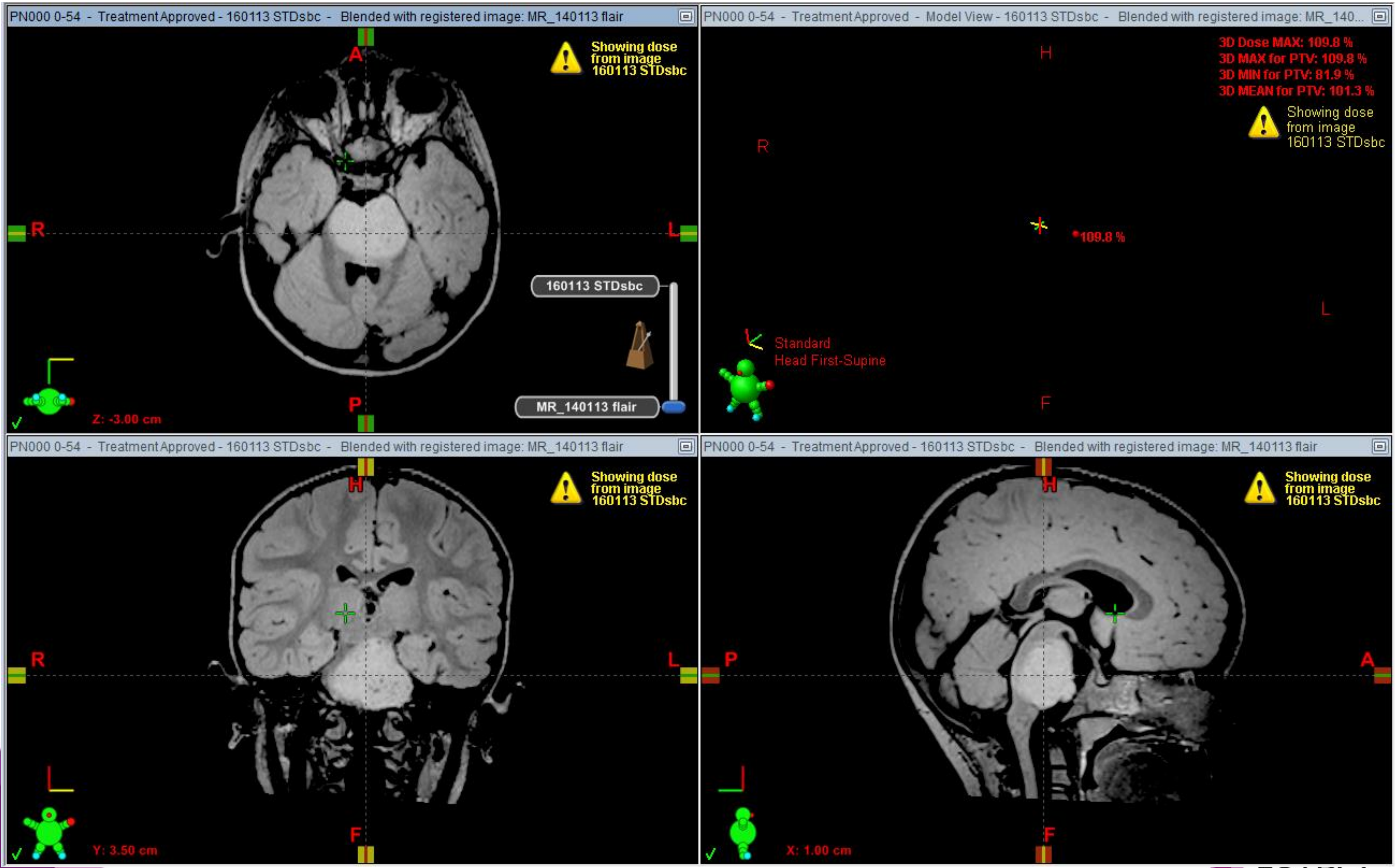
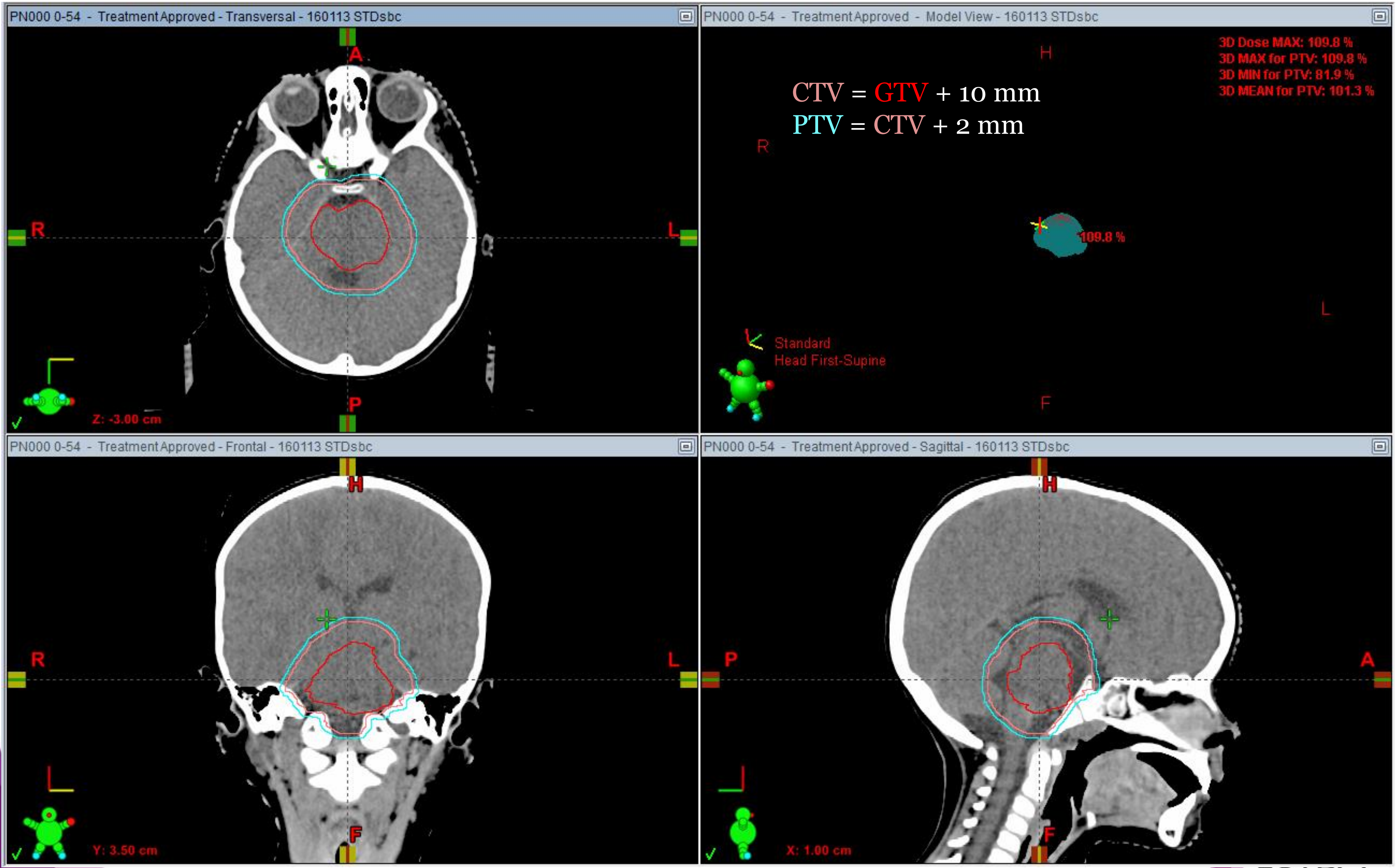
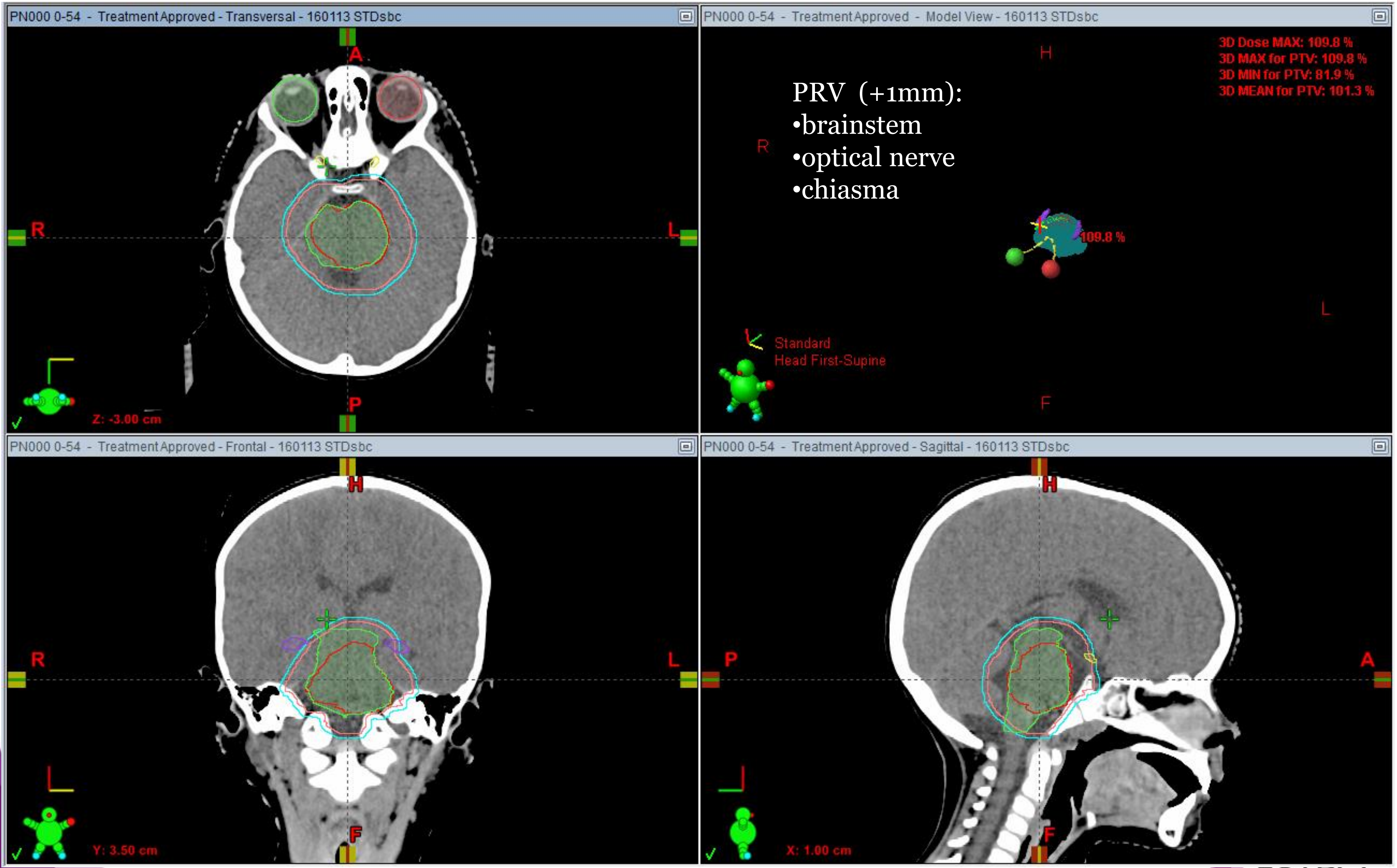

PN000 0-54 - Treatment Approved - 160113 STDsbc - Blended with registered image: MR_140113 flair
Showing dose from image 160113 STDsbc
A
R
L
P
160113 STDsbc
MR_140113 flair
Z: -3.00 cm
PN000 0-54 - Treatment Approved - Model View - 160113 STDsbc - Blended with registered image: MR_140...
3D Dose MAX: 109.8 %
3D MAX for PTV: 109.8 %
3D MIN for PTV: 81.9 %
3D MEAN for PTV: 101.3 %
Showing dose from image 160113 STDsbc
H
R
109.8 %
L
Standard
Head First-Supine
F
PN000 0-54 - Treatment Approved - 160113 STDsbc - Blended with registered image: MR_140113 flair
Showing dose from image 160113 STDsbc
H
R
L
F
Y: 3.50 cm
PN000 0-54 - Treatment Approved - 160113 STDsbc - Blended with registered image: MR_140113 flair
Showing dose from image 160113 STDsbc
H
P
A
F
X: 1.00 cm


PN000 0-54 - Treatment Approved - Transversal - 160113 STDsbc
PN000 0-54 - Treatment Approved - Model View - 160113 STDsbc
CTV = GTV + 10 mm
PTV = CTV + 2 mm
3D Dose MAX: 109.8 %
3D MAX for PTV: 109.8 %
3D MIN for PTV: 81.9 %
3D MEAN for PTV: 101.3 %
109.8 %
Standard
Head First-Supine
Z: -3.00 cm
PN000 0-54 - Treatment Approved - Frontal - 160113 STDsbc
Y: 3.50 cm
PN000 0-54 - Treatment Approved - Sagittal - 160113 STDsbc
X: 1.00 cm



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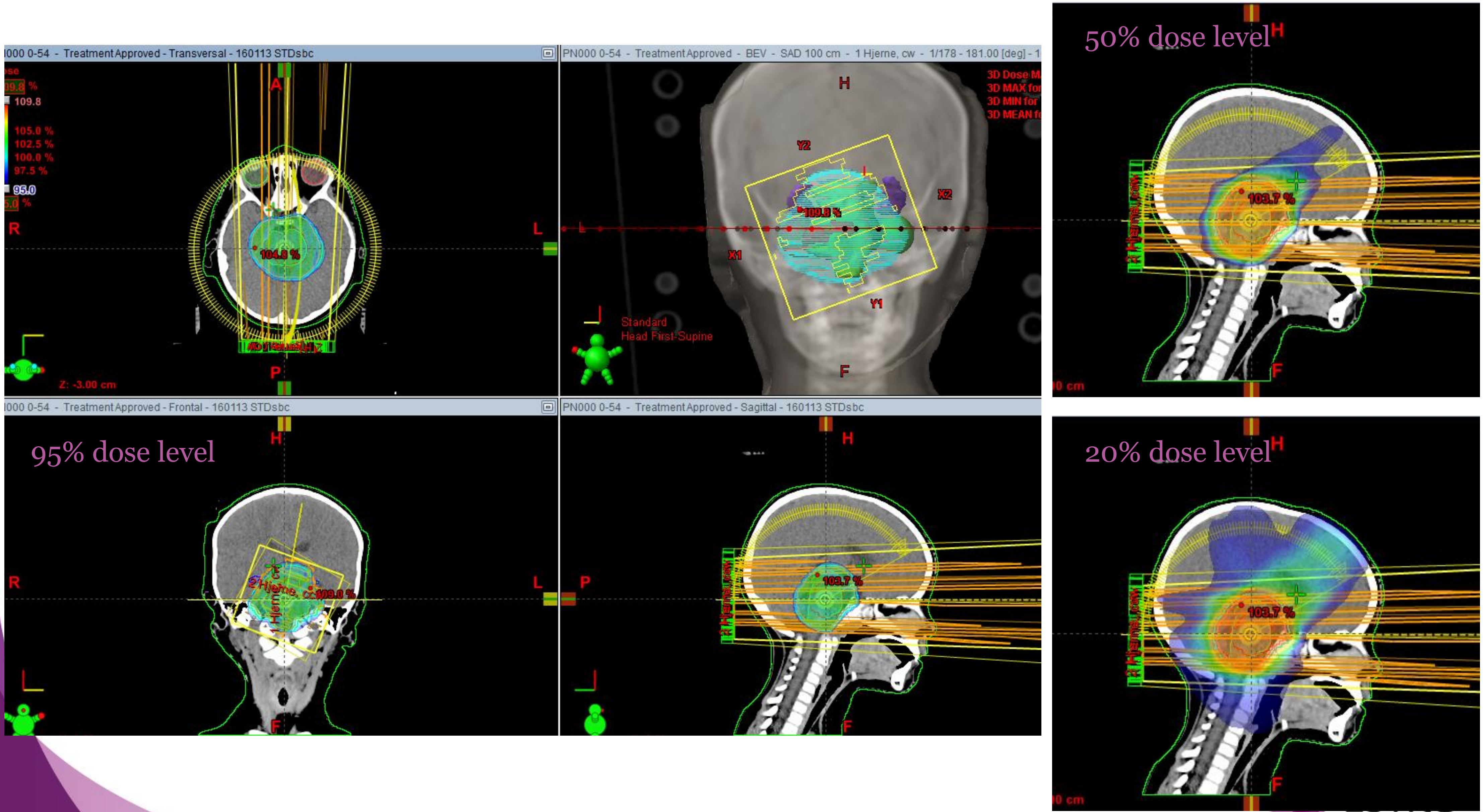
VMAT plan – 2 arcs



Radiotherapy

Radiotherapy techniques

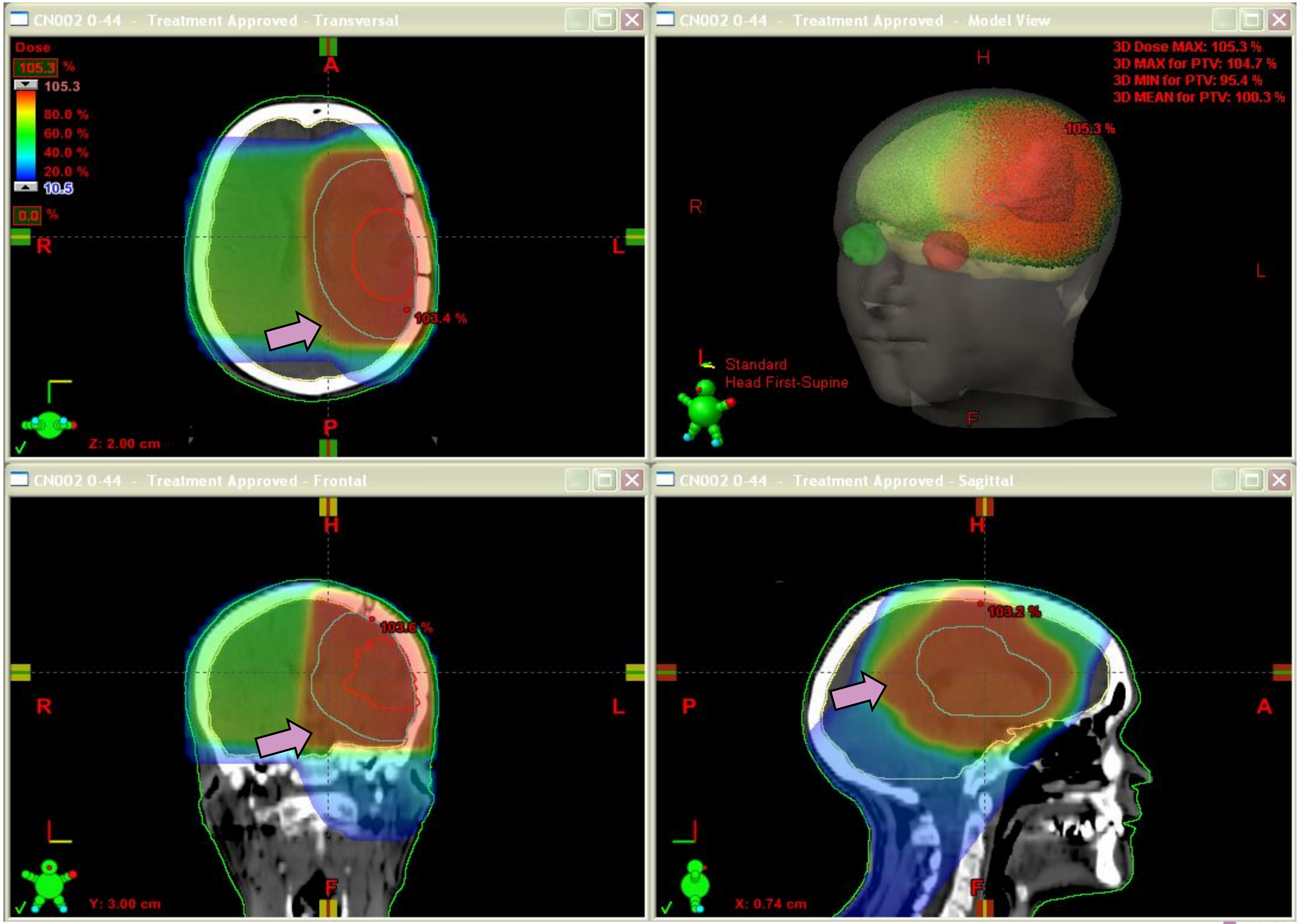
- 3DC
- IMRT
- VMAT
- Proton therapy

Fractionation schemes (Rigshospitalet, CPH)

- 2 Gy x 30
- 1.8 Gy x 30 (if brainstem is involved)

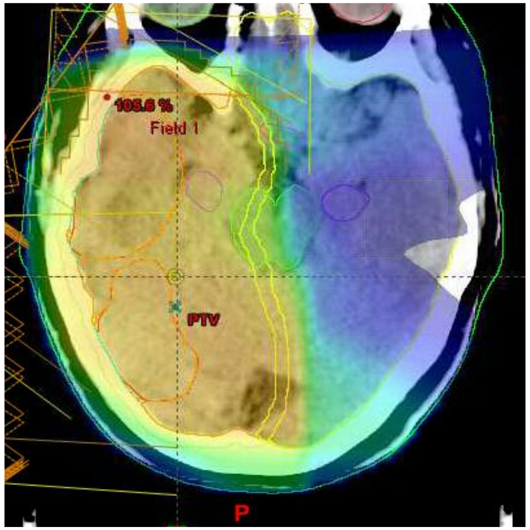
- 18 Gy x 1 (very small targets, stereotactic RT)
  - ➢ Prescribed as minimum dose to target

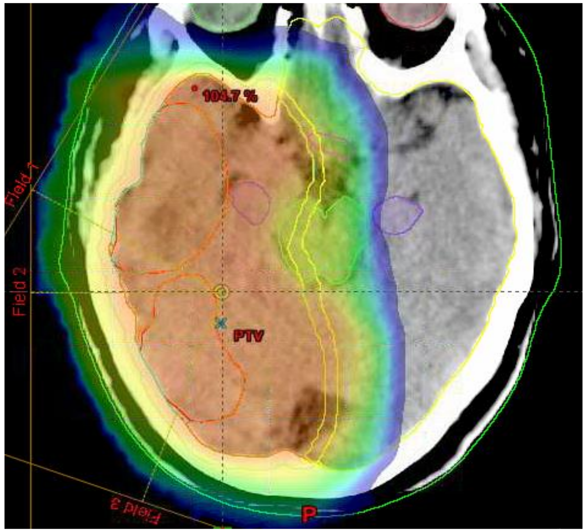
3DC plan

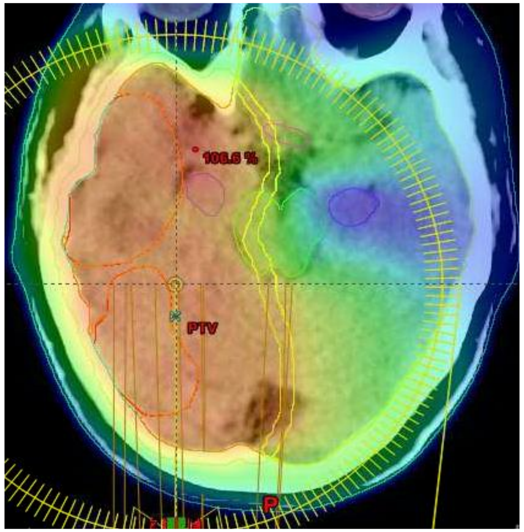


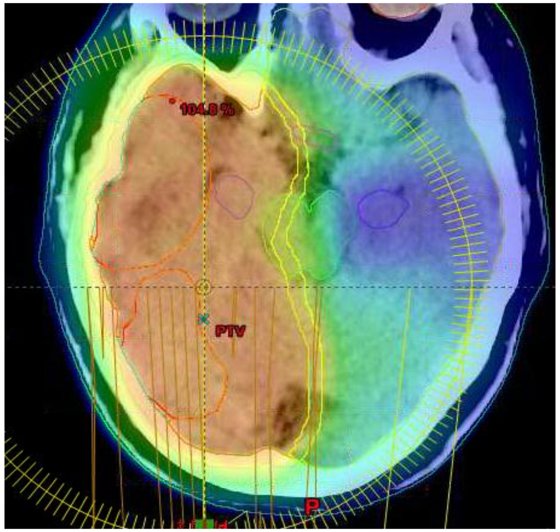
CN002 0-44 - Treatment Approved - Transversal
Dose
105.3 %
105.3
80.0 %
60.0 %
40.0 %
20.0 %
10.5
0.0 %
A
R
L
P
103.4 %
Z: 2.00 cm
CN002 0-44 - Treatment Approved - Model View
3D Dose MAX: 105.3 %
3D MAX for PTV: 104.7 %
3D MIN for PTV: 95.4 %
3D MEAN for PTV: 100.3 %
H
105.3 %
R
L
F
Standard
Head First-Supine
CN002 0-44 - Treatment Approved - Frontal
H
103.6 %
R
L
F
Y: 3.00 cm
CN002 0-44 - Treatment Approved - Sagittal
H
103.2 %
P
A
F
X: 0.74 cm

IMRT vs. protons vs. VMAT









IMRT

worst plan conformity

IMPT protons

best plan conformity

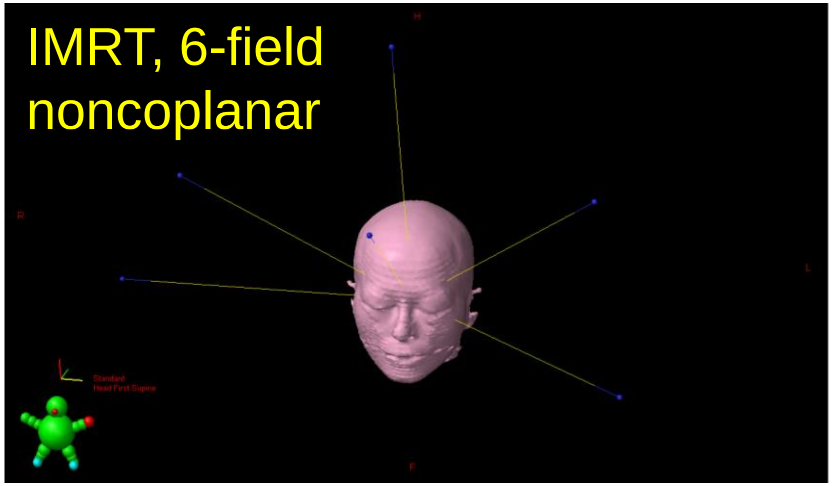
VMAT (co-planar)

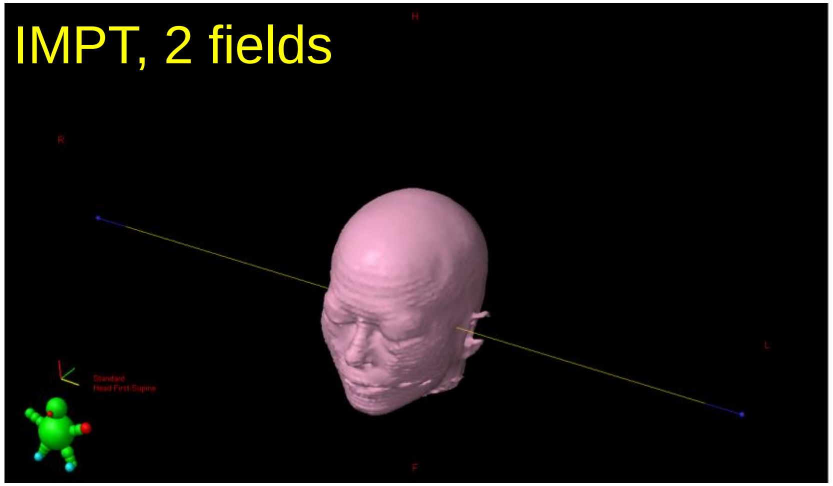
VMAT (non co-planar)

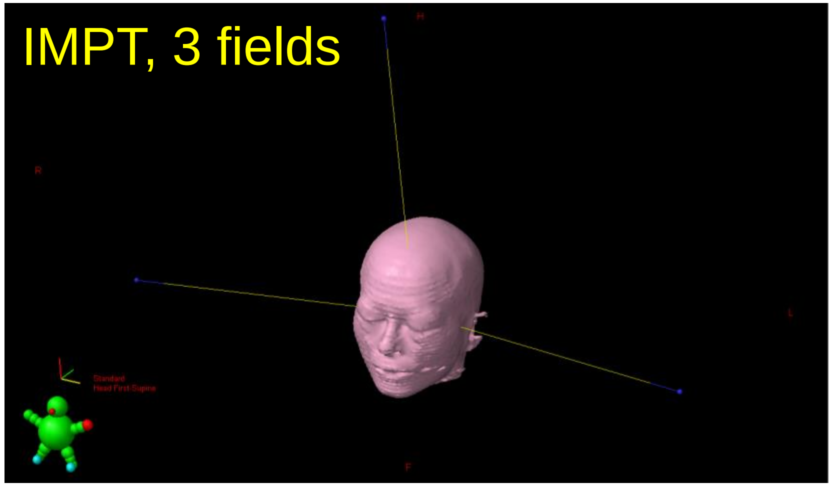
Courtesy of P Munck af Rosenschöld

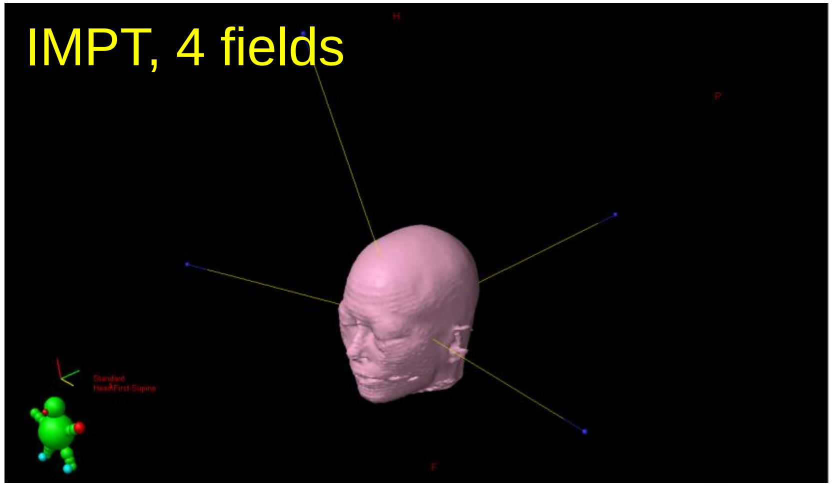
Photons or protons – how to decide?

- Many geometrical possibilities









Images courtesy of Klaus Seiersen & Jørgen Petersen,
Danish national center for particle radiotherapy

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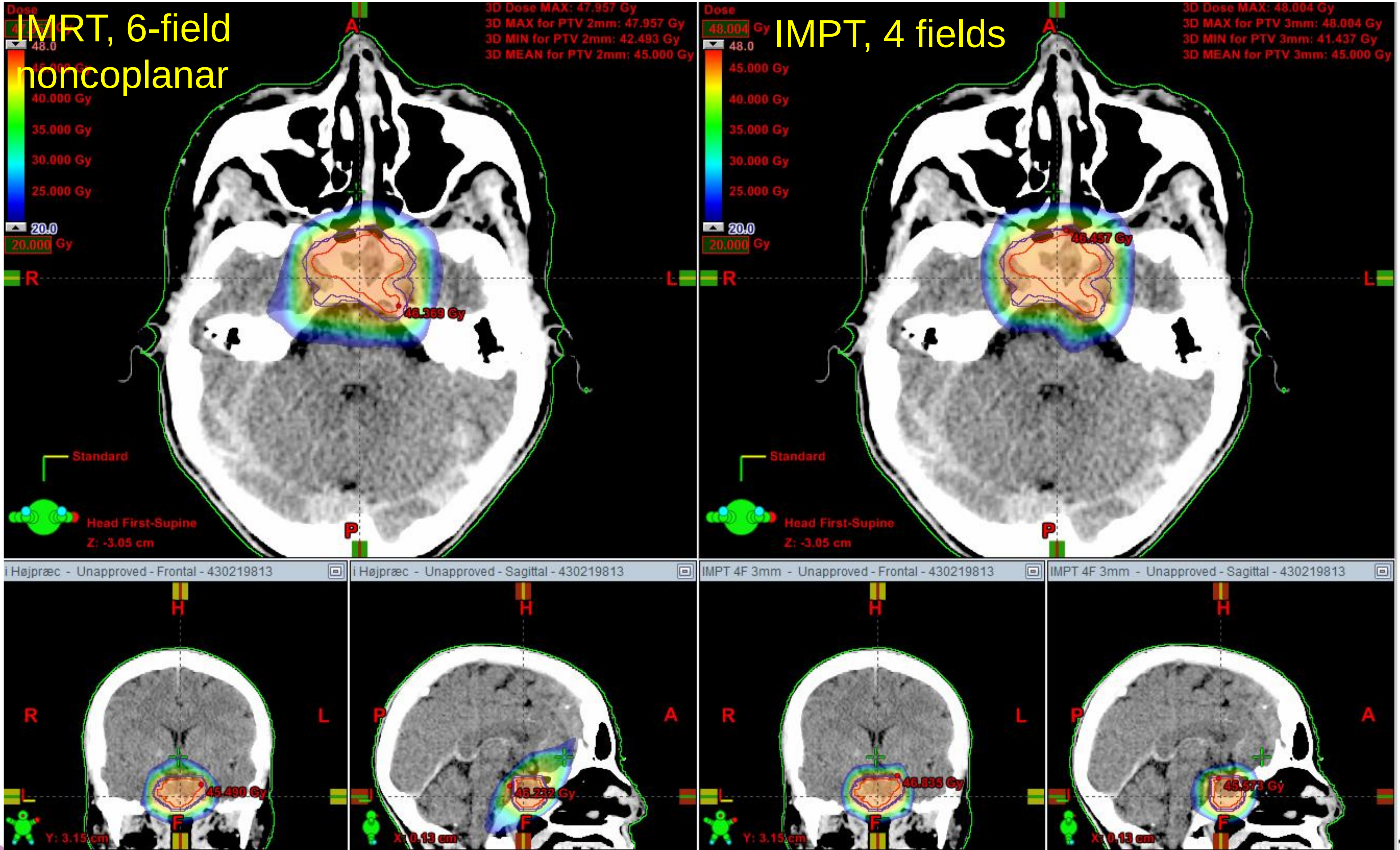
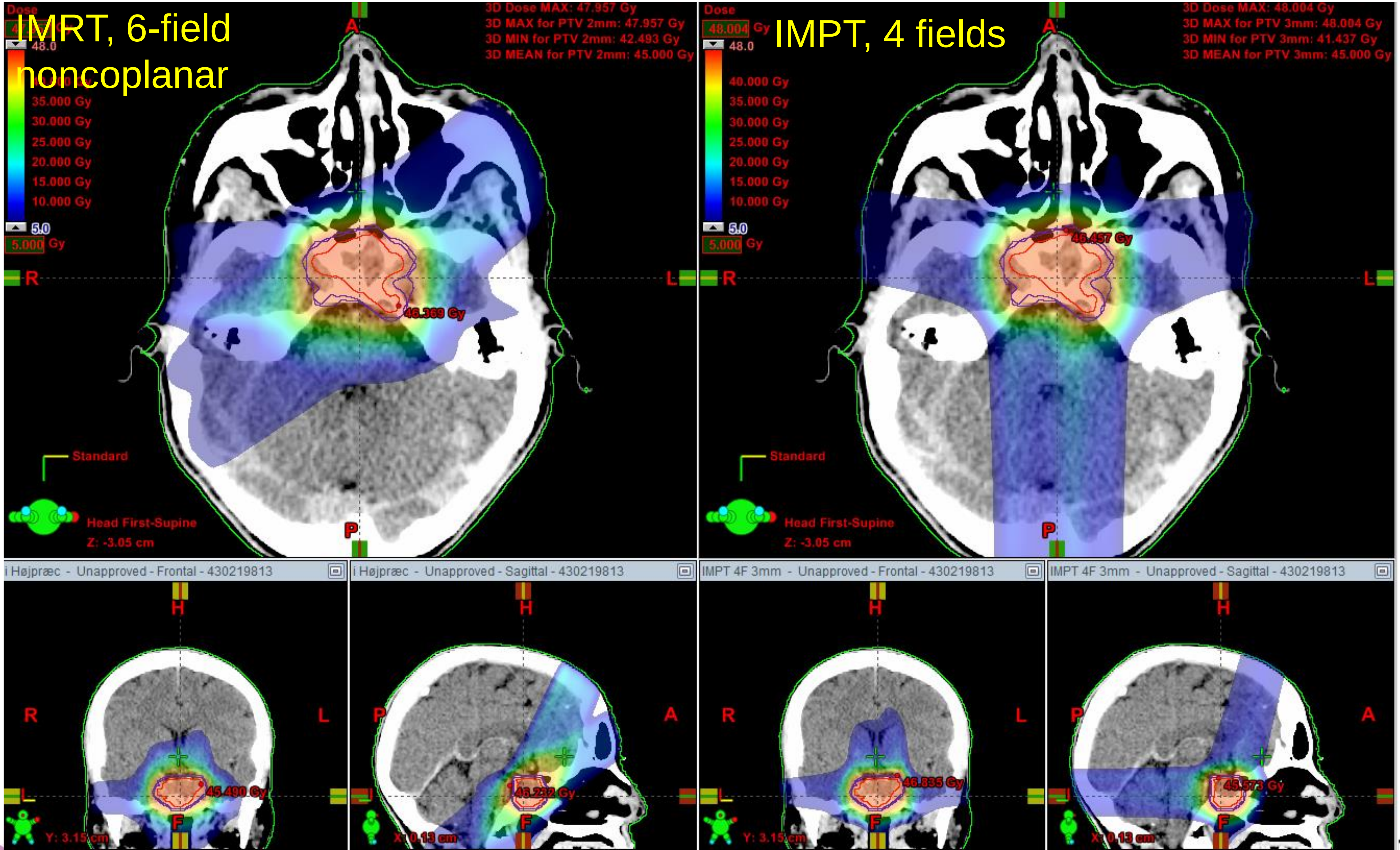
Photons or protons – how to decide?



Images courtesy of Klaus Seiersen & Jørgen Petersen,
Danish national center for particle radiotherapy

Photons or protons – how to decide?



Images courtesy of Klaus Seiersen & Jørgen Petersen,
Danish national center for particle radiotherapy

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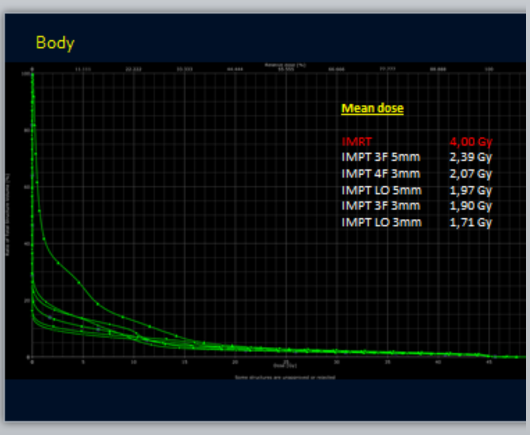
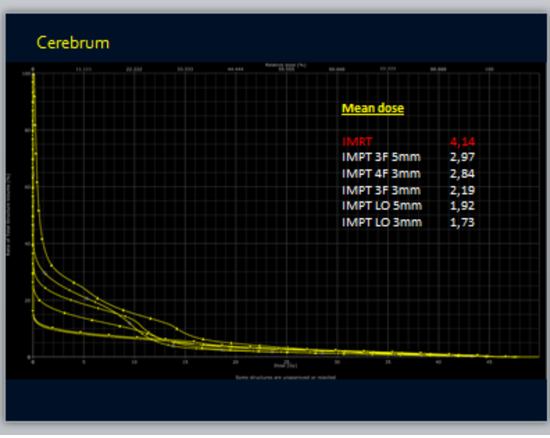
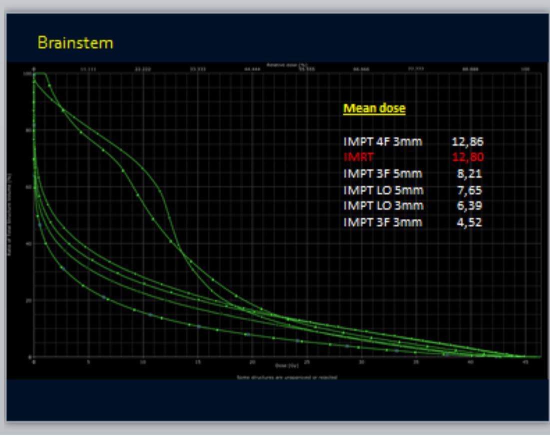
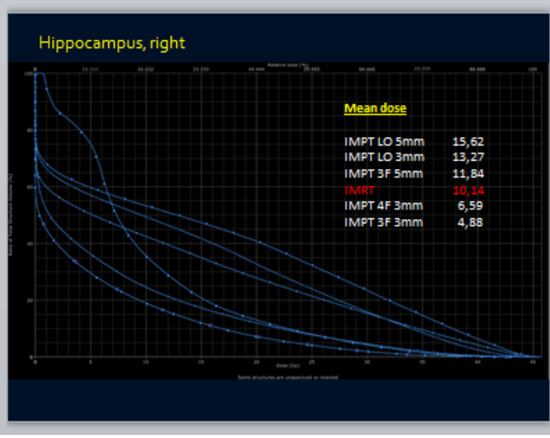
Photons or protons – how to decide?

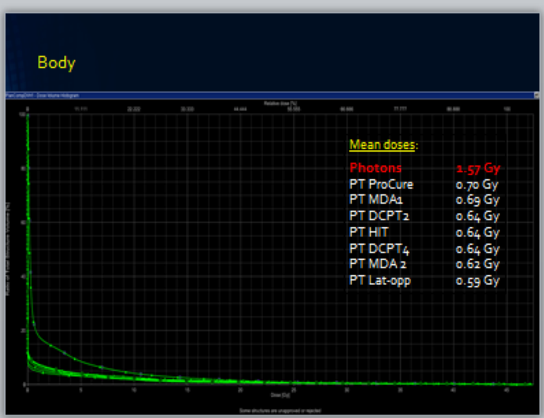
RED = photon IMRT

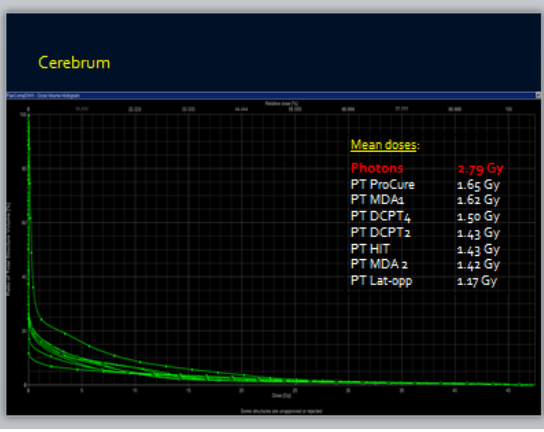


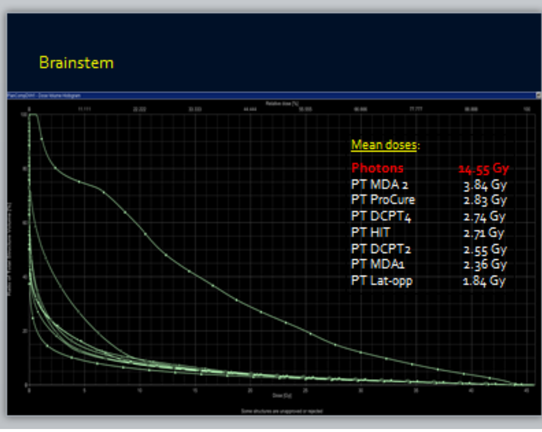


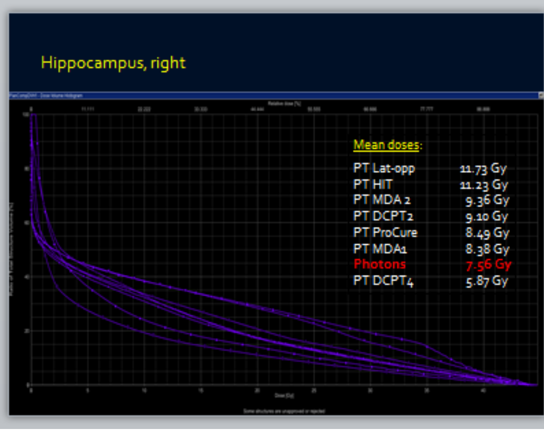












Images courtesy of Klaus Seiersen & Jørgen Petersen,
Danish national center for particle radiotherapy

Photons or protons – how to decide?

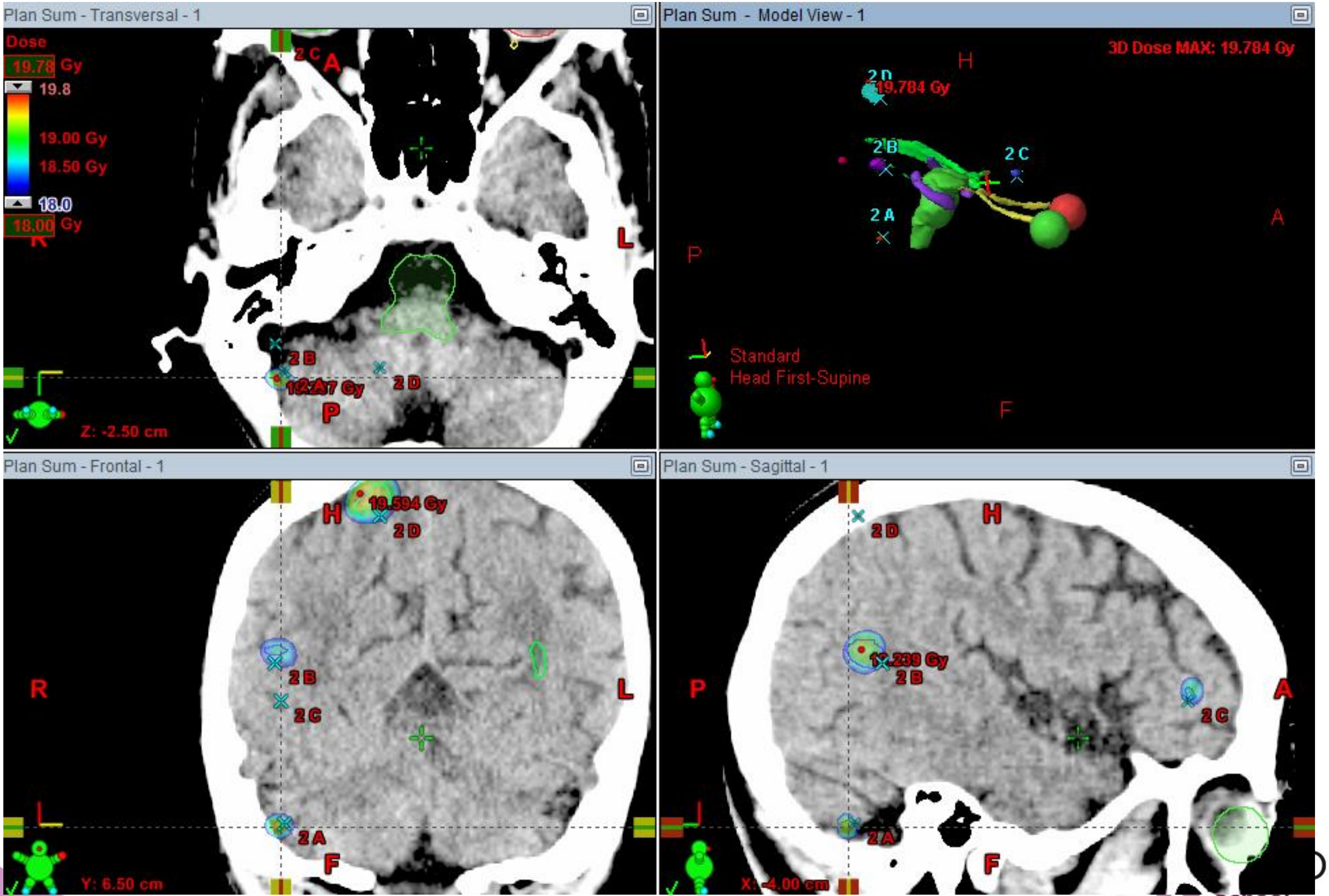
- OAR sparing depends on choice of treatment fields/angles

- Which organ to prioritise?
  - Doctor's order = "dose as low as possible"

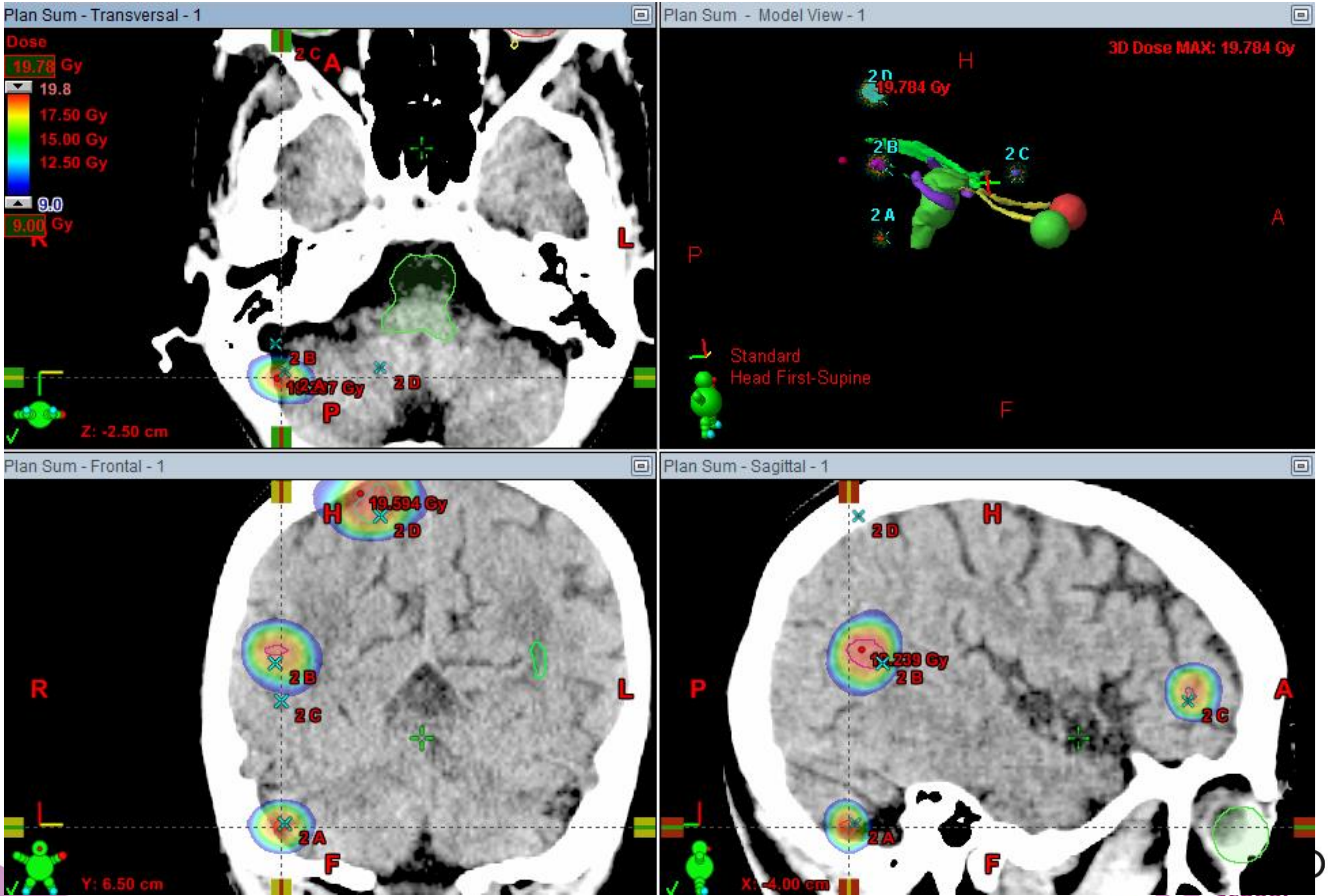
- Integral dose is always lower with protons
  - Risk of secondary cancer

Stereotactic treatment – brain metastases

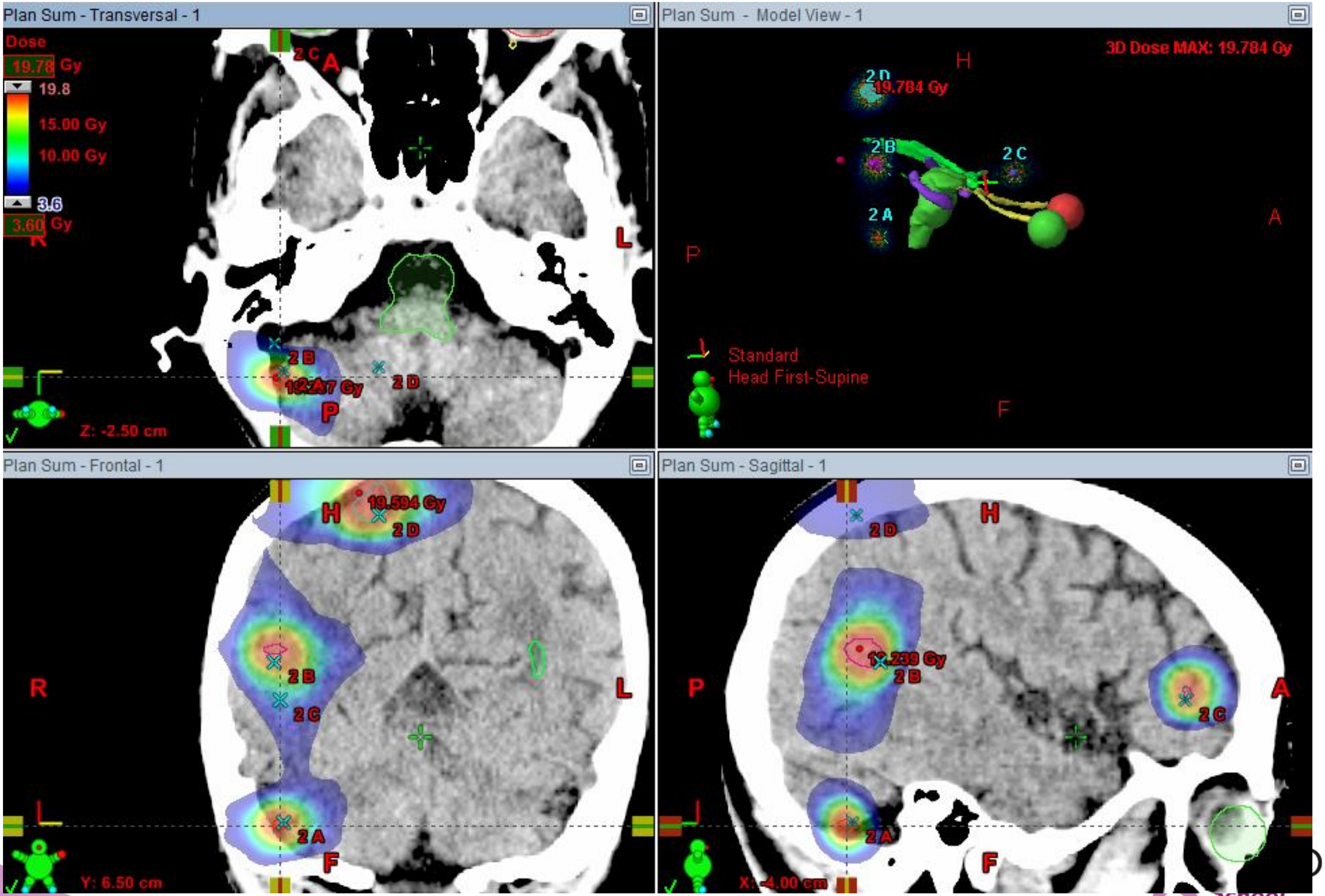
Stereotactic treatment – 4 targets!



Stereotactic treatment – 4 targets!



Stereotactic treatment – 4 targets!



Delivery of stereotactic brain RT

IGRT

- Small PTV margins
- 6D corrections

- Rigs tolerance:
  - <1mm
  - <1°

- Non-coplanar RT delivery
  - Repeat imaging after couch rotation

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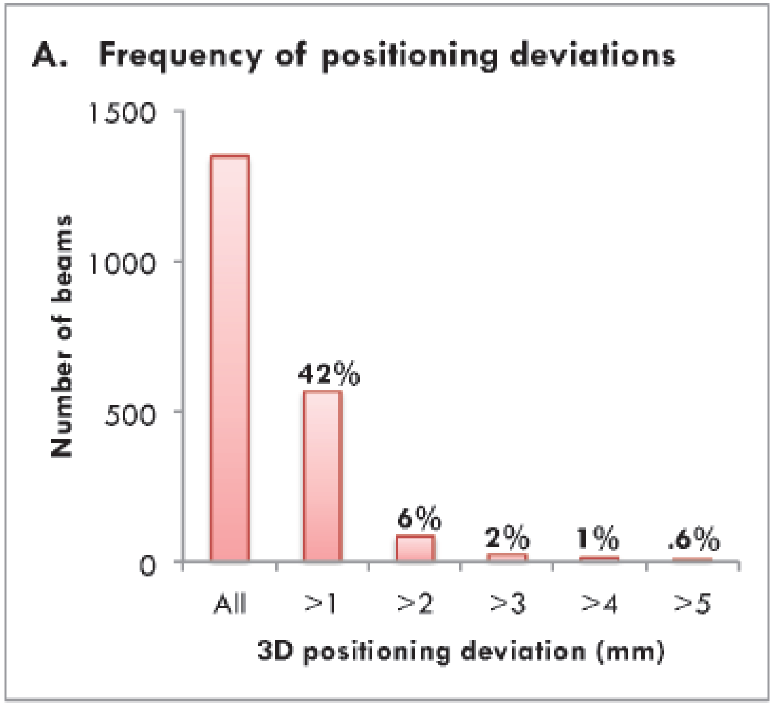
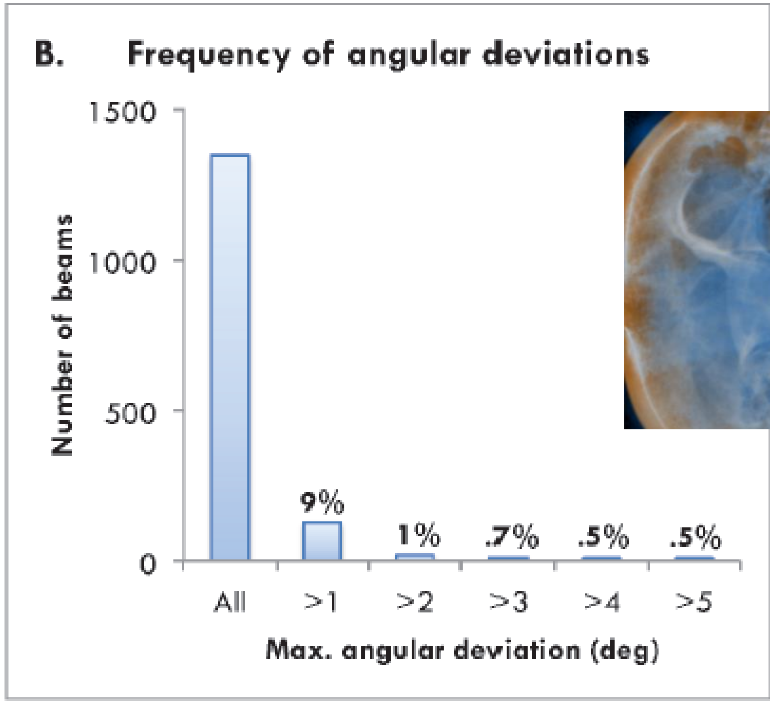
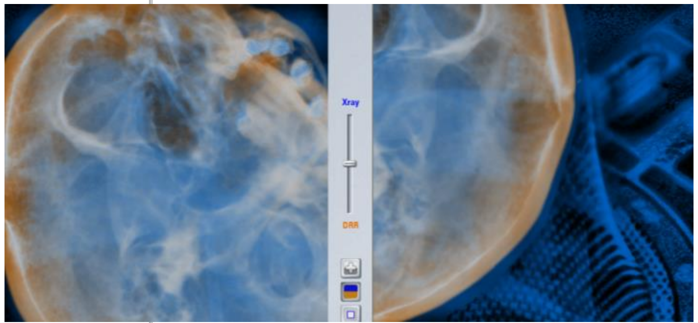
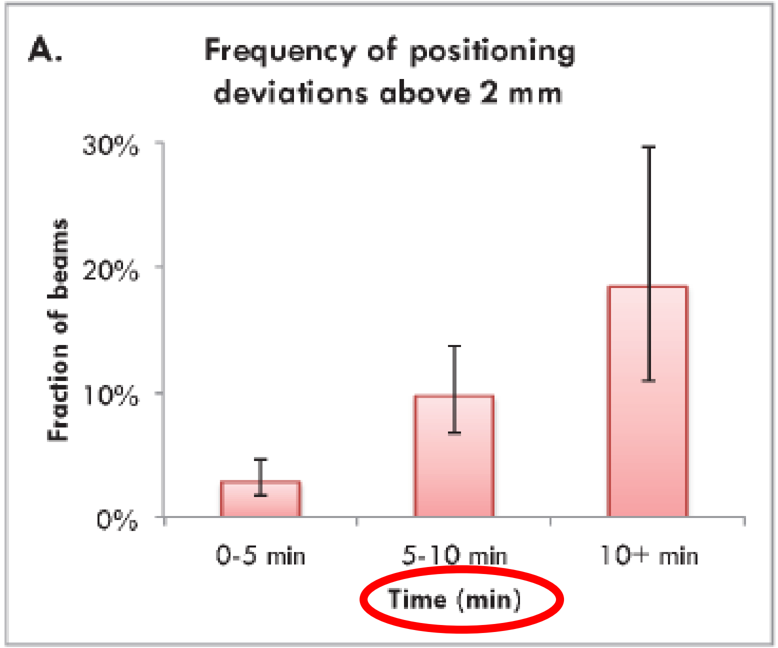
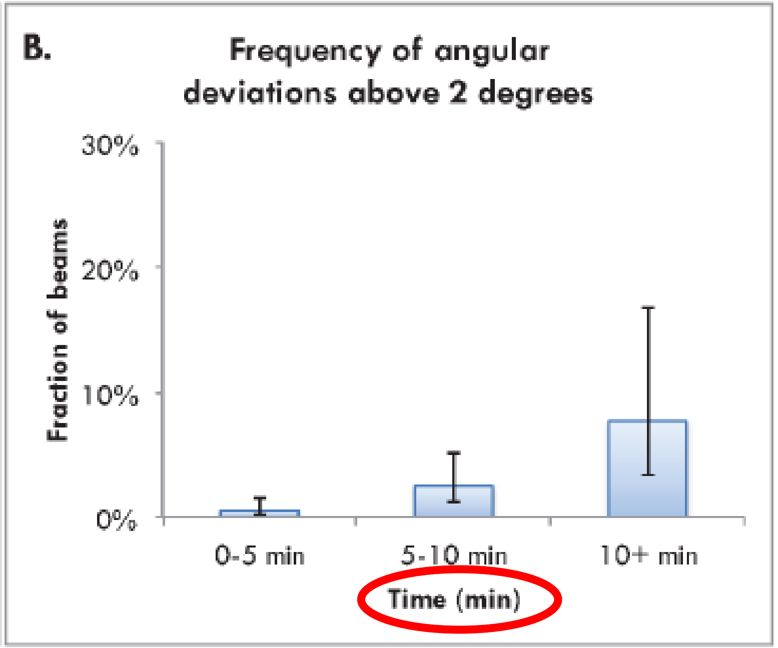






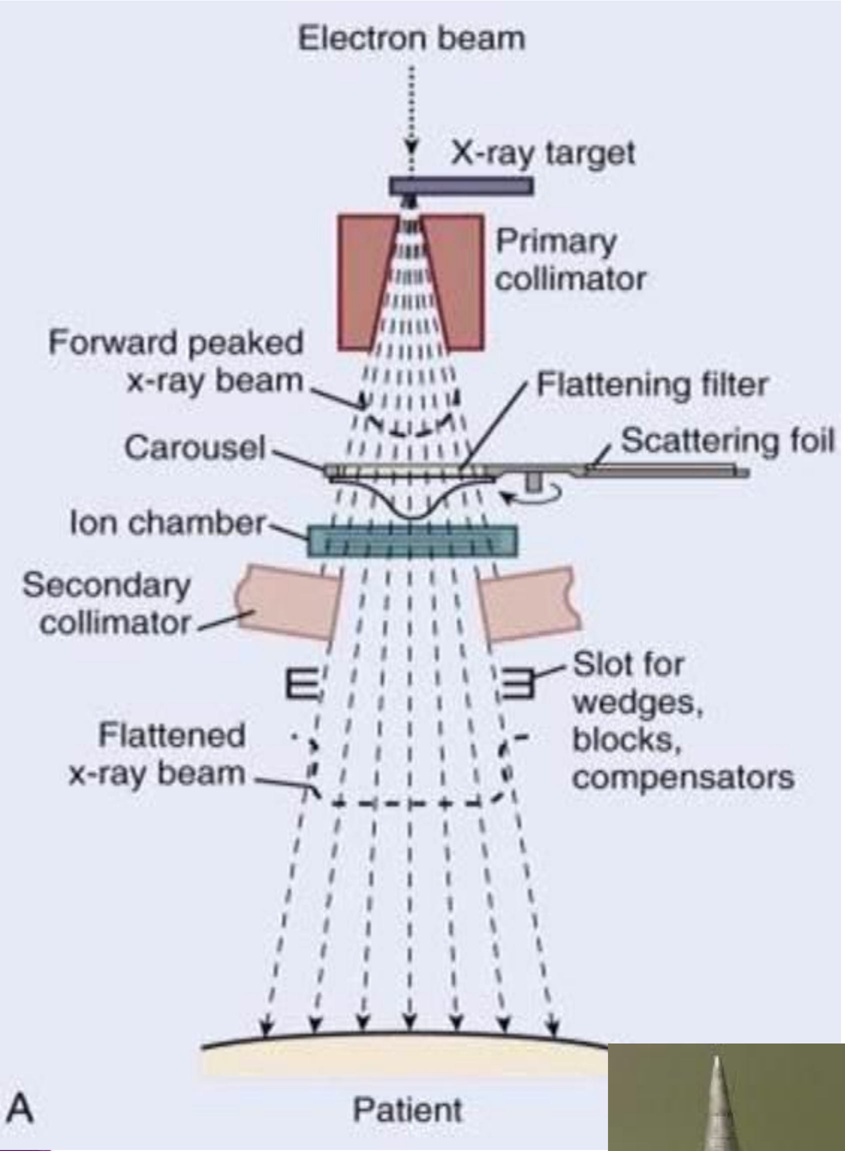
Intra-fractional uncertainties



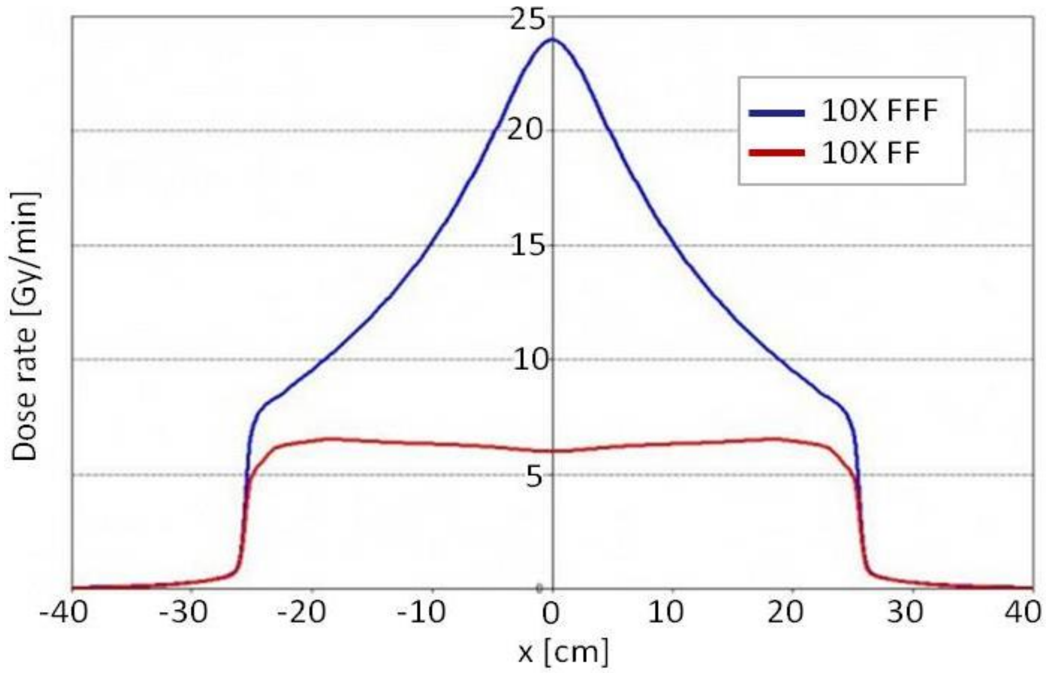


Tarnavski et al. Jour. of Radiosurgery and SBRT 2016

FFF – flattening filter free



Intensity modulated RT does not necessitate flat beams



FFF facilitates increase in dose rate & decrease in beam time by a factor of up to 6

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A bit about the margins…

Margins depend on:

- RT technique
- IGRT strategy (Rianne's talk)

Example:

- 3DC RT & field verification at first treatment
  - 5 mm CTV-PTV margin

- VMAT & daily IGRT with 6D:
  - 1-2 mm CTV-PTV margin

Considering the margins vs. daily IGRT workload

margins of 5 mm increase the treated volume by 50%

D. Verellen et al. nature reviews | **cancer** volume 7 | december 2007 | 949

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Brain

Rianne de Jong *RTT*,
Academic Medical Centre, Amsterdam
Prague 2017

m.a.j.dejong@amc.uva.nl

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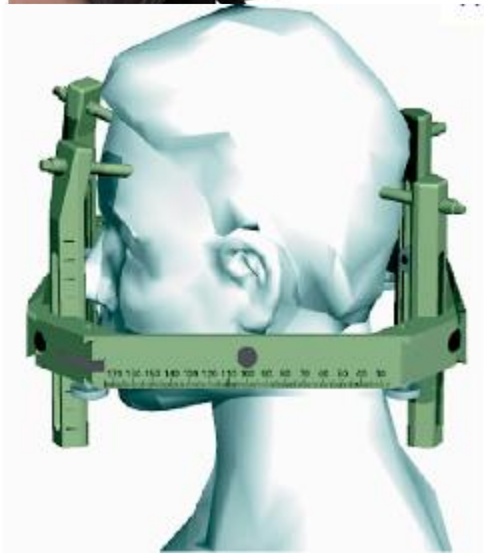
Brain @the treatment machine

- How well can we set up the patient?
- How well can we image the target volume?
- How well can we correct the patient position?
- How stable is the patient position?
- Imaging dose for children

Commercial Immobilisation Options

- Thermoplastic mask
- Mask + bite block
- Frames
- Invasive frames




Set-up accuracy: interfraction motion → based on bony anatomy registration

Study	Positioning system	Imaging modality	Position error
2D-2D image registration for verification of set-up			
Rosenthal 1995	Dental fixation	Ortogonal radiographs	**2.3mm ±1.6mm**
Sweeny 2001	Vogely Bale Hohner head Holder	Portal imaging	**1.9mm ± 1.2mm**
Kumar 2005	Gill-Thomas-Cosman	Portal imaging	**1.8mm ± 0.8mm**
Georg 2006	Brain Lab Mask	Portal imaging	**1.3mm ± 0.9mm**
3D-3D image registration for verification of set-up			
Baumert 2005	Stereotactic mast	CT	**3.7mm ± 0.8mm**
Boda-Heggermann 2006	Scotch cast mask	CBCT	**3.1mm ± 1.5mm**
Guckenberger 2007	Scotch cast mask	CBCT	**3.0mm ± 1.7mm**
Masi 2008	Thermoplastic mask & Bite block	CBCT	**2.9mm ± 1.3mm**
	Bite-block	CBCT	**3.2mm ± 1.5mm**

Courtesy M. Guckenberger, ESTRO IGRT course

Set-up accuracy: interfraction motion → based on bony anatomy registration

Study	Positioning system	Imaging modality	Position error
2D-2D image registration for verification of set-up			
Rosenthal 1995	Dental fixation	Ortogonal radiographs	**2.3mm ±1.6mm**
Sweeny 2001	Vogely Bale Hohner head Holder	Portal imaging	**1.9mm ± 1.2mm**
Kumar 2005	Gill-Thomas-Cosman	Portal imaging	**1.8mm ± 0.8mm**
Georg 2006	Brain Lab Mask	Portal imaging	**1.3mm ± 0.9mm**
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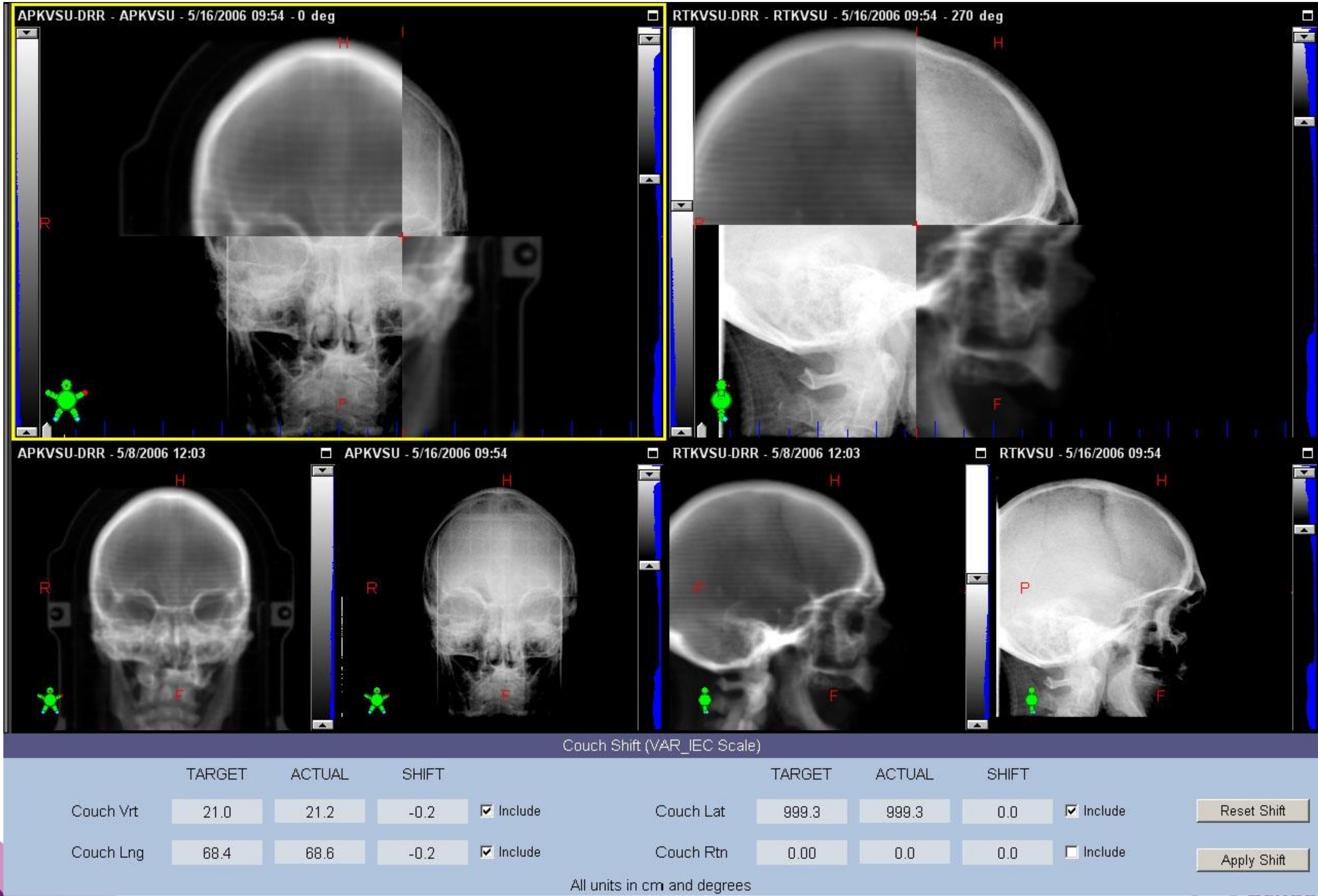
Masi 2008	Thermoplastic mask & Bite block	CBCT	**2.9mm ± 1.3mm**
	Bite-block	CBCT	**3.2mm ± 1.5mm**

!

Courtesy M. Guckenberger, ESTRO IGRT course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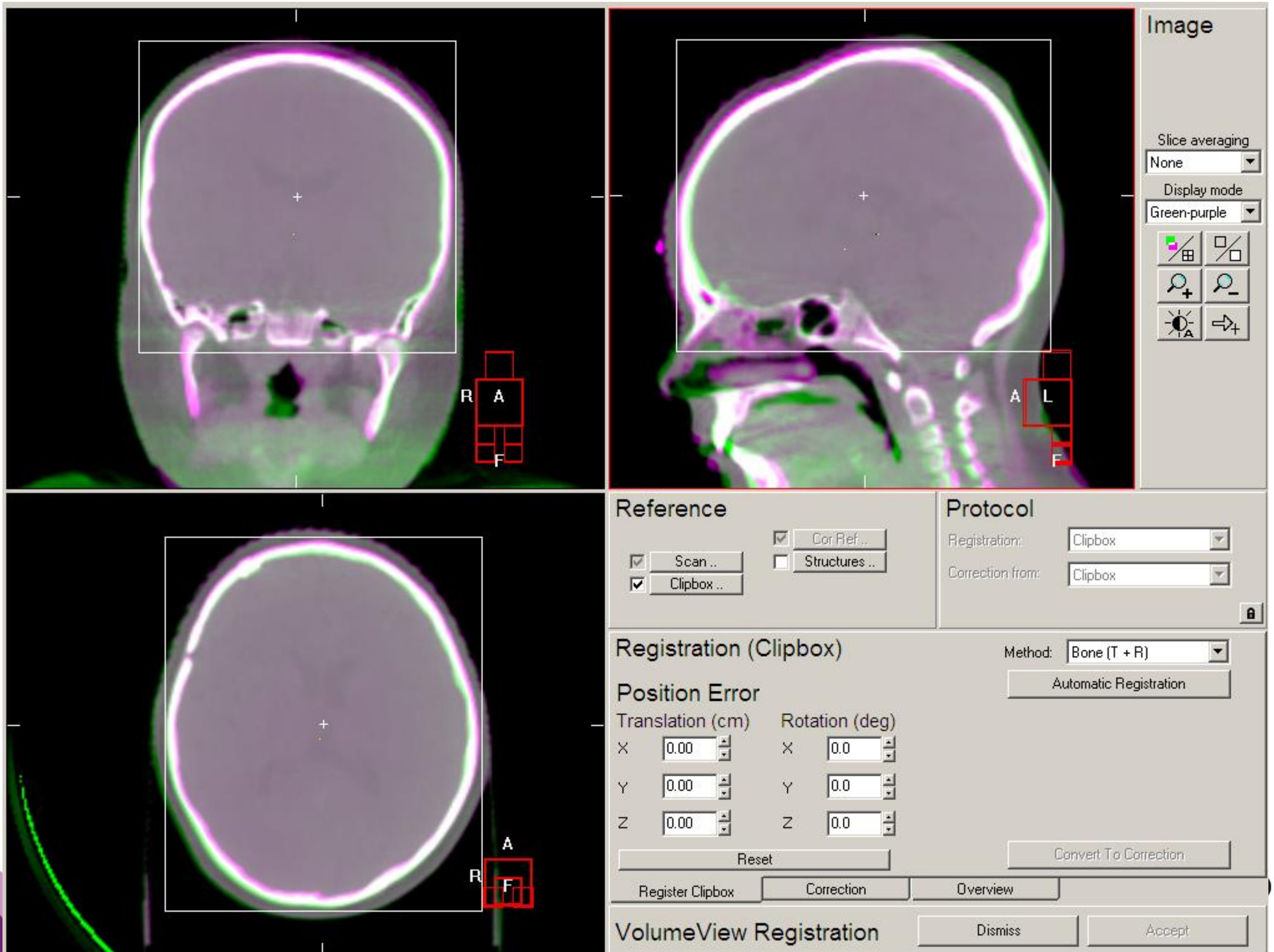
RTKVSU-DRR - RTKVSU - 5/16/2006 09:54 - 270 deg
APKVSU-DRR - 5/8/2006 12:03
APKVSU - 5/16/2006 09:54
RTKVSU-DRR - 5/8/2006 12:03
RTKVSU - 5/16/2006 09:54
Couch Shift (VAR_IEC Scale)
TARGET ACTUAL SHIFT
Couch Vrt 21.0 21.2 -0.2 Include
Couch Lng 68.4 68.6 -0.2 Include
TARGET ACTUAL SHIFT
Couch Lat 999.3 999.3 0.0 Include
Couch Rtn 0.00 0.0 0.0 Include
Reset Shift
Apply Shift
All units in cm and degrees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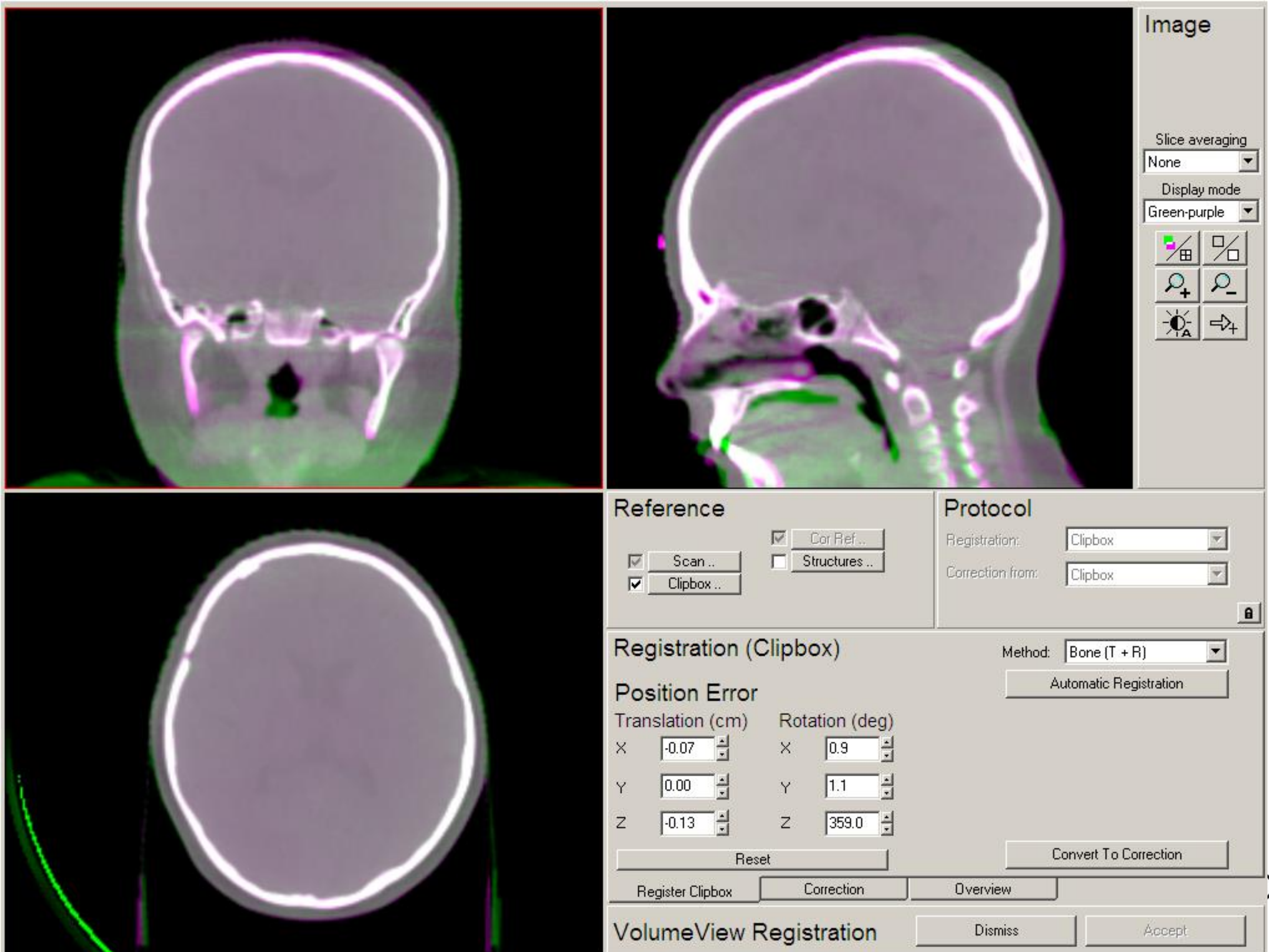
Scan ..
Structures ..
Clipbox ..
Protocol
Registration:
Clipbox
Correction from:
Clipbox
Registration (Clipbox)
Method:
Bone (T + R)
Automatic Registration
Position Error
Translation (cm)
Rotation (deg)
X 0.00
X 0.0
Y 0.00
Y 0.0
Z 0.00
Z 0.0
Reset
Convert To Correction
Register Clipbox
Correction
Overview
VolumeView Registration
Dismiss
Accept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Clipbox
Correction from:
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Registration (Clipbox)
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Bone (T + R)
Automatic Registration
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Y
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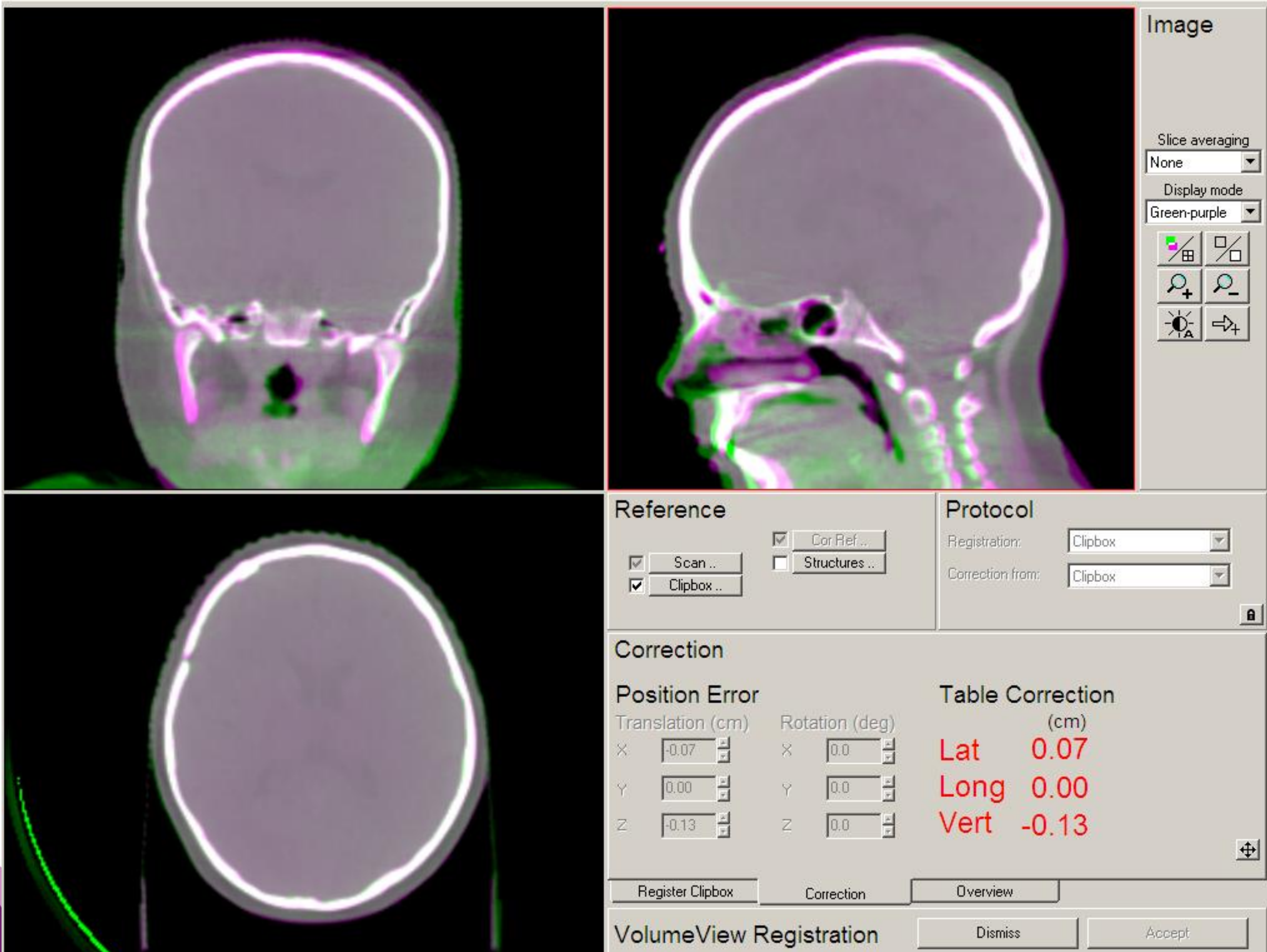
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Registration:
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Correction from:
Clipbox
Correction
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Translation (cm)
X -0.07
Y 0.00
Z -0.13
Rotation (deg)
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Y 0.0
Z 0.0
Table Correction
(cm)
Lat 0.07
Long 0.00
Vert -0.13
Register Clipbox
Correction
Overview
VolumeView Registration
Dismiss
Accept

Image registration

→ Bony anatomy a good surrogate?

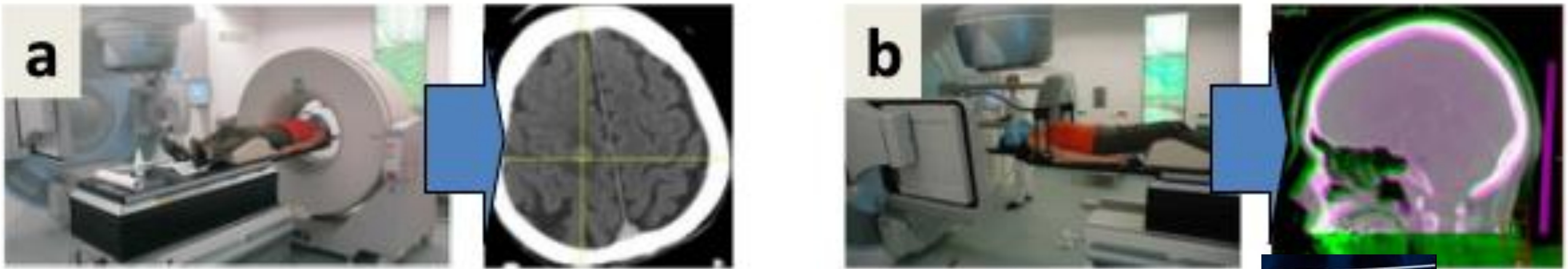
Internal motion of the intra cerebral tumor could be caused by

- Tumor progression
- Tumor shrinkage
- Changes of peritumoral edema

Set-up prior to treatment was verified based on the

a) position of the metastasis (soft tissue match): imaging using an in-room CT scanner after application of iv contrast

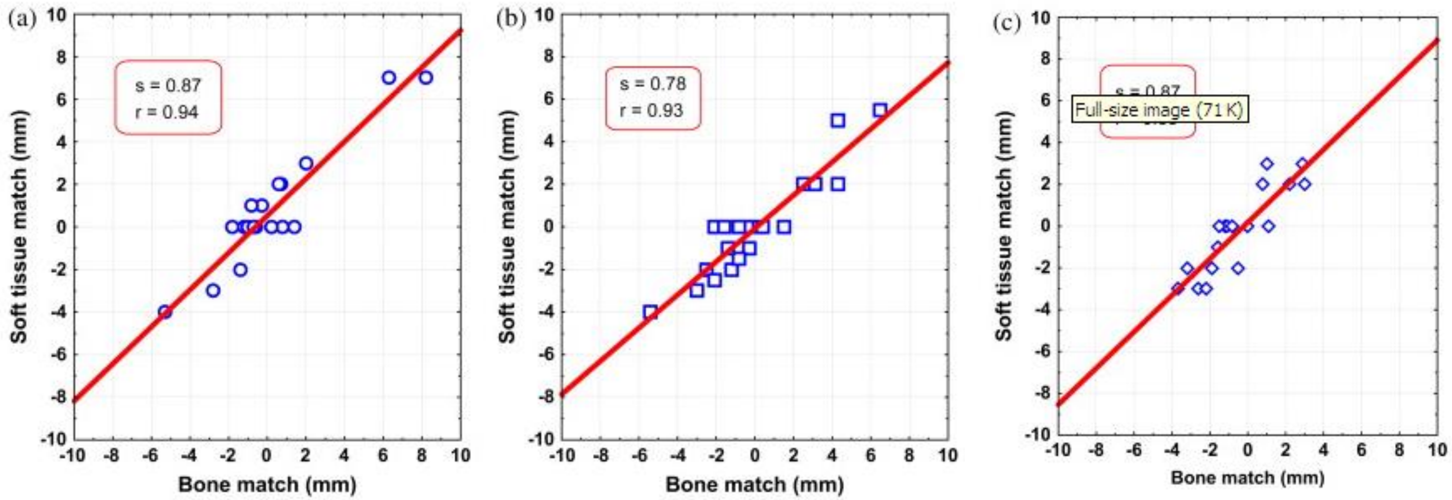
b) position of the bony anatomy (bone match): imaging using cone-beam CT



M. Guckenberger 2007

Image registration

→ Bony anatomy a good surrogate?



	Difference between bone match and tumor match (mm)		
	LR	SI	AP
Mean ± SD	-0.5 ± 1.0	0.1 ± 1.1	-0.2 ± 1.0
Maximum	1.8	2.3	2

M. Guckenberger 2007

Image registration

→ Bony anatomy a good surrogate?

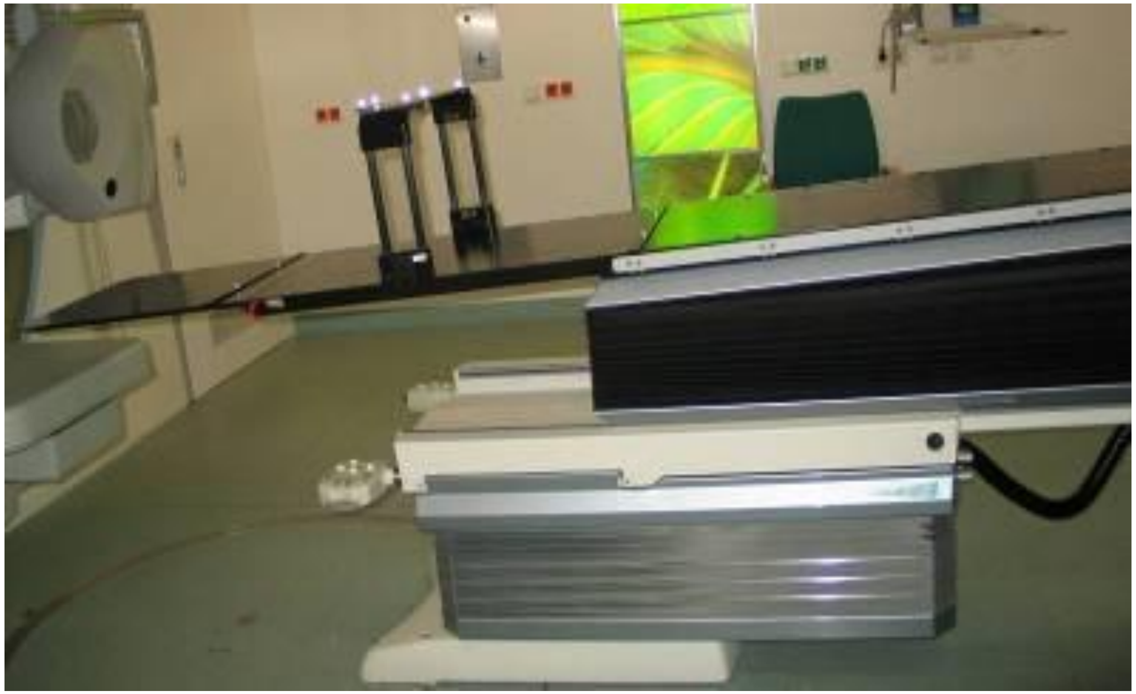
Yes, but keep the time interval to a minimum!

M. Guckenberger 2007

Image registration

→ How well can we correct errors?

Ask your physicist your table accuracy!



- Corrections up to 3°
- Target is often spherical

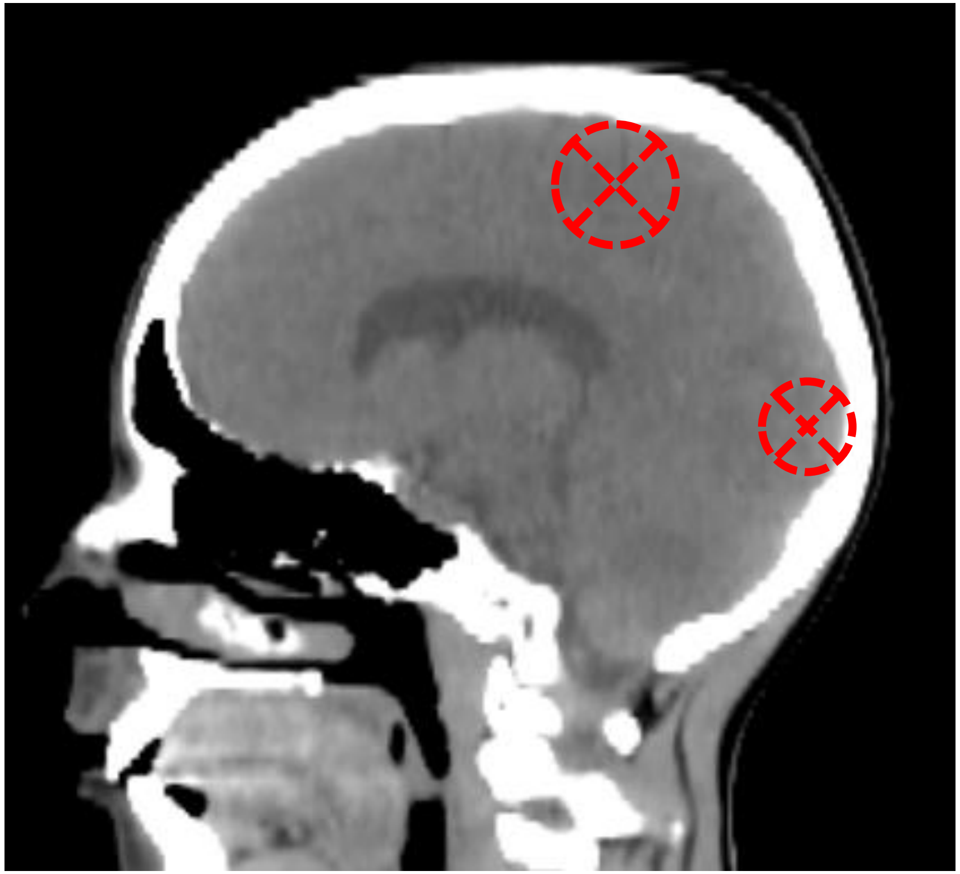
Residual errors after image guidance with CBCT and robotic couch:

< 0.3mm **<0.3°**

Meyer 2008

Image registration

→ How well can we correct errors?

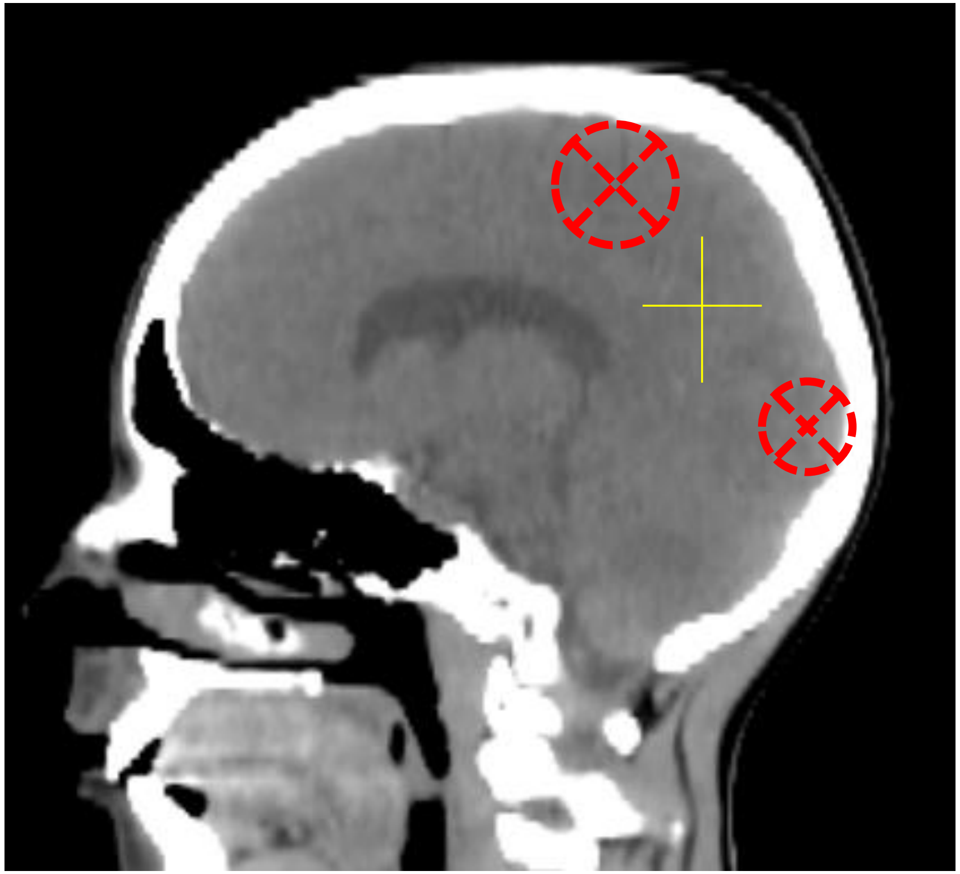


When multiple targets:

Rotations become important!

Image registration

→ How well can we correct errors?



When multiple targets:

Rotations become important!

Use limit on rotations !

Correcting Patient position

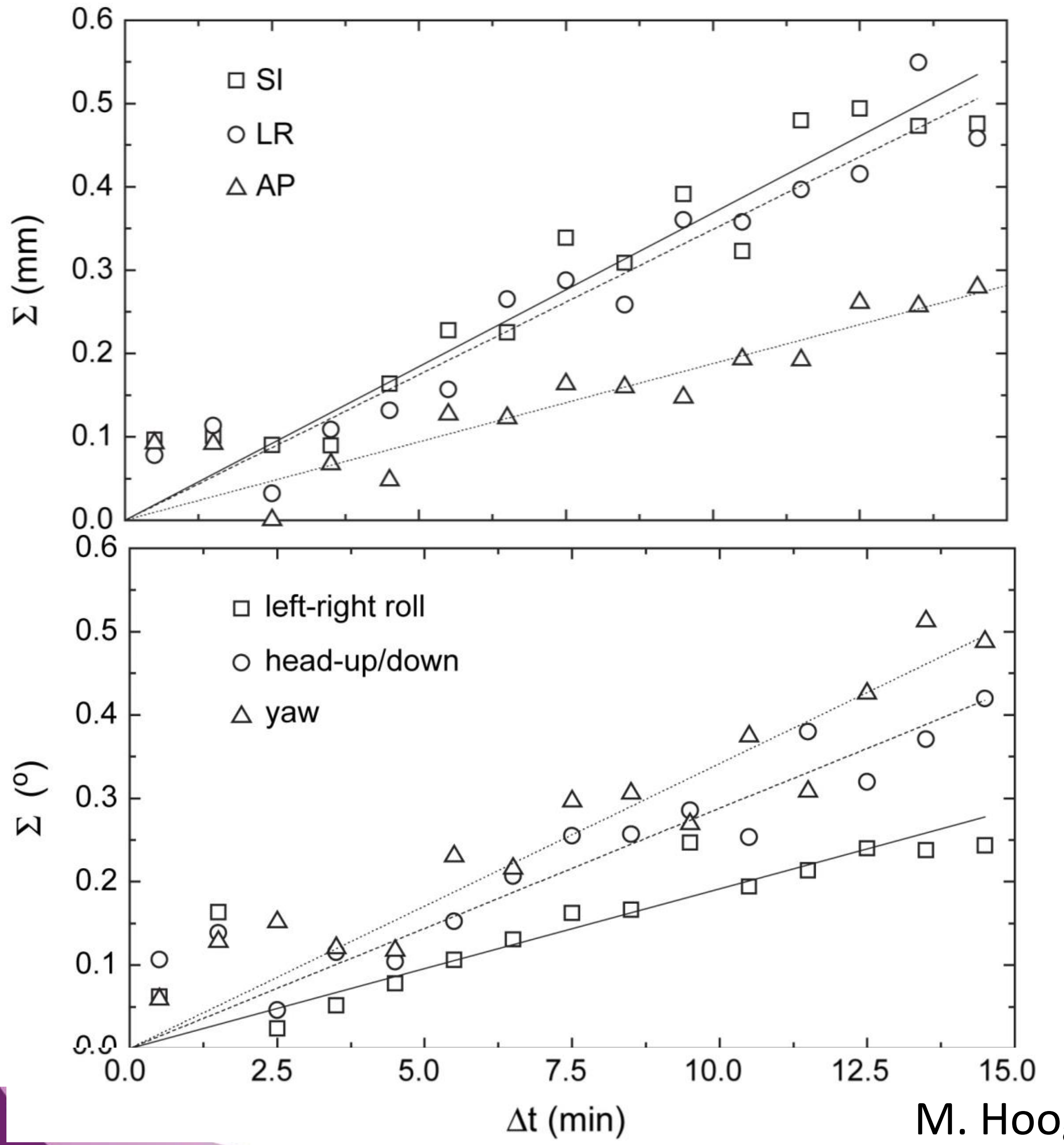
→ How stable is a mask?

Study	Immobilisation system	Imaging modality	Position error
Boda Heggeman 2006	Thermoplastic mask	CBCT	1.8mm ± 0.7mm1.3mm
	Scotsch cast mask		1.3mm ± 1.4mm
Masi 2008	Thermoplasic mask & Bite block	CBCT	<1.0mm
	Bite block		<1.0mm
Lamda 2009	BrainLab mask	2D kV images	0.5mm ± 0.3mm
Ramakrishna 2010	BrainLab mask	2D kV images	0.7mm ± 0.5mm
Guckenberger 2007	Scotsch cast mask	CBCT	0.8mm ± 0.4mm
	Thermoplastic mask		0.8mm ± 0.5mm

Courtesy M. Guckenberger, ESTRO IGRT course

Correcting Patient position

→ How stable is a mask?



- 32 intracranial patients
- Cyberknife @ Rotterdam
- immobilized with a thermoplastic mask

Keep total treatment time as short as possible!

M. Hoogeman 2008

Margins for small leasions hypo fractionated

Adding up some/al the errors:

Delineation uncertainty	2 mm
Residual set up error after imaging (2D or 3D)	
• bone registration	0.5 mm
• soft tissue changes	0.6 mm
Intrafraction motion	0.6 mm

PTV margin = 2.5 Σ + 0.7 σ

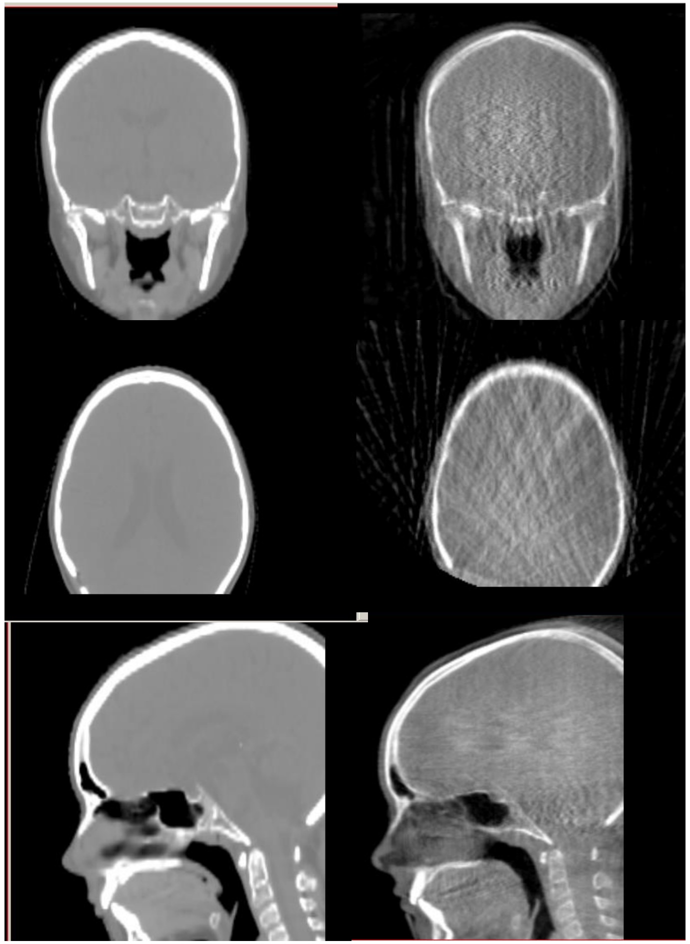
→ ***1mm margin/ 0mm margin??***

Literature show excellent local control!

Imaging dose

→ Can we reduce dose for children?

100%, (0.5rpm) 8%



Lowest exposure settings

10ms & 10mA per projection

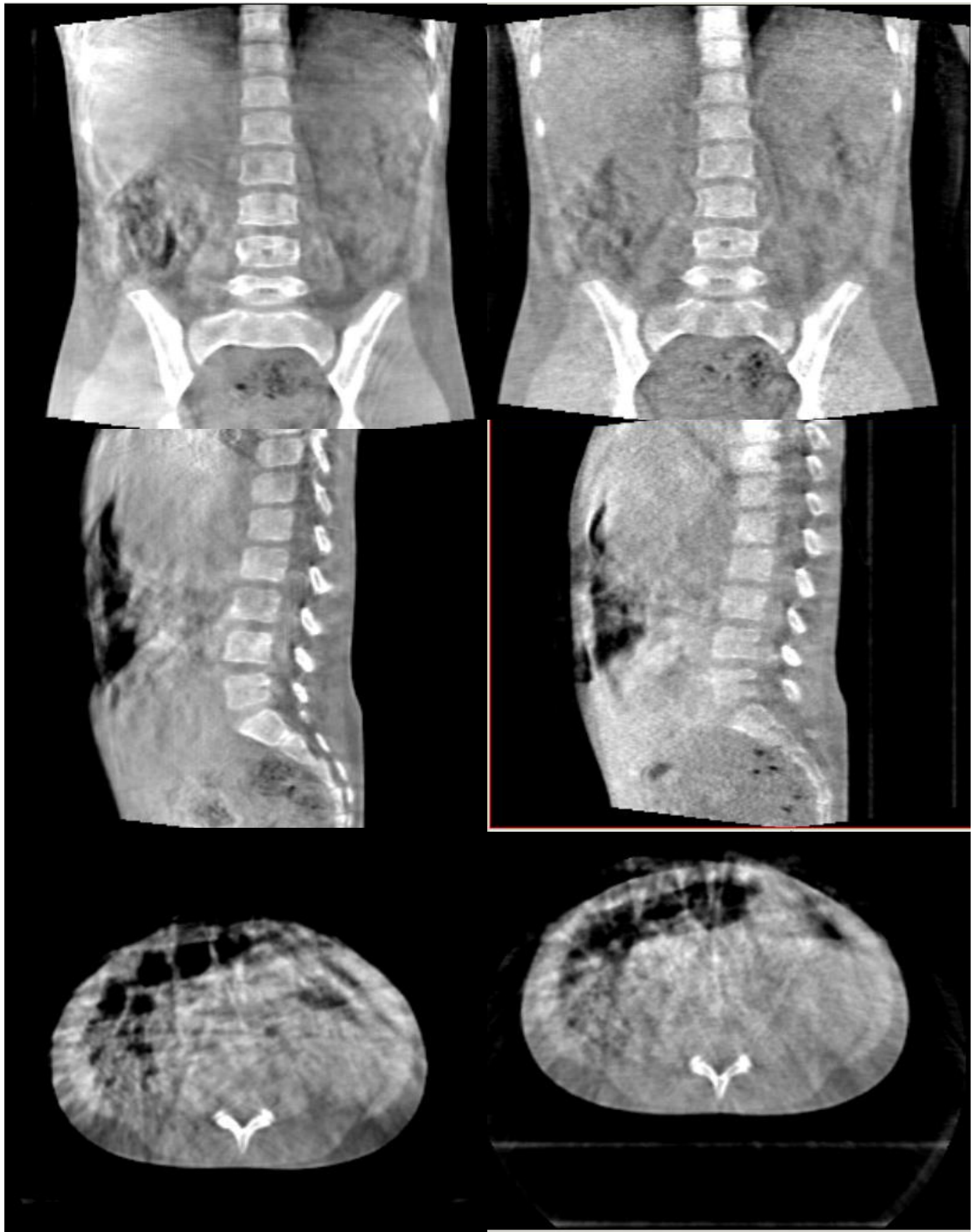
Using 'slice averaging' for display

	maximum deviation in outcome of registration			
	bony algorithm		grey value algorithm	
	translations (cm)	rotations (°)	translations (cm)	rotations (°)
skull	0.03	0.2	0.05	0.6
thoracic region	0.03	0.4	0.03	0.5
lumbar region	0.02	0.4	0.03	0.5

Imaging dose

→ Can we reduce dose for children?

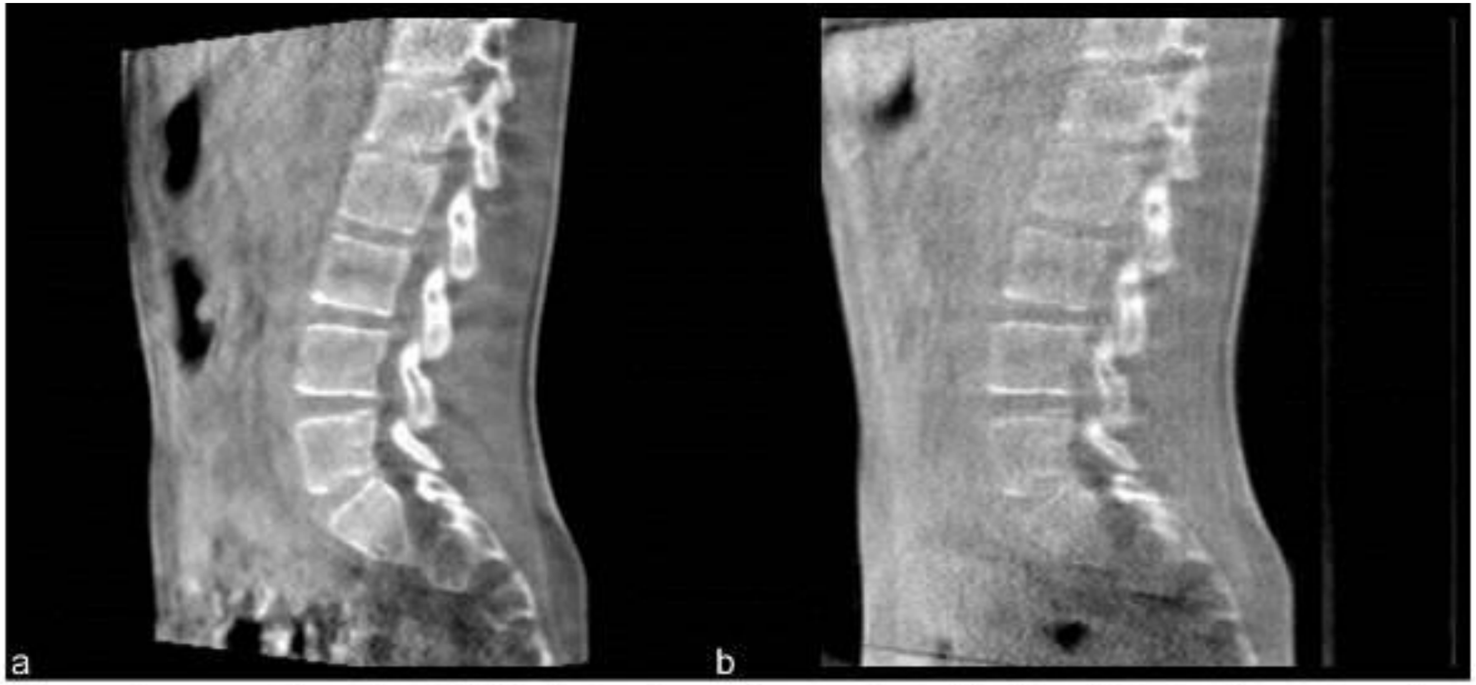
Adult exposure
40ms, 32mA



Kids exposure
10ms, 10mA

Imaging dose

→ Can we reduce dose for children?



40ms, 32mA, 0.5 rpm
Display using slice averaging

10ms, 10mA, 1.0 rpm
Display using slice averaging

5%

Case report: **Head and Neck**

ESTRO School

Jesper Eriksen, Odense University hospital, Denmark
Sofia Rivera, Gustave Roussy, Villejuif, France

Advanced skills in modern radiotherapy
June 2017

FALCON
Fellowship in Anatomic deLineation & CONtouring

WWW.ESTRO.ORG/SCHOOL

Changing traditional scenario in H&N cancer

- Increasing incidence of HPV positive tumors (+++ Oral Cavity)
- Improved outcome compared with HPV-negative tumors
- younger patients with limited comorbidity and good performance status, less likely to abuse tobacco and alcohol

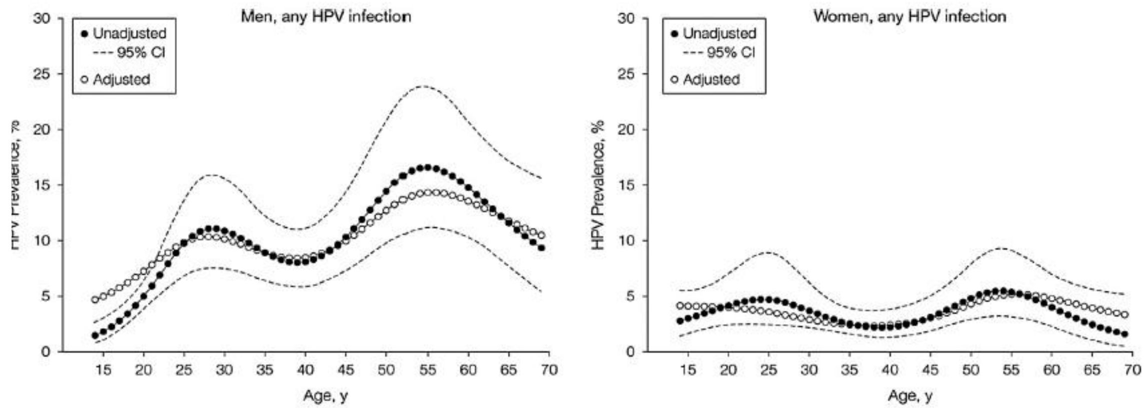
Epidemiology of oral human papillomavirus infection

Christine H. Chung [a,b], Ashley Bagheri [a], Gypsyamber D'Souza [c,*]

[a] Department of Oncology, Johns Hopkins Medical Institute, Baltimore, MD, United States
[b] Department of Otolaryngology, Head and Neck Surgery, Sidney Kimmel Comprehensive Cancer Center, Johns Hopkins Medical Institute, Baltimore, MD, United States
[c] Department of Epidemiology, Johns Hopkins Bloomberg School of Public Health, Baltimore, MD, United States

S U M M A R Y

Objective: To describe what is known about the epidemiology of oral human papillomavirus (HPV) infection.
Methods: In this article we review current data on HPV prevalence, natural history, mode of acquisition, and risk factors for oral HPV infection.
Results & Conclusion: Over the past several years new studies have informed our understanding of oral HPV infection. These data suggest oral HPV prevalence is higher in men than women and support the sexual transmission of HPV to the mouth by oral sex. Data is emerging suggesting that most oral HPV infections usually clear within a year on and describing risk factors for prevalent and persistent infection. Recent data support likely efficacy of the HPV vaccine for oral HPV, suggesting vaccination may reduce risk of HPV-related oropharyngeal cancer.



Lassen et al ;Radiother oncol 2013
Chung et al; oral oncol 2013

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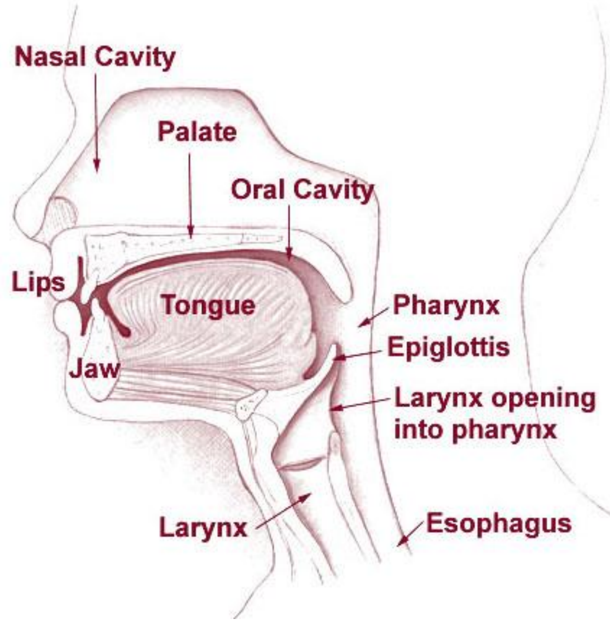
Patient history



- 60-year old man.
- 3 week history of nodal swelling , left side of the neck.
- No pain or dysphagia. No weight loss.
- No co-morbidity except from back pain.
- Ceased smoking in 1990, 10 pack-years.
- No daily use of alcohol.

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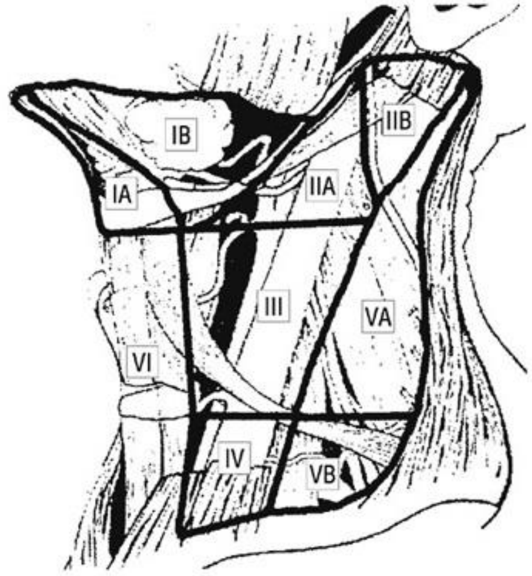
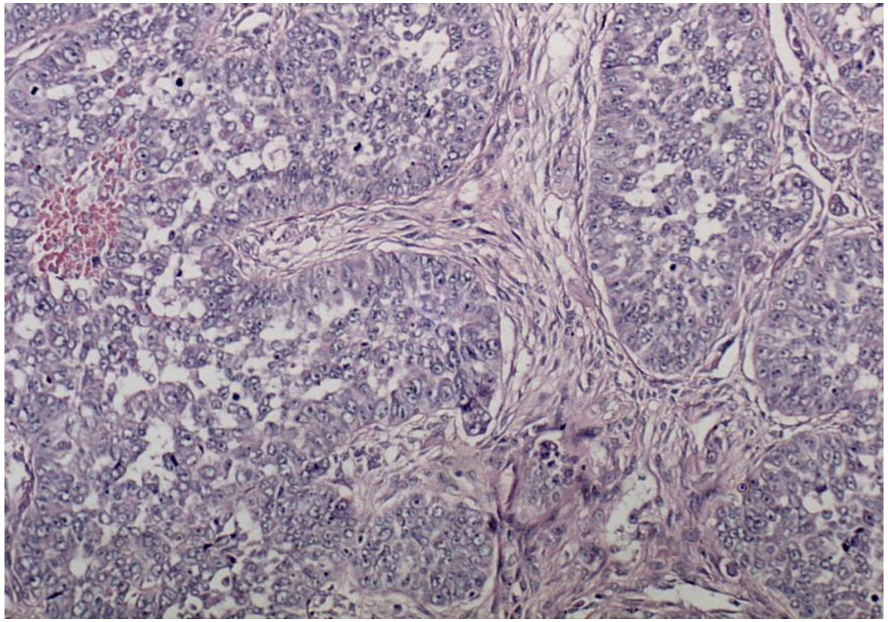
Clinical examination

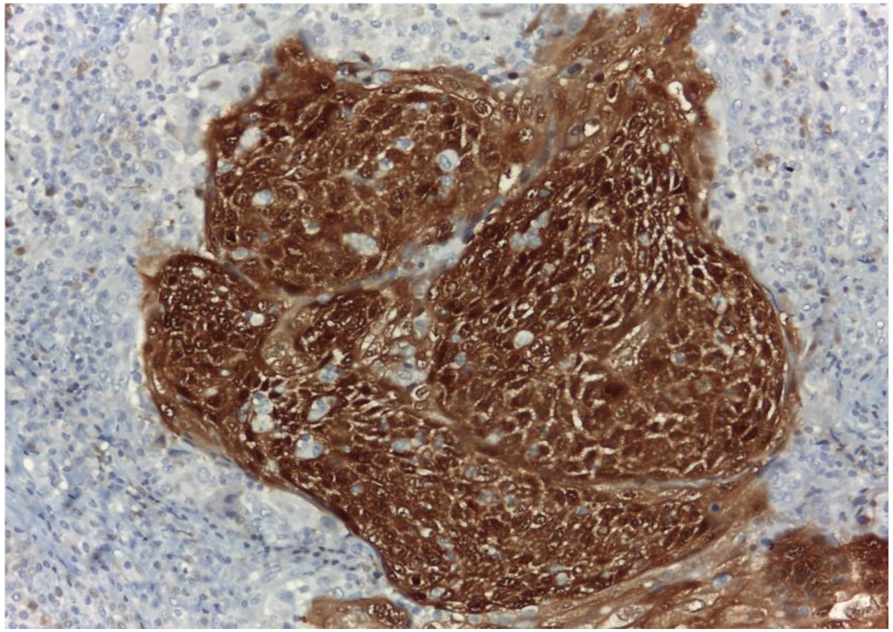


- Good performance (WHO PS 0)
- Base of tongue/vallecula area a 3x2x2cm large tumour is seen.
- Proximal border of the tumour seems to be close to the lower pole of the left tonsil
- Otherwise normal fiber optic examination.
- Palpable node in region II, left side.
- Contralateral side normal.

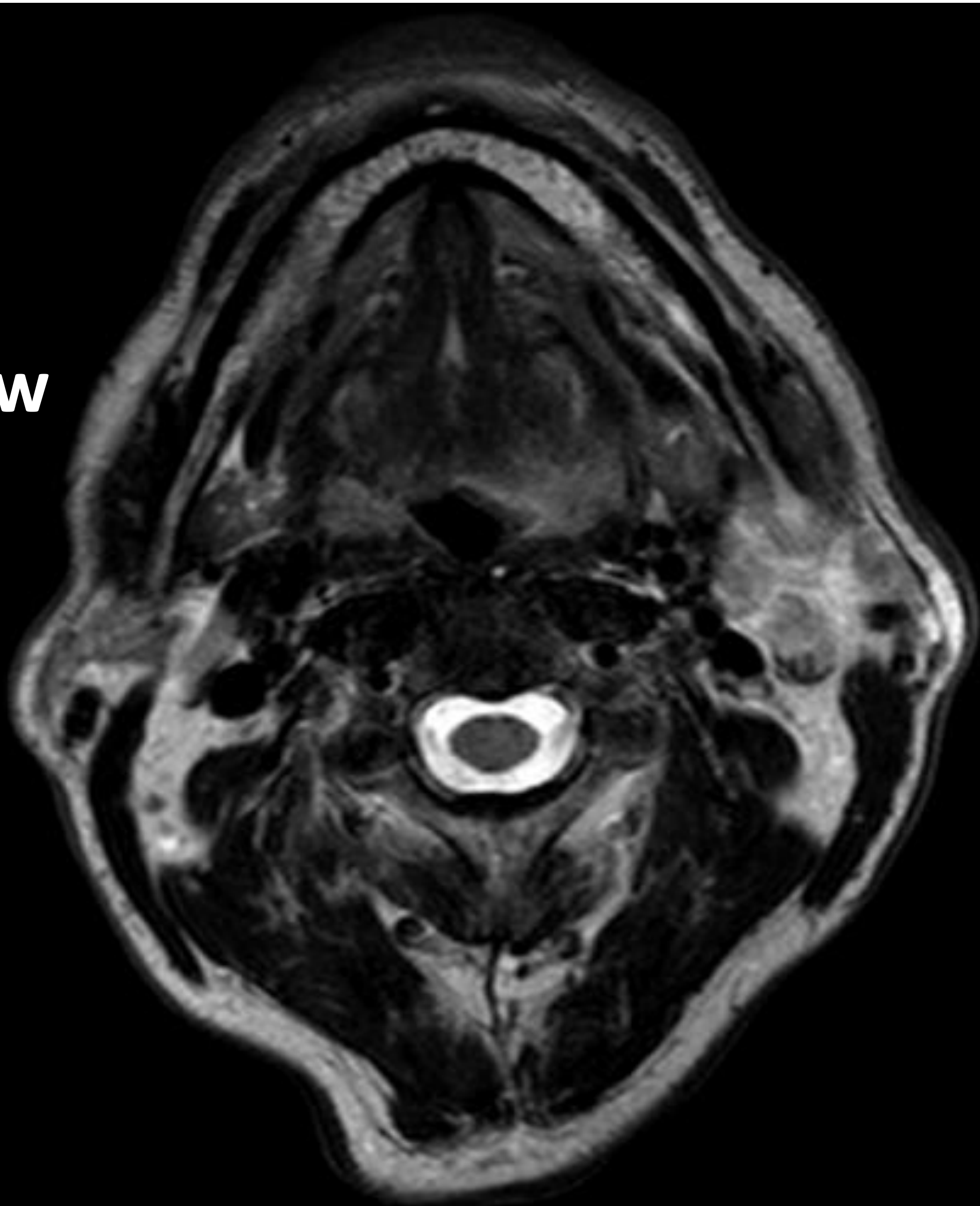
Pathology

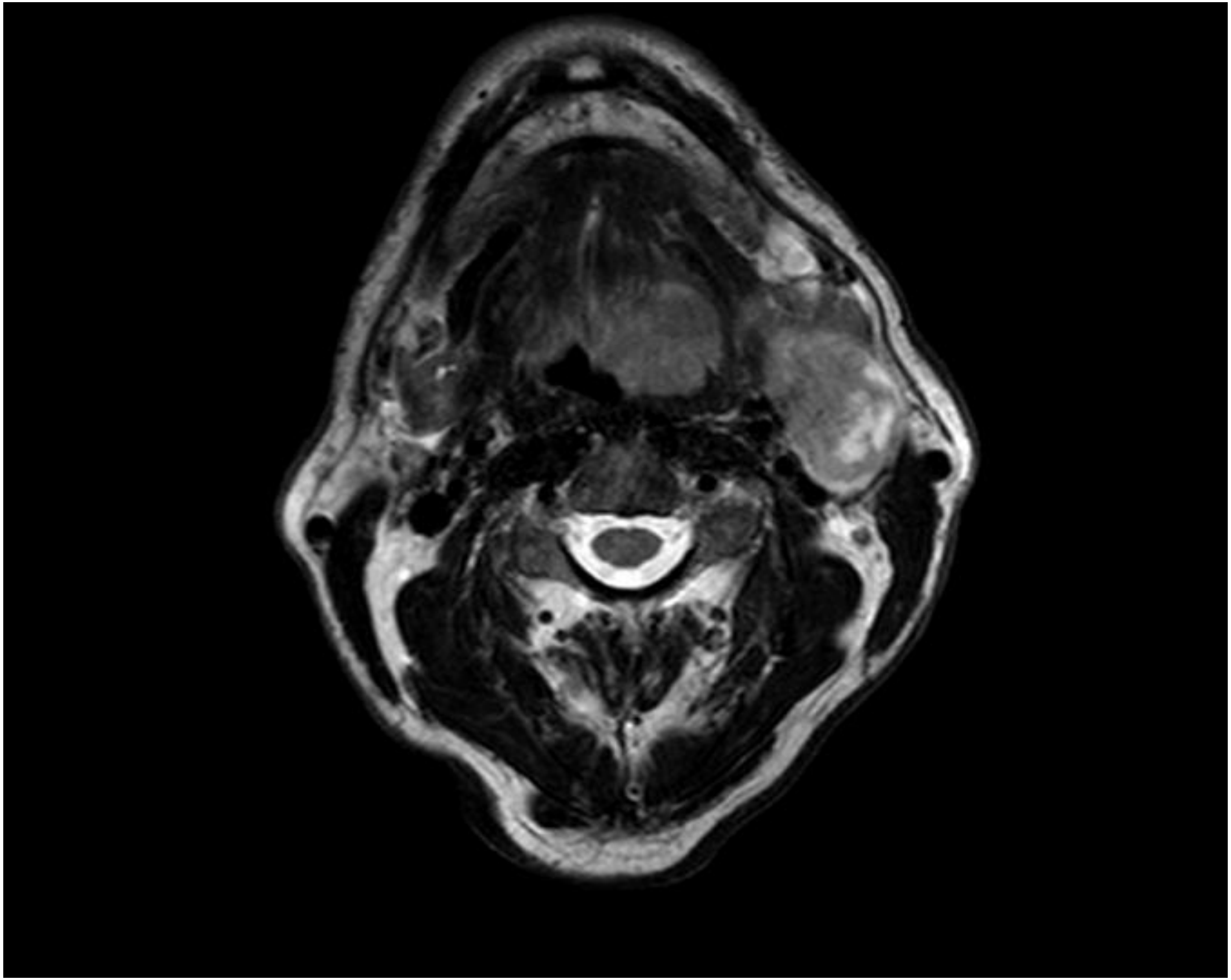
- Moderate differentiated squamous cell carcinoma (G2).
- p16 positive (HPV marker)

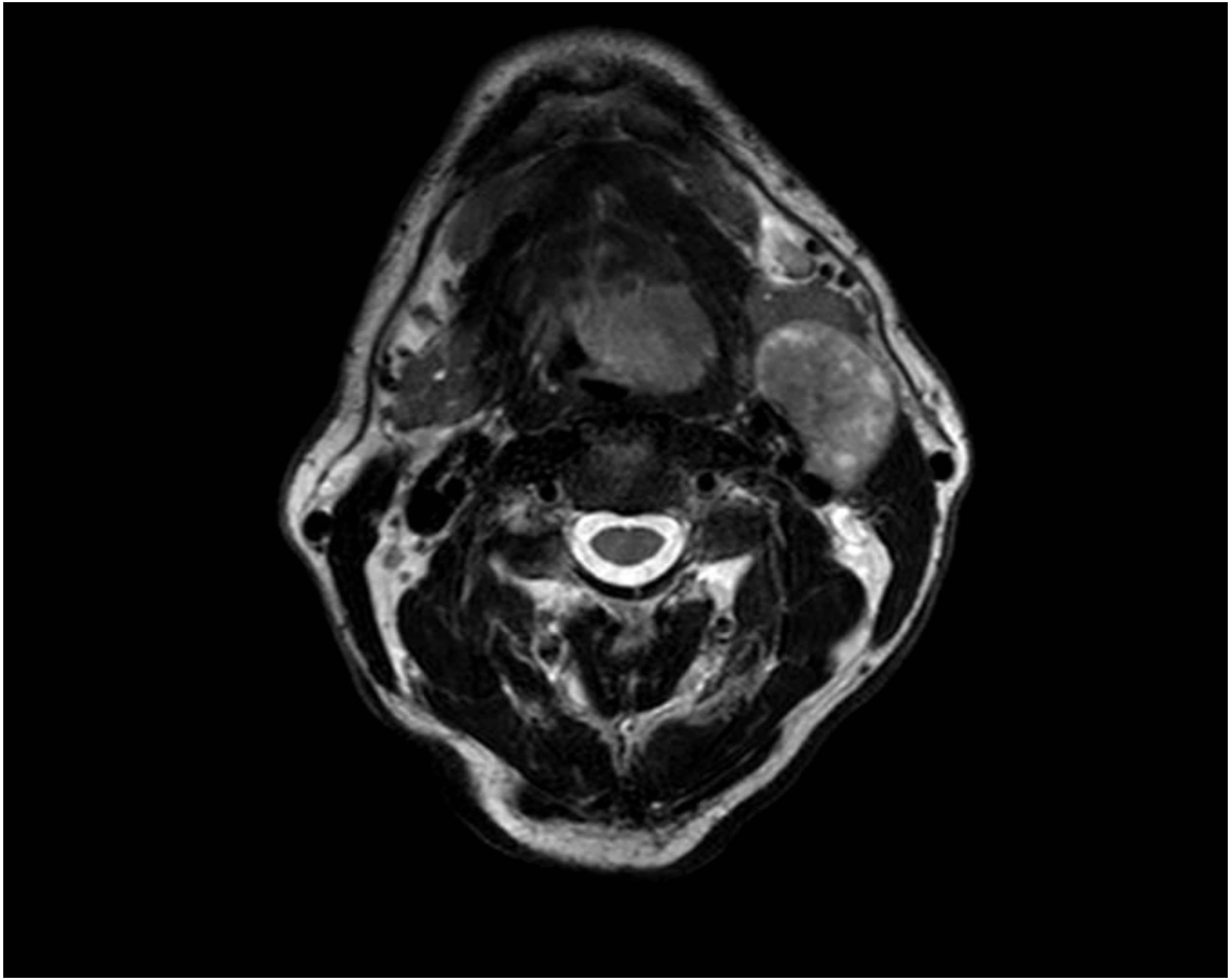


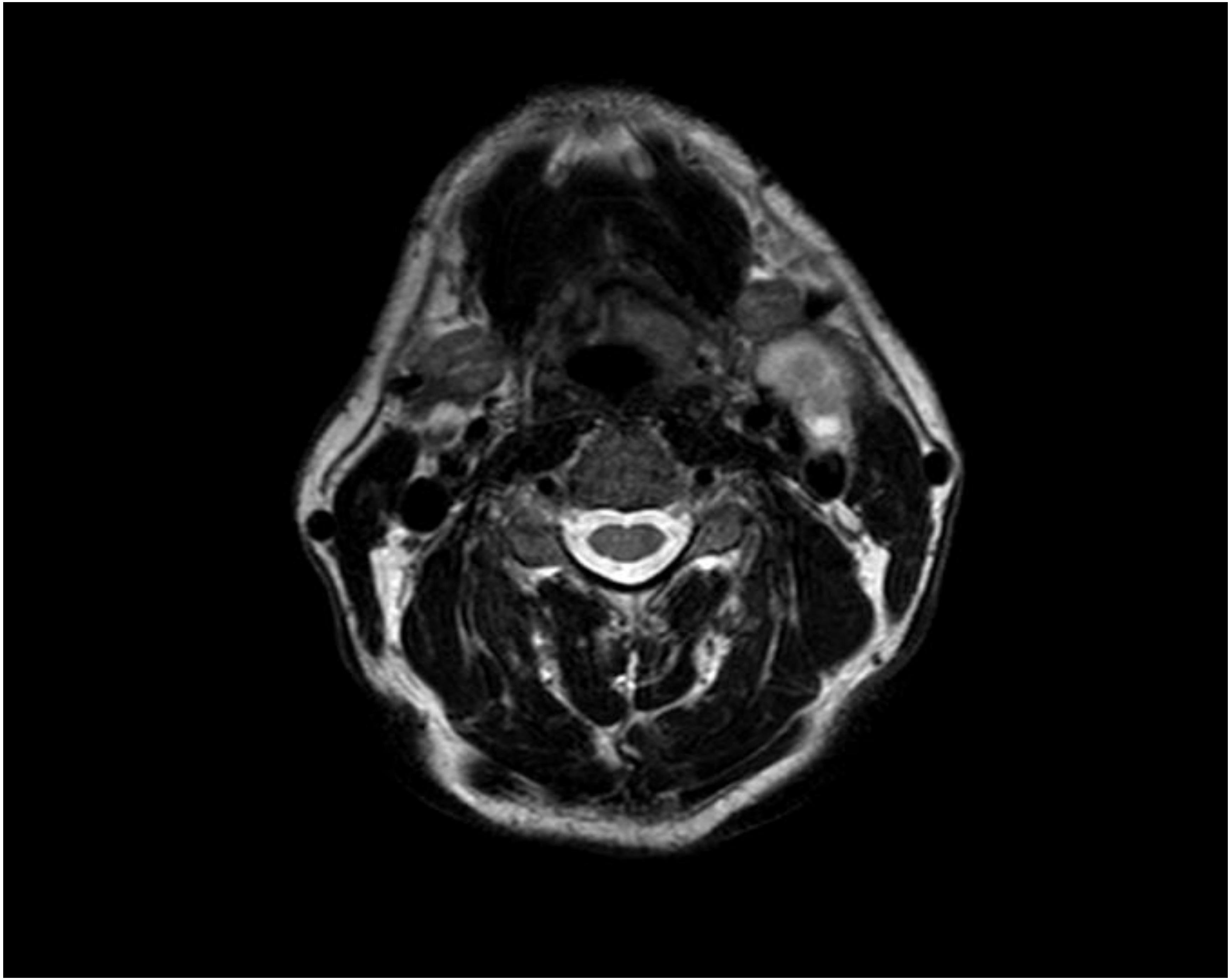


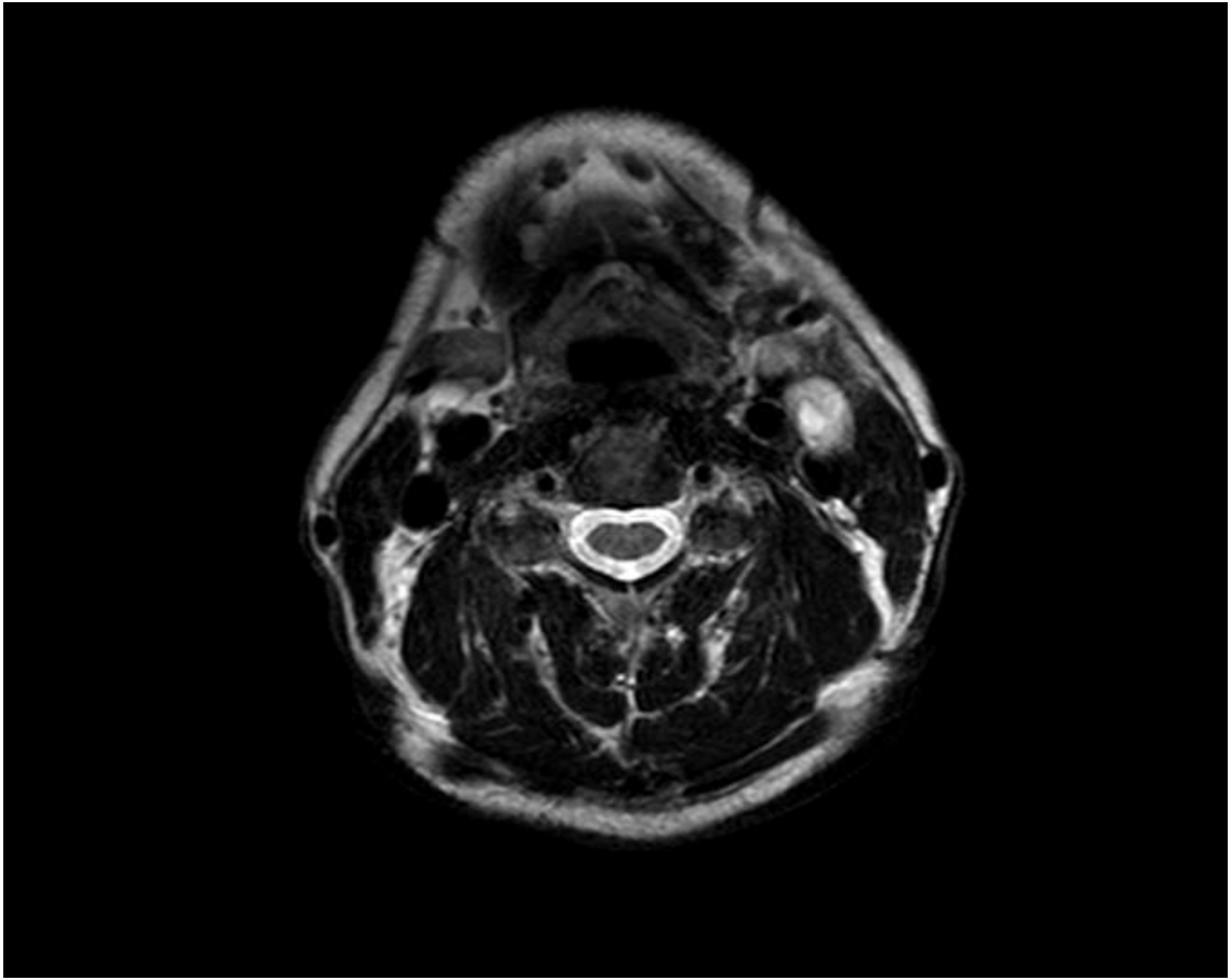
MR
Axial view

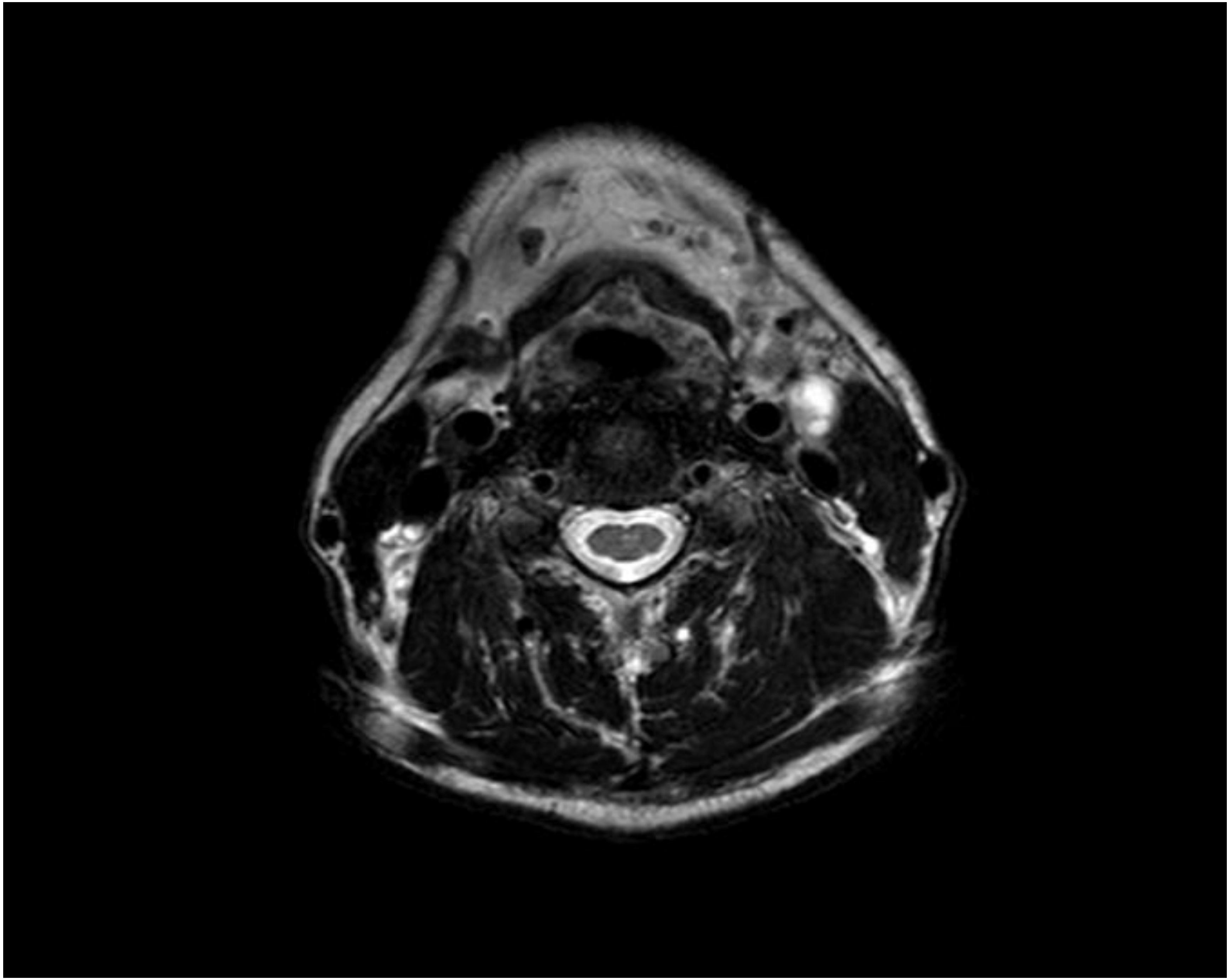


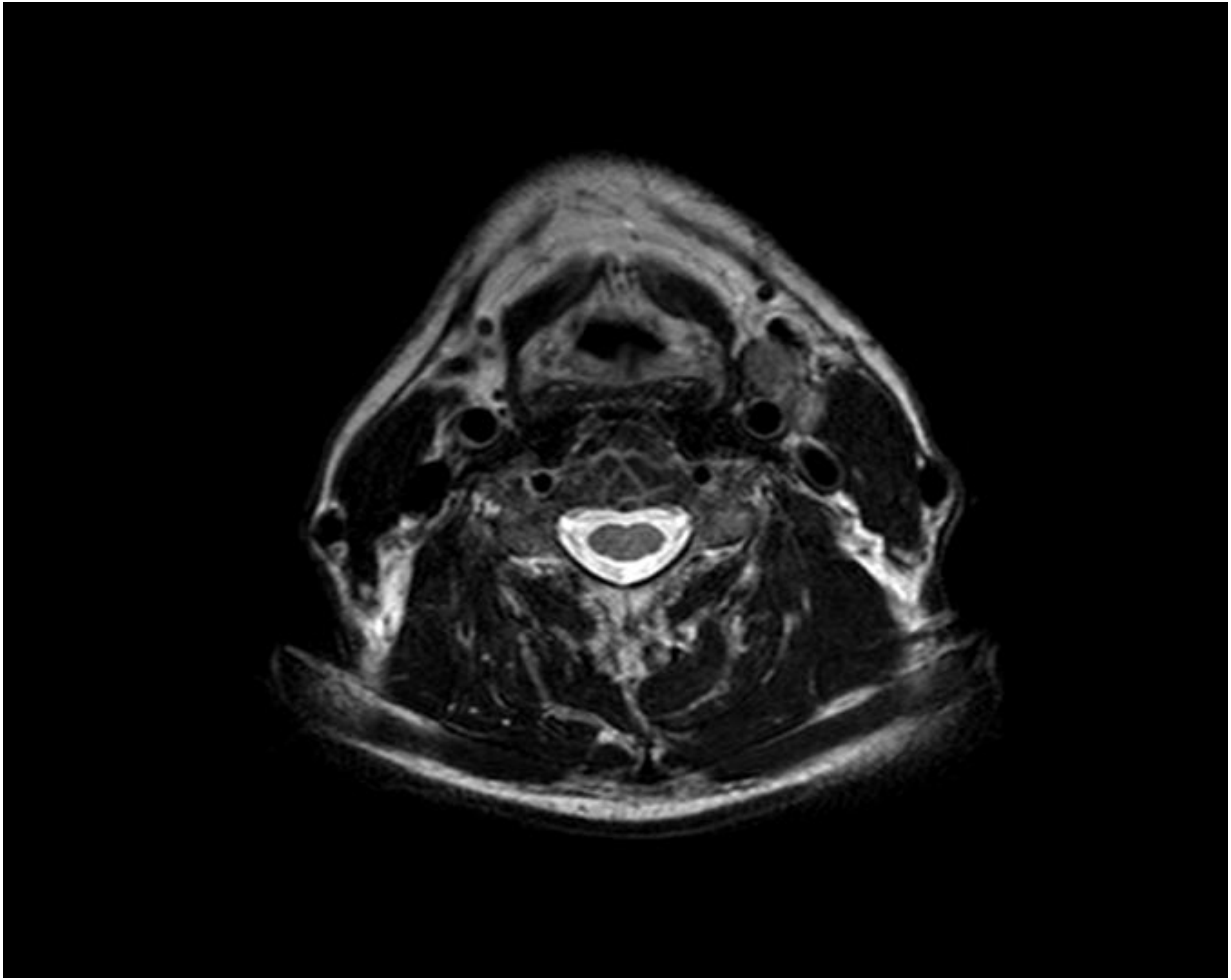




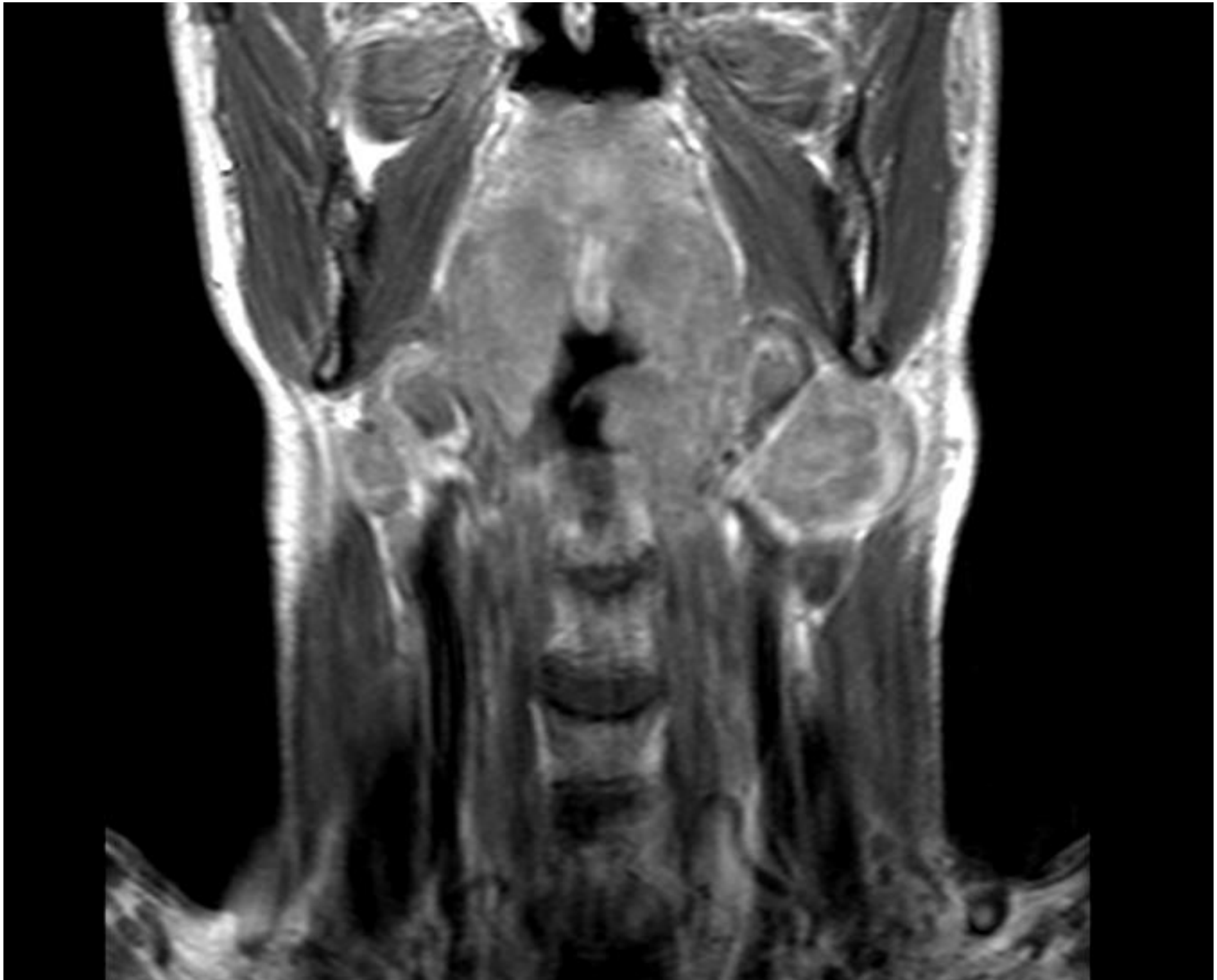


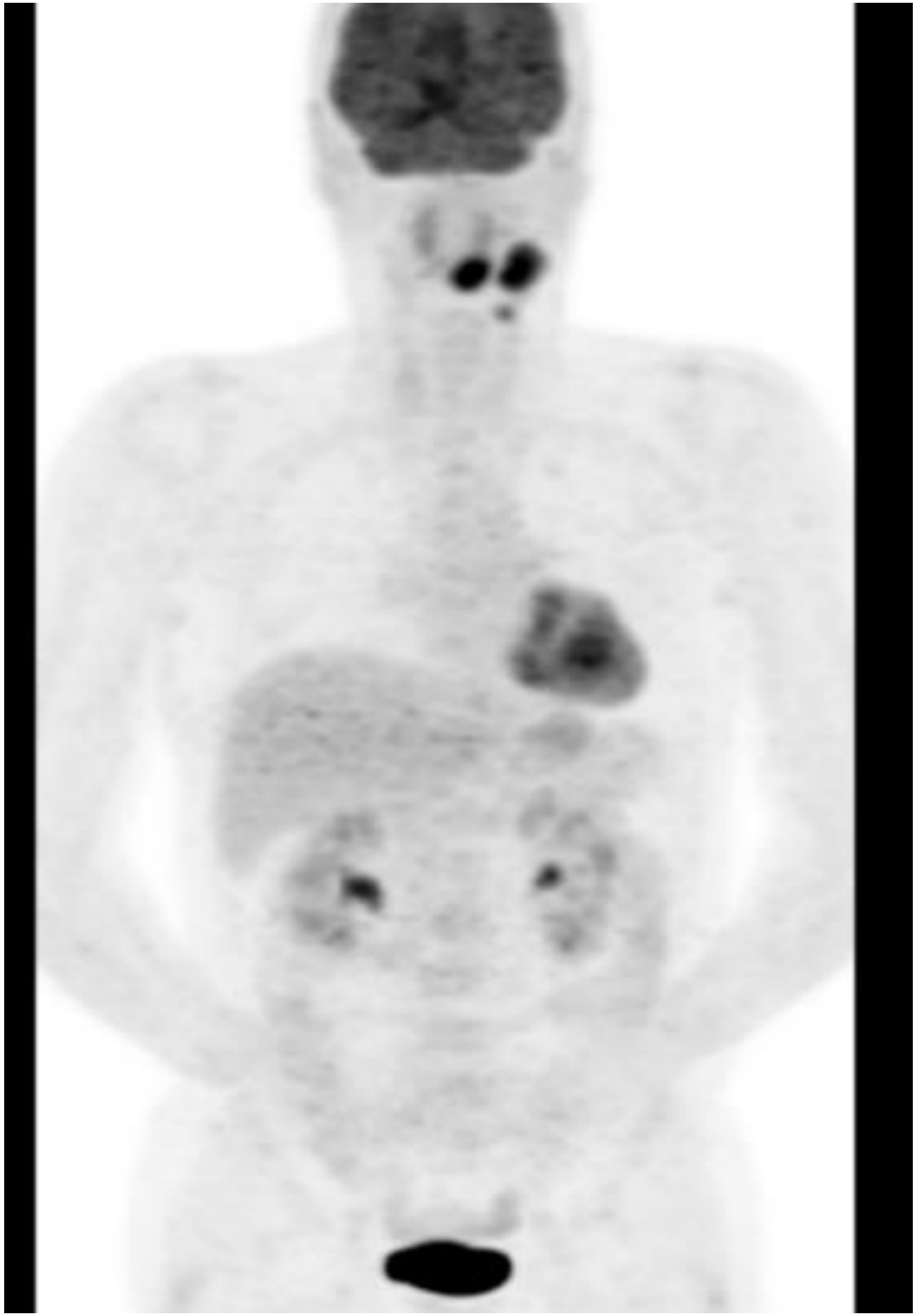


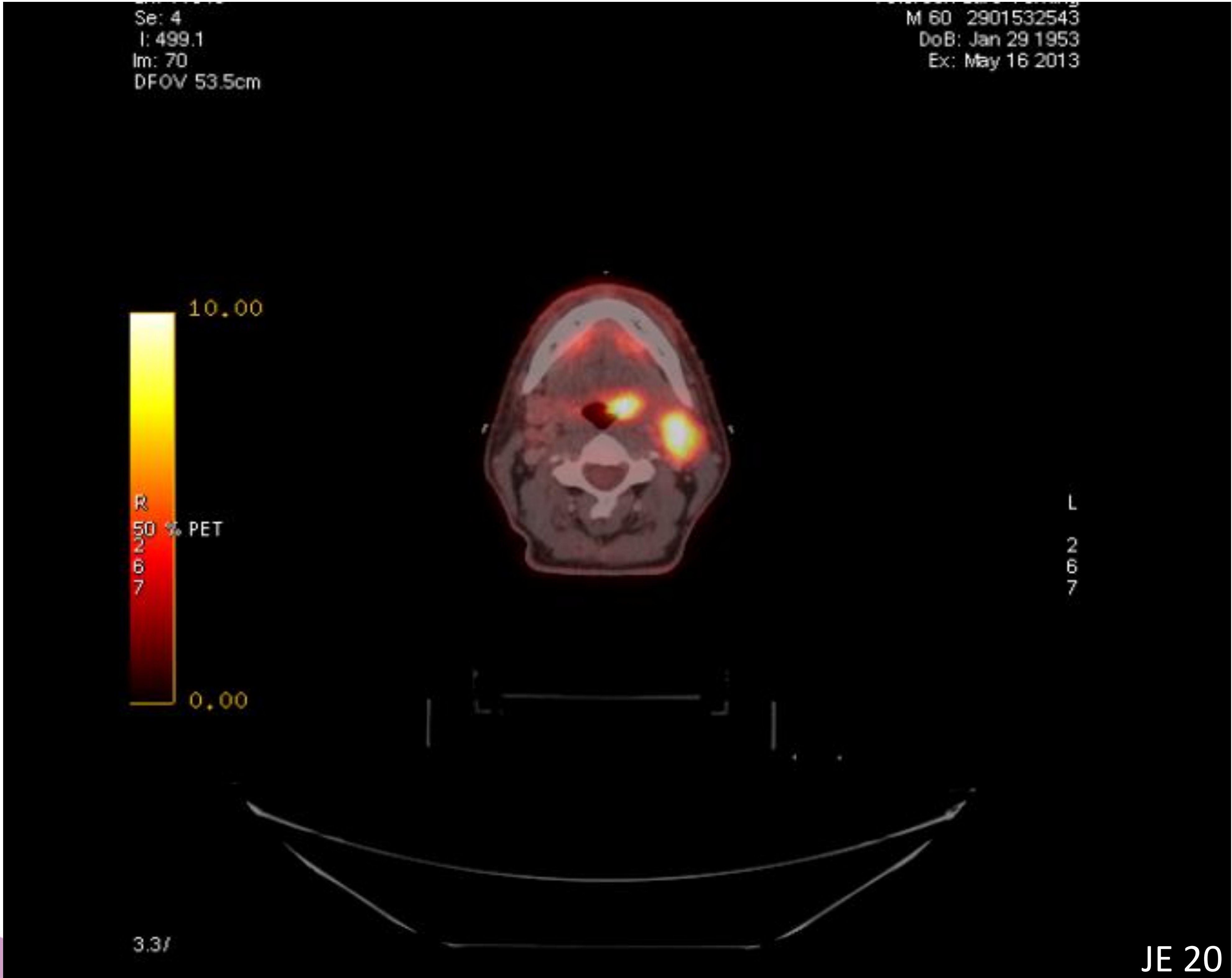





MR
Coronal view







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Im: 70
DFOV 53.5cm
M 60 2901532543
DoB: Jan 29 1953
Ex: May 16 2013
10.00
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50 % PET
2
6
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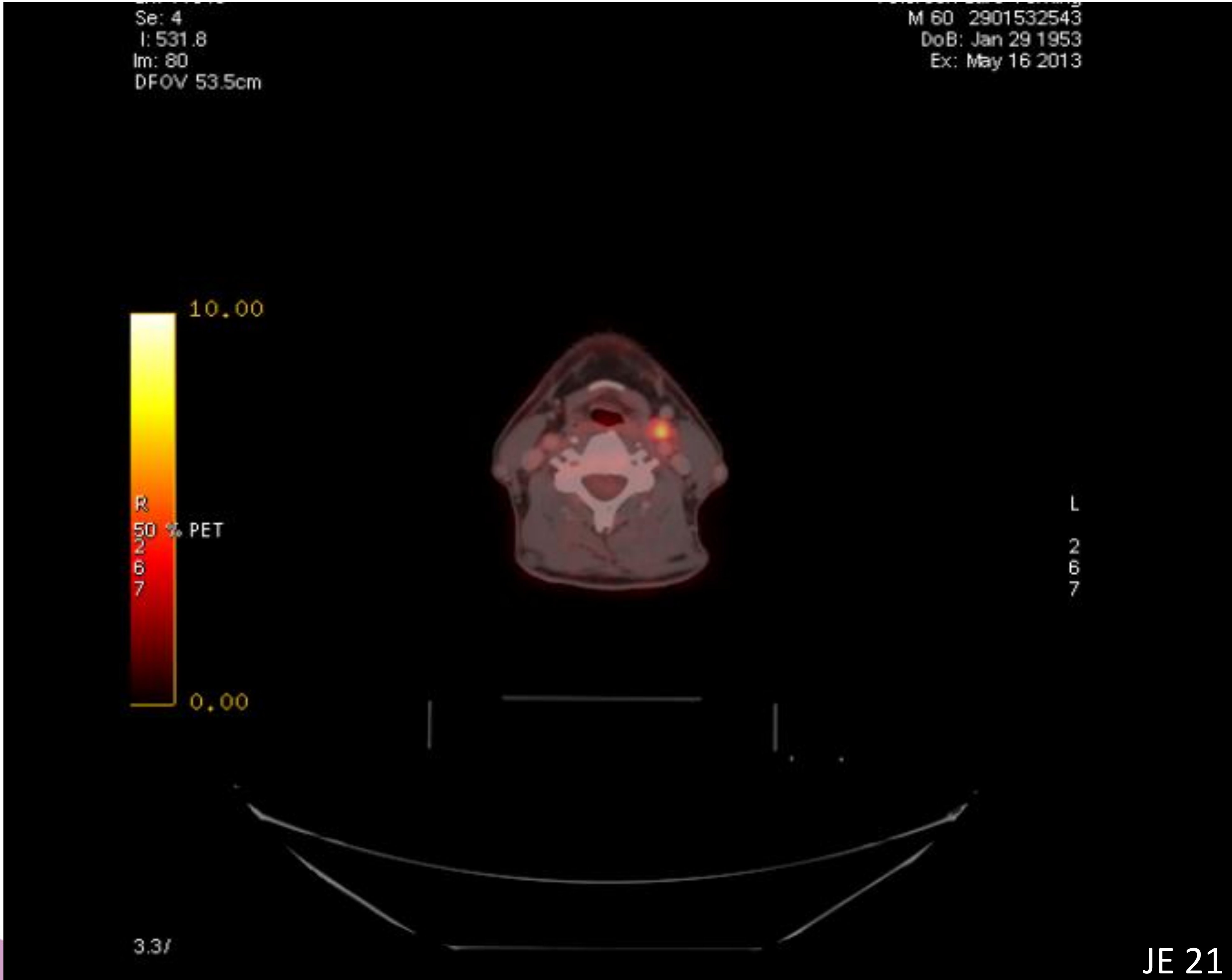
3.3/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Im: 80
DFOV 53.5cm
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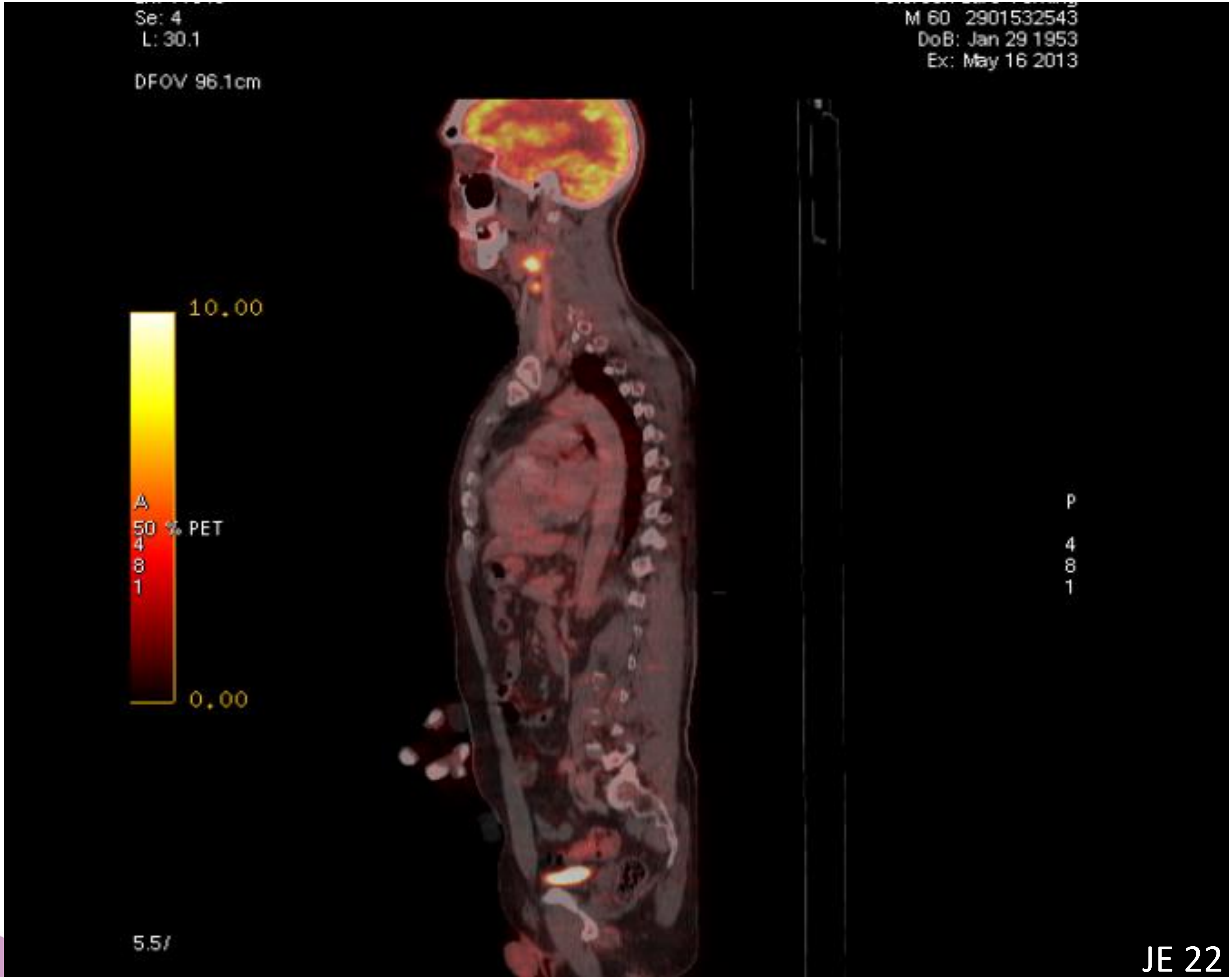
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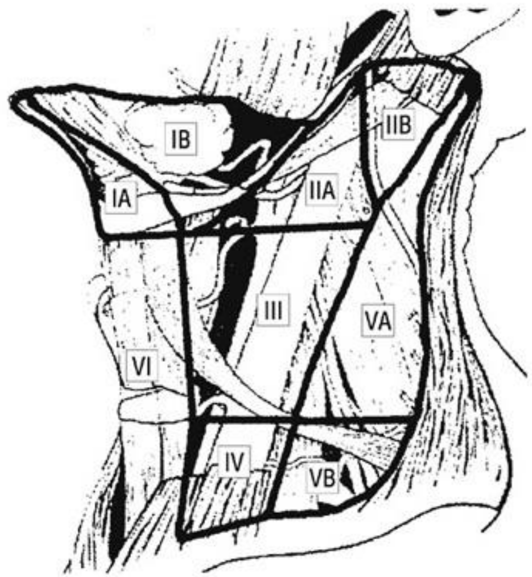
L: 30.1
DFOV 96.1cm
M 60 2901532543
DoB: Jan 29 1953
Ex: May 16 2013
10.00
A
50 % PET
4
8
1
0.00
P
4
8
1
5.5/

JE 22

Ultrasound of neck

- One necrotic node in the upper part of left region II close to the submandibular gland; 3.5x2x2 cm.
- One node in left region III, 1.5x1x1 cm without preserved hilar region.
- Right side of the neck is normal.



Conclusions after diagnostic workup

- T2N2bM0 (stage IVa) SCC oropharyngeal tumour.
- Patient in a good performance with no relevant co-morbidity.

Treatment done

- 66 Gy/33 Fx; 2 Gy/Fx; 6 Fx/week.
- Concomitant weekly low-dose cisplatinum 40 mg/m² (maximum 70 mg/m²).
- Concomitant hypoxic radiosensitization with nimorazole according to DAHANCA guidelines

Contouring guidelines

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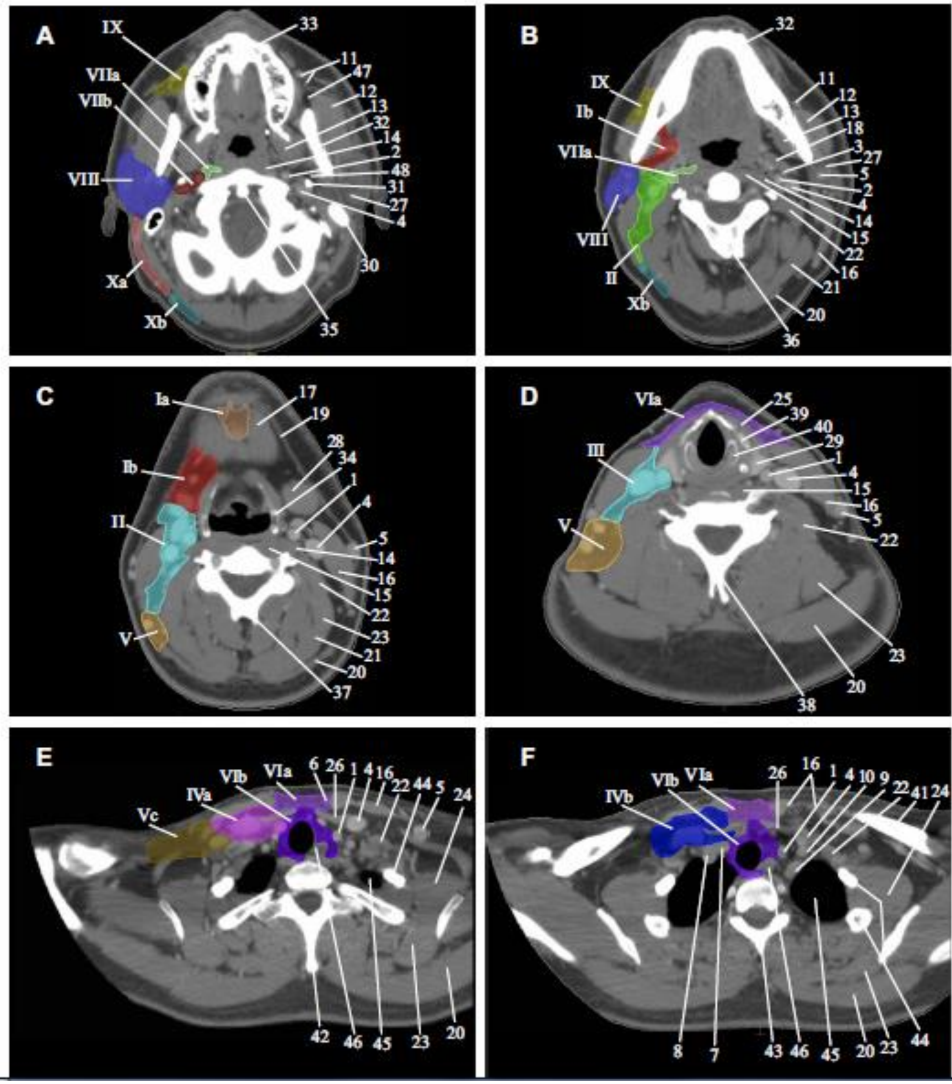
ELSEVIER

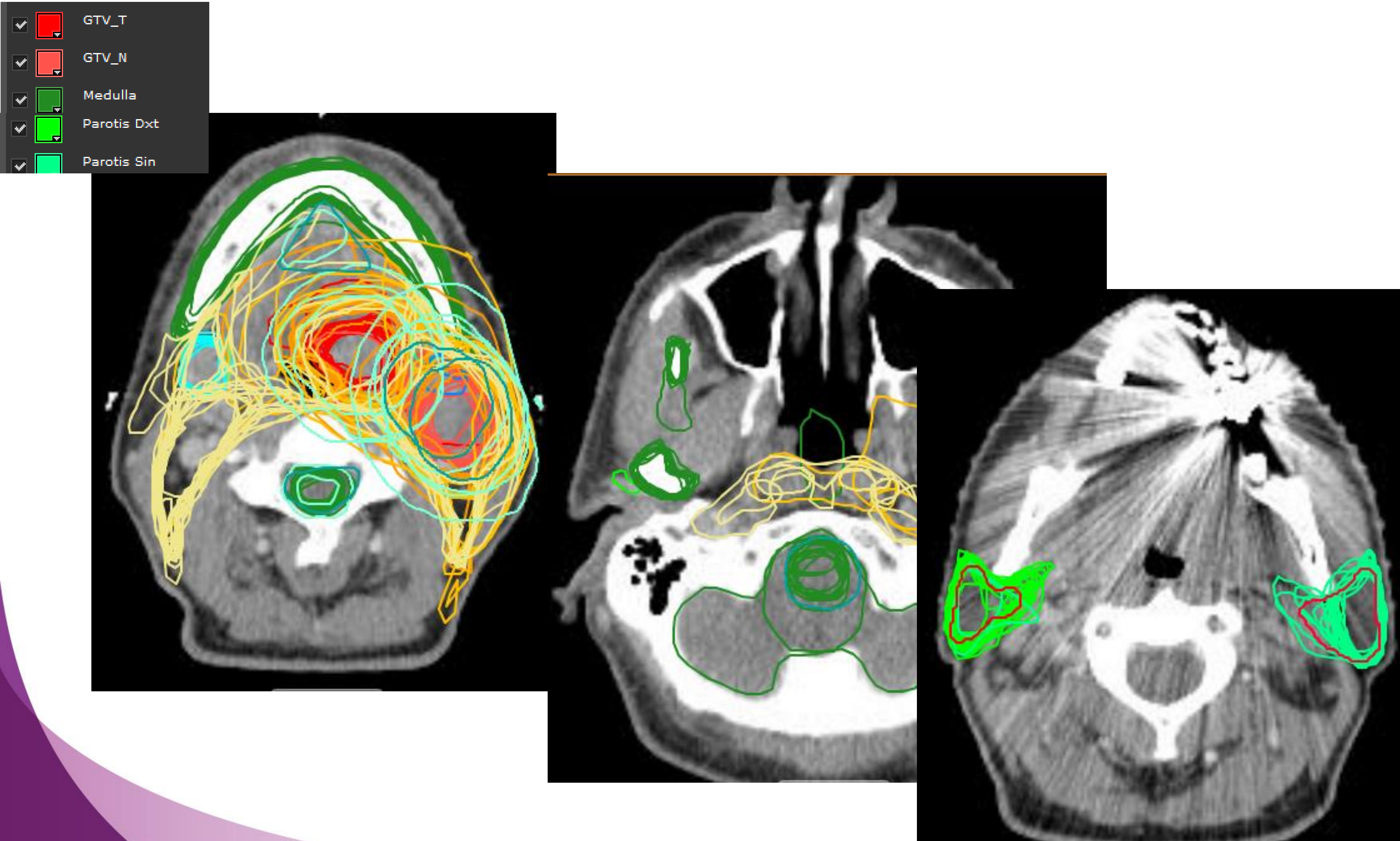
Original article

Delineation of the neck node levels for head and neck tumors: A 2013 update. DAHANCA, EORTC, HKNPCSG, NCIC CTG, NCRI, RTOG, TROG consensus guidelines ☆

Vincent Grégoire [a,*], Kian Ang [b], Wilfried Budach [c], Cai Grau [d], Marc Hamoir [e], Johannes A. Langendijk [f], Anne Lee [g], Quynh-Thu Le [h,i], Philippe Maingon [j], Chris Nutting [k], Brian O'Sullivan [l], Sandro V. Porceddu [m], Benoit Lengele [n]



Case used for H&N Falcon online WS



Take home messages:

- HPV positive tumors are changing H&N cancer traditional scenario

- Positioning remain key points for these highly conformal treatments (IMRT+++)

- Target and OAR contouring remains an issue: Highly heterogeneous contours

- Crucial need for contouring guidelines and training

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H&N case – Physics considerations

Peter Remeijer

Head and neck

- Complex target volume (GTV, CTV, lymph nodes, PTV)

- Many organs at risk (OARs)
  - Spine
  - Brainstem
  - Salivary glands
  - …

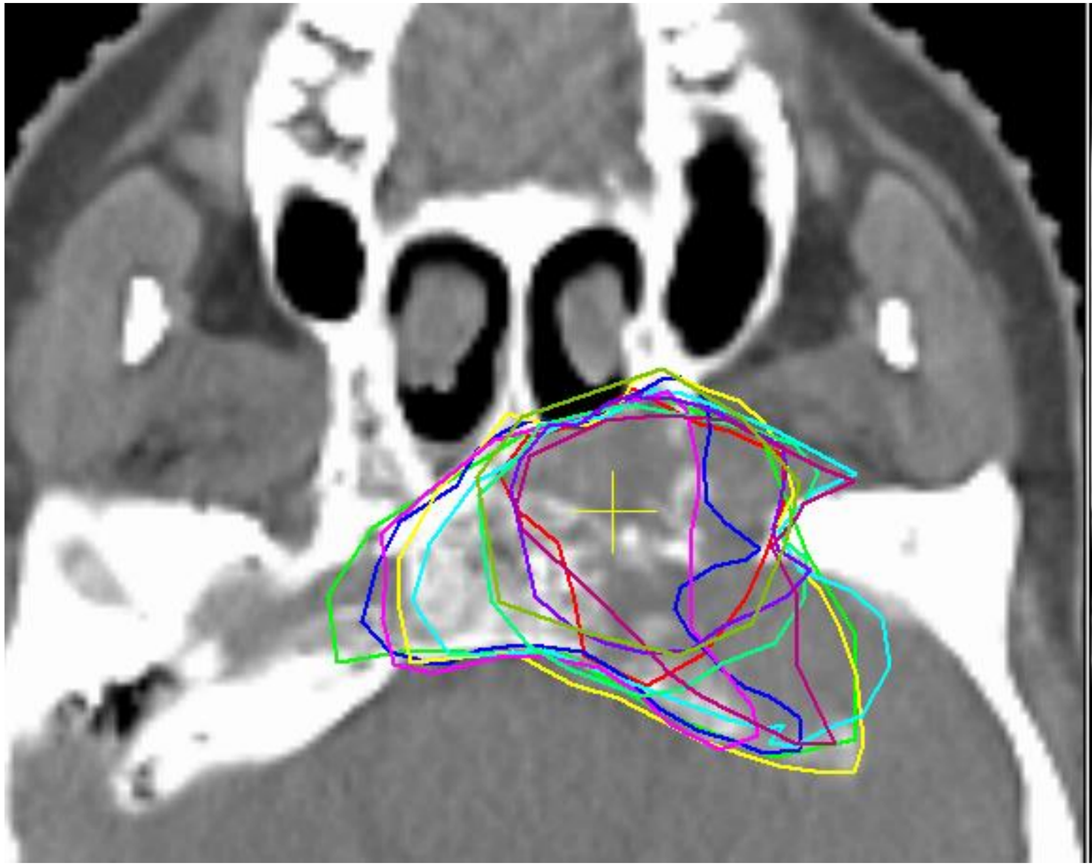
- OARs often close to PTV

Delineation and planning

- Multi-modality imaging (PET/MR) has a large impact on delineation uncertainties
- Image registration becomes important
- PET/MR scans preferably in treatment pose
  - Minimizes errors due to deformations

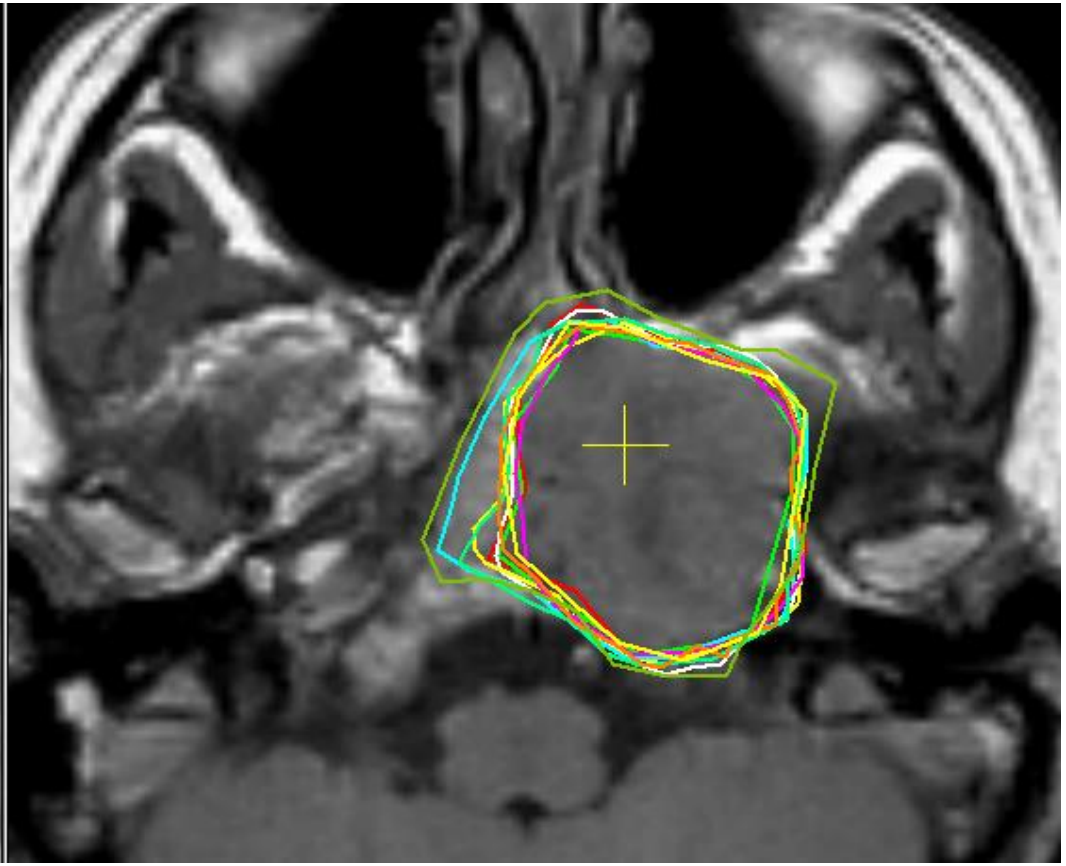
Mirada Medical - RTx Advanced 1.6 - Fusion and Contouring (1)
File Edit View Image Registration Quantify Tools Window Help Messages
Planning and MR and PET-CT
Layers
[1] tT1_TSE
27.9
398.4
Contouring Tools
Structures
Region 1 Series
clipbox oropharynx Series
50%suv Series
30%suv Series
40%suv Series
60%suv Series
70%suv Series
CTV Series
Image Gallery
Cine
MIRADA medical
KNO1
Scale 1:1.70 FOV 24.3 × 10.9cm
[1] W = 250.00 L = 50.00
Region 1
Volume 3020.4 cm³
Axial
Slice 70 / 140 (71) Z=-12 mm
27/11/2014
[1] Planning CT 11 HU
hals+supraclav +C 3.0 B40s PLAN (CT AXIAL)
Scale 1:3.95 FOV 56.4 × 25.2cm
Coronal
Slice 256 / 512 (71)
Sagittal
Slice 256 / 512 (71)
[1] W = 370.48 L = 213.19
Region 1
Slice 16 / 34 (16) Z=-58.6 mm
[1] MR 71 US
tT1_TSE
Slice 287 / 512 (16)
Slice 242 / 512 (16)
[1] W = 350.00 L = 35.00
Volume 3021.9 cm³
Slice 87 / 185 (87) Z=381 mm
13/11/2014
[1] CT 27 HU
HN Low Dose CT (CT HELIX, AXIAL)
Slice 243 / 512 (87)
Slice 250 / 512 (87)
Slice 81 / 174 (81) Z=381.1 mm
[1] PET -/-
[HN_CTAC] PET KNO (PET AC)
Slice 137 / 288 (81)
Slice 141 / 288 (81)

Multiple modalities improve H&N delineation



CT

SD 4.4 mm



CT + MRI

SD 3.3 mm

Steenbakkers *et al*

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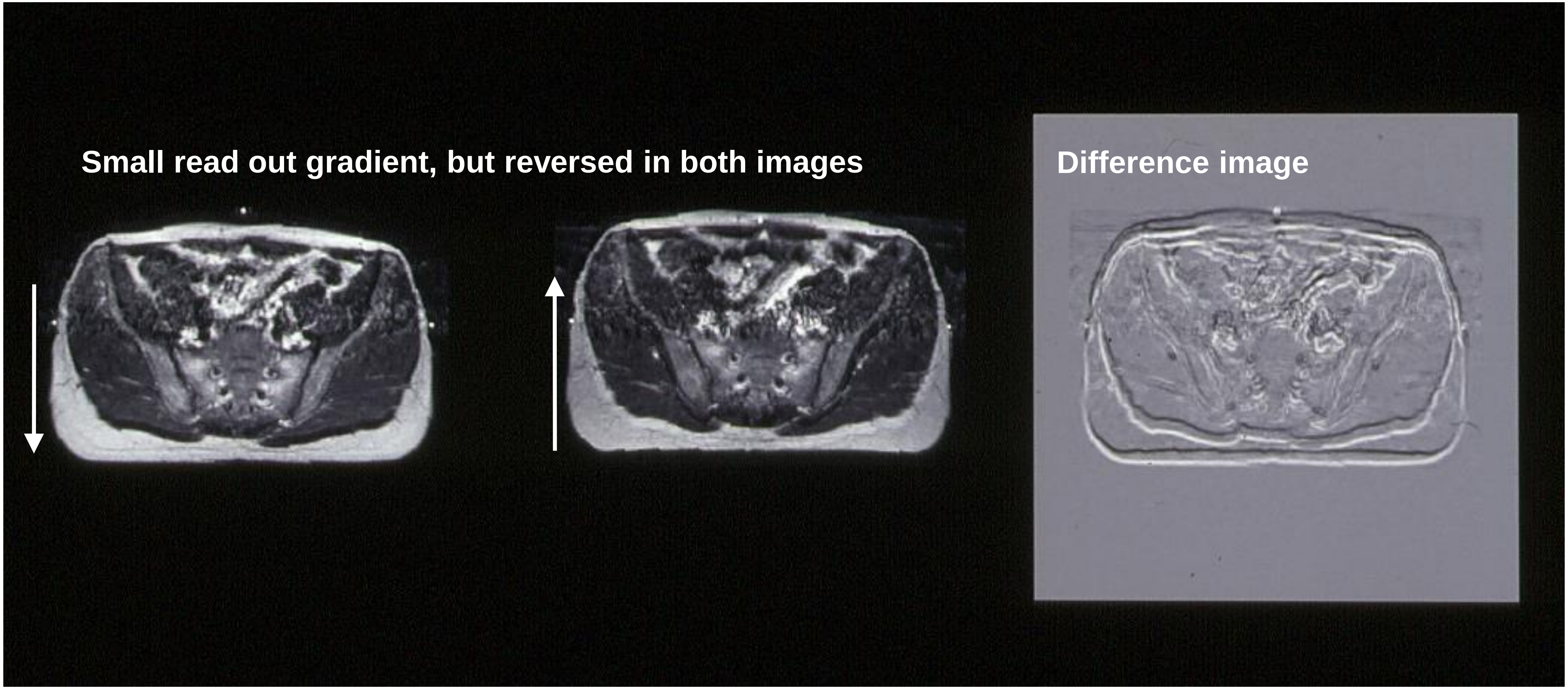
MRI artifacts can cause invisible geometrical errors!

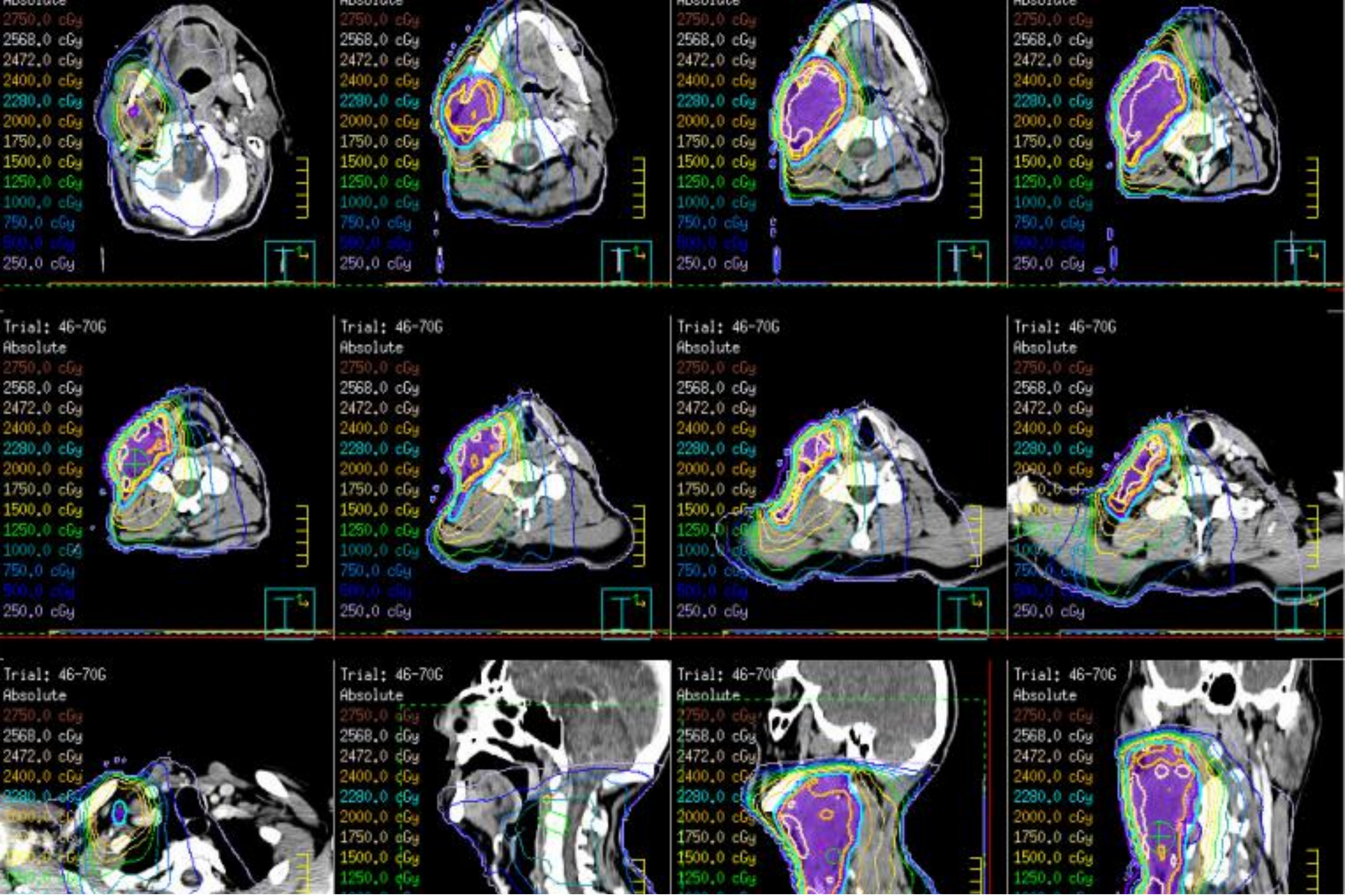


What you see is not always what you get

Courtesy U. van der Heide

Delineation and planning

- Multi-modality imaging (PET/MR) has a large impact on delineation uncertainties
- Image registration becomes important
- PET/MR scans preferably in treatment pose
  - Minimizes errors due to deformations
  - Focus on the main region of interest
- Planning: IMRT or VMAT



Complex planning techniques → Margin becomes more critical

Treatment - All is well?

# Patients	# Images	Direction	σ_{sys} (mm)	σ_{random} (mm)	Reference
31		ml cc ap	1.8 1.7 2.0	1.5 1.1 1.6	(Bel et al., 1995)
26	356	ml cc ap rot ant rot lat	1.8 2.7 1.7 1.2° 0.7°	1.6 1.5 1.2 0.8° 1.0°	(Vos et al., 1997)
12	192	cc ap	2.0 1.3	1.4 1.7	(Yan et al., 1997b)
12	290	ml cc ap	1.8 [a] 2.2 [a] 1.7 [a]	1.4 1.4 1.4	(Gildersleve et al., 1995)

Portal imaging data from a long time ago…

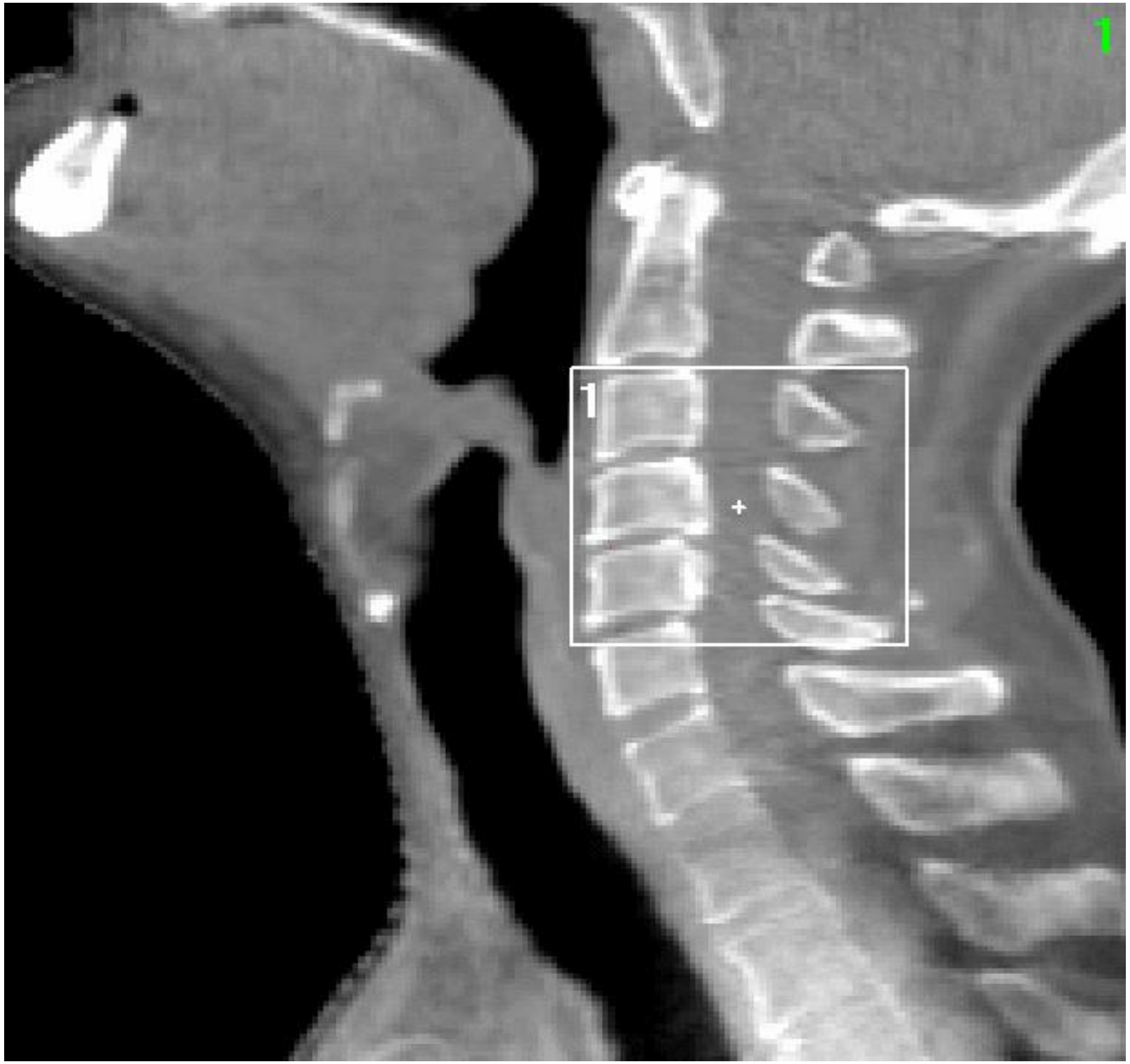
- Systematic errors: 1 to 2 mm (SD)
- Random errors: 1 to 2 mm (SD)

Hurkmans *et al*

Cone beam CT → Shape changes!

- Pose
- Weight loss
- Tumor regression
- ...

→ Non rigid

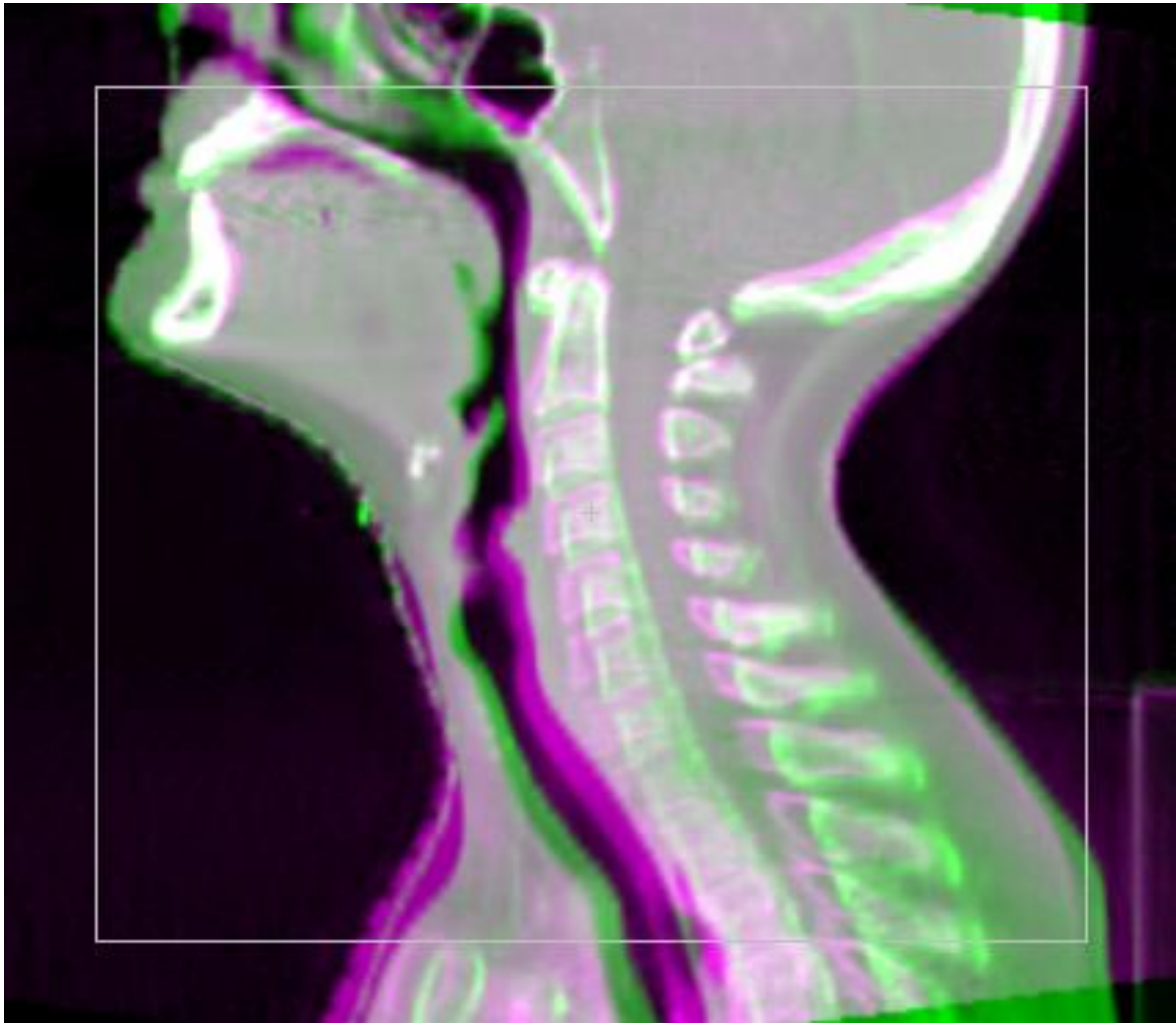


Treatment – image registration

Single ROI

ROI encompasses:

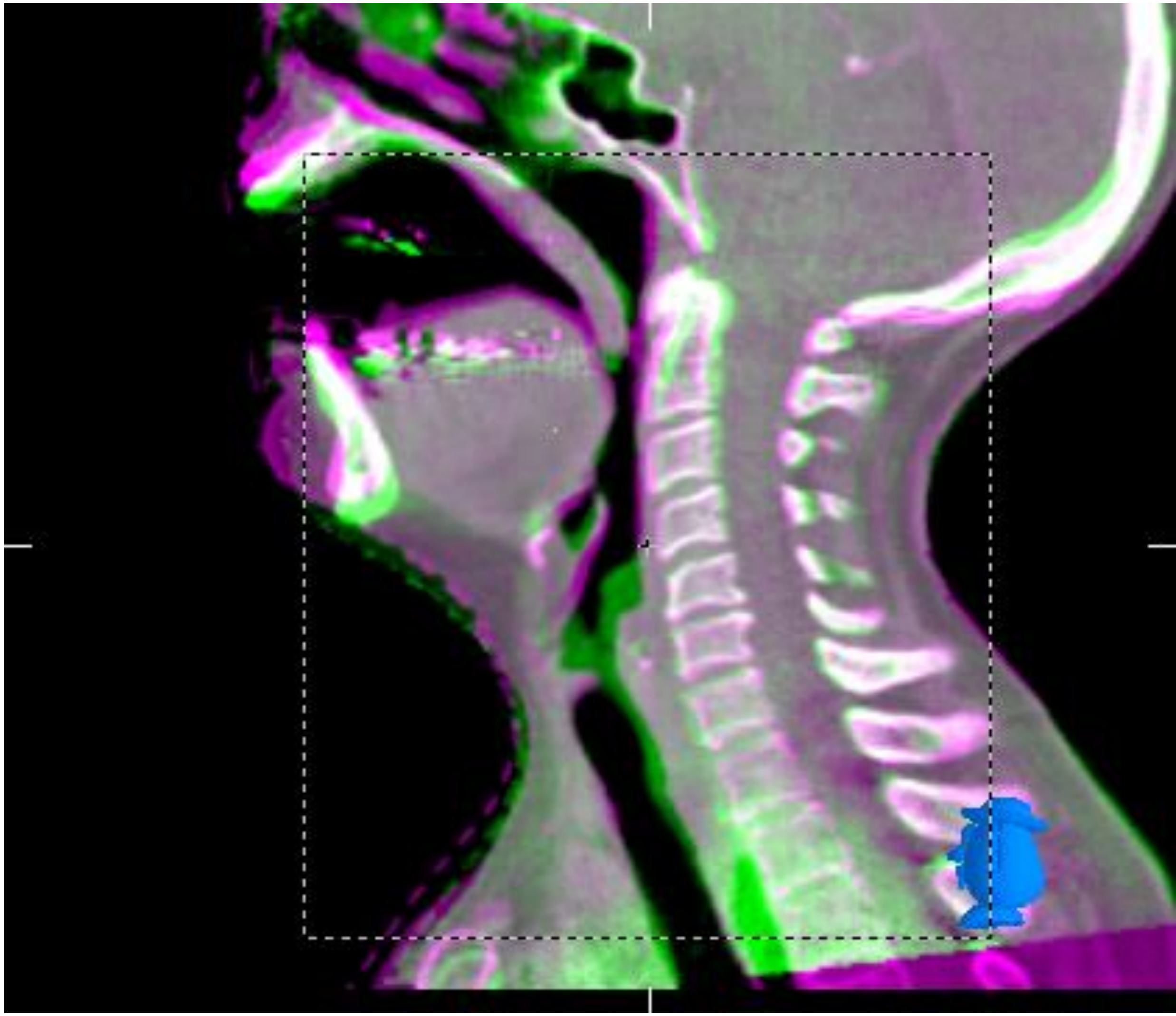
- PTV
- Vertebrae
- Base of skull
- Jaw



Purple: CBCT
Green: planning CT
Overlay: white = match

Single ROI registration

- Match inaccurate
  - ➢ Misregistration?
  - ➢ Deformation?



Use multiple ROIs

Allows:

- Accurate local registration
- Assessment of local setup errors

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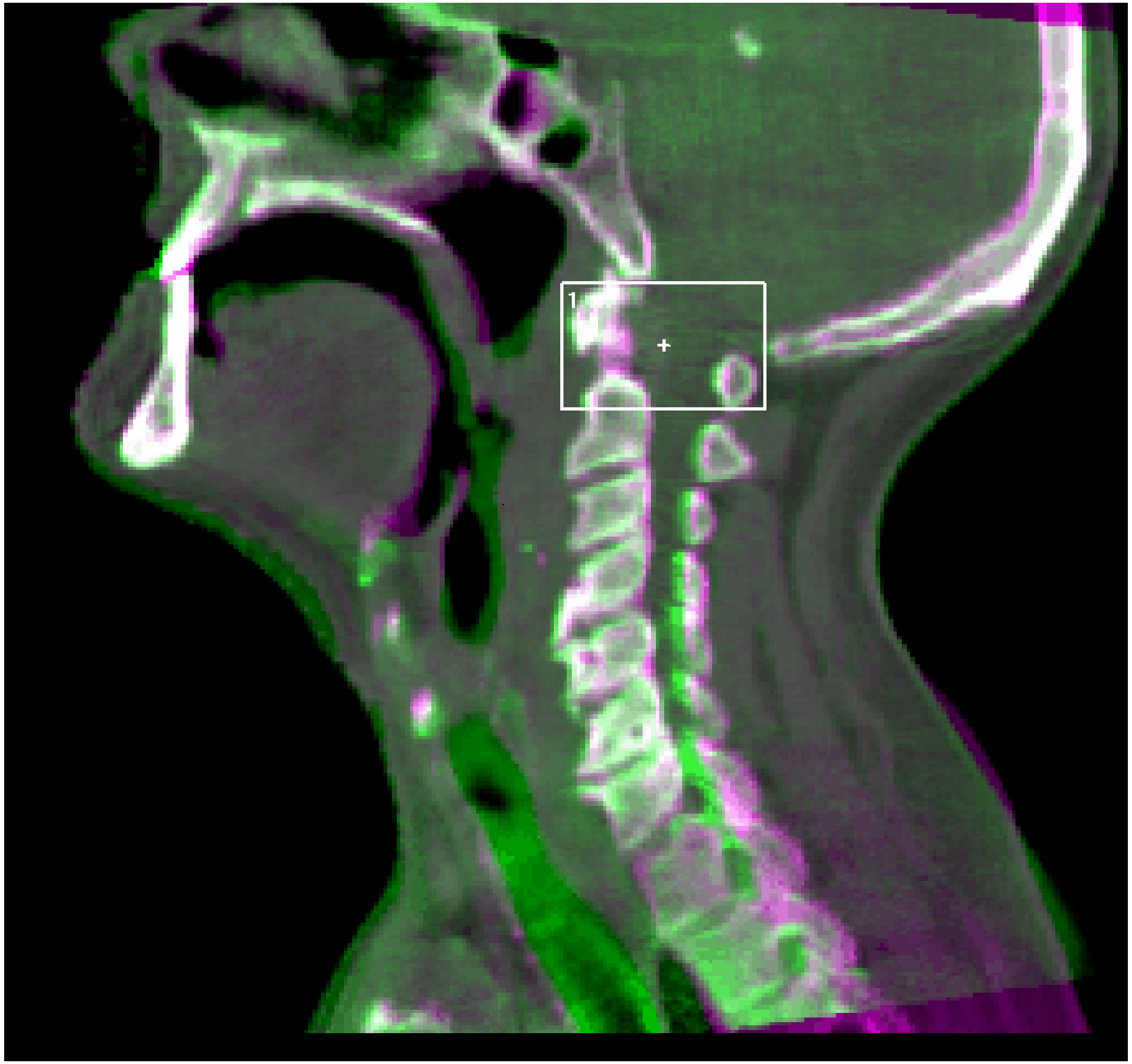
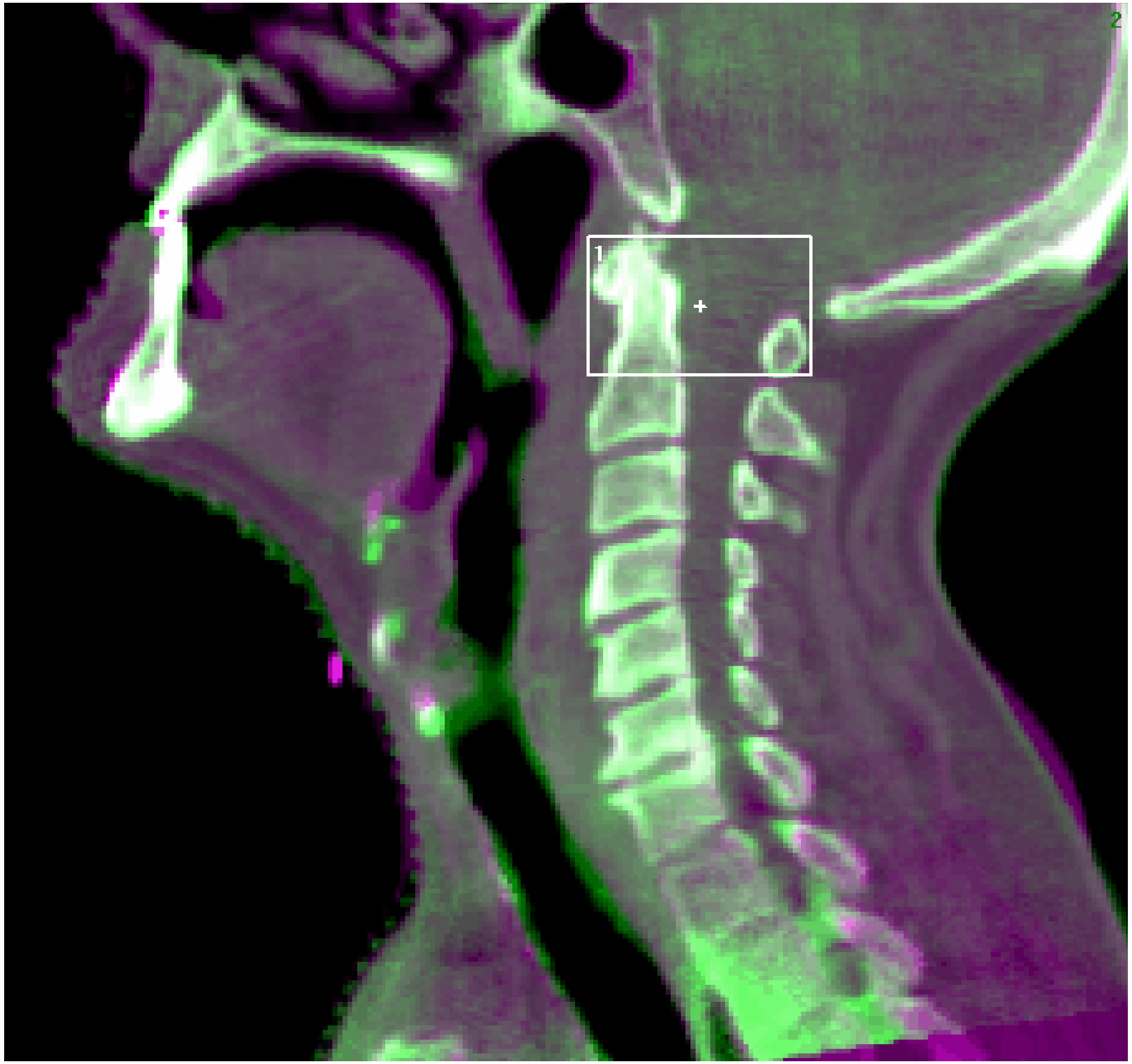
Image registration



- bony anatomy registration
- Loop over ROIs

Purple: planning CT
Green: CBCT

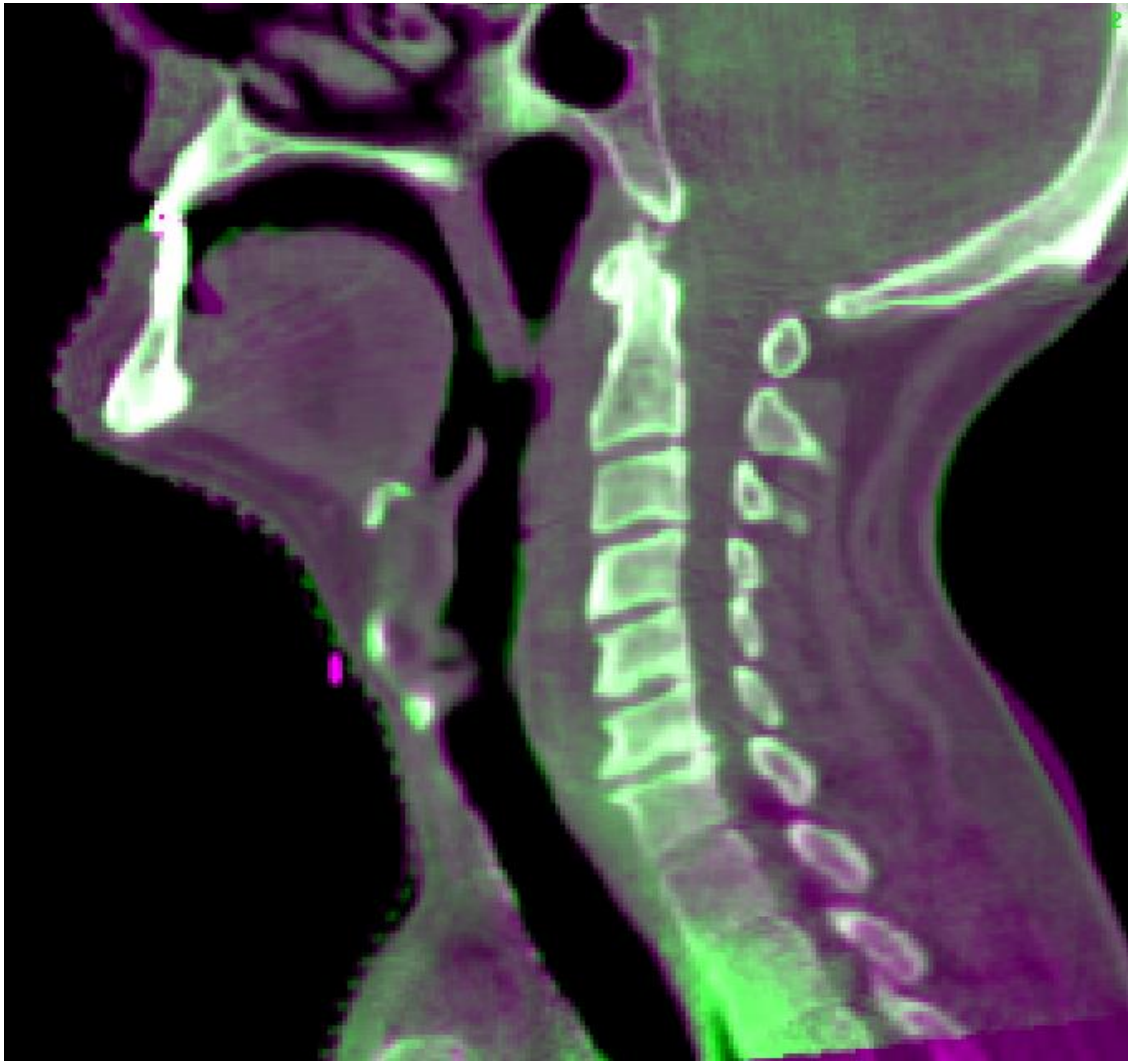
Validation of registration



All registrations separately

→ Easy

Validation of registration

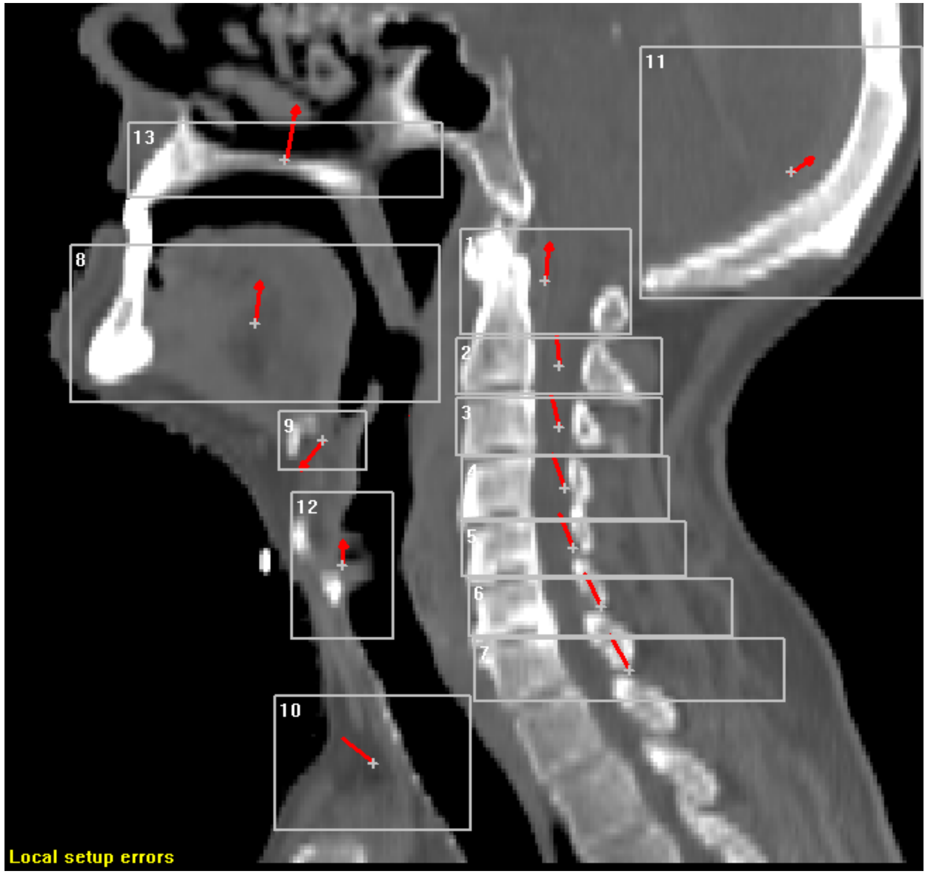


All registrations at once by warping

→Fast

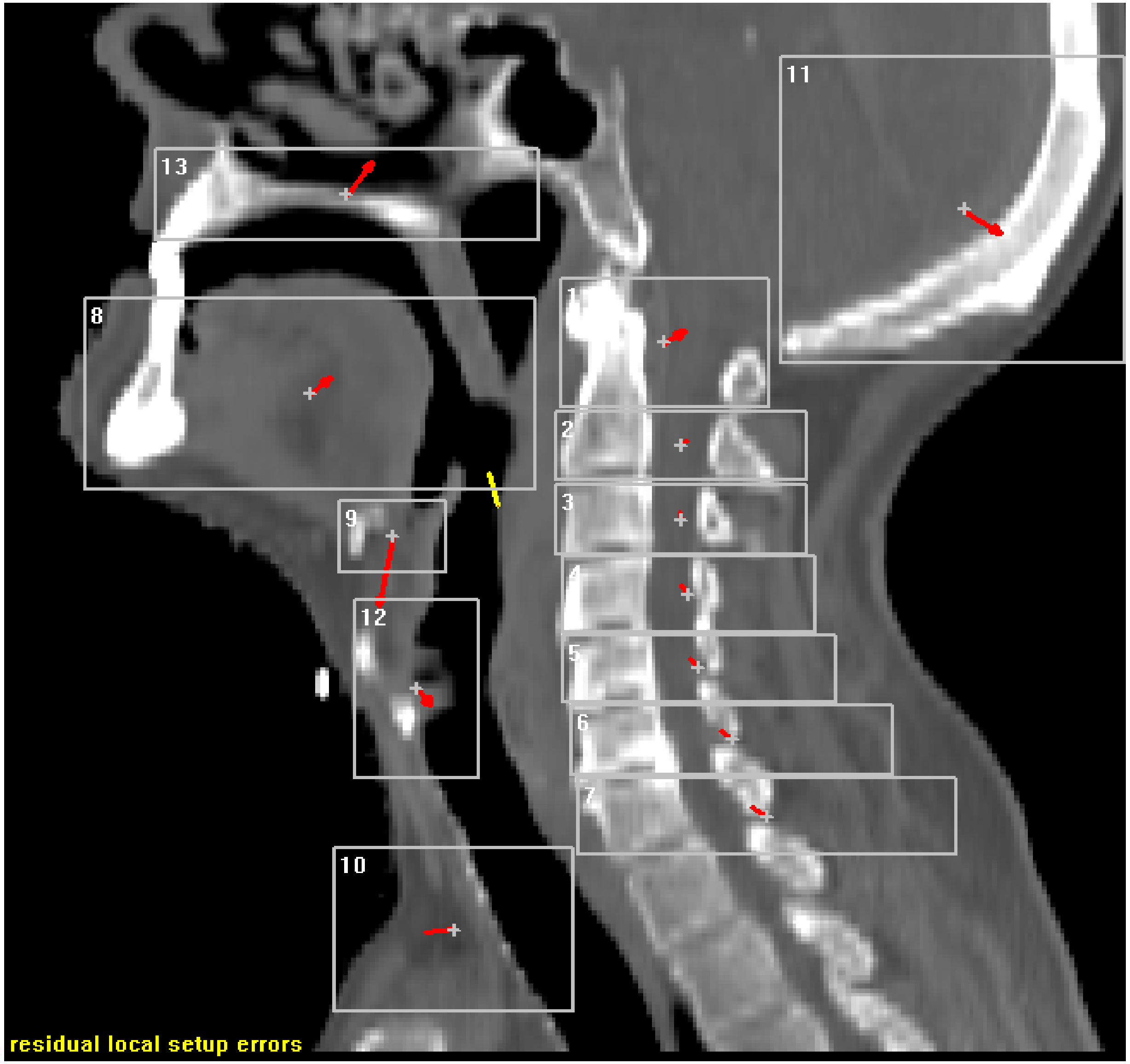
Corrections

Couch shift: Average setup errors



Correct average

Corrections



- Residual errors!

Corrections

- Residual errors

- Warnings:
  5 mm or 5°

Overview — Residuals after correction

Clipbox 2	-0.31	0.31	0.04	5.1	-4.4	-0.1
Clipbox 3	-0.25	0.20	0.07	3.3	-3.7	0.0
Clipbox 4	-0.10	0.05	0.21	0.6	-2.1	0.9
Clipbox 5	0.11	-0.13	0.54	-2.6	-0.2	1.9
Clipbox 6	0.14	-0.17	0.61	-3.0	0.5	1.6
Clipbox 7	0.23	-0.14	0.59	-2.8	0.5	2.3
Clipbox 8	0.04	0.02	-0.18	1.4	1.5	0.1
Clipbox 9	0.02	0.16	0.02	5.5	0.4	0.3
Clipbox 10	0.09	0.11	0.26	0.5	1.4	0.1

Register Clipbox | Correction | Overview

- 3 consecutive warnings:

→ Evaluate → Possible re-plan

Alternatives?

- If only one region of interest
  - ➢ Limit size to most important structures – e.g. the boost area
  - ➢ If deviations are visible outside this area…
    → Retrospectively register and discuss

- If two regions of interest (Dual registration in XVI)
  - ➢ Use one region of interest for most important structures – e.g. the boost area
  - ➢ Use other region of interest for larger area and specify tolerance limits. When limit is exceeded…
    → Discuss

- Re-plan if deformation is persistent → ART

Margins

- Delineation: 2-3 mm SD
- Setup: 1-2 mm SD (Portal imaging)

	Systematic	Random
Delineation	2-3 mm	-
Setup	1-2 / 1-4 mm	1-2 / 1-4 mm
Organ motion	Depends on tumor location	Depends on tumor location
Total	2-4	1-4 mm

- Margin: 5 mm (best case) .... 13 mm (worst case)
- E.g. boost area → high precision/small margins

  Nodal regions → less precision/but CTV!

Take home messages

- Head and neck is a complex site
- Geometrical uncertainties are underestimated
  - Especially with portal imaging
  - Deformations are an important factor
- Margins will depend on correction strategy
- For persistent anatomical changes replanning is a good option
- Search for best correction strategy ongoing ☺

Head and Neck IGRT: An RTT Perspective

Liz Forde, RTT
Assistant Professor
The Discipline of Radiation Therapy
School of Medicine
Trinity College Dublin

Applied Radiation Therapy Trinity Research Group

Trinity College Dublin
Coláiste na Tríonóide, Baile Átha Cliath
The University of Dublin

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Fundamental IGRT Questions

- ***When*** *should I image?*
  - *Frequency*
- ***How*** *should I image?*
  - *Technology*
  - *Projection*
- ***What*** *can I see?*
  - *What is my target*
- ***What*** *should I match to?*
  - *Surrogate for target position*

Site Specific Points to Consider

- The head and neck is a regions rich in radiosensitive structures (serial organs)

- Margins are typically tight
  - 0.3cm -0.5cm

- IMRT or VMAT are now standard and carry with them highly conformal dose distributions and multiple targets

Site Specific Points to Consider

- In addition to standard match structures also review:

- Position of mouth bung (if used) is correctly in place

- Bolus is positioned correctly (no gaps)

- Change in tumour size

Site Specific Points to Consider

- Gaps between skin and mask

- Shoulder position
  - Neubauer *et al.*, 2012

- Direct clinical impact of translations and rotations have on adjacent structures
  - True OAR
  - OAR PRV

Pre Treatment

CT Simulation

Slice thickness

- Accurate delineation
- Accurate dose calculation
- Improved DRR resolution
- 2.5-3.0mm

Registration of diagnostic imaging

Contrast

IV

No pre contrast scan

Bolus

Scan with bolus on

Planning

3DCRT

IMRT
VMAT
} Standard for this patient group

Beware the steep dose gradients

Shoulders

Avoid?

Match Anatomy

- Bony landmarks

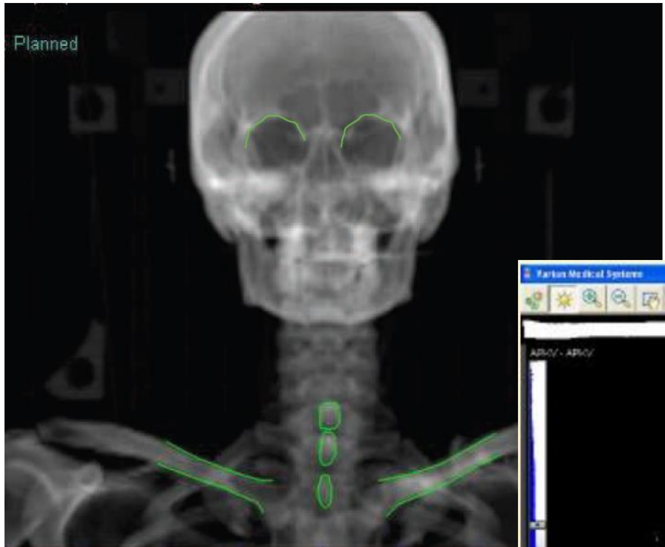
- Vertebrae
- Angle of mandible
- Orbital rim
- Frontal sinus
- Pituitary fossa

2D

- MV (EPI) is adequate for visualisation of bony anatomy
- Single projection ***not*** recommended for H&N
- Need to confirm isocentre in two planes
- Of less value when treating with IMRT
  - ➢ Field borders
  - ➢ Ciao images
- Impact of dose when imaging daily with MV

2D/2D

- Improved visualisation and image quality
- Large FOV assess anatomy across whole target volumes and patient straightening

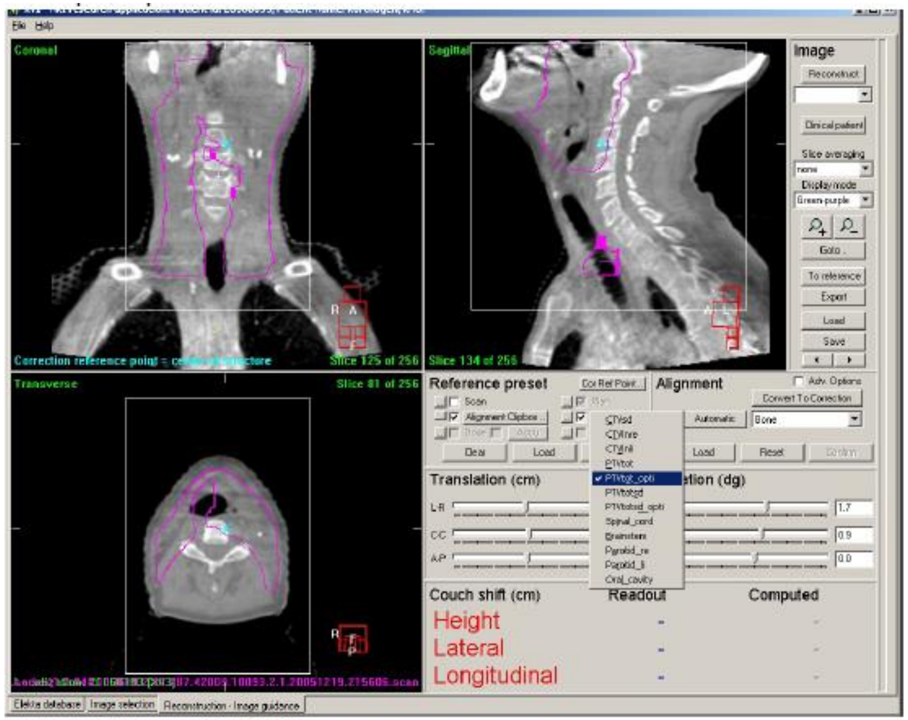


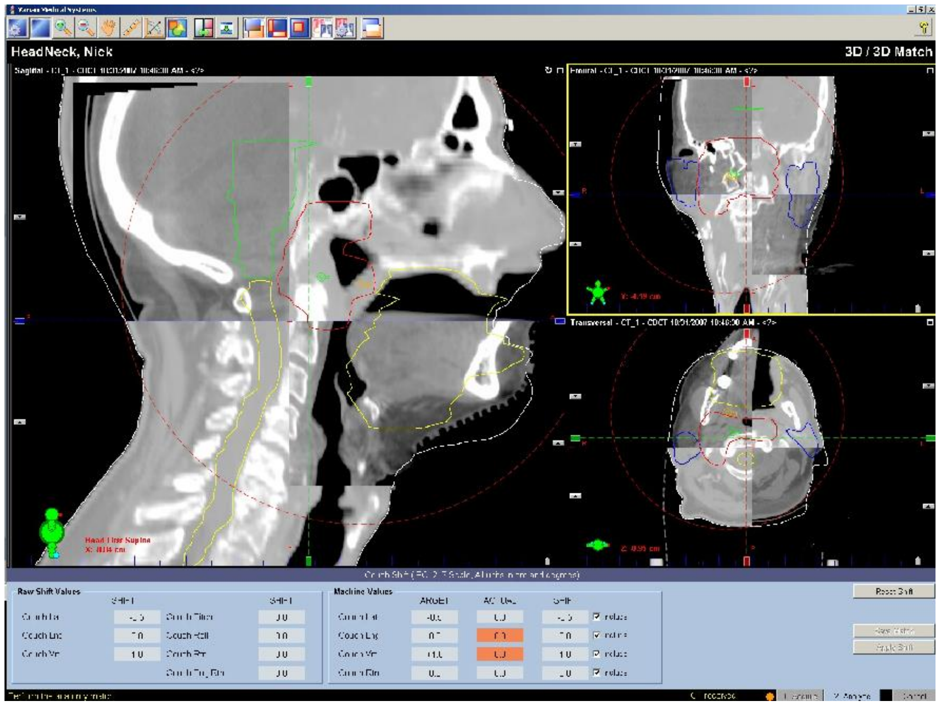
Mechalakos et al., 2007

3D

- Peter has covered this in excellent detail!

- Consider other structures to review
  - ➢ 45Gy isodose line





All Very Straightforward!

- But wait…there's more…

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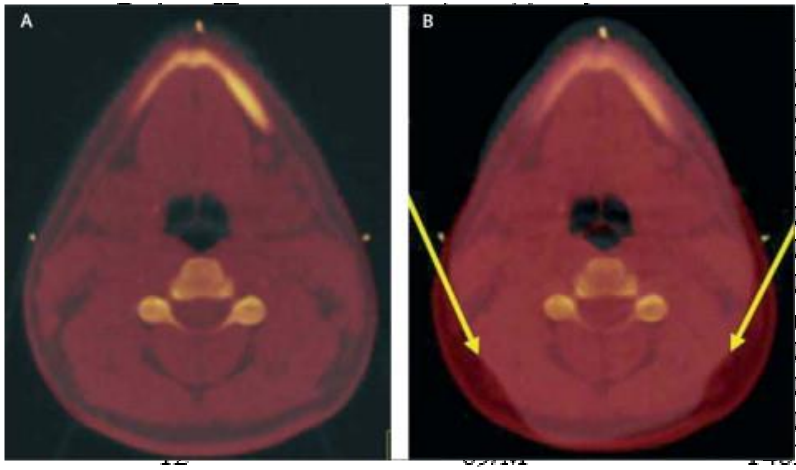
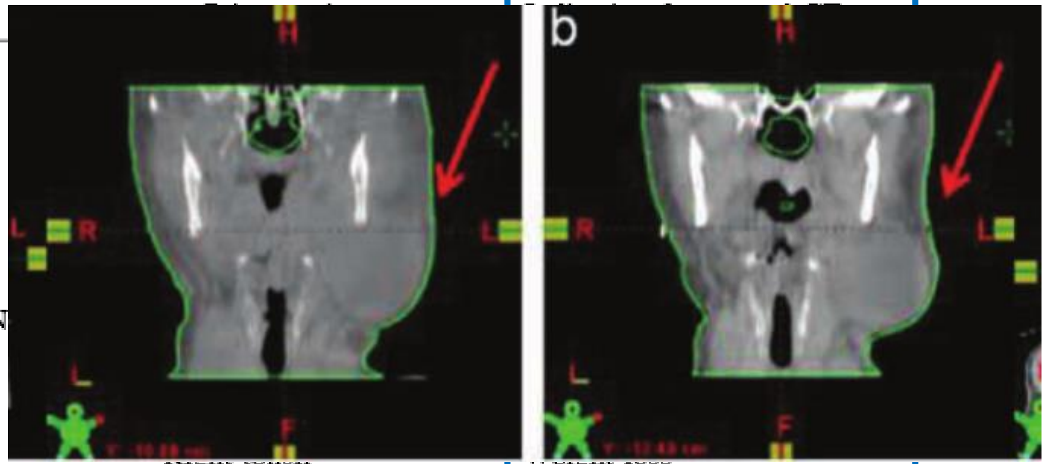
Tumour Shrinkage and Weight Loss

- Despite nutritional support these patients typically suffer significant weight loss during treatment
    - ➢ Impact on setup accuracy
    - ➢ Role of prophylactic PEG

Table 1. Patient characteristics





		Stage		
12	[illegible]	...N1	[illegible]	[illegible]
13	54/M	TXN2b	Unknown primary	Weight loss, tumor shrinkage

Abbreviations: ID = identification number; M = male; F = female; NPX = nasopharynx; BOT = base of tongue.
* Patient died of pneumonia after completing 23 fractions.

Tumour Shrinkage and Weight Loss

- Dosimetric Impact!

Replanning during IMRT for H&N cancer ● E. K. Hansen *et al.*

Table 3. Dosimetric comparisons of the 2nd portion of treatment with and without replanning

Dosimetric end point (mean values)	1st portion of treatment (1st CT/1st plan)	2nd portion of treatment: Replanned (2nd CT/2nd plan)	2nd portion of treatment: Not replanned (2nd CT/1st plan)	*p* value
PTV_{GTV}				
D_{99}	38.1 Gy	28.3 Gy	26.0 Gy	0.05
D_{95}	40.3 Gy	30.3 Gy	28.1 Gy	0.02
V_{93}	99.5%	99.4%	92.5%	<0.001
PTV_{CTV}				
D_{99}	30.9 Gy	22.9 Gy	18.3 Gy	<0.001
D_{95}	34.0 Gy	25.7 Gy	22.7 Gy	0.003
V_{93}	98.7%	98.7%	90.5%	<0.001
Spinal cord				
D_{max}	25.7 Gy	19.3 Gy	23.3 Gy	0.003
$D_{1\ cc}$	23.0 Gy	17.1 Gy	20.2 Gy	0.04
Brainstem				
D_{max}	28.2 Gy	22.3 Gy	24.9 Gy	0.007
$D_{1\ cc}$	25.0 Gy	19.4 Gy	21.7 Gy	0.20
$D_{1\%}$	26.1 Gy	20.2 Gy	22.9 Gy	0.12
Right parotid	(n = 12)			
D_{mean}	15.5 Gy	12.0 Gy	14.9 Gy	0.05
D_{50}	13.0 Gy	10.6 Gy	13.6 Gy	0.06
V_{26}	44.6%	45.5%	55.5%	0.04
Left parotid				
D_{mean}	15.2 Gy	11.9 Gy	12.1 Gy	0.81
D_{50}	13.2 Gy	10.2 Gy	11.2 Gy	0.47
V_{26}	45.2%	42.9%	42.2%	0.89
Mandible (n = 9)				
D_{max}	39.2 Gy	29.6 Gy	31.3 Gy	0.01
V_{60}	11.0%	11.3%	18.2%	0.08
V_{70}	0.04%	0.05%	4.5%	0.32

Abbreviations: PTV_{GTV} PTV_{CTV} = planning target volumes of gross tumor volume and clinical tumor volume, respectively; D_{max} = maximum dose; D_{99} = dose to 99% of the volume; D_{95} = dose to 95% of the volume; V_{93} = percent of volume receiving ≥93% of the prescribed dose; $D_{1\ cc}$ = dose to 1 cc of the volume; $D_{1\%}$ = dose to 1% of the volume; D_{mean} = mean dose; D_{50} = dose to 50% of the volume; V_{26}, V_{60}, and V_{70} = percent of volume receiving ≥26 Gy, ≥60 Gy, and ≥70 Gy, respectively.

Assessed impact on OAR doses not target dose

Contoured OARs on CBCTs and recalc'd with correction for HU differences

Clinical Investigation: Head-and-Neck Cancer

Monitoring Dosimetric Impact of Weight Loss With Kilovoltage (KV) Cone Beam CT (CBCT) During Parotid-Sparing IMRT and Concurrent Chemotherapy

Kean Fatt Ho, F.R.C.R.,* Tom Marchant, Ph.D.,† Chris Moore, Ph.D.,† Gareth Webster, Ph.D.,† Carl Rowbottom, Ph.D.,† Hazel Penington, B.Sc.,‡ Lip Lee, F.R.C.R.,§ Beng Yap, F.R.C.R.,§ Andrew Sykes, F.R.C.R.,§ and Nick Slevin, F.R.C.R.§

*From *Academic Radiation Oncology, †North Western Medical Physics, ‡Wade Radiotherapy Research Centre, and §Department of Clinical Oncology, The Christie NHS Foundation Trust, Manchester, UK*

Received Oct 10, 2010. Accepted for publication Jul 6, 2011

Where did this weight loss occur?

Weight loss and parotid shrinking did occur, but insignificant impact on OAR doses

Results inconsistent with previous studies
Impact of neoadjuvant therapy?

Demonstrates the benefit of 3D imaging
Discusses options of dose calculation from CBCT

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Tumour Shrinkage and Weight Loss

- A lot of literature!!!
- Every patient is individual
    - RTTs treat them and can see these subtle changes
- Dosimetric (and clinical) impact will depend on original DVH results
- Without 3D imaging, you cannot accurately visualise or account for this
- *"The dosimetric impact of anatomic changes during radiotherapy was of lesser importance than the effects of IGRT repositioning"* (Graff et al., 2012)

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What Else?
Variation in Shoulder Position

- The shoulders move independently from the isocentre
- This shoulder motion changes the path length of the beam
- Superior shoulder shift results in target coverage loss

Table 3 Target coverage in the C6-C7 region

	IMRT			VMAT		
	100%	98%	95%	100%	98%	95%
C6-C7						
No shift	97	98	100	94	97	99
5 mm superior	90	98	100	84	96	99
15 mm superior	23	53	94	16	35	72
C7-T2						
No shift	98	100	100	–	–	–
15 mm posterior	89	99	100	–	–	–

Percentage of the clinical target volume (CTV) in the C6-C7 region covered by the 100%, 98%, and 95% isodose lines with no shift and with superior shifts for IMRT and VMAT plans, as well as the percent coverage of the CTV in the C7-T2 region with no shift and a 15 mm posterior shift. All percentages were evaluated for Patient 1.

What Else?
Variation in Shoulder Position

- This positional variation cannot be corrected with translational or rotational corrections

- This variation also caused an increase in OAR dose
  - ➢ Brachial Plexus increased by up to 7.2Gy

- In the absence of CBCT the angle of clavicle on AP EPI

Take Home Message

- *"Complex and multifactorial dosimetric variations occur during head and neck IMRT."* (Graff et al., 2012)

- Take caution due to tight margins, conformal techniques and proximity of radiosensitive structures

- Have an understanding of dosimetric impact of weight loss and shoulder motion

- Appropriate immobilisation is key. IGRT may help in assessment of this, but can not always correct for this.

- Recommend clear protocols to mandate imaging frequency and match structures

RTTs! If you are going to read one head and neck paper this year...
Let it be this one!

Technical Innovations & Patient Support in Radiation Oncology 1 (2017) 1–7

Contents lists available at ScienceDirect

Technical Innovations & Patient Support in Radiation Oncology

journal homepage: www.elsevier.com/locate/tipsro

Practice guidelines

ESTRO ACROP guidelines for positioning, immobilisation and position verification of head and neck patients for radiation therapists

Michelle Leech [a,*], Mary Coffey [a], Mirjam Mast [b], Filipe Moura [c], Andreas Osztavics [d], Danilo Pasini [e], Aude Vaandering [f]

[a] *Applied Radiation Therapy Trinity (ARTT), Discipline of Radiation Therapy, School of Medicine, Trinity College, Dublin 2, Ireland*
[b] *Radiotherapy Centre West/Medical Center Haaglanden, The Hague, The Netherlands*
[c] *Hospital CUF Descobertas, Lisboa, Portugal*
[d] *Universitätsklinik für Strahlentherapie, Vienna, Austria*
[e] *USCU Policlinico A. Gemelli, Rome, Italy*
[f] *Radiation Oncology Department, Cliniques Universitaires St Luc, Brussels, Belgium*

Implementation of new protocols

Martijn Kamphuis MSc MBA
Research Radiation Therapist IGRT

Department of Radiotherapy @AMC
Amsterdam, the Netherlands

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The Aim of the presentation

- Describing the process of implementing new technology and protocols
    - Illustrated with different examples

- Sharing experience, tips and tricks

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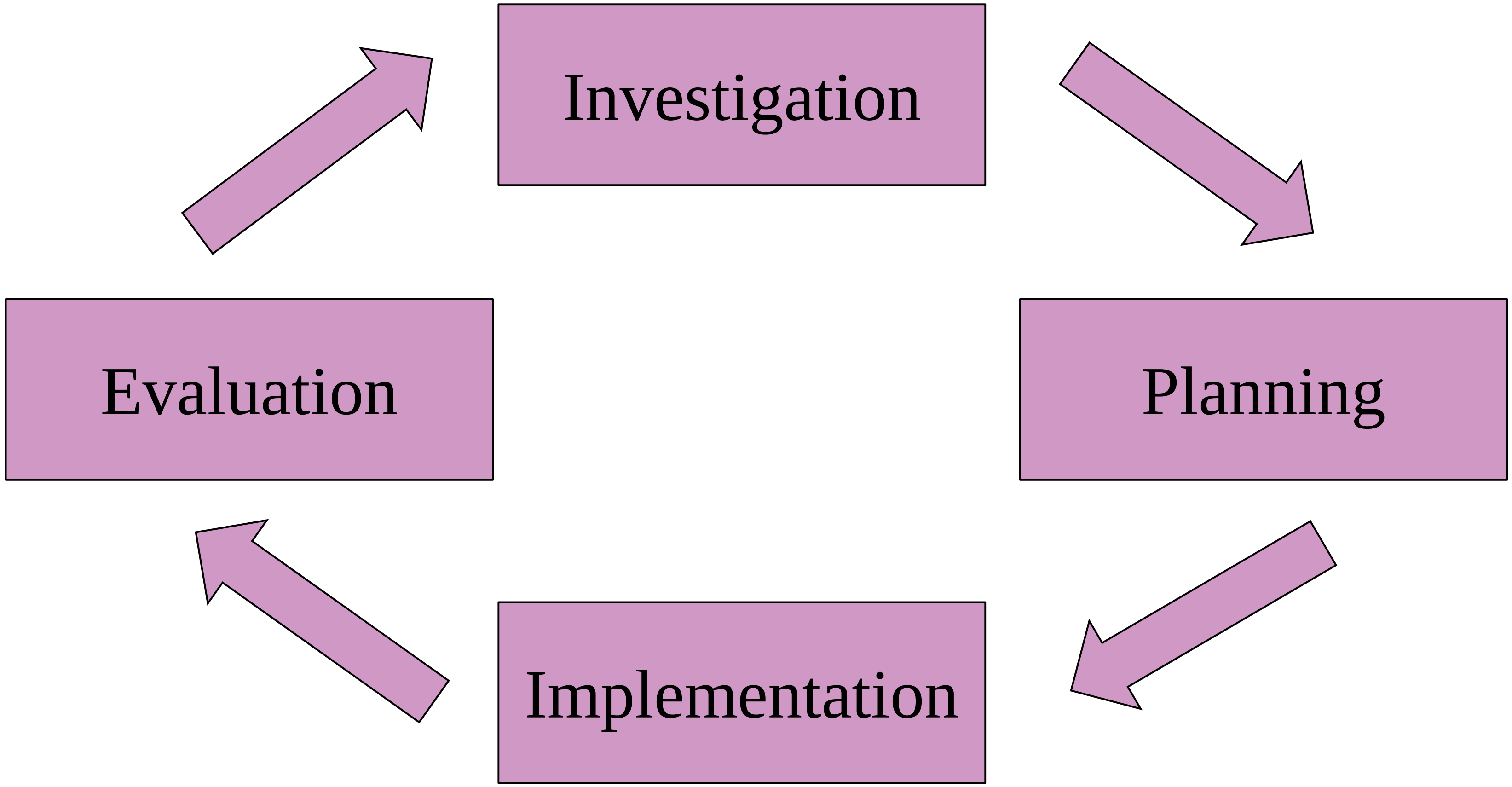
Have you ever been involved in clinical implementations of new protocols?

A. Yes

B. No

Protocol implementation



Preparation phase

- Defining your goal, make sure it's clear
  - E.g. Implementing hypofractioned radiotherapy in your department for stage one and two lung cancer
  - Implementing adaptive radiotherapy for bladder cancer using a library of plans

- Creating a multidisciplinary team
  - Include all stakeholders that will get involved
    - Not only MD, physicist and RTT, but also manager, technicians
  - Define roles of individual team members
    - Who is doing what?

Preparation phase: Investigate!

- Literature reading
  - ➢ Articles
  - ➢ Guidelines e.g. AAPM
- Join trails if possible
- Visit other institutes:
  - ➢ Learn from other ones' experience (and then do it better ☺)
- Follow vendor trainings/courses/workshops
- ESTRO
  - ➢ (Live) Courses
  - ➢ Dove (www.estro.org)
  - ➢ Technology transfer grant

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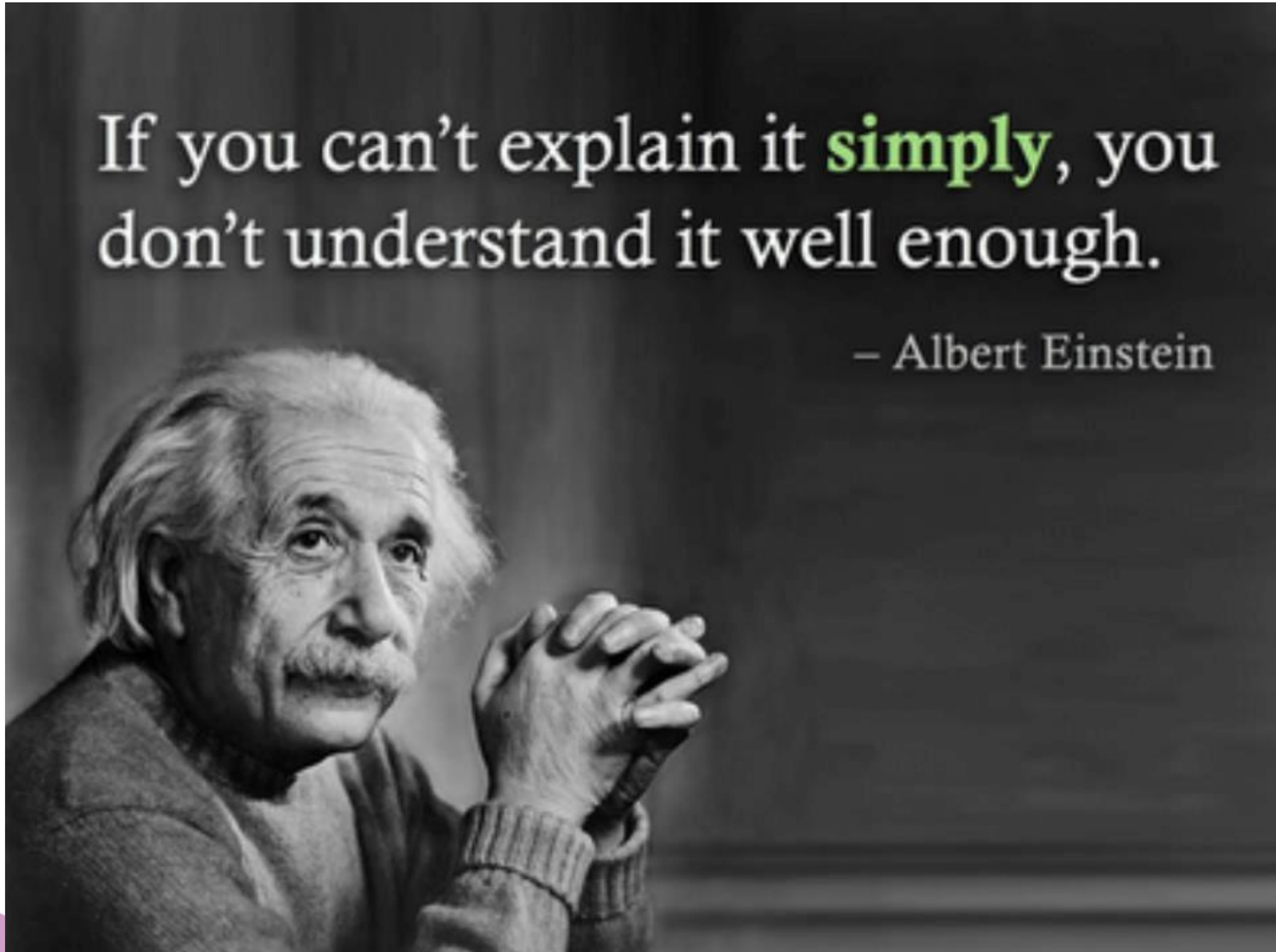

If you can't explain it simply, you don't understand it well enough.
– Albert Einstein

Planning/protocol writing phase

- Organize multiple meetings to discus the protocol
  - Come to a shared vision

- Write a project plan/protocol
  - Define all tasks and responsibilities
  - Check weather task can be performed parallel
  - Create a timeline
    - Start from the deadline ☺
    - Decisions have to been made, sooner or later

- Prospective Risk Analyses
  - Helps to think ahead

Implementation Phase

Critical conditions for proper implementation

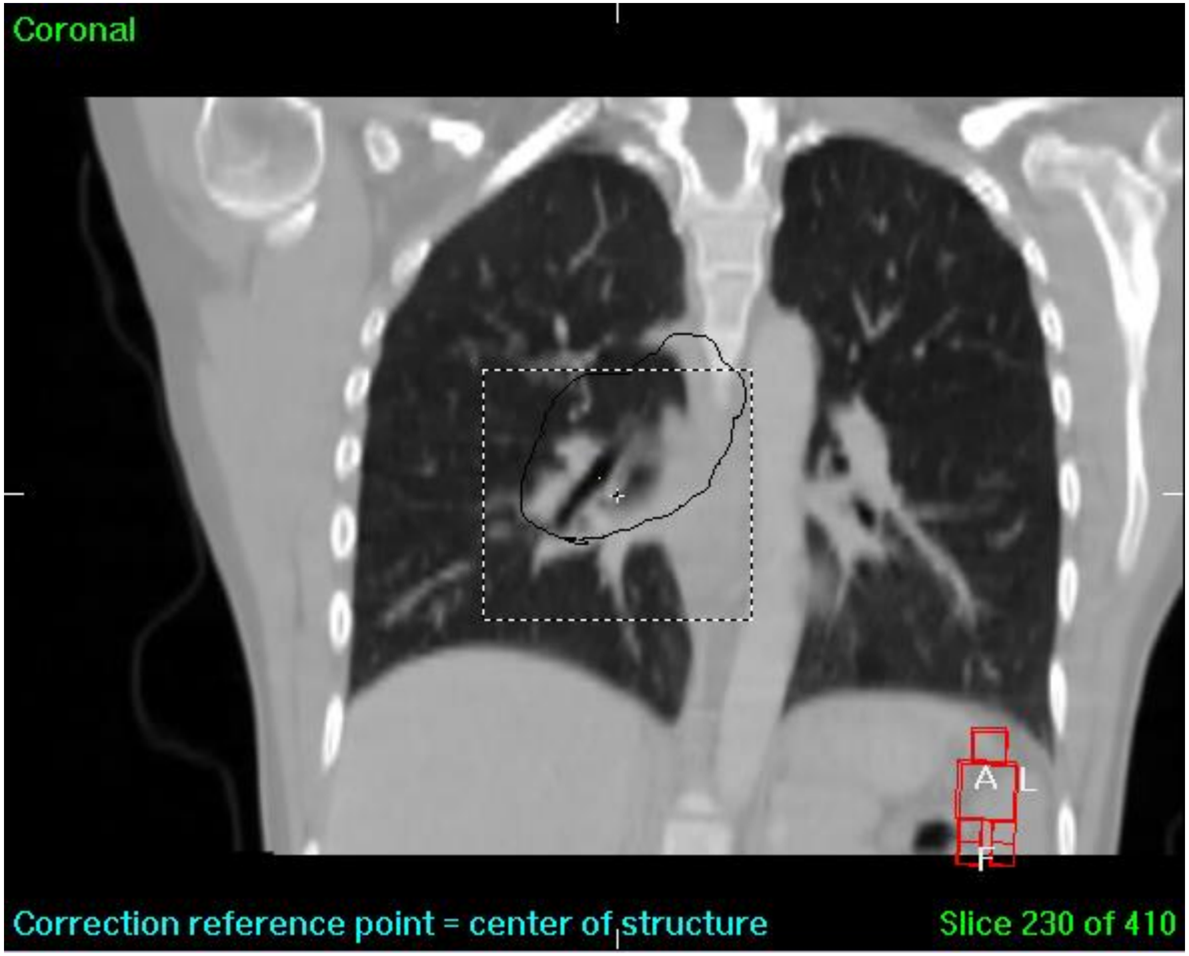
- Treatment protocol should be:
  - ➢ Well described and well defined task
  - ➢ Approved by staff
  - ➢ Available for everyone

Well described and well defined tasks

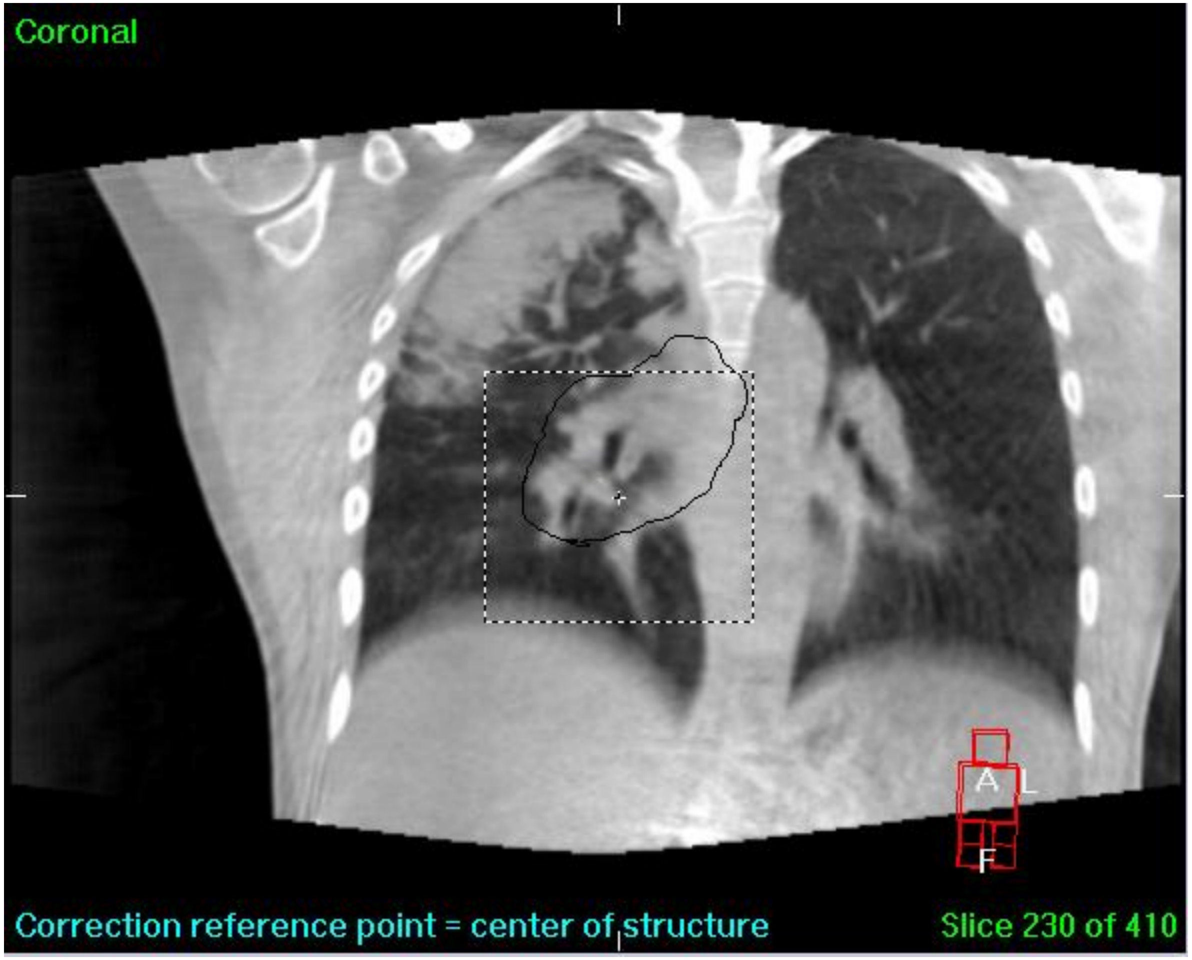
Example: protocol for dealing with anatomical changes

- In room imaging started off as a single check between CT and Linac
- Nowadays we are more aware of anatomical changes

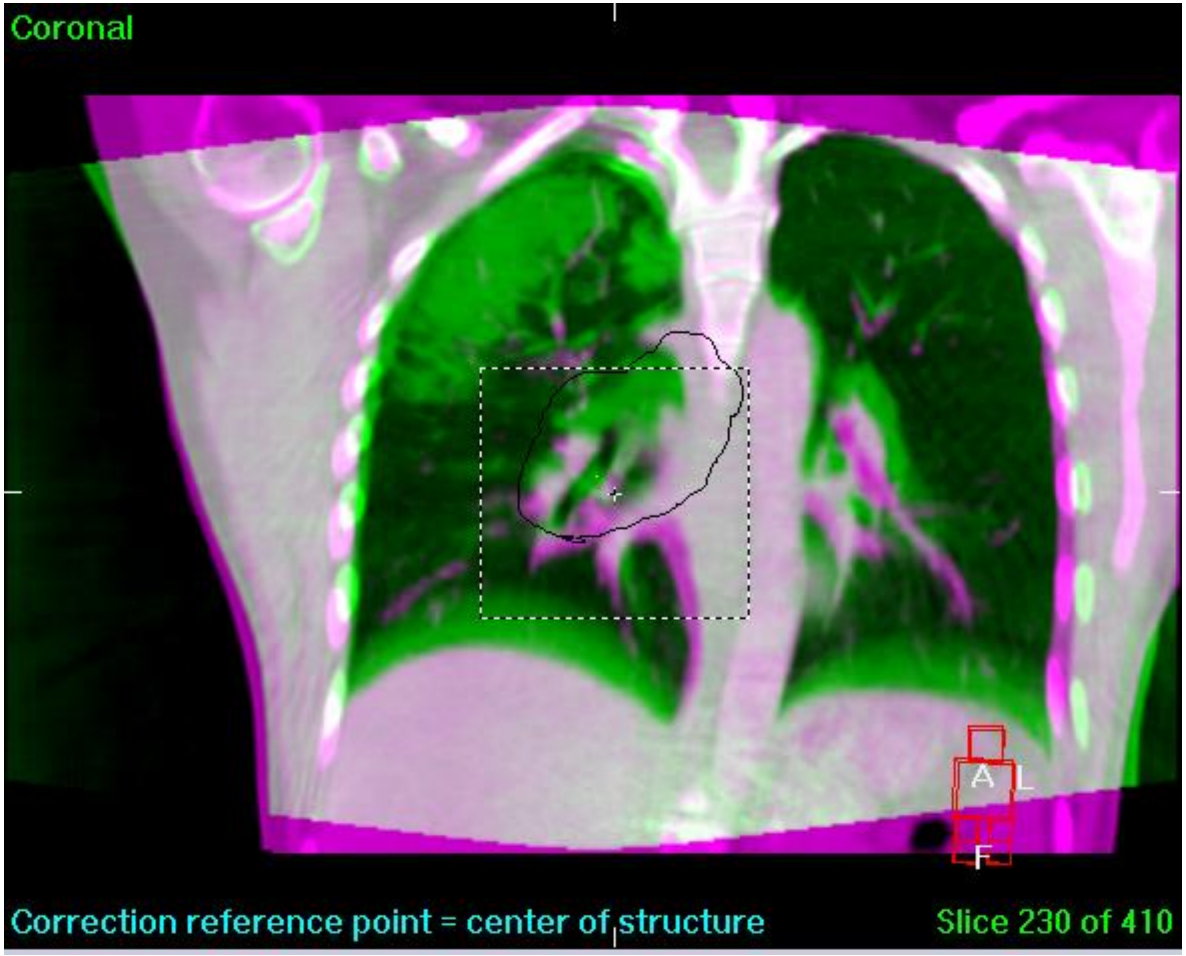
Anatomical changes



Ref-CT


Coronal
A L
F
Correction reference point = center of structure
Slice 230 of 410

CBCT

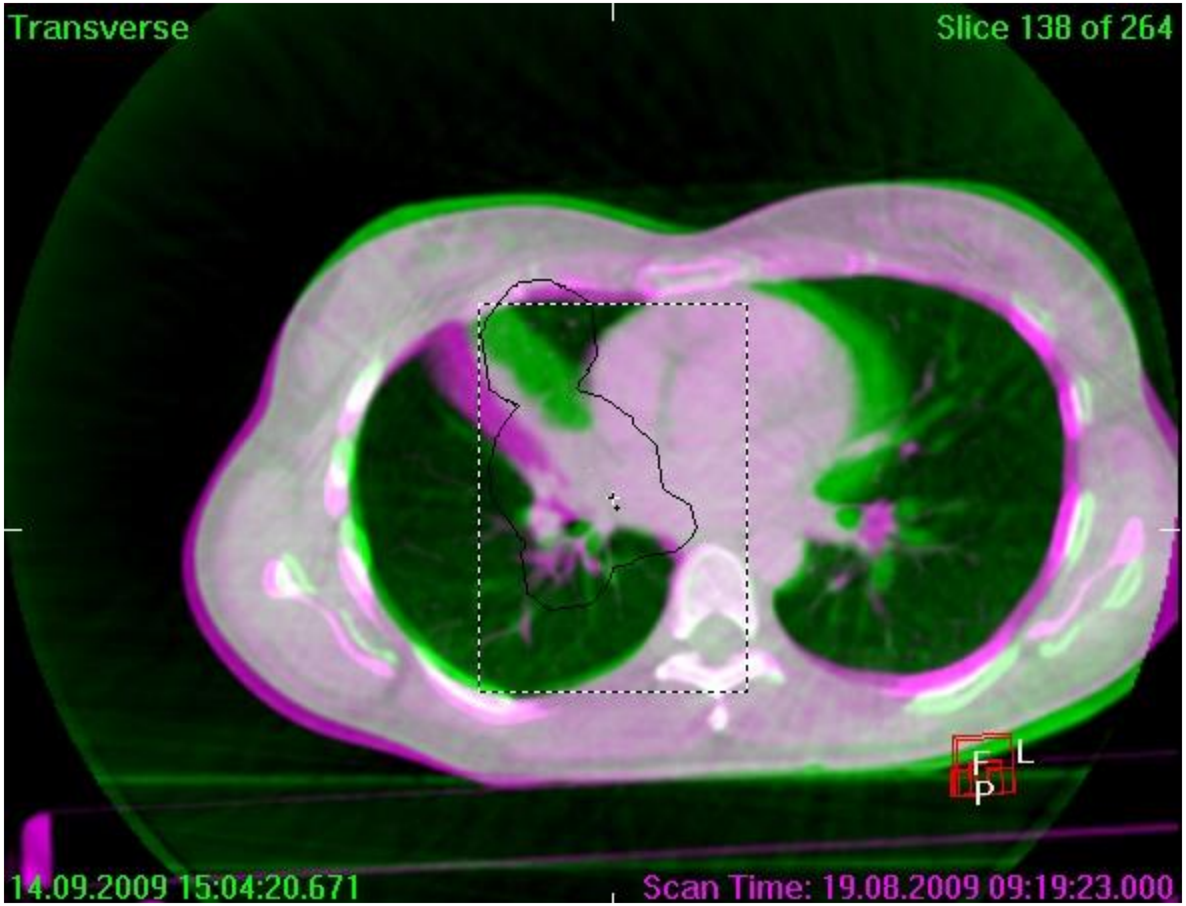

Coronal
A
L
F
Correction reference point = center of structure
Slice 230 of 410

CBCT

Ref-CT

CBCT

Ref-CT


Transverse
Slice 138 of 264
L
F
P
14.09.2009 15:04:20.671
Scan Time: 19.08.2009 09:19:23.000

Atelectases

- Dosimetry changes due to atelectases
- Tumor position changed

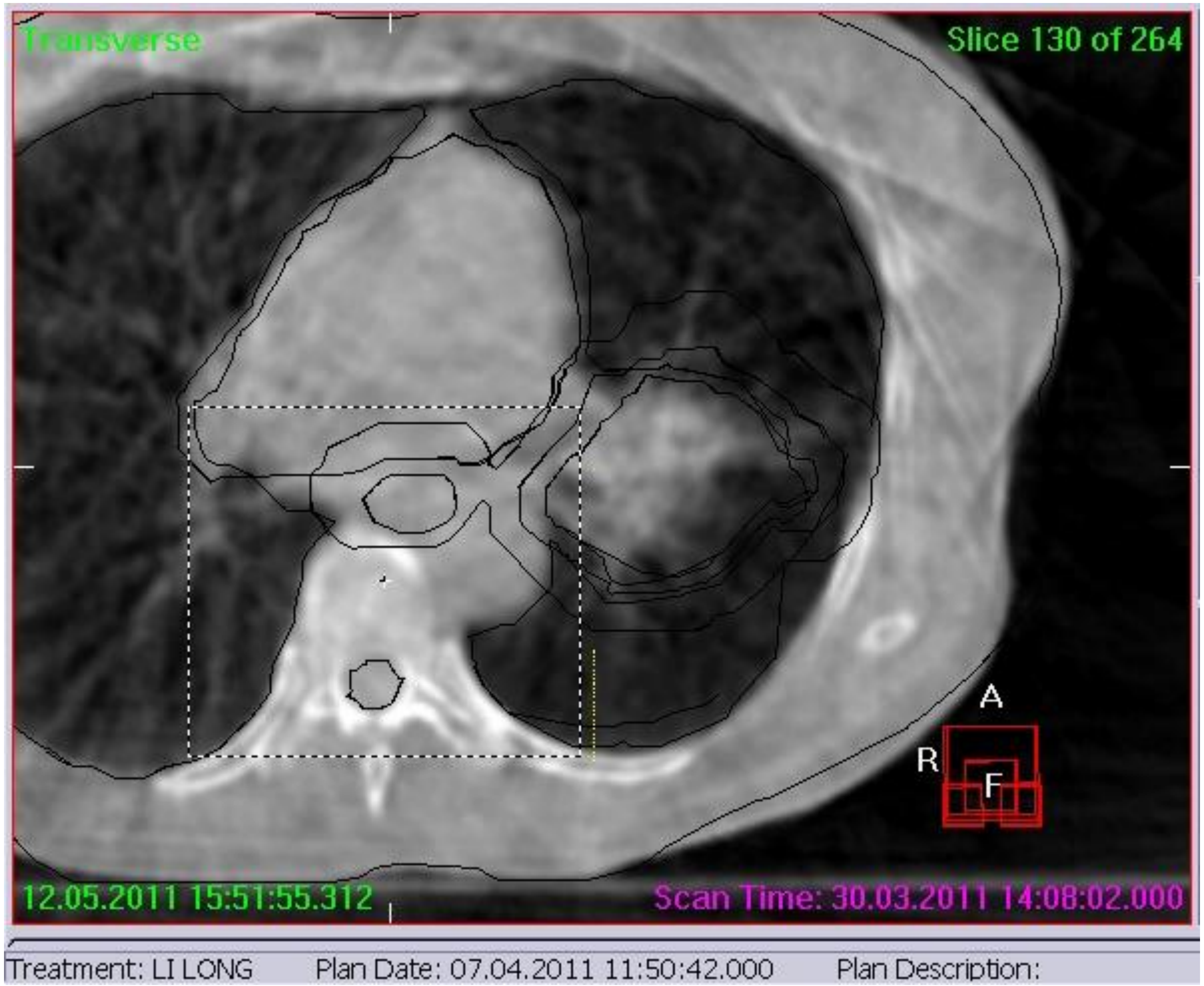
- Rescanning/replanning necessary


Coronal
Marker set
A
L
F
Correction reference point = center of structure
Slice 217 of 410

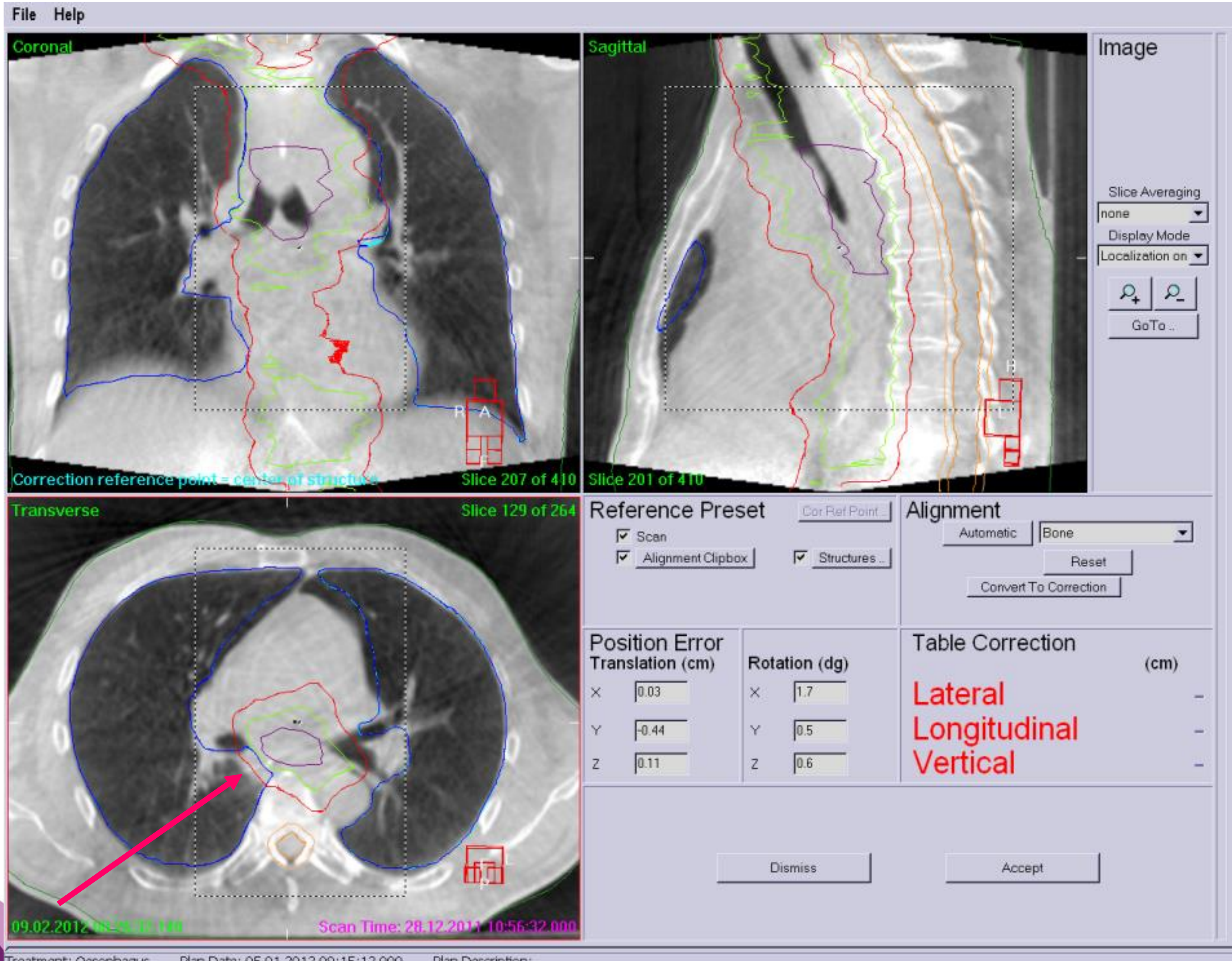
CBCT

Ref-CT

Tumor regression



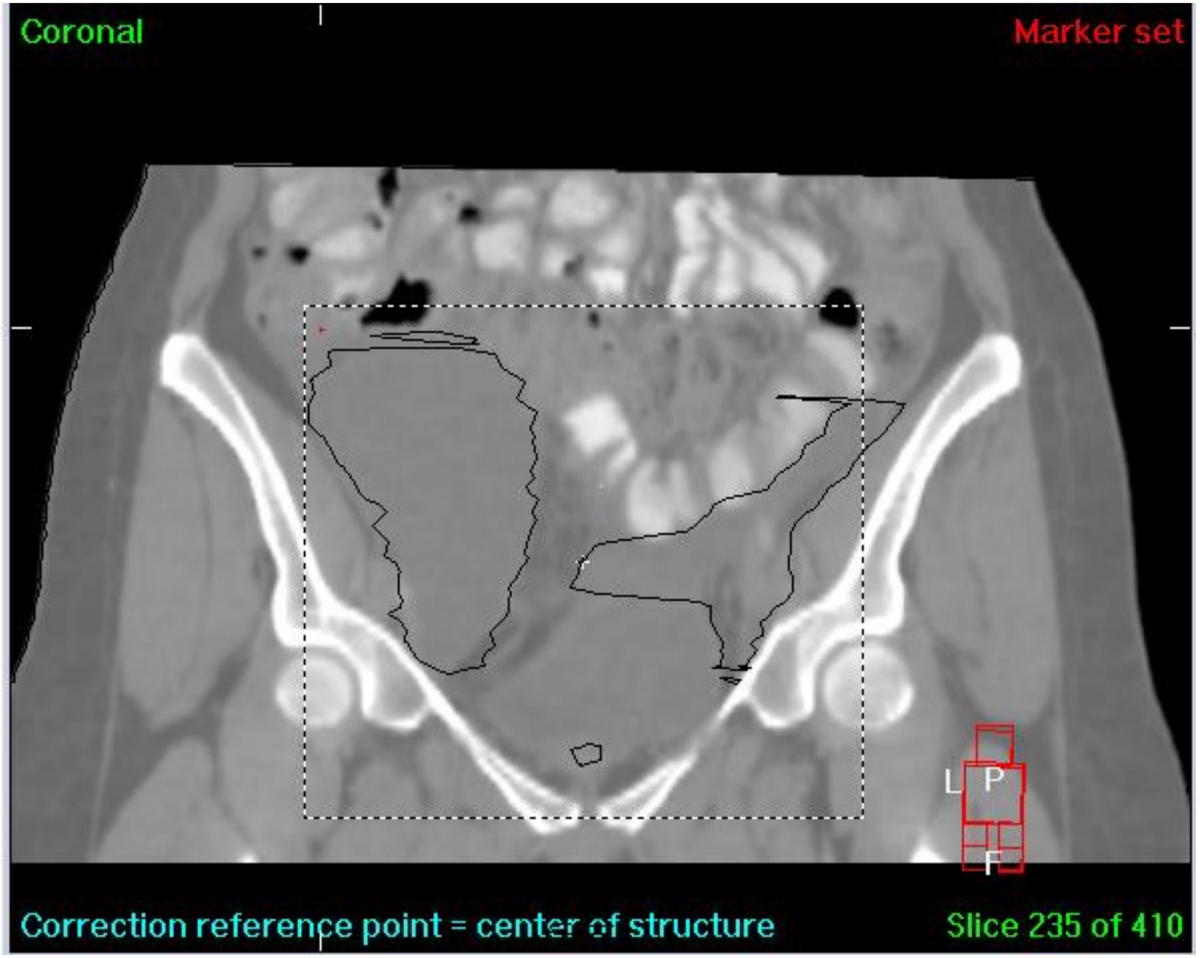
Tumor shift



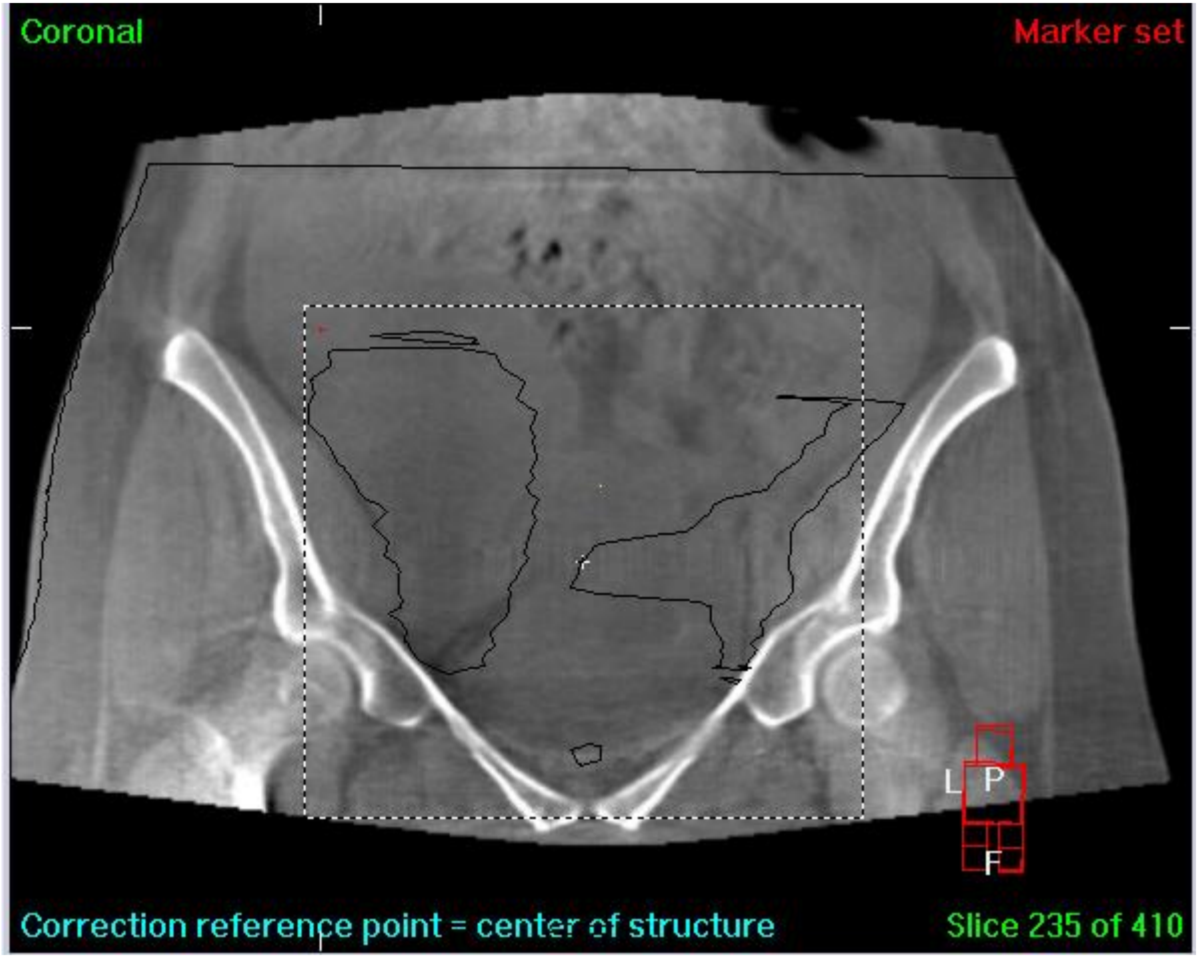
File Help
Coronal
Sagittal
Image
Slice Averaging
none
Display Mode
Localization on
GoTo ..
Correction reference point = center of structure
Slice 207 of 410
Slice 201 of 410
Transverse
Slice 129 of 264
Reference Preset
Cor Ref Point
Scan
Alignment Clipbox
Structures ..
Alignment
Automatic
Bone
Reset
Convert To Correction
Position Error
Translation (cm)
Rotation (dg)
X 0.03
Y -0.44
Z 0.11
X 1.7
Y 0.5
Z 0.6
Table Correction
(cm)
Lateral
Longitudinal
Vertical
Dismiss
Accept
Scan Time: 28.12.2011 10:56:32.000
Treatment: Oesophagus
Plan Date: 05.01.2012 09:15:12.000
Plan Description:

Rare changes

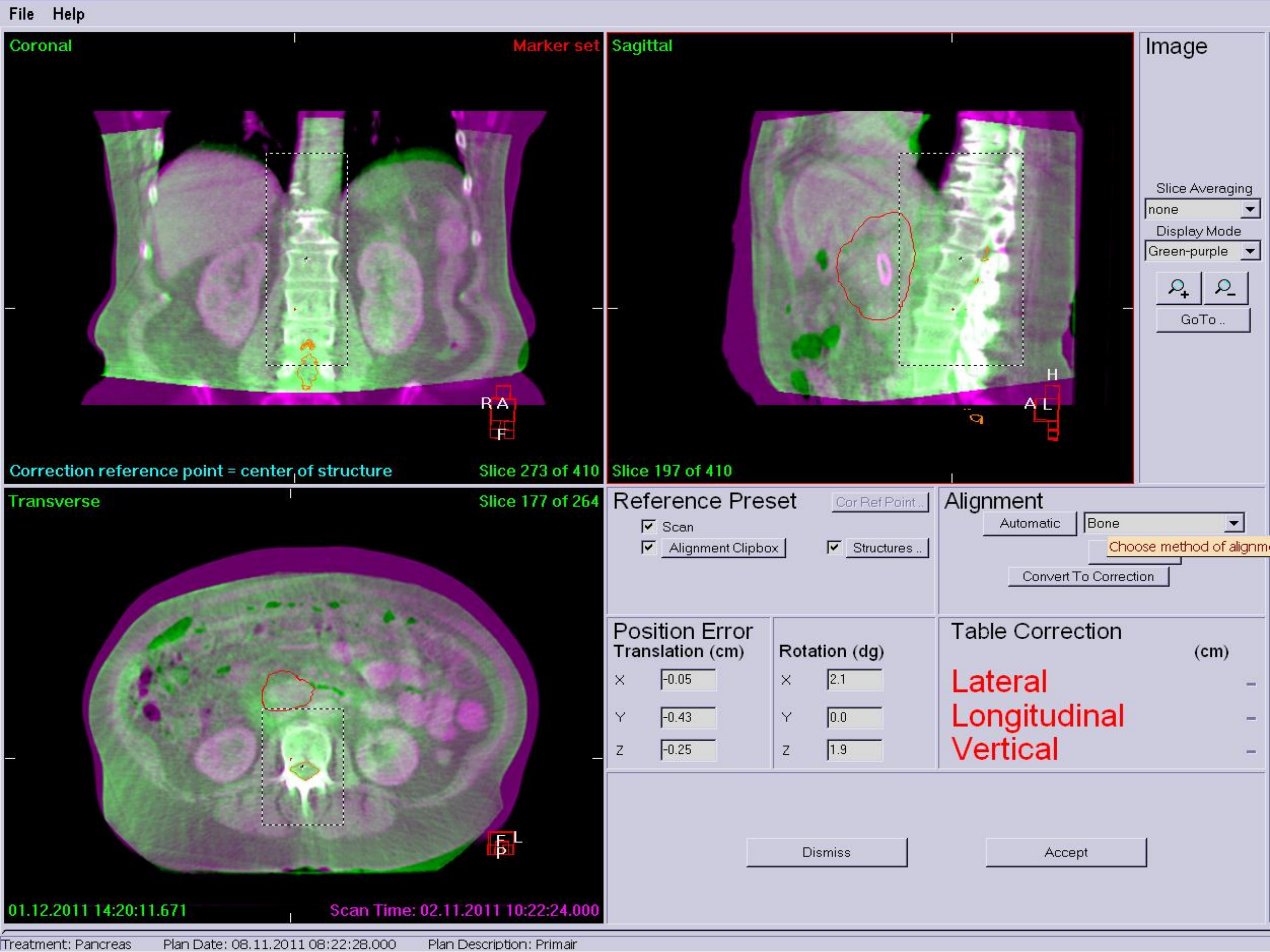
Rare changes



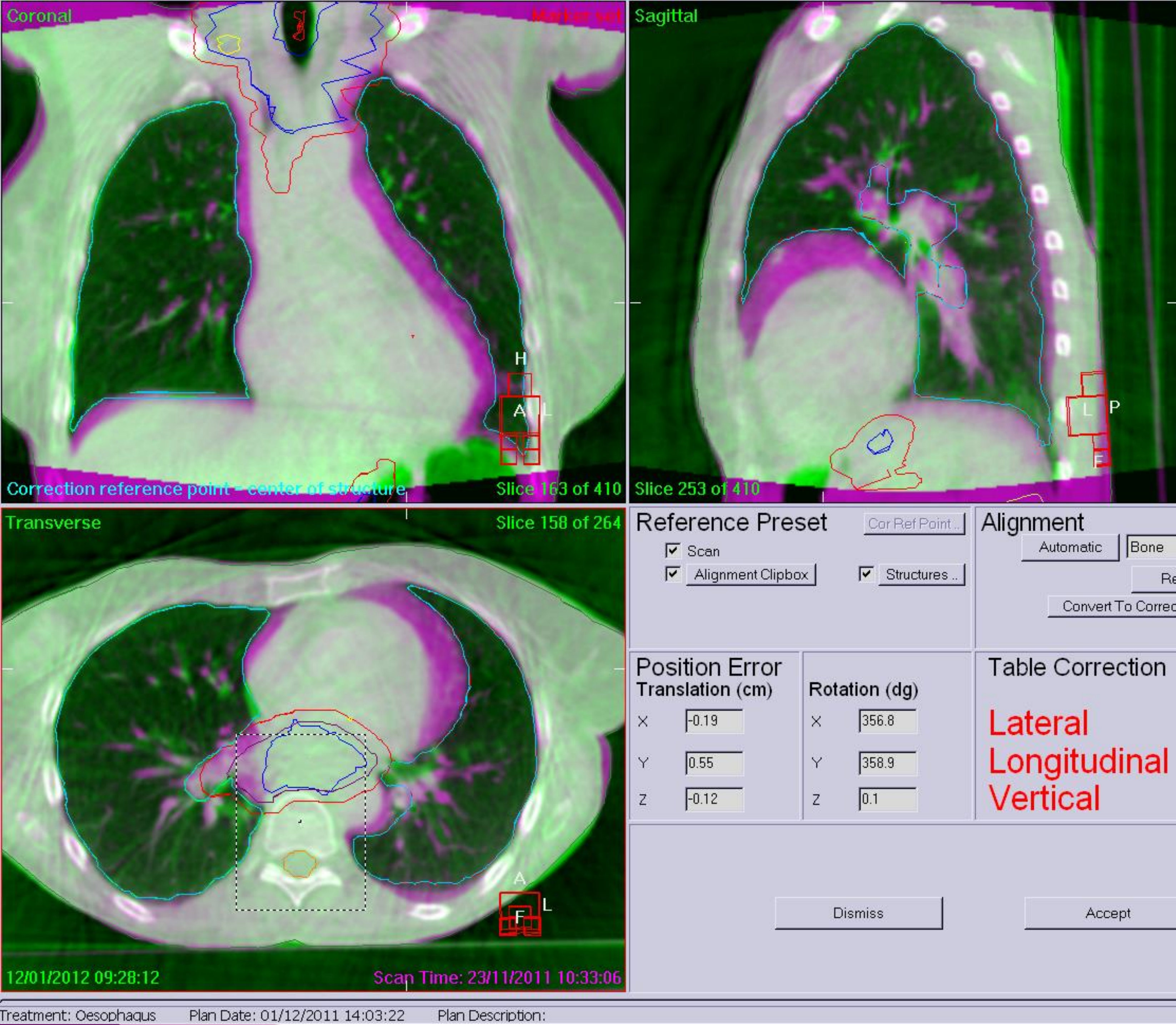
Change in lymphocele



Weight loss


File
Help
Coronal
Marker set
Sagittal
Image
Slice Averaging
none
Display Mode
Green-purple
GoTo ..
R A
F
H
A L
Correction reference point = center of structure
Slice 273 of 410
Slice 197 of 410
Transverse
Slice 177 of 264
F L
P
01.12.2011 14:20:11.671
Scan Time: 02.11.2011 10:22:24.000
Reference Preset
Cor Ref Point ..
Scan
Alignment Clipbox
Structures ..
Alignment
Automatic
Bone
Choose method of alignm
Convert To Correction
Position Error
Translation (cm)
X -0.05
Y -0.43
Z -0.25
Rotation (dg)
X 2.1
Y 0.0
Z 1.9
Table Correction
(cm)
Lateral
Longitudinal
Vertical
Dismiss
Accept
Treatment: Pancreas
Plan Date: 08.11.2011 08:22:28.000
Plan Description: Primair

Cardiac changes



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Summary

- Anatomy is changing during treatment
- RTT is the person most likely to detect
  - Should be her/his responsibility
- You can’t bother the doctor or physicist with everything…

How to deal with changing anatomy?*

- Call doctor before treatment
  - Change in atelectases
  - GTV and/or CTV outside PTV
- Contact doctor that day or the day after
  - Mild tumor progression
  - Tumor regression
- Contour changes (physicist)
  - >2 cm
  - >1cm H&N and extremities

***Inspired by:**
INTRA THORACIC ANATOMICAL CHANGES FOR LUNG CANCER PATIENTS DURING THE COURSE OF IRRADIATION: HOW TO RESPOND?
S. Conijn[1] , J. Belderbos[1] , J. Knegjens[1] , M. Rossi[1] , J. J. Sonke[1] , P. Remeijer[1]

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The protocol…

- *Describes were to look at*
- *Describes what do*
- *Describes who to contact*
- *Describes at what speed actions have to take place*

Implementation Phase

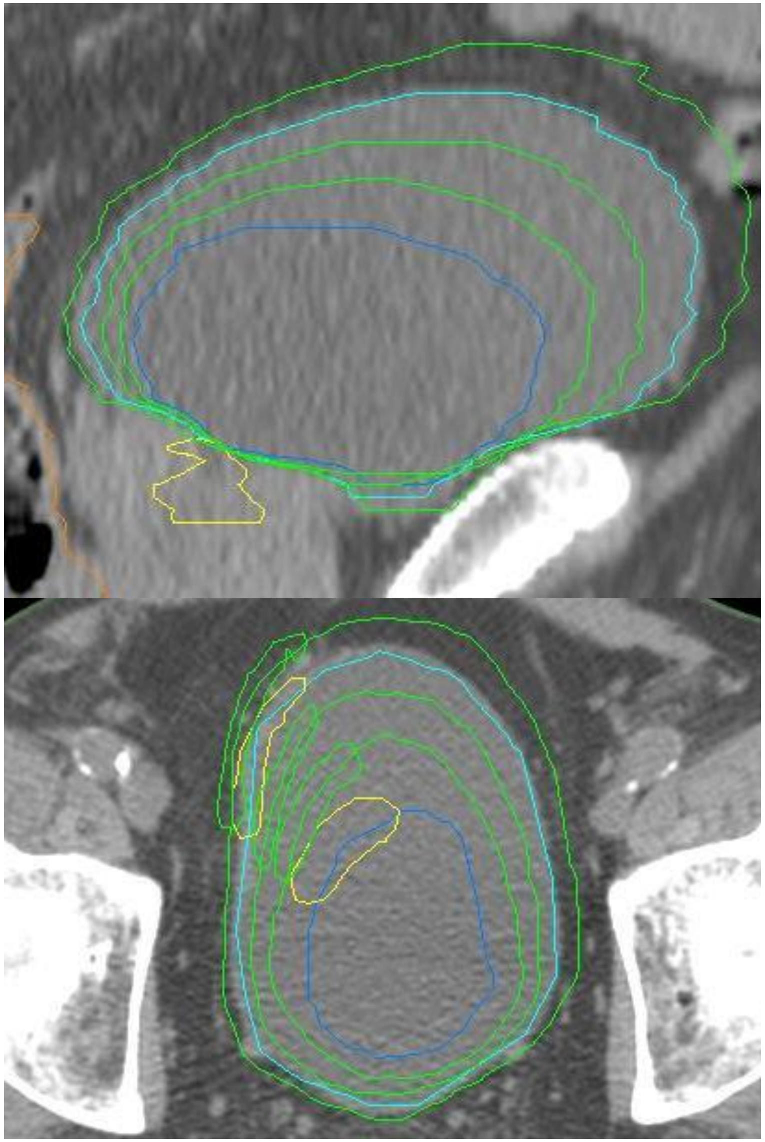
Critical conditions for proper implementation

- Treatment protocol should be:
  - Well described and tasks well defined
  - Approved by staff
  - Available for everyone
- Education and training of professionals:
  - Really depends on subject
  - Preferable as practical as possible
- Example: *Bladder ART*

Plan of the day

Inter- and extrapolation of bladder contours

– 5 plans are generated on the TPS (Oncentra, Elekta)



Images: Jorrit Visser

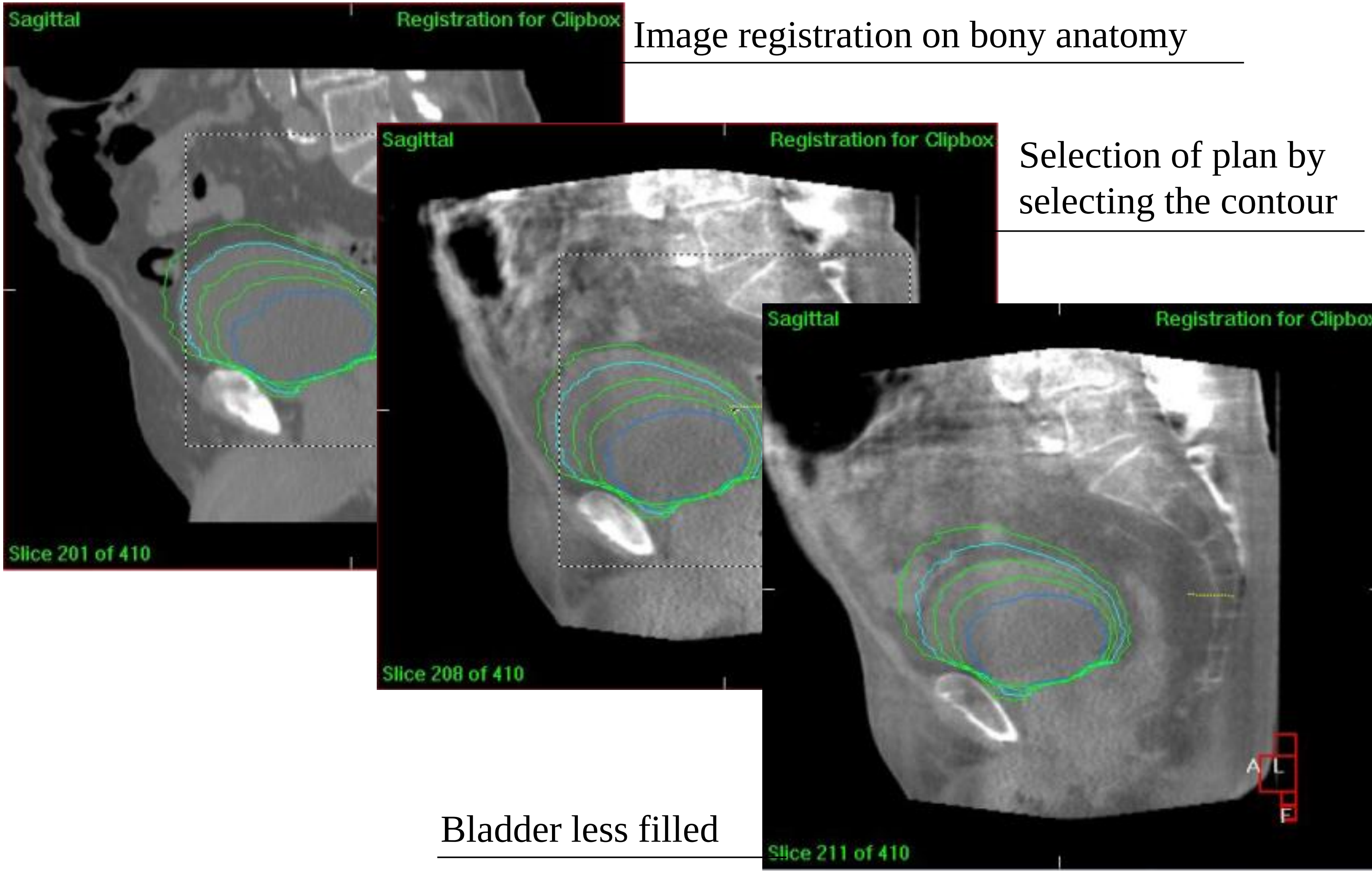


Image registration on bony anatomy

Selection of plan by selecting the contour

Bladder less filled

Images: Rianne de Jong

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Demo database ART blaas

4 patients with two reference CT

82 Conebeam CT-scans

5 structures per patient/scan:

0 – 33 – 67 – 100 – 133%

12 observers

Interobserver study: *1ᵉ measurement*

workshop

2ᵉ measurement

Implementation Phase

Critical conditions for proper implementation

- Treatment protocol should be:
  - Well described and well defined task
  - Approved by staff
  - Available for everyone

- Education and training of professionals:
  - Really depends on subject

- **Implementation date**
  - **Properly communicated**
  - **Repeat communication just before start**

- **Use a predefined checklist**

Evaluation phase

- Phase that ignored often
  - The work just started….

- Space to correct for mistakes

- Evaluate
  - ➢ Ask for feedback from your colleagues:
    - ▪ Pro active: create a feedback session
  - ➢ Data to validate new procedure
    - ▪ publish

  - ➢ Monitor your processes

Bladder ART: Safety-net plan selection

1e week

- Doctor, physicist and IGART RTT on the linac
- Fixed moment

Starting of the 2e week

- IGART RTT on the linac
- Fixed moment

After 10 patients

- evaluation and feedback - database oefenpatiënten? -

Once weekly one dedicated IGART RTT check all decisions:

- Was the "right" selected?
- Is the used model still valid?
- Was the used treatment plan in the R&V system selected?

Conclusions

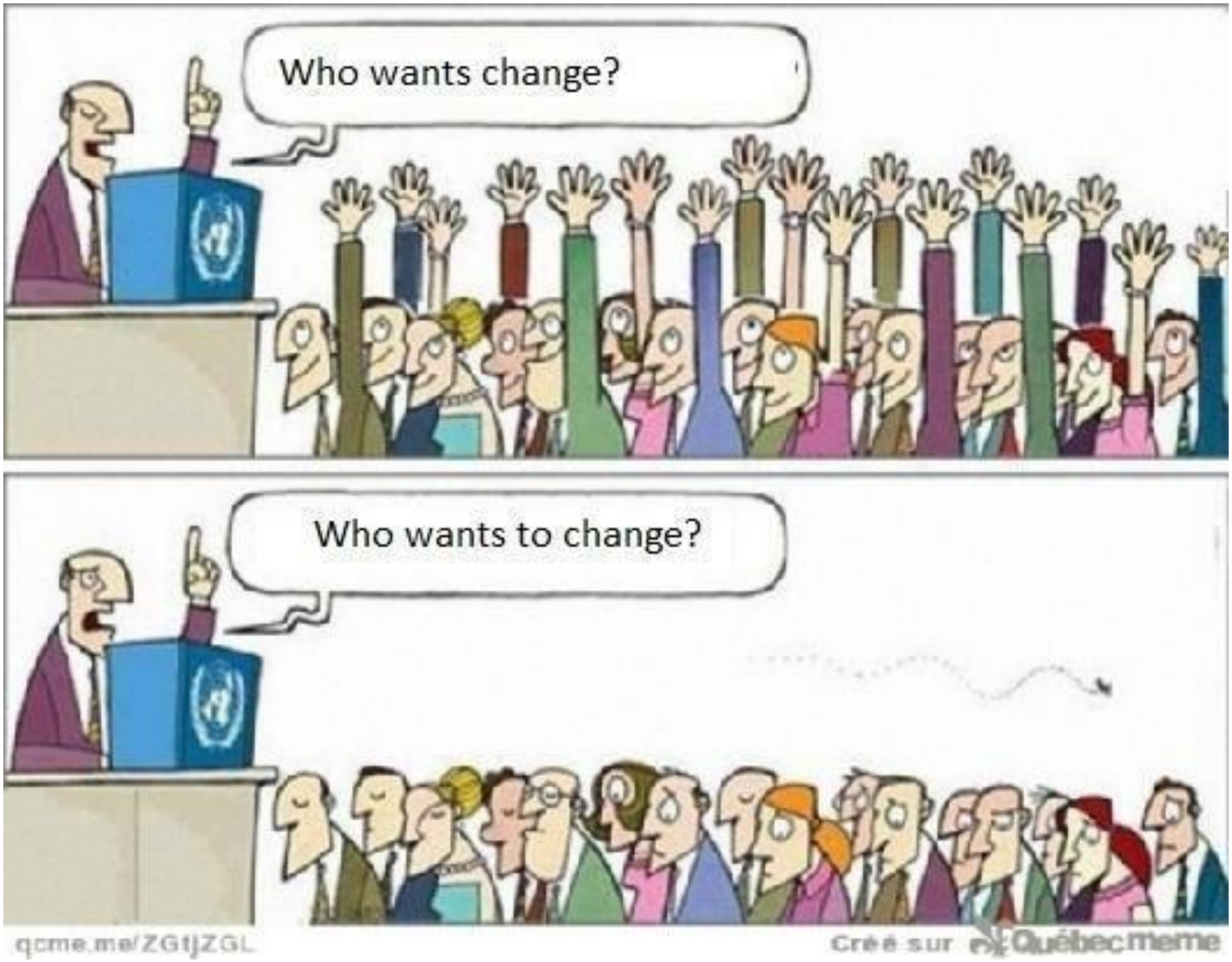
Implementing protocols:

- Investigate
- Plan
- Implement
- Evaluate

Implementing protocols is a change process:

John Kotter's 8 steps of change

John Kotter: Leading Change (1995)


Who wants change?
Who wants to change?
qcme.me/ZGtjZGL
Créé sur Québecmeme

Thank you for your attention!

Who is doing what in Radiation Therapy

Rianne de Jong *RTT*,
Amsterdam Medical Centre

m.a.j.dejong@amc.uva.nl

NKI-AVL
The Netherlands Cancer Institute
Antoni van Leeuwenhoek Hospital

Survey

Questionnaires to participants of ESTRO course on "IGRT in clinical practice" in 2006-2010:

48 hospitals

19 countries

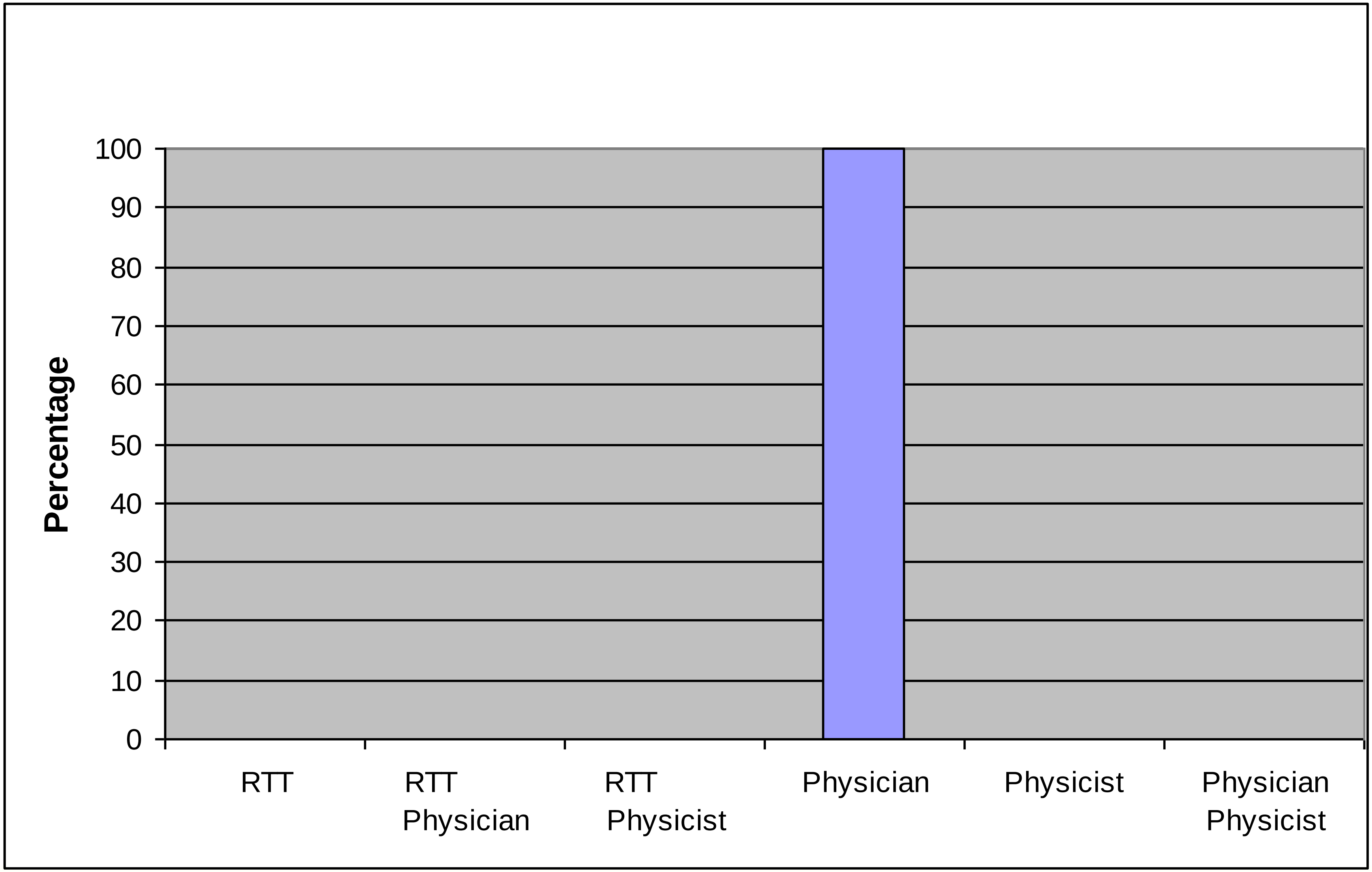
Survey

1. Indication/Design of Radiation Treatment
2. Pre treatment imaging: CT/simulation
3. Delineation
4. Treatment Planning
5. Treatment
6. Image Guidance/Adaptation treatment

→

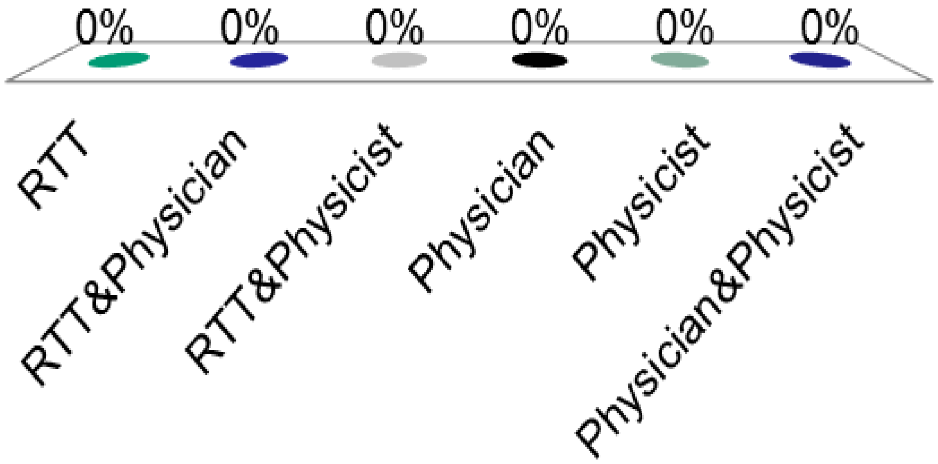
- Radiation Therapy Technicians (RTT)
- Physicians
- Physicists

1. Indication of treatment

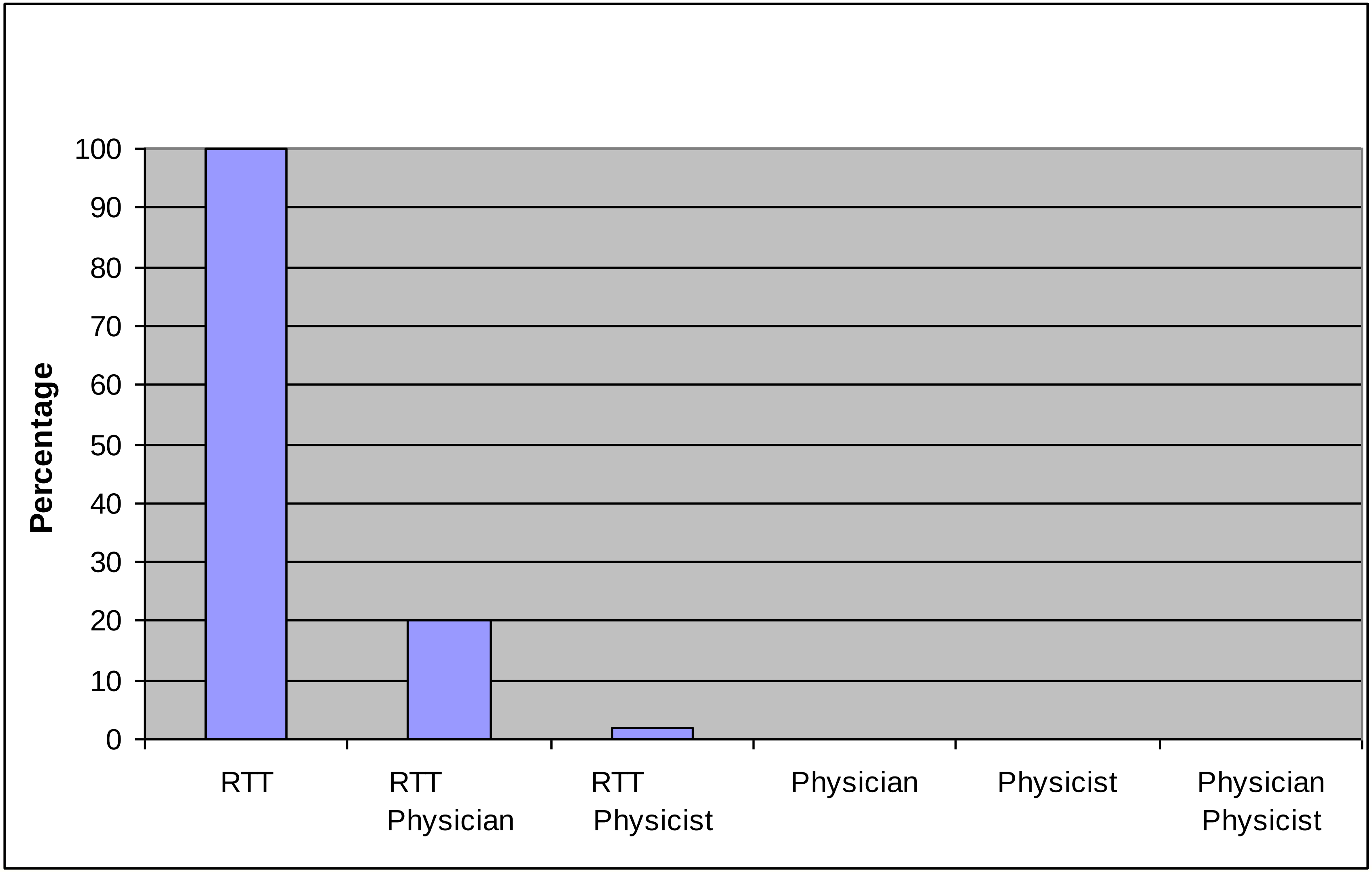


1. Indication of treatment

A. RTT
B. RTT&Physician
C. RTT&Physicist
D. Physician
E. Physicist
F. Physician&Physicist

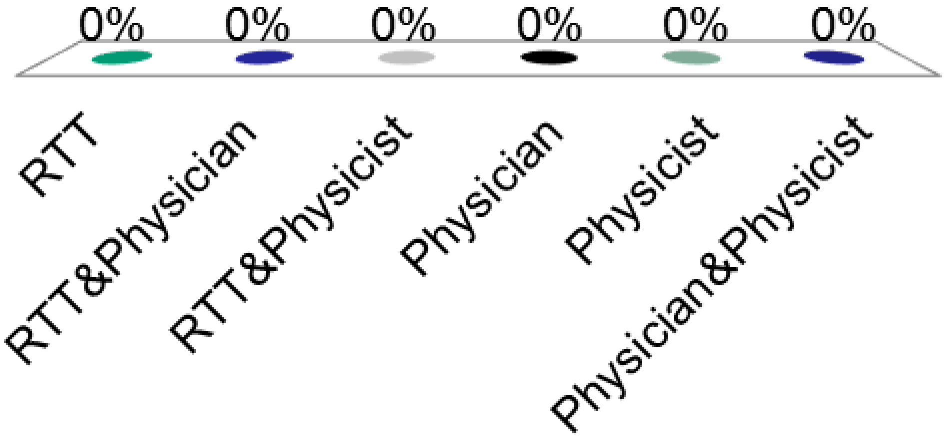


2. Pre-treatment Imaging

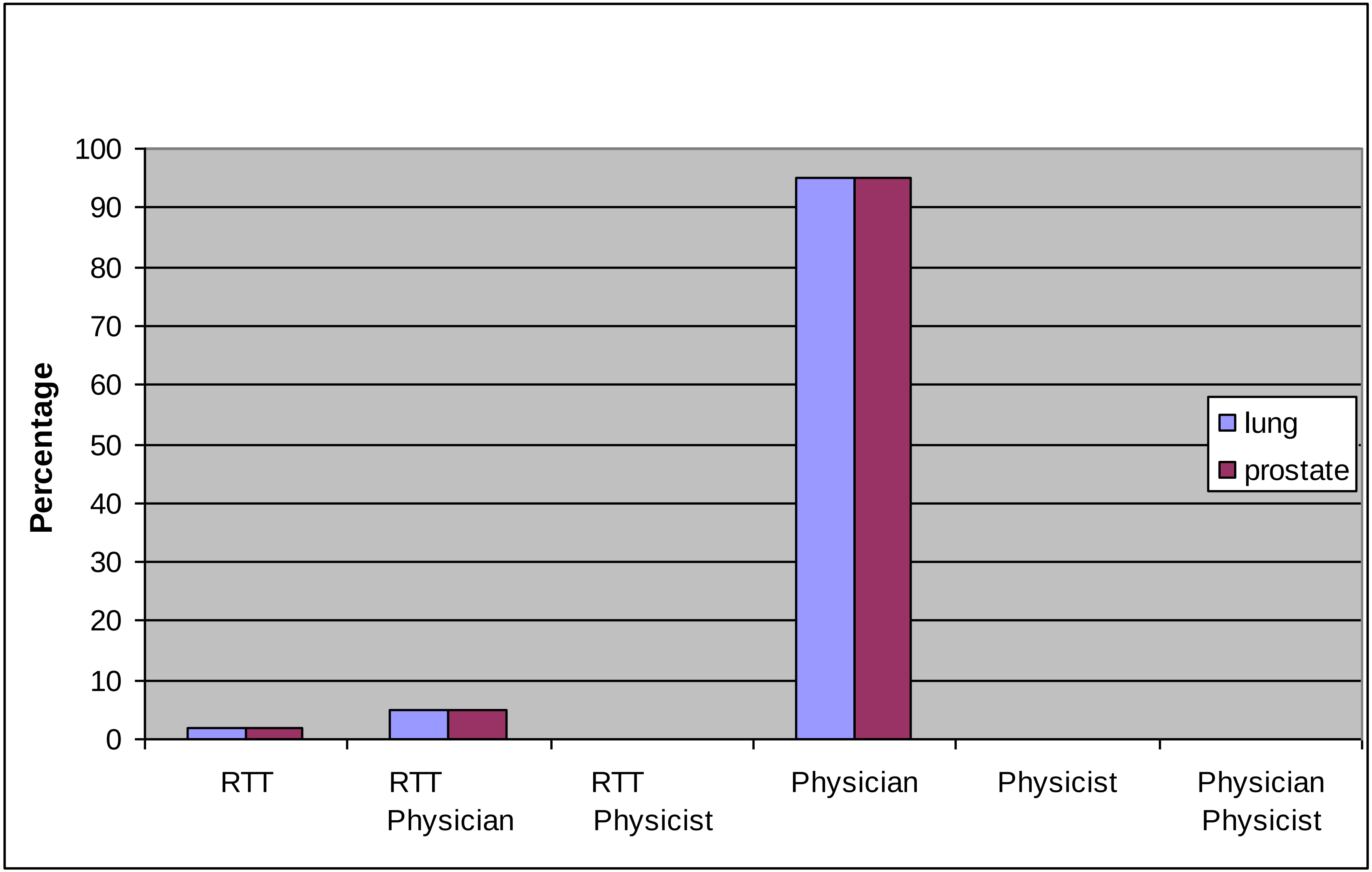


2. Pre treatment Imaging

A. RTT
B. RTT&Physician
C. RTT&Physicist
D. Physician
E. Physicist
F. Physician&Physicist

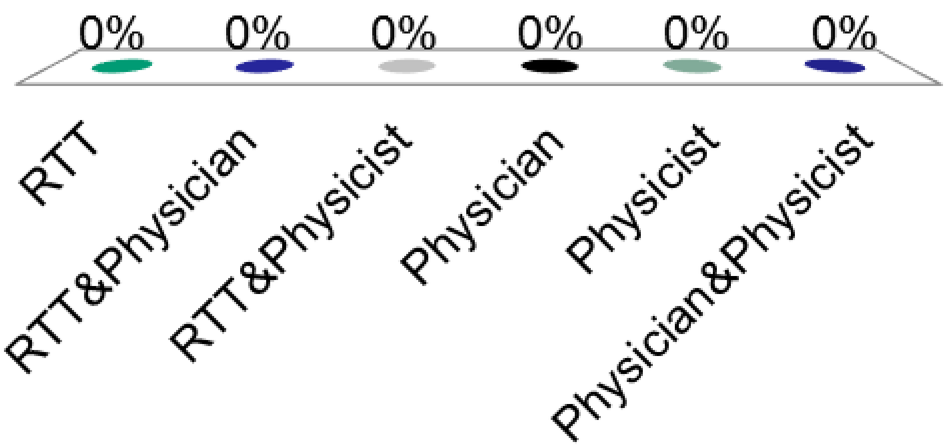


3. Delineation: Target Volume

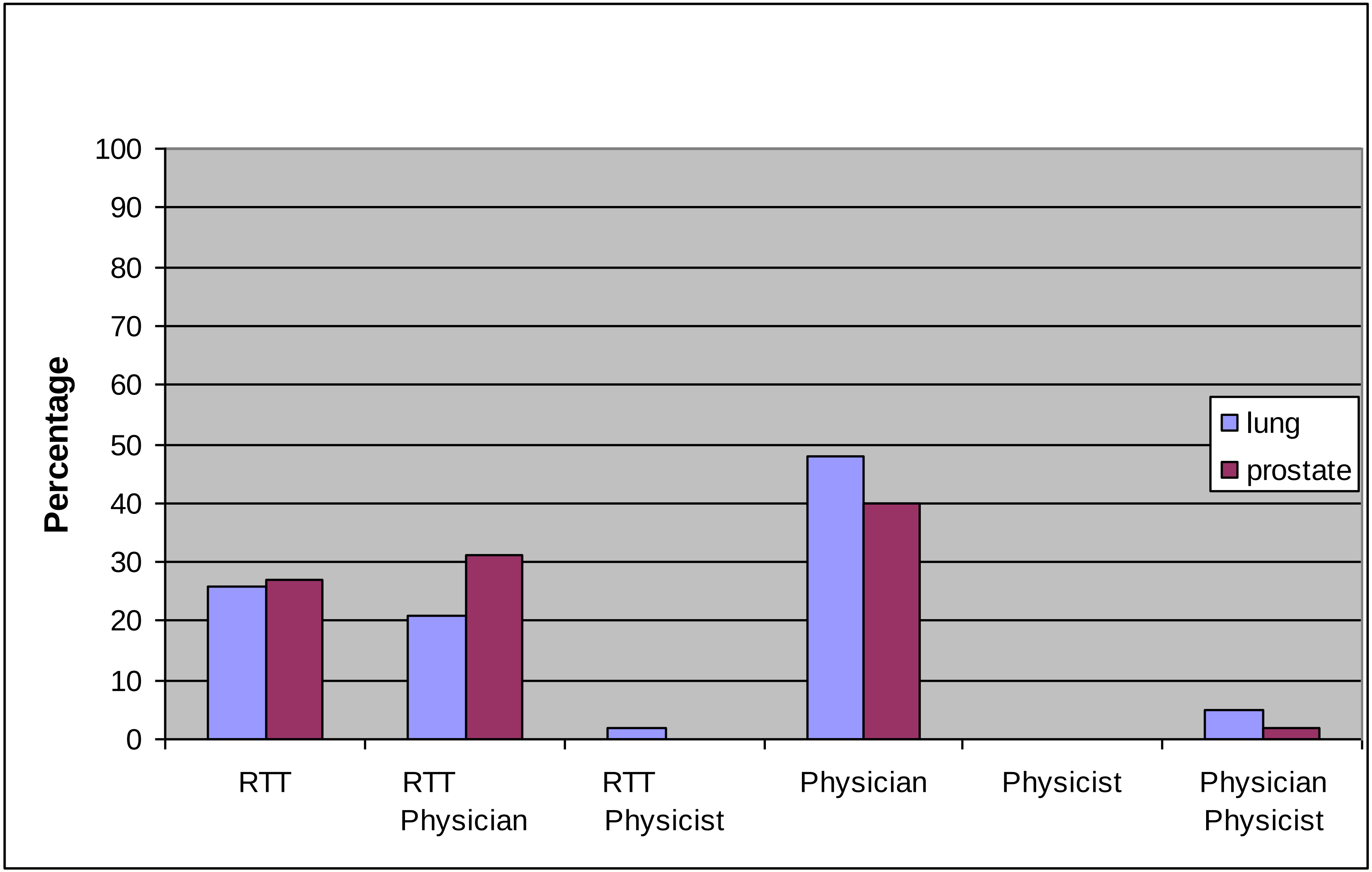


3. Delineation Target Volume

A. RTT
B. RTT&Physician
C. RTT&Physicist
D. Physician
E. Physicist
F. Physician&Physicist

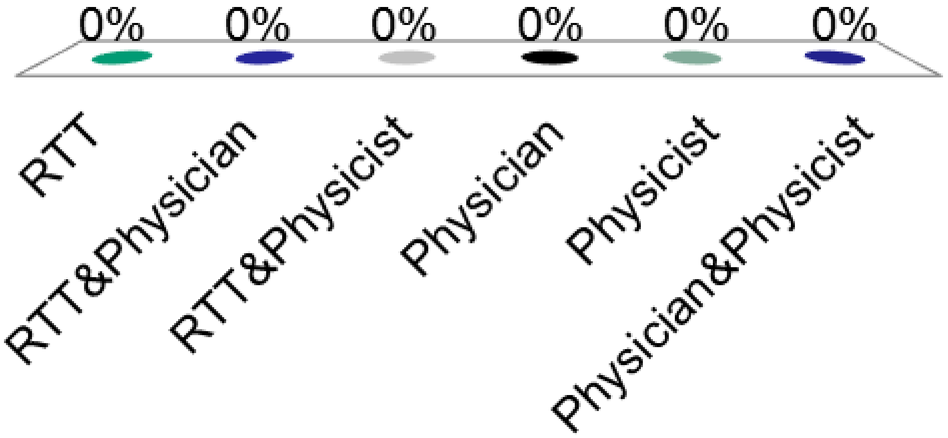


3. Delineation: Organs at Risk

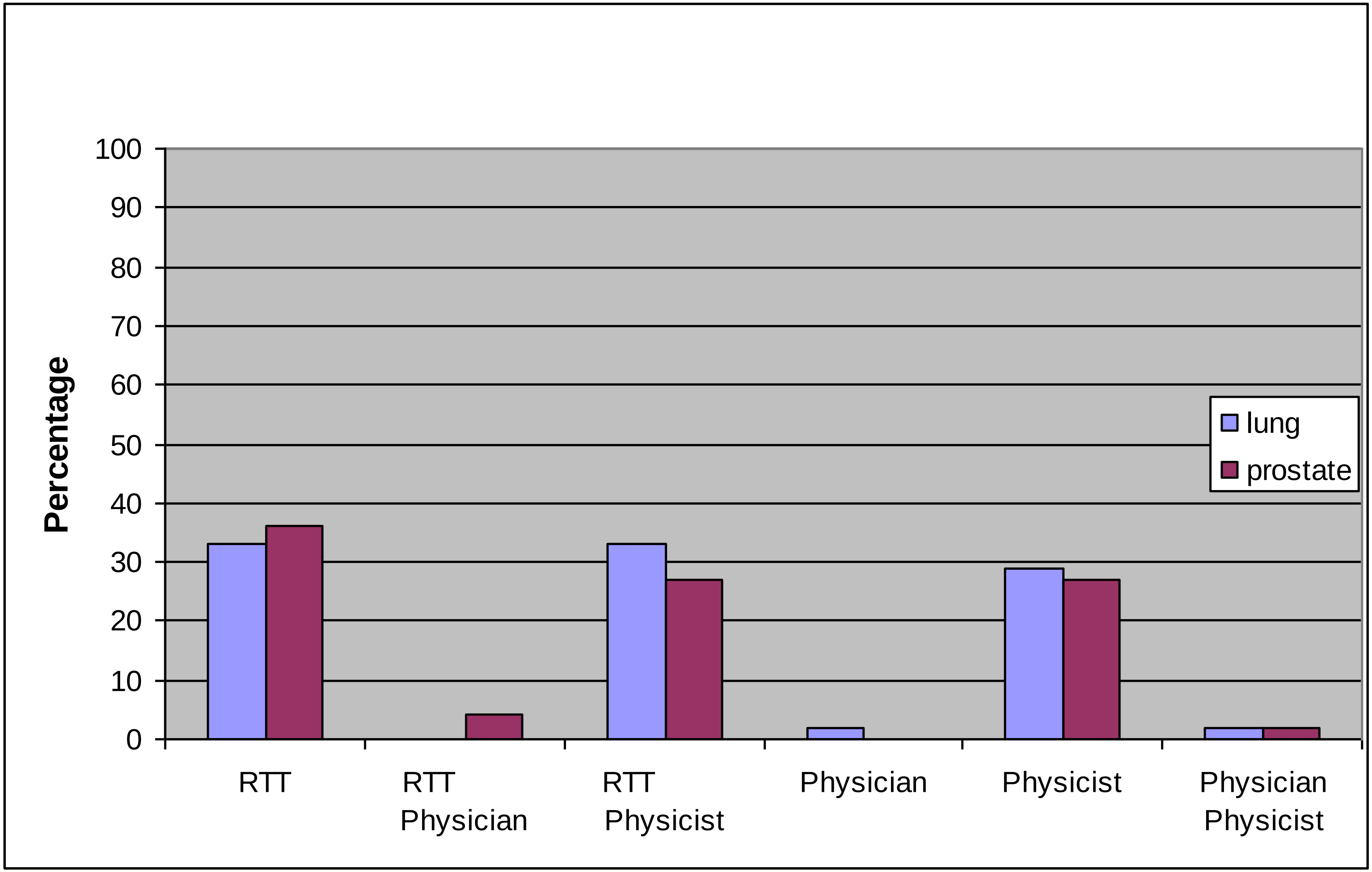


3. Delineation Organs at Risk

A. RTT
B. RTT&Physician
C. RTT&Physicist
D. Physician
E. Physicist
F. Physician&Physicist



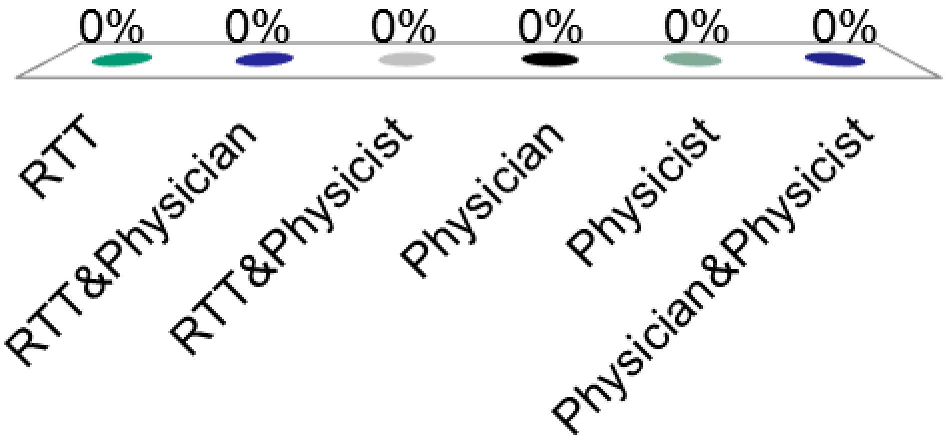
4. Treatment Planning



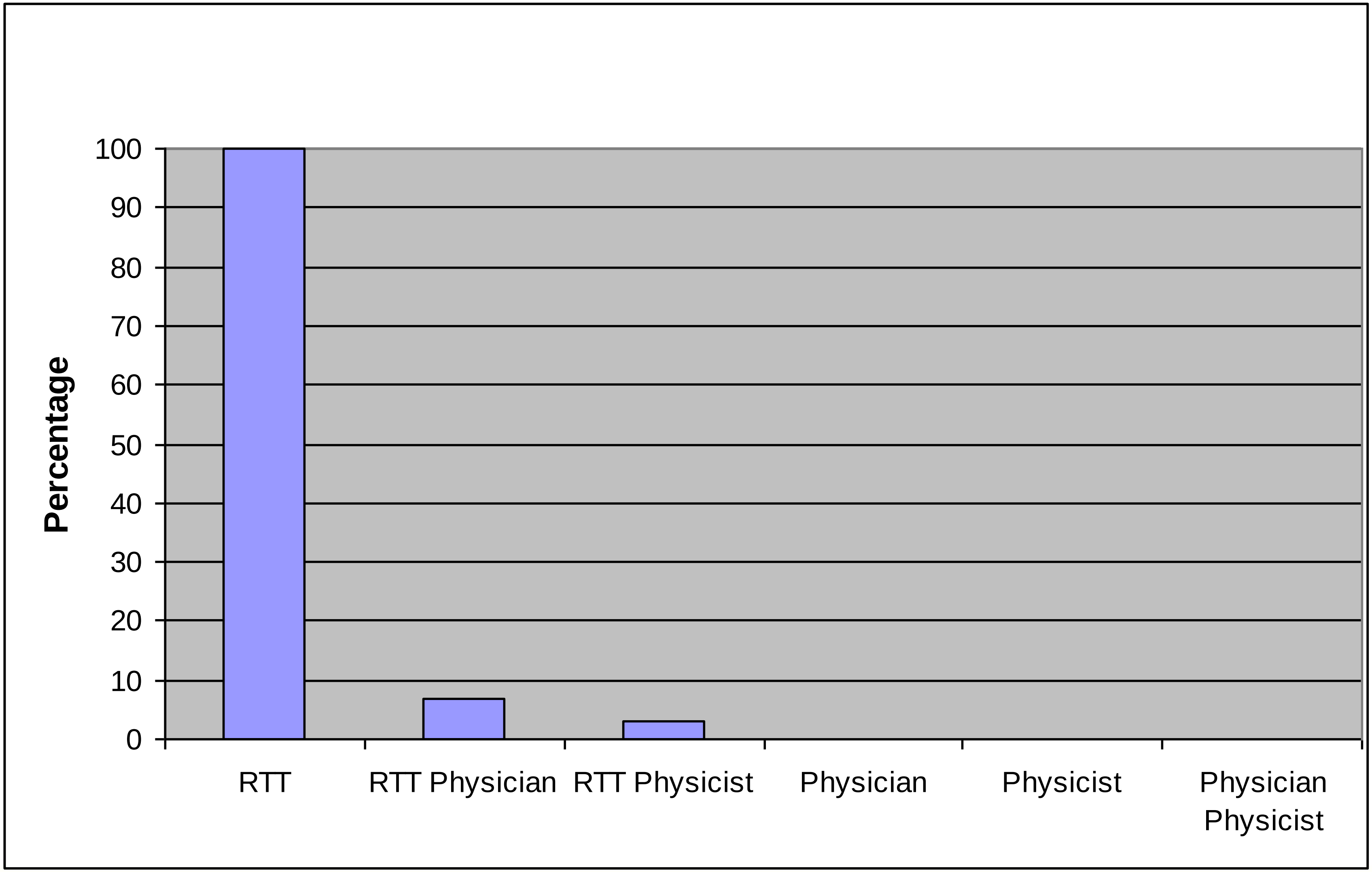
RTT: supervised and/or accepted by physician or physicist

4. Treatment Planning

A. RTT
B. RTT&Physician
C. RTT&Physicist
D. Physician
E. Physicist
F. Physician&Physicist

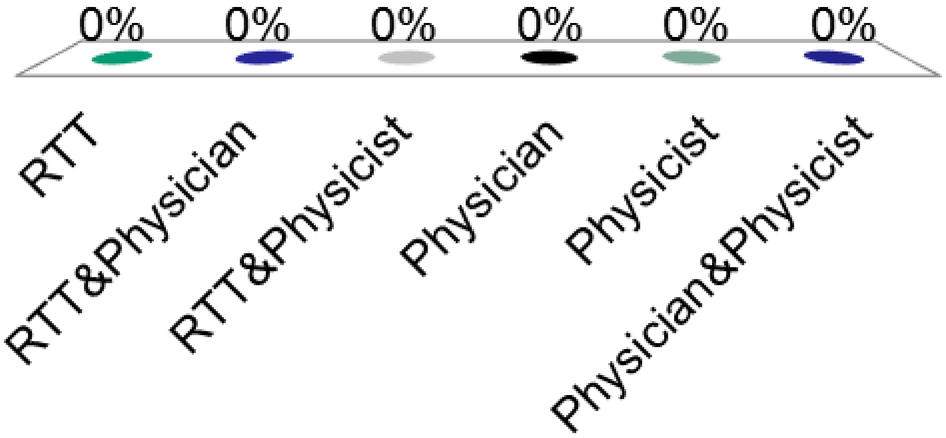


5. Treatment Delivery

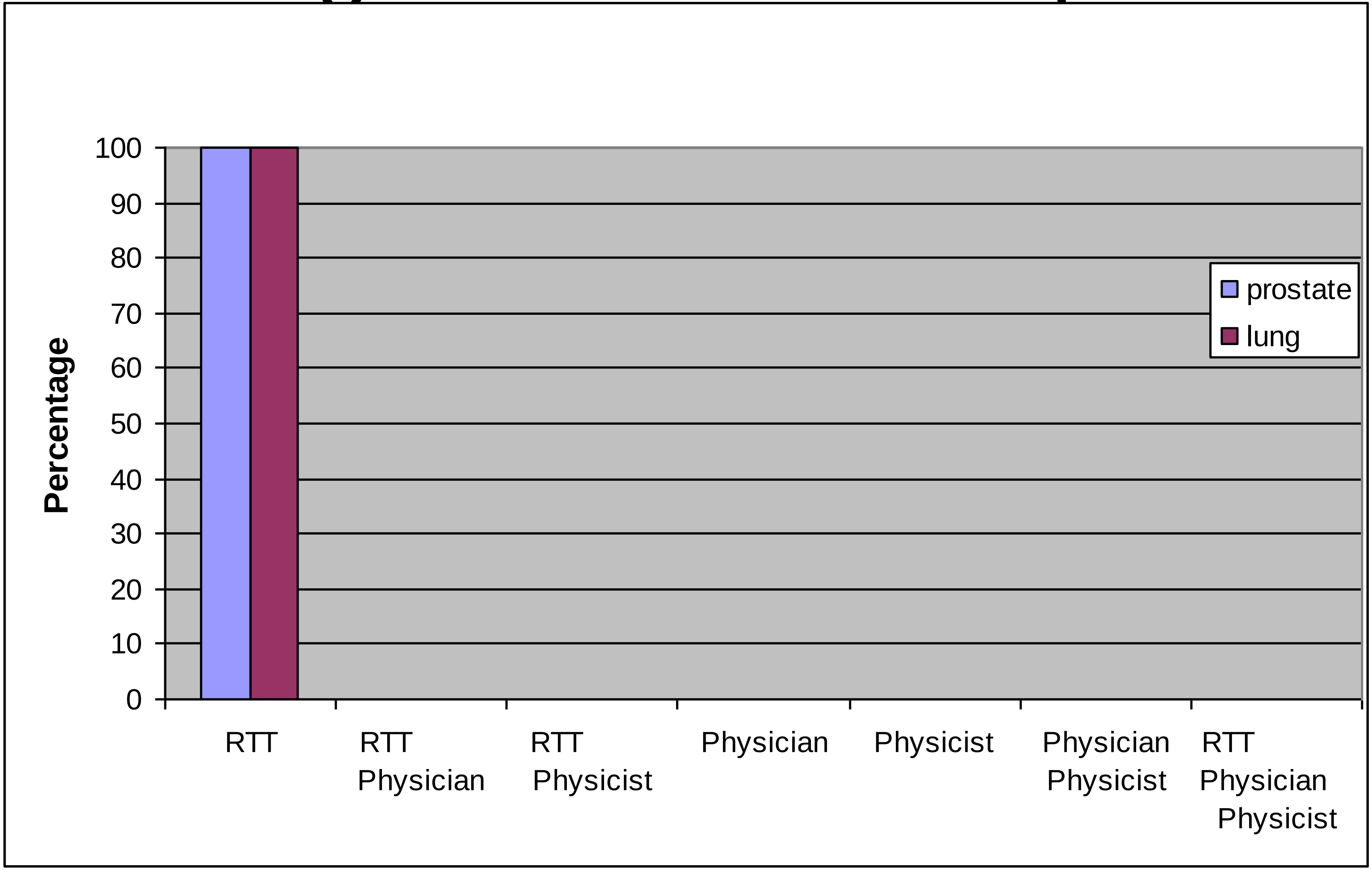


5. Treatment Delivery

A. RTT
B. RTT&Physician
C. RTT&Physicist
D. Physician
E. Physicist
F. Physician&Physicist

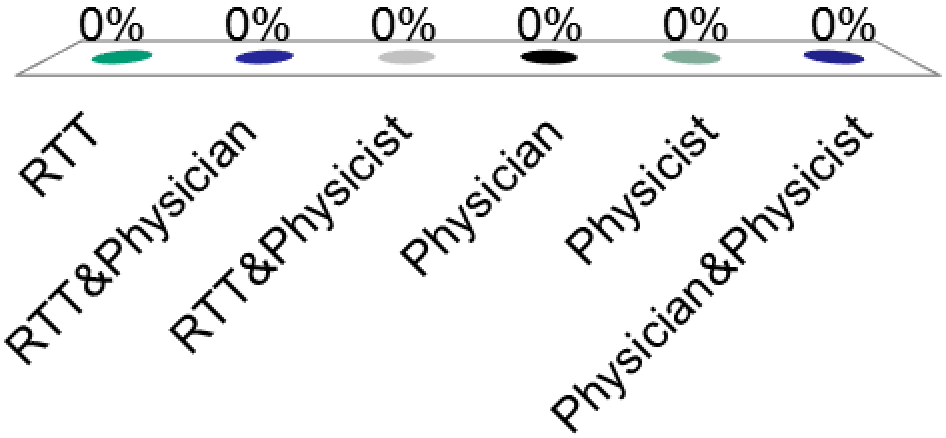


6a. Image Guidance: Acquisition

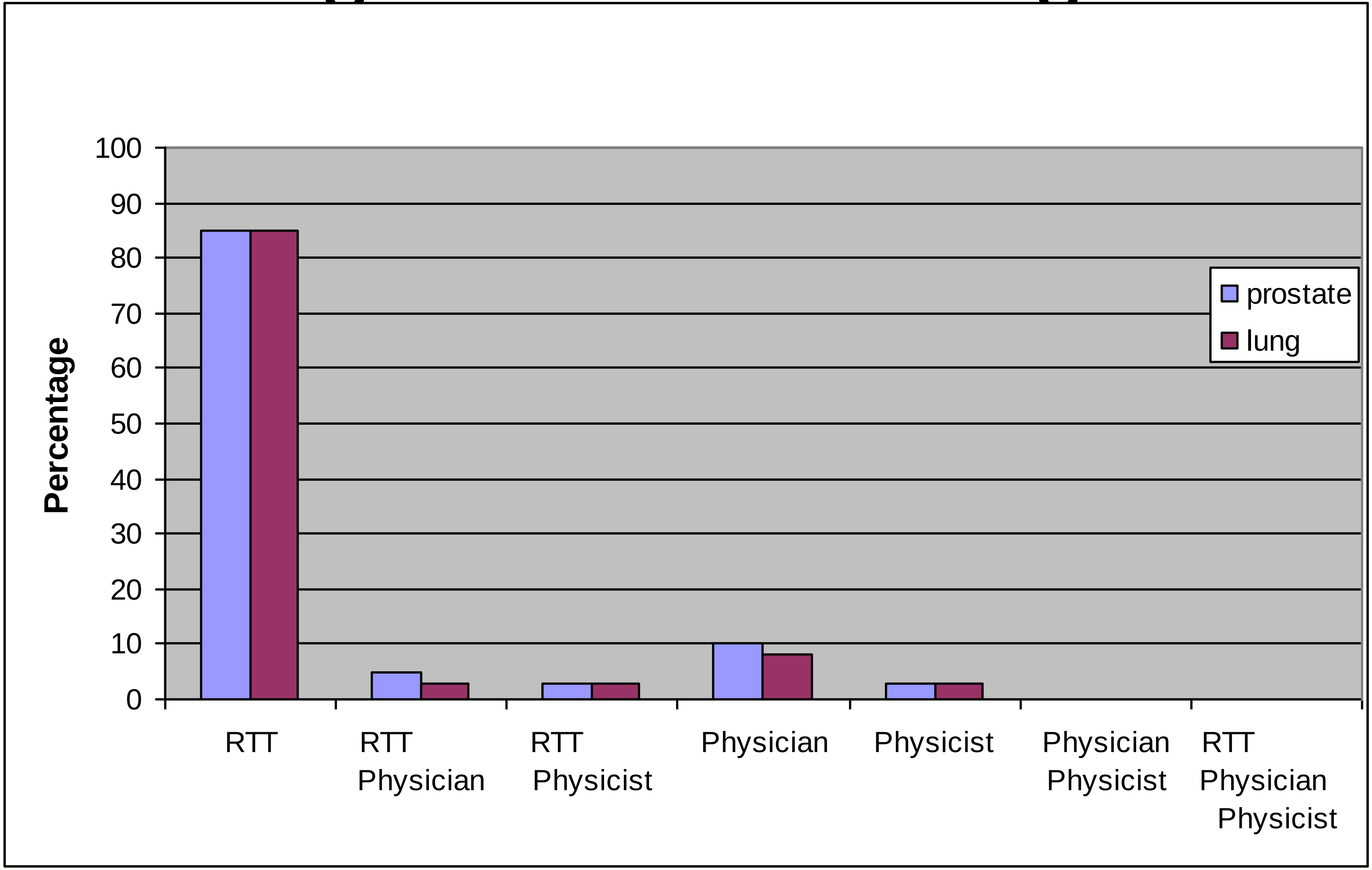


6a. Image guidance: Acquisition

A. RTT
B. RTT&Physician
C. RTT&Physicist
D. Physician
E. Physicist
F. Physician&Physicist

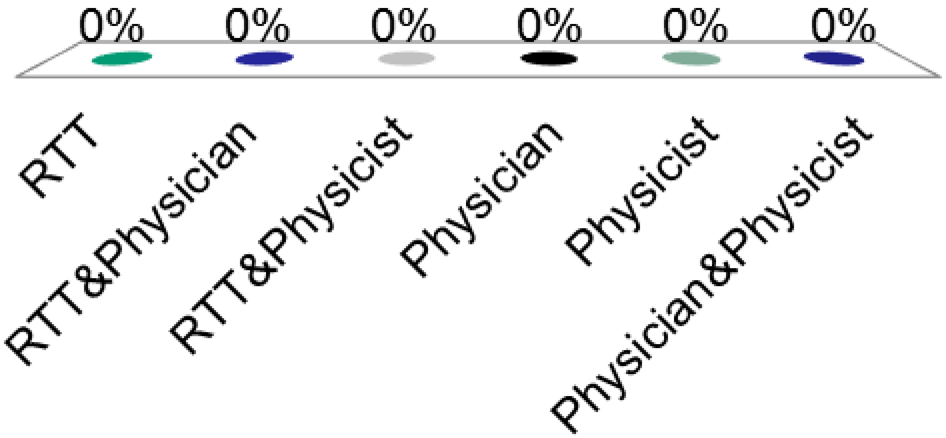


6b. Image Guidance: Registration

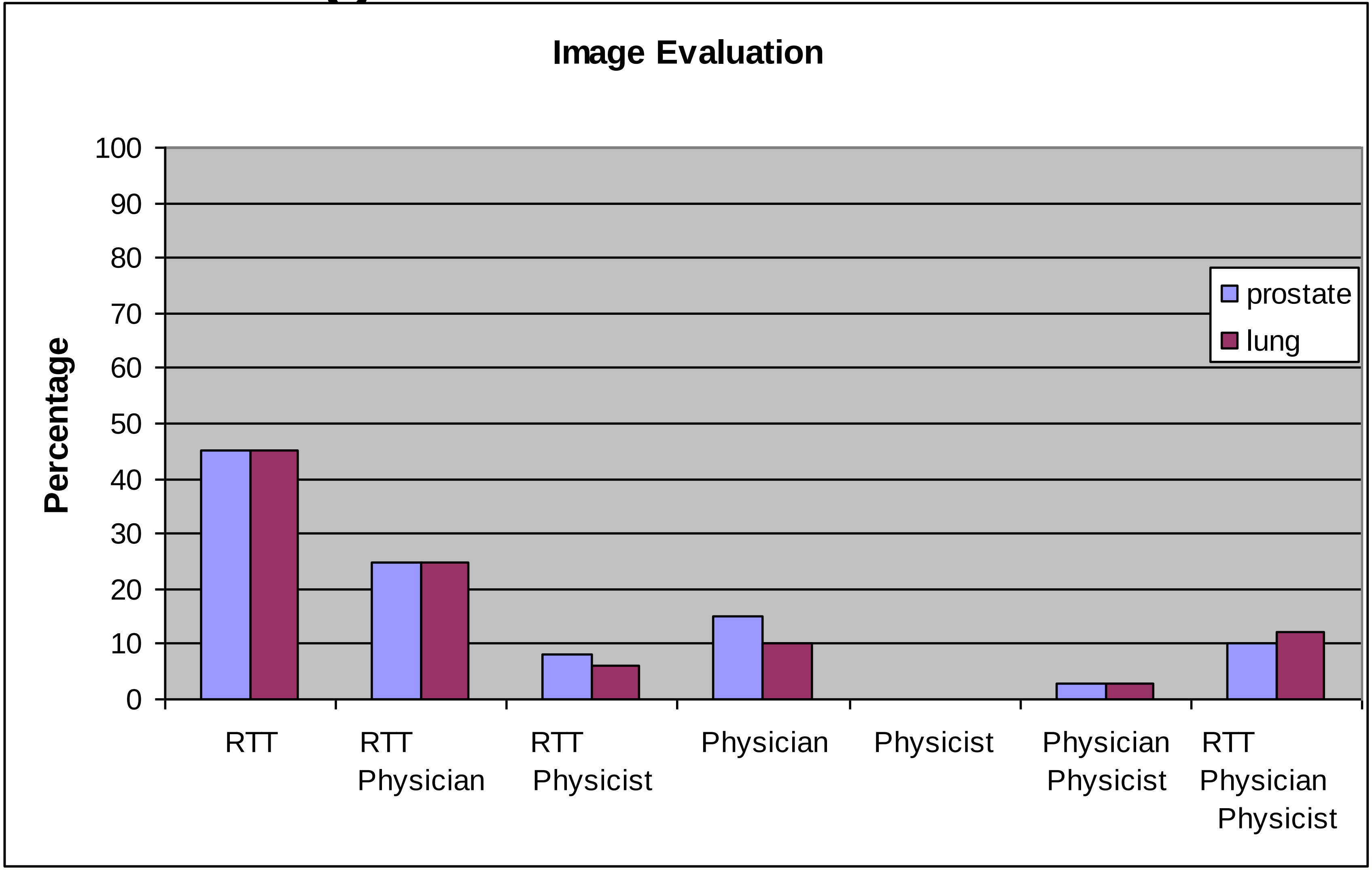


6b. Image Guidance: Registration

A. RTT
B. RTT&Physician
C. RTT&Physicist
D. Physician
E. Physicist
F. Physician&Physicist

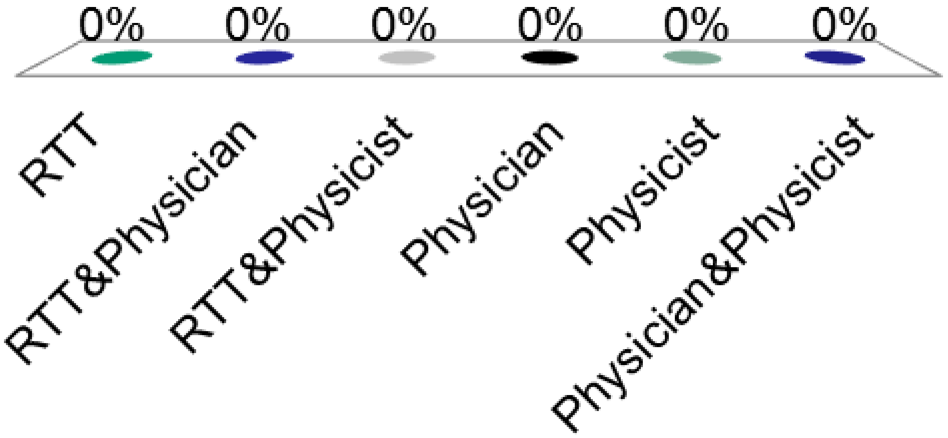


6c. Image Guidance: Evaluation



6c. Image Guidance: Evaluation

A. RTT
B. RTT&Physician
C. RTT&Physicist
D. Physician
E. Physicist
F. Physician&Physicist



Who is doing what?

Conclusion: Largest differences in ***Treatment Planning*** and ***Image Guidance***.

Why? What are the **variables** in the different departments that could have an influence on these differences?

- RTT – education / training
- Department size
- Resources per treatment machine
- IGRT modalities
- *Culture / History*
- *Money*

RTT training / Education

Majority:

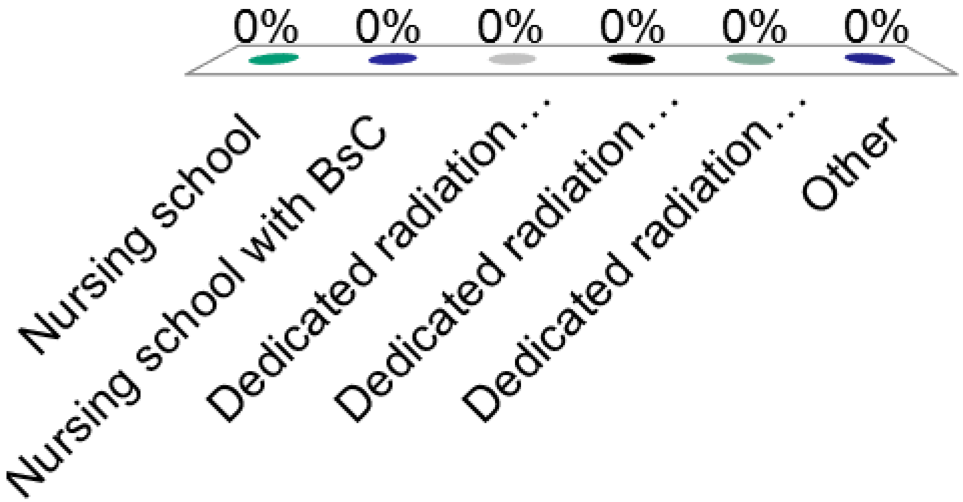
- 3 years of classroom combined with clinical intern hours → bachelor degree

Also:

- 2 or 4 years of classroom combined with clinical intern hours → bachelor degree
- 3 years of nursing school with bachelor degree with additional theoretical or clinical RTT training ~1 year.

Training & Education

A. Nursing school
B. Nursing school with BsC
C. Dedicated radiation therapy
D. Dedicated radiation therapy with Bsc
E. Dedicated radiation therapy with MsC
F. Other



RTT training / Education

Majority:

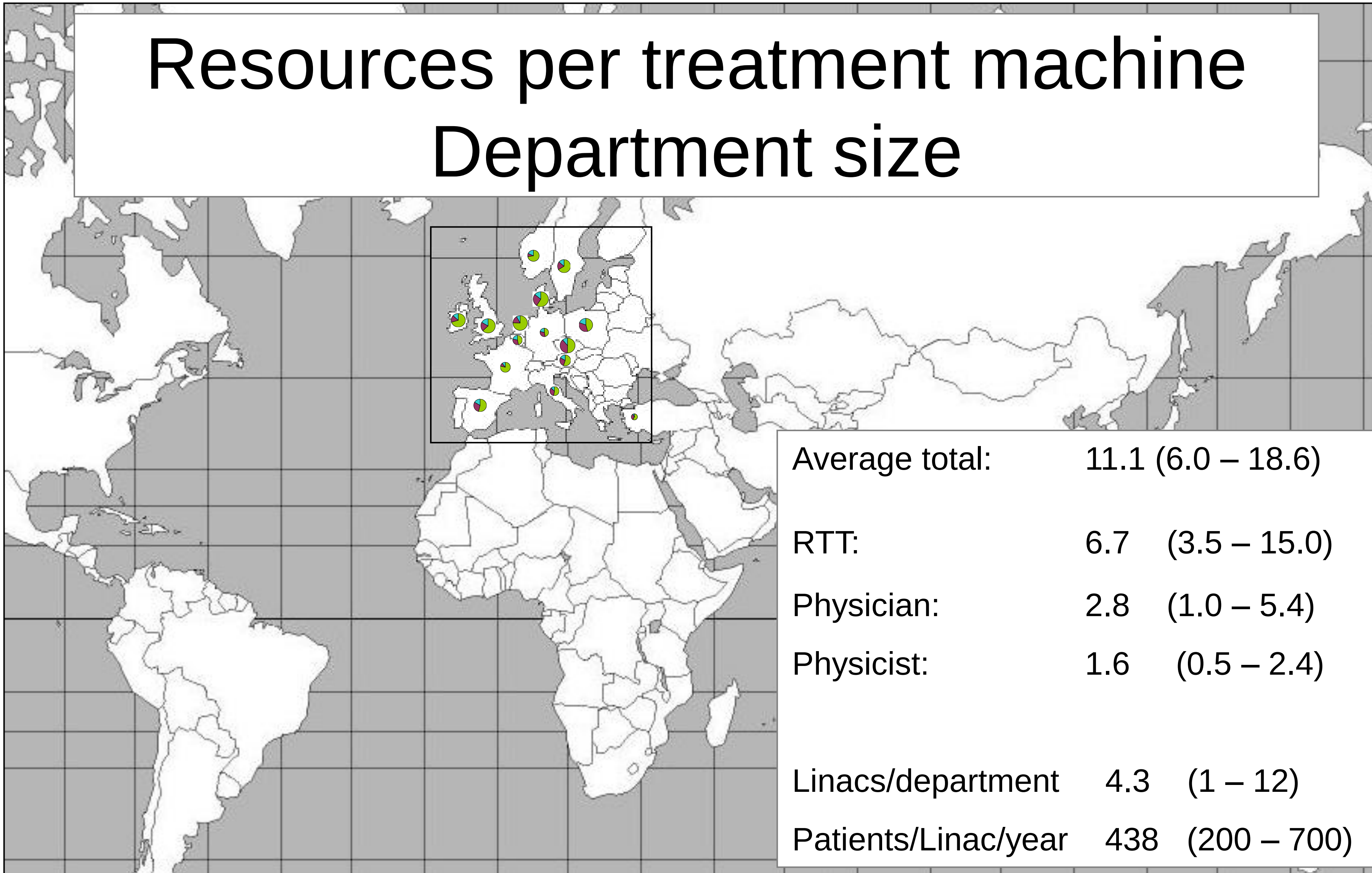
- 3 years of classroom combined with clinical intern hours
  → bachelor degree

Does not correlate

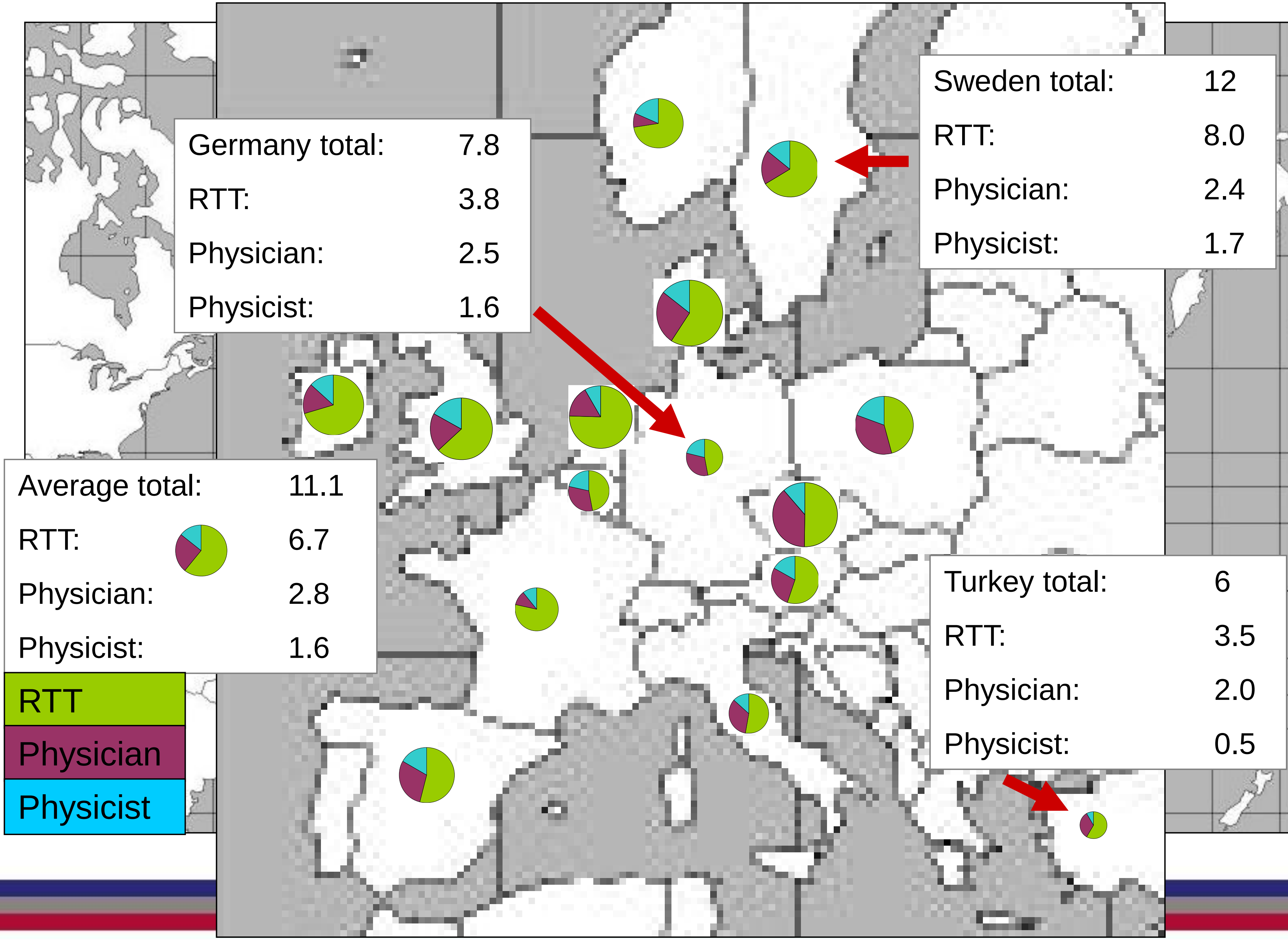
Also:

- 2 or 4 years of classroom combined with clinical intern hours → bachelor degree
- 3 years of nursing school with bachelor degree with additional theoretical or clinical RTT training ~1 year.

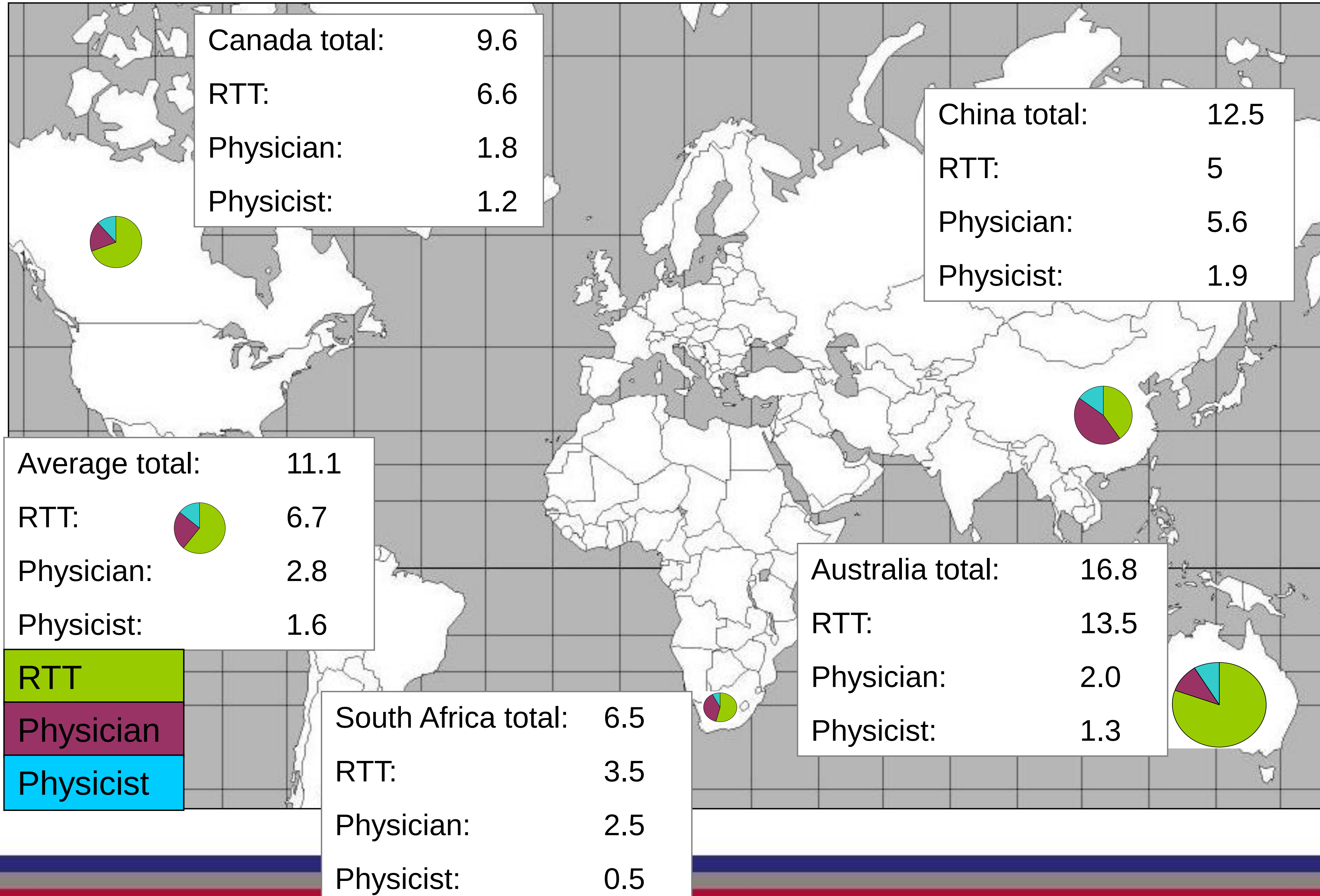
Resources per treatment machine
Department size

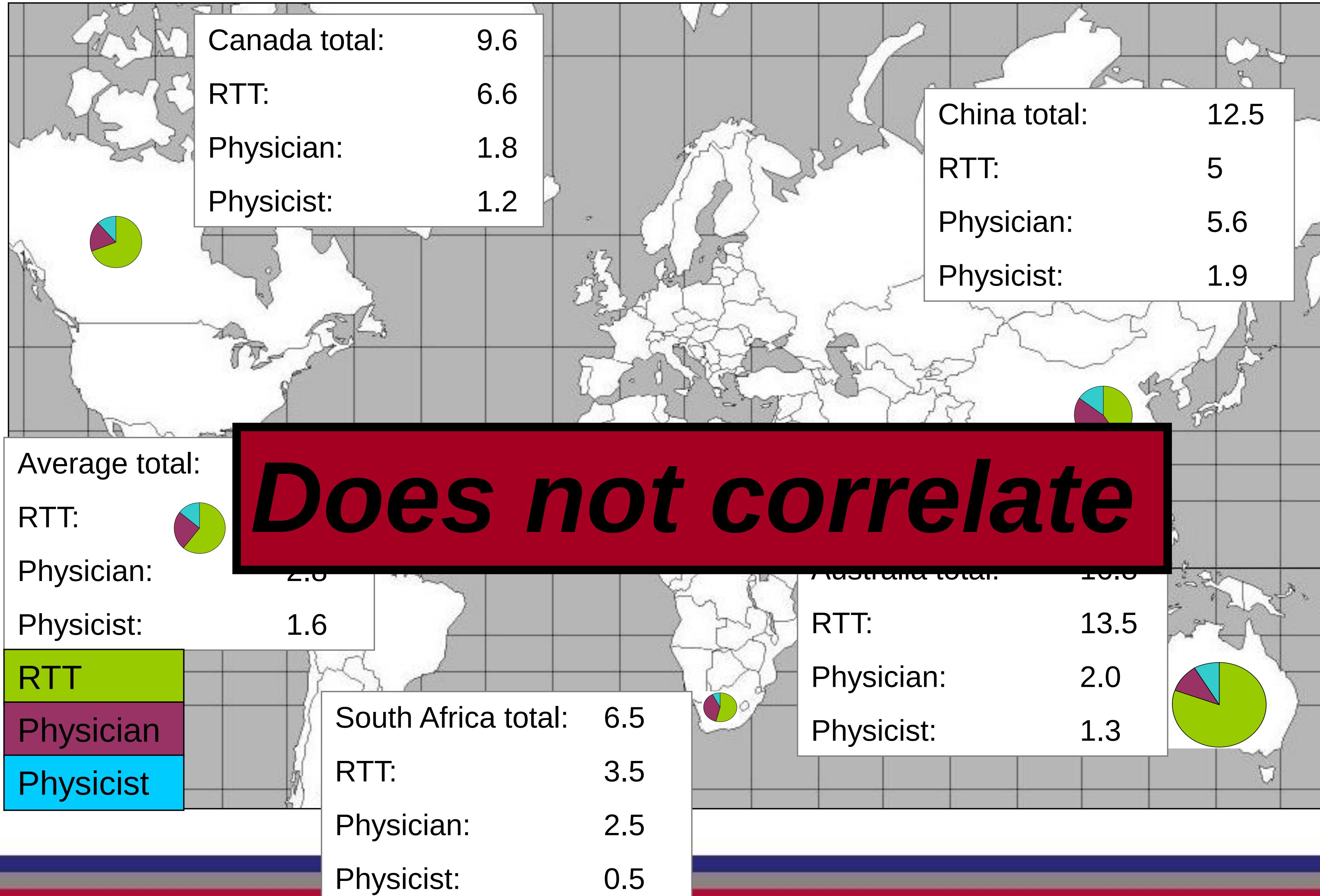


Average total:	11.1	(6.0 – 18.6)
RTT:	6.7	(3.5 – 15.0)
Physician:	2.8	(1.0 – 5.4)
Physicist:	1.6	(0.5 – 2.4)
Linacs/department	4.3	(1 – 12)
Patients/Linac/year	438	(200 – 700)



Sweden total: 12
RTT: 8.0
Physician: 2.4
Physicist: 1.7
Germany total: 7.8
RTT: 3.8
Physician: 2.5
Physicist: 1.6
Average total: 11.1
RTT: 6.7
Physician: 2.8
Physicist: 1.6
Turkey total: 6
RTT: 3.5
Physician: 2.0
Physicist: 0.5
RTT
Physician
Physicist


Canada total: 9.6
RTT: 6.6
Physician: 1.8
Physicist: 1.2
China total: 12.5
RTT: 5
Physician: 5.6
Physicist: 1.9
Average total: 11.1
RTT: 6.7
Physician: 2.8
Physicist: 1.6
RTT
Physician
Physicist
Australia total: 16.8
RTT: 13.5
Physician: 2.0
Physicist: 1.3
South Africa total: 6.5
RTT: 3.5
Physician: 2.5
Physicist: 0.5


Canada total: 9.6
RTT: 6.6
Physician: 1.8
Physicist: 1.2
China total: 12.5
RTT: 5
Physician: 5.6
Physicist: 1.9
Average total:
RTT:
Physician:
Physicist: 1.6
Does not correlate
RTT: 13.5
Physician: 2.0
Physicist: 1.3
South Africa total: 6.5
RTT: 3.5
Physician: 2.5
Physicist: 0.5
RTT
Physician
Physicist

IGRT

<u>IGRT Modalities:</u>

2D Portal Images	79%
2D kV Images	6%
kV Conebeam CT	66%
MV Conebeam CT	17%

<u>IGRT protocols are:</u>

– **Tumor site specific**	**100%**
– Patient specific	18%
– Physician specific	2%

IGRT modalities: 2D MV

A. Yes
B. No

IGRT modalities: 2D kV

A. Yes
B. No

IGRT modalities: 3D kV

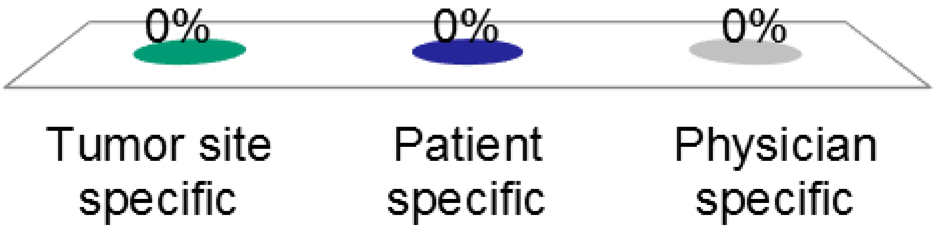
A. Yes
B. No

IGRT modalities: 3D MV

A. Yes
B. No

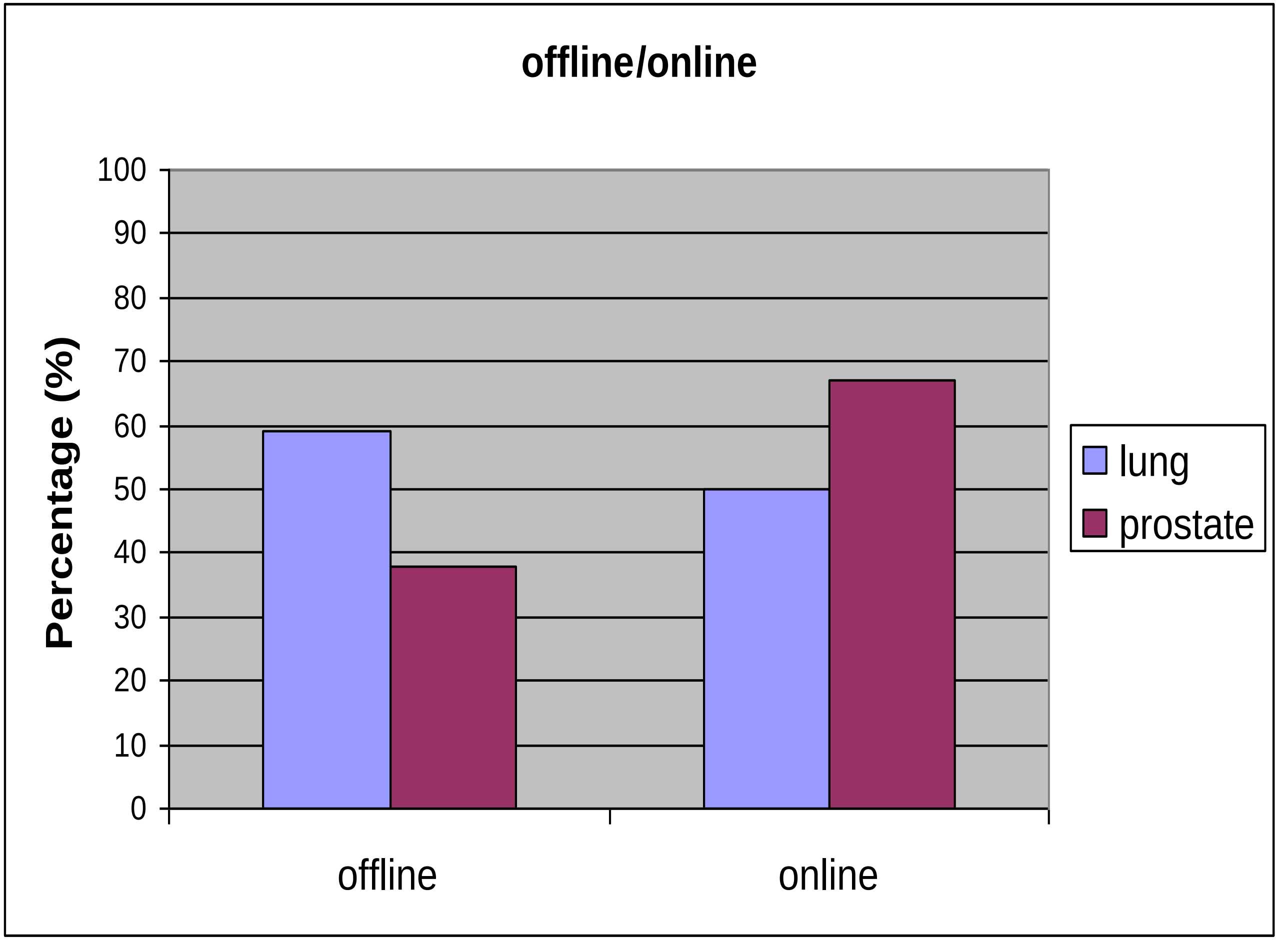
IGRT protocols are

A. Tumor site specific
B. Patient specific
C. Physician specific



IGRT

2D Portal Images	69%
kV Conebeam CT	67%
MV Conebeam CT	18%



IGRT

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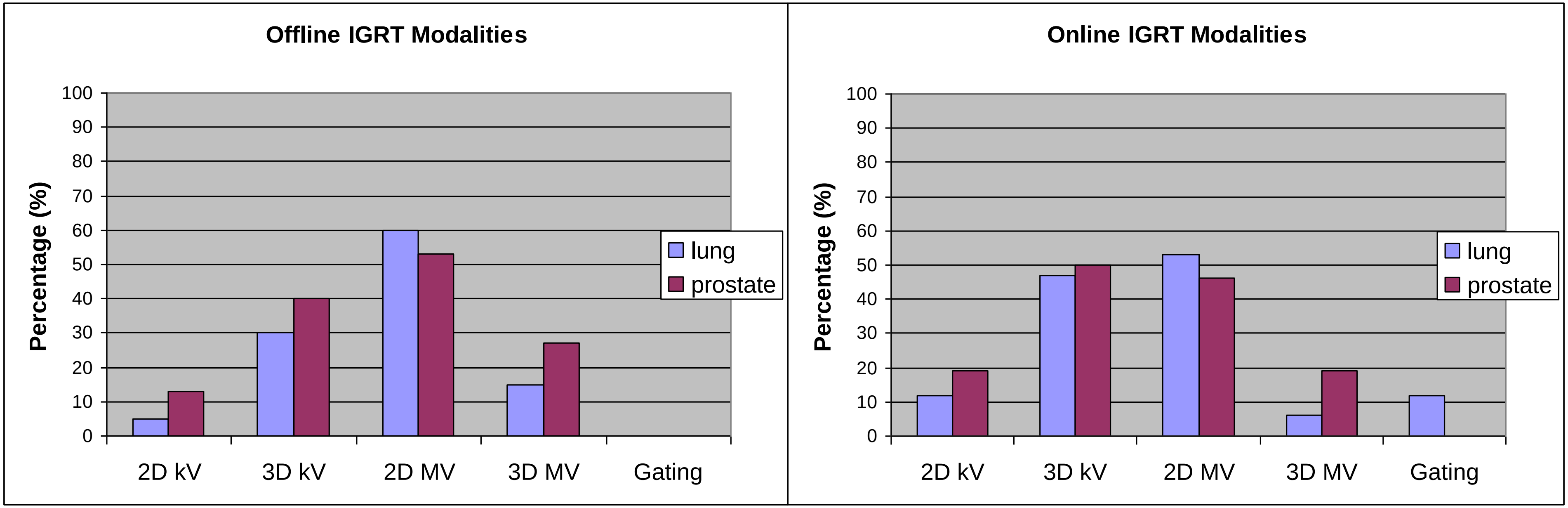
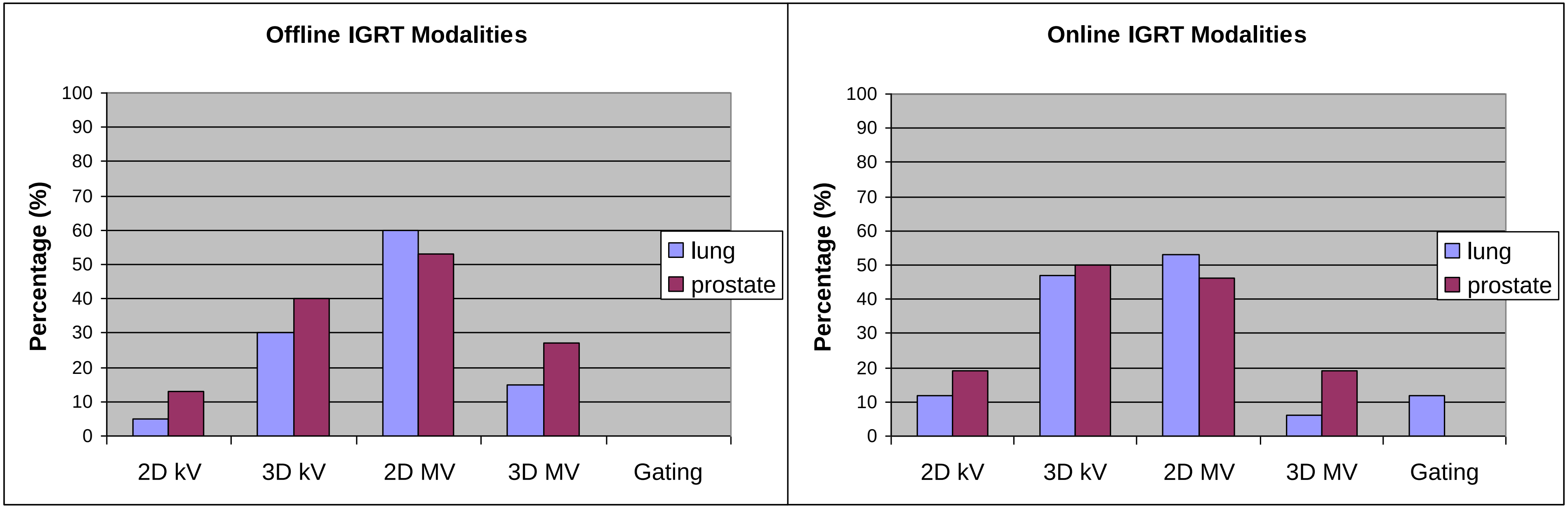
kV Conebeam CT	67%
MV Conebeam CT	18%



IGRT

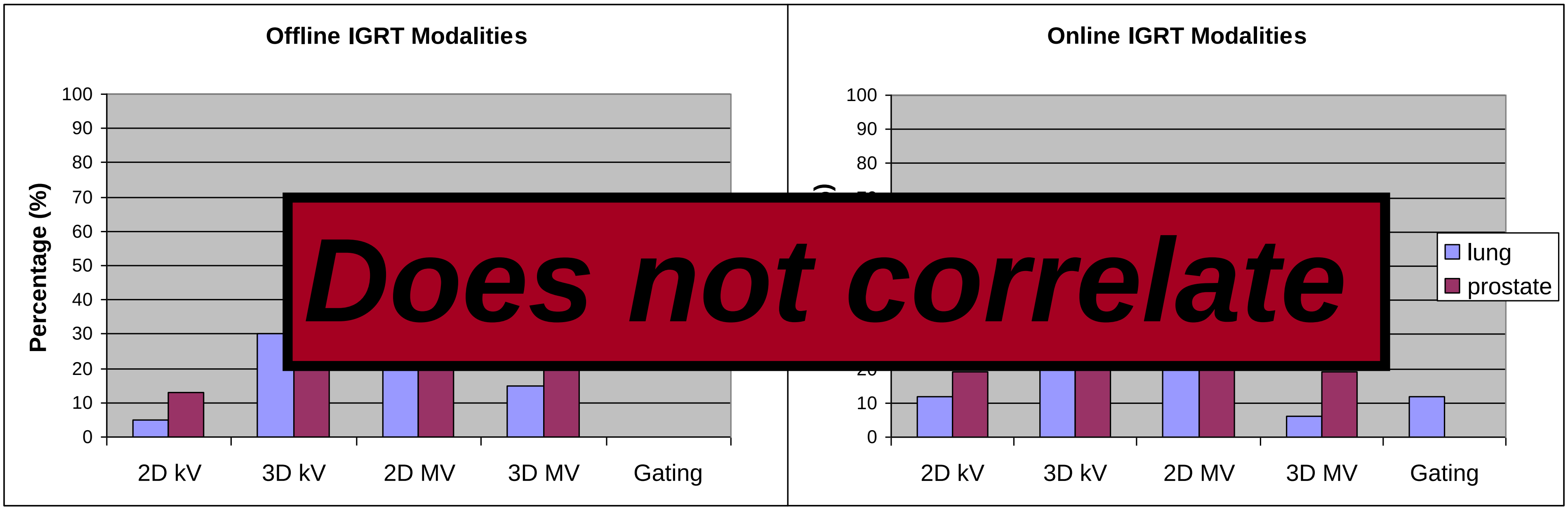
2D Portal Images	69%
kV Conebeam CT	67%
MV Conebeam CT	18%



→ Adaptive Radiation Therapy… 0%

IGRT

2D Portal Images	69%
kV Conebeam CT	67%
MV Conebeam CT	18%



→ Adaptive Radiation Therapy… 0%

Who is doing ART?

A. Yes

B. No

Summary

Large variation between departments in:

- Amount of resources per linac
- Their distribution in different disciplines:
  - Treatment planning
  - IGRT evaluation

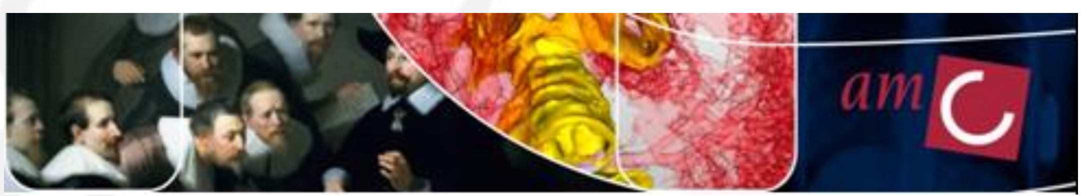
Some Variables

- RTT training and education
- Department size
- Resources per treatment machine
- IGRT Modalities
  - » Culture – History
  - » Money

Not decisive

Might consider different solutions?

Questions & Discussion



m.a.j.dejong@amc.uva.nl

NKI-AVL

The Netherlands Cancer Institute
Antoni van Leeuwenhoek Hospital

ESTRO School

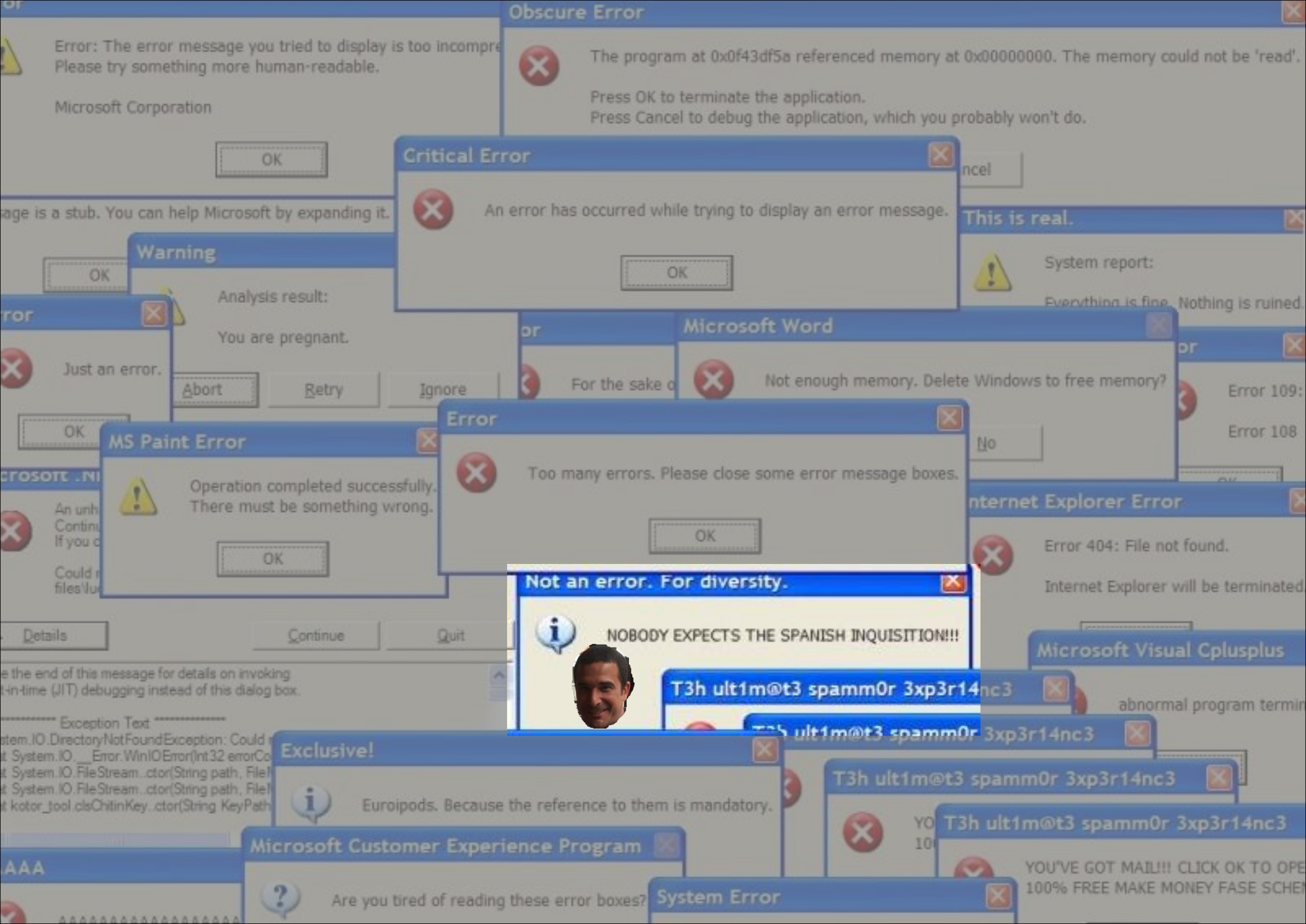
WWW.ESTRO.ORG/SCHOOL

Error management

Peter Remeijer
Department of Radiation Oncology
The Netherlands Cancer Institute

NETHERLANDS CANCER INSTITUTE
ANTONI VAN LEEUWENHOEK

ESTRO School


Error: The error message you tried to display is too incompre
Please try something more human-readable.
Microsoft Corporation
OK
Obscure Error
The program at 0x0f43df5a referenced memory at 0x00000000. The memory could not be 'read'.
Press OK to terminate the application.
Press Cancel to debug the application, which you probably won't do.
ncel
Critical Error
An error has occurred while trying to display an error message.
OK
age is a stub. You can help Microsoft by expanding it.
OK
Warning
Analysis result:
You are pregnant.
Abort
Retry
Ignore
This is real.
System report:
Everything is fine. Nothing is ruined.
ror
Just an error.
OK
For the sake o
Microsoft Word
Not enough memory. Delete Windows to free memory?
No
Error 109:
Error 108
MS Paint Error
Operation completed successfully.
There must be something wrong.
OK
Error
Too many errors. Please close some error message boxes.
OK
nternet Explorer Error
Error 404: File not found.
Internet Explorer will be terminated
Details
Continue
Quit
Not an error. For diversity.
NOBODY EXPECTS THE SPANISH INQUISITION!!!
Microsoft Visual Cplusplus
abnormal program termi
T3h ult1m@t3 spamm0r 3xp3r14nc3
T3h ult1m@t3 spamm0r 3xp3r14nc3
T3h ult1m@t3 spamm0r 3xp3r14nc3
T3h ult1m@t3 spamm0r 3xp3r14nc3
YOU'VE GOT MAIL!!! CLICK OK TO OPE
100% FREE MAKE MONEY FASE SCHE
Exclusive!
Euroipods. Because the reference to them is mandatory.
Microsoft Customer Experience Program
Are you tired of reading these error boxes?
System Error
AAA

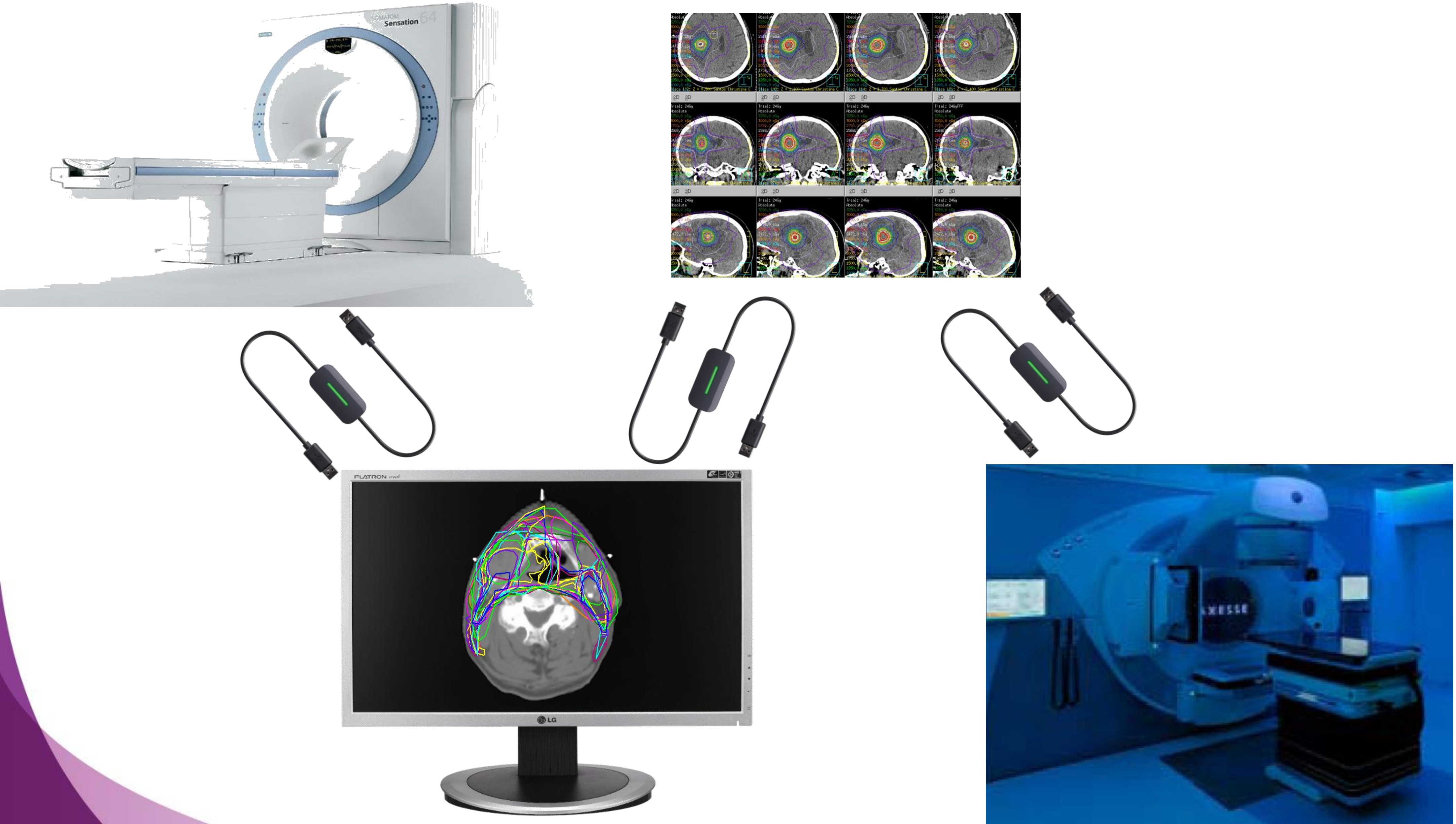
More errors?

- Transfer errors (planning → linac)
- Linac errors (both dosimetric and geometric)
- Dosimetric errors in plan
- Input errors
- Patient setup (e.g. CT reference to isoc shifts)
- Select the right patient / treatment in all systems

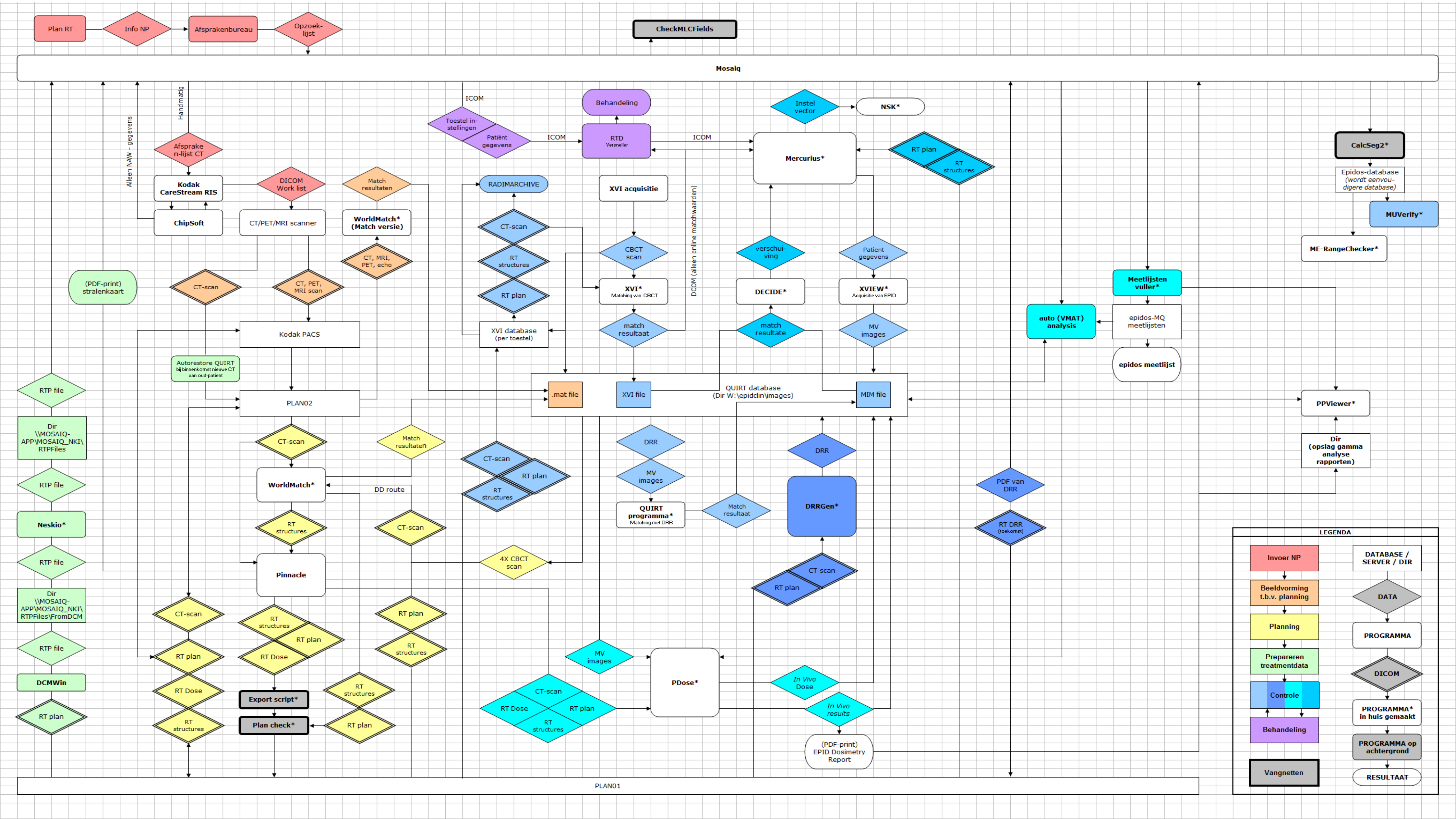
More errors?

- Transfer errors (planning → linac)
- Linac errors (both dosimetric and geometric)
- Dosimetric errors in plan
- Patient setup (e.g. CT reference to isoc shifts)
- Input errors
- Select the right patient / treatment in all systems

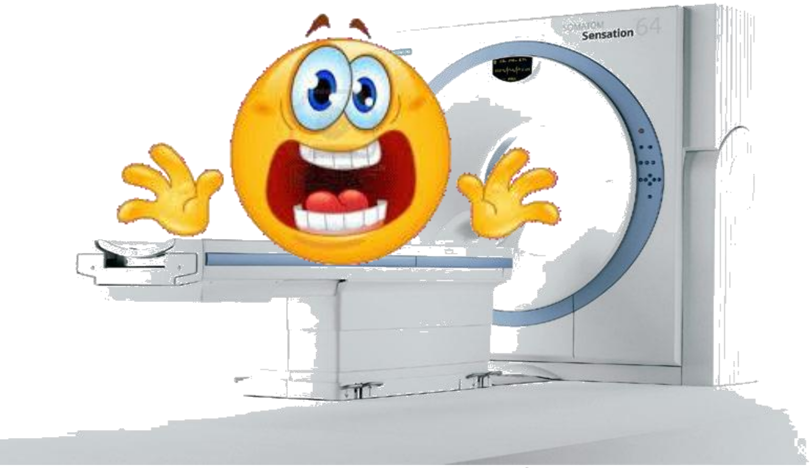
Errors and the radiotherapy "chain"

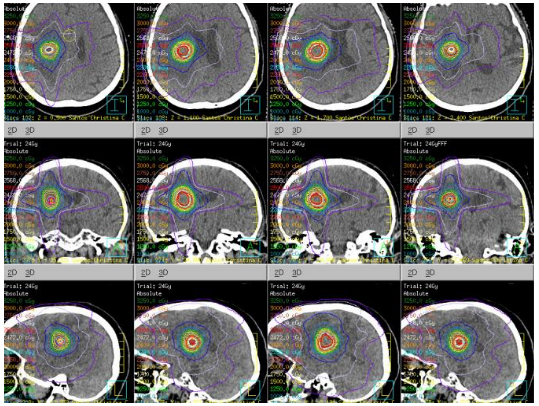


The radiotherapy “chain”



“Chain test” a.k.a regression test with phantom





Regression testing

- Run a phantom through the whole treatment chain and check for problems / errors
  - May be necessary to do this for different situations, i.e. HFS, HFP, etc
  - New methods, e.g. ART, library of plans, new planning techniques (VMAT)
- This will check
  - Connectivity
  - Systematic equipment and software errors
  - Overall dosimetry
  - Overall geometry

More errors?

- Transfer errors (planning → linac)
- Linac errors (both dosimetric and geometric)
- Dosimetric errors in plan
- Patient setup (e.g. CT reference to isoc shifts)
- Input errors
- Select the right patient / treatment in all systems

Independent MU checks

- Recalculates the dose, based on the plan parameters from the planning system (or v.v.)

- This will check (in theory)
  - Amount of monitor units
  - Problems with plan normalization
  - Computation errors of planning system

- Third party software
  - Lots of software around (small companies)
  - Check what it really checks
  - Test with intentional errors

MU range checking

- In house NKI development, but easy to build

- Plans following a certain protocol, e.g. prostate
  - Amount of MU for a VMAT plan will be similar for each patient
  - Depends a little on patient size, etc

  → MU range check

  - If patient does not fall within the range, something may have gone wrong
  - Check by physics
  - About 5-10%
  - Usually anatomical reasons
  - Some errors found (wrong dose specification point, #fractions)

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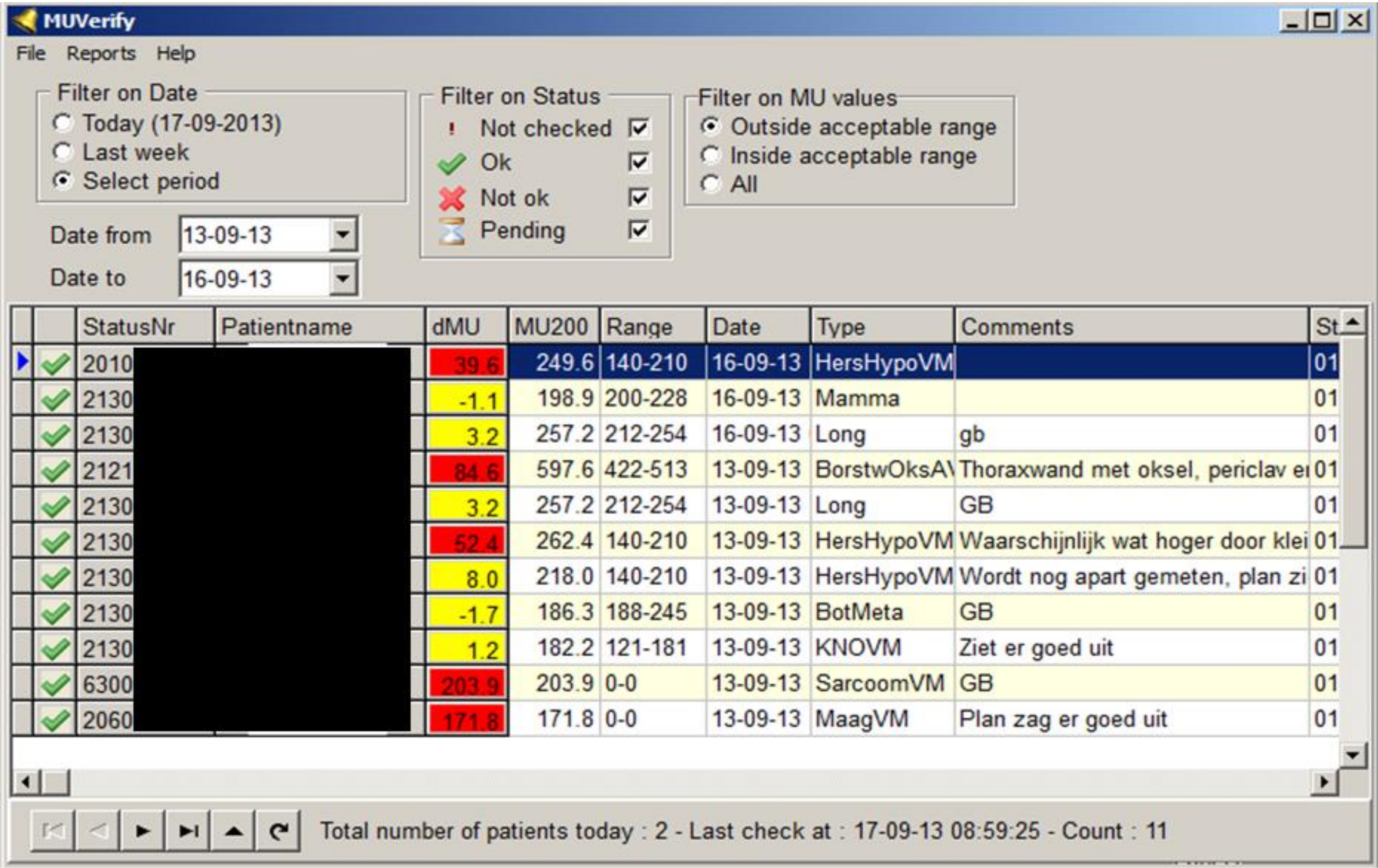
MU range checking

- Plan type depends on
  - Careplan name (brain, breast, prostate, etc)
  - RX-site name (plan name), e.g. Sacrum <231290>
  - Number of beams
  - Number of segments
  - Energy
  - Fraction dose

- Range for each type

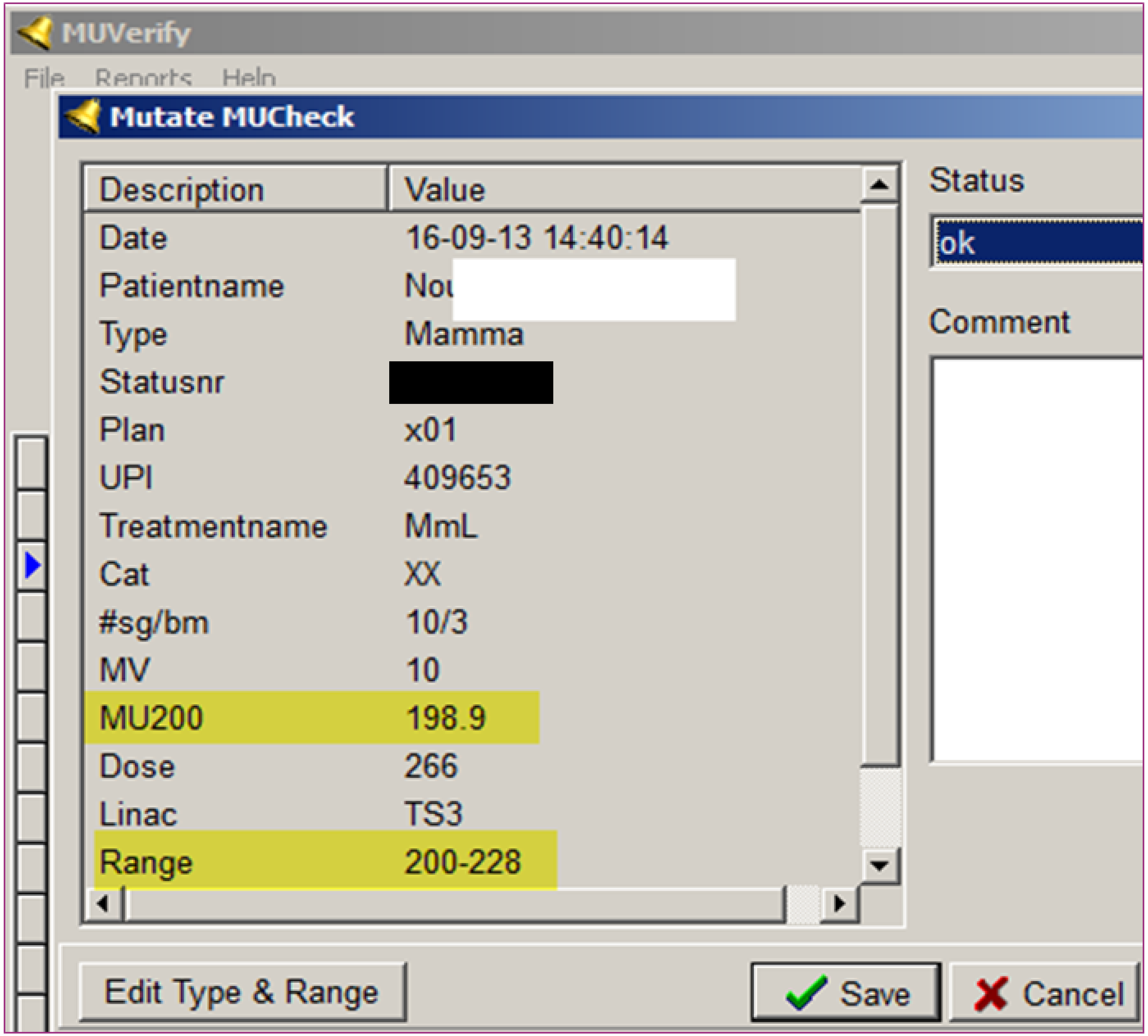
CP	Nbeam		Nsegm		Energy		Fr.Dosis		Type	Min	Max
Anus	2	8	2	70	6	10	180	300	Anus	188	261
Blaas	1	2	70	180	6	10	180	400	BlaasVM	158	218
Cervix	2	10	2	60	6	10	180	800	Gyn	221	284

Automated message on desktop of physicist



StatusNr	Patientname	dMU	MU200	Range	Date	Type	Comments	St
2010	[redacted]	39.6	249.6	140-210	16-09-13	HersHypoVM		01
2130		-1.1	198.9	200-228	16-09-13	Mamma		01
2130		3.2	257.2	212-254	16-09-13	Long	gb	01
2121		84.6	597.6	422-513	13-09-13	BorstwOksA\	Thoraxwand met oksel, periclav e	01
2130		3.2	257.2	212-254	13-09-13	Long	GB	01
2130		52.4	262.4	140-210	13-09-13	HersHypoVM	Waarschijnlijk wat hoger door klei	01
2130		8.0	218.0	140-210	13-09-13	HersHypoVM	Wordt nog apart gemeten, plan zi	01
2130		-1.7	186.3	188-245	13-09-13	BotMeta	GB	01
2130		1.2	182.2	121-181	13-09-13	KNOVM	Ziet er goed uit	01
6300		203.9	203.9	0-0	13-09-13	SarcoomVM	GB	01
2060		171.8	171.8	0-0	13-09-13	MaagVM	Plan zag er goed uit	01

Automated message on desktop of physicist



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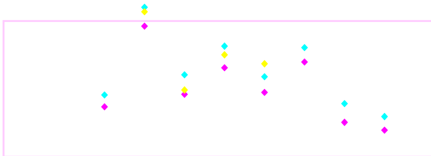
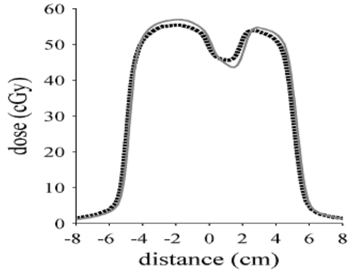
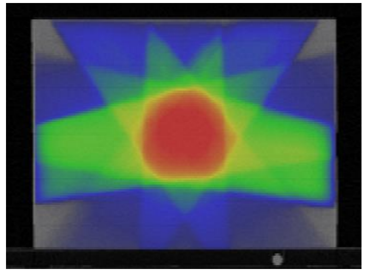
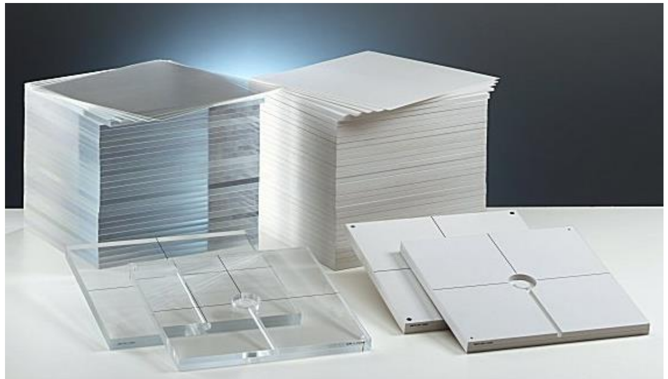
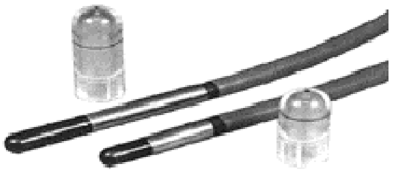
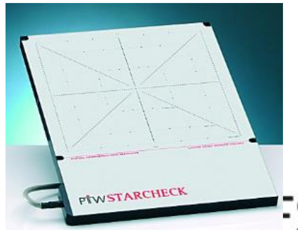
In-vivo portal dosimetry

in most centres today:

	0D	**1D**	**2D**
not 3D			
not *in vivo*			
not with an EPID			

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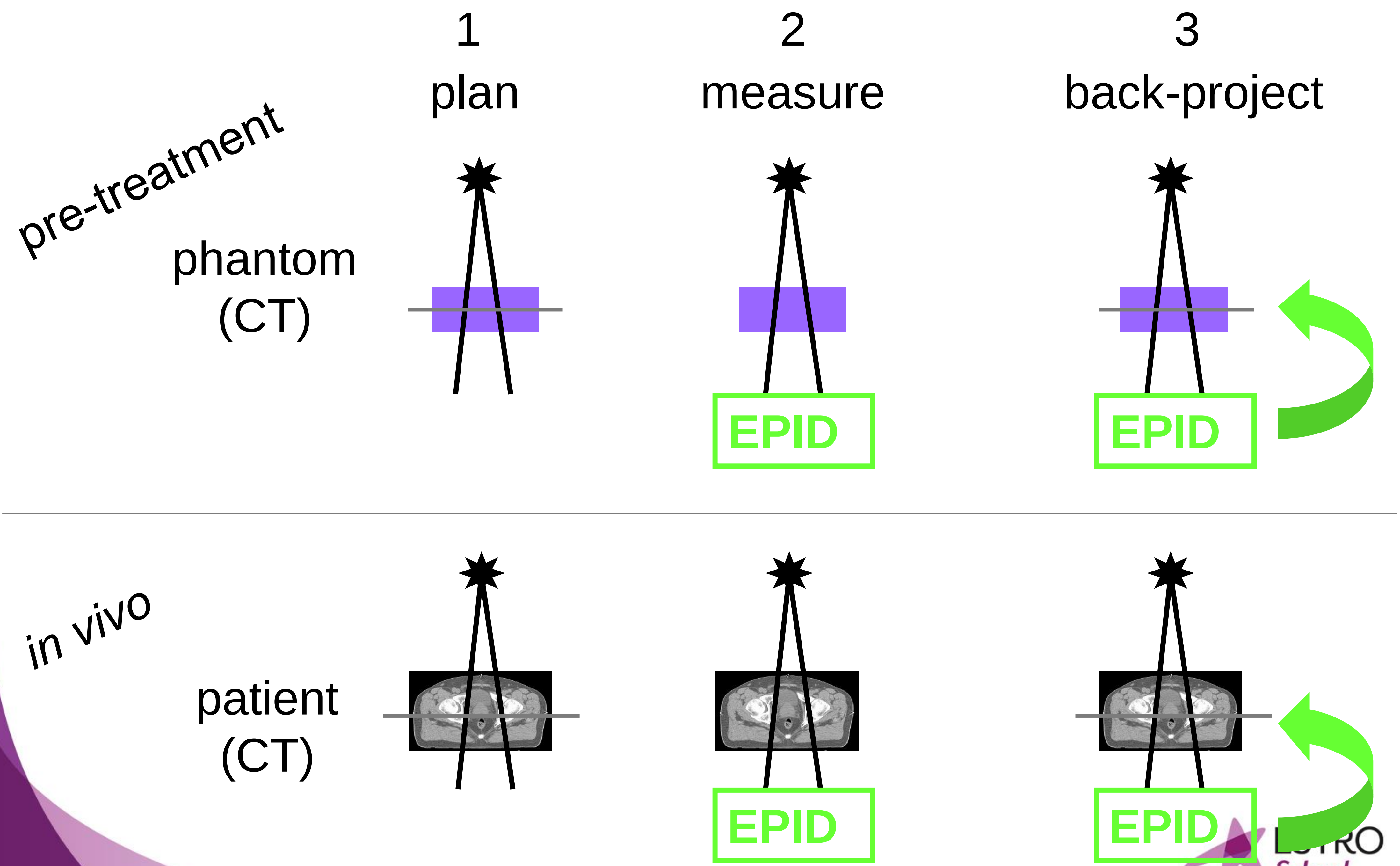
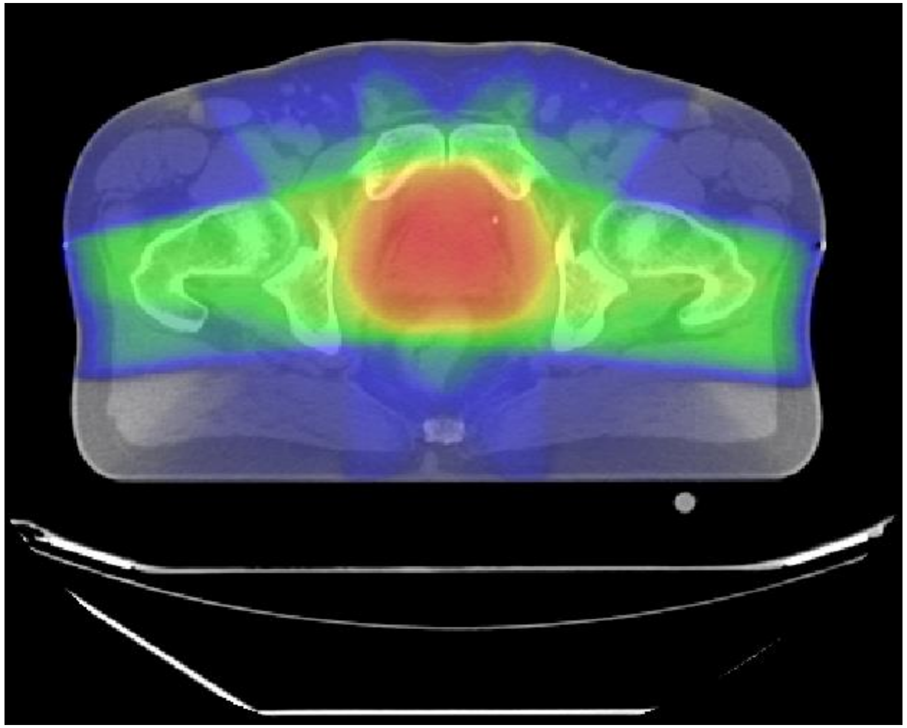
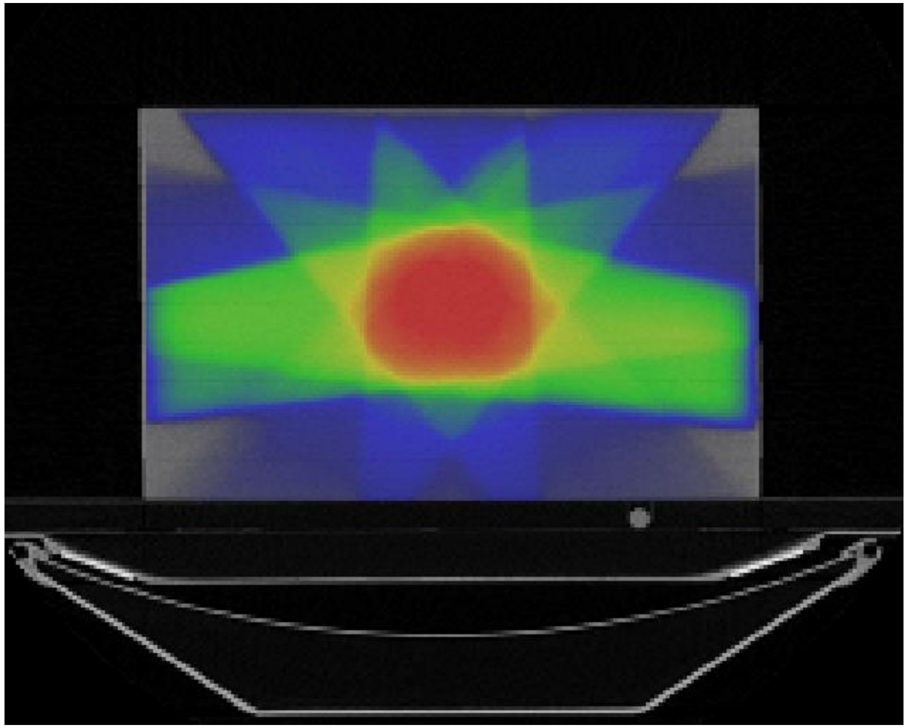
The NKI back-projection approach



Pre-treatment : in a phantom



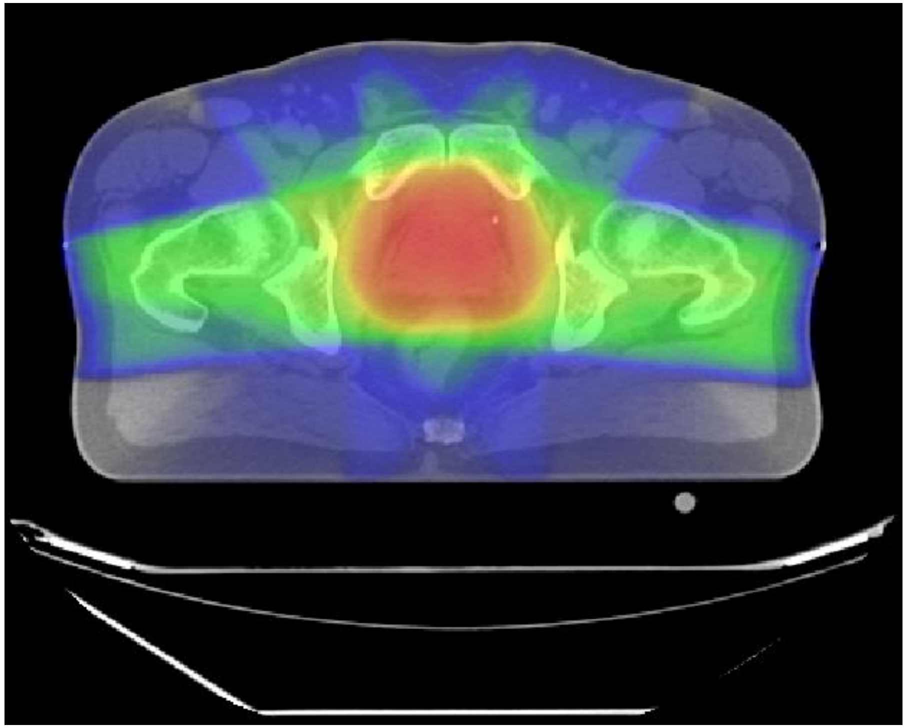


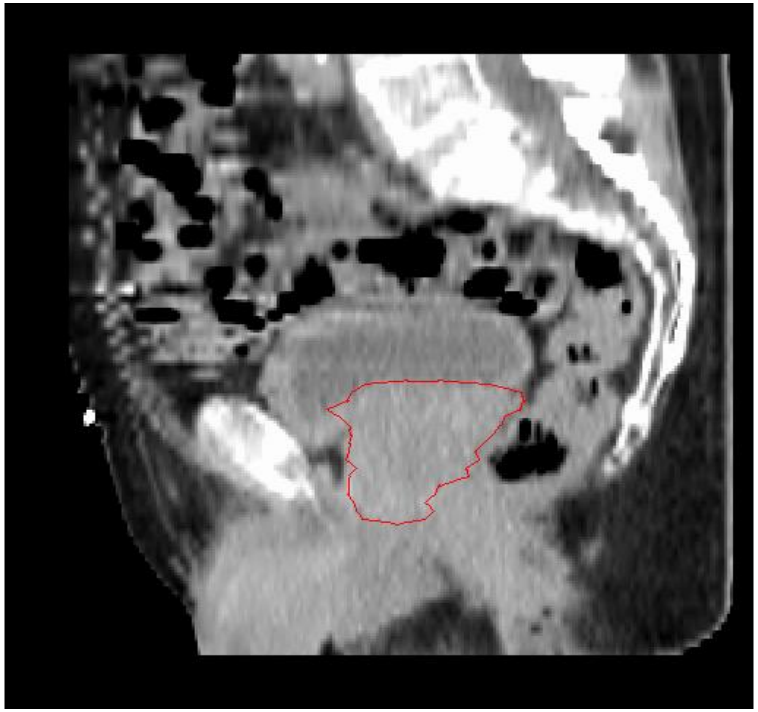
checks: plan deliverability

dose calculation

extra time : about 1 hour

In vivo : in the patient

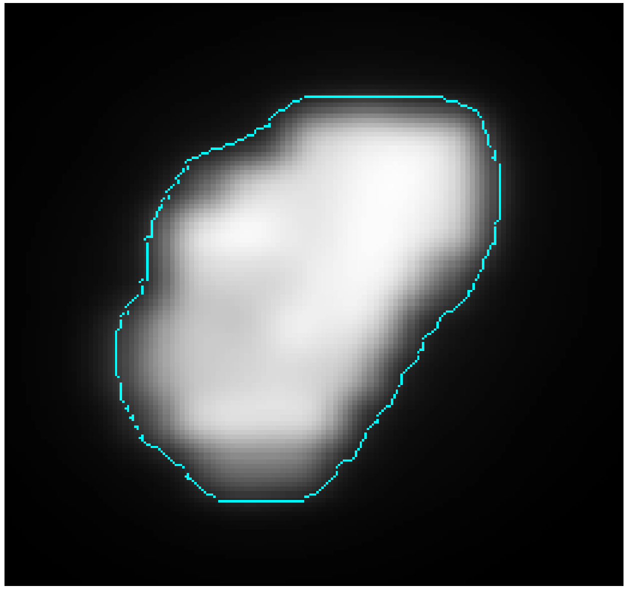




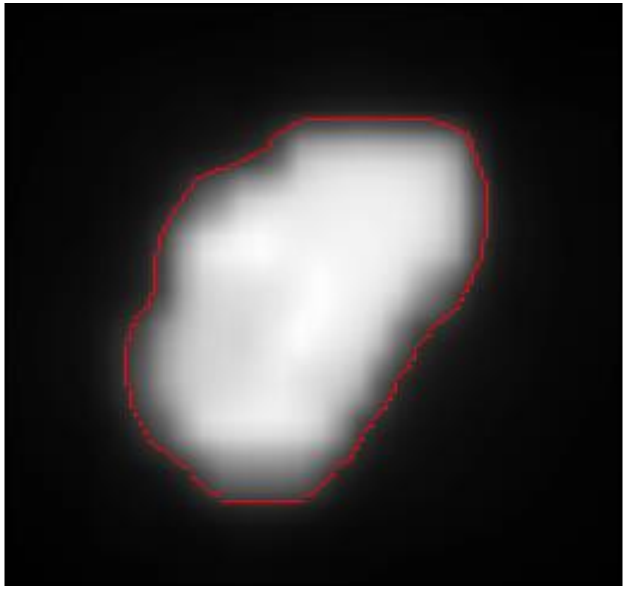
checks:	plan deliverability
	dose calculation
	anatomy changes
	random delivery errors
extra time : + 30s/day	~ 25 min in case of an error

Field-by field
reference vs calculated or measured dose

how do we compare them in 2D?

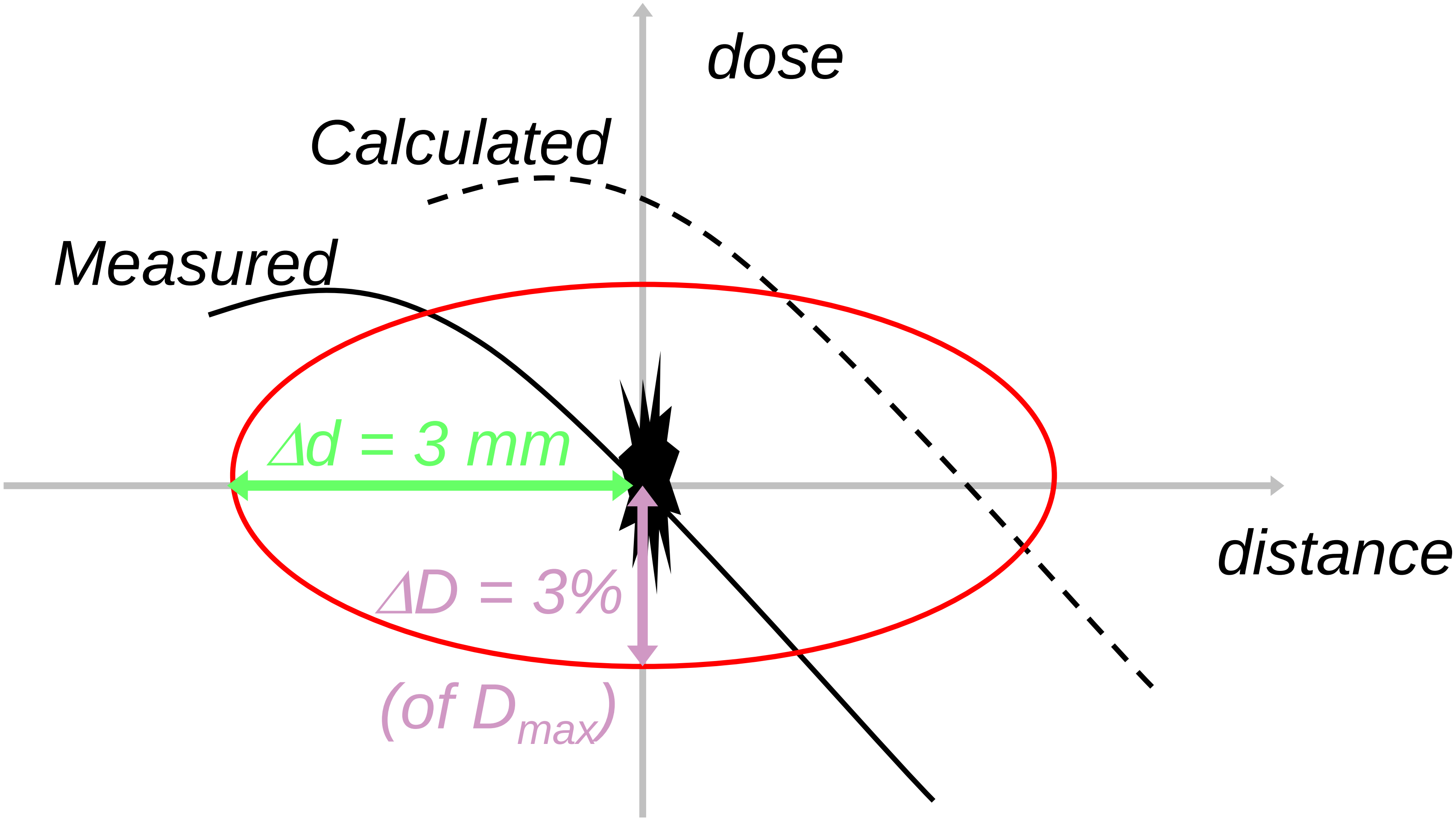


PLAN



EPID

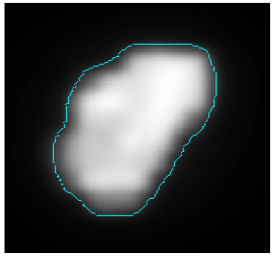
γ-evaluation: calculation vs measurement



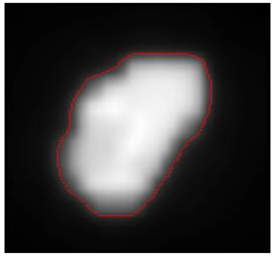
combines dose and distance criterion

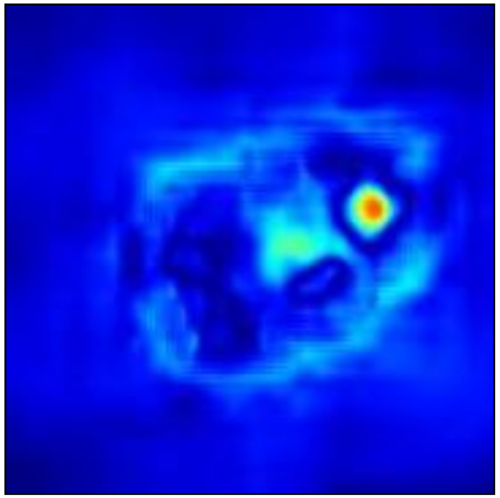
To compare the dose in 2D

plan



EPID

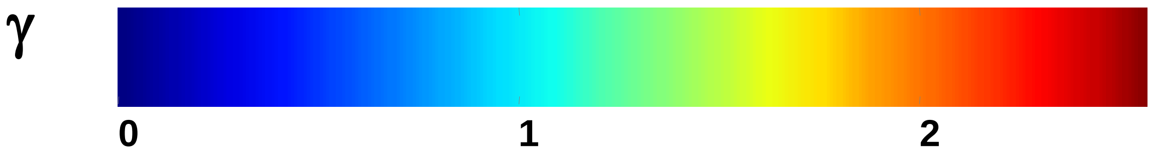


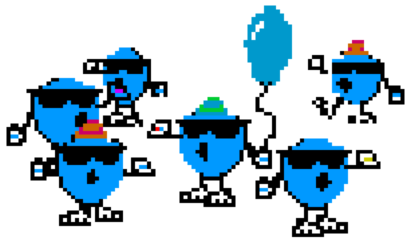


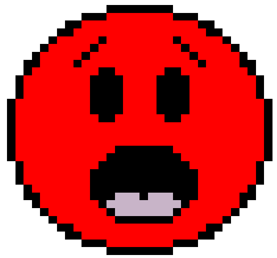
γ image

3% or 3mm

6% or 6mm







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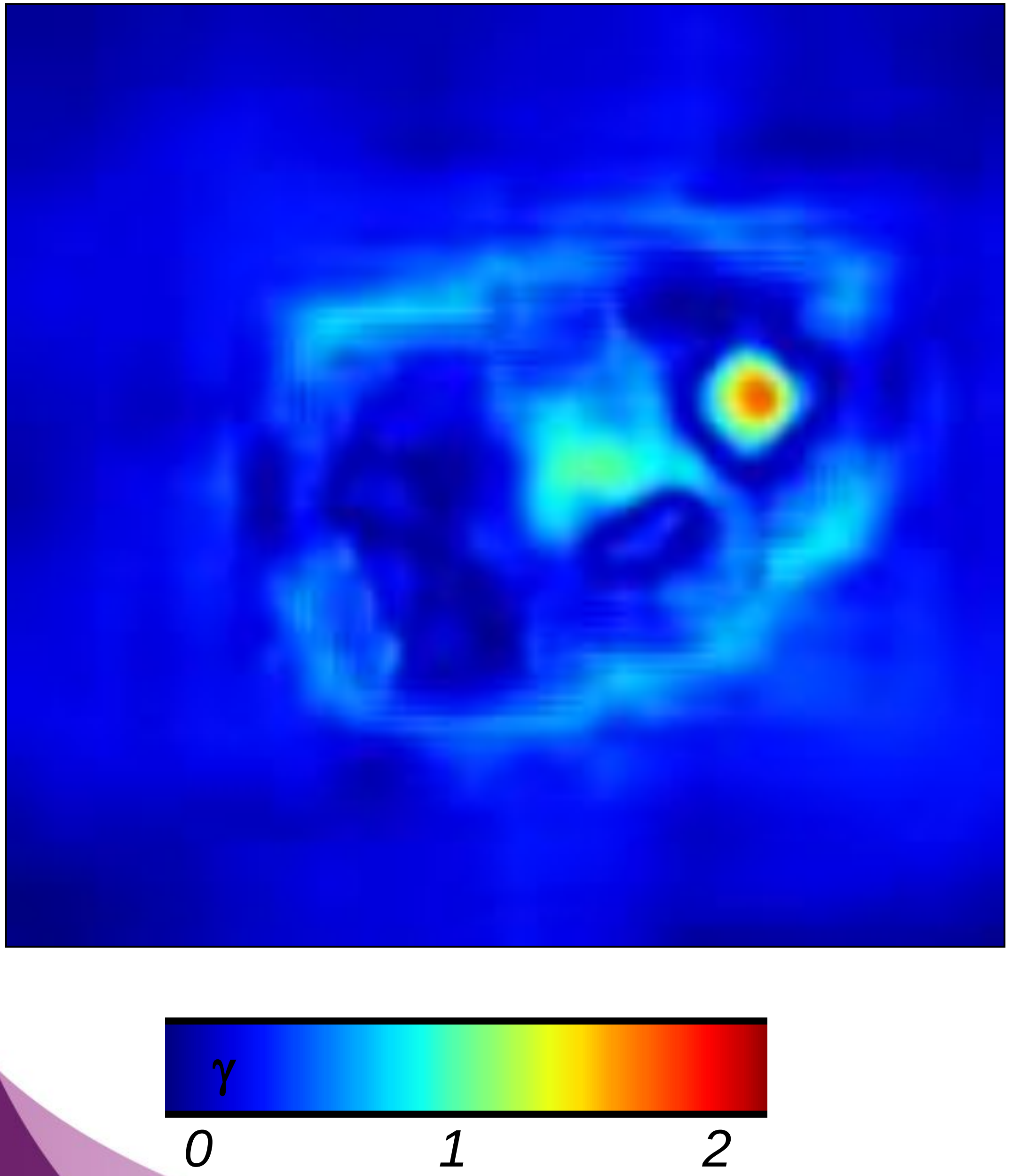
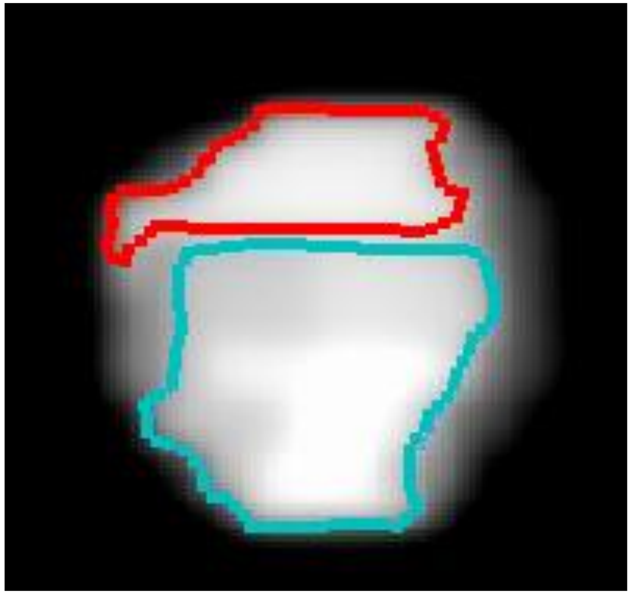
What can you detect?

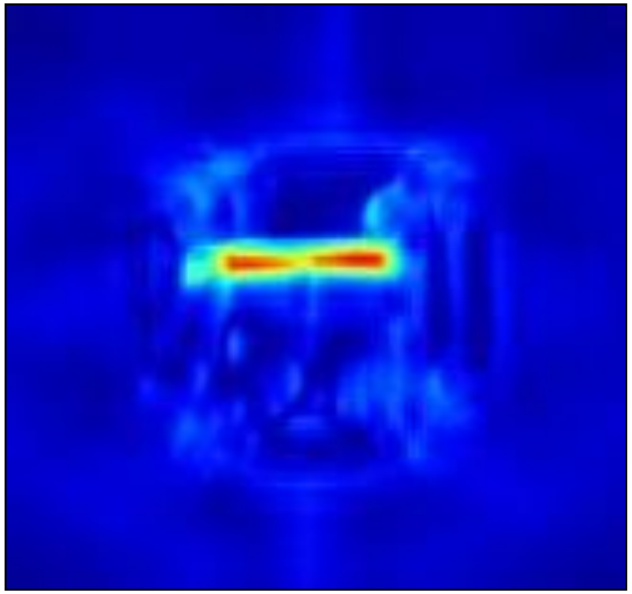
Gas pockets



abutting leaves



isodose lines
segments 3 & 6



γ-evaluation
3% / 3mm
EPID vs plan

More errors?

- Transfer errors (planning → linac)
- Linac errors (both dosimetric and geometric)
- Dosimetric errors in plan
- Patient setup (e.g. CT reference to isoc shifts)
- Input errors
- Select the right patient / treatment in all systems

Patient setup

- CT reference to isocenter shift
  - Potentially really large errors (e.g. 10cm!)
  - They DO occur

- Possible countermeasures
  - Online imaging for ALL patients
  - Table shift surveillance software

ZERO

LCS: B2 PATID:

Please align patient

to CT Ref

Automatically retrieved from planning system

Includes shifts from offline protocols as well
Height:
Longitudinal
-10.0
2.4
-3.1
TABLE:
Height:
Lateral:
Longitudinal:
0.0
0.0
0.0

ZERO

Interlock released when numbers are the same

Height:	Lateral:	Longitudinal
-10.0	2.4	-3.1

TABLE:

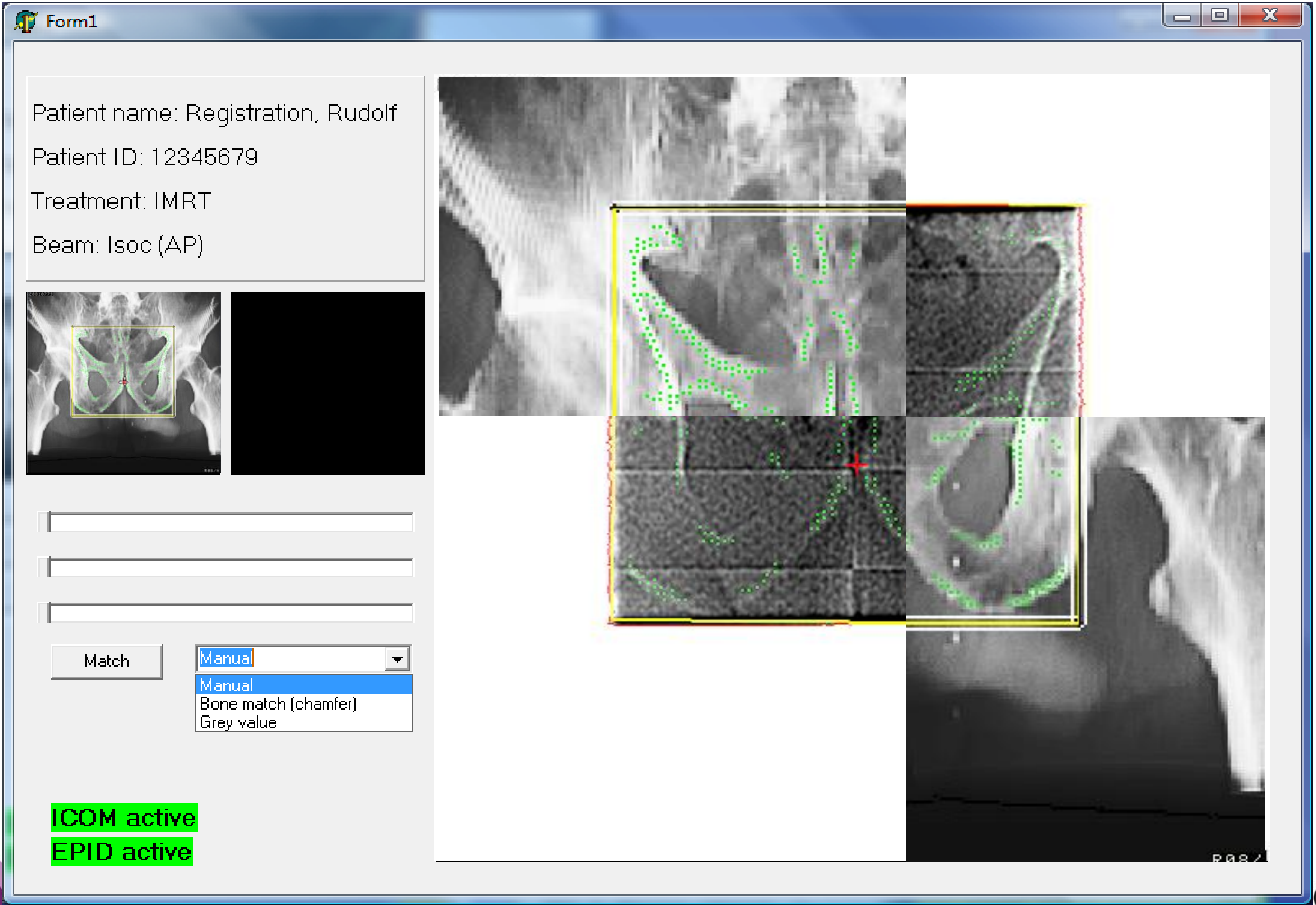
Height:	Lateral:	Longitudinal
-10.0	2.4	-3.1

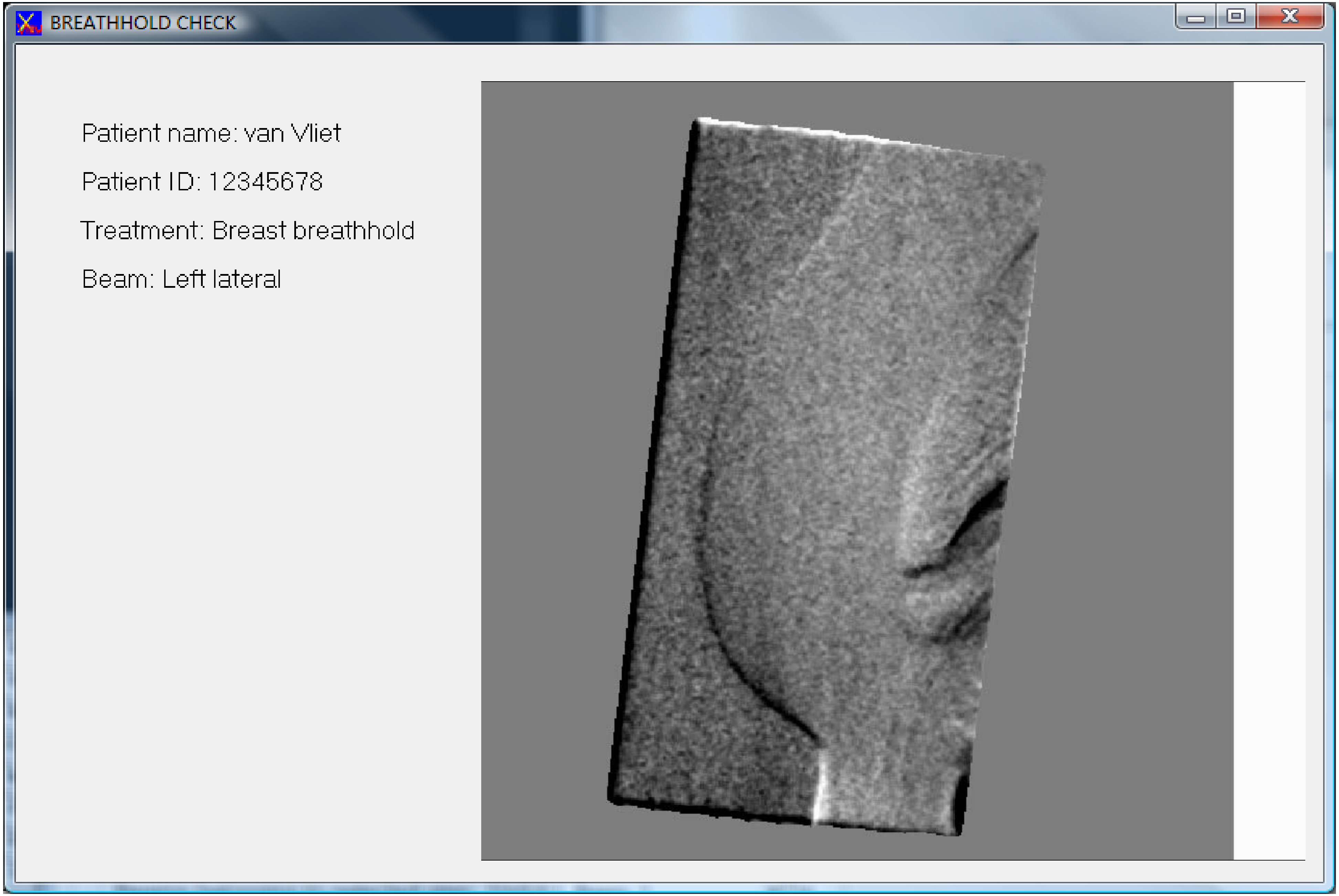
Input errors / patient / treatment selection

- Automation. Make the number of user interaction as small as possible
- Intuitive user interfaces
- Double checks
- New technology, like RFIDs?

Automation: EPID acquisition

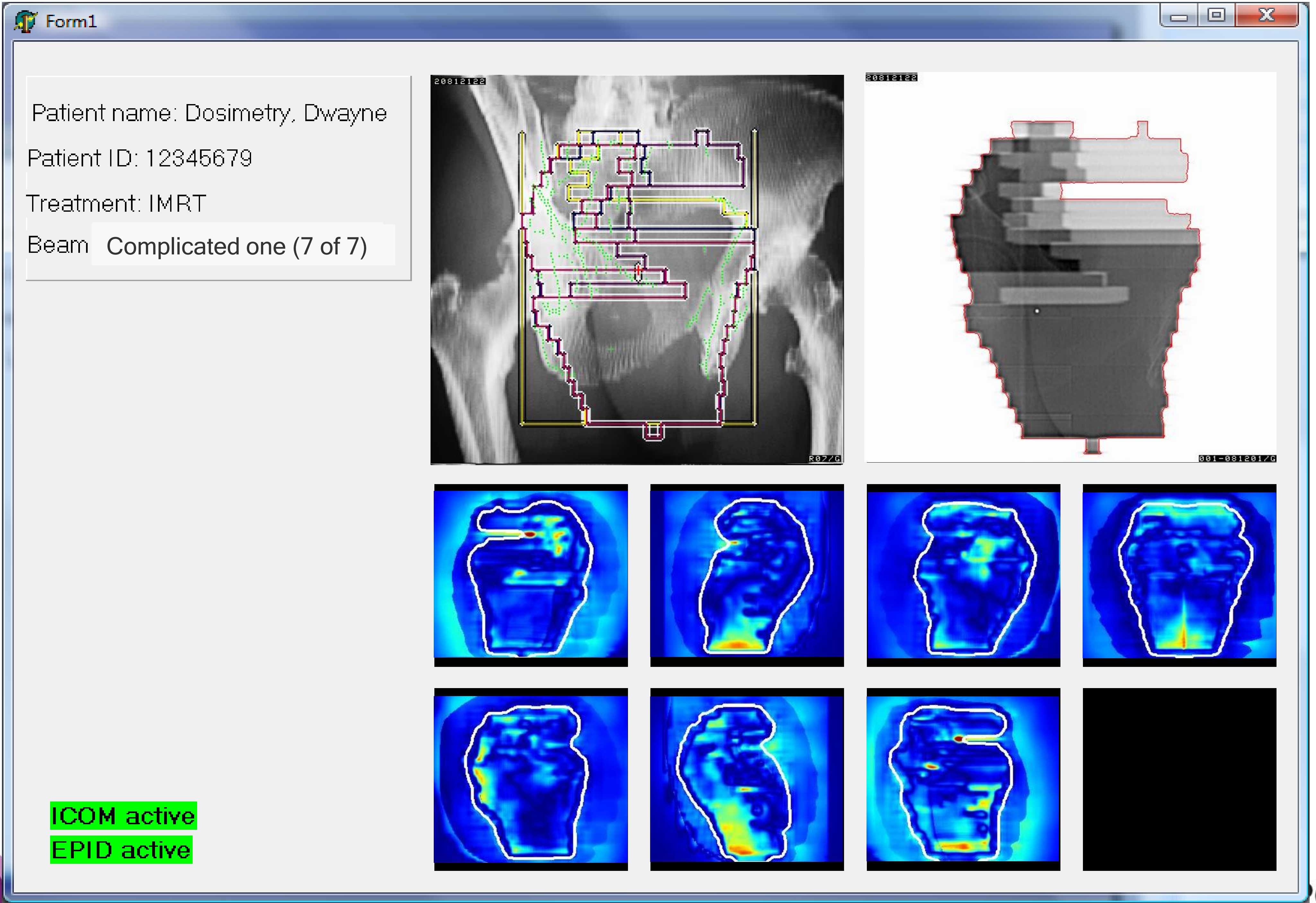
- Radiographer…
  - Deploys the imager
- Application…
  - Selects patient and beam
  - Saves data in database without any user intervention
- Different screens, depending on beam property, e.g.
  - Dosimetry screen
  - Online registration screen
  - Breathhold screen


Form1
Patient name: Registration, Rudolf
Patient ID: 12345679
Treatment: IMRT
Beam: Isoc (AP)
Match
Manual
Manual
Bone match (chamfer)
Grey value
ICOM active
EPID active


BREATHHOLD CHECK
Patient name: van Vliet
Patient ID: 12345678
Treatment: Breast breathhold
Beam: Left lateral

Automation: Zero button EPID dosimetry

- Radiographer…
  - Deploys the imager and treats the patient
- Application…
  - ‘Triggers’ on new images from EPID acquisition application
  - Computes dose
  - Sends a report to physics
  - Notifies physics when something is wrong


Form1
Patient name: Dosimetry, Dwayne
Patient ID: 12345679
Treatment: IMRT
Beam
Complicated one (7 of 7)
ICOM active
EPID active

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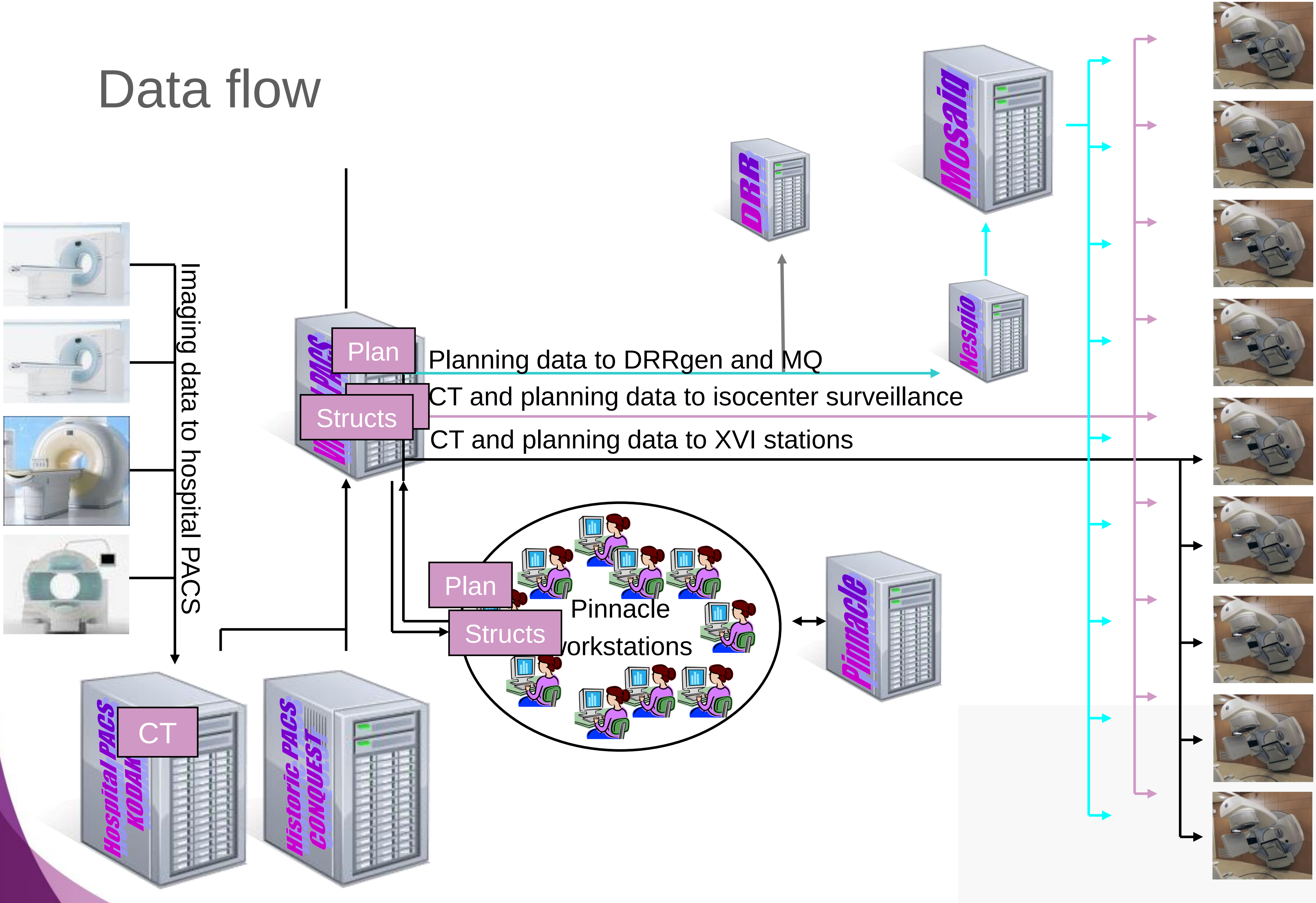
Automated dataflow example

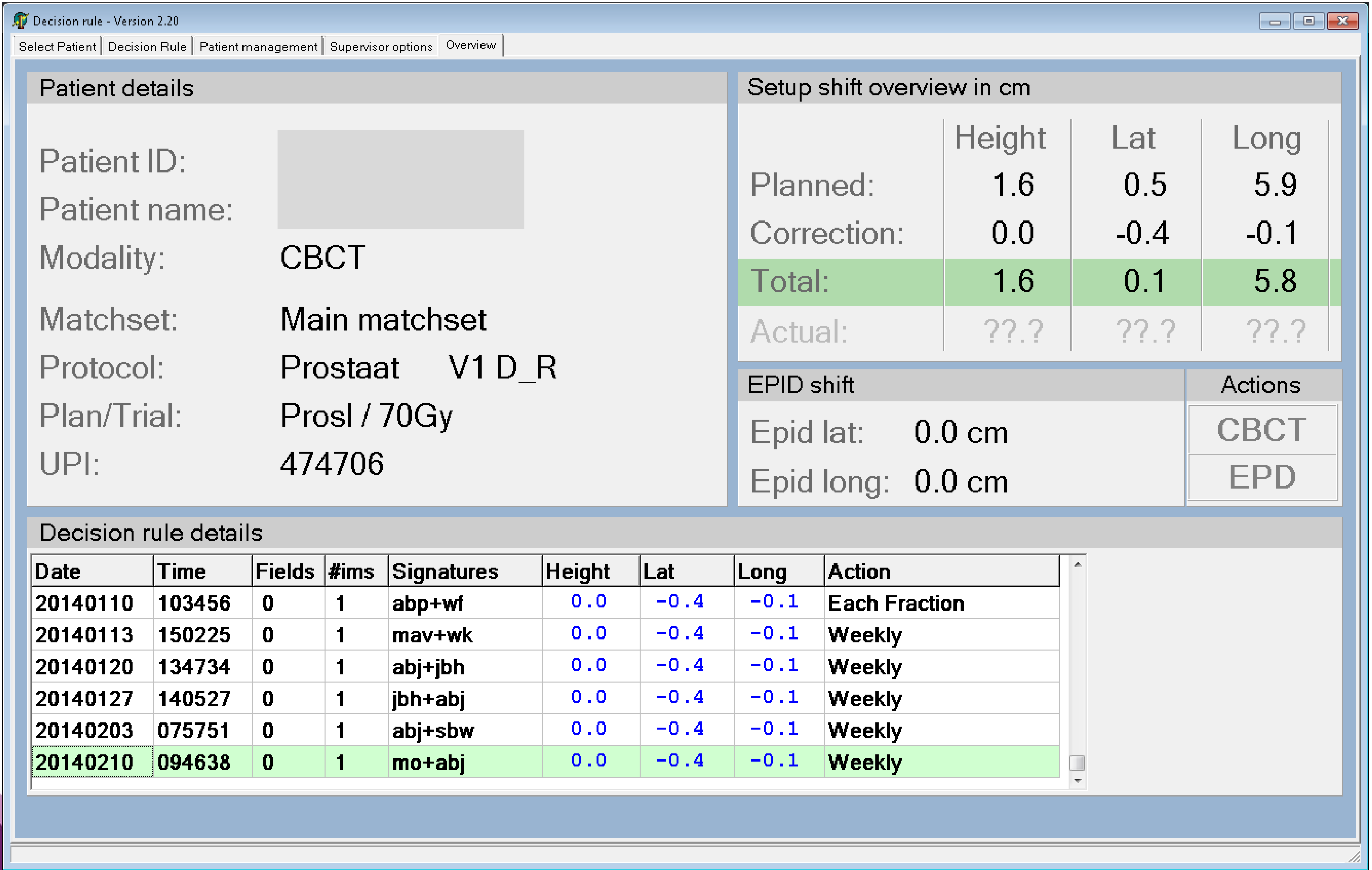
- Dosimetrist sends plan for linac B5 to central server
- Server finds corresponding CT scan and structure set
- All data is then automatically sent to XVI station on B5
- Plan is sent to Mosaiq
- Plan and structures are sent to hospital PACS
- DRRs are automatically generated
- Patient is automatically entered in imaging database

Data flow



Imaging data to hospital PACS
Plan
Structs
Planning data to DRRgen and MQ
CT and planning data to isocenter surveillance
CT and planning data to XVI stations
DRR
Mosaiq
Plan
Structs
Pinnacle
orkstations
Pinnacle
CT
Hospital PACS
KODAK
Historic PACS
CONQUEST

User interface



Take home messages

- IGRT is good but not enough
- Take countermeasures to catch gross errors
- Try to find the simplest workflow (user interface, protocols, forms)
- **Be especially aware when introducing new systems, protocols, or technologies**

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Incident management

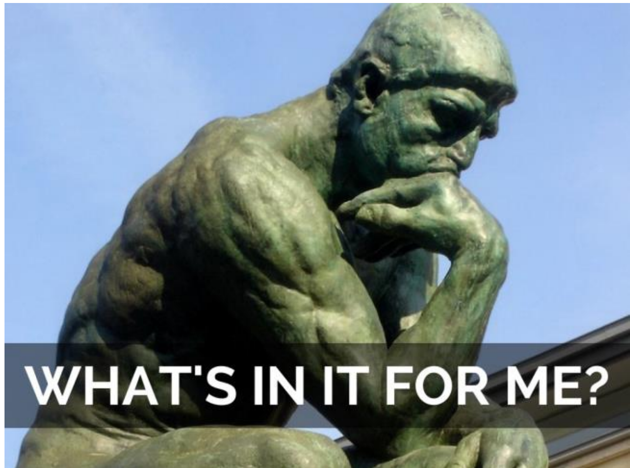
Mirjana Josipovic

Dept. of Oncology, Rigshospitalet
& Niels Bohr Institute, University of Copenhagen
Denmark

Advanced skills in modern radiotherapy
June 2017

Intended learning outcomes

- Define an incident in radiotherapy context
- Discuss the importance of an incident reporting system
- Analyse the potential causes for an incident to have happened



Definitions

Incident

- Any unintended event, including operating errors, equipment failures, initiating events, accident precursors, near misses or other mishaps, or unauthorized act, malicious or non-malicious, the consequences or potential consequences of which are not negligible from the point of view of protection or safety.

(IAEA Safety Glossary, 2007)

Radiation incident

- The delivery of radiation during a course of RT is other than intended by prescription, and could have or did result in unnecessary harm to the patient.

(Towards safer radiotherapy, BJR 2008)

Incident

- An *unplanned, undesired* event that hinders completion of a task and may cause injury, illness, or property damage or some combination of all three in varying degrees from minor to catastrophic. Unplanned and undesired do not mean *unable to prevent*.

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Unintended
does not mean
unable to prevent!

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Incidents

Actual incident = accident:

- The unforeseen event, that has affected the treatment of the patient

Potential incident:

- "Near miss"
- The unforeseen event, that was discovered and halted before it affected the treatment of the patient

From IAEA database of radiation incidents

Independent calculation checks 1998-2003 on 27830 charts/plans

An unintended "potential incident" was found:
- in ~3 % of all plans, during primary check
- in ~½ % of all plans, during secondary check

Actual incidents = accidents:
- in ~¼ % of cases

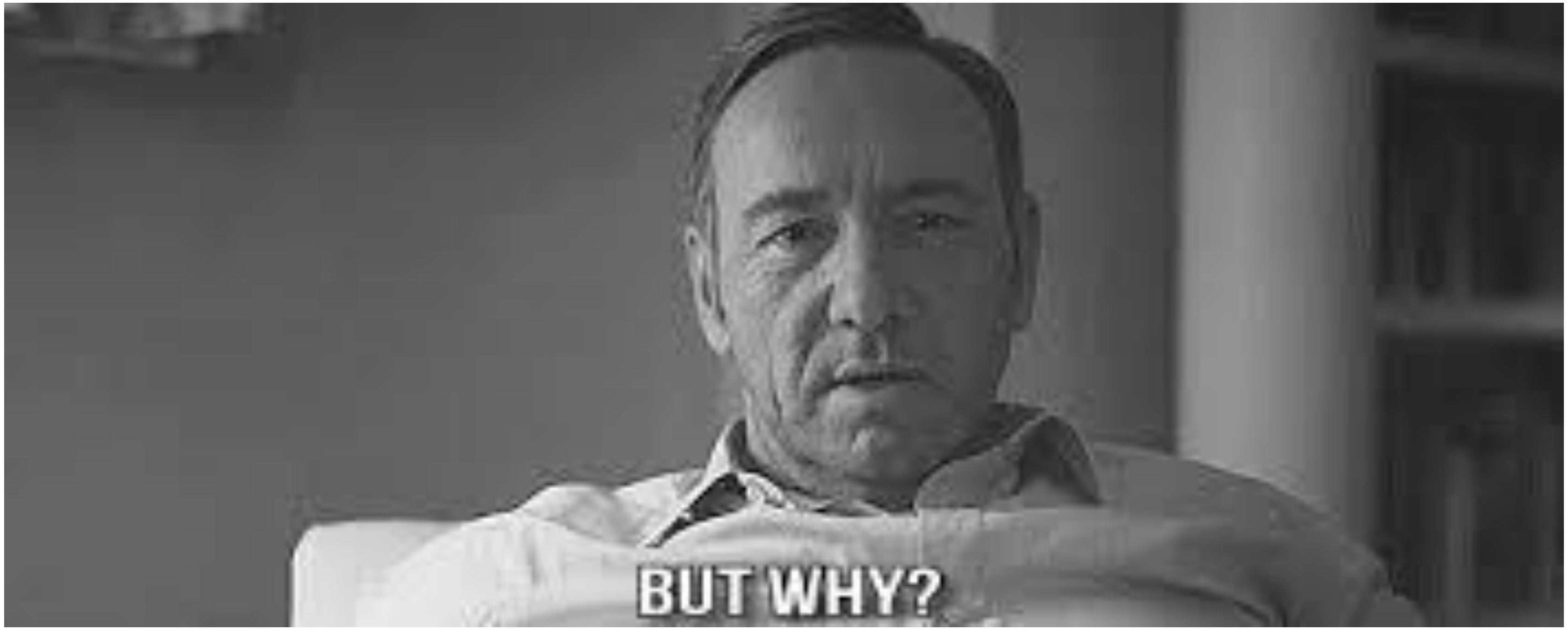
For each actual incident, ~14 potential incidents were found through checking.

An incident frequency of 3% could be seen in a "typical clinic".

Incidents are more numerous than accidents:

- there are more opportunities to learn and improve the safety, than by only looking at major accidents.

But we do have a check procedure…



Incident frequency in modern radiotherapy

3011 reported incidents from 2012-2015 in single institution

- 552 potentially severe or critical

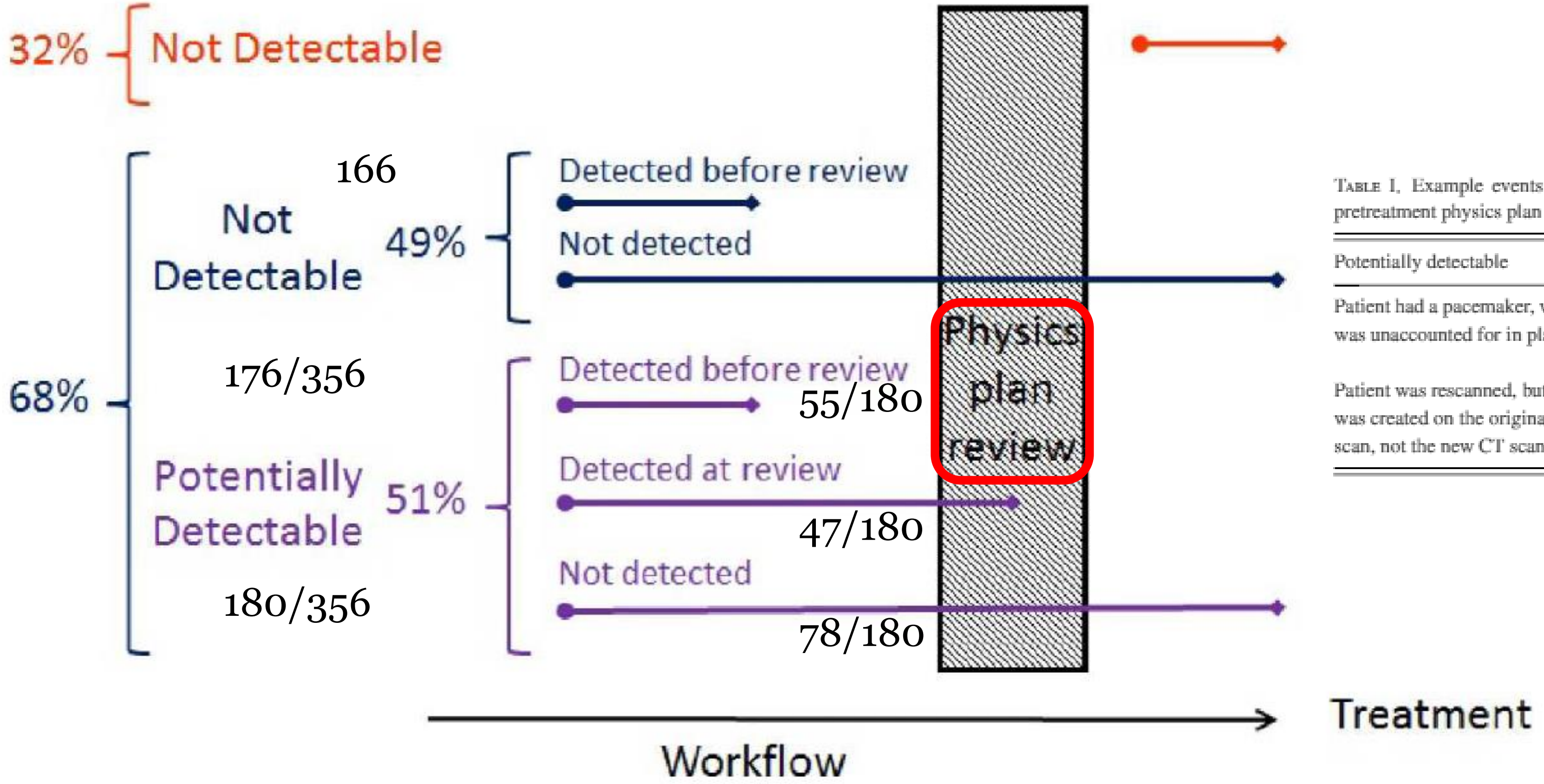


Table I. Example events potentially detectable and not detectable by the pretreatment physics plan review.

Potentially detectable	Not detectable
Patient had a pacemaker, which was unaccounted for in planning	Patient starts oral chemotherapy not on the day of radiation therapy as prescribed, but earlier
Patient was rescanned, but plan was created on the original CT scan, not the new CT scan	Physician changes the prescription midway through the treatment, but the change is not communicated

Gopan et al Med Phys 2016

Incident frequency in modern radiotherapy

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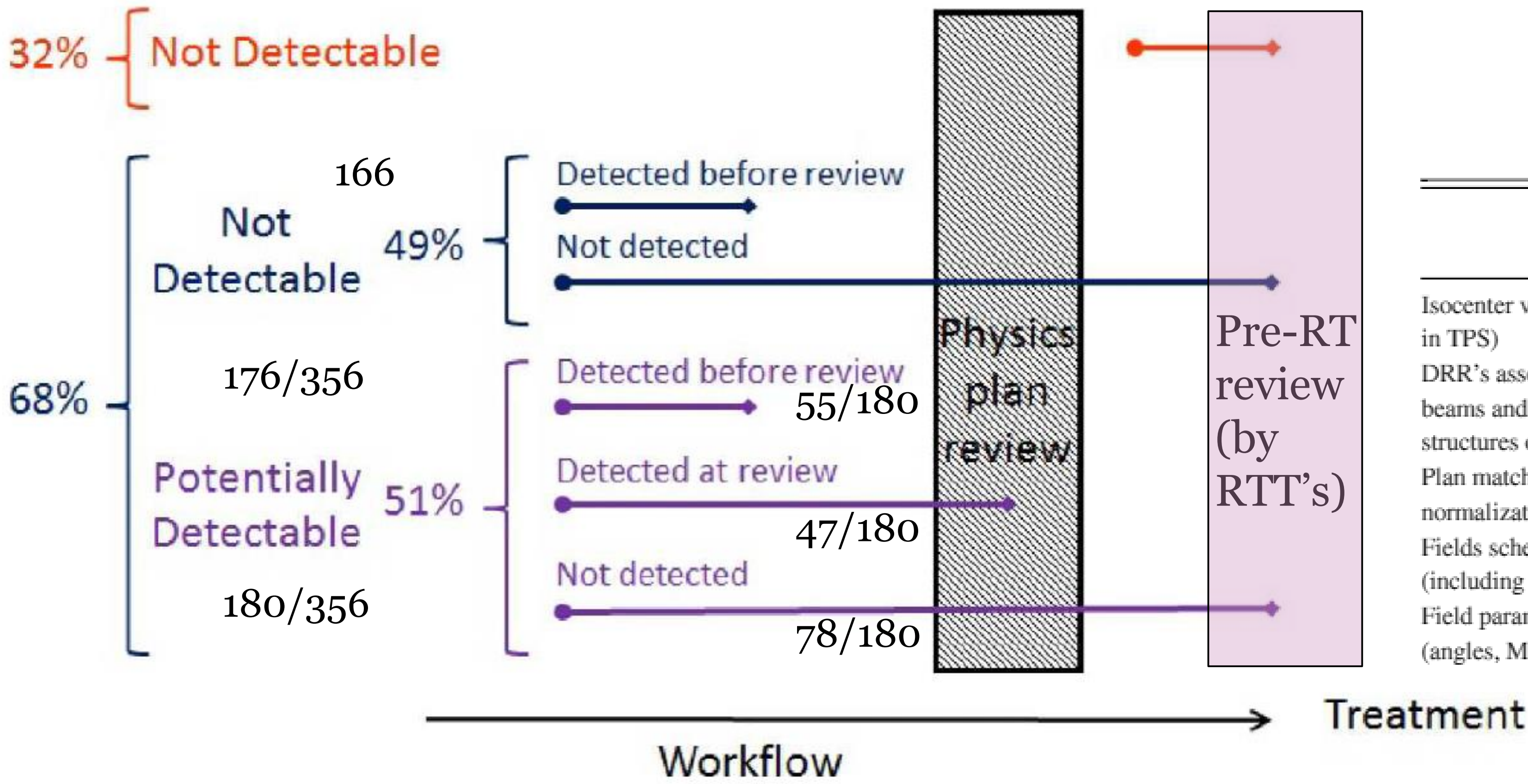

	Departmental ($n = 180$)
Isocenter verified (i.e., localization in TPS)	39
DRR's associated with correct beams and are appropriate (e.g., structures on)	17
Plan matched Rx (dose, normalization, etc.)	12
Fields scheduled appropriately (including imaging)	8
Field parameters verified vs plan (angles, MU, wedges, etc.)	7

- Majority of potentially severe incidents occure before physics review (68%) – ~1/3 of them is detected by review

Gopan et al Med Phys 2016

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Incident frequency in modern radiotherapy

3011 reported incidents from 2012-2015 in single institution

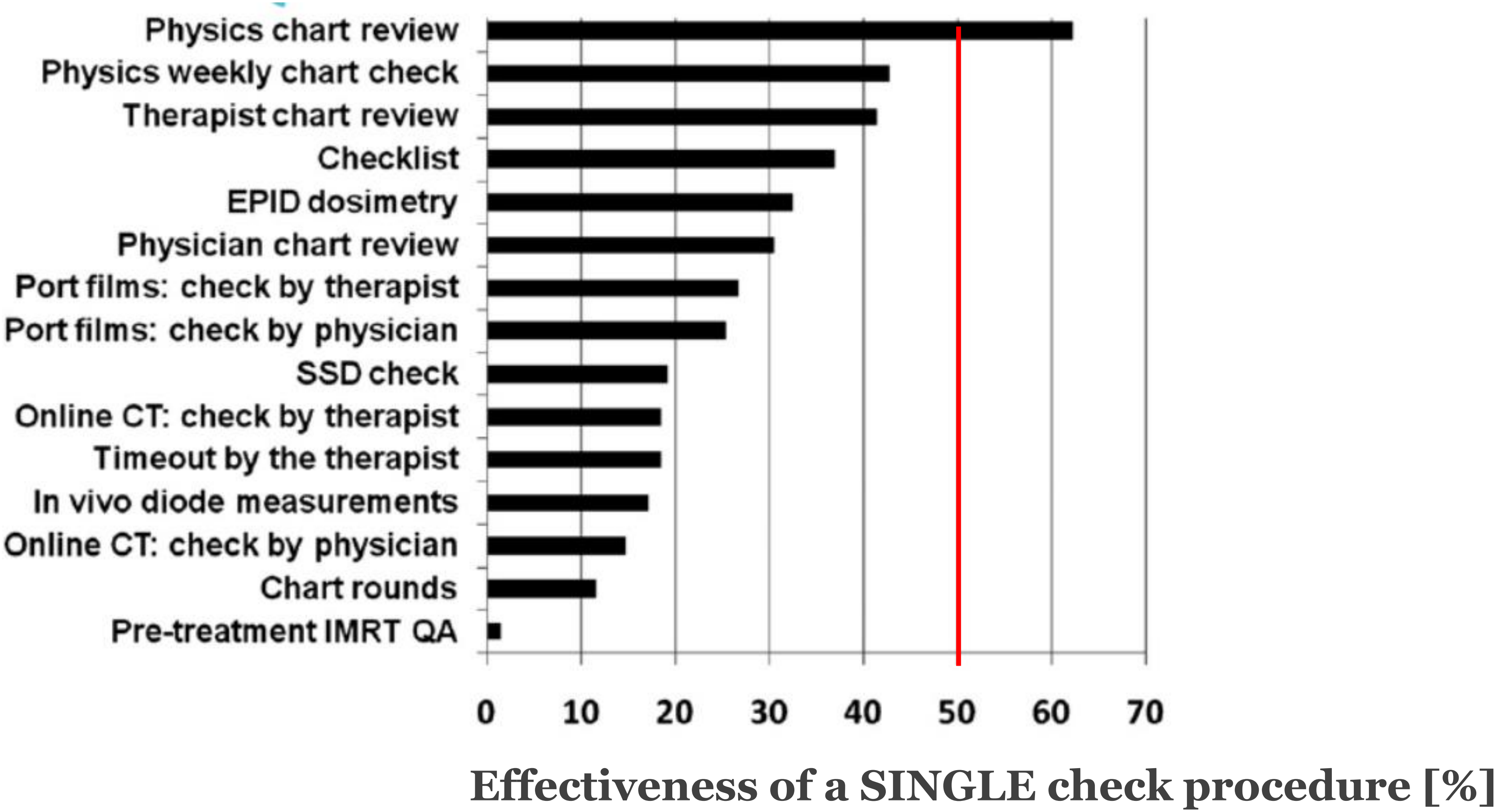
TABLE III. The percentage of potentially detectable and all events from the institutional ILS, which originated and were found at each step in the radiation therapy process.

Workflow step	% of potentially detectable events originating at this step	% of potentially detectable events found at this step	% of ALL events originating at this step	% of ALL events found at this step
Patient assessment	7.7	0.6	22.4	3.5
Simulation	28.2	3.3	13.0	8.2
Treatment planning	49.2	26.5	29.6	18.9
Plan review	1.7	38.1	4.7	22.3
Treatment delivery	2.8	14.9	8.9	29.1
On-treatment QM	1.6	8.8	2.8	9.4
Post-tx completion	0	0.6	11.4	6.6
Equipment and software QM	2.2	6.1	0.3	1.4
Not-defined	6.6	1.1	6.8	0.5

- Manual checks
- Majority detected by plan review – need for improvement
- Recommendation for automatisation of check procedures

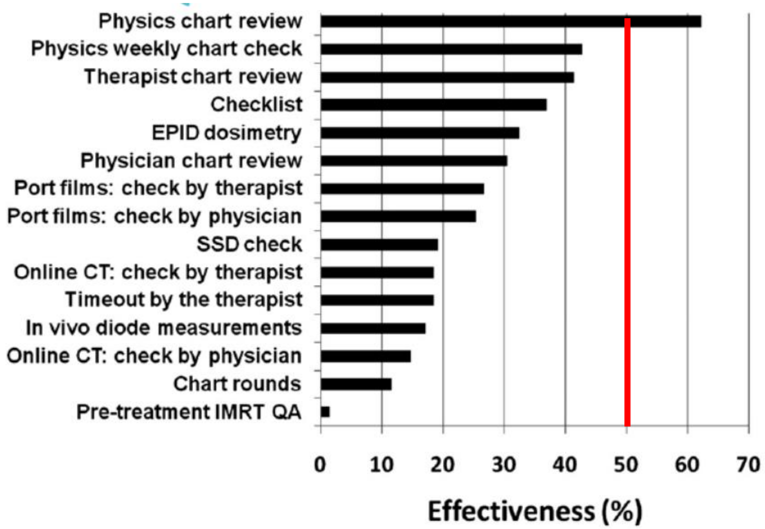
Gopan et al Med Phys 2016

Are the check tools / procedures effective?



Ford et al IJROBP 2012

Are the check tools / procedures effective?

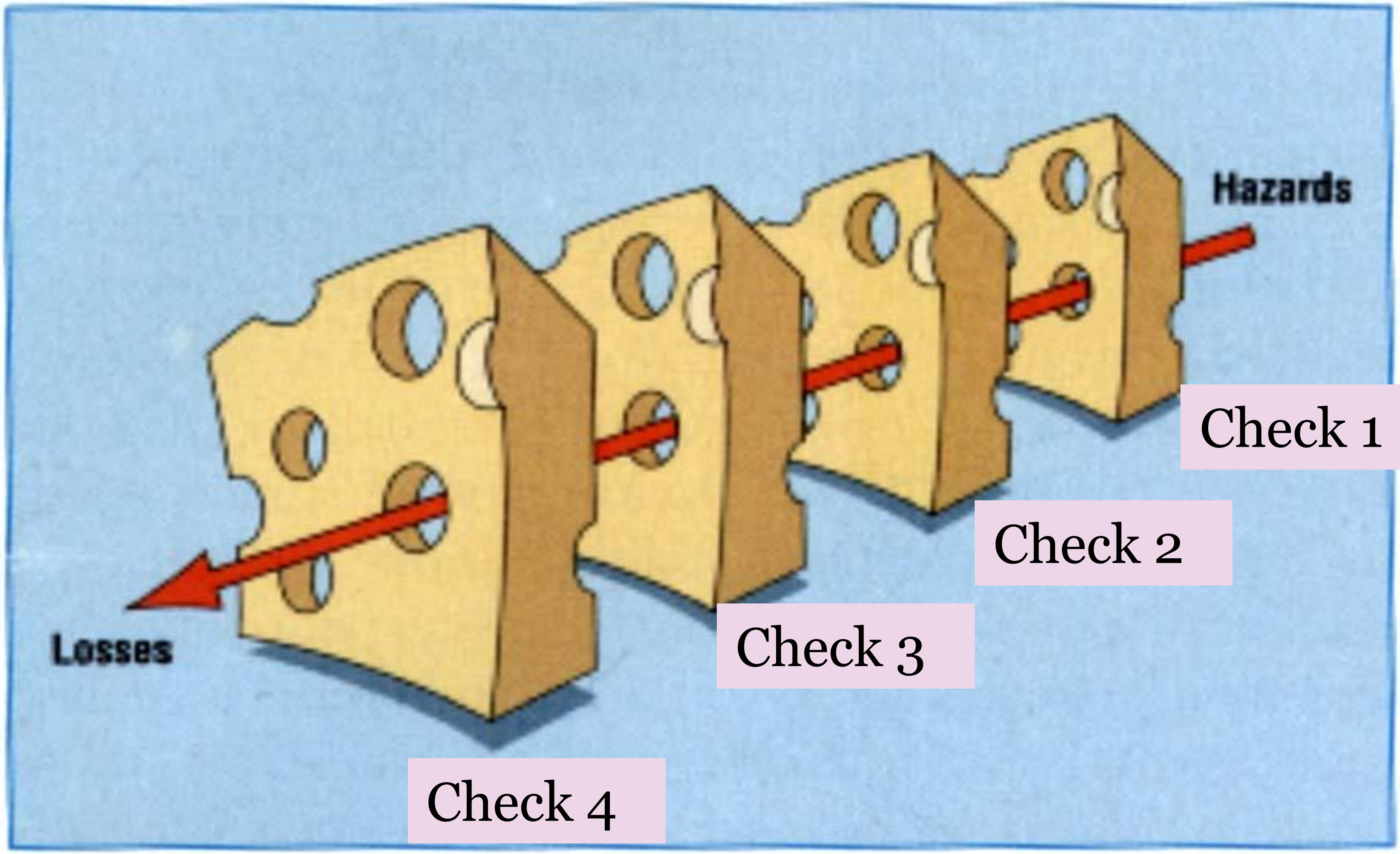


Combined effect of check procedures:

- 7 checks → 97% effectiveness

Ford et al IJROBP 2012

Swiss cheese model of accident causation



J Reason BMJ 2000

Many incidents have a variable magnitude:

- same type of incident can have different impact on different patients / treatment sites
- next time the same incident happens, it may become an accident

Incident prevention to improve patient safety

Proactive

- Patient safety rounds
- Leadership tool

Reactive

- Reporting and analysing incidents

Incident reporting

- Blaming individuals is emotionally more satisfying than targeting institutions
- We cannot change the human condition, but we can change the conditions under which the humans work

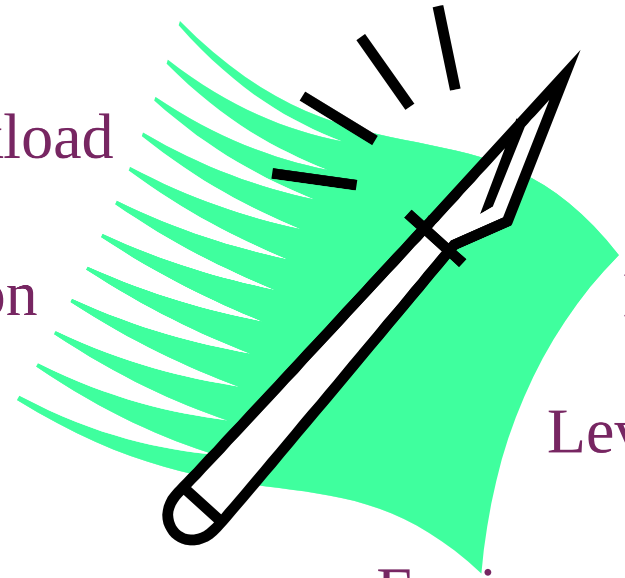
Human Error: models and management - J Reason, BMJ 2000

Incident reporting

- Incident reporting must not result in disciplinary investigation as a consequence of reporting

Frontline person

Workload



Communication

Leadership

Teamwork

Level of skill and qualification

Equipment

Organisation

Incident reporting

internal ⟷ external

internal
- locally
- inside your dept / institution

external
- outside your organisation
- sharing with peers

mandatory
- to regulatory authorities

voluntary
- to professional (inter)national organisation

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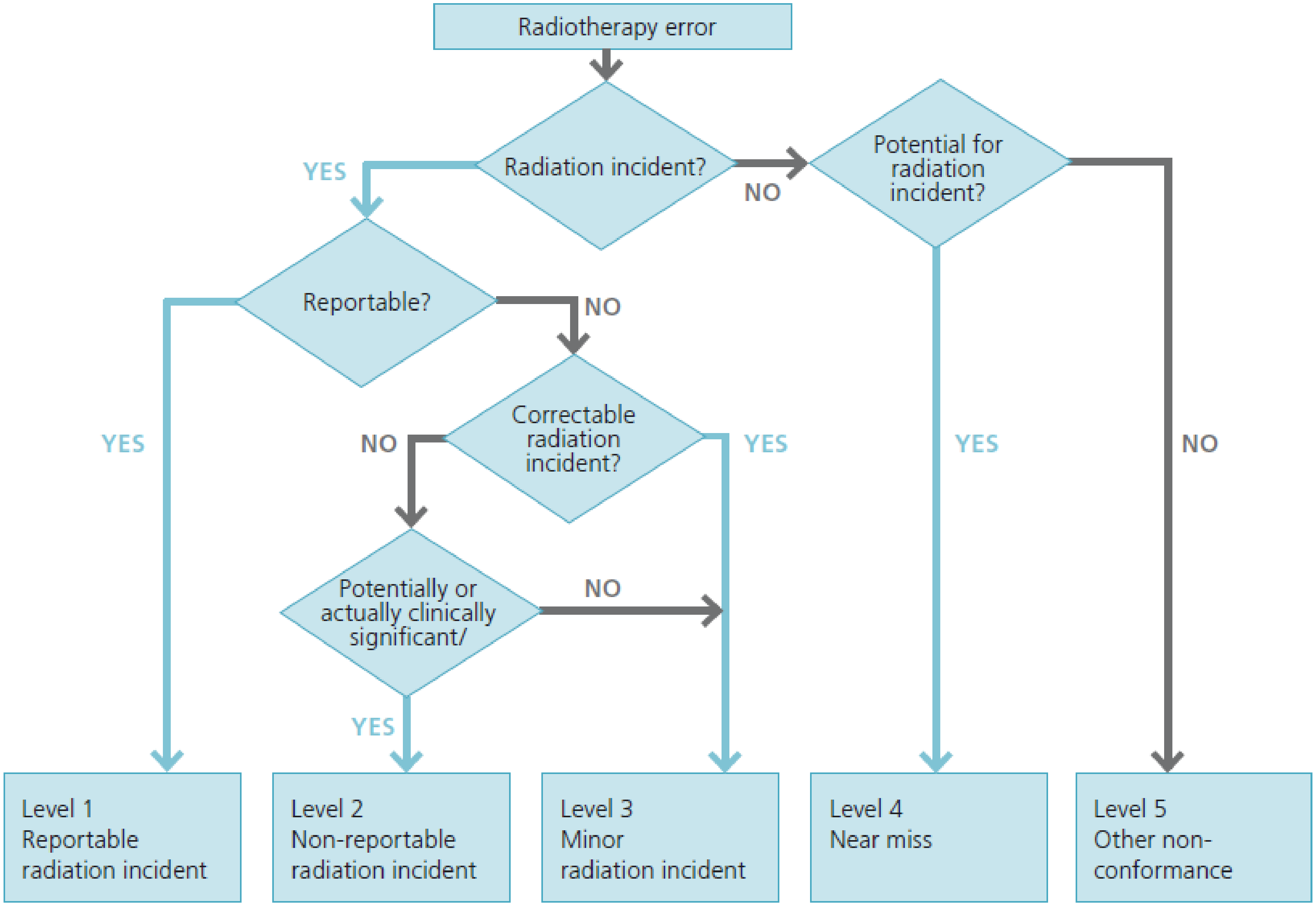
Incident reporting

internal ⟷ external

- Bigger "pool of events" facilitate better identification of safety critical steps in the process of radiotherapy
- Incidents from another hospital can lead to early identification of hazard in your own hospital, before an actual incident occurrence
- Providing general culture of safety awareness

What to report?



from *Towards safer radiotherapy*

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What to report?

You should report all unintended incidents:

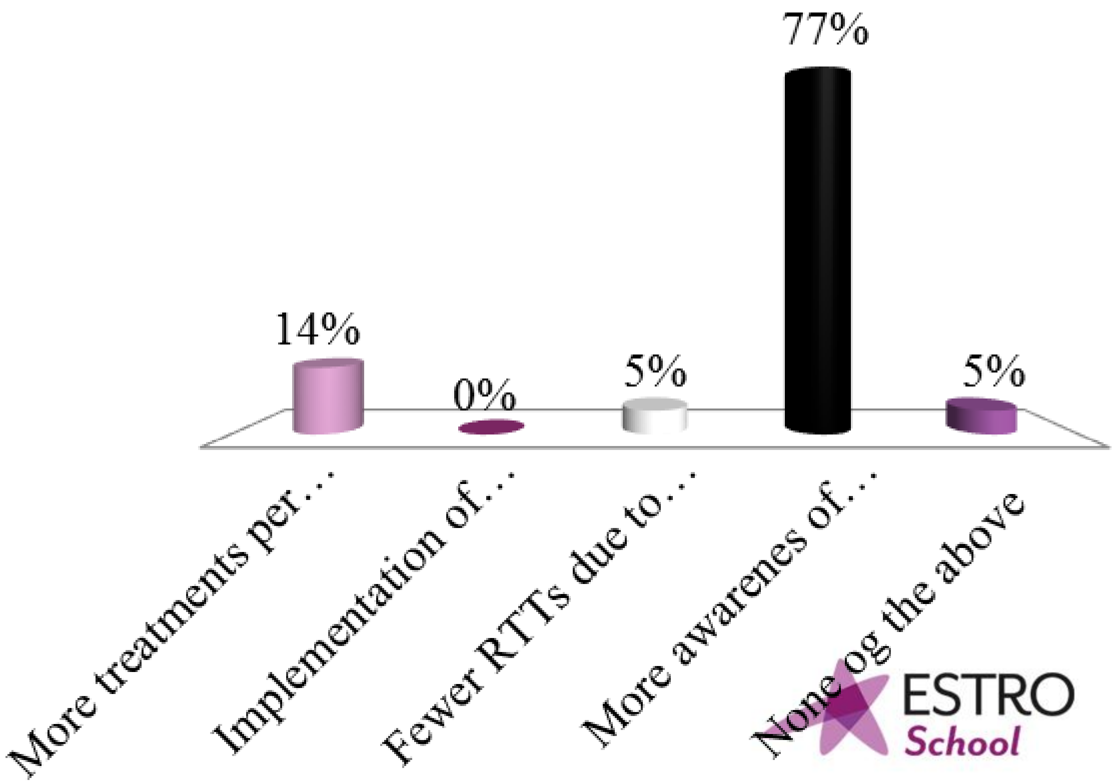
- Observed by you, during involvement in the incident
- Observed by observing others
- Made to attention at a later point in time

All incidents
affecting patient safety
or
potentially affecting patient safety

How to explain the increase of incidents?

Year	2008	2009	2010	2011
# of incidents reported	14	30	115	122

A. More treatments per linac
B. Implementation of advanced technology
C. Fewer RTTs due to budget cut downs
D. More awarenes of incident reporting
E. None og the above



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Role of incident reporting system

- To **identify** system design flaws and critical steps in the radiotherapy pathway
- To highlight **critical problems and patterns** of causes of these problems
- To **spread knowledge** on new risks or involving new technology
- To **promote safety culture** and awareness through involvement of and feedback to staff and managers
- To **prevent** repeated incidents

Role of incident reporting system

Incident reporting system has to be a part of a longer chain:

- Incident Identification
- Reporting
- Investigation
- Analysis
- Management
- Learning

Analysis methods

- Root cause analysis
- Journalaudit
- Mortality analysis
- Global Trigger Tool

Root cause analysis

A systematic method to identify

- WHAT happened
  …the actual chain of events leading to the incident

- WHY could it happen
  …identification of what caused the incident

- HOW to prevent the incident to happen again
  …action plan & follow up

•…NEVER, who caused the incident

Take home message

- Incidents are more numerous and varying than actual accidents
- By learning from the incidents happening in your clinic you can avoid a potential future accident
- Incident report is an essential tool for safer radiotherapy

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Workshop on Plan Selection

Rianne de Jong *RTT*
Academic Medical Centre, Amsterdam
Prague 2017

m.a.j.dejong@amc.uva.nl

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Contents workshop

Plan selection strategies (IGRT-part); theoretical background and AMC experience

Bladder:

- Registration protocol for bladder
- Live Observer Study

Cervix:

- Registration protocol for cervix
- Live Observer Study

Rectum:

- Registration protocol for cervix
- Live Observer Study

Flavours in selection structures

- GTV/CTV
- PTV
- 95% (dose lines)
- ITV
- PTV + 3mm

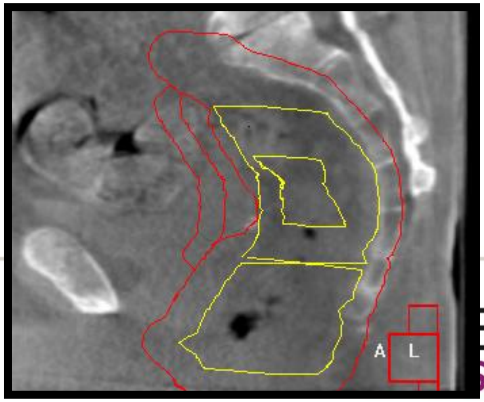
Plan selection at AMC

Bladder

- Start 2013
- Selection based on ***CTV***
- Full and empty bladder CT

Cervix

- Start 2015
- Selection based on ***ITV***
- Full and empty bladder CT



Rectum

- Start 2016 - March
- Selection based on ***variable margins***
- Full bladder CT only

Plan selection at AMC

Bladder

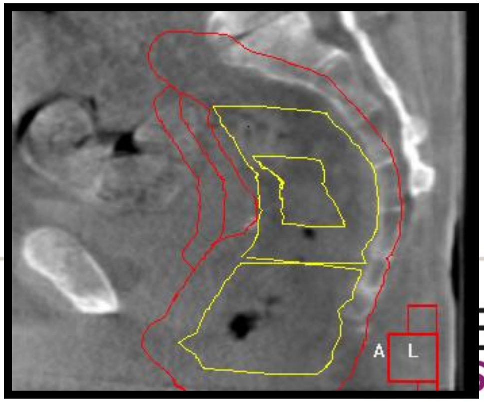
- Start 2013
- Selection based on ***CTV***
- Full and empty bladder CT

Cervix

- Start 2015
- Selection based on ***ITV***
- Full and empty bladder CT

Rectum

- Start 2016 - March
- Selection based on ***variable margins***
- Full bladder CT only

Plan selection Rectum

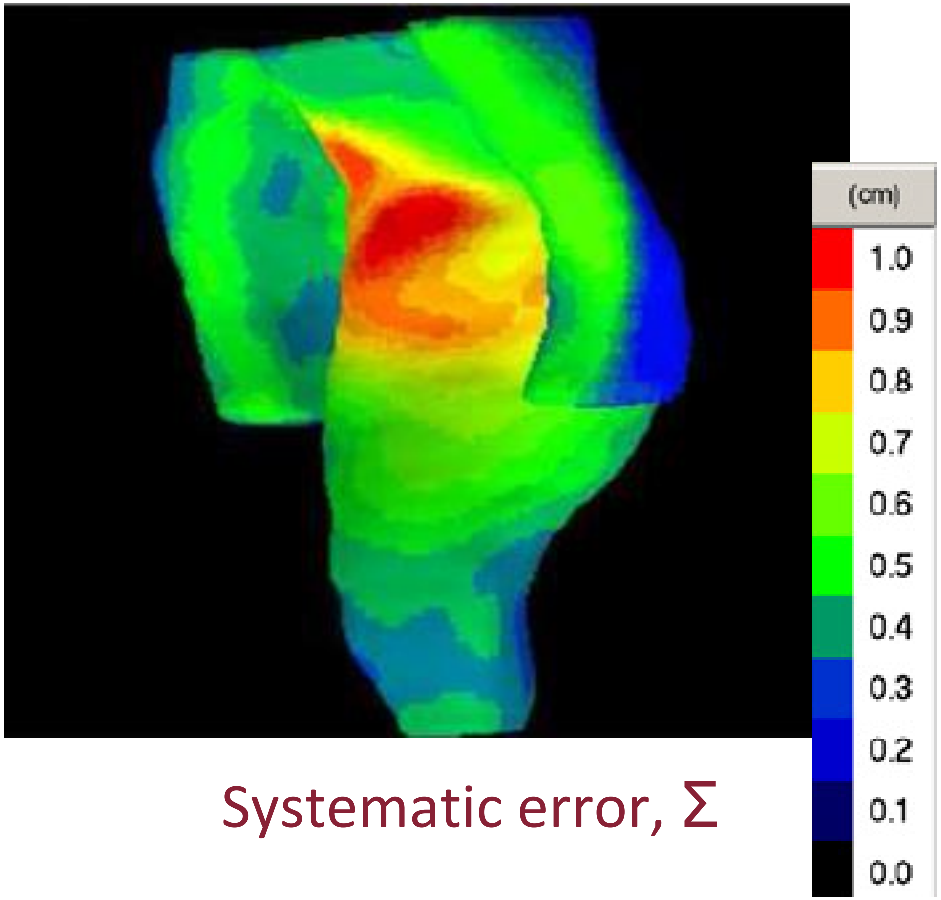
Largest uncertainty:

Upper-anterior side

No correlation with bladder but <u>rectum filling!</u>

Choice & Number margins:

- Encompass largest uncertainty
- Feasible workload for treatment planning
- Complexity of selection at Linac



Systematic error, Σ

Nijkamp et al. (2012), Radiother. Oncol.

Implementation Strategy

Initial strategy plan selection: straightforward

- Only 1 CT scan – no extreme bladder/rectum fillings
- No need of algorithm

But personally, concerns:

- *More complex target definition target volume compared to bladder and cervix?*
- *Larger patient numbers – more RTTs to be trained*
- *Dosimetric benefit given anatomy of target and OAR*

Implementation strategy:

✓ Observer study to assess feasibility and support training and implementation (large number RTTs) *

✓ Dosimetric study to assess dose to OAR **

*de Jong et al.(2016), Radiother. Oncol.
**Lutkenhuis et al. (2016), Radiother. Oncol.

Design of the observer study

- *Select the tightest fitting plan -*

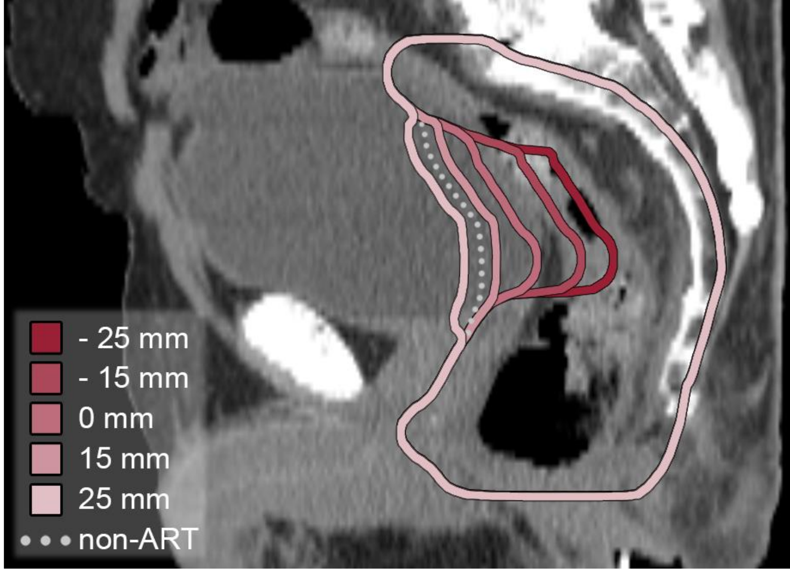
- 20 observers
  - 15 RTT's, 1 PhD student, 4 Physicists
- 11 patients
  - 5 prone with BB, 6 supine
- 5 CBCT scans per patient
- Delineations according to *Roels et al, 2006, IJROPB*

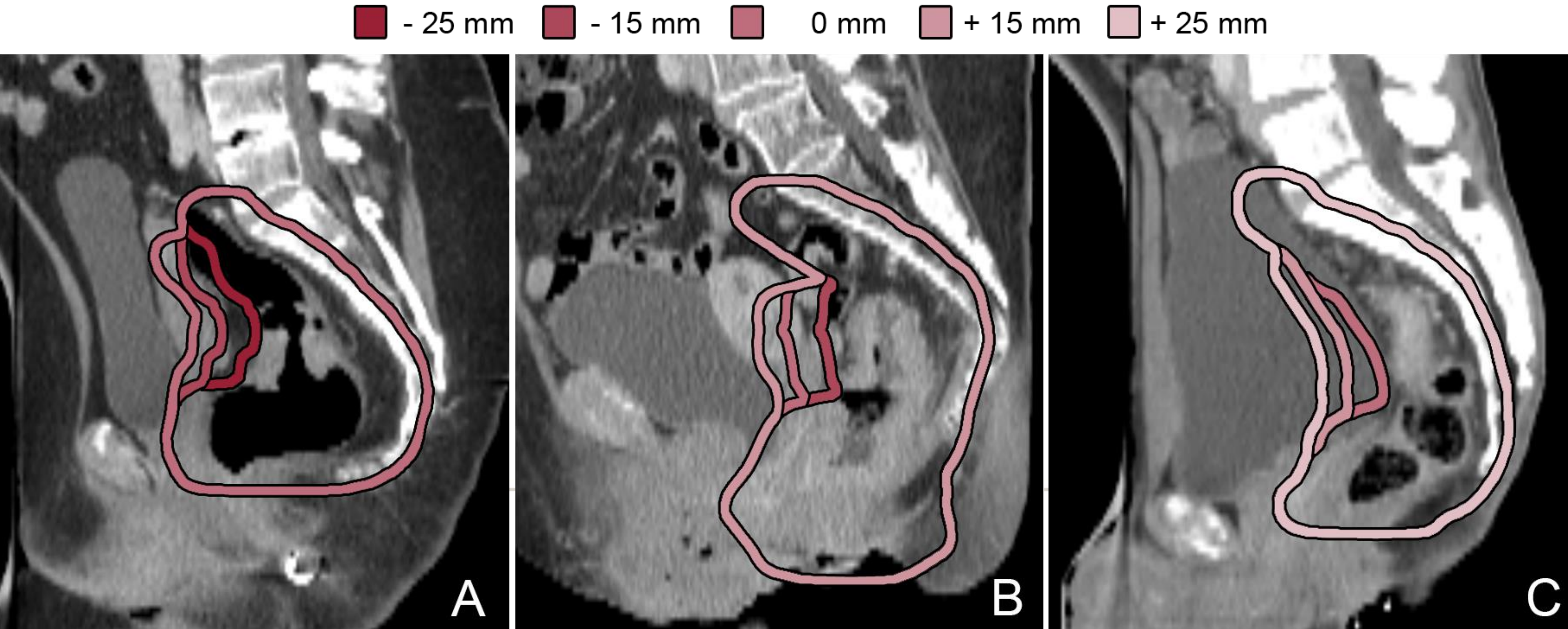
3 margins for ventral side upper mesorectum depending on anatomy captured on CTref:

Rectum	Full	Medium	Empty
Margins	-25 mm, -15 mm, 0 mm	-15 mm, 0 mm, 15 mm	0 mm, 15 mm, 25 mm

Margins plan selection

Visual representation of the variable margins to ventral upper side mesorectum:





Design of the study

1. Lecture on target definition by expert Radiation Oncologist

⇩

2. First measurement - single observers

⇩

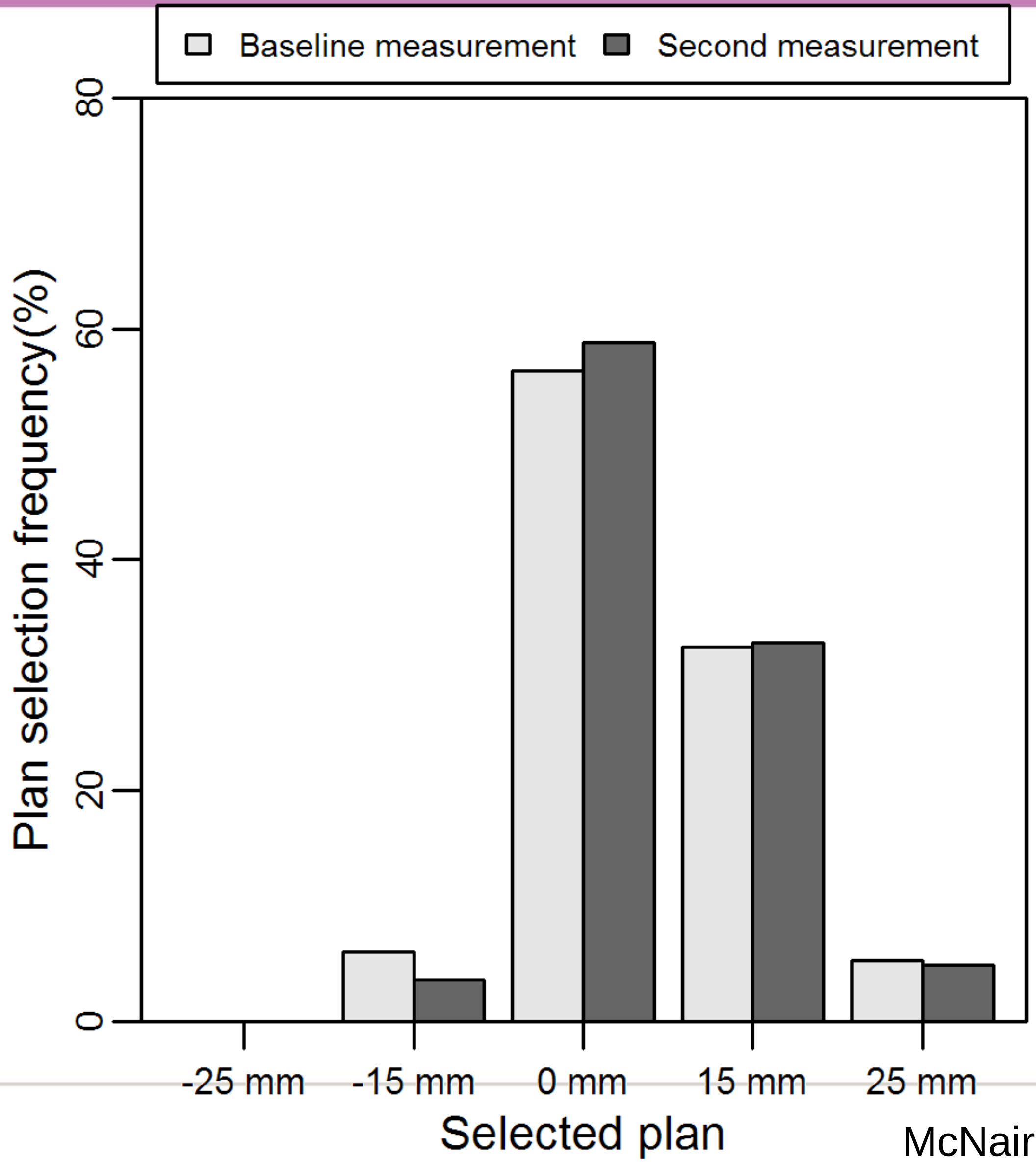
3. Consensus meeting - reviewing all patients, all CBCT scans with all observers and expert radiation oncologists:
defining the gold standard

Veto

⇩

4. Second measurement - single observers

Outcome of the study



Non adaptive margin 20mm

McNair et al. (2015) Br J Radiol.

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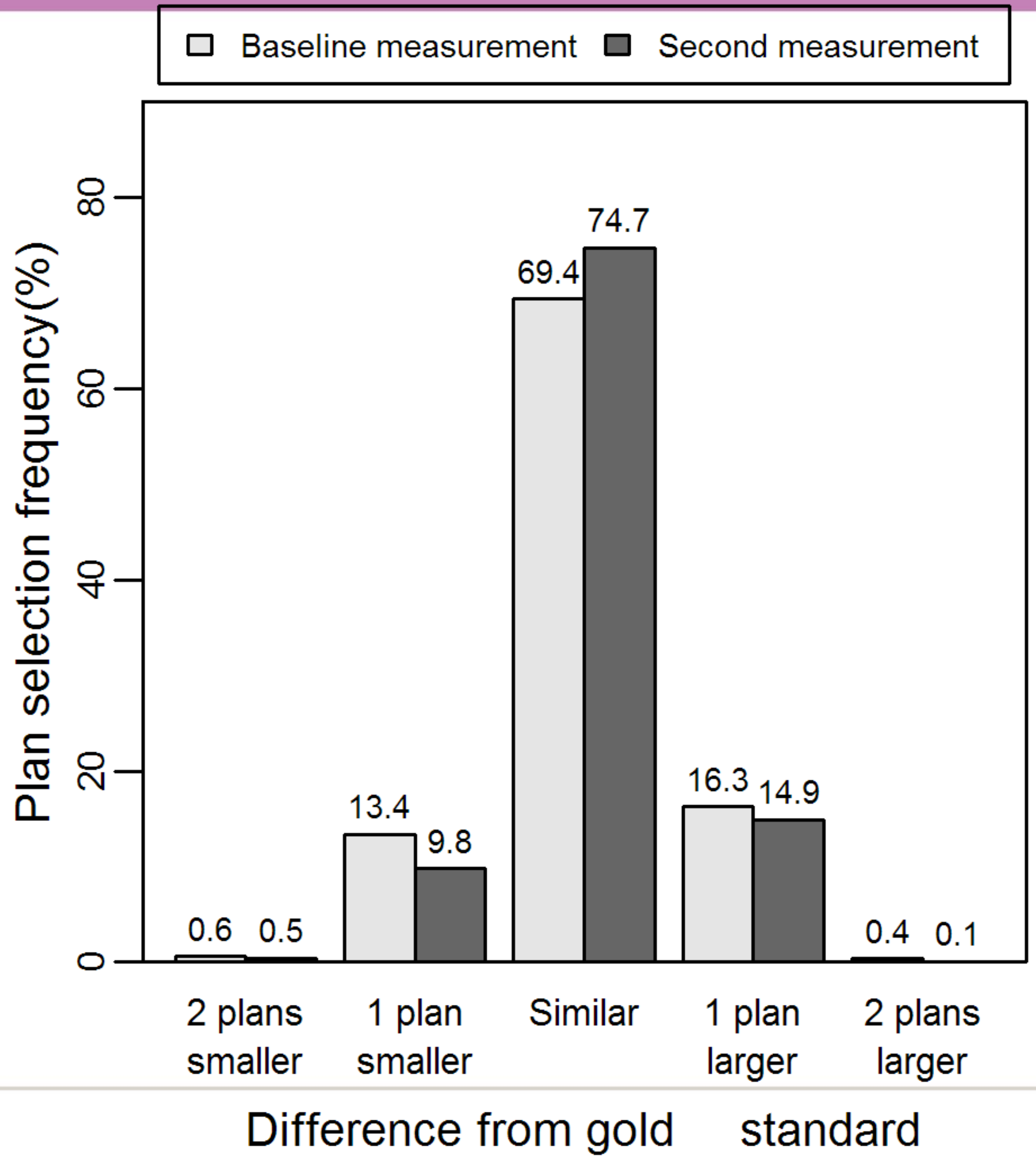
Outcome of the study



Outcome of the study

Did we select a too small plan fewer times 2nd time around?

- Yes, 15,6% - 10.3% ($p = 0.002$)

Did we select a too big plan fewer times 2nd time around?

- No, 16.6% -15.0% ($p = 0.130$)

Was there a difference between supine and prone BB?

- Maybe, in favor of supine

  measurement 1 70.0% versus 64.2% $p > 0.05$

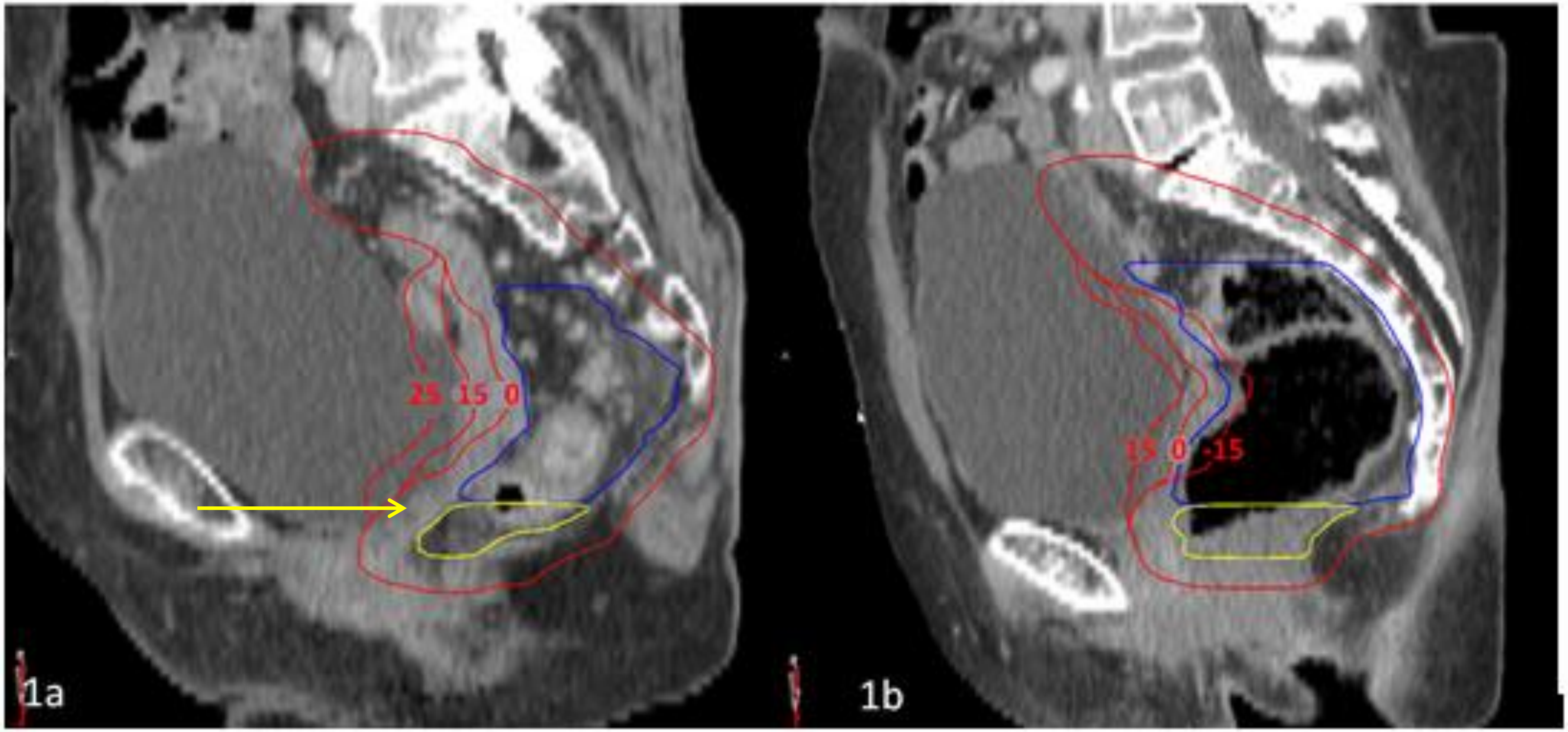
  measurement 2 74.2% versus 67.0% $p > 0.05$

Implementation - conclusion

Observer study:

- Plan selection is feasible: 75% concordance with gold standard
- Observer study also served as training tool
- Margin of -25 mm never selected

Clinical Protocol plan selection Rectum



1 Planning CT scan with full bladder

A. Empty rectum on planning CT: *25 mm, 15 mm, 0 mm* anterior margins

B. Full rectum on planning CT: *15 mm, 0 mm, -15 mm* anterior margins

Clinical protocol plan selection Rectum

- 2 sets of 3 margins
- Long (25x2Gy) and short (5x5Gy) treatment
- VMAT
- Daily CBCT
- 1/w post treatment CBCT: intra fraction motion
- 1/w retrospective review: all plan selections

  consistency imaging- and management system

Clinical protocol plan selection Rectum

Exclusion criteria:

- Dual hip prostetics
- T4 tumors
- Time constraints can not be met

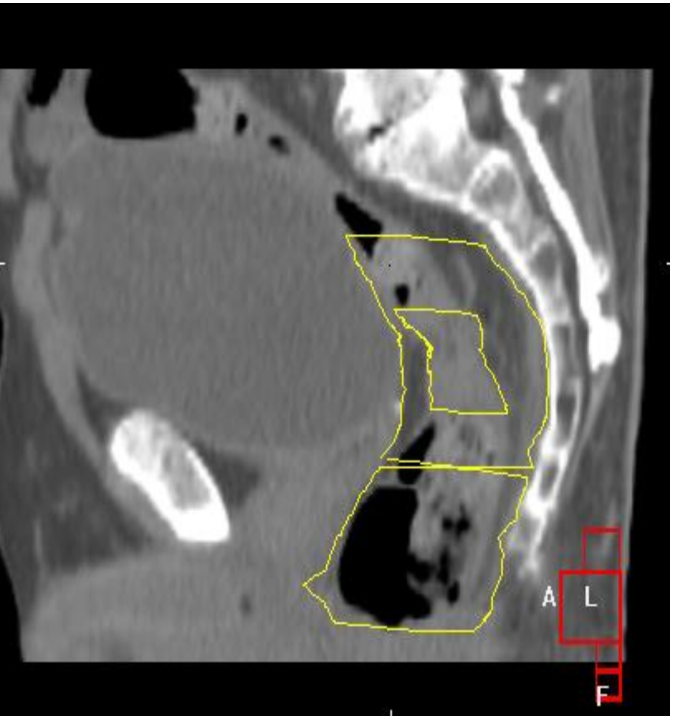
  - *Inguinal lymfe nodes*
  - *Length CTV_Mesorectum_up < 5 cm in CC direction*

At the treatment machine

Plan selection at the treatment machine:

First week: *1 trained RTT and 1 physicist, 1 physician*

Second week: *2 RTTs (1 trained)*



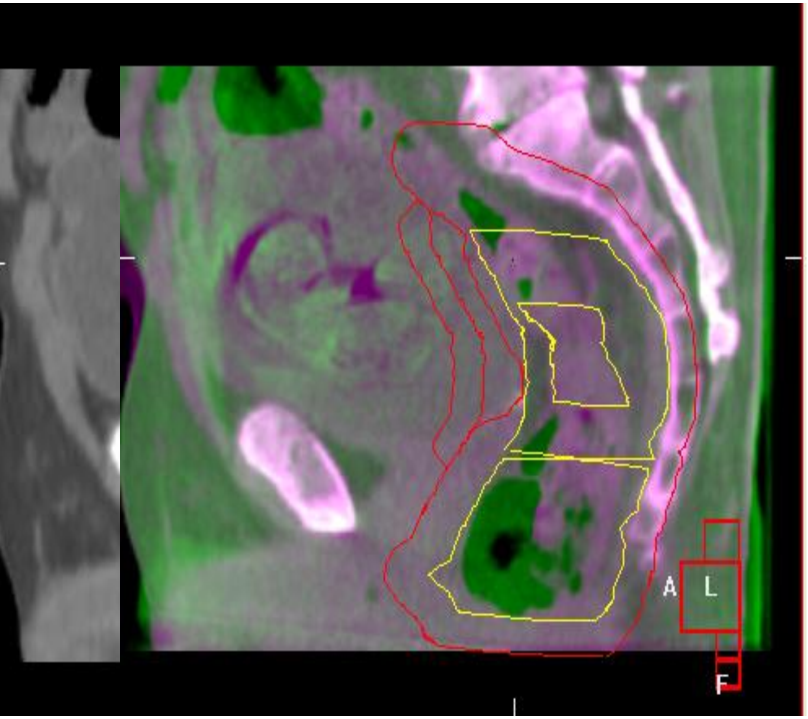
Target volume
on Planning CT

At the treatment machine

Plan selection at the treatment machine:

First week: *1 trained* RTT and 1 physicist, 1 physician*

Second week: *2 RTTs (1 trained)*



Bone match
Overlay CT/CBCT

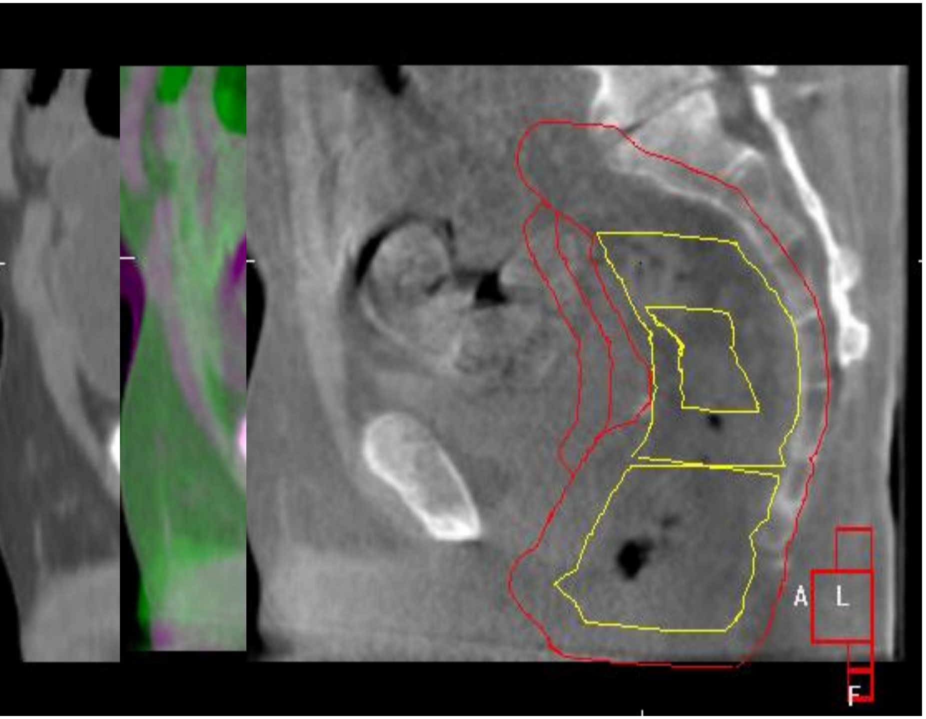
* de Jong *et al.(2016), Radiother. Oncol.*

At the treatment machine

Plan selection at the treatment machine:

First week: *1 trained* RTT and 1 physicist, 1 physician*

Second week: *2 RTTs (1 trained)*



Target volume & margins on CBCT

* de Jong *et al.(2016), Radiother. Oncol.*

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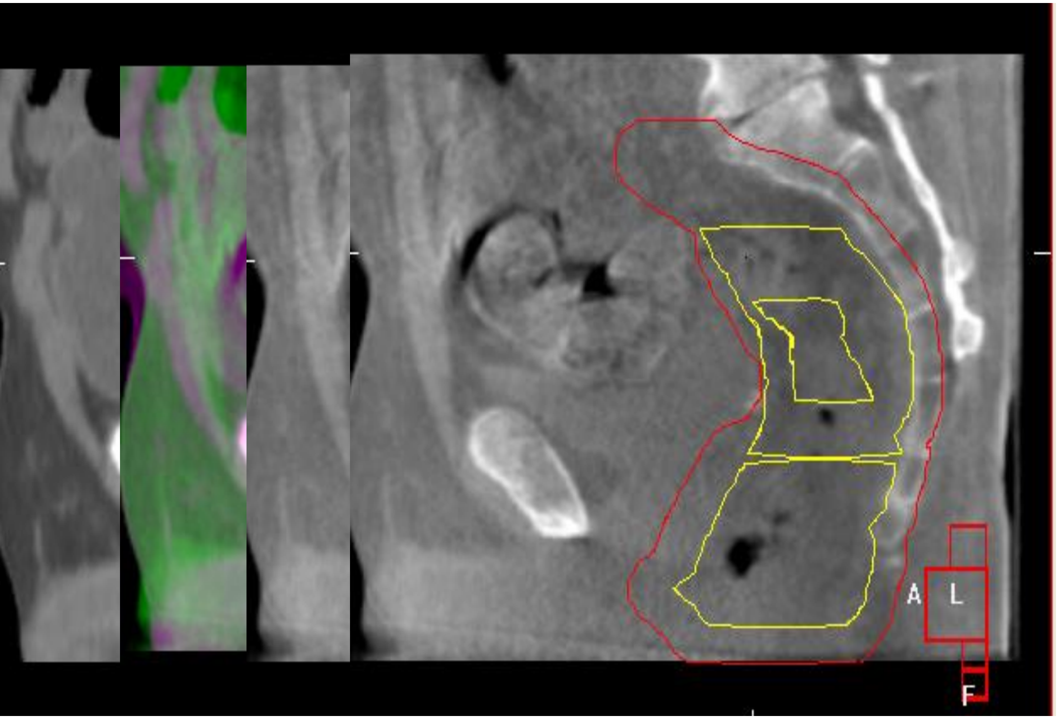
At the treatment machine

Plan selection at the treatment machine:

First week: *1 trained* RTT and 1 physicist, 1 physician*

Second week: *2 RTTs (1 trained)*



Selected margin
On CBCT

* de Jong *et al.(2016), Radiother. Oncol.*

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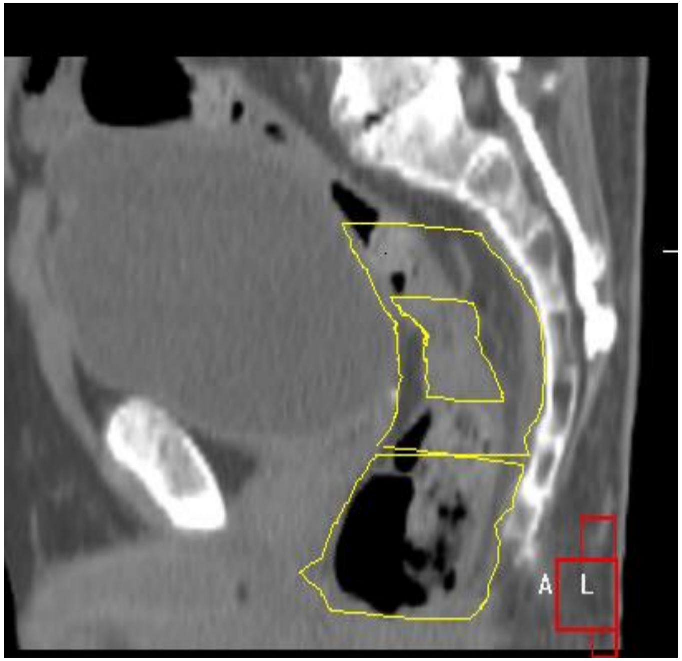
At the treatment machine

Plan selection at the treatment machine:

First week: *1 trained* RTT and 1 physicist, 1 physician*

Second week: *2 RTTs (1 trained)*



Empty bladder but smallest margin!

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Evaluation

March 2016 – May 2017

70 patients treated with plan selection

*Evaluation of the **first 20** (consecutive) patients*

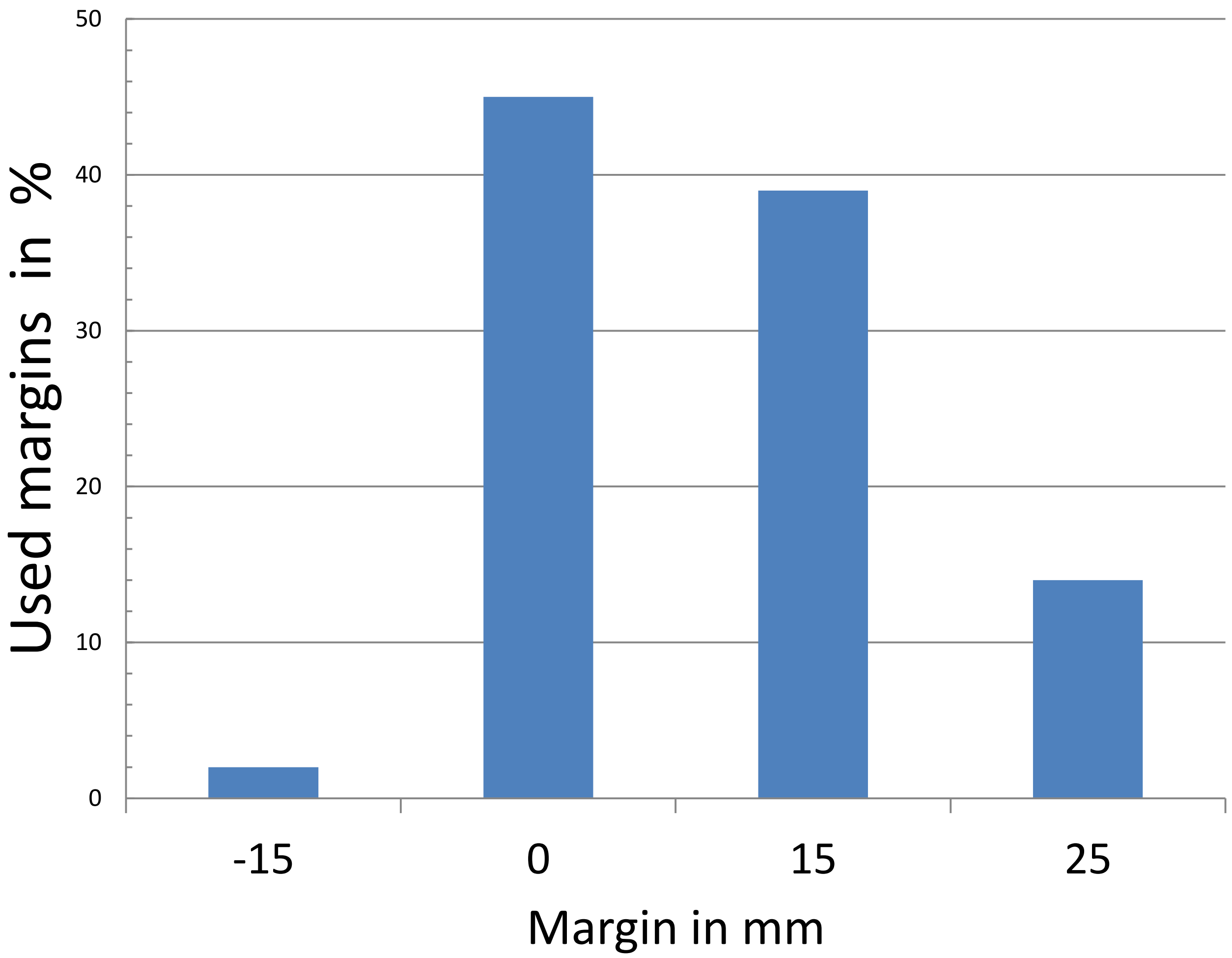
10x short treatment scheme (5x5Gy)

10x long treatment scheme (25x2Gy)

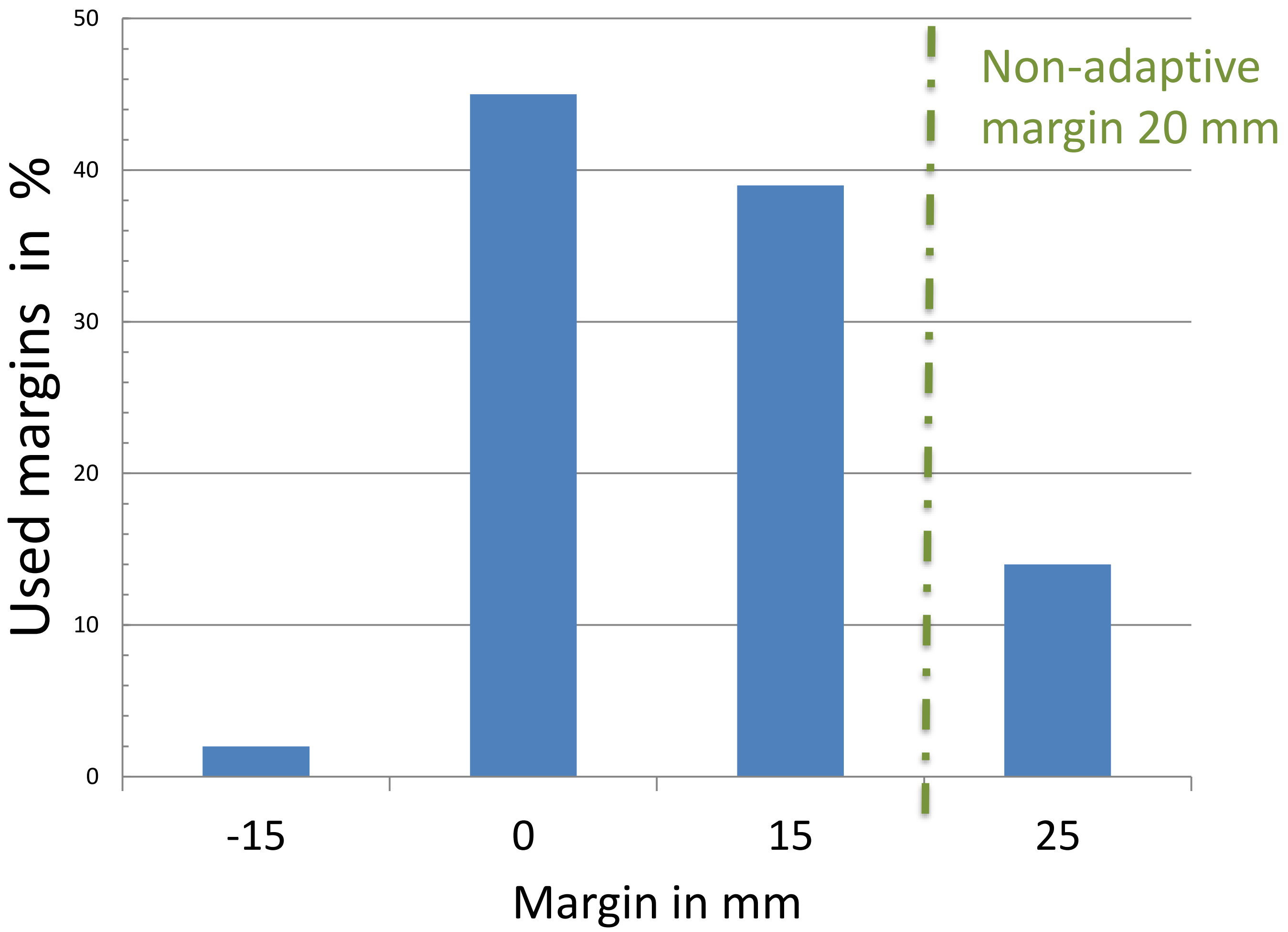
Margins sets used:

Full rectum	(+15 / 0 / -15mm)	30%	
Empty rectum	(+25/ +15 / 0 mm)	65%	
Full rectum	(+15 / 0 mm)	5%	(insufficient TP time)

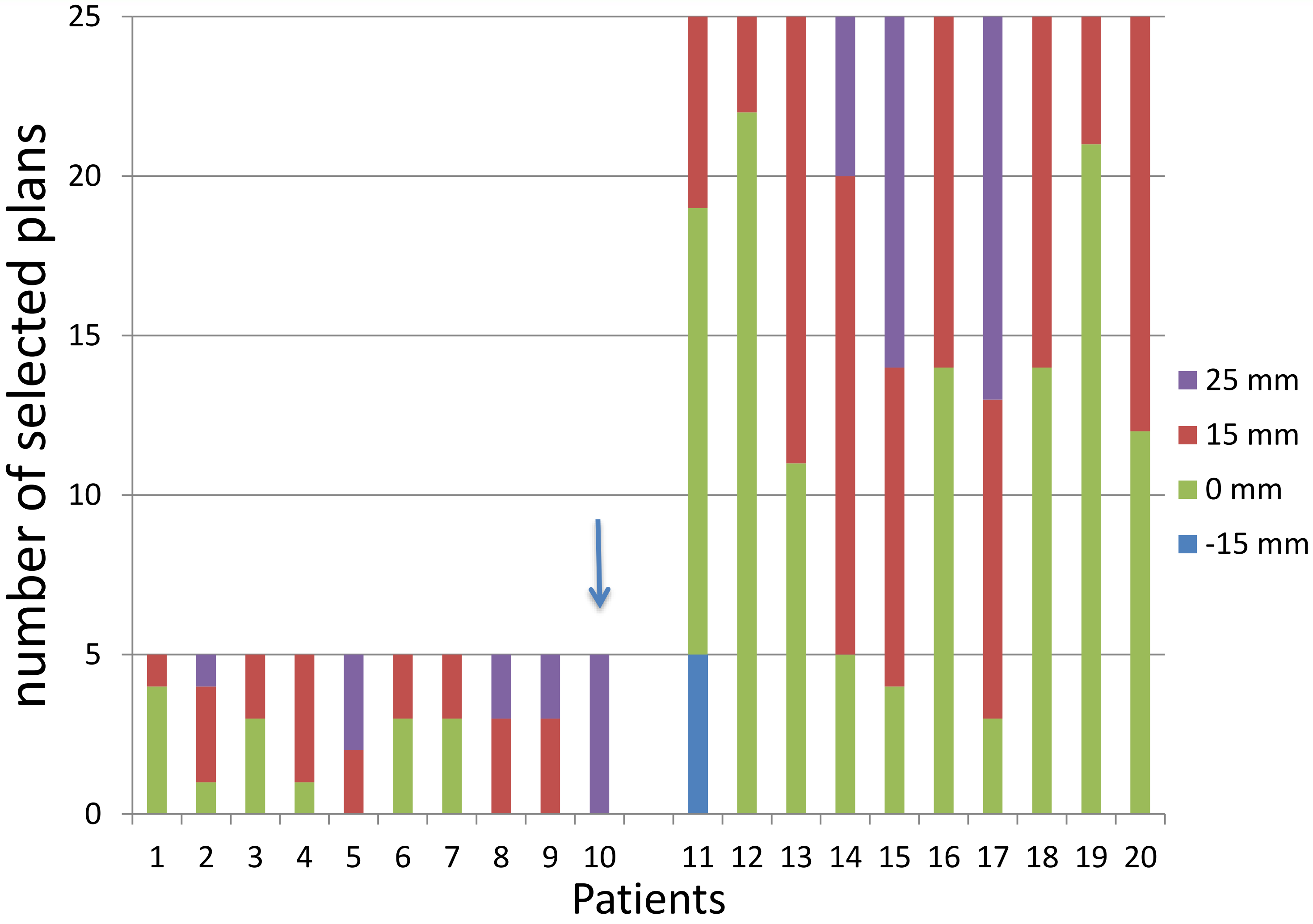
Selected plans



Selected plans

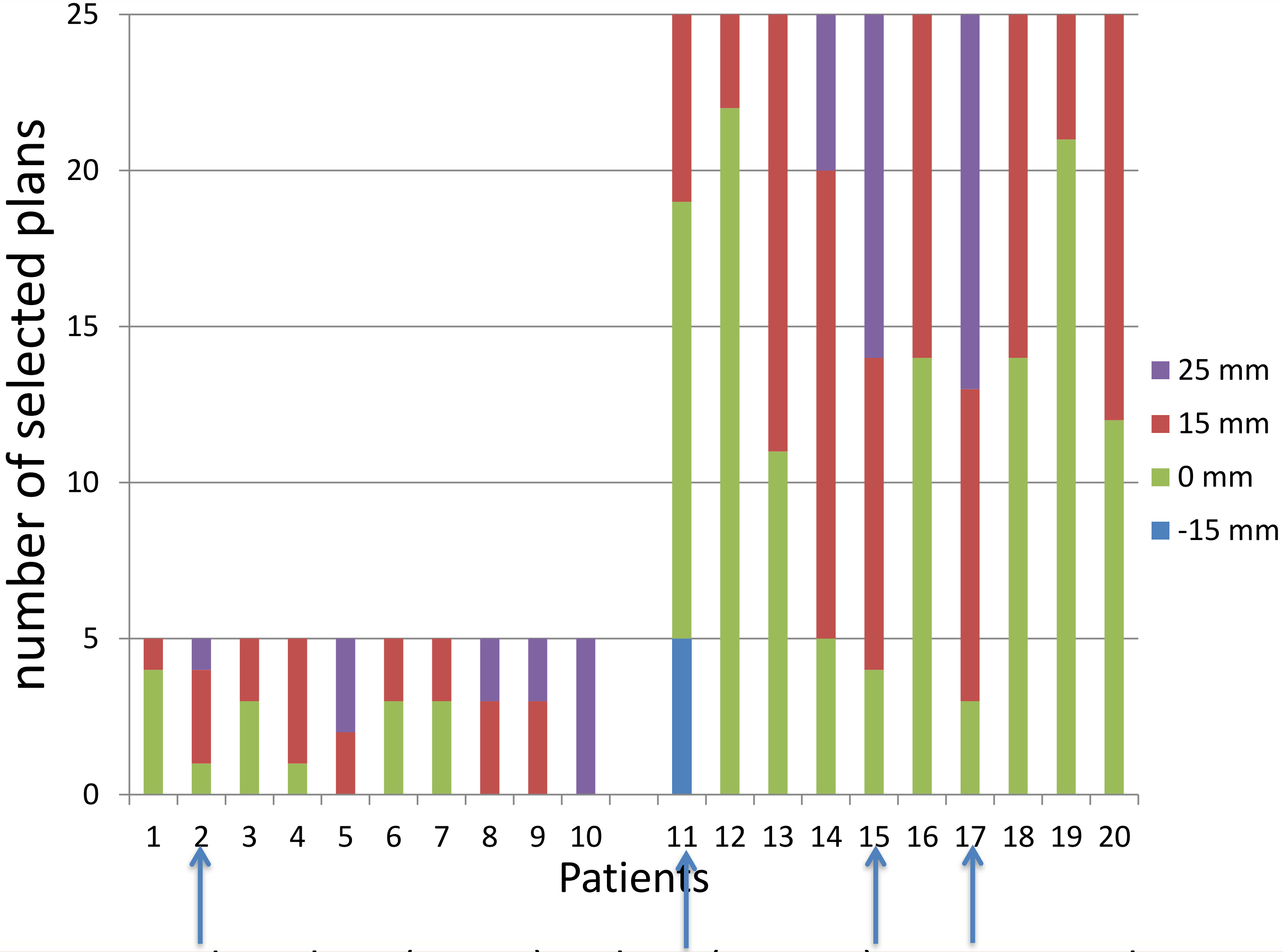


Selected plans



Sorted on short (5x5Gy) en long (25x2Gy) treatment scheme

Selected plans



Sorted on short (5x5Gy) en long (25x2Gy) treatment scheme

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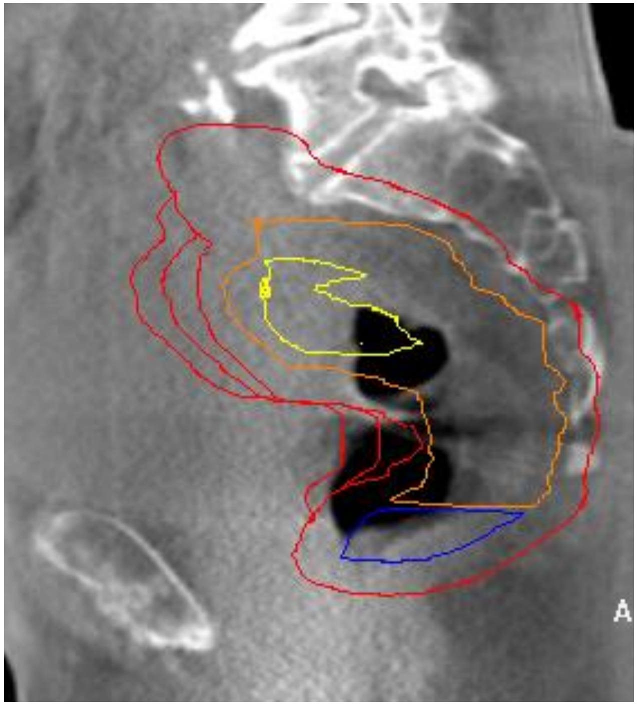
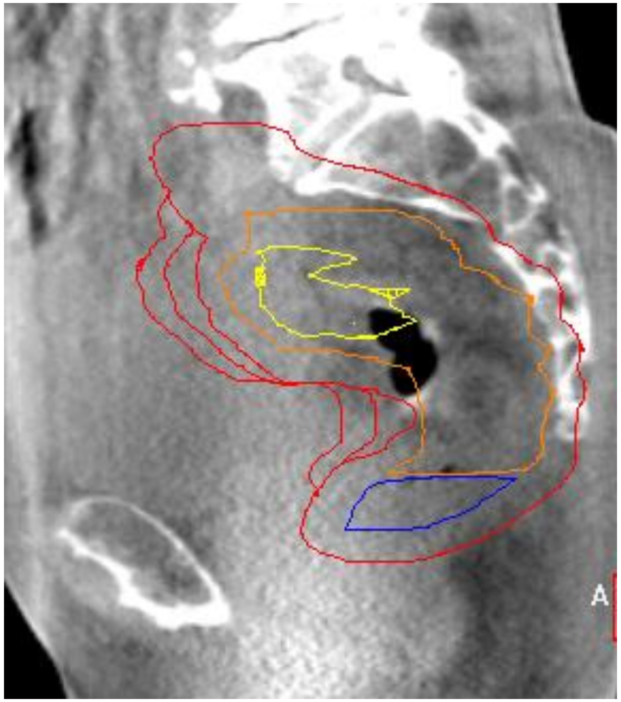
Evaluation

Delayed treatment: 7 x   (5 x in 1 patient)

To obtain a more favorable anatomy in case of a very full rectum, usually caused by gas pockets





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Evaluation

Delayed treatment: 7 x (5 x in 1 patient)

To obtain a more favorable anatomy in case of a very full rectum, usually caused by gas pockets

Post-treatment CBCT 1pw:

1 fraction the selected plan was no longer suitable due to a moving gas pocket

Evaluation

Delayed treatment: 7 x (5 x in 1 patient)

- To obtain a more favorable anatomy in case of a very full rectum, usually caused by gas pockets

Post-treatment CBCT 1pw:

- 1 fraction the selected plan was no longer suitable due to a moving gas pocket

The weekly review:

- Smaller margin could have been selected in 20% of fractions, and a larger margin in 2% of fractions
- No inconsistencies between the imaging system and radiotherapy management system!

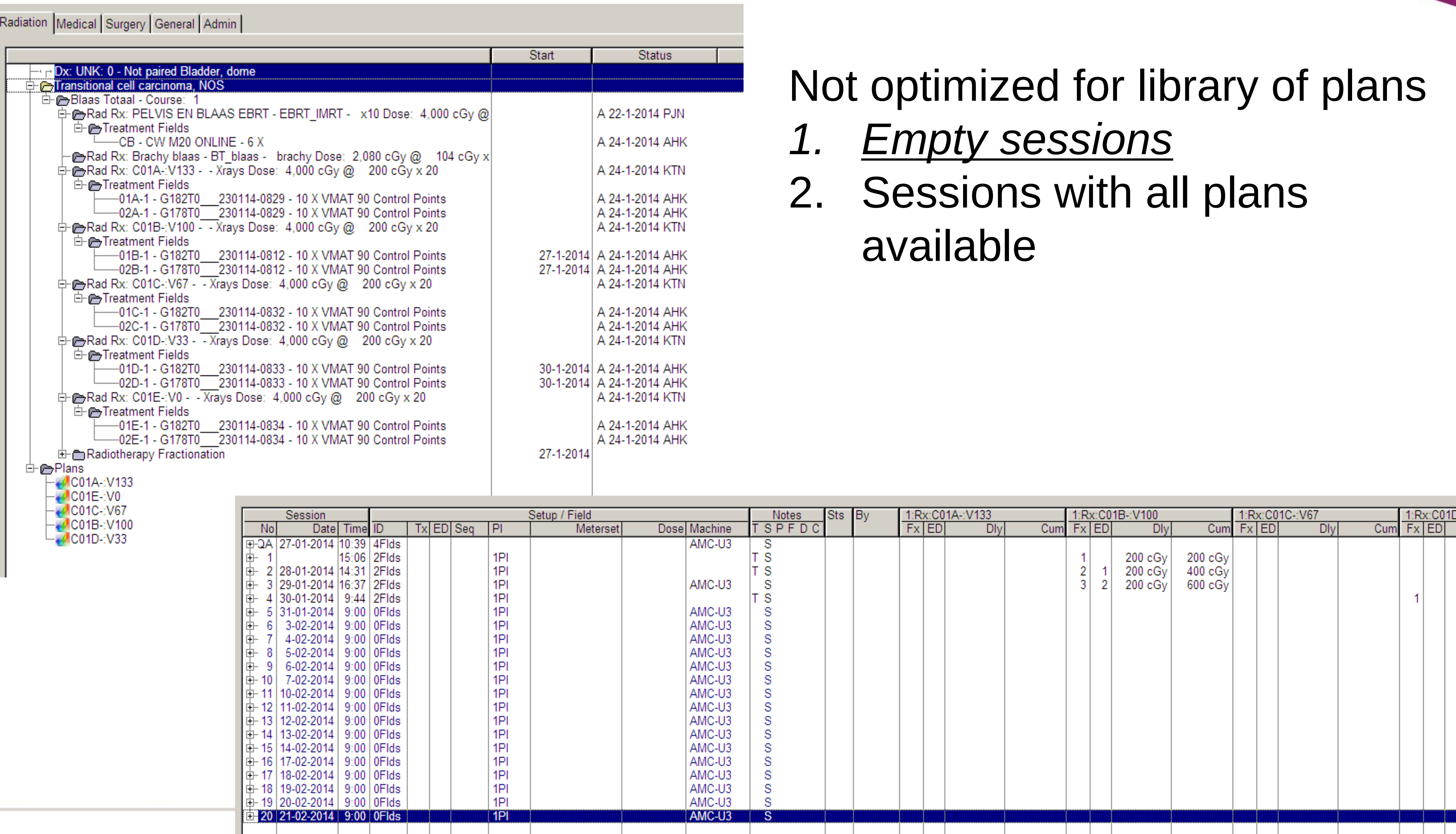
Summary evaluation

Plan selection for rectum cancer with variable margins for upper mesorectum for first 20 patients:

- Both sets of margins used
- Majority of patients needed multiple margins
- Limited influence of intra fraction motion
- Good consistency in weekly review
- No errors between imaging and management system
- Limited delay remains due to anatomy on CBCT

- Successfully and safely implemented! -

Management system - Mosaiq



Not optimized for library of plans

1. *Empty sessions*
2. Sessions with all plans available

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Extra checks at AMC

ART - Rectum

Patiënt naam:	
Patiënt nummer:	2650976
Course:	1
Plannen:	-15 tot +15

Gegevens opslaan

				Post CBCT				
Fractie	Laborant(en)	Datum	Plan	X	Y	Z	Binnen PTV?	Opmerkingen
1	mms lba ahk	30-05-16	0	-0,02	-0,02	-0,08	☑	geen fysicus bereikbaar in Amsterdam!
2	mka ahk jwa	31-05-16	+15					zaten te twijfelen tussen 0 en +15
3	ahk nwn	01-06-16	0					
4	ahk/pen/awn	02-06-16	0					
5	eac/awn/wls	03-06-16	+15					
6							☐	
7								
8								
9								
10								
11							☐	
12								
13								
14								
15								
16							☐	
17								
18								
19								
20								
21							☐	
22								
23								
24								
25								

Week	Eval.	Door	Opmerkingen
1	☐		
2	☐		
3	☐		
4	☐		
5	☐		

Per 8 februari 2016 zijn we begonnen met planselectie voor rectumpatiënten: ART rectum. Zie voor complete werkinstructie Kwadraat 'Rectum ART'. Iedere dag moet er iemand van de IGART-groep aanwezig zijn bij planselectie.

NB: In tegenstelling tot ART-Blaas mag er bij ART-Rectum NOOIT getweakt worden!

Vragen en/of opmerkingen horen wij graag. Alvast dank.

Jorrit (62594)
Rianne (66857)

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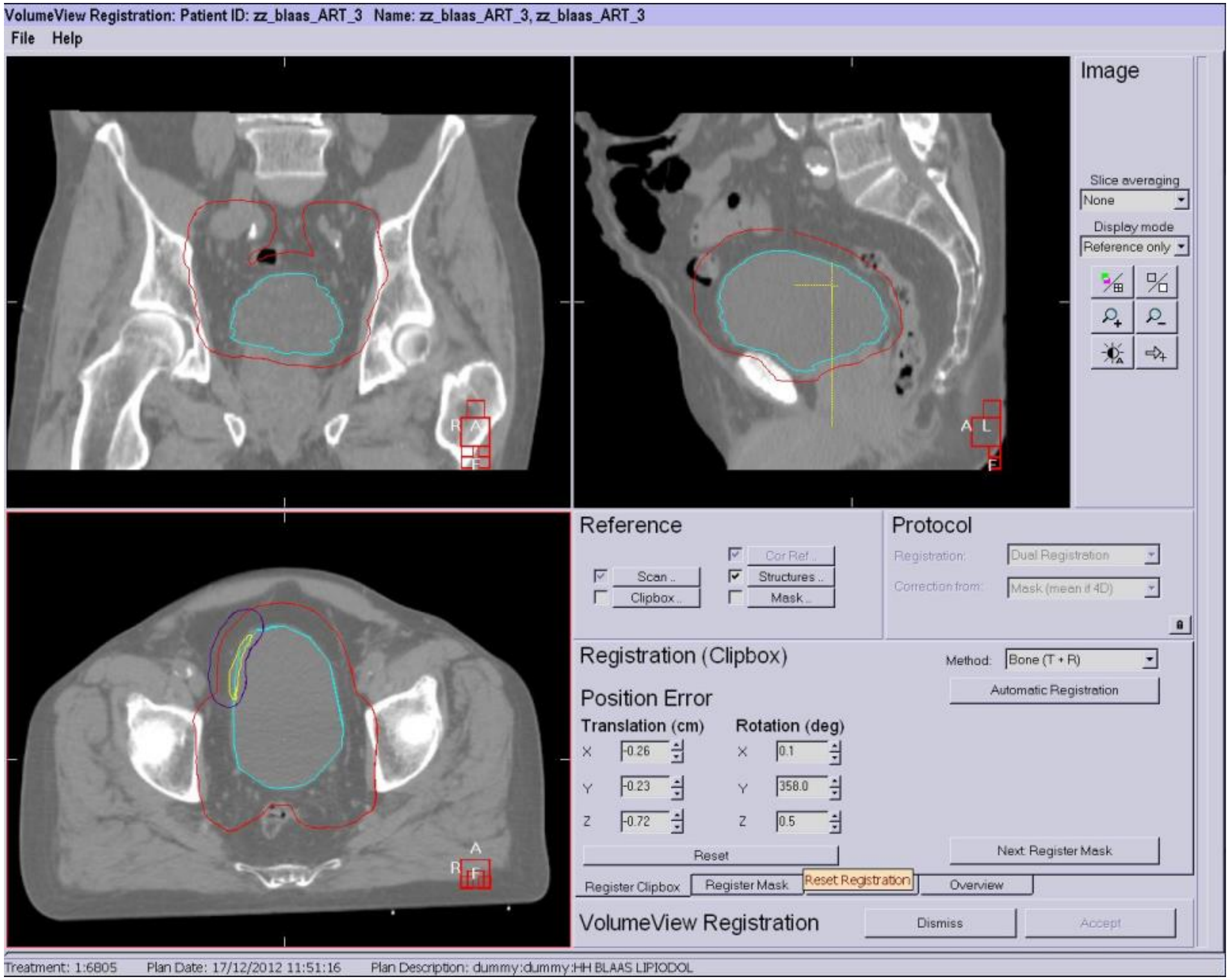
Live plan selection

Bladder

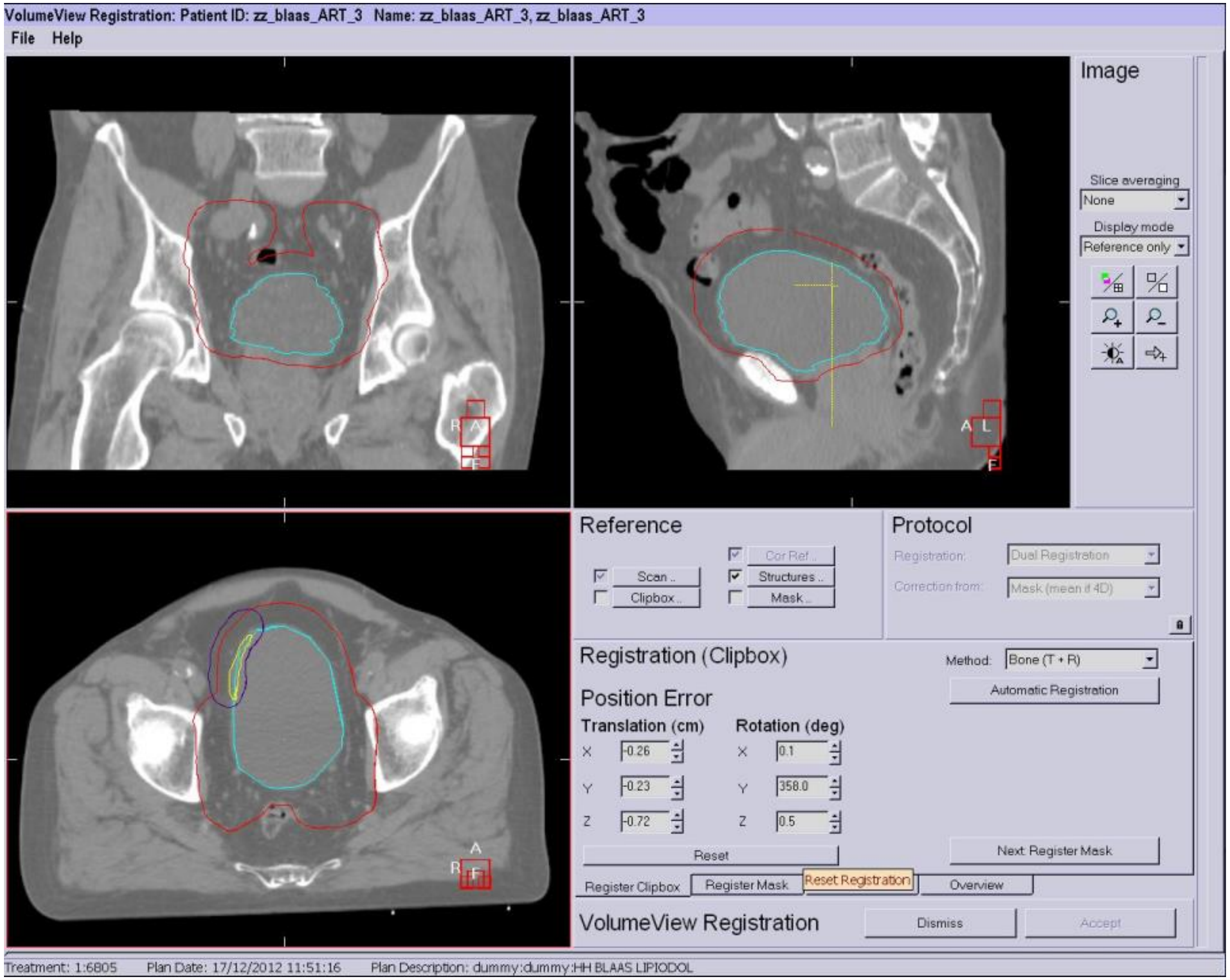


Bladder plan selection @AMC

Targetvolume:

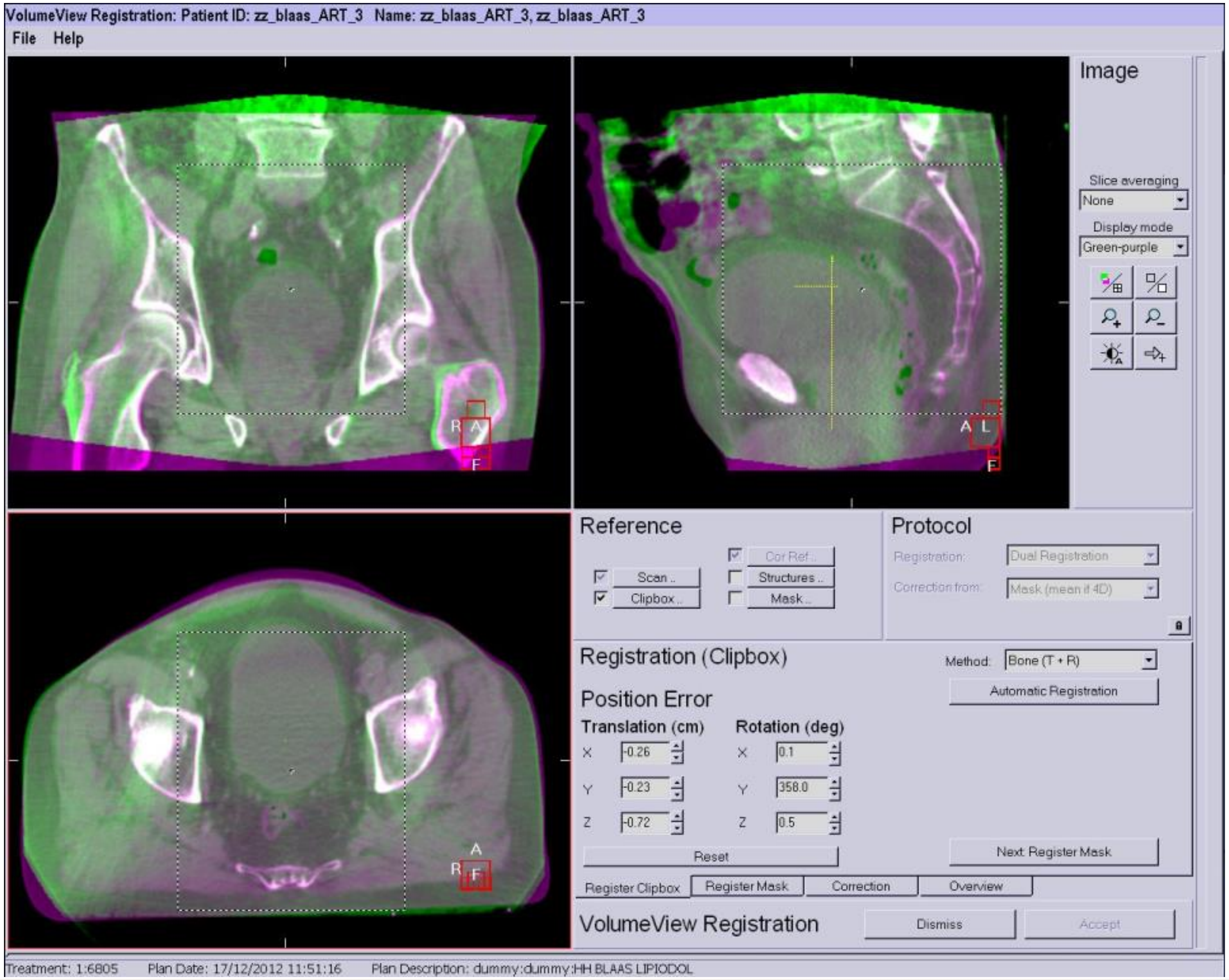
- Whole bladder low dose
- Boost part bladder high dose
- Nodal area up to L5

VMAT delivery



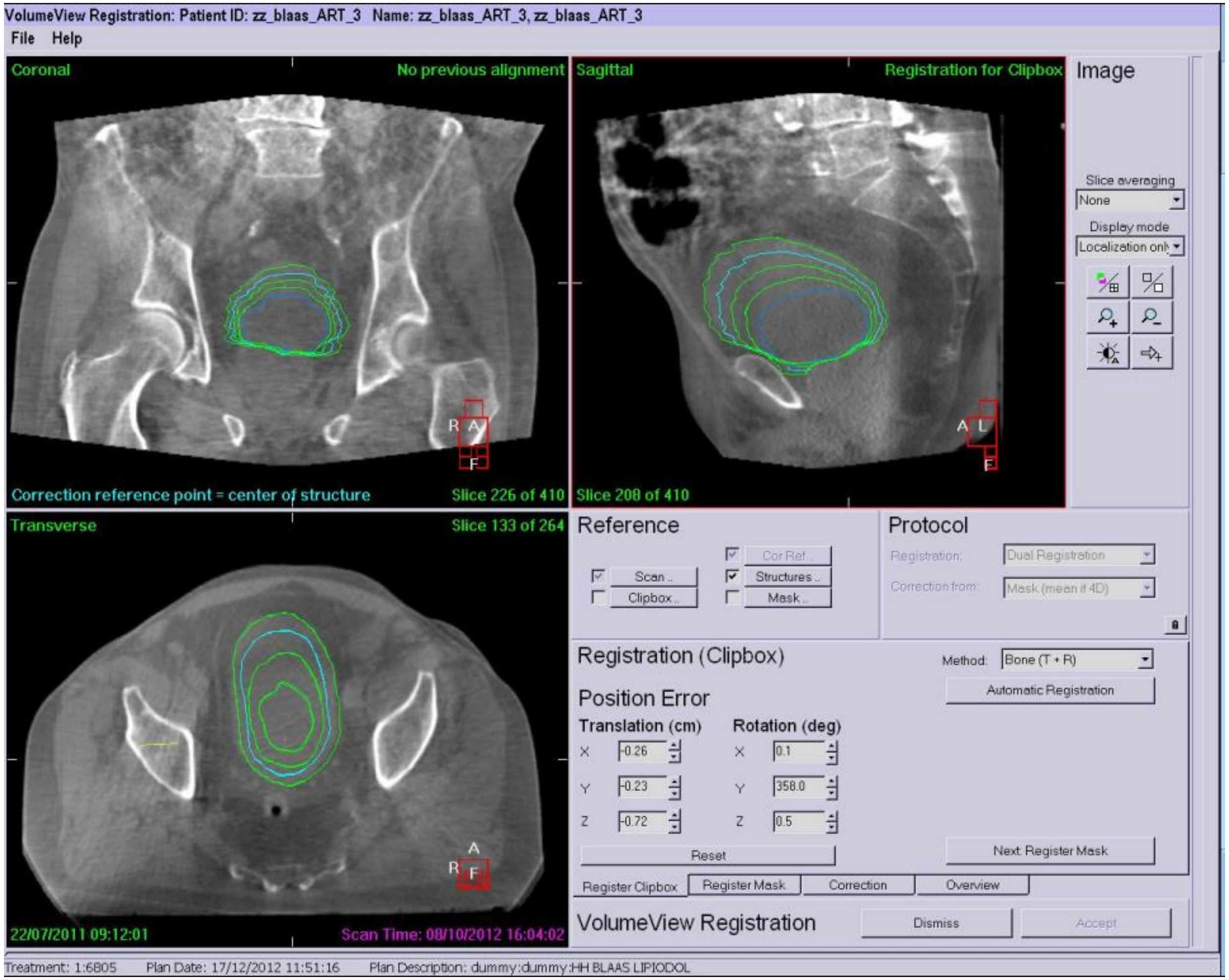
Bladder plan selection @AMC

1. Full bladder protocol
2. Bony anatomy registration for nodes
3. Selection of plan for whole bladder
4. *Optional: tweak for the high dose region*



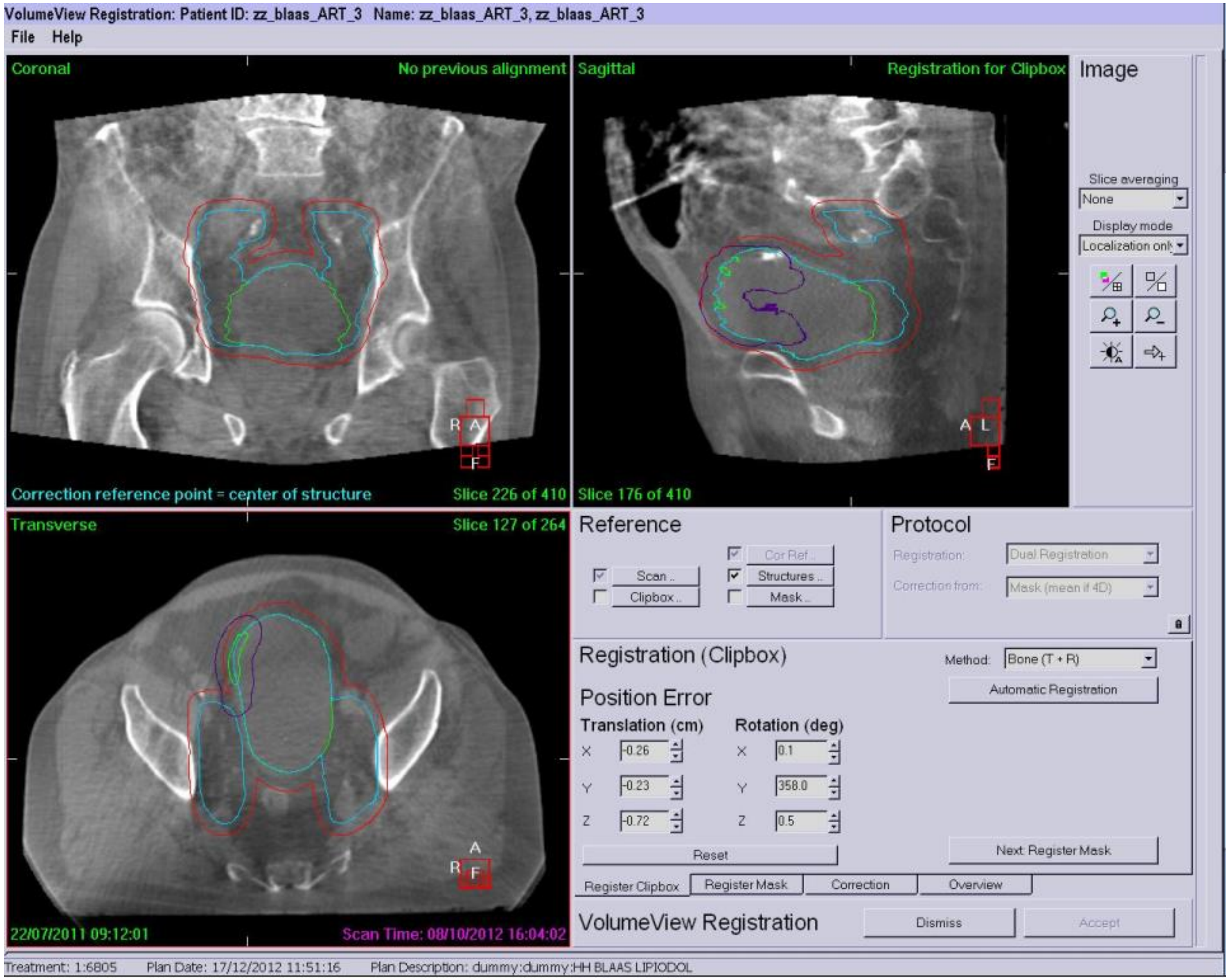
1

- Bony anatomy registration in green-purple with bone algorithme



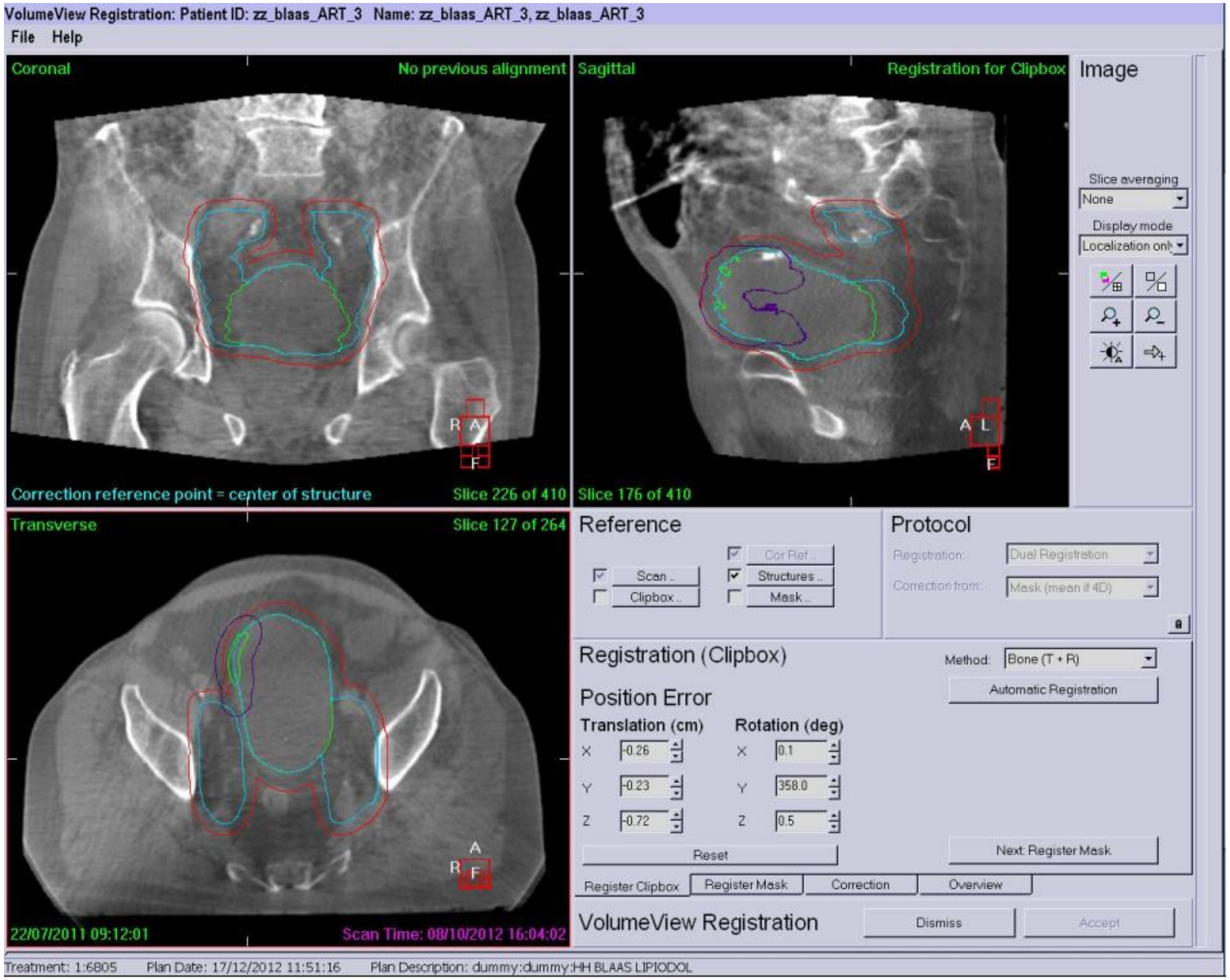
2

- Overlay of structures on the CBCT
- Do not use CT scan anymore at this point!
- Pick the plans that fits best based on bladder structure, by means of deduction



3

- Display accompanying structures
- Check target coverage in PTV, both before and after correction for rotations



4

Optional tweak: manual adjustement for the high dose region

?

Do not overstep on the tweak. Take the marginsize of the nodes into account

Live Observer Study

4 bladder patients x 3 CBCT's

1. Individual selection by turning point
2. Group discussion
3. Selection by turning point

Live plan selection

Cervix

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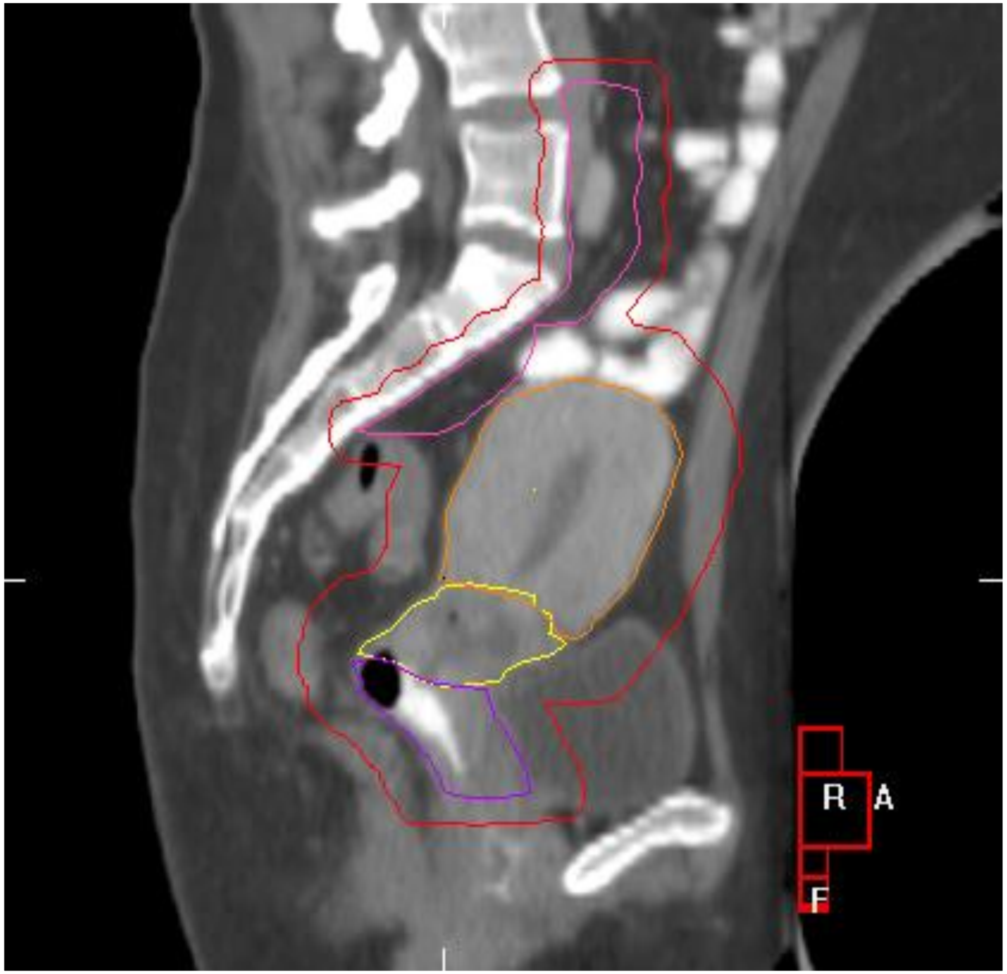
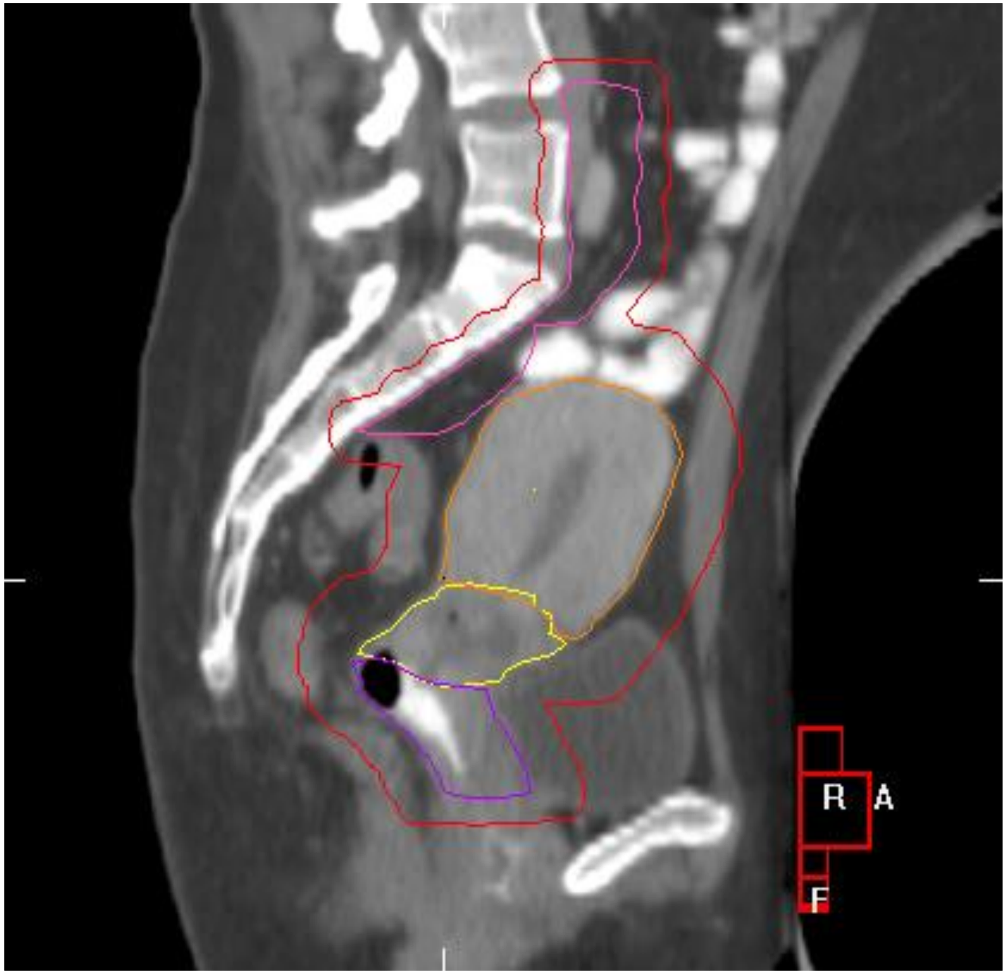


Cervix plan selection @AMC

Target volume:

- Cervix
- Uterus
- Nodal region up to L2

VMAT delivery



Cervix plan selection @AMC

1. Full bladder protocol
2. Bony anatomy registration for nodes
3. Selection of plan for cervix&uterus
4. Marker check
5. **NO tweak**

1

Bony anatomy registration in green purple overlay with bone algorithm

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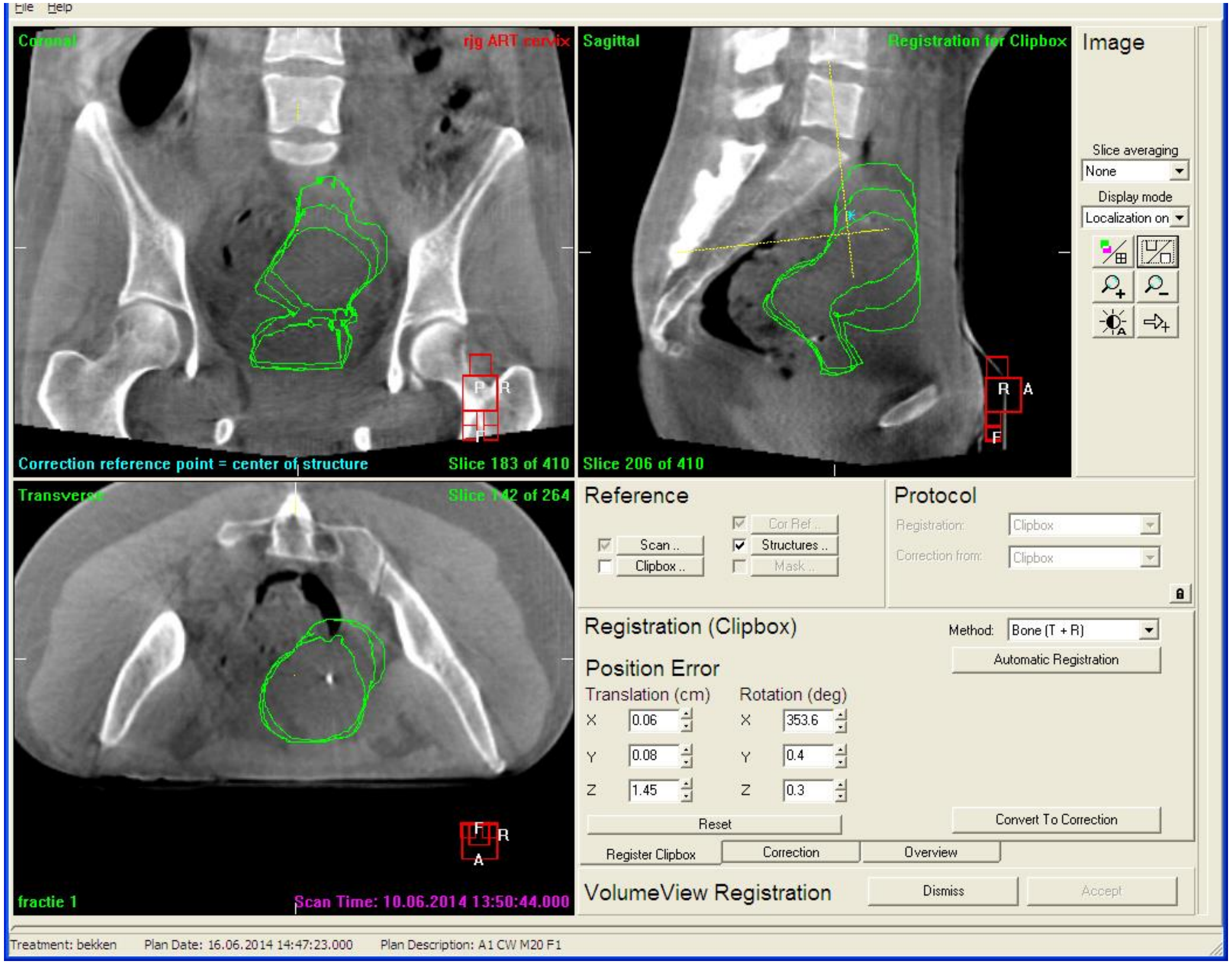
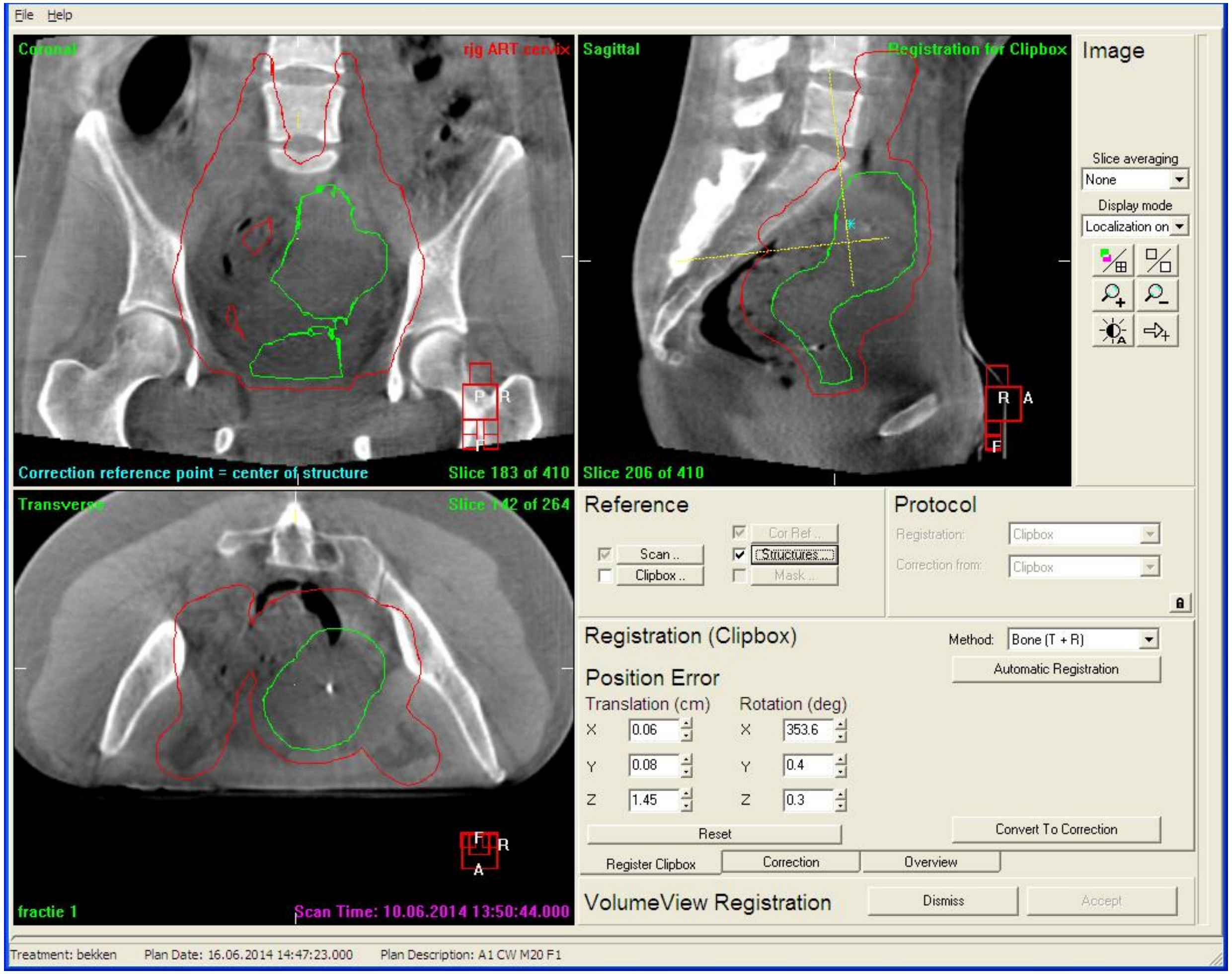


2

- Overlay of (ITV) structures on the CBCT
- Do not use CT scan anymore at this point!
- Pick the plans that fits best based on ITV structure, by means of deduction



3

- Display accompanying structures
- Check target coverage in PTV, both before and after correction for rotations
- Check markers

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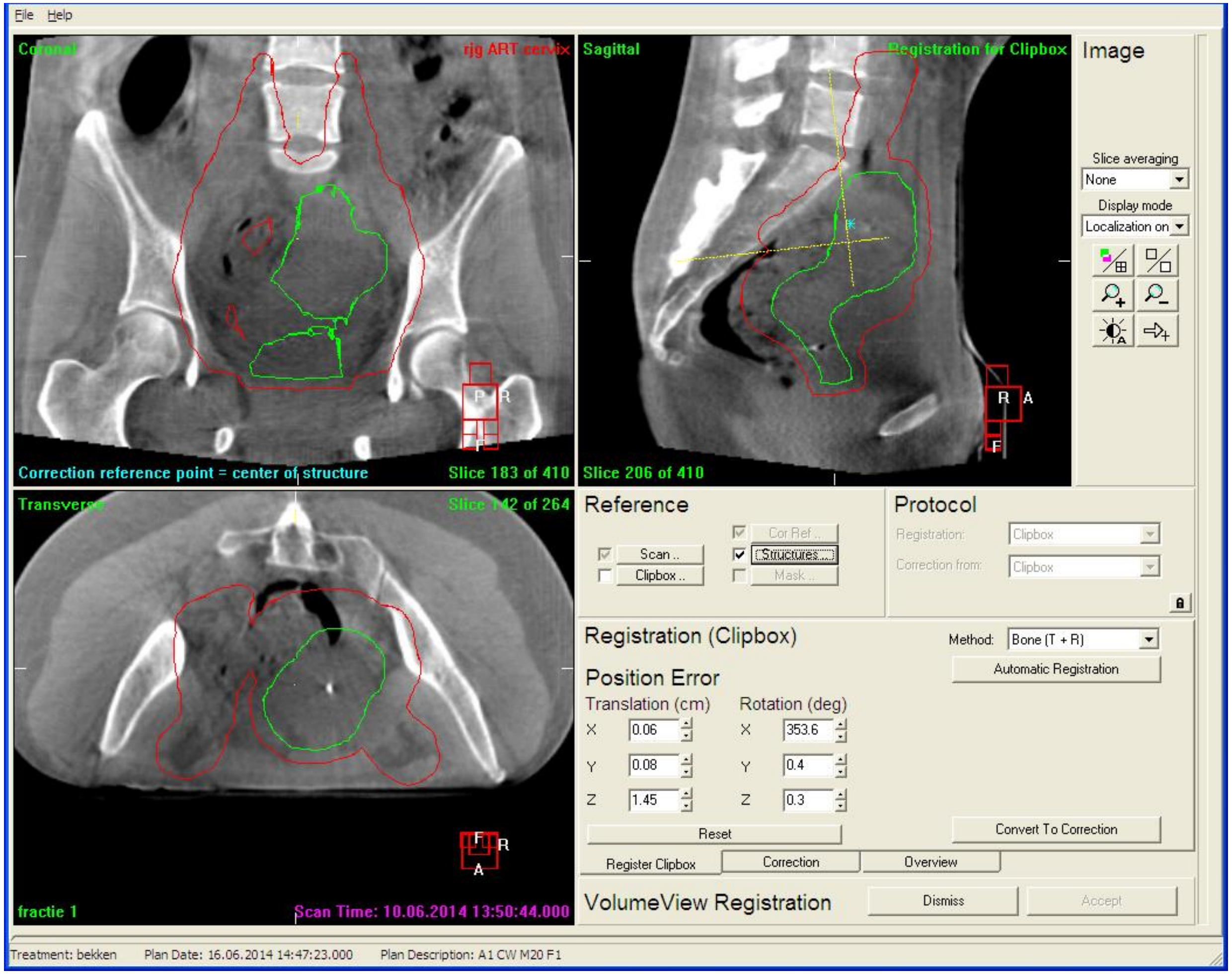

File Help
Coronal
rjg ART cervix
Correction reference point = center of structure
Slice 183 of 410
Sagittal
Registration for Clipbox
Slice 206 of 410
Image
Slice averaging
None
Display mode
Localization on
Transverse
Slice 142 of 264
fractie 1
Scan Time: 10.06.2014 13:50:44.000
Reference
Scan ..
Clipbox ..
Cor Ref ..
Structures ..
Mask ..
Protocol
Registration:
Clipbox
Correction from:
Clipbox
Registration (Clipbox)
Method:
Bone (T + R)
Automatic Registration
Position Error
Translation (cm)
X 0.06
Y 0.08
Z 1.45
Rotation (deg)
X 353.6
Y 0.4
Z 0.3
Reset
Convert To Correction
Register Clipbox
Correction
Overview
VolumeView Registration
Dismiss
Accept
Treatment: bekken
Plan Date: 16.06.2014 14:47:23.000
Plan Description: A1 CW M20 F1

4

No Tweak!!

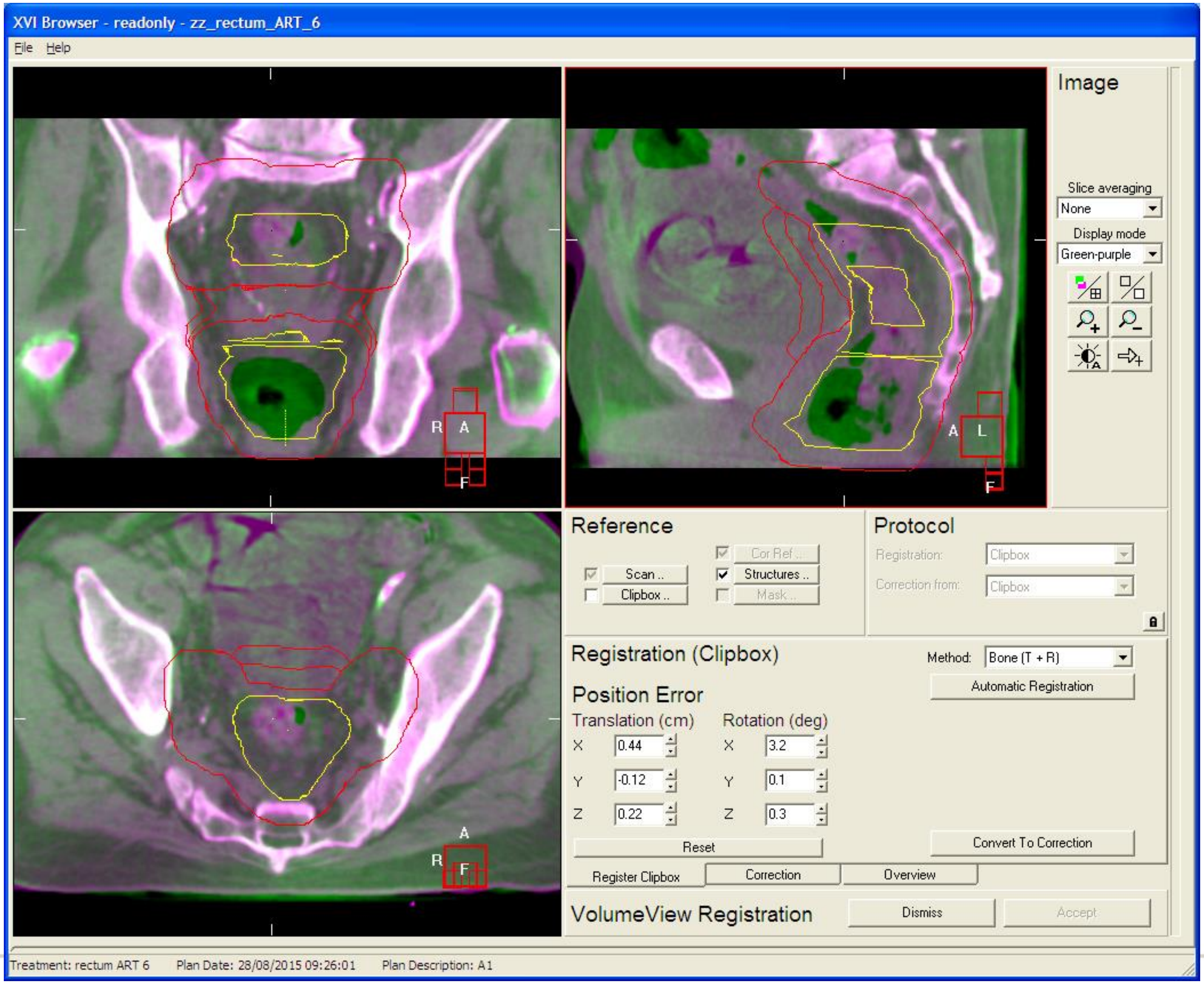
Live Observer Study

4 cervix

1. Individual selection by turning point
2. Group discussion
3. Selection by turning point

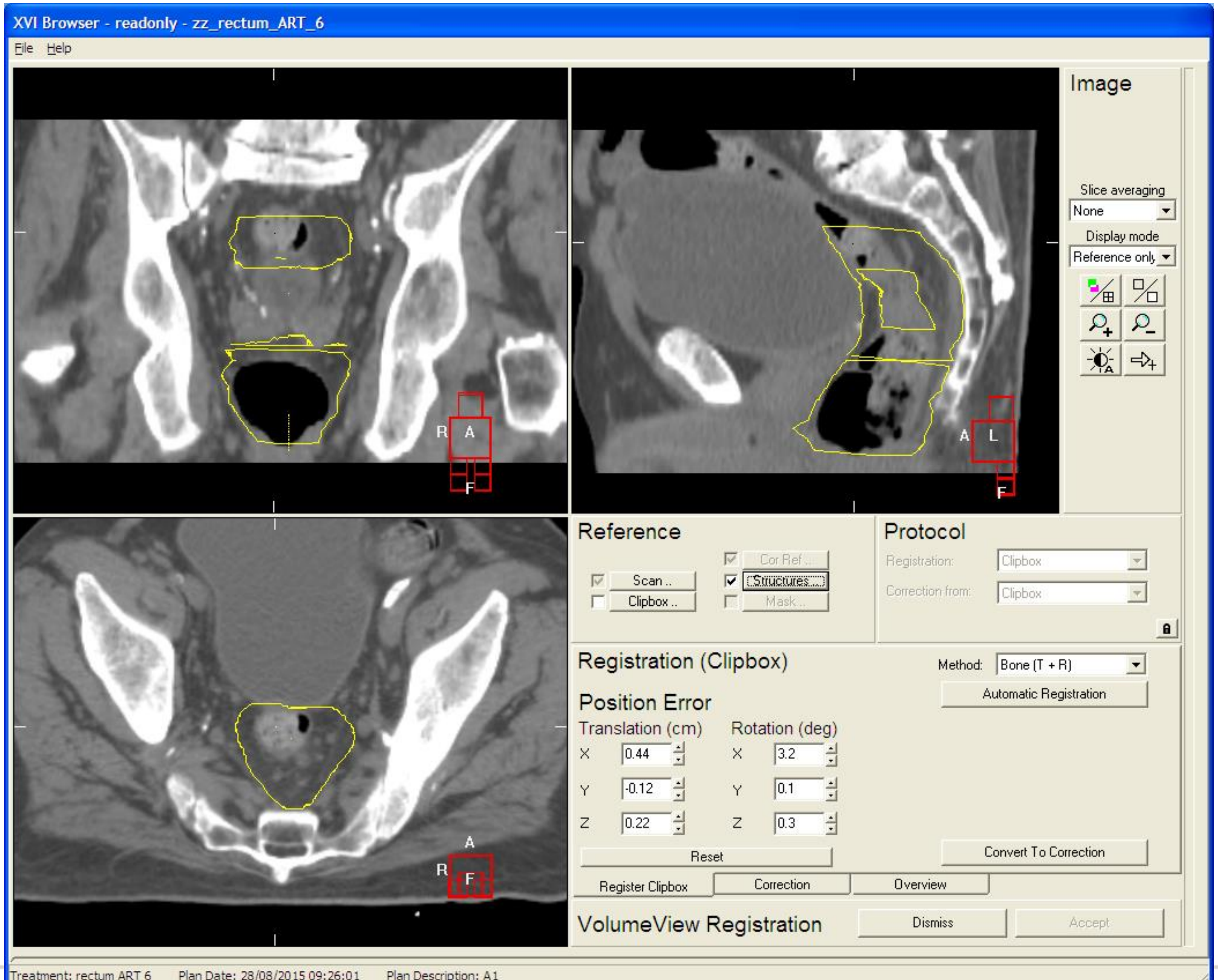
Live plan selection

Rectum



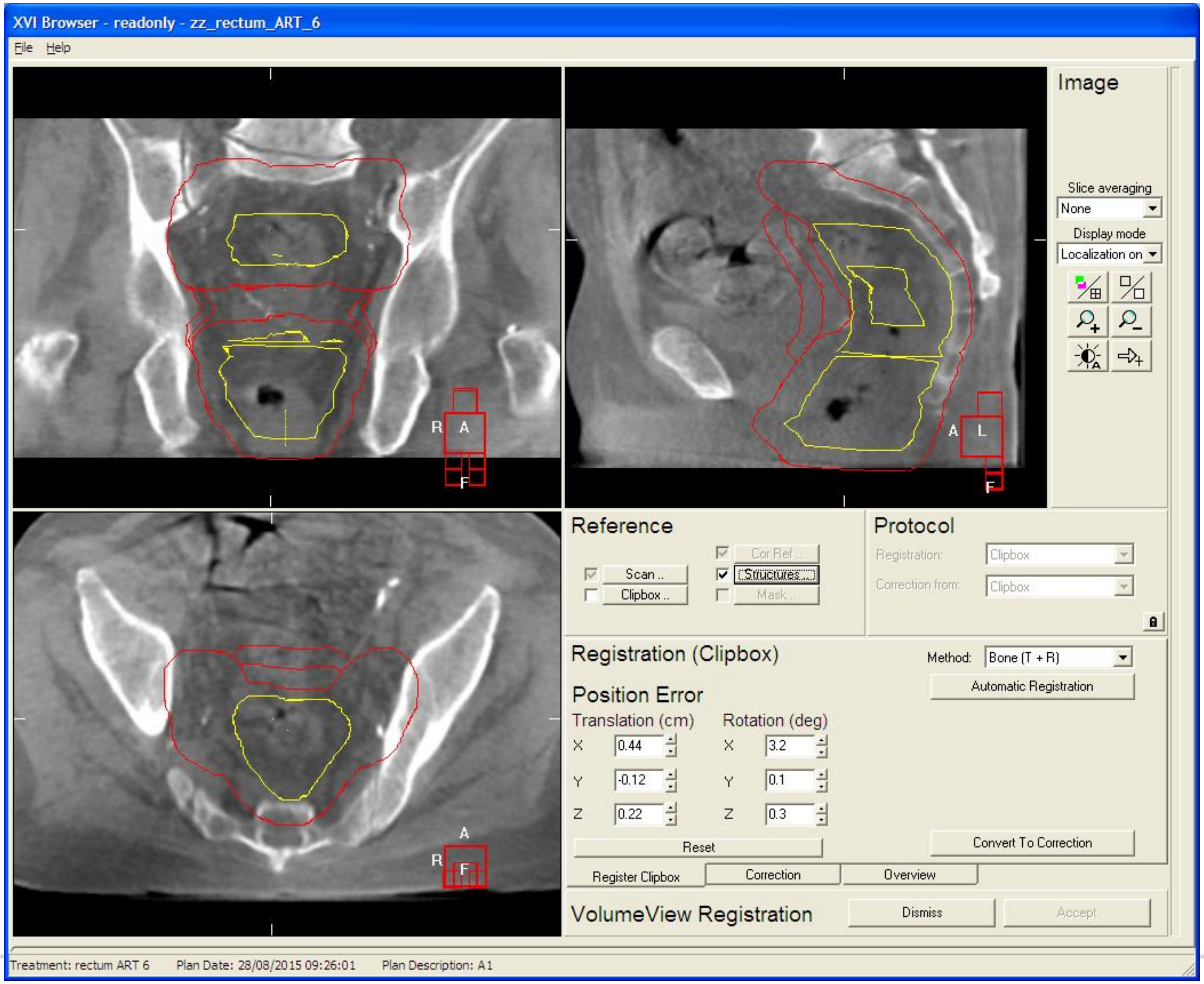
1

Bony anatomy registration (T+R)



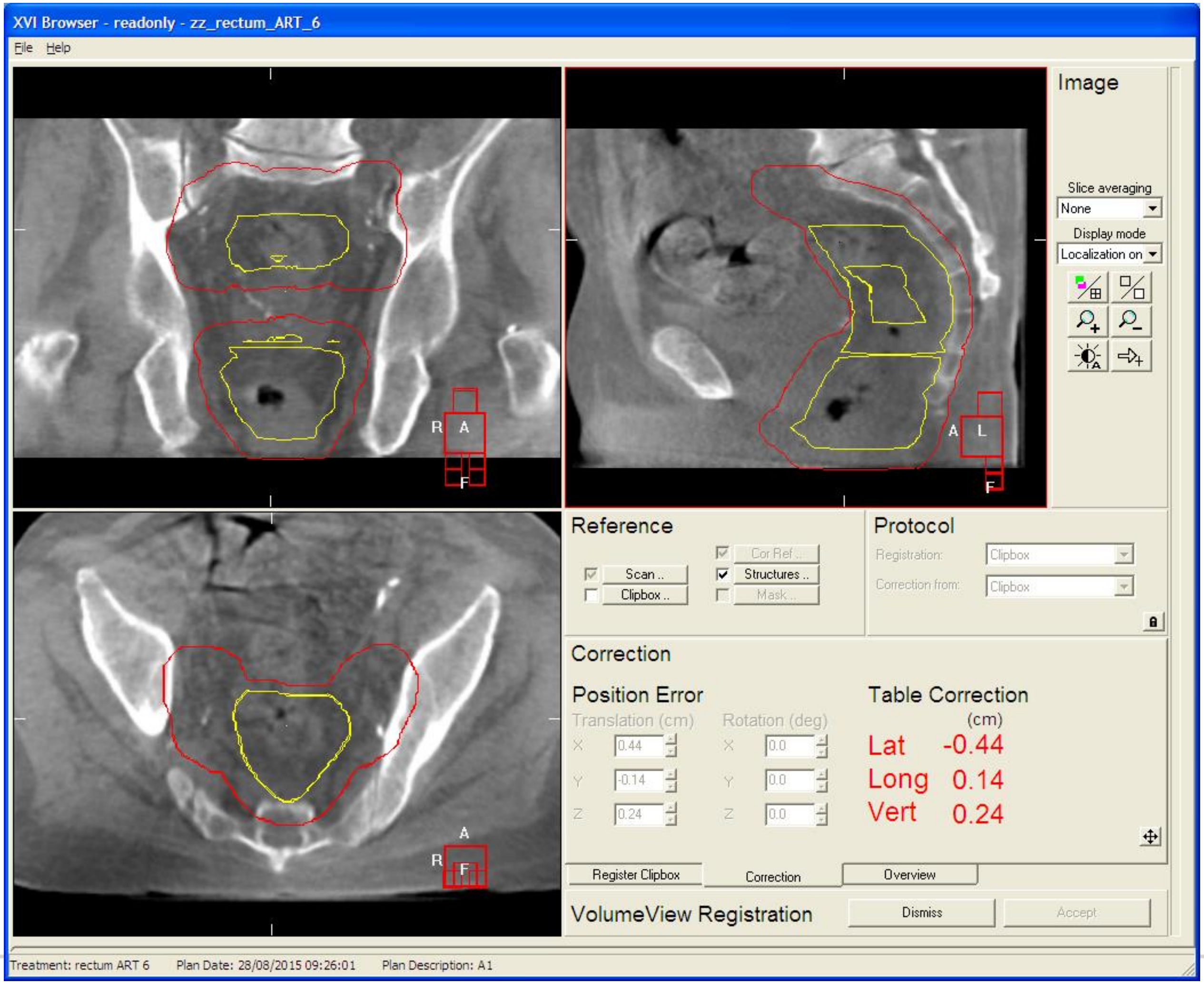
2

Inspection of delineation of upper mesorectum and lower mesorectum at reference CT scan



3

Select thigthest fitting plan (margin) based on CBCT



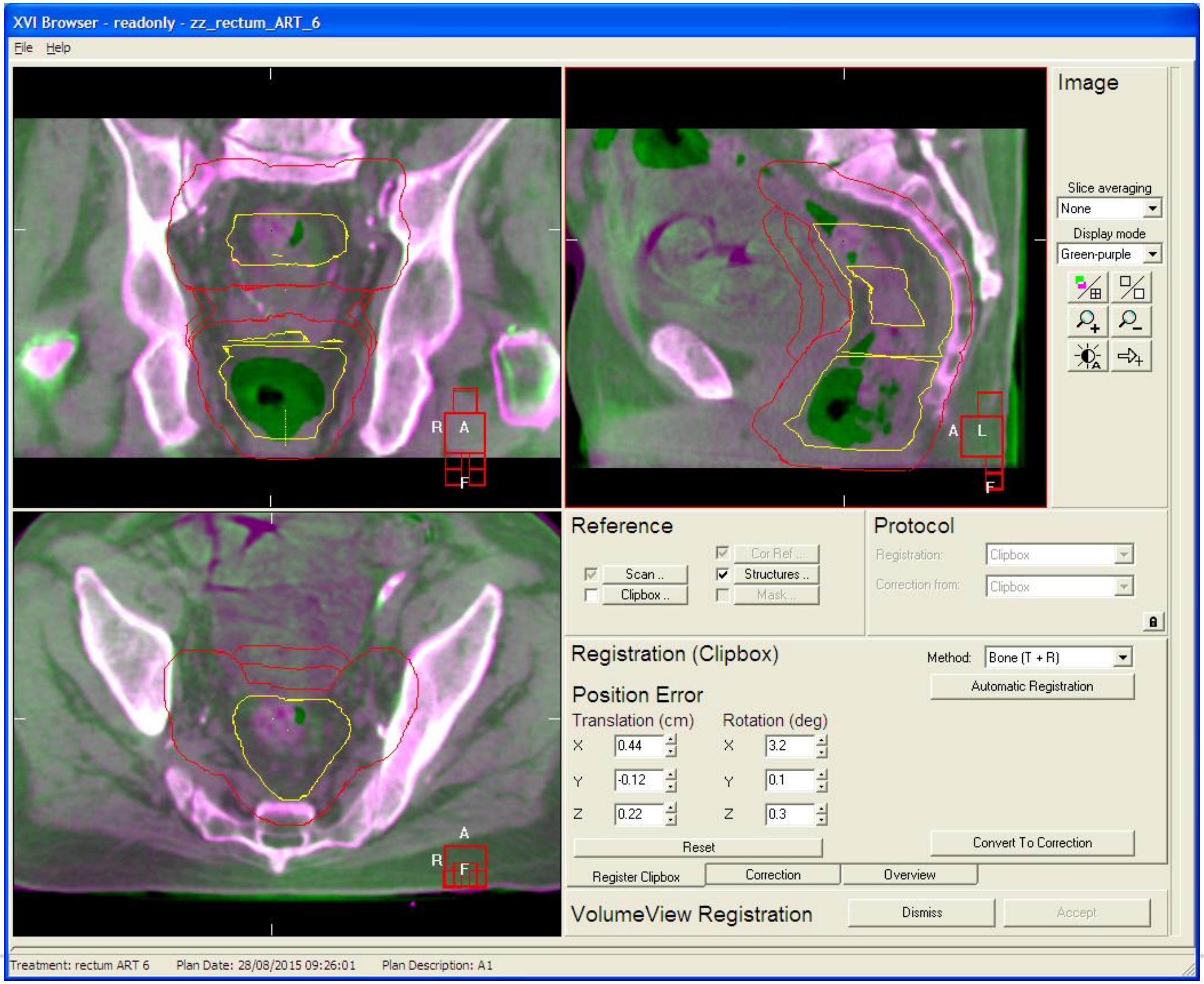
4

Check coverage again after recalculation of rotations

NO TWEAK!

Think lymfe nodes

Workflow registration and selection



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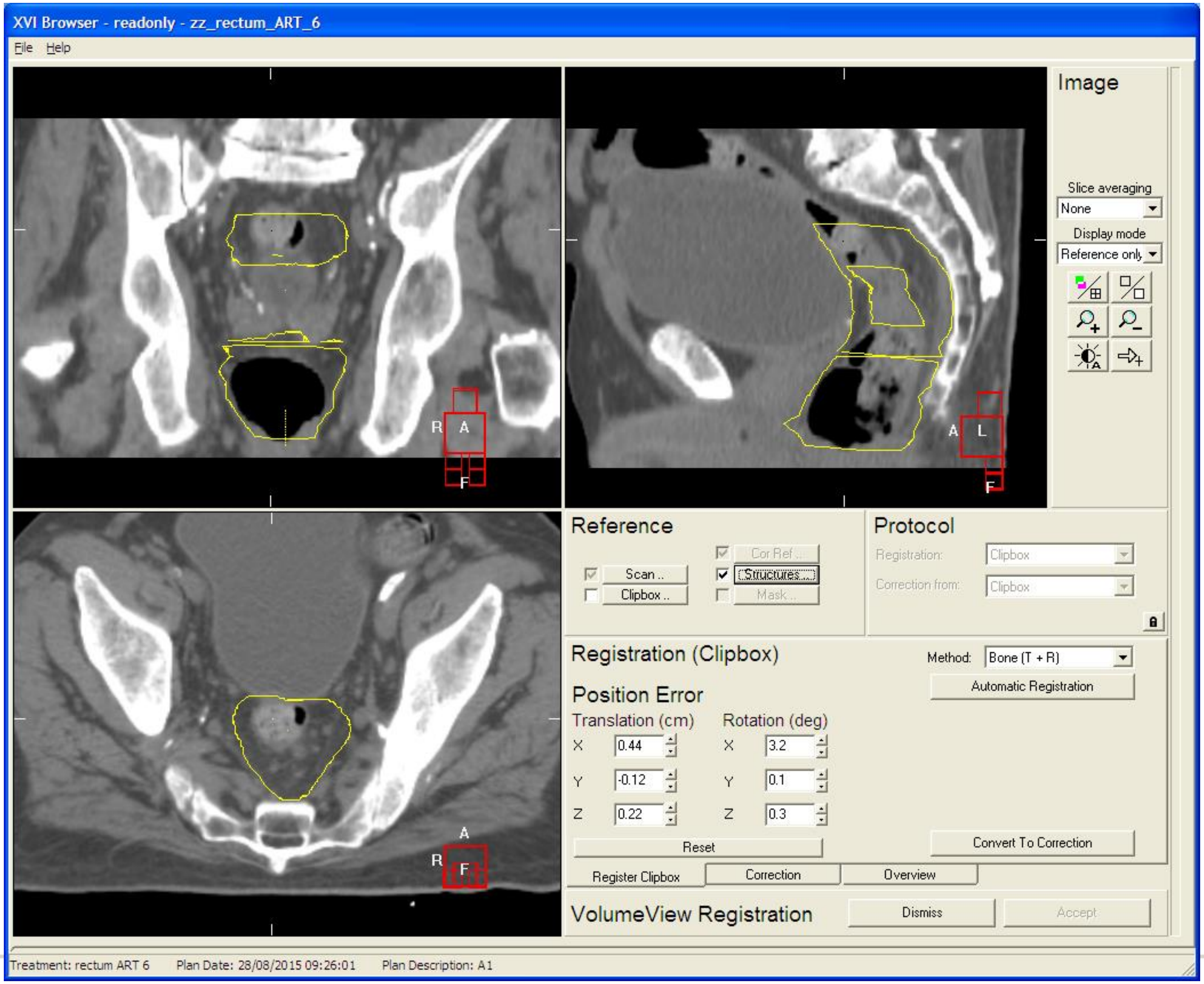
Workflow registration and selection



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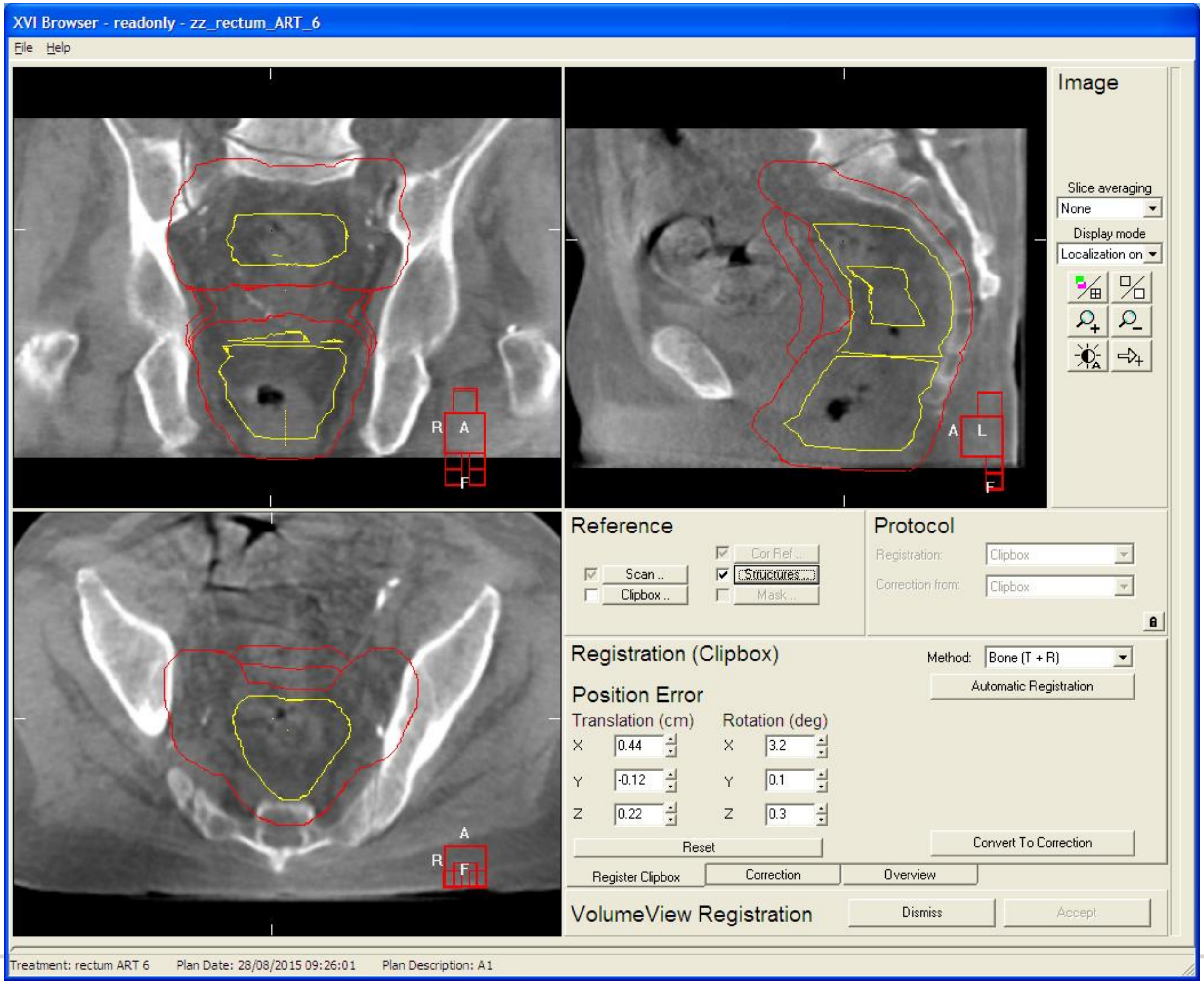

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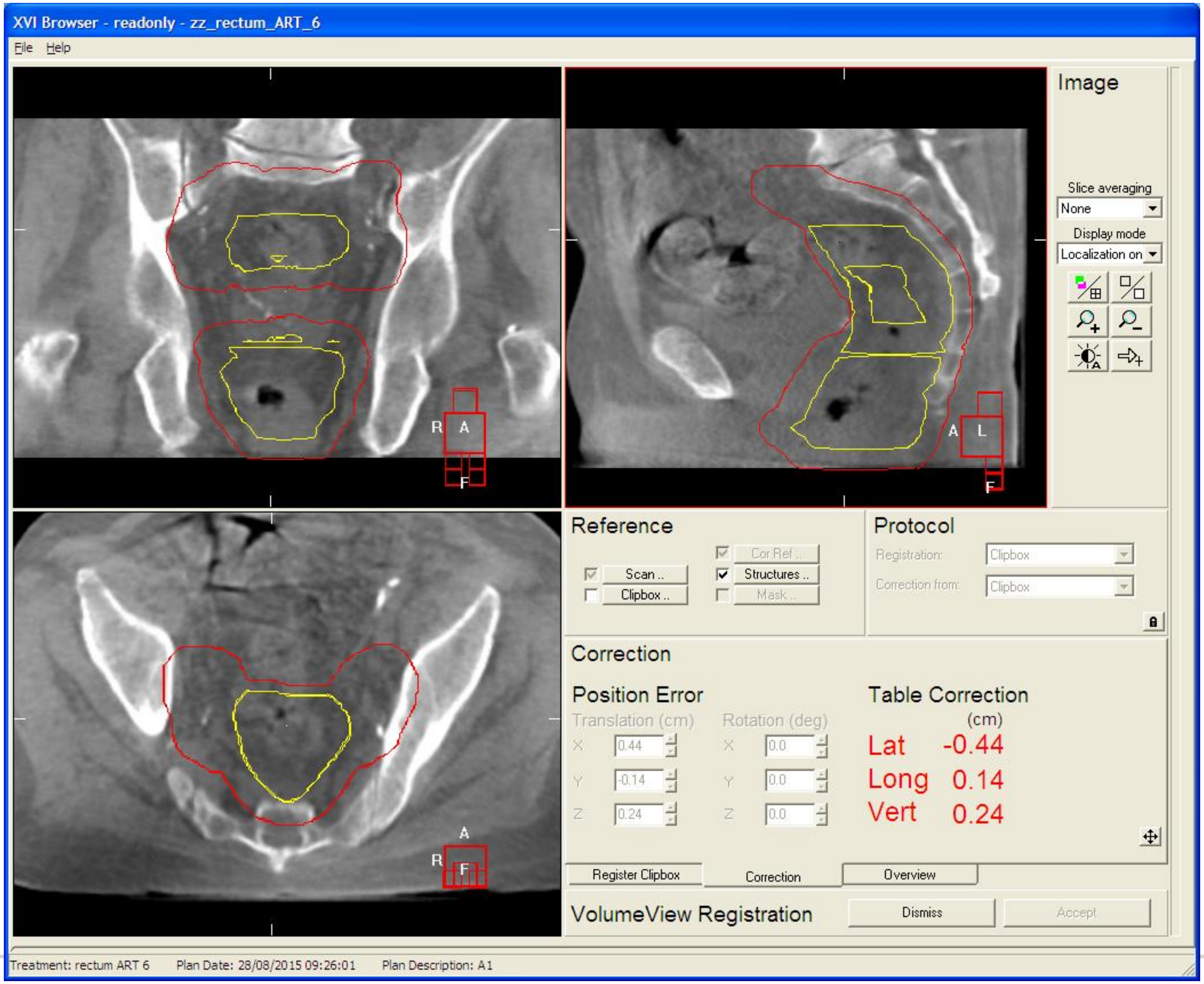

4

Check coverage again after recalculation of rotations

Prospective Adverse Event Reporting and the Role of the RTT

Liz Forde, RTT
Assistant Professor
The Discipline of Radiation Therapy
School of Medicine
Trinity College Dublin

Toxicity in Oncology

- Toxicity and tolerance differs for each organ
- Toxicity has an undeniable impact on patients psychosocial well being and quality of life
- Factors impacting on toxicity and patient tolerance:
  - Biological
  - Subjective
  - Duration of reaction
  - Response to medical intervention

Toxicity in Oncology

- Acute reactions
  - ➢ During or shortly after treatment
  - ➢ Common for epithelial tissue damage
  - ➢ Typically temporary
  - ➢ Support through the most severe phase
    - ▪ Medical intervention
  - ➢ Psychosocial
  - ➢ *Do not ignore unexpected acute toxicities*

- Late reactions
  - ➢ Months or even years following treatment
  - ➢ Too late for a change in treatment
  - ➢ Often in deeply seated organs
  - ➢ Clinical observation difficult

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Need for Recording and Reporting

- Survival and success stories frequently reported
- Adverse events and poor outcome data rarely reported

- Large variation in grading, analysing and reporting
  - ➢ Standardisation is required
  - ➢ Comparison between trials, patients groups, institutions

- More combined therapies
- More aggressive therapies
- More complex treatment regimes

} Associated with higher acute toxicity

Need for Recording and Reporting

- Routine reporting involves commitment to prospective documentation, analysis and long term follow up

- Culture of the department and education of staff
  - ➢ Radiation oncology vs. Medical oncology vs. Surgical oncology
  - ➢ Single modality vs. multi modality trials

The Four Domains of Adverse Event Reporting

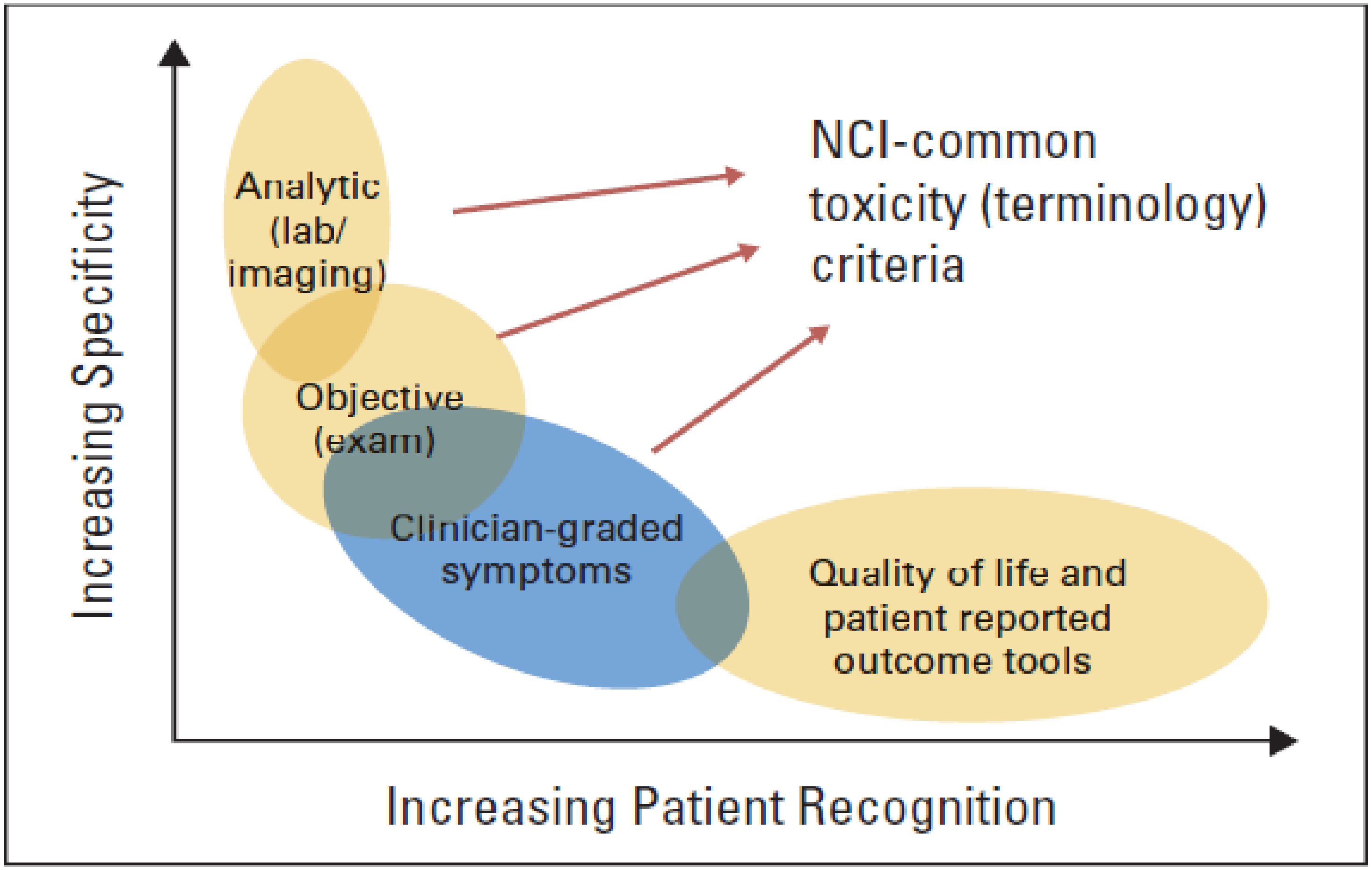

Fig 1. Adverse effects domains. NCI, National Cancer Institute. Adapted with permission.[8]

Trotti et al., Patient reported outcomes and the evolution of adverse reporting in oncology. J Clin Oncol. 2007; 25(32): 5121-5127

Assessment and Reporting of Adverse Events

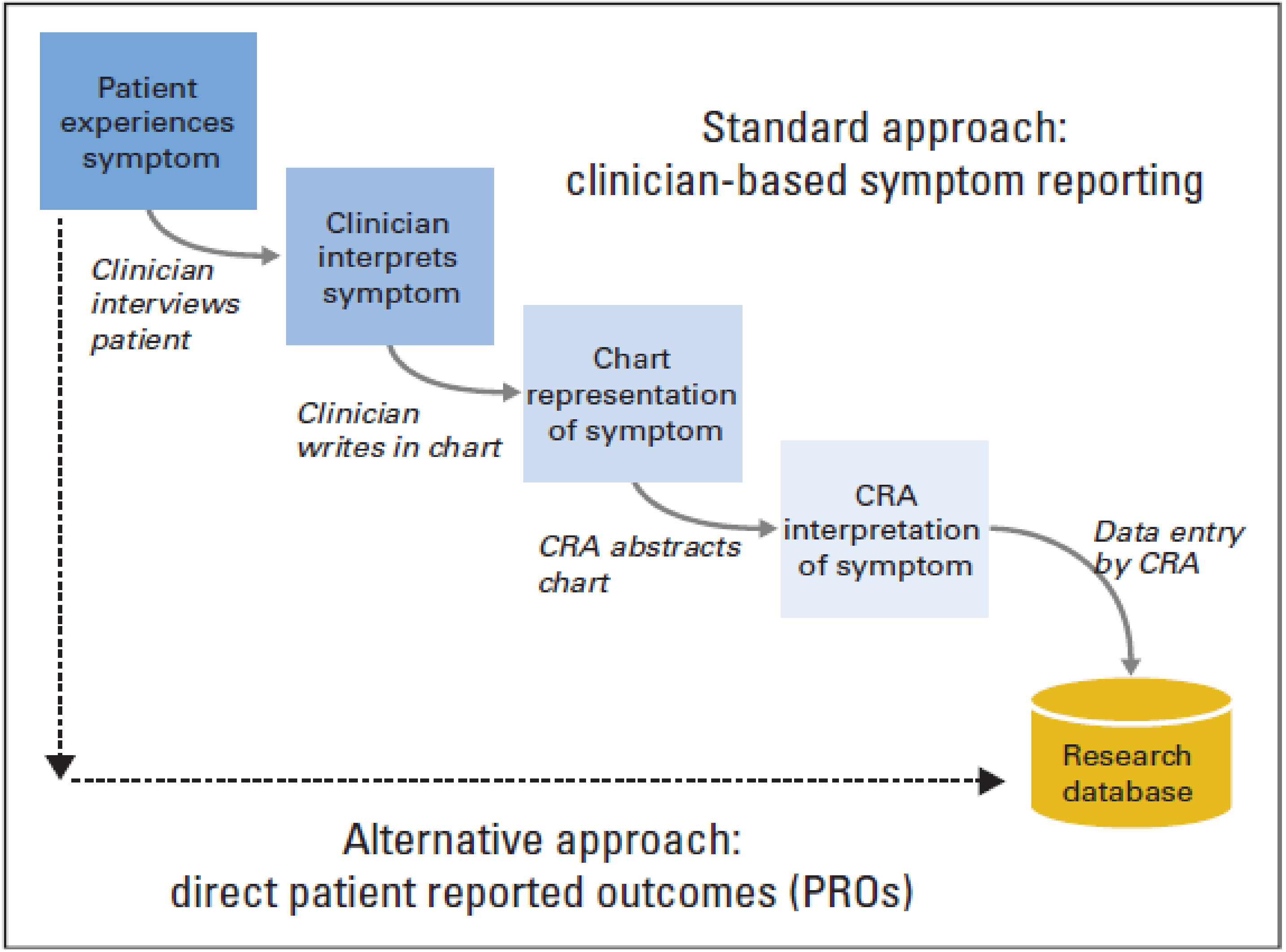

Fig 2. Flow of symptom information in cancer treatment trials. CRA, clinical research assistant. Reprinted with permission.[36]

Trotti et al., Patient reported outcomes and the evolution of adverse reporting in oncology. J Clin Oncol. 2007; 25(32): 5121-5127

Features of a Scoring System

- Specific descriptions
- Unambiguous language
- Consistency and reliability
  - Decreased inter-user variation and misinterpretation
- Grading of severity
  - Intervention required
  - Impact on QoL or daily activities

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Systems Developed

- WHO – 1979
- NCI - CTC – 1983
- RTOG – 1984
- RTOG/EORTC – 1984
- Franco-Italian Dictionary
- The Dische grading dictionary
- ***LENT-SOMA – 1995***
- CTCAE Version 3 - 2003
- CTCAE Version 4 – 2010

Chemotherapy only

Radiation Oncology, Acute Only

- All with varying degrees of content and severity of scaling

- Need for standardisation and amalgamation of acute and late effects…

LENT SOMA

- Perception of toxicity between patient and physician can be very different
  - Irreversible
  - Protracted
  - Uncontrollable
  - Social debilitating

- Combination of data from functional tests and also a ***subjective*** score

The Work of the NCI

- CTC v1.0 developed in 1983
  - Chemotherapy only
  - Acute reactions only

- CTC v2. updated in 1997
  - Intended for ***all oncology modalities***
  - >250 descriptive criteria
  - Still only addressed grading of ***acute*** toxicity

NCI - CTCAE v3.0

- 2003
- All organ systems covered with a total of 370 criteria listed
- Amalgamation of ***acute and late*** effects
- Can be applied to ***all modalities*** (Surgical, medical and radiation oncology)
- Duration and sequence of an adverse event should be recorded
- This is a "grading dictionary" not intended to assess treatment regimes or determine what is acceptable or not
  - This is still a clinical judgement of risks vs. benefits

CTCAE v4

- 2010
- Harmonise terminology with MedDRA
- Organisation of document changes
  - Version 3 was divided into categories based on either pathophysiology or anatomy
  - Version 4 is based on system organ class (SOC)
- Result: Decreased number of terms (1059 down to 790)
- FAQ document available online

Common Terminology Criteria for Adverse Events v4.0 (CTCAE)

Publish Date: May 28, 2009

Quick Reference

The NCI Common Terminology Criteria for Adverse Events is a descriptive terminology which can be utilized for Adverse Event (AE) reporting. A grading (severity) scale is provided for each AE term.

Components and Organization

SOC

System Organ Class, the highest level of the MedDRA hierarchy, is identified by anatomical or physiological system, etiology, or purpose (e.g., SOC Investigations for laboratory test results). CTCAE terms are grouped by MedDRA Primary SOCs. Within each SOC, AEs are listed and accompanied by descriptions of severity (Grade).

CTCAE Terms

An Adverse Event (AE) is any unfavorable and unintended sign (including an abnormal laboratory finding), symptom, or disease temporally associated with the use of a medical treatment or procedure that may or may *not* be considered related to the medical treatment or procedure. An AE is a term that is a unique representation of a specific event used for medical documentation and scientific analyses. Each CTCAE v4.0 term is a MedDRA LLT (Lowest Level Term).

Definitions

A brief definition is provided to clarify the meaning of each AE term.

Grades

Grade refers to the severity of the AE. The CTCAE displays Grades 1 through 5 with unique clinical descriptions of severity for each AE based on this general guideline:

Grade 1	Mild; asymptomatic or mild symptoms; clinical or diagnostic observations only; intervention not indicated.
Grade 2	Moderate; minimal, local or noninvasive intervention indicated; limiting age-appropriate instrumental ADL*.
Grade 3	Severe or medically significant but not immediately life-threatening; hospitalization or prolongation of hospitalization indicated; disabling; limiting self care ADL**.
Grade 4	Life-threatening consequences; urgent intervention indicated.
Grade 5	Death related to AE.

A Semi-colon indicates 'or' within the description of the grade.

Not all Grades are appropriate for all AEs. Therefore, some AEs are listed with fewer than five options for Grade selection.

Grade 5

Grade 5 (Death) is not appropriate for some AEs and therefore is not an option.

Activities of Daily Living (ADL)

*Instrumental ADL refer to preparing meals, shopping for groceries or clothes, using the telephone, managing money, etc.

**Self care ADL refer to bathing, dressing and undressing, feeding self, using the toilet, taking medications, and not bedridden.

CTCAE v4

- Example of AEs potentially experienced by prostate radiotherapy patients

	Grade 1	Grade 2	Grade 3	Grade 4	Grade
Diarrhea	Increase of <4 stools per day over baseline; mild increase in ostomy output compared to baseline	Increase of 4 - 6 stools per day over baseline; moderate increase in ostomy output compared to baseline	Increase of >=7 stools per day over baseline; incontinence; hospitalization indicated; severe increase in ostomy output compared to baseline; limiting self care ADL	Life-threatening consequences; urgent intervention indicated	Death
Definition: A disorder characterized by frequent and watery bowel movements.					
Proctitis	Rectal discomfort, intervention not indicated	Symptoms (e.g., rectal discomfort, passing blood or mucus); medical intervention indicated; limiting instrumental ADL	Severe symptoms; fecal urgency or stool incontinence; limiting self care ADL	Life-threatening consequences; urgent intervention indicated	Death
Definition: A disorder characterized by inflammation of the rectum.					
Fatigue	Fatigue relieved by rest	Fatigue not relieved by rest; limiting instrumental ADL	Fatigue not relieved by rest, limiting self care ADL	-	-
Definition: A disorder characterized by a state of generalized weakness with a pronounced inability to summon sufficient energy to accomplish daily activities.					

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Even with advances in toxicity reporting using CTCAE variability still remains

Patient Reported Outcomes (PRO)

- HCP generally ***underestimate*** side effect presentation, severity and duration compared with patients

- Agreement is generally closer for observable side effects than for subjective ones
  - ➢ E.g. diarrhoea is observable and fatigue is subjective

- PROs cover the ***subjective*** domain
  - ➢ E.g. Pain

- Issues re literacy
  - ➢ Questionnaires to guide a consult is not considered a true PRO as there is still some level of interpretation and collection by someone other than the patient

PROs

- The NCI have since developed a web based PRO for the CTCAE
- 81 symptoms have been identified for inclusion in a PRO
- 126 questions assess the different attributes of these symptoms
- Language has been adjusted for patients
  - Myalgia is "translated" as aching muscles

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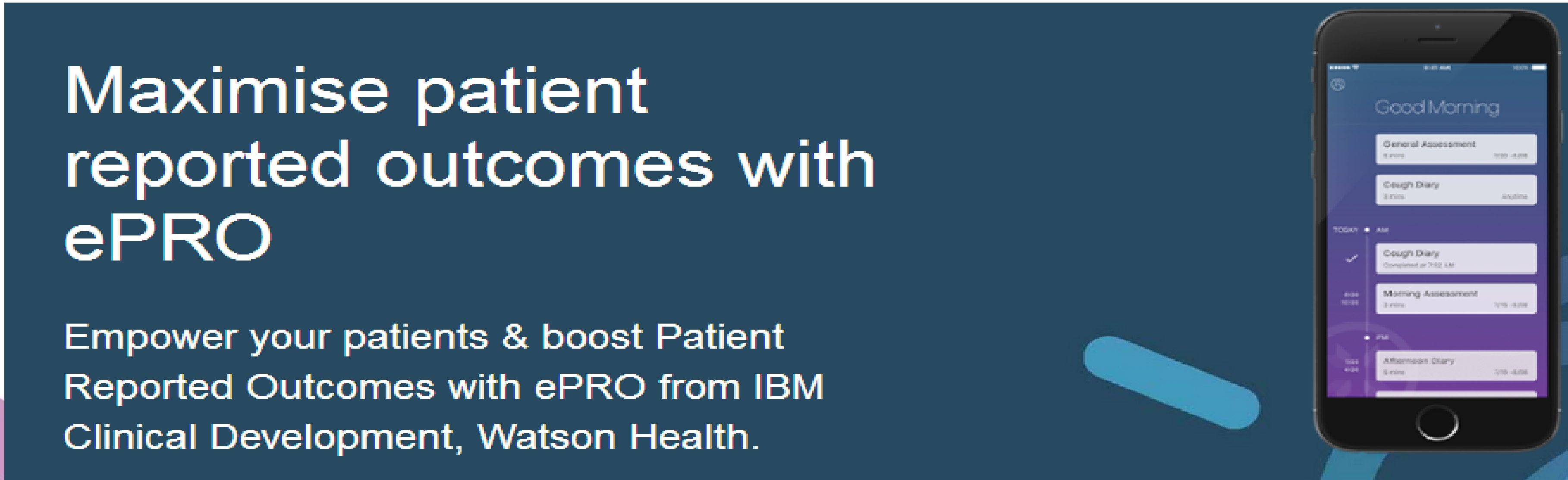
ePRO

- Basche presented at ASCO in June 2017
  - ➢ >700 patients treated at MSKCC
  - ➢ Breast and lung
- "Real time" reporting of side effects
- Web based PRO for chemo patients
- Works on smart phones
- Nurses get sent an email when side effects worsen



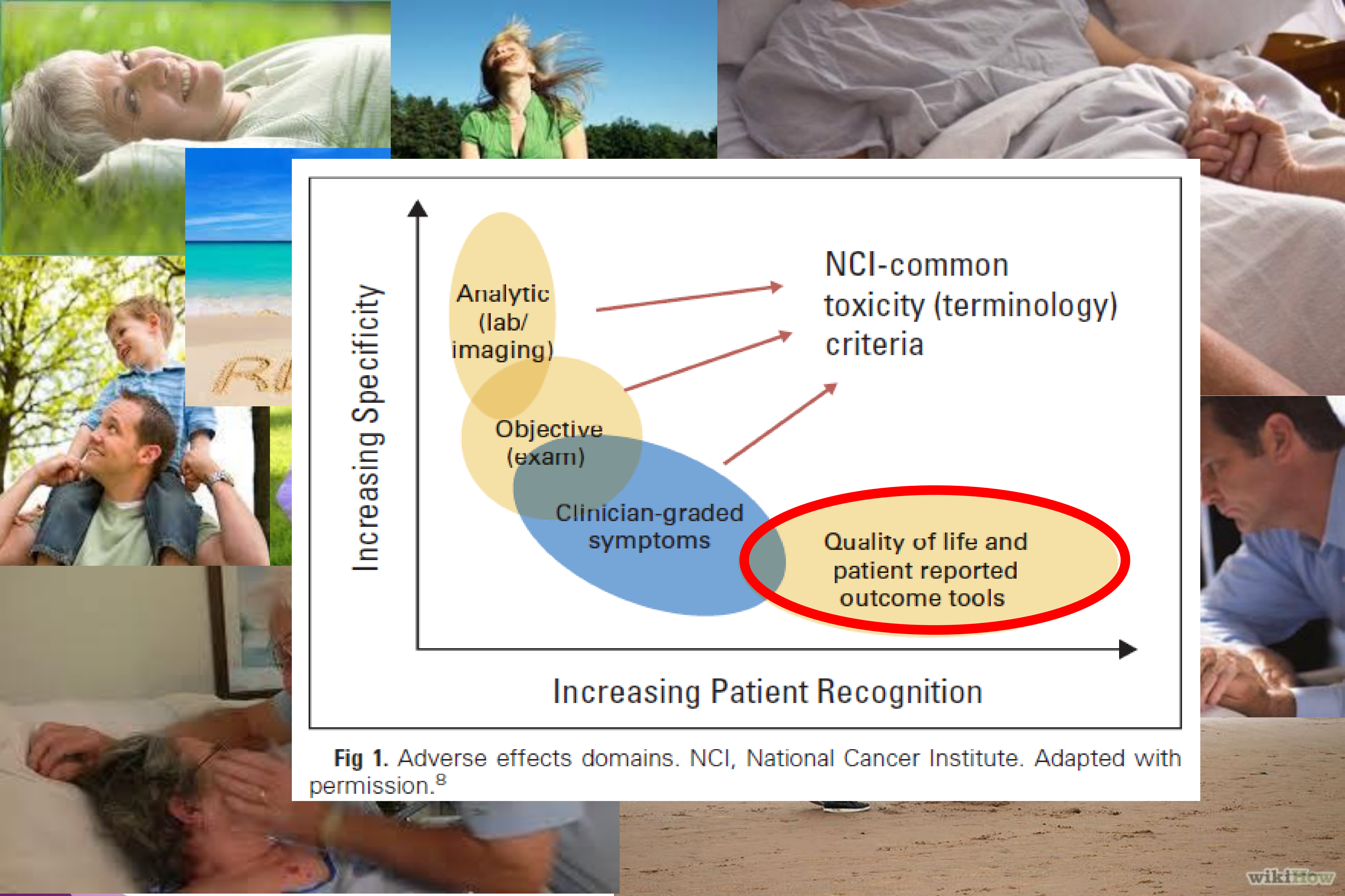


Fig 1. Adverse effects domains. NCI, National Cancer Institute. Adapted with permission.[8]

Quote read directly from: *Pavy et al., Late effects toxicity scoring: the SOMA scale. Radiother Oncol. 1995;*

“To the clinician and the biologist the preservation of functions that are essential to life would seem of paramount importance. But to the patient, the obligation to live a long and painful existence may be worse than death itself. The economic consequence of being unable to work, and even more, being utterly dependent on others for day to day activities like feeding, dressing and washing are not easy for a third person to appreciate. Similarly facial disfigurement and anal or bladder incontinence may impose such social consequences on the patient that may become effectively housebound even though their other vital organs function, motor activities and pain threshold are virtually unimpaired.”

Pavy et al., Late effects toxicity scoring: the SOMA scale. Radiother Oncol. 1995; 35:11-15

Quality of Life Assessment

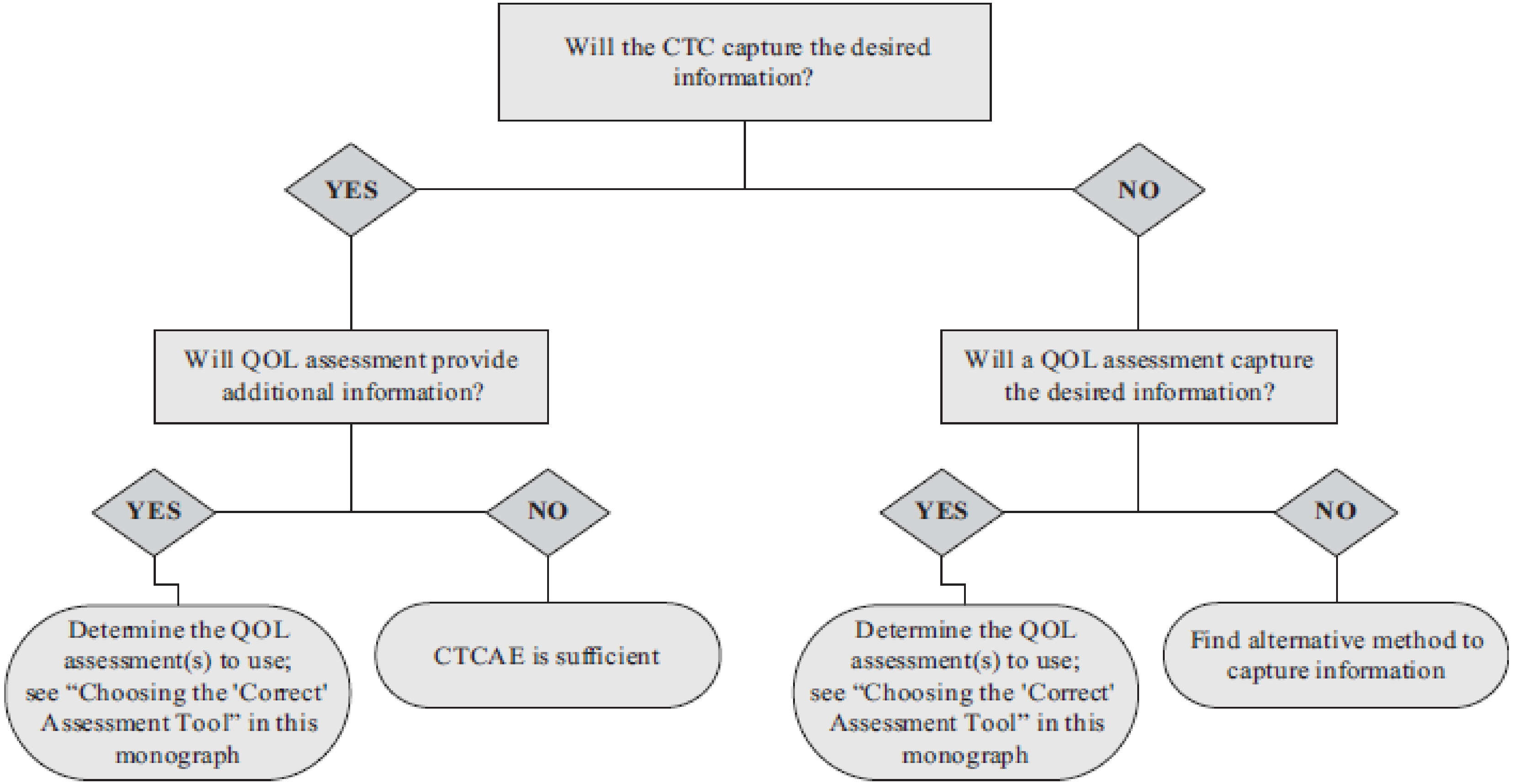


FIG 2. Flow diagram to determine the method for adverse event and QOL data collection.

Huschka M and Burger K. Does QOL provide the same information as toxicity data? Curr Probl Cancer. 2006; 30(6): 244-254

QoL Assessment

- QoL is ***subjective*** and depends on patients ability to adapt to a certain extent
  - ➢ QoL measures not the AE itself but the how it impacts on daily activities

- QoL includes psychosocial support networks and patient’s spirituality

- QoL and AE reporting are complimentary to each other

- This combination strengthens the patient physician relationship
  - ➢ Recognition of different goals
  - ➢ Overall survival, but at what cost

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QoL Assessment

- QoL assessment also lacks consistency between trials, countries, departments and patient groups

- Assessment Scales available
  - The Symptom Distress Scale
  - The Lung Cancer Symptom Scale
  - Functional Assessment of Chronic Illness Therapy – Diarrhoea
  - The International Prostate Symptom Score
    - 8 questions includes 1 QoL question
  - The Expanded Prostate Cancer Index Composite (EPIC)
    - Urinary
    - Bowel
    - Sexual function
    - Hormonal changes

EORTC Quality of Life

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1 2 3 4 5

QUESTIONNAIRES

The EORTC Quality of Life questionnaires are developed to assess the quality of life of cancer patients.

The EORTC QLQ-C30 assesses the quality of life of cancer patients. It has been translated and validated into 81 languages and is used in more than 3,000 studies worldwide. Various modules have been developed for disease specific treatement measurements.

- EORTC QLQ-C30
- EORTC CAT
- EORTC QLQ-C15-PAL
- EORTC IN-PATSAT32
- MODULES Specific Diseases

LATEST NEWS

03/10/2013

Quality of Life Department 20 Year Anniversary

13/09/2013

EORTC QLQ-CML24 has just been published in "Quality of Life Research"

EVENTS

12/09/2013

Autumn 2013 Quality of Life Group Meeting

Canterbury, UK

24/04/2014

QoL Assessment

- QLQ - C30
- Current version = version 3
- Translated into 81 languages
- 3000 studies internationally

- Disease specific modules also available for use:
  - Breast, Lung, Head & Neck, Oesophageal, Ovarian, Gastric, Cervical cancer, Multiple Myeloma, Oesophago-Gastric, Prostate, Colorectal Liver Metastases, Colorectal and Brain

During the past week:	Not at All	A Little	Quite a Bit	Ve Mu
17. Have you had diarrhea?	1	2	3	4
18. Were you tired?	1	2	3	4
19. Did pain interfere with your daily activities?	1	2	3	4
20. Have you had difficulty in concentrating on things, like reading a newspaper or watching television?	1	2	3	4
21. Did you feel tense?	1	2	3	4
22. Did you worry?	1	2	3	4
23. Did you feel irritable?	1	2	3	4
24. Did you feel depressed?	1	2	3	4
25. Have you had difficulty remembering things?	1	2	3	4
26. Has your physical condition or medical treatment interfered with your family life?	1	2	3	4
27. Has your physical condition or medical treatment interfered with your social activities?	1	2	3	4
28. Has your physical condition or medical treatment				

Some Limitations of Scoring Systems in General

- Inconsistencies in the timing of data recording
- Time consuming and resource intensive data collection
- Transfer of information and data collection
  - Interpretation of information from patient to clinician
  - Manually entered into database
- Underreporting of lower grades (Grade 1 and Grade 2)

Is There a Role for the RTT?

Treatment Review Clinics

- Clinical examination
- Side effects are explained and assessed
- Medication or intervention may be required
- Nutritional advice
- CAM advice
- Psycho social issues are addressed
- Documentation of intervention and progress
- Unrelated medical advice
- Quality assurance for the progression of treatment
- Logistical information

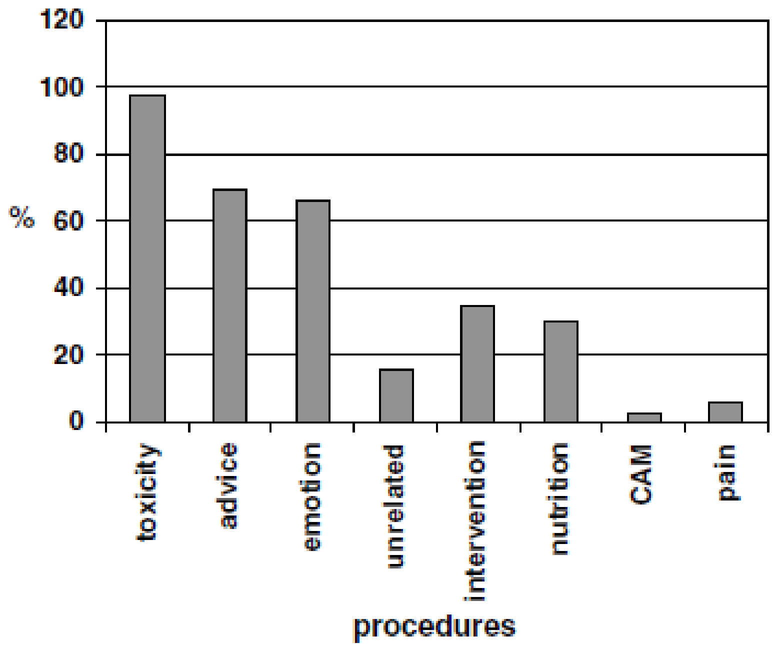

Fig. I. Frequency of procedures observed during treatment reviews. Toxicity, toxicity scoring indicated; Advice, advice on side effects; Emotion, emotional support given in terms of assurance and information given; Unrelated, unrelated medical problems addressed; Intervention, medical intervention given in the form of drug prescription, liaison with other physicians, ordering of wound dressing, or any other investigations; Nutrition, nutritional advice given; CAM, complementary and alternative medicine addressed; Pain, pain score taken.

Shi et al., 2009

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Table I
Medical intervention rates versus treatment site observed in Phase 2

Treatment site	Breast	Brain	H & N	Thorax	Pelvis	Other	Total	Pearson's Chi-square
Number (% within site)	11 (19%)	6 (54.5%)	13 (40.6%)	8 (38.1%)	15 (65.2%)	3 (20%)	56 (35%)	$P = 0.001$

Shi et al., 2009

Table 1. Breakdown of treatment review clinics requiring medical intervention (MI) and no MI according to the site of the cancer being treated.

Treatment site	MI required *n* (%)	No MI required *n* (%)	Total clinics *n* (%)
Head and neck	41 (93)	3 (7)	44 (22)
Prostate	11 (28)	29 (73)	40 (20)
Chest	18 (78)	5 (22)	23 (12)
Rectum	13 (59)	9 (41)	22 (11)
Breast	7 (33)	14 (67)	21 (11)
Brain	8 (73)	3 (27)	11 (6)
Gynaecological	10 (91)	1 (9)	11 (6)
Bladder	3 (33)	6 (67)	9 (5)
Superficial	2 (33)	4 (67)	6 (3)
Bone metastases	2 (40)	3 (60)	5 (3)
Pelvis	2 (50)	2 (50)	4 (2)
Abdomen	1 (50)	1 (50)	2 (1)
Extremity	0 (0)	2 (100)	2 (1)
Total clinics	118 (59)	82 (41)	200 (100)

As an initial step limit RT lead review to sites of low MI

Monk et al., 2013

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Table III

ROs' and RTTs' concerns with regards to RTT-led treatment reviews

ROs' concerns	RTTs' concerns
(1) Training [9]	(1) Medico-legal responsibility [21]
(2) Scope of practice – RTTs must know when to refer to ROs [7]	(2) Training [18]
(3) Medico-legal responsibility [5]	(3) Resource, time and manpower constraints [16]
(4) Resource, time and manpower constraints [4]	(4) Remuneration [14]
(5) Patients' perspective [2]	(5) Support from ROs and management [14]
(6) Compromise in RTT work performance due to diversification of role [1]	(6) Patients' perspective [13]
(7) Overconfidence of RTTs [1]	(7) Increase workload for RTTs [12]
	(8) Lack of licensing – prescription, decision making, recognition for leading reviews [6]
	(9) Sensitivities of job overlap with nurses and ROs [5]

Shi et al., 2009

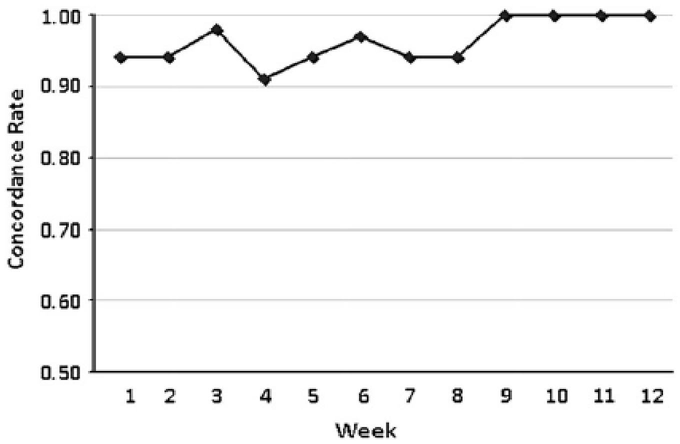

Figure 2. Average weekly concordance rates between the clinical specialist radiation therapist and radiation oncologist.

Lee et al., 2012

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Impact of This Approach?

For the *Individual*?

- Increased job satisfaction
- Mutual respect as a professional
- Specialisation
- Autonomy in the workplace
- Personal growth
- Career advancement in a field that has a historical "ceiling"

For the *Institution?*

- Improved MDT dynamics
- Increased efficiency
- Better use of staff skills
- Education of peers
  - Mentorship

Take Home Messages

- ***Diligent*** adverse event reporting should not be reserved for clinical trials

- ***Prospective*** data collection that is electronic and easily accessible

- Language needs to be clear for ***all*** members of the team accessing patient notes

- Better equipped to assess impact of treatment in an evidence based approach